

Article A Green Approach for the Synthesis of Silver Nanoparticle-Embedded Chitosan Bionanocomposite as a Potential Device for the Sustained Release of the Itraconazole Drug and Its Antibacterial Characteristics

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Abstract: The present research work intended to demonstrate the green synthesis of silver nanoparticles (AgNPs) using the plant extract *Saccharum officinarum*, and then the development of chitosansilver (CH-Ag) bionanocomposite. The synthesized AgNPs were characterized using UV spectroscopy, Fourier transform infrared (FTIR), and transmission electron microscopy (TEM). The maximum absorption spectrum peak was observed at 420 nm, revealing the formation of AgNPs by the stem extract of *S. officinarum*. The AgNPs sizes were in the range of 10–50 nm. Itraconazole is an antifungal that is used as a novel drug to study its release through synthesized bionanocomposite. Different kinetic models, such as zero order, first order, Korsmeyer–Peppas, Hixson–Crowell and Higuchi, were used to study the drug release profile from the synthesized CH-Ag bionanocomposite. The first-order kinetic model showed the best fit for the drug release with the maximum regression coefficient value. The antibacterial activity of the synthesized CH-Ag bionanocomposite was examined against *Bacillus cereus, Staphylococcus*, and *Escherichia coli*, and it was shown to be efficient against these strains.

Keywords: *Saccharum officinarum*; silver nanoparticles; chitosan; bionanocomposite; antibacterial activity

1. Introduction

The recent years have observed remarkable growth in research and applications in the areas of nanotechnology and nanoscience. Nanotechnology has been utilized in different fields, such as environmental, health care, chemical industries, photo-electrochemical applications, etc. Nanobiotechnology provides methods for the nontoxic and environmentally friendly synthesis of metal nanoparticles [1–3]. Silver nanoparticles (AgNPs) possess numerous anti-inflammatory and anti-bacterial properties that facilitate quick wound healing. Additionally, silver nanoparticles can be used for wound dressings, medical implants, pharmaceutical preparations, and biomedical applications. Nanoparticles possess a high surface area-to-volume ratio, making them excellent catalysts [4–7].

Globally, sugarcane is the leading sugar crop. In addition to liquids, syrups, and capsules, sugarcane is essential for preserving various kinds of medicine. It is an excellent source of energy drinks [8–10]. Triazoles are the first-line managers for the preclusion



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and cure of persistent and allergic fungal infections. Itraconazole (cis-4[4-4-4[[2-(2-4-dichlorophenyl)-2-(1H-1,2,4,triazol-1-methyl)-1,3-dioxolan-4-yl]-1-piperazinyl]phenyl]-2,4-dihydro-2-(1-methyl-propyl)-3H-1,2,4-triazol-3-one) was initially synthesized in 1980, and has broad-spectrum antifungal activity (especially in filamentous fungi, such as *Aspergillus* spp.), potency and toxicity profiles, because of the presence of the triazole ring in the side chain, which makes it very active. It acts as an anti-allergic agent, and is used for the treatment of aspergillosis, candidiasis, dermatophyte infections, sporotrichosis, blastomycosis, histoplasmosis, etc. [11–13]. Chitosan is a natural polysaccharide, which is a cationic copolymer and is hydrophilic in nature. It is biocompatible, as well as biodegradable, and for that reason it is widely used in the pharmaceutical and food industries [14].

This study targets the green synthesis of AgNPs using the plant extract *Saccharum officinarum* and the synthesis of chitosan–Ag-based bionanocomposites. The antifungal drug itraconazole was released under controlled conditions using CH-Ag nanocomposites. A number of bacterial strains were also tested for the antibacterial activity of the CH-Ag bionanocomposite, including *Bacillus cereus, Staphylococcus,* and *Escherichia coli.*

2. Materials and Methods

2.1. Materials

Sugarcane was taken from Nakodar co-operative sugar mill (NCSM), Gaggarwal Village, Mehatpur Road, Nakodar, Jalandhar, Punjab, India Silver nitrate (AgNO₃) (AVARICE, ISO 9001:2015, Ghaziabad, India) and chitosan (C₆H₁₁NO₄)n (AVARICE, ISO 9001:2015, Ghaziabad, India) were used as received; itraconazole was gifted by the pharmaceutical industry (Cipla Pvt. Ltd. Baddi, India). Erythromycin and ampicillin were purchased from (MP Biomedia, Maharashtra, India).

