

# A note on the iterative MRI reconstruction from nonuniform k-space data

Tobias Knopp\*      Stefan Kunis<sup>†</sup>      Daniel Potts<sup>‡</sup>

In magnetic resonance imaging (MRI), methods that use a non-Cartesian grid in k-space are becoming increasingly important. In this paper, we use a recently proposed implicit discretisation scheme which generalises the standard approach based on gridding. While the latter succeeds for sufficiently uniform sampling sets and accurate estimated density compensation weights, the implicit method further improves the reconstruction quality when the sampling scheme or the weights are less regular. Both approaches can be solved efficiently with the nonequispaced FFT. Due to several new techniques for the storage of an involved sparse matrix, our examples include also the reconstruction of a large  $3d$  data set. We present four case studies and report on efficient implementation of the related algorithms.

*Key words and phrases:*  $2d/3d$  image reconstruction, magnetic resonance imaging, spiral scan, iterative methods, gridding, Fourier transform, FFT, Nonequispaced FFT.

## 1 Introduction

The raw data for magnetic resonance imaging (MRI) is measured in k-space, the domain of spatial frequencies, where non-Cartesian sampling schemes like spiral or radial scans have received much attention. In contrast to the use of the computationally efficient fast Fourier transform (FFT) for the reconstruction from Cartesian grids, the more general sampling trajectories ask for so-called nonequispaced FFTs. On the other hand, iterative image reconstruction algorithms play an important role in modern tomographic systems [16]. Recently, iterative image reconstruction in combination with the nonequispaced FFT has been applied to data on spiral k-space trajectories [29] and in the presence of field inhomogeneities [30]. Efficient reconstruction procedures for sensitivity encoding with arbitrary k-space trajectories were proposed in [24]. Its authors present methods that combine the gridding principles with the conjugate gradient scheme, but mention the the long computation times due to their nonoptimised preliminary software.

---

\*tobias.knopp@informatik.uni-luebeck.de, University of Lübeck, Institute of Mathematics,

<sup>†</sup>kunis@mathematik.tu-chemnitz.de, Chemnitz University of Technology, Department of Mathematics,

<sup>‡</sup>potts@mathematik.tu-chemnitz.de, Chemnitz University of Technology, Department of Mathematics,

In this paper, we use a similar method, compare the gridding approach [19] and an approach based on an implicit discretisation [5], where we focus for the reader’s convenience on a simplified signal equation. It turns out that the iterative solution of the latter approach resembles the gridding method in its first iteration. Both reconstruction problems are easily solved by our mature software package [14] for the nonequispaced fast Fourier transform (NFFT) [23,28]. For readers not familiar with the NFFT we suggest to read the appendix of this paper first. The publicly available implementation easily allows for the efficient treatment of large  $3d$  data sets by the use of new sparse matrix storage techniques [15]. Moreover, we compare different density compensation weights arising from the discretisation of the underlying integrals. We present numerical results, based on the Shepp-Logan phantom as well as on data acquired by an MR scanner.

The outline of this paper is as follows: Section 2 gives a brief introduction to the theory of Fourier transform image reconstruction and unifies the two considered approaches in MRI. We suggest the conjugate gradient method for the reconstruction problem and show that the solution is efficiently computed by the iterative use of the nonequispaced FFT. Subsequently, Section 3 presents the used  $k$ -space trajectories, considers sampling density compensation, and introduces the tested simulated and acquired data sets. Section 4 shows our numerical tests emphasising the reconstruction quality with respect to the number of iterations and different density compensation weights. Moreover, we give detailed information on the computational requirements of the suggested scheme. Finally, a short discussion of our results is contained in Section 5 and an introduction to the nonequispaced FFT might be found in the appendix.

## 2 Theory

Given a trajectory  $\mathbf{k} = \mathbf{k}(t)$ , the relation between the MR signal  $s$  during the readout and the object  $p$  can be modelled by the simplified signal equation

$$s(\mathbf{k}) = \int_{\mathbb{R}^3} p(\mathbf{r}) e^{2\pi i \mathbf{r} \mathbf{k}} d\mathbf{r}. \quad (2.1)$$

In the following we describe two different approaches. For convenience let the available samples in  $k$ -space be contained in the shifted unit cube, i.e.  $\mathbf{k} \in [-\frac{1}{2}, \frac{1}{2}]^3$ , and the field of view be restricted to  $\Omega_{\mathbf{N}} \subset [-\frac{N_1}{2}, \frac{N_1}{2}] \times [-\frac{N_2}{2}, \frac{N_2}{2}] \times [-\frac{N_3}{2}, \frac{N_3}{2}]$ , where  $\mathbf{N} = (N_1, N_2, N_3)^\top \in 2\mathbb{N}^3$ . Then, the discretisation of integral (2.1) on equispaced points leads to

$$s(\mathbf{k}) \approx \tilde{s}(\mathbf{k}) := \sum_{\mathbf{r} \in I_{\mathbf{N}}^3} p(\mathbf{r}) e^{2\pi i \mathbf{r} \mathbf{k}}, \quad (2.2)$$

where  $I_{\mathbf{N}}^3 := \{-\frac{N_1}{2}, \dots, \frac{N_1}{2} - 1\} \times \{-\frac{N_2}{2}, \dots, \frac{N_2}{2} - 1\} \times \{-\frac{N_3}{2}, \dots, \frac{N_3}{2} - 1\}$ . Thus, the unknown object  $p$  is given *implicitly* by (2.2). The authors of [5] call this the “inverse model”.

