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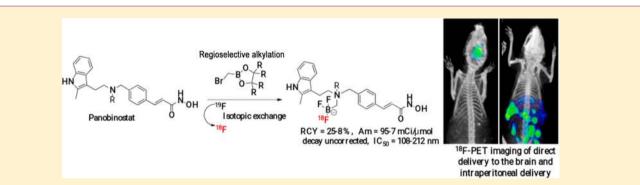
¹⁸F-Radiolabeled Panobinostat Allows for Positron Emission Tomography Guided Delivery of a Histone Deacetylase Inhibitor

Harikrishna Kommidi,[†] Umberto Tosi,[‡] Uday B. Maachani,[‡] Hua Guo,[†] Christopher S. Marnell,[‡] Benedict Law,[†] Mark M. Souweidane,[‡] and Richard Ting^{*,†}

[†]Department of Radiology, Molecular Imaging Innovations Institute, Weill Cornell Medicine, New York, New York 10065, United States

[‡]Department of Neurological Surgery, Weill Cornell Medicine, New York, New York 10065, United States

Supporting Information



ABSTRACT: Histone deacetylase (HDAC) inhibition is becoming an increasingly popular approach to treat cancer, as HDAC overexpression is common in many malignancies. The blood-brain barrier (BBB) prevents systemically delivered drugs from reaching brain at effective concentration, making small-molecule-HDAC inhibition in brain tumors particularly challenging. To circumvent the BBB, novel routes for administering therapeutics are being considered in the clinic, and a need exists for drugs whose deliveries can be directly imaged, so that effective delivery across the BBB can be monitored. We report chemistry for radiolabeling the HDAC inhibitor, panobinostat, with fluoride-18 (compound-1). Like panobinostat, compound 1 retains nanomolar efficacy in diffuse intrinsic pontine glioma (DIPG IV and XIII) cells (IC₅₀ = 122 and 108 nM, respectively), with lesser activity against U87 glioma. With a favorable therapeutic ratio, 1 is highly selective to glioma and demonstrates considerably less toxicity toward healthy astrocyte controls (IC₅₀ = 5265 nM). Compound 1 is stable in aqueous solution at physiological pH (>7 days, fetal bovine serum), and its delivery can be imaged by positron emission tomography (PET). Compound 1 is synthesized in two steps, and employs rapid, late-stage aqueous isotopic exchange ¹⁸F-radiochemistry. PET is used to image the in vivo delivery of [¹⁸F]-1 to the murine central nervous system via convection enhanced delivery.

KEYWORDS: positron emission tomography, drug delivery, glioblastoma, histone deacetylase, panobinostat, imaging

High grade brain tumors, like diffuse intrinsic pontine glioma (DIPG), have high mortality rates, are inoperable, and do not respond to chemotherapy. DIPG is especially morbid, as it appears during childhood and has a very short median survival of 1 year.¹ There are no known survivors of a DIPG diagnosis. Effective chemotherapeutics for curing DIPG do not currently exist, despite numerous clinical trials.² A recent multicenter drug screening study has identified the HDAC inhibitor panobinostat, as a compound with particular promise in the treatment of high grade glioma.³

Trials for brain cancer are traditionally performed with oral or intravenous dosing, where systemic drug delivery into the brain can be impaired by the blood-brain barrier (BBB). The high failure rate of drugs in brain tumor trials are often attributed to the impermeability of the BBB.⁴⁻⁶ Unfortunately, panobinostat bears a limited solubility and a limited ability to cross the BBB.⁷ To overcome this issue, several alternative drug