2.2. Methods

2.2.1. Preparation of Sugarcane Extract

A small sugarcane stem was cut into slices and washed properly in distilled water. After that, 10.0 g of small sugarcane slices were crushed properly in the pestle and mortar. The extracted organic material was filtered on Whatman no. 1 filter paper (Figure 1).



Figure 1. Pictorial presentation of extraction of sugarcane extract from sugarcane.

2.2.2. Green Synthesis of AgNPs

The synthesis of AgNPs was achieved by putting 90 mL of a 1 mM silver nitrate solution in a reaction flask and stirring it with 10 mL of sugarcane extract. During incubation, the reaction mixture was maintained at 37 °C. After the sugarcane extract was added, the solution changed color from pale yellow to brown. This is a clear indication that silver nanoparticles were forming (Figure 2) [15–18].



Figure 2. Synthesis of AgNPs using sugarcane extract.

2.2.3. Synthesis of AgNP-Embedded Chitosan (CH-Ag) Bionanocomposite

AgNP-embedded chitosan (CH-Ag) bionanocomposite was prepared by placing 1g of chitosan in a reaction flask. To this, 0.5 mL of acetic acid was added, followed by the addition of 50 mL of distilled water. This dissolved the chitosan powder properly in the reaction flask. Then, 1.0 mM of silver nitrate was added to the reaction flask while stirring using a magnetic stirrer. The formed suspension was kept for 2 h and then 10 mL of *S. officinarum* extract was added. In the present study, sugarcane was used as a stabilizing and reducing agent. The main function of using the reducing agent for the synthesis of NPs is to reduce what is present in the metal salts to atoms. In the sugarcane leaf extract, there are phenolic compounds present, which act as reducing agents for the synthesis of AgNPs from its precursor. After the addition of *S. officinarum* stem extract, the color of the reaction solution changed from pale yellow to brown, indicating the formation of AgNPs in the suspension (Figure 2). The formed reaction solution was then centrifuged at 10,000 rpm for 10 min. The attained filtrate was washed with double distilled water. The formed pellets were dried in a hot air oven and used for advanced studies [19–21].

2.3. Characterization of AgNPs

The synthesized AgNPs were analyzed by a UV–Vis spectrophotometer (MODEL LT-29). Transmission electron microscopy (TEM) utilizes energetic electrons, which provide the morphological nature of AgNPs. TEM was performed at Punjab Agriculture University, Ludhiana, Punjab, India. Fourier transform infrared (FTIR) analysis of the synthesized materials was performed at NIT Jalandhar, Punjab, India.

2.4. Drug Loading

The drug carrier device should have a high drug-loading capacity, so that a lesser quantity of matrix materials is required for administration. There are two methods for drug loading:

- Incorporation of the drug at the time of nanoparticle synthesis;
- Imbibing the drug after the formation of nanoparticles.

In the present work, the itraconazole drug was loaded in synthesized bionanocomposite using the swelling–diffusion method. Synthesized bionanocomposite (0.5 g) was immersed in the drug solution (0.2 mg/mL). It was incubated at 37 °C for 48 h. After 48 h, drug-loaded bionanocomposites were taken out and washed with double distilled water to remove any surface-adhered drug particles. After washing, the sample was kept in a hot air oven at 45 °C until it was dried. The drug release behavior was studied with the help of a double-beam UV–VIS spectrophotometer. Drug entrapment efficiency (*EE*) was calculated using the following equation [22–25]:

$$EE(\%) = \left(\frac{W_f}{W_o}\right) \times 100\tag{1}$$

In this equation, W_f and W_o are the total amount of drug in the solution before loading and after loading, respectively.