A second approach uses the Fourier inversion theorem  $p(\mathbf{r}) = \int_{\mathbb{R}^3} s(\mathbf{k}) e^{-2\pi i \mathbf{r} \mathbf{k}} d\mathbf{k}$  first. The discretisation of this integral leads to

$$p(\mathbf{r}) \approx \tilde{p}(\mathbf{r}) := \sum_{j=0}^{M-1} s(\mathbf{k}_j) e^{-2\pi i \mathbf{r} \mathbf{k}_j} w_j, \quad (2.3)$$

where  $w_j$  are weights, which compensate for local variations of the sampling density. Here, the unknown object  $p \approx \tilde{p}$  can be computed *explicitly*.

The important difference between (2.2) and (2.3) is that the former is discretised in the image domain with pixels on a uniform grid and hence with unit weighting coefficients and the latter is an integral discretised in k-space with non-uniform samples and specific weights. We reformulate problem (2.2) and (2.3) in matrix vector notation and denote the vector of the given measurements by  $\mathbf{s} := (s(\mathbf{k}_j))_{j=0,\dots,M-1} \in \mathbb{C}^M$ , the reshaped vector of the unknown object by  $\mathbf{p} := (p(\mathbf{r}))_{\mathbf{r} \in I_N^3} \in \mathbb{C}^{N_1 \times N_2 \times N_3}$ , the density compensation matrix by  $\mathbf{W} := \text{diag}(w_j)_{j=0,\dots,M-1}$ , and the nonequispaced Fourier matrix by

$$\mathbf{A} := \left( e^{2\pi i \mathbf{r} \mathbf{k}_j} \right)_{j=0,\dots,M-1; \mathbf{r} \in I_N^3}, \quad (2.4)$$

whereas  $\mathbf{A}^H$  denotes its adjoint (conjugate transpose).

The gridding approximation (2.3) is easily computed by one matrix vector multiplication

$$\tilde{\mathbf{p}} = \mathbf{A}^H \mathbf{W} \mathbf{s}. \quad (2.5)$$

The adjoint NFFT takes  $\mathcal{O}(|I_N^3| \log |I_N^3| + M)$  floating point operations for this task.

Slightly more involved, the reconstruction problem (2.2) is solved by the method of least squares and hence, consists in solving the weighted normal equation of first kind

$$\mathbf{A}^H \mathbf{W} \mathbf{A} \mathbf{p} = \mathbf{A}^H \mathbf{W} \mathbf{s} \quad (2.6)$$

for the unknown vector  $\mathbf{p}$ . In contrast to [5], we include density compensation weights also for the implicit discretisation since this is more natural with respect to the ‘‘continuous residual’’ in k-space and has been proven to be better conditioned in [2]. From the mathematical point of view, equation (2.6) is solved most efficiently by the conjugate gradients (CG) method, cf. [4, pp. 288]. We prefer to solve (2.6) by a factorised variant of conjugated gradients, where the two multiplications with the (adjoint) nonequispaced Fourier matrix per iteration are computed by the NFFT. This scheme is denoted by CGNR, N for ‘Normal equation’ and R for ‘Residual minimisation’, cf. [26]. Note that the CG method applied directly to (2.6) as suggested in [24] generates the same sequence of approximations in exact arithmetic, but the CGNR approach is considered to be more stable with respect to round-off errors, cf. [20, Sec. 7.1]. In summary, we suggest the following Algorithm 1.

Remarkably, this algorithm resembles an optimised gridding solution after one iteration. More formally, let the weighted residual norm  $\|\mathbf{r}\|_{\mathbf{W}}^2 := \mathbf{r}^H \mathbf{W} \mathbf{r}$  be given. Then, the first iteration obeys

$$\mathbf{p}_1 = \arg \min_{\mathbf{p}=\alpha \tilde{\mathbf{p}}} \|\mathbf{s} - \mathbf{A} \mathbf{p}\|_{\mathbf{W}}, \quad (2.7)$$

since for the first residual  $\mathbf{r}_1 = \mathbf{s} - \mathbf{A} \mathbf{p}_1$  holds the perpendicular condition

$$\mathbf{r}_1^H \mathbf{W} \mathbf{A} \tilde{\mathbf{p}} = \left( \mathbf{A}^H \mathbf{W} \mathbf{s} \right)^H \tilde{\mathbf{p}} - \frac{\tilde{\mathbf{p}}^H \tilde{\mathbf{p}}}{(\mathbf{A} \tilde{\mathbf{p}})^H \mathbf{W} \mathbf{A} \tilde{\mathbf{p}}} (\mathbf{A} \tilde{\mathbf{p}})^H \mathbf{W} \mathbf{A} \tilde{\mathbf{p}} = 0. \quad (2.8)$$

In other words, the gridding solution  $\tilde{\mathbf{p}}$  in (2.5) is scaled such that its residual is minimised and we do not consider a gridding approach separately anymore.