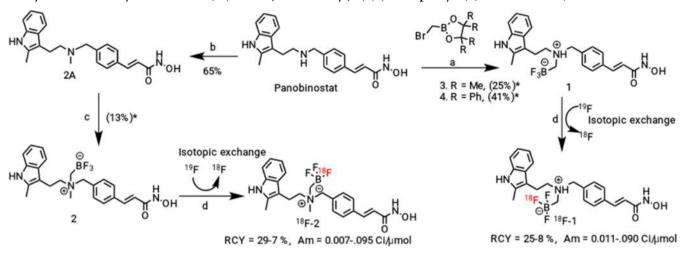
delivery strategies are being investigated, such as convection enhanced delivery (CED), transient osmotic disruption of the BBB, inhibition of membrane efflux pumps, intra-arterial, and intranasal chemotherapy.^{4–6} These interventions are new and would benefit from technologies that allow us to quantitate and monitor effective drug delivery across physiological barriers.

Positron emission tomography (PET) labeled probes that allow the evaluation of nanomolar drug distribution are an active field of research. The development of PET-labeled HDAC inhibitors include [¹⁸F]-fluoroacetamide-1-hexanoicani-lide (FAHA), [¹¹C]-MS-275,^{8–10} and [¹⁸F]-fluoroacetamide-1-hexanoicanilide hydroxamic acid (SAHA).¹¹ [¹⁸F]-panobinostat has not been described.

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Scheme 1. Syntheses of ¹⁹F-N-Ammoniomethyltrifluoroborate Panobinostat; Ammoniomethyltrifluoroborate (AMBF₃), 1; N-methyl ammoniomethyltrifluoroborate, 2; and 2-(Bromomethyl)-4,4,5,5-tetraphenyl-1,3,2-dioxaborolane, $4^{a,b}$



^{*a*}Reagents and conditions: (a) 1.1 equiv of bromomethylboronic acid pinacol ester, 1.1 equiv of DIPEA, DMF/THF (2:1), rt, 4 h, (2) 3 M KHF₂, 1 M HCl, rt, 1 h; (b) HCHO, 2.5 equiv of Na(OAc)₃BH; (c) (1) 1.1 equiv of bromomethylboronic acid pinacol ester, DIPEA, DMF/THF (2:1), rt, (2) 3 M KHF₂, 1 M HCl, 0 °C to rt, 1 h; (d) 1 M pyridazine–HCl buffer (pH = 2.5), aq ¹⁸F (1.0 mci/ μ L), 80 °C, 20–30 min. ^{*b*}RCY = radiochemical yield, Am = molar activity.

To allow researchers to quantitate advanced methods of delivery to brain tumors, we report the synthesis and radiolabeling of ¹⁸F-ammoniomethyltrifluoroborate—panobino-stat for PET-guided delivery. This ¹⁸F-fluoride bearing derivative of panobinostat differs from previously reported ¹¹C-carbon-labeled panobinostat derivatives.^{7,12} The longer half-life of ¹⁸F-fluoride ($t_{1/2} = 110$ min) allows for longer imaging sessions and is accommodative of unforeseen delays that can be common in neurosurgery. Additionally, we incorporate boron-based, aqueous fluoride capture technology onto panobinostat in a radiolabeling strategy that proceeds in one step through water-insensitive, isotopic-exchange (IE).^{13–23} Purification is performed through precipitation in a relatively simple strategy for generating ¹⁸F-radiolabeled panobinostat.

The reported synthesis of [¹⁸F]-1 describes a PET-active, chemotherapeutic drug that nearly matches the sensitivity, antitumor activities, and mechanisms of unmodified panobinostat (Farydak, Novartis) in DIPG and U87 glioma. This agent is visible by PET, allowing for quantitation of in vivo drug delivery and clearance in novel drug delivery methods, such as CED.²⁴ New drug delivery strategies are relevant, as CED is recommended for panobinostat.³

RESULTS AND DISCUSSION

Oral panobinostat (Farydak) is a HDAC inhibitor that is approved for multiple myeloma in combination with bortezomib and dexamethasone. Panobinostat is a nonselective inhibitor with multiple pathways of antitumor activity.^{7,8} Two trifluoroborate-bearing derivatives of panobinostat have been synthesized and studied (Scheme 1). The first panobinostat derivate, 1, is highly active. Compound 1 bears an *N*-trialkylsubstituted ammoniomethyltrifluoroborate. A second panobinostat derivative, 2, bears an *N*-tetraalkyl-substituted (quaternary) ammoniomethyltrifluoroborate (AMBF₃). Although 1 and 2 are structurally similar, 2 is >20-fold less active than 1 in DIPG cell lines. Compounds 1 and 2 are both generated by alkylating a secondary amine present on panobinostat.

