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## **A Neural Signature of Regularity in Sound is Reduced in Older Adults** — [Source link](#)

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26

## Abstract

Sensitivity to repetitions in sound amplitude and frequency is crucial for sound perception. As with other aspects of sound processing, sensitivity to such patterns may change with age, and may help explain some age-related changes in hearing such as segregating speech from background sound. We recorded magnetoencephalography to characterize differences in the processing of sound patterns between younger and older adults. We presented tone sequences that either contained a pattern (made of a repeated set of tones) or did not contain a pattern. We show that auditory cortex in older, compared to younger, adults is hyperresponsive to sound onsets, but that sustained neural activity in auditory cortex, indexing the processing of a sound pattern, is reduced. Hence, the sensitivity of neural populations in auditory cortex fundamentally differs between younger and older individuals, overresponding to sound onsets, while underresponding to patterns in sounds. This may help to explain some age-related changes in hearing such as increased sensitivity to distracting sounds and difficulties tracking speech in the presence of other sound.

**Keywords:** magnetoencephalography, regularity processing, aging, hyperexcitability, auditory pattern; hearing loss

50

## Introduction

51 Many adults aged 50 or older experience challenges understanding speech in the presence of  
52 background sound (Pichora-Fuller, 2003; Pichora-Fuller et al., 2016), but the underlying neural sources  
53 contributing to such deficits are not fully understood. Speech contains rich, regular patterns, such as  
54 quasi-regular amplitude fluctuations at 4–5 Hz (Rosen, 1992; Varnet et al., 2017), and perceptual  
55 sensitivity to sound pattern and speech-in-noise perception correlate with each other (Holmes and  
56 Griffiths, 2019), suggesting shared mechanisms (Holmes et al., 2021). The perceptual processes through  
57 which sensitivity to such patterns may contribute to speech perception likely include the segregation of  
58 unique, concurrent sound streams (Schröger, 2005, 2007; Snyder and Alain, 2007; Winkler et al., 2009;  
59 Bendixen, 2014) and the recognition and prediction of relevant sound features (Jones and Boltz, 1989;  
60 Nobre et al., 2007; Henry and Herrmann, 2014; Nobre and van Ede, 2018). The current study is  
61 concerned with the degree to which patterns are represented in the brains of older individuals and  
62 whether neural sensitivity to patterns differs between younger and older adults.

63 Sustained neural activity is a DC response evident in cortical electroencephalography (EEG) in  
64 response to regular auditory patterns (Barascud et al., 2016; Southwell et al., 2017; Herrmann and  
65 Johnsrude, 2018a). This response manifests as soon as a pattern, such as repetition of a set of tones, is  
66 present (Southwell et al., 2017; Herrmann and Johnsrude, 2018a; Southwell and Chait, 2018). It also  
67 manifests for spectrally coherent chord fluctuations (Teki et al., 2016), complex sounds made of  
68 isochronous tone sequences (Sohoglu and Chait, 2016), and repeated amplitude or frequency  
69 modulations (Gutschalk et al., 2002; Ross et al., 2002; Herrmann and Johnsrude, 2018a; Herrmann et  
70 al., 2019). Sustained activity increases with the degree of regularity of a pattern, for example, with  
71 increasingly coherent frequency modulation in sounds (Teki et al., 2016; Herrmann and Johnsrude,  
72 2018a).

73 Accumulating evidence suggests that aging and age-related hearing loss are associated with a  
74 loss of inhibition throughout the auditory pathway following peripheral decline (Caspary et al., 2008;  
75 Rabang et al., 2012; Ouellet and de Villers-Sidani, 2014). This may render neurons in the aged auditory  
76 system hyperresponsive to sound (Hughes et al., 2010; Alain et al., 2012; Bidelman et al., 2014; Overton  
77 and Recanzone, 2016; Presacco et al., 2016a, b; Herrmann et al., 2018) and shorten the time it takes for  
78 neurons to regain responsiveness following adaptation to sound (de Villers-Sidani et al., 2010; Mishra et

79 al., 2014; Herrmann et al., 2016; Herrmann et al., 2019). Changes in inhibition, responsivity, and  
80 adaptation associated with aging and hearing loss likely affect all aspects of hearing (Herrmann and  
81 Butler, 2020), including sensitivity to sound patterns.

82         Some initial evidence suggests that sustained neural activity may be reduced in older compared  
83 to younger people. Many years ago, Pfefferbaum and colleagues (1979) demonstrated that sustained  
84 activity elicited by a short sine tone is reduced for older compared to younger adults. More recent work  
85 indicates that younger individuals exhibit pattern-related sustained activity in response to amplitude-  
86 modulated sounds, whereas older adults do not appear to, although the difference between these  
87 groups was not significant (Herrmann et al., 2019). Another study yielded data suggestive of reduced  
88 sustained activity in older compared to younger people in response to repeated tone sequences (Al Jaja  
89 et al., 2020), but stimulus parameters differed between age groups in this paper. A controlled  
90 experiment is thus required to elucidate whether sustained neural activity to regular sound patterns  
91 differs between younger and older people.

92         Previous work investigating sustained neural activity in older adults has utilized low-density  
93 electroencephalography (EEG; <20 electrodes; Pfefferbaum et al., 1979; Herrmann et al., 2019; Al Jaja  
94 et al., 2020). This type of EEG is not very well suited for the localization of neural sources generating  
95 scalp-recorded signals. Magnetoencephalography (MEG) typically allows for better source  
96 reconstruction than EEG, because magnetic fields are less distorted by the skull and scalp than the EEG-  
97 recorded electric potentials (Hämäläinen et al., 1993; Hämäläinen and Hari, 2002). Previous MEG source  
98 localizations in younger adults suggest that the auditory cortex underlies sustained neural activity  
99 (Pantev et al., 1994; Pantev et al., 1996; Gutschalk et al., 2002; Ross et al., 2002; Okamoto et al., 2011;  
100 Barascud et al., 2016; Teki et al., 2016) and that additional brain regions in parietal cortex, frontal cortex,  
101 and hippocampus may also contribute (Tiitinen et al., 2012; Barascud et al., 2016; Teki et al., 2016).  
102 Whether the neural sources of pattern-related sustained activity differ between younger and older  
103 adults is unknown.