2.5. In Vitro Drug Release Studies

Phosphate buffer solution was prepared in distilled water using di-sodium hydrogen phosphate and sodium di-hydrogen phosphate, and the pH of the solution was maintained at 2, 7 and 9.2 with the help of 1 M NaOH. Drug release was studied at pH 2, 7 and 9.2, which corresponds with the pH of gastric fluid, blood stream and intestinal fluid, respectively. Drug release through CH-Ag bionanocomposite was deliberated by immersing the drug-loaded bionanocomposite in different pH solutions at a temperature of 37 °C. Drug release concentration in the solution was studied every one hour using a double-beam UV–VIS spectrophotometer [26–29].

2.6. Mechanism of Drug Release

Drug release behavior of the synthesized bionanocomposite was studied using the power law equation, which is expressed as [30–33]:

$$\frac{M_t}{M_{\infty}} = kt^n \tag{2}$$

where M_t/M_{∞} is the drug release at time *t*, and *k* and *n* are the rate constant and diffusion exponent of drug release, respectively. The *n* value showed the type of drug release mechanism. The drug release experiments were conducted in triplicate, so as to avoid any error. Drug diffusion mechanism is explained by Fick's first and second laws, as follow:

λ

λ

$$A_s = kt^n \tag{3}$$

where *k* and *n* are gel characteristic constant and diffusion exponent, respectively. Further, n = 0.5, 0.5 to 1, and 1 or >1 signify a Fickian, non-Fickian, and case II diffusion mechanism, respectively. Fick's power law equation was used to calculate the drug release via synthesized CH-Ag bionanocomposite.

$$\Lambda_t / M_\infty = k t^n \tag{4}$$

where M_t and M_{∞} are the fractional release of the drug at different time intervals and at equilibrium, respectively. The value of n and k are obtained from the slope and intercept of the plot between M_t/M_{∞} and lnt.

Initial diffusion coefficient (D_i) was calculated using the following equation:

$$M_t/M_\infty = 4 \times D_i/\pi l^2 \tag{5}$$

where *l* is the thickness of the IPN sample used.

Average diffusion (D_A) was calculated from the following equation:

$$D_A = 0.049 l^2 / t^{1/2} \tag{6}$$

where $t_{1/2}$ is the time required for 50% release of the drug.

Lateral diffusion coefficient (D_L) was calculated via the slope of the plot between $\ln(1 - M_t/M_{oo})$ and time.

$$D_L = (\text{slope } l^2/8) \tag{7}$$

2.7. Kinetics of Drug Release

The kinetics of drug release from the CH-Ag bionanocomposite was studied by finding the best fit on the kinetic models, such as zero order(Equation (8)), first order (Equation (9)), Higuchi model (Equation (10)), Korsmeyer–Peppas model (Equation (11)) and Hixson–Crowell model (Equation (12)) [34–36].

$$\frac{M_t}{M_{\infty}} = k_0 t \tag{8}$$

$$\ln(1 - \frac{M_t}{M_{\infty}}) = -k_1 t \tag{9}$$

$$\frac{M_t}{M_{\infty}} = k_2 t^{\frac{1}{2}} \tag{10}$$

$$\frac{M_t}{M_{\infty}} = k_3 t^n \tag{11}$$

$$\sqrt[3]{Q_o} - \sqrt[3]{Q_t} = k_4 t$$
 (12)

In these equations, t is the drug release time, n represents the release exponent, and Q_0 and Q_t are the amount of drug loaded and drug release at time t in the synthesized bionanocomposite, respectively. k_0 , k_1 , k_2 , k_3 and k_4 are rate constants of the drug release of different kinetics models.