Initial attempts for the synthesis of 1 were performed with bromomethylboronic acid tetramethylpinacol ester, 3, as an alkylating agent (a synthon previously described by Perrin et al.).¹³ Alkylation, followed by a potassium hydrogen fluoride workup (KHF₂ (1 M) in 3 M HCl), gives 1 as a minor product (25%). Yields of 1 could be improved significantly when the bromomethyl boronic acid alkylating agent is substituted for a sterically hindered bromomethyl boronic ester. Reaction of diisopropyl (bromomethyl)boronate with 1,1,2,2-tetraphenyl-1,2-ethanediol at 120 °C in toluene gives 2-(bromomethyl)-4,4,5,5-tetraphenyl-1,3,2-dioxaborolane, 4 (solid, 62% yield) (Supporting Information). Alkylation of panobinostat with 4, followed by KHF2 deprotection, gives 1 at improved yield (41%, vs tetramethylpinacol ester¹³). Indole–amine protection is not necessary in the synthesis of 1 when 4 is used as an alkylating agent. Proof of alkylation at the secondary amine (and not the indole) is demonstrated in comprehensive ¹H, ¹³C, HSQC, and HMBC NMR spectroscopy (Supporting Information). Compound 2 was synthesized from an Nmethylated panobinostat precursor. Panobinostat was alkylated through reductive amination using formaldehyde solution (37%) and sodium triacetoxyborohydride. The isolated product was reacted with bromomethyl boronate and fluoridated with KHF_2 (1 M) and HCl (3 M) in the same pot to give 2 (13%). A quaternary amine is isolated as demonstrated by comprehensive ¹H, ¹³C, HSQC, and HMBC NMR spectroscopy (Supporting Information). Product corresponding to alkylation at the indole-amine is not isolated. Compounds 1 and 2 are stable in physiological solution. Compound instability/fluoride loss/deboronation is not observed when 1 and 2 are incubated in phosphate buffered saline (1x PBS, a phosphate buffer concentrated at 10 mM, containing, 137 mM sodium chloride, pH 7.4 ± 0.2 (25 °C))/fetal bovine serum (FBS) at pH 7.4) for >7 days, in ¹⁹F-NMR stability studies^{15,25} ($t_{1/2}$ defluoridation >7 days, see the Supporting Information).

Radiochemistry. Aqueous IE based radiolabeling of 1 and 2 proceed best when small total volumes ($<50 \ \mu$ L) of ¹⁸F-fluoride-ion containing water are employed. Many cyclotrons and commercial suppliers already provide fluoride-ion-contain-

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ing water at high specific concentration (~1 mCi/ μ L). These solutions can be used as is, without concentration. Radiosyntheses are initiated (i.e., the time of synthesis (TOS) = 0min) with the addition of ~10 to 15 μ L of concentrated, but not fully evaporated, ¹⁸F-fluoride-ion-containing water to solutions of 1 and 2. Reactions are performed with ~35 mCi of radioactivity in 1500 μ L polypropylene tubes. It is recommended that one begin synthesis with at least 90 μ g of compound ¹⁹F-1 or ¹⁹F-2, dissolved in 10 μ L of DMSO. Although lesser quantities of ¹⁹F-1 or ¹⁹F-2 would improve radiosynthetic molar activity in IE experiments, these lesser auantities of ¹⁹F-1 or ¹⁹F-2 approach the solubility product constant (K_{sp}) of panobinostat in deionized water. Therefore, purification through precipitation, as described, may not be used to purify lesser quantities of $[{}^{18}F]$ -1 or $[{}^{18}F]$ -2. An acid catalyst was required to facilitate fluoride IE. As described in Liu et al.,¹³ 10 μ L of aqueous pyridazine HCl (1.25 M, pH 2.5) and heating at 80 °C for 25 min facilitate IE. Full solubility of 1