104         In the current study we record MEG from younger and older adults while they listen to sound  
105 sequences. Sequences were made by taking pure tones at different frequencies and either repeating  
106 the same small set of these in the same order, so that a regular pattern is heard, or by presenting them  
107 pseudo-randomly so that no pattern is present. We investigate whether sustained neural activity to a

108 regular sound pattern differs between younger and older individuals. We also examine whether auditory  
109 cortex is generally more responsive to sound in older, compared to younger adults, as has been  
110 previously reported (Bidelman et al., 2014; Herrmann et al., 2018).

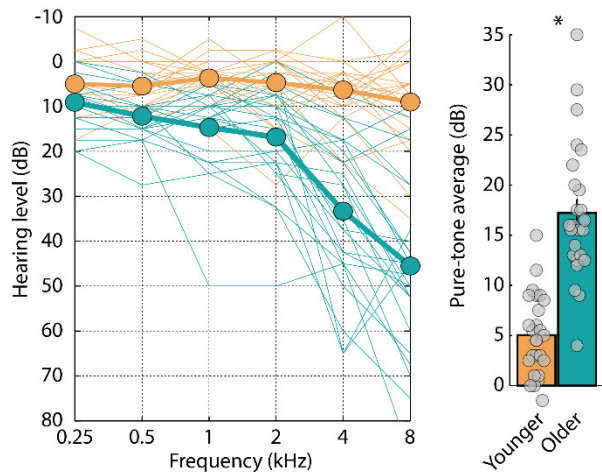
## 111 **Methods and Materials**

### 112 ***Participants***

113 Twenty-six younger (mean: 26.7 years; range: 21–33 years; 13 male) and twenty-five older adults (mean:  
114 63.9 years; range: 53–73 years; 11 male) participated in the current study. Participants reported no  
115 neurological disease or hearing impairment, gave written informed consent, and were paid for their  
116 participation. None of the participants wore a hearing aid or reported having been prescribed a hearing  
117 aid. We focused on a typical sample of older individuals, allowing for the possibility of some degree of  
118 hearing impairment. The study was conducted in two sessions on separate days (range: 1-43 days apart;  
119 median: 7 days apart; no age-group difference:  $t_{49} = 0.99$ ,  $p = 0.327$ ). The study was conducted in  
120 accordance with the Declaration of Helsinki, the Canadian Tri-Council Policy Statement on Ethical  
121 Conduct for Research Involving Humans (TCPS2-2014), and was approved by the local Nonmedical  
122 Research Ethics Board of the University of Western Ontario (protocol ID: 106570).

### 123 ***Hearing assessment and hearing thresholds***

124 Pure-tone audiometric data were acquired for each participant (Figure 1). The pure-tone average  
125 hearing threshold (i.e., the mean across the 0.25, 0.5, 1, 2, and 4 kHz frequencies) was larger for older  
126 compared to younger adults ( $t_{49} = 7.79$ ,  $p = 4 \times 10^{-10}$ ,  $r_e = 0.744$ ; Figure 1, right). This indicates a mild-to-  
127 moderate hearing impairment in many of the older adults and is consistent with the high-frequency  
128 sloping loss characteristic of age-related hearing impairment (Moore, 2007; Plack, 2014) as well as with  
129 previous electrophysiological studies that investigated differences in sound processing between younger  
130 and older adults (Presacco et al., 2016a; Herrmann et al., 2018).



**Figure 1: Audiograms and pure-tone average hearing threshold.** Left: Audiograms for each participant. Thin lines reflect individual participant data. Thick lines reflect the mean across participants. Right: Pure-tone average hearing threshold (mean across 0.25, 0.5, 1, 2, and 4 kHz). Gray dots reflect the threshold for individuals.

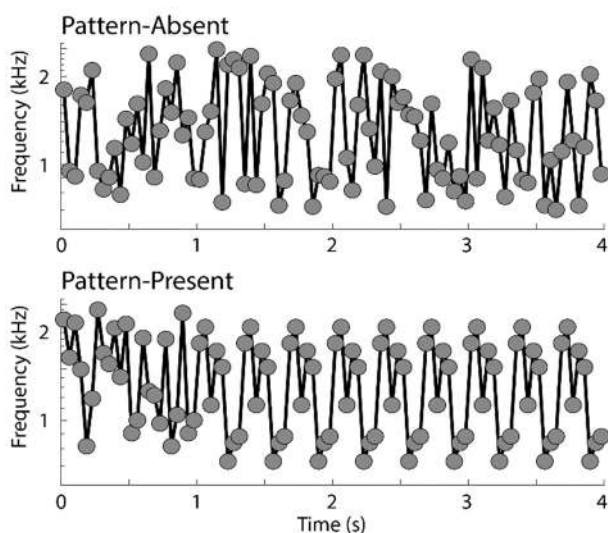
131 For each participant, we measured the hearing threshold (i.e., sensation level [SL]) using a  
132 method-of-limits procedure (Herrmann and Johnsrude, 2018b; Herrmann et al., 2019) as a reference  
133 threshold in MATLAB software for sound presentation. Participants listened to a 12-s pure tone with a  
134 frequency of 1323 Hz that changed continuously in intensity at a rate of 5 dB/s (either decreased [i.e.,  
135 starting at suprathreshold levels] or increased [i.e., starting at subthreshold levels]). Participants pressed  
136 a button when they could no longer hear the tone (intensity decrease) or when they started to hear the  
137 tone (intensity increase); the sound stopped after button press. The sound intensity at the time of the  
138 button press was noted for 6 decreasing sounds and 6 increasing sounds (decreasing and increasing  
139 sounds alternated), and these were averaged to determine the individual hearing threshold. The mean  
140 hearing threshold was elevated for older compared to younger adults ( $t_{49} = 5.208$ ,  $p = 3.7 \times 10^{-6}$ ,  $r_e =$   
141  $0.597$ ; younger mean [ $\pm$ sd]:  $-94.16 \pm 1.39$ , older mean [ $\pm$ sd]:  $-93.36 \pm 2.65$ ), which was expected given the  
142 audiograms (Figure 1).