3. Results and Discussion

3.1. Characterization

3.1.1. TEM Analysis

The morphology and size of the synthesized AgNPs were studied using an JEOL-JEM-2100 transmission electron microscope (TEM). The TEM sample was prepared by placing the sample onto a carbon film, supported on a copper grid, followed by solvent evaporation under vacuum. The TEM images of AgNPs synthesized by *S. officinarum* are shown in (Figure 3a,b), which reveal the formation of AgNPs produced by *S. officinarum*. It was revealed, from the results, that there were stabilizing agents around the AgNPs ('N' depicted NPs and 'S' depicted the stabilizing agents). As was clear from Figure 3a,b, the presence of large sums of sucrose in *S. officinarum* might be accountable for the reduction and stabilizing of AgNPs.



Figure 3. TEM images (100 nm scale bar) of AgNPs synthesized by *S. officinarum* extract: (**a**) AgNPs surrounded by stabilizing agents and (**b**) AgNPs.

The phytochemicals in the *S. officinarum* extract entailed in NPs synthesis were identified by FTIR. The FTIR spectrum of the synthesized AgNPs is shown in Figure 4. The peaks at 3937 cm⁻¹ and 3271 cm⁻¹ are due to the H-OH stretching of phenols. The reducing sugars of the *S. officinarum* extract might be acting as reducing agents to synthesize AgNPs. The adsorption peak at 1629 cm⁻¹ is due to the C=O stretching of aldehydes and ketones. The peak at 1519 cm⁻¹ corresponds to the N=O bending of nitro groups. The bands observed at 1446 cm⁻¹ and 1396 cm⁻¹ represent the C-O stretching of esters. The peaks at 1229, 1043 and 461 cm⁻¹ correspond to the C-H stretching of alkenes.



Figure 4. FTIR spectrums of AgNPs synthesized by S. officinarum extract.

3.1.3. Visual Observation

The production of NPs from plant extracts is gaining significant interest, due to the low production cost and eco-friendly nature. A color change is an indication of the synthesis of AgNPs using biological materials [34–36]. After the addition of *S. officinarum* extract to the silver nitrate solution, there is a change in the color of the solution, which is an indication of the formation of AgNPs. The appearance of a brown color occurred within 5 min after the addition of *S. officinarum* extract, and the intensity of the brown color increased with time, and it attained a constant color after 12 h (Figure 5b). This change in the color was due to the excitation of surface plasmon resonance (SPR) of the synthesized AgNPs. Silver nitrate was treated as the control (Figure 5a). After 12 h, the change in colour from white to dark brown indicate the synthesized silver nanoparticles indicates the complete reduction of silver metal ions into silver nanoparticles, the color changed from white to brown.

The time-dependent visible spectra of AgNPs with *S. officinarum* aqueous leaf extract are shown in Figure 6. The visible spectra of AgNPs were recorded at different time intervals, from 0 h (initiation of reaction) to 12 h (Table 1). It was clear from the absorption results that after the addition of *S. officinarum* extract to silver nitrate, the intensity of the peak gradually increased with an increase in the reaction time from 0 to 12 h, which indicated that there was an increase in the concentration of silver nanoparticles in the reaction mixture with the passage of time.



Figure 5. Visual examination of the synthesis of AgNPs: (**a**) silver nitrate solution without *S. officinarum* extract and (**b**) after the addition of *S. officinarum* extract to silver nitrate solution.



Figure 6. Absorbance of AgNPs synthesized by S. officinarum extracts at different time intervals.

Time (h)	Absorbance
0	0.356
1	0.569
2	0.781
3	0.954
4	1.114
5	1.217
6	1.423
7	1.586
8	1.715
9	1.8
10	1.892
11	1.915
12	1.937

Table 1. Visual observation of AgNPs with time.

3.2. Drug Loading and Release Studies

The drug entrapment efficiency of the synthesized bionanocomposite depends upon the physical and chemical nature and interaction of the drug and synthesized bionanocomposite. In this research work, itraconazole was used as a model drug. The results of drug entrapment efficiency in varied media are represented in Table 2. The higher EE of drugs was found in pH 7, followed by alkaline and acidic media. The results showed that synthesized bionanocomposite is very efficient for the entrapment of the drug, and can be utilized as a device for drug delivery [37,38].