---

**Algorithm 1** Conjugate gradients for normal equations (CGNR)

---

Input  $M \in \mathbb{N}$  number of given samples  
 $N_1, N_2, N_3 \in \mathbb{N}$  number of unknowns  
 $(\mathbf{k}_j, s_j)_{j=0, \dots, M-1}$  sampling points and values  
 $\mathbf{W} = \text{diag}(w_j)_{j=0, \dots, M-1}$  diagonal matrix, density compensation weights

$\mathbf{p}_0 = \mathbf{0}$   
 $\mathbf{r}_0 = \mathbf{s}$   
 $\tilde{\mathbf{p}}_0 = \tilde{\mathbf{z}}_0 = \mathbf{A}^H \mathbf{W} \mathbf{r}_0$   
**for**  $l = 0, 1, \dots$  **do**  
   $\mathbf{v}_l = \mathbf{A} \tilde{\mathbf{p}}_l$   
   $\alpha_l = \tilde{\mathbf{z}}_l^H \tilde{\mathbf{z}}_l / \mathbf{v}_l^H \mathbf{W} \mathbf{v}_l$   
   $\mathbf{p}_{l+1} = \mathbf{p}_l + \alpha_l \tilde{\mathbf{p}}_l$   
   $\mathbf{r}_{l+1} = \mathbf{r}_l - \alpha_l \mathbf{v}_l$   
   $\tilde{\mathbf{z}}_{l+1} = \mathbf{A}^H \mathbf{W} \mathbf{r}_{l+1}$   
   $\beta_l = \tilde{\mathbf{z}}_{l+1}^H \tilde{\mathbf{z}}_{l+1} / \tilde{\mathbf{z}}_l^H \tilde{\mathbf{z}}_l$   
   $\tilde{\mathbf{p}}_{l+1} = \tilde{\mathbf{z}}_{l+1} + \beta_l \tilde{\mathbf{p}}_l$   
**end for**

Output  $\mathbf{p}_l$  approximate solution

---

Moreover note, that the proposed scheme should be stopped as soon as the current residual  $\|\mathbf{s} - \mathbf{A}\mathbf{p}_l\|_{\mathbf{W}}$  drops below the discretisation error or the level of noise in the measurements  $\mathbf{s}$ . For our first evaluation, we terminate the suggested algorithm after a fixed number of iterations.

### 3 Methods

We are concerned with the reconstruction from data acquired by an MR scanner as well as the reconstruction quality and the usage of time and memory resources for simulated data. Algorithm 1 has been tested with MR measurements of a physical phantom by the Philips Achieva 1.5T device. Here, the sampling scheme consists of 36 equidistant radial trajectories with  $M = 7, 557, 120$  points in total, whereas the reconstructed image contains  $256 \times 256 \times 36 = 2, 359, 296$  voxels.

Moreover, we compare different reconstructions for simulated MR data. We use two 3d-Shepp-Logan phantoms of sizes  $256 \times 256 \times 36$  and  $128 \times 128 \times 128$  (2, 097, 152 voxels) as shown in Figure 3.1. Comparison is done with respect to the number of iterations, sampling schemes, and density compensation weights. The simulated MR data is computed by a 3d-NFFT using the following k-space trajectories. Note, that all but the first trajectory are of a special  $2d \otimes 1d$  type, i.e., they consist of a stack of 36 equidistant planes where the  $M_1$  points within each are distributed accordingly. In these cases, the first two coordinates of a k-space point  $\mathbf{k} = (k_1, k_2, k_3)^\top$  form the 2d-point  $\tilde{\mathbf{k}} = (k_1, k_2)^\top \in [-\frac{1}{2}, \frac{1}{2}]^2$ .



Figure 3.1: Slice plot of our 3d-Shepp-Logan phantom

- i) (3d-RADIAL) The only 3d-k-space trajectory, which is not of  $2d \otimes 1d$  type, is given by

$$\mathbf{k}_{p,q,r} = \frac{r+1}{\sqrt{2}R} (\cos \phi_p \sin \theta_q, \sin \phi_p \sin \theta_q, \cos \theta_q)^\top$$

where  $\phi_p = \frac{2\pi p}{P}$ ,  $p = 0, \dots, P-1$ ,  $\theta_q = \frac{\pi(2q+1)}{2Q}$ ,  $q = 0, \dots, Q-1$ , and  $r = 0, \dots, R-1$ . Furthermore, we restrict this set to the unit cube  $(-\frac{1}{2}, \frac{1}{2})^3$ . Choosing  $P = Q = R = 160$  in our experiments yields a total number of  $M = 3,398,033$  points in k-space.