143 All acoustic stimuli described below were presented at 55 dB above each individual's hearing  
144 threshold – that is, at 55 dB sensation level – in order to match audibility across age groups. However,  
145 higher sound levels can lead to larger brain responses (Picton et al., 1974; Picton et al., 1978;  
146 Pfefferbaum et al., 1979; Polich et al., 1988; Schadow et al., 2007; Herrmann et al., 2018). A higher sound  
147 level for older compared to younger adults could thus bias statistical analyses for which we expect larger  
148 responses in older compared to younger adults. Hence, for these analyses, we also used a subgroup of  
149 14 participants of each age group for which the hearing threshold – and thus the sound level of the  
150 acoustic presentation – did not differ ( $t_{26} = 0.956$ ,  $p = 0.348$ ,  $r_e = 0.184$ ) to confirm our results.

151 ***Acoustic stimulation and procedure***

152 Acoustic stimuli were 4-s long sequences that each consisted of 96 pure-tone pips arranged in twelve  
153 sets of eight tones each (see also Barascud et al., 2016; Herrmann and Johnsrude, 2018a; Southwell and  
154 Chait, 2018). Each set had a duration of 0.333 s. Pips were 0.0417 s in duration with attack and decay  
155 times of 0.007 s, and no gap between tones, or sets. The frequency of each tone was one of 150 possible  
156 values between 700 and 2500 Hz (logarithmically spaced).

157 Acoustic stimuli were presented in two conditions, ‘Pattern-Absent’ and ‘Pattern-Present’, which  
158 occurred with equal probability (50%). In the ‘Pattern-Absent’ condition, tones with different  
159 frequencies were presented in pseudo-random order without a pattern, whereas in the ‘Pattern-  
160 Present’ condition, tones transitioned from random to a regular pattern 1 s (3 sets) after sound onset.  
161 For the ‘Pattern-Absent’ condition, 8 new frequency values were randomly selected for each of the 12  
162 sets (Figure 2, top). In the ‘Pattern-Present’ condition, 8 new frequency values were randomly selected  
163 for each of the first 3 sets (0–1 s; similar to ‘Pattern-Absent’), and then 8 new random frequency values  
164 were selected and repeated in the same order for the remaining 9 sets, thereby creating a regular  
165 pattern (Figure 2, bottom). These conditions are similar to the sounds used in previous studies that  
166 investigated sustained neural activity (Barascud et al., 2016; Southwell et al., 2017; Herrmann and  
167 Johnsrude, 2018a).



**Figure 2: Schematic of acoustic stimulation for ‘Pattern-Absent’ and ‘Pattern-Present’ conditions.** Sound frequency is displayed on the y-axis and dots reflect the sound frequency of individual tones of the tone sequence.

168 In each of the two recording sessions, participants were presented with one 12-min block of  
169 stimulation (as part of recording sessions for an additional project not presented here). Participants  
170 listened passively to 60 trials of each condition per session, while watching a movie of their choice, with



171 subtitles, that was projected into the electromagnetically shielded room via a mirror system. Trials of  
172 the Pattern-Absent and the Pattern-Present conditions were presented pseudo-randomly throughout  
173 the block, such that each condition could occur maximally three times in direct succession. Across both  
174 sessions, participants listened to 120 trials per condition. Trials were separated by a 2-s inter-stimulus  
175 interval.

### 176 *Magnetoencephalographic recordings and initial preprocessing*

177 Magnetoencephalographic data were recorded using a 306-channel Neuromag Vectorview MEG  
178 (MEGIN Oy, Helsinki, Finland; sampling rate: 1000 Hz, online filter: DC–330 Hz) at the Max Planck  
179 Institute for Human Cognitive and Brain Sciences in Leipzig, Germany. Data were recorded in an  
180 electromagnetically shielded room (AK3b, Vacuumschmelze, Hanau, Germany). The signal space  
181 separation (SSS) method (maxfilter© version 2.2.15; default parameter setting  $L_{in} = 8$ ;  $L_{out} = 3$ ) was used  
182 to suppress external interference, interpolate bad channels, and transform each person’s individual data  
183 to the sensor space of the first block of the first session to ensure the data are in a common space (Taulu  
184 et al., 2004; Taulu et al., 2005).

### 185 *Combination of magnetometer and gradiometer channels*

186 The Vectorview MEG device records magnetic fields using 102 magnetometers and 204 gradiometers in  
187 102 locations distributed around the head. In order to account for all data that were recorded, we  
188 combined signals from magnetometer and gradiometer channels (Herrmann et al., 2018).  
189 Magnetometers and gradiometer differ in their configuration, such that magnetometers measure  
190 magnetic fields in Tesla (T), while gradiometers (a coupled pair of magnetometers) measure differences  
191 in the same magnetic fields over a distance of 0.0168 m in Tesla per meter (T/m). The combination of  
192 channel types requires accounting for their different units. We transformed all channels into  
193 magnetometer channels, because such a model only requires a linear interpolation that results in the  
194 same unit for all channels. To this end, we applied the following transformation matrix to each of the  
195 102 sensor triplets (i.e., one triplet comprises two gradiometer channels and one magnetometer  
196 channel):

$$197 \quad X_{scaled} = S \times X$$

198 where  $\mathbf{X}$  consists of a  $3 \times n$  matrix (with  $n$  being the number of data samples over time). The three  
199 rows of  $\mathbf{X}$  refer to the two gradiometers and one magnetometer (i.e., one triplet).  $\mathbf{S}$  refers to a  $5 \times 3$   
200 scaling matrix with the following elements:

$$201 \quad S = \begin{matrix} & -0.0084 & 0 & 1 \\ & 0.0084 & 0 & 1 \\ & 0 & -0.0084 & 1 \\ & 0 & 0.0084 & 1 \\ & 0 & 0 & 1 \end{matrix}$$

202 The value 0.0084 reflects half of the distance between the two gradiometer loops measured in  
203 meters, and the transformation constitutes a linear approximation of the magnetic field at each of the  
204 triplets. The transformation replaces the sensor triplet by a sensor quintet of magnetometers. The  
205 columns of  $\mathbf{S}$  refer to the triplet of two gradiometers and one magnetometer and the rows of  $\mathbf{S}$  refer to  
206 the resulting five magnetometers. This procedure resulted in signals from 510 magnetometer channels  
207 centered on and around 102 locations around a participant's head (Herrmann et al., 2018).