Table 2. Itraconazole drug entrapment efficiency onto synthesized CH-Ag bionanocomposite at different pH.

Druge	pH 2 pH 7		рН 9.2			
Diugs	Drug Entrapment Efficiency (EE) %					
Itraconazole	64.12 ± 0.10	94.56 ± 0.11	75.03 ± 0.09			

In vitro drug release, through synthesized CH-Ag bionanocomposite, was studied at pH 2, 7 and 9, as they provide the same physiological conditions as the gastric, blood stream and intestine, respectively. The drug release behavior through the synthesized CH-Ag bionanocomposite is given in Figure 7, which shows that the maximum drug release was found at pH 7 (93%), followed by pH 9.2 (79%), and the minimum was found at pH 2 (61%) (Figure 7) [39–41].The release behavior of the drug from the synthesized bionanocomposite was sustained release, without any burst. The interactions between the bionanocomposite and drug molecules lead to the prolonged and sustained release of the drug [42–44].

As the synthesized bionanocomposite matrix comes into contact with the aqueous solution, it starts to achieve a swollen state, where diffusion of the drug molecules takes place from the porous network of the CH-Ag bionanocomposite to the outer medium. Drug release from the CH-Ag bionanocomposite takes place by a diffusion mechanism. The values n and k for the release of itraconazole from the CH-Ag bionanocomposite were taken from the slope and intercept of the plot of M_t/M_{∞} versus t in different pH conditions. The results of itraconazole clearly depicted that the drug release from the CH-Ag bionanocomposite followed a non-Fickian diffusion mechanism at pH 7, while it showed a Fickian mechanism in acidic and alkaline medium [44,45]. Drug release in a Fickian diffusion mechanism is controlled by concentration gradient-driven diffusion, and

in the case of a non-Fickian diffusion mechanism, it is driven by polymer relaxation. Di were found to be higher than D_L (Table 3). The diffusion coefficient was higher at pH 7, demonstrating that drug diffusion was higher at a neutral pH, due to higher swelling in the network of the CH-Ag bionanocomposite at a neutral pH, followed by an alkaline and an acidic pH, respectively.



Figure 7. Effect of pH on release of itraconazole from CH-Ag bionanocomposite at different time intervals.

Table 3. Diffusion exponent 'n', gel characteristic constant 'k'and diffusion coefficient of itraconazole drug release through CH-Ag bionanocomposite at different pH.

Drug	pН	Drug Release (mg) Itraconazole		'n'	'k'	Diffusion Coefficient (cm^2h^{-1})			Mechanism
		Initial	Final	- 11	ĸ	Di	D _A	DL	
	2	0.75	9.2	0.462	1.431	0.176	0.021	0.08	Fickian
Itraconazole	7	1.14	14.3	1.064	1.256	0.329	0.189	0.094	Non-Fickian
	9.2	0.89	11.45	0.492	1.123	0.297	0.079	0.091	Fickian

Varied kinetic models were used to study the in vitro drug release behavior. Different kinetics equations (8–12) were used for the linear plotting of drug release, as shown in Figures 8a–c and 9a–e, producing the values of regression coefficient and rate constant. Drug release models were assessed from the values of the regression coefficient of the linear relationship between the releases of the drug at different times. The drug release results of different kinetic models are summarized in Table 4. The drug release profile corresponded best with the first-order kinetic model, having the highest regression coefficient value (Table 4). The first-order kinetic model of drug release from the synthesized CH-Ag bionanocomposite depicted a time-dependent profile, where the drug release rate constant depended upon the initial concentration of the drug present in the bionanocomposite [45,46].



Figure 8. Plot of (a) $\ln (M_t/M_{\infty})$ vs. ln t; (b) $\ln(1 - M_t/M_{\infty})$ vs. time and (c) M_t/M_{∞} vs. $t^{1/2}$ for the release of itraconazole from synthesized CH-Ag bionanocomposite.