and 2 is observed upon heating. Isolation of pure $[^{18}F]$ -1 or $[^{18}F]$ -2 is achieved by removing unreacted, contaminating ¹⁸F-fluoride-ion. Room temperature deionized water (1.3 mL) is added to the labeling mixture, also at room temperature. This results in instantaneous precipitate formation. $[^{18}F]$ -1 and 2 are pelleted by centrifugation at 18000g for 1 min. Supernatant containing contaminating ¹⁸Ffluoride ion was decanted and 10 μ L of DMSO was added to fully resuspend the $[^{18}F]$ -1 and 2 containing pellet. This wash process was repeated three more times to completely remove ^{18}F -fluoride ion from $[^{18}F]$ -1 or 2. In a typical experiment, 6.2 mCi or 49 mCi/ μ mol of $[^{18}F]$ -1 and 5.5 mCi or 45 mCi/ μ mol of $[^{18}F]$ -2 are obtained as pure solids. Total synthesis time was 25 min, while purification takes 15 min.

Like panobinostat, [18F]-1 and 2 are highly insoluble in aqueous solution. $[^{18}F]$ -1 or 2 must be formulated in 1% DMSO containing 1× PBS for in vivo experiments. This formulation is compatible with direct intracranial injection.²⁶ To formulate $[^{18}F]$ -1 or 2, DMSO (~20 μ L) must first be added to the pellet, to fully solubilize [18F]-1 or 2. Subsequent addition of PBS (580 μ L) will result in a saturated 1% DMSO solution. Precipitates ($[^{18}F]$ -1 or 2) will be present and must be removed through centrifugation. Typically, $\sim 300 \ \mu$ Ci of a 4 mCi pellet (7.5%, ~ 16 nmols, 27 μ M) was solubilized in a 600 μ L a 1% DMSO 10 mM/1× PBS solution. Higher percentages of DMSO can be used to solubilize greater activities of [¹⁸F]-1 or 2, however large percentages of DMSO are not biocompatible, and pure solutions of DMSO are toxic for the central nervous system (CNS). Reversed-phase HPLC analysis was used to confirm $[^{18}F]$ -1 or 2 radiolabeling and purity (Figure 1).

In Vitro Bioactivity. Panobinostat can be alkylated at its secondary amine without affecting bioactivity.²⁷ Panobinostat (control), 1, and 2 are tested for their ability to affect the viability of DIPG-IV, DIPG-XIII, and U87 (glioblastoma) cells. Cell viability assays (CellTiter-Glo, Promega, catalog no. G7572) are performed on U87 and normal astrocytes (control) to demonstrate unmodified panobinostat bioactivity and compound selectivity toward diseased cell lines. At 48 (Figure 2) and 96 h (Supporting Figure S1), 1 demonstrates a bioactivity against DIPG cells that is similar to unmodified panobinostat (Figure 3).³ Compound 2 demonstrates significantly reduced bioactivity against all cell lines, with micromolar IC₅₀ values vs panobinostat's nanomolar values. Panobinostat, 1, and 2 are selective toward DIPG-IV and DIPG-XIII cells and