### 208 ***Preprocessing of magnetoencephalographic data***

209 Data were high-pass filtered (0.7 Hz; 2391 points, Hann window), low-pass filtered (20.3 Hz, 119 points,  
210 Kaiser window), down-sampled to 250 Hz, and divided into 6-s long epochs time-locked to sound onset  
211 (from 1 s before to 5 s after sound onset). Independent components analysis (runica method, Makeig et  
212 al., 1996; logistic infomax algorithm, Bell and Sejnowski, 1995; Fieldtrip implementation, v20130727,  
213 Oostenveld et al., 2011) was used to identify and remove activity related to blinks, horizontal eye  
214 movements, muscle activity, and noisy channels. Epochs in which a signal change larger than 8 Picotesla  
215 (pT) occurred in any channel were excluded. These data were used to investigate age differences in  
216 evoked responses to the onset of the sounds.

217 In order to investigate the sustained neural activity, the same pipeline was computed a second  
218 time, with the exception that high-pass filtering was omitted. Omission of the high-pass filter is necessary  
219 to investigate the sustained response, because the response is a very low-frequency signal reflecting a  
220 DC shift (Barascud et al., 2016; Southwell et al., 2017; Herrmann and Johnsrude, 2018a). Activity related  
221 to blinks, horizontal eye movements, muscle activity, and noisy channels was removed using the  
222 identified components from the high-pass filtered data. Epochs in which a signal change larger than 8  
223 pT occurred in any channel were excluded.

224 ***Analysis of responses to sound onset***

225 High-pass filtered data were used to investigate whether neural responses to the onset of the sounds  
226 differed between age groups. This analysis aimed to test whether the auditory cortex of older adults is  
227 hyperresponsive to sound; consistent with reduced inhibition (Casparry et al., 2008; Hughes et al., 2010;  
228 Juarez-Salinas et al., 2010). Data from the Pattern-Absent and Pattern-Present conditions were averaged  
229 because both conditions were identical for the first second of the sound. Epochs ranging from -0.15 s to  
230 0.5 s time-locked to sound onset were extracted. Absolute values were calculated for signals of each  
231 channel (because magnetic fields have opposite polarities in directions perpendicular to the tangential  
232 orientation aspect of the underlying neural source). The mean signal from the pre-stimulus period (-0.15  
233 to 0 s) was subtracted from the signal at each time point, separately for each channel (baseline  
234 correction). Responses were averaged across channels, resulting in one response time course per  
235 participant.

236 For the statistical analysis, differences in response amplitude between age groups were assessed  
237 for each time point using independent samples t-tests. False discovery rate was used to account for  
238 multiple comparisons (Benjamini and Hochberg, 1995; Genovese et al., 2002). We confirmed the results  
239 with two independent samples t-tests that contrasted the amplitudes of the M50 (0.03–0.06 s) and  
240 M100 (0.09–0.13 s) between age groups, which have previously been shown to differ between younger  
241 and older adults (Sörös et al., 2009; Alain et al., 2012; Herrmann et al., 2018).

242 ***Analysis of pattern-related sustained activity***

243 Non-high-pass filtered data were used to investigate whether sustained neural activity associated with  
244 a pattern in sounds differs between age groups. The 6-s epochs (-1 to 5 s, time-locked to sound onset)  
245 were used. Absolute values were calculated for signals of each channel and the mean signal from the  
246 pre-stimulus period (-1 to 0 s) was subtracted from the signal at each time point, separately for each  
247 channel (baseline correction). Responses were averaged across channels, resulting in one response time  
248 course per condition and per participant.

249 Statistical analysis focused on responses during the last half of each stimulus: the 2–4 s time  
250 window. By 2 s, the repeating set of tones would have been presented 3 times (2 full repetitions) in the  
251 Pattern-Present condition (Barascud et al., 2016; Teki et al., 2016; Herrmann and Johnsrude, 2018a). An

252 ANOVA with the within-subjects factor Condition (Pattern-Absent, Pattern-Present) and the between-  
253 subjects factor Age Group (younger, older) was calculated.

#### 254 ***Source localization of magnetoencephalographic data***

255 Anatomically constrained source localization was used to localize the sources underlying the neural  
256 activity in sensor space. Individual T1-weighted MR images (3T Magnetom Trio, Siemens AG, Germany)  
257 were available for each participant. The MR images were used to construct inner skull surfaces (volume  
258 conductor) and mid-gray matter cortical surfaces (source model; using Freesurfer and MNE software;  
259 <https://surfer.nmr.mgh.harvard.edu/>; <http://www.martinos.org/mne/>). The MR and the MEG  
260 coordinate systems were co-registered using MNE software which included an automated and iterative  
261 procedure that fitted the >300 digitized head surface points (Polhemus FASTRAK 3D digitizer) to the MR  
262 reconstructed head surface (Besl and McKay, 1992). The inner skull was extracted from the MR images  
263 using MNE software and used to calculate lead fields using the boundary element model as  
264 implemented in Fieldtrip software (Nolte, 2003). Inverse solutions were calculated using the sLORETA  
265 method (Pascual-Marqui, 2002). Neural activity was spatially smoothed across the surface using an  
266 approximation to a 6-mm FWHM Gaussian kernel (Han et al., 2006). Individual cortical representations  
267 were transformed to a common coordinate system (fsaverage standard brain; Fischl et al., 1999b).  
268 Workbench software (v1.4.2; <https://www.humanconnectome.org/>) was used for visualization of source  
269 localizations morphed to the pial cortical surface of the fsaverage standard brain (Fischl et al., 1999a).  
270 Source localizations were calculated for onset responses and for sustained neural activity. In order to  
271 visualize and analyze pattern-related auditory cortex activity, we averaged source-localization  
272 amplitudes across regions of the superior temporal plane (A1, A4, PBelt, MBelt, and LBelt) using the  
273 brain parcellations of the Human Connectome Project (Glasser et al., 2016).