- ii) (RADIAL) Popular also within computer tomography is the 2d-radial trajectory

$$\tilde{\mathbf{k}}_{p,r} = (-1)^r \left( \frac{r}{R} - 0.5 \right) \left( \cos \frac{\pi p}{P}, \sin \frac{\pi p}{P} \right)^\top,$$

with  $p = 0 \dots P-1$ ,  $r = 0, \dots, R-1$ . We set  $P = 410$  and  $R = 512$  yielding a total number of  $M = 36M_1 = 36PR = 7,557,120$  points in k-space.

- iii) (SPIRAL) This 2d-k-space trajectory is given by one Archimedean spiral, i.e.,

$$\tilde{\mathbf{k}}_j = \frac{\sqrt{j}}{2\sqrt{M_1}} (\cos \omega_j, \sin \omega_j)^\top,$$

where  $\omega_j = \frac{8\pi}{5}\sqrt{j}$ , and  $j = 0, \dots, M_1 - 1$ . We have chosen  $M_1 = 65,536$  yielding a total number of  $M = 36M_1 = 2,359,296$  points in k-space.

Examples of the trajectories are shown in Figure 3.2. Note that each proposed sampling scheme obeys a Nyquist rate near the origin of the k-space. Nevertheless, all sampling sets violate the Nyquist criteria in their periphery since there exist boxes larger than the reciprocal field of view  $\frac{1}{N_1} \times \frac{1}{N_2} \times \frac{1}{N_3}$  containing no single sampling point  $\mathbf{k}_j$ .

In the following different weights  $\mathbf{W}$  in (2.6) are used to take into account the local sampling density in k-space. We propose formulations

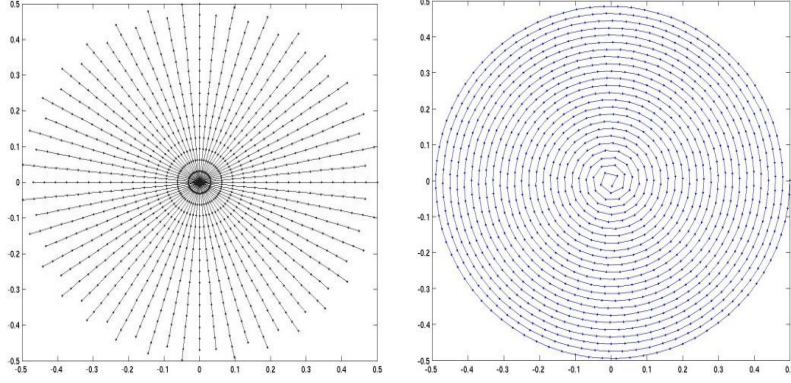


Figure 3.2: Typical k-space trajectories, RADIAL ( $P = R = 32$ , left) and SPIRAL ( $M_1 = 1024$ , right).

- i) with no weights, i.e.  $\mathbf{W}$  being the identity,
- ii) with analytic weights in the case of the 3d-RADIAL trajectory, given by

$$w_{p,q,r} = \frac{r+1}{R} \sin \frac{\pi(2q+1)}{2Q},$$

- iii) with approximate weights computed in a very cheap way by counting the number of sample points in the  $256 \times 256$  box tessellation of the k-space  $[-\frac{1}{2}, \frac{1}{2}]^2$ , and
- iv) with weights obtained as the area of the Voronoi cell

$$\Omega_j = \left\{ \tilde{\mathbf{k}} \in \left[ -\frac{1}{2}, \frac{1}{2} \right)^2 : \|\tilde{\mathbf{k}} - \tilde{\mathbf{k}}_j\|_2 \leq \min_{l=0, \dots, M-1} \|\tilde{\mathbf{k}} - \tilde{\mathbf{k}}_l\|_2 \right\}$$

around each sample point  $\tilde{\mathbf{k}}_j$ , see also [1, 25].

It was pointed out, e.g. in [25], that the use of Voronoi weights as a measure of the local sampling density is a very reliable and general technique. For the gridding approach (2.3), a detailed discussion of sampling density compensation for sampling sets violating the Nyquist criteria is given in [22].

## 4 Numerical results

Algorithm 1 was implemented as part of the NFFT library [14]. All tests were implemented in Matlab&C and tested on a AMD Athlon XP 2700+, 2GB memory, SuSe-Linux, kernel 2.4.20-4GB-athlon, FFTW3.0.1, and NFFT2 (Kaiser-Bessel window function with cut-off parameter  $m = 6$  and oversampling factor  $\sigma \geq 1.5$ ). Besides a couple of representative examples, our webpage on this project [www.tu-chemnitz.de/~potts/projects/mri](http://www.tu-chemnitz.de/~potts/projects/mri) collects a more thorough set of tests as pointed out in the subsequent examples. In particular, this includes animated graphics showing the progress during the iterations or slicing through the 3d data set.