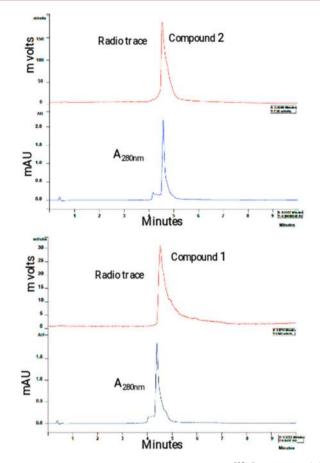


Figure 1. Radio-HPLC confirms the purity of $[^{18}\text{F}]$ -1 and 2. (B) Reversed-phase HPLC of radiolabeled $[^{18}\text{F}]$ -1 and $[^{18}\text{F}]$ -2 on a Varian HPLC equipped with a Waters SunfireTM C18 3.5 μ m 4.6 × 50 mm column (186002551), was used to demonstrate a pure synthesis of $[^{18}\text{F}]$ -1 and 2. Elution using a 10–90% H₂O/ACN (0.05% TFA), 10 min gradient with a flow rate of 2 mL/min demonstrate a pure synthesis with minimal contaminating fluoride (fluoride would appear between 0 and 1 min).

show a reduced toxicity toward U87 and normal astrocytes. Minimal bioactivity (μ M) is exhibited toward normal, nondiseased, control astrocytes across the three compounds; i.e., all three compounds show low toxicity toward astrocytes that line the normal brain parenchyma (Table 1).

The effects of panobinostat, **1**, and **2** on U87 cell proliferation are shown in Figure 3A. Panobinostat and its analogues reduce U87 cell proliferation vs normal cell control. As expected, panobinostat-mediated inhibition of proliferation was more pronounced than that of compounds **1** and **2** at 200 nM. This is consistent with cell viability data described in Figure 2.

To demonstrate that compounds 1 and 2 have an unchanged mechanism of action relative to panobinostat (i.e, panobinostat's mechanism of action is preserved despite chemical modification), DIPG Western blot histone H3 acetylation (acetyl-H3) and cell cycle analyses are performed. In Western blots (Figure 3B), panobinostat treatment induces significant H3 acetylation. This was observed in cells that are treated with 1 and 2 (100 nM, 24 h). To confirm that 1 and 2 have a mechanism of action that is unchanged from panobinostat, cell cycle analyses of panobinostat, 1, 2, and untreated U87 cells are conducted (200 nM, 48 h). U87 cell cycle arrest was similar for all 3 compounds at submicromolar concentration. As shown in

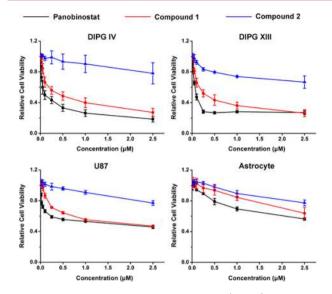


Figure 2. In vitro bioactivity of the unmodified (parent) panobinostat and its two analogues after 48-h exposure. Compound 1 has bioactivity similar to that of unmodified panobinostat against all cell lines (Table 1) and is especially active against pediatric glioma lines DIPG IV and DIPG XIII.

Figure 3C, an enhanced accumulation of sub diploid population was observed in cells either treated with panobinostat, 1 and 2, suggesting apoptosis. Panobinostat, 1 and 2, also induce significant G2/M cell cycle arrest, which is consistent with a report by Pettazzoni et al., where G2/M arrest was observed in panobinostat treated prostate cancer cells.²⁸

In Vivo Imaging. Neurooncologists and neurosurgeons recommend convection enhanced delivery (CED) for treating DIPG with panobinostat.³ Compound 1 demonstrates both nanomolar bioactivity against DIPG cells and bears a positron emitting isotope for PET imaging. These properties make compound 1 an ideal candidate for evaluating different methods of HDAC delivery in vivo. Solutions of [¹⁸F]-1 (300 μ Ci, in 1% DMSO/1× PBS) are delivered to mice through different methods, including CED,²⁶ to illustrate the use of quantitative imaging in drug delivery, [¹⁸F]-1 was delivered to naive mice by CED,²⁶ intraperitoneally (Figure 4), and intravenously (IV, not shown).