#### 274 ***Effect sizes***

275 Effect sizes are provided as partial  $\eta^2$  for ANOVAs and as  $r_e$  ( $r_{\text{equivalent}}$ ) for t-tests (Rosenthal and Rubin,  
276 2003).  $r_e$  is equivalent to the square root of partial  $\eta^2$  for ANOVAs.

#### 277 ***Data availability***

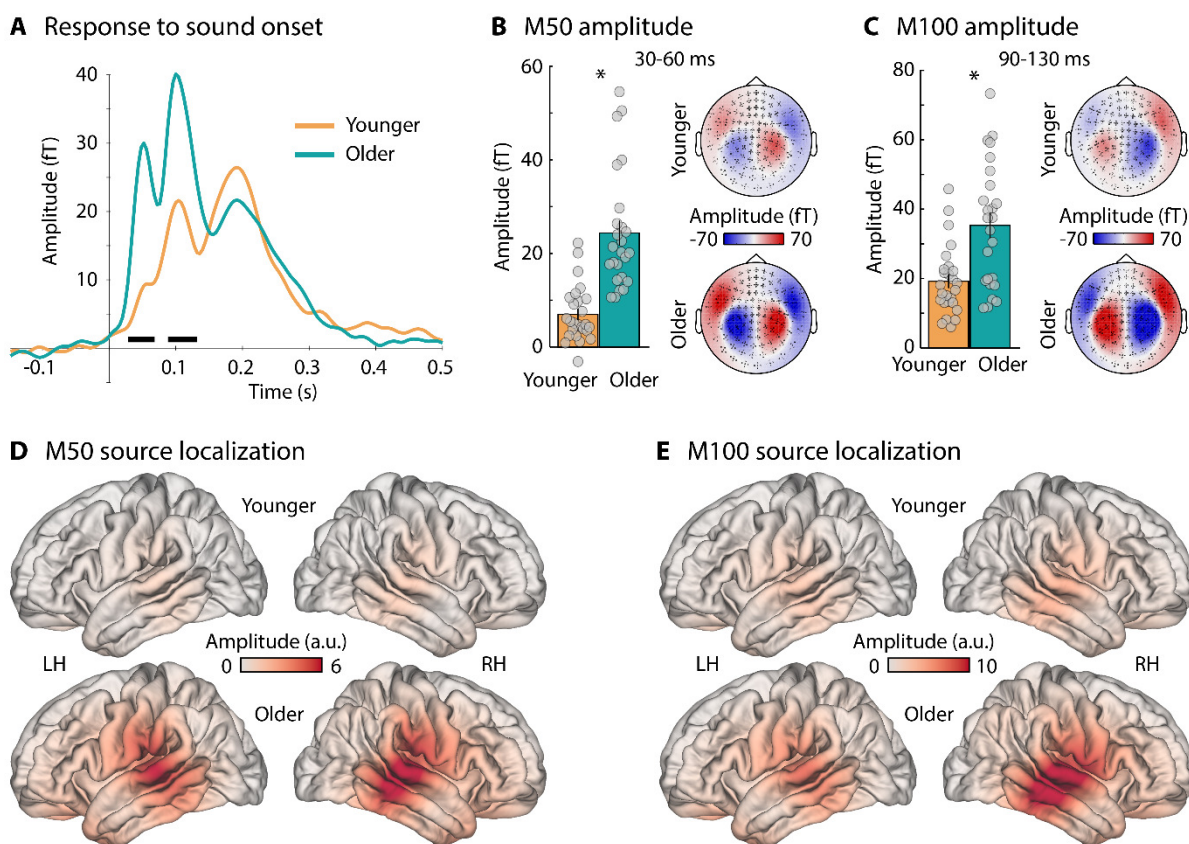
278 This study was not pre-registered. MEG data in BIDS format (Pernet et al., 2019) are available at <link  
279 will be provided upon acceptance of publication>.

280

## Results

### 281 *Responses to sound onset are enhanced in older compared to younger adults*

282 Figure 3A displays the neural response time courses elicited by the onset of the sounds. Responses were  
283 larger in older compared to younger adults in the M50 and M100 time windows (black line in Figure 3A,  
284 FDR-thresholded). Figure 3B/C shows the mean amplitudes and topographical distributions for the M50  
285 and M100 time windows. Larger neural responses for older compared to younger adults were also  
286 observed for the subgroups of 14 participants per age group for which hearing thresholds – and thus  
287 sound-presentation levels – did not differ (M50:  $t_{26} = 4.861$ ,  $p = 4.8 \times 10^{-5}$ ;  $r_e = 0.69$ ; M100:  $t_{26} = 4.381$ ,  $p$   
288  $= 1.7 \times 10^{-4}$ ,  $r_e = 0.652$ ). These results demonstrate that even when sound level does not differ between  
289 younger and older adults, older adults exhibit hyperresponsiveness. Source localizations show activity in  
290 superior temporal cortex, including auditory cortex, underlying M50 and M100 responses in both age  
291 groups (Figure 3D/E).