**Numerical Example 1** First of all, we apply Algorithm 1 to MR measurements taken by the Philips Achieva 1.5T device. Figure 4.1 shows the result after one iteration, where we used Voronoi weights for sampling density compensation.  $\square$

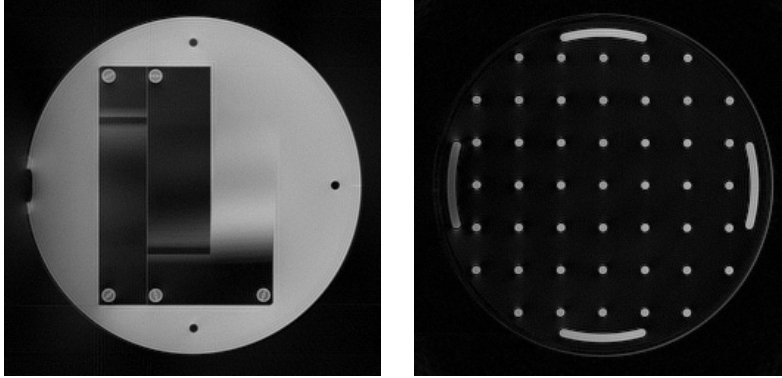


Figure 4.1: Two slices of the reconstruction from MR measurements with Voronoi weights after one iteration.

**Numerical Example 2** We compare the reconstruction quality with respect to the three different k-space trajectories and sampling density compensation weights. For the  $2d \otimes 1d$  type of the trajectories, we reconstruct each slice separately and compute the overall reconstruction by  $256^2$  regular  $1d$ -FFTs of length  $N_3 = 36$  within the third component. Table 4.1 shows the normalised root-mean-square error

$$\text{RMS}(\tilde{\mathbf{p}}, \mathbf{p}) := \frac{\|\mathbf{p} - \tilde{\mathbf{p}}\|_2}{\|\mathbf{p}\|_2}, \quad (4.1)$$

where  $\tilde{\mathbf{p}}$  is our reconstruction and  $\mathbf{p}$  denotes the original image of size  $128 \times 128 \times 128$  for the  $3d$ -RADIAL trajectory and of size  $256 \times 256 \times 36$  for all others.

Additionally, we computed 30 iterations for the  $3d$ -RADIAL example which yields a RMS of 0.3309 and 0.2104 for no weights and analytic weights, respectively. A first hint on the stability of the reconstruction process with respect to noisy data is given in the last line of Table 4.1. We show the RMS for the reconstruction from simulated SPIRAL data which is perturbed by 20 percent standard normally distributed noise.  $\square$

**Numerical Example 3** We present some reconstructions our algorithm achieves. The main purpose of the  $3d$ -RADIAL example is to demonstrate that the NFFT-based reconstruction is straightforward. Figure 4.2 shows the 64th slice and the profile of the 64th row of this slice after one, five and ten iterations for analytic weights. The same experiment using no weights is presented on our web-page.

Furthermore, we show the 18th slice and the profile of the 128th row of this slice after one and ten iterations for different weights and the  $2d \otimes 1d$  k-space trajectory RADIAL in Figure 4.3. The same experiment using the SPIRAL trajectory and an interleaved spiral trajectory is presented on our web-page.  $\square$

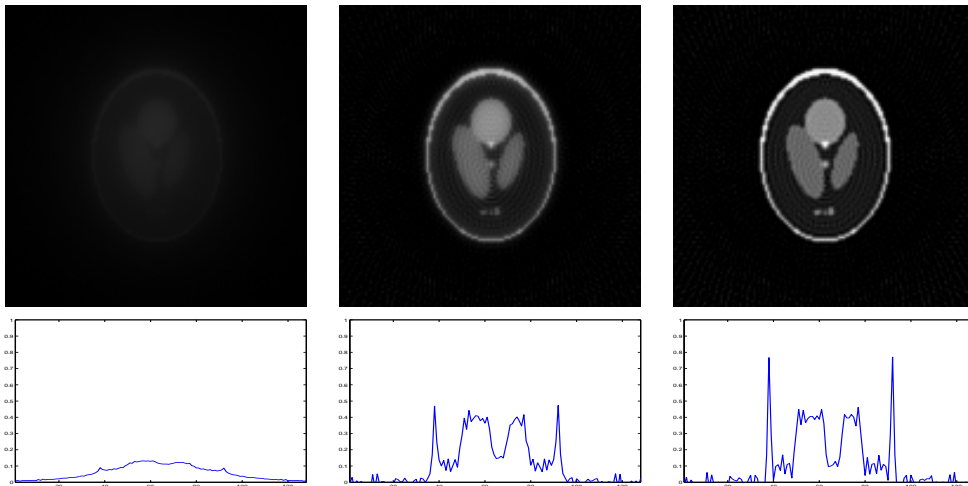


Figure 4.2: 64th slice of the phantom (top) and the profile of the 64th row of this slice (bottom) with  $3d$ -RADIAL data and **analytic weights**: from left to right after one, five and ten iterations.