Figure 9. (a) Plot of M_t/M_{∞} vs. time; (b) plots of M_t/M_{∞} vs. t^n (n = 0.54) at pH 7; (c) plots of M_t/M_{∞} vs. t^n (n = 0.53) at pH 2; (d) plots of M_t/M_{∞} vs. t^n (n = 0.53) at pH 9.2; and (e) plot of root cube of $\sqrt{Q_o} - \sqrt{Q_t}$ vs. time for the release of itraconazole from the synthesized CH-Ag bionanocomposite.

Drug	Kinetic Model		pH 2	pH 7	pH 9.2
Itraconazole	Zero order	R ²	0.769	0.929	0.842
	Zelo oldel	$k_0 \ (mg \ h^{-1})$	0.102	0.181	0.135
	First order	R ²	0.994	0.999	0.997
		k_1 (h ⁻¹)	0.163	0.192	0.187
	Higuchi	R ²	0.936	0.954	0.949
		$k_2 (h^{-1/2})$	0.489	0.672	0.598
	Korsmeyer–Peppas	R ²	0.967	0.993	0.982
		$k_3 (h^{-n})$	0.479	0.596	0.501
	Hixson–Crowell	R ²	0.714	0.798	0.752
		k_4 (h ^{-1/3})	0.132	0.167	0.149

Table 4. Kinetic interpretation of different models for the release of itraconazole from CH-Ag bionanocomposite.

3.3. Antibacterial Activity of AgNPs and CH-Ag Bionanocomposite

Bacterial infections are always a concern for the researcher, and extensive research is ongoing to find new antimicrobial drugs isolated from different sources. The present work utilized the synthesized AgNPs and CH-Ag bionanocomposite as an alternative to the antibacterial drug, as they have the capacity to be used against resistant bacteria [47,48]. The antibacterial activity of AgNPs and CH-Ag bionanocomposite was analyzed through the agar well diffusion method against *Bacillus cereus*, *Staphylococcus*, and *Escherichiacoli*. Erythromycin and ampicillin are antibiotics, which were used as the control. A single colony of bacterial strain was grown in a nutrient broth and incubated at 37 °C for 24 h. After incubation, each bacterial strain was spread onto the sterile agar plates. Then, the CH-Ag bionanocomposite (50 ppm) was poured in the well and the plates were incubated again at 37 °C for 24 h. After incubation, the zone of inhibition was measured. The zone of inhibition was found to be 10 mm, 11 mm, 11 mm and 9 mm in *Bacillus cereus*, *Staphylococcus*, and *Escherichiacoli*, respectively (Figure 10a–c). Thus, it is clear from the results that synthesized AgNPs and CH-Ag bionanocomposite are potentially very effective against different strains of bacteria [49,50].





Figure 10. Antibacterial activity of NPs and CH-Ag bionanocomposite against (**a**) *Bacillus cereus,* (**b**)*Staphylococcus,* and (**c**) *Escherichia coli* by agar well diffusion method.

4. Conclusions

An environmentally friendly method was used to synthesize the silver nanoparticles using *Saccharum officinarum* plant extracts, and then form CH-Ag bionanocomposite. The AgNPs were found to have a size between 50 and 100 nm. The synthesized CH-Ag bionanocomposite was then evaluated as a tool to determine the release profile of drugs, such as itraconazole, at different pH levels (pH 2, 7, and 9). It was clear from the results that drug release from the CH-Ag bionanocomposite occurred in a sustained manner. The maximum drug release occurred at pH 7, followed by pH 9.2, and the minimum drug release occurred at pH 2. The drug release followed a non-Fickian diffusion mechanism at neutral pH, and a Fickian diffusion mechanism at pH 2 and 9.2. The release profiles of the drug were best fitted in the first-order kinetic model. The synthesized CH-Ag bionanocomposite has been shown to be effective against different bacterial strains, including *Bacillus cereus, Staphylococcus*, and *Escherichia coli*. Hence, from the foregoing discussion, it can be concluded that

the synthesized CH-Ag bionanocomposite could be a potential drug delivery device with controlled and site-specific delivery.

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