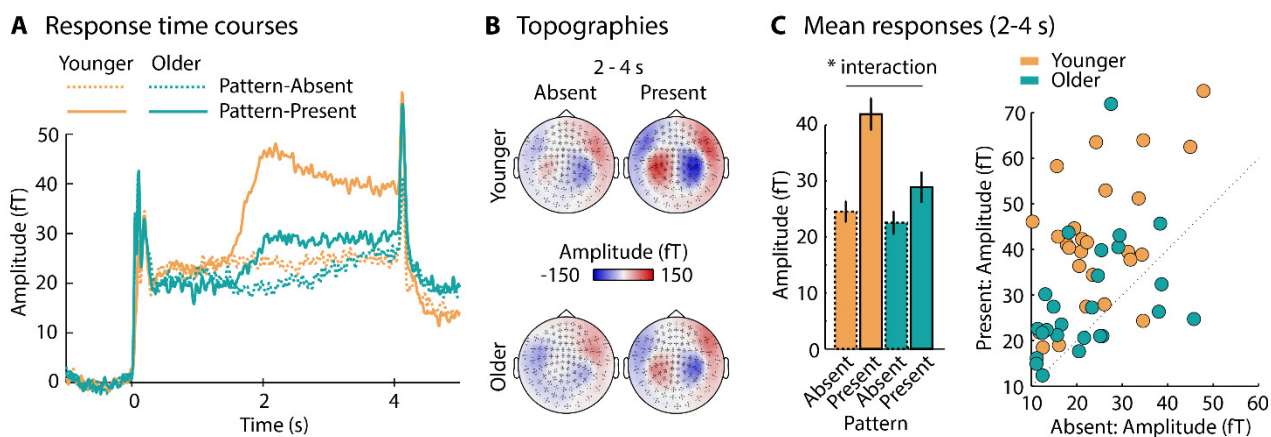


**Figure 3: Neural responses to the onset of sounds.** A: Time courses of neural activity (root-mean square amplitude, averaged across all channels). The black line indicates a significant difference between age groups

**B:** Mean activity and topographies for the M50 time window (30–60 ms). **C:** Mean activity and topographies for the M50 time window (90–130 ms). **D:** Source localization for the M50 time window. **E:** Source localization for the M100 time window. \* $p \leq 0.05$

292 **Pattern-related sustained activity is reduced in older compared to younger adults**

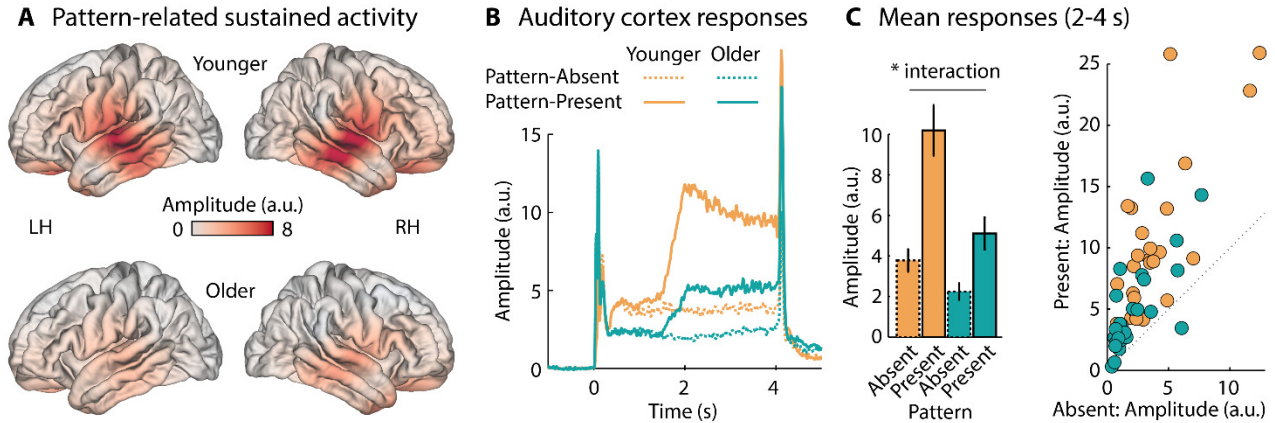
293 Figure 4A and B shows responses time courses and topographical distributions for the Pattern-Absent  
294 and the Pattern-Present condition for both age groups. The ANOVA for the 2-4 s time window revealed  
295 a Condition  $\times$  Age Group interaction ( $F_{1,49} = 9.839$ ,  $p = 0.003$ ,  $\eta_p^2 = 0.167$ ; also significant for the subset  
296 of participants for which sound level did not differ:  $F_{1,26} = 6.792$ ,  $p = 0.015$ ,  $\eta_p^2 = 0.207$ ): While both age  
297 groups show larger sustained activity for the Pattern-Present compared to the Pattern-Absent condition  
298 (younger:  $F_{1,25} = 49.692$ ,  $p \leq 1 \times 10^{-6}$ ,  $\eta_p^2 = 0.665$ ; older:  $F_{1,24} = 6.287$ ,  $p = 0.019$ ,  $\eta_p^2 = 0.208$ ), this  
299 differences was larger in younger compared to older adults (Figure 4C). There was no difference  
300 between age groups for the Pattern-Absent condition ( $F_{1,49} = 0.528$ ,  $p = 0.471$ ,  $\eta_p^2 = 0.011$ ). The main  
301 effect of Condition ( $F_{1,49} = 45.185$ ,  $p \leq 1 \times 10^{-6}$ ,  $\eta_p^2 = 0.48$ ) and the main effect of Age Group ( $F_{1,49} = 6.994$ ,  
302  $p = 0.011$ ,  $\eta_p^2 = 0.125$ ) were also significant.



**Figure 4: Pattern-related sustained activity.** **A:** Response time courses (root-mean square amplitude, averaged across all channels). **B:** Topographical distributions for each condition and age group for the 2-4 s time window. **C:** Mean responses in the 2-4 s time window. Bar graphs reflect the mean across participants. Error bars are the standard error of the mean. Data points for each participant are shown on the right. Data points above the diagonal (dashed line) reflect a larger response for the Pattern-Present compared to the Pattern-Absent condition.