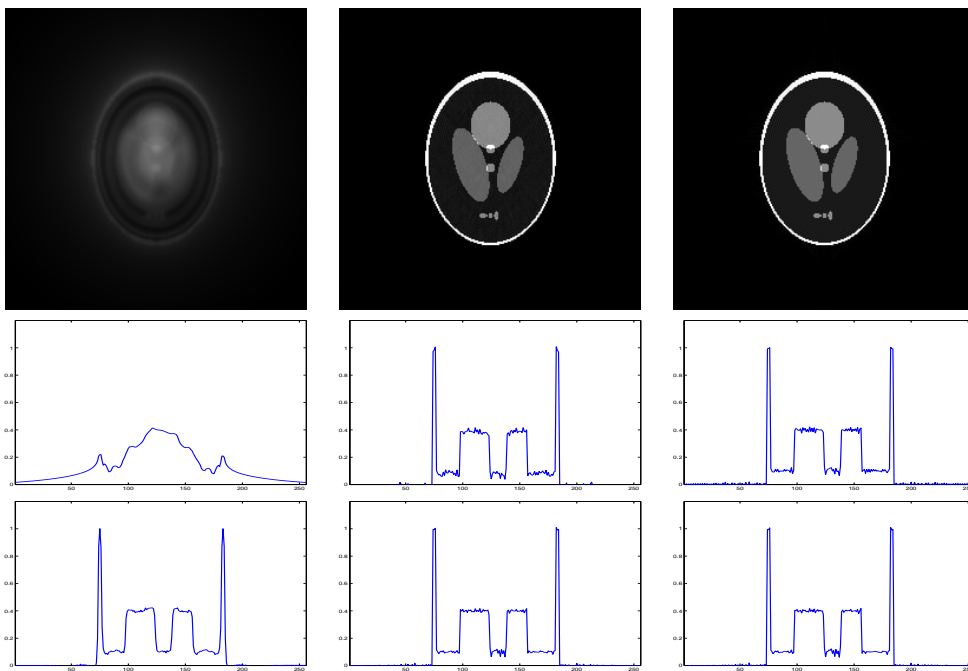


Figure 4.3: 18th slice of the phantom (top) and the profile of the 128th row of this slice (middle) after **one iteration** with RADIAL data: from left to right, without weights, with approximative weights and with Voronoi weights. The same profile is shown after **ten iterations** (bottom).



weights \ iter.	1	2	5	10
<i>3d</i> -RADIAL				
none	0.8281	0.7491	0.6482	0.5509
analytic	0.6981	0.5685	0.3047	0.2146
RADIAL				
none	0.6458	0.5276	0.3025	0.1170
approximation	0.1597	0.0773	0.0767	0.0764
Voronoi	0.0776	0.0775	0.0772	0.0769
SPIRAL				
none	0.1658	0.0908	0.0769	0.0767
approximation	0.1686	0.0864	0.0773	0.0768
Voronoi	0.1360	0.0812	0.0781	0.0779
SPIRAL with noise				
Voronoi	0.1444	0.0937	0.0971	0.1010

Table 4.1: RMS for different weights and k-space trajectories after 1, 2, 5, and 10 iterations.

**Numerical Example 4** In the last test, we measure CPU-time and used memory of our algorithms with respect to the size of the reconstruction problem  $N$ , i.e., the size of the reconstructed image is  $N \times N \times 36$  and the total number of SPIRAL k-space samples is  $36N^2$ . We compare Algorithm 1 exploiting the  $2d \otimes 1d$  type of the trajectory with Algorithm 1 using the full  $3d$  NFFT. Both algorithms produce almost the same sequence of reconstructions.

The optimisation of the computing time is done by different NFFT-flags which affect the last step of the NFFT. In this last step we compute by  $\mathcal{O}(M)$  floating point operations the matrix vector product with the sparse matrix  $\mathbf{B}$  as defined in the appendix, equation (6.2). We propose different methods for the precomputation and storage of this matrix that basically trade main memory for computation speed. We were able to store all nonzero entries of the matrix  $\mathbf{B}$  together with their row and column index by the flag PRE\_FULL\_PSI in all  $2d \otimes 1d$  tests, see [13] for a similar approach. A lossless compressed form, flag PRE\_PSI, is used in the  $3d$ -tests up to  $N = 256$ . Finally, we use a lossy compressed version which is independent of the actual trajectory, uses a lookup table, and linear interpolation for the entries of the sparse matrix (PRE\_LIN\_PSI) in the  $3d$ -tests for  $N = 512$ , see the manual to [14] and [15] for details. Table 4.2 shows our results for the Shepp-Logan phantom, the SPIRAL trajectory, and Voronoi weights. The measured CPU-times grow as expected like  $N^2 \log N$ . Clearly, the method based

on the  $2d \otimes 1d$  model is faster, however our algorithms can handle arbitrary scattered data in  $d$  dimensions by storing a heavily compressed form of the sparse matrix  $B$ .  $\square$

	CPU-time in seconds				MByte
$N \setminus \#$	1	2	5	10	
$2d \otimes 1d$ trajectory					
512	118.95	178.04	355.08	650.55	691
256	29.24	43.55	87.21	159.71	172
128	6.56	9.84	19.73	35.78	43
64	1.45	2.16	4.31	8.00	10
$3d$ trajectory					
512	11422	17114	34189	62650	1952
256	1865.9	2800.4	5603.3	10274	1244
128	452.31	679.28	1344.9	2454.4	311
64	89.24	133.72	267.18	489.59	77

Table 4.2: CPU-time and memory usage for different iteration numbers  $\#$  and sizes  $N$  of the k-space data and the reconstructed phantom.