As expected, CED was the superior method for delivering large doses of [18F]-1 to the brain. In Figure 4, compound [¹⁸F]-1 was delivered at high concentration to the brain, via CED, and is retained in the brain for at least 1 h. In comparative studies where [18F]-1 was delivered intraperitoneally or intravenously, very little [18F]-1 was detected in the brain post injection,¹² even after [¹⁸F]-1 was allowed to distribute for 4 h. PET imaging also allows for dynamic monitoring of delivery and clearance. As shown in Supporting Figure S2, 2 mm diameter, elliptical, regions-of-interest (4.19 μ L, ROI) are placed over the site of injection to image drug delivery. CED was 120 times more effective at delivering $[^{18}F]$ -1 panobinostat to the pons in naïve mice. $[^{18}F]$ -1 panobinostat clears from the brain quickly. At 240 min post injection, the concentration of $[^{18}F]$ -1 remains 44.6-fold higher in the pons vs intraperitoneal injection.

DISCUSSION

In this study, we demonstrate simplified radiochemistry for transforming the HDAC inhibitor panobinostat into an agent

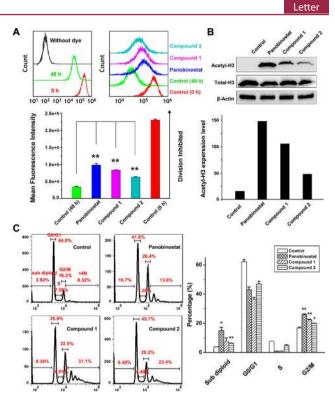


Figure 3. Assays that compare biological activity between panobinostat and its analogues (1 and 2) on U87 and DIPG biological activity. (A) Panobinostat and analogue impact on U87 cell proliferation. Cells are stained with a proliferation tracking dye (CellTraceTM Far Red) prior to treatment with 200 nM drug for 48 h. (B) Western blot analysis showing panobinostat and analogue impact on DIPG IV acetyl-H3 expression in cells. DIPG IV cells are treated with 100 nM panobinostat, 1, and 2 for 24 h and are analyzed for changes in acetyl-H3 expression. The total histone H3 (Total-H3) and β -actin content serve as controls. (C) Panobinostat and analogues impact on U87 cell-cycle. Cell cycle status was determined by staining treated cells (200 nM) with propidium iodine before fluorescence activated sorting analysis (FACS). The percentage of cells in sub diploid (apoptosis), G0/G1, S, and G2/M phases are shown in representative histograms (left) and are summarized as mean \pm SD in right. *Represents a statistically significant difference between control group and treatment group (*: p < 0.05, **: p < 0.01).

Table 1. Inhibitory Profile of Panobinostat Derivatives 1 and 2 and against Glioma Cell Lines IC_{50} (nM) after 48 h Exposure

compd	DIPG-IV	DIPG-XIII	U87	astrocytes
panobinostat	64	38	65	76
1	122	108	212	5265
2	4358	310	4483	5125

^{*a*}Mean from three different cell viability assays (standard error is in the range of $\pm 2-5\%$ of reported IC₅₀).

that can be imaged by ¹⁸F-PET. This labeled HDAC inhibitor could be used by itself or in combination with panobinostat to treat and explore new routes of drug delivery in the treatment of cancer. We look forward to using compounds 1 and 2 in identifying new routes of drug delivery, combining old routes of delivery, and in quantitatively comparing advanced strategies to standard (intravenous, peritoneal, and intradermal) modes of drug delivery. The synthesis of 1 was performed in 2 steps from commercially available panobinostat. The ¹⁸F-radiolabeling and generation of millicurie amounts of [¹⁸F]-1 is performed under