303 Source localization show strongest activity related to pattern-related sustained activity in  
304 superior temporal cortex and auditory cortex (Figure 5A). Indeed, we observed the same interaction for

305 auditory cortex activity ( $F_{1,49} = 10.68$ ,  $p = 0.002$ ,  $\eta_p^2 = 0.179$ ; Figure 5B/C; for the subset of participants:  
306  $F_{1,26} = 7.299$ ,  $p = 0.012$ ,  $\eta_p^2 = 0.219$ ) that we observed in sensor space (Figure 4C), such that the increase  
307 in sustained activity for the Pattern-Present compared to the Pattern-Absent condition was significant  
308 for both age groups (younger:  $F_{1,25} = 50.652$ ,  $p \leq 1 \times 10^{-6}$ ,  $\eta_p^2 = 0.670$ ; older:  $F_{1,24} = 23.833$ ,  $p = 5.6 \times 10^{-5}$ ,  
309  $\eta_p^2 = 0.498$ ), with a larger difference in younger compared to older adults. In contrast to the sensor  
310 space data of sustained activity, sustained activity in auditory cortex elicited by the Pattern-Absent  
311 condition was also larger for younger compared to older adults ( $F_{1,49} = 4.704$ ,  $p = 0.035$ ,  $\eta_p^2 = 0.088$ ;  
312 Figure 5B/C), consistent with observations of reduced sustained activity to a sine tone in older compared  
313 to younger adults (Pfefferbaum et al., 1979). Main effects of Condition ( $F_{1,49} = 73.205$ ,  $p \leq 1 \times 10^{-6}$ ,  $\eta_p^2 =$   
314  $0.599$ ) and Age Group ( $F_{1,49} = 10.176$ ,  $p = 0.002$ ,  $\eta_p^2 = 0.172$ ) were also significant.



**Figure 5: Source localization of pattern-evoked sustained activity.** **A:** Source localization of pattern-related sustained activity (difference between Pattern-Present and Pattern-Absent conditions). **B:** Response time courses from auditory cortex. **C:** Mean auditory cortex responses in the 2-4 s time window. Bar graphs reflect the mean across participants. Error bars are the standard error of the mean. Data points for each participant are shown on the right. Data points above the diagonal (dashed line) reflect a larger response for the Pattern-Present compared to the Pattern-Absent condition.

315

## Discussion

316 The current magnetoencephalography study investigated age related differences in auditory cortical  
317 responsivity to sound onsets and to the presence of a pattern in sounds. We showed that older adults  
318 elicit larger responses in auditory cortex to sound onsets compared to younger adults. This response  
319 enhancement indicates that auditory cortex of older adults is hyperresponsive to sound. Despite this  
320 age-related hyperresponsiveness, sustained neural activity in auditory cortex to sound patterns was

321 diminished in older compared to younger people. Our results suggest that neural responses in auditory  
322 cortex are fundamentally altered in older adults such that sound onsets are overrepresented, whereas  
323 temporally coherent structure in sounds is underrepresented.

#### 324 ***Hyperresponsiveness of auditory cortex in older adults***

325 We demonstrated that neural responses in the M50 and M100 time window following sound onset are  
326 enhanced in older compared to younger adults (Figure 3A-C). We localized the M50 and M100 responses  
327 to auditory cortex (Figure 3D/E; consistent with previous work Pantev et al., 1988; Maess et al., 2007;  
328 Okamoto and Kakigi, 2014; Herrmann et al., 2018), suggesting that auditory cortex in older adults is  
329 hyperresponsive. This is in line with a growing literature showing that neural responses to sound onsets  
330 are enhanced in older compared to younger adults (Ross and Tremblay, 2009; Sörös et al., 2009; Lister  
331 et al., 2011; Alain et al., 2012; Bidelman et al., 2014; Herrmann et al., 2016; Herrmann and Johnsrude,  
332 2018b). Similar observations have been made for aged monkeys (Juarez-Salinas et al., 2010; Recanzone,  
333 2018) and aged rodents (Hughes et al., 2010), as well as for non-human mammals whose auditory  
334 periphery was damaged through high-intensity sound exposure (Popelár et al., 1987; Syka et al., 1994;  
335 Schormans et al., 2019) or ototoxic drugs (Qiu et al., 2000; for detailed reviews see Auerbach et al., 2014;  
336 Zhao et al., 2016; Salvi et al., 2017; Herrmann and Butler, 2020).

337         Hyperresponsiveness to sound is thought to result from hyperexcitable neural circuits due to a  
338 loss of inhibition in the auditory system following peripheral decline (Caspary et al., 2008; Takesian et  
339 al., 2012). The functional role of the loss of inhibition and hyperexcitability is still debated (Zhao et al.,  
340 2016; Asokan et al., 2018; Herrmann and Butler, 2020), but likely includes homeostatic processes to  
341 regulate excitation (Caspary et al., 2008; Zhao et al., 2016) and a state of increased plasticity that enables  
342 cortical reorganization (Cisneros-Franco et al., 2018; Cisneros-Franco and de Villers-Sidani, 2019). A  
343 balanced level of excitation and inhibition is crucial for neural function (Wehr and Zador, 2003; Silver,  
344 2010; Isaacson and Scanziani, 2011), and the fact that we observed hyperresponsiveness to sound in  
345 older compared to younger adults suggests that neural function of auditory cortex was altered in our  
346 sample of older individuals. Hyperresponsivity to sharp attacks in sound may underlie increased  
347 distractibility by irrelevant sounds in older compared to younger adults (Parmentier and Andrés, 2010)  
348 and difficulties comprehending speech in the presence of an interfering, modulated background masker  
349 (Millman et al., 2017; Goossens et al., 2018).