## 5 Discussion

Magnetic resonance signals are measured in k-space, where magnetic field gradients determine the specific trajectories that form the sampling points. We have shown that the reconstruction from non-Cartesian grids is easily computed by means of the nonequispaced FFT where at least an approximate compensation of the non-uniform sampling density proves necessary for highly nonuniform sampling sets.

The gridding approach, based on an explicit discretisation, and the “inverse model” [5], based on an implicit discretisation, are unified and solved by Algorithm 1. In particular, the gridding solution is optimised in one iteration to minimise the residual, see (2.7), and further refined in subsequent iterations. We see that already the gridding method may lead to very good results in Table 4.1 and in Figure 4.3. However, using no density compensation weights gives reasonable results only if the trajectory covers the k-space uniformly as for the SPIRAL trajectory, see Table 4.1 “weights: none” and our web-page. Gridding without density compensation gives non satisfactory results for  $3d$ -RADIAL and RADIAL trajectories as shown in the leftmost images of Figure 4.2 and 4.3. Including approximate weights improves the reconstruction quality, the best gridding results are obtained using the more expensive Voronoi weights. However, substantial

improvement of the reconstruction quality is achieved during a small number of iterations for all used trajectories and weights. Furthermore, only the iterative method in conjunction with a reasonable approximation of weights gives an acceptable reconstruction from the  $3d$ -RADIAL trajectory, cf. Figure 4.2 and our web-page. Finally, we have compared the computation time and memory usage of the proposed algorithm for the  $2d \otimes 1d$  model and a full  $3d$ -model.

In summary, the implicit discretisation and its iterative solution generalises the gridding approach in a natural way and refines the image quality. Particularly, a poor gridding solution from a highly non-uniform trajectory with approximated density compensation weights is improved substantially by a few iterations of our scheme. We have shown that very efficient methods are available, which can be generalised to reconstruction methods for sensitivity encoding as proposed in [24] and to reconstruction methods in presence of field inhomogeneities [8, 30].

Note however, that the computation times reported in Table 4.2 depend on the stopping criterion. Directions for our future research include the development of reliable stopping criteria for the iterative reconstruction and proven convergence rates when the Nyquist criteria is violated.

## 6 Appendix

In recent years, the nonequispaced fast Fourier transform (NFFT) has attracted much attention due to the fact that it generalises the FFT for arbitrary sampling geometries. Common names for these algorithms are *nonequispaced FFT* [11, 23, 28], *non-uniform FFT* [10], *generalised FFT* [7], or *unequally-spaced FFT* [3]. Its accuracy is adjusted to the practical requirements by an oversampling factor and a cut-off parameter, whereas no dependency on the sampling points occurs. In contrast, the inverse NFFT can be computed with a CG-type algorithm utilising one NFFT and one adjoint NFFT per iteration and its reconstruction error depends strongly on the sampling geometry and used compensation weights. In what follows, we briefly describe the NFFT, the adjoint NFFT, and the inverse NFFT. These methods are implemented in our public software package [14].

### Nonequispaced FFT

The first problem to be addressed here, can be regarded as a matrix vector multiplication. For a finite number of given Fourier coefficients  $\hat{f}_{\mathbf{r}} \in \mathbb{C}$ ,  $\mathbf{r} \in I_{\mathbf{N}}^d := \{-\frac{N_1}{2}, \dots, \frac{N_1}{2} - 1\} \times \{-\frac{N_2}{2}, \dots, \frac{N_2}{2} - 1\} \times \dots \times \{-\frac{N_d}{2}, \dots, \frac{N_d}{2} - 1\}$  with  $\mathbf{N} := (N_1, \dots, N_d)^{\top} \in 2\mathbb{N}^d$  one wants to evaluate the trigonometric polynomial

$$f(\mathbf{x}) := \sum_{\mathbf{r} \in I_{\mathbf{N}}^d} \hat{f}_{\mathbf{r}} e^{2\pi i \mathbf{r} \mathbf{x}} \quad (6.1)$$

at given points  $\mathbf{x}_j \in [-\frac{1}{2}, \frac{1}{2})^d$ ,  $j = 0, \dots, M - 1$ . In matrix vector notation, see also (2.4), this reads as  $\mathbf{f} = \mathbf{A} \hat{\mathbf{f}}$ .