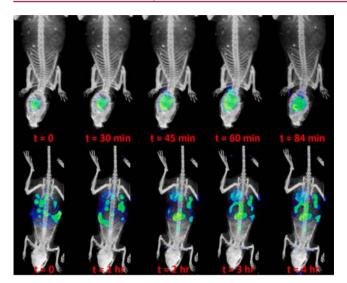


Figure 4. Panobinostat compound [¹⁸F]-1 allows for real time, *in vivo* imaging of drug delivery via CED (top) or IP delivery (bottom). The former achieves delivery of greater concentrations of panobinostat to the brain. [¹⁸F]-1 PET allows quantitation of drug delivery and clearance (see the Supporting Information) of both delivery mechanisms.

acidic, IE conditions where a nonradioactive ¹⁹F atom on compound **1** and **2** was exchanged with ¹⁸F-fluoride ion in acidic water. Compounds **1** and **2** are stable at physiological pH. In our hands, [¹⁸F]-**1** radiolabeling was infallible (a 100% success rate was observed) when reactions are performed with aqueous specific concentrations of ~1 mCi/ μ L. In employing trifluoroborate IE technology, the nonradioactive starting compound ¹⁹F-**1** is electronically identical to its radioactive ¹⁸F counterpart, therefore advanced chromatographic separation is not needed to remove precursor, and simple precipitation could be used to isolate pure samples of [¹⁸F]-**1**. Radiochemical yields and molar activities range from 96 ± 10 mCi/ μ mol (decay uncorrected). The radiochemical precursor ¹⁹F-**1** is useful in pharmacological assays (Figure 3) as is, without manipulation.

Radiochemical approaches are needed to study the accumulation of effective nanomolar anticancer drugs at the site of disease. These approaches would allow immediate determination of accurate drug delivery and clearance, providing crucial data in redosing. Using [¹⁸F]-1, cases of missed HDAC delivery can be immediately recognized by PET/CT or PET/MR, allowing for prompt intervention in the case of failed or inaccurate delivery. Currently, real-time imaging is not used to confirm drug delivery. Without drugs like [¹⁸F]-1, inaccurate drug delivery cannot be immediately recognized. One would currently realize drug misdelivery by observing significant disease progression, after the window for meaningful intervention has passed.²⁹ By imaging delivery will no longer be incorrectly interpreted as a lack of drug efficacy.

CONCLUSIONS

Here, we report the synthesis and radiolabeling of a nanomolar analog of panobinostat that bears ¹⁸F-fluoride, allowing the delivery of $[^{18}F]$ -1 to be imaged by PET. Like the parent drug, panobinostat, 1 is found to inhibit the growth of DIPG IV, XIII, and U87 cells at nanomolar concentration, while leaving normal

astrocytes unaffected. A close structural analog 2, does not demonstrate the same inhibitory activity. Compound 1 is relevant because of its newfound importance in glioma.³ The use of [¹⁸F]-1 in PET allows for noninvasive, quantitative, image-guided HDAC inhibitor delivery at high resolution.³⁰ PET imaging would promptly identify cases of missed or inadequate HDAC inhibitor delivery in a patient.

ASSOCIATED CONTENT

S Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsmedchem-lett.7b00471.

Methods for panobonostat–AMBF₃ preparation, characterization, in vitro stability verification, and in vivo data (PDF)

AUTHOR INFORMATION

Corresponding Author

*E-mail: rct2001@med.cornell.edu. Phone: (+1) (646) 962-6195.

ORCID 🔍

Umberto Tosi: 0000-0003-0847-2400 Richard Ting: 0000-0003-2096-5232

Author Contributions

The manuscript was written through contributions of all authors. All authors have given approval to the final version of the manuscript.

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Notes

The authors declare no competing financial interest.

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ABBREVIATIONS

AMBF₃, alkylammoniomethyltrifluoroborate; CED, convention enhanced delivery; HDAC, histone deacetylase; PET, positron emission tomography; CT, computed tomography; DIPEA, N,N-diisopropylethylamine; EDCI, 1-ethyl-3-(3-(dimethylamino)propyl)carbodiimide

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