350 ***Pattern-related activity is reduced in older compared to younger adults***

351 In order to investigate whether neural sensitivity to a pattern in sounds differs between younger and  
352 older adults, we presented sounds that either contained a pattern (made of a sequence of a repeated  
353 set of pure tones at different frequencies) or did not contain a pattern (made of a sequence of tones at  
354 pseudo-randomly selected frequencies; Figure 2). For both younger and older adults, we observed that  
355 sustained neural activity increased after the onset of a sound pattern relative to sounds without a  
356 pattern. Previous work in younger adults has revealed similar increases in sustained activity for different  
357 types of patterns, including tone sequences we have utilized here (Gutschalk et al., 2002; Ross et al.,  
358 2002; Keceli et al., 2012; Barascud et al., 2016; Sohoglu and Chait, 2016; Teki et al., 2016; Southwell et  
359 al., 2017; Herrmann and Johnsrude, 2018a; Southwell and Chait, 2018; Herrmann et al., 2019).

360 We showed that sustained neural activity to a pattern in sounds is reduced in older compared to  
361 younger adults. Hence, although neural responses to the onset of sound was enhanced in older adults,  
362 neural sensitivity to a pattern in sounds was reduced. Diminished sustained activity for older compared  
363 to younger adults is consistent with previous indications of an age-related reduction in sustained activity  
364 for short (<1 s) pure tones (Pfefferbaum et al., 1979), amplitude modulations (Herrmann et al., 2019),  
365 and repeated patterns in tone sequences (Al Jaja et al., 2020). However, low statistical reliability and  
366 differences in stimulus parameters between age groups did not allow drawing firm conclusions from the  
367 latter two studies. Our results demonstrate clearly that pattern-related sustained activity indeed is  
368 reduced in older adults.

369 Sensitivity to sound patterns is crucial for a variety of auditory functions, enabling a listener to  
370 segregate concurrent sound streams (Schröger, 2005, 2007; Snyder and Alain, 2007; Winkler et al., 2009;  
371 Bendixen, 2014) and recognize and predict relevant sounds (Jones and Boltz, 1989; Nobre et al., 2007;  
372 Henry and Herrmann, 2014; Nobre and van Ede, 2018). By demonstrating a correlation between  
373 perceptual sensitivity to sound patterns and speech comprehension abilities (Holmes and Griffiths,  
374 2019) and common substrates in auditory cortex (Holmes et al., 2021), previous work further indicates  
375 a functional relation or common underlying mechanism between the processing of regularities in sounds  
376 and speech comprehension. A reduction in sustained activity may thus indicate that sound patterns are  
377 processed less well in neural circuits in older compared to younger adults, which may, in part, explain  
378 the challenges older adults experience comprehending speech in the presence of background sound.

379           The current source localizations suggest that auditory cortex is the main source underlying  
380 pattern-related sustained activity in both younger and older adults (Figure 5A). Previous work in younger  
381 individuals also indicated that auditory cortex underlies sustained neural activity (Pantev et al., 1994;  
382 Pantev et al., 1996; Gutschalk et al., 2002; Ross et al., 2002; Gutschalk et al., 2004; Gutschalk et al., 2007;  
383 Okamoto et al., 2011; Keceli et al., 2012; Barascud et al., 2016; Teki et al., 2016), but that brain regions  
384 in frontal cortex, parietal cortex, and hippocampus may additionally contribute (Tiitinen et al., 2012;  
385 Barascud et al., 2016; Teki et al., 2016). However, in the latter work, statistical difference maps were  
386 calculated and used to identify neural sources. Statistical difference maps may also capture effects  
387 related to activity spread due to volume conduction and may thus not reflect activity originating from  
388 these higher-level brain regions (e.g., auditory responses to sound onset were spread to parietal cortex  
389 in Teki et al., 2016, suggesting that spread may also affect their sustained activity in parietal cortex  
390 related to sound patterns).

391           We further showed that sustained activity in auditory cortex to sounds that did not contain a  
392 pattern was also reduced in older compared to younger adults (Figure 5B/C). Sounds without a pattern  
393 were made of a sequence of pure tones whose frequency changed randomly for each tone. Such tone  
394 sequences are perceptually more structured than noise and the auditory system may treat them as a  
395 pattern of low saliency. This is consistent with the observation of reduced sustained activity to short  
396 pure tones in older compared to younger adults (Pfefferbaum et al., 1979). Our data thus indicate that  
397 the sensitivity of the aged auditory cortex is reduced for sounds containing a pattern (here repetition of  
398 a set of tones at different frequencies) as well as for sequences with random tone frequencies.

399           It is clear from previous work that temporally regular – and thus predictable – structure in sounds  
400 that forms a pattern elicits sustained neural activity (Gutschalk et al., 2002; Barascud et al., 2016;  
401 Herrmann and Johnsrude, 2018a). However, additional work suggests that the magnitude of pattern-  
402 related sustained activity is related to the degree of novelty or predictability of a pattern, such that  
403 sustained activity decreases when a pattern is frequently, compared to infrequently, heard (Gutschalk  
404 et al., 2007). A reduction in sustained activity in older adults may thus result from reduced processing of  
405 the pattern as well as from a sense of reduced novelty of the pattern.

406

## Conclusions

407 In the current study, we recorded magnetoencephalography to characterize differences between  
408 younger and older adults in the processing of a pattern in sounds. We presented continuous tone  
409 sequences that either contained a pattern (made of a repeated set of tones at different frequencies) or  
410 did not contain a pattern (random tone frequencies). We showed that auditory cortex in older adults is  
411 hyperresponsive to sound onsets, but that sustained neural activity in auditory cortex, indexing the  
412 processing of sound patterns, is reduced. Hence, neural populations in auditory cortex fundamentally  
413 differ between younger and older individuals in their sensitivity to sound features, hyperresponding to  
414 sound onsets, while underresponding to patterns in sounds. This may help to explain some age-related  
415 changes in hearing such as increased sensitivity to distracting sounds and difficulties tracking speech in  
416 the presence of other sound.

417

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423

## Author contributions

424 BH conceptualized and designed the study, recorded data, analyzed the data, interpreted the results,  
425 and wrote the manuscript. BM analyzed the data, interpreted the results, and edited the manuscript. ISJ  
426 conceptualized and designed the study, interpreted the results, and edited the manuscript.

427

## Declaration of conflicts of interest

428 None.

429

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