Fast approximate matrix vector multiplication with  $\mathbf{A}$  and its adjoint matrix  $\mathbf{A}^{\text{H}}$  are known as NFFT and adjoint NFFT, respectively. A unified approach for this task was suggested in [23, 28] and is based on the factorisation  $\mathbf{A} \approx \mathbf{BFD}$  and the use of a simultaneously in space and frequency localised window function  $\varphi$ . The diagonal matrix  $\mathbf{D}$  collects the inverse of the sampled

Fourier transform of the window function  $\mathbf{D} = [\mathbf{0}, \text{diag}(1/\hat{\varphi}(\mathbf{r}))_{\mathbf{r} \in I_N^d}, \mathbf{0}]^\top$ . Subsequently, we apply an oversampled Fourier matrix  $\mathbf{F} = \mathbf{F}_{\sigma N}$ , where  $\sigma > 1$  denotes a chosen oversampling factor. Finally, we multiply with the sparse matrix  $\mathbf{B} = (b_{j,\mathbf{l}})_{j=0,\dots,M-1, \mathbf{l} \in I_N^d}$  having for some cut-off parameter  $m \in \mathbb{N}$  at most  $(2m+1)^d$  nonzero entries per row, i.e.,

$$b_{j,\mathbf{l}} = \varphi\left(\mathbf{x}_j - \frac{\mathbf{l}}{\sigma N}\right), \quad -\frac{m}{\sigma N} \leq \mathbf{x}_j - \frac{\mathbf{l}}{\sigma N} \leq \frac{m}{\sigma N}. \quad (6.2)$$

The relation between speed and accuracy of the algorithm was initially investigated in [3, 7, 23, 28]. The accuracy of the NFFT increases exponentially with the cut-off parameter  $m$  for each fixed oversampling factor  $\sigma > 1$ . The total number of floating point operations is of order  $\mathcal{O}(|\sigma I_N^d| \log |\sigma I_N^d| + m^d M)$ .

In various papers, different window functions  $\varphi$  for the NFFT were considered, e.g. a Gaussian pulse tapered with a Hanning window in [6], Gaussian kernels combined with sinc kernels in [21], and special optimised windows in [6, 12]. Furthermore, special approaches based on scaling vectors [17], based on minimising a discrete norm of certain error matrices [18], or based on min-max interpolation [10] are proposed. We remark that the NFFT and its adjoint can be realised with a broad class of these window functions yielding the same accuracy by changing the cut-off parameter  $m$ . In particular, the obtained reconstruction quality in MRI is fairly independent of the particularly chosen window function. However, numerical results in [10, 11, 18] show that the Kaiser-Bessel window function provides the best accuracy for a fixed cut-off parameter  $m$ , i.e., number of nonzeros per row of the matrix  $\mathbf{B}$ . Moreover, the library adapts over a wide class of available memory through so called flags, see e.g. the Numerical Example 4. The manual to [14] and [15] present details for a suitable choice of the window function, the cut-off parameter, and the oversampling factor with respect to accuracy, speed and memory usage.

The adjoint algorithm, i.e., the evaluation of the sums  $\hat{\mathbf{g}}_{\mathbf{r}} := \sum_{j=0}^{M-1} f_j e^{-2\pi i \mathbf{r} \mathbf{x}_j}$ ,  $\mathbf{r} \in I_N^d$ , can be computed by the matrix vector multiplication with  $\mathbf{A}^H$ , where we obtain a fast algorithm by using the same factorisation  $\mathbf{A}^H \approx \mathbf{D}^\top \mathbf{F}^H \mathbf{B}^\top$ . It was already pointed out in [23, 27], that the gridding method is simply a fast algorithm for the multiplication of the matrix  $\mathbf{A}^H$  with a vector. Including a sampling density compensation yields the following gridding algorithm, see also [12, 21]:

- i) sampling density compensation, i.e., multiplication with a diagonal matrix  $\mathbf{W}$ ,
- ii) approximation to an oversampled Cartesian grid, i.e., multiplication with the matrix  $\mathbf{B}^\top$ ,
- iii) inverse fast Fourier transform, i.e., multiplication with  $\mathbf{F}^H$ ,
- iv) roll-off correction, i.e., multiplication with  $\mathbf{D}^\top$ .

Note, that the role of the window function, appearing in the matrices  $\mathbf{D}$  and  $\mathbf{B}$ , and the sampling density compensation, appearing in  $\mathbf{W}$ , should not be mixed up.

We stress again, that the NFFT and the adjoint NFFT (gridding) are algorithms that realise the matrix vector multiplications in a fast and efficient way.

## Inverse nonequispaced FFT

The aim of the inverse NFFT is to construct a trigonometric polynomial  $f$ , respectively its Fourier coefficients  $\hat{f}_{\mathbf{r}}$ ,  $\mathbf{r} \in I_N^d$ , such that  $f(\mathbf{x}_j)$  approximates given values  $y_j \in \mathbb{C}$ , i.e.,

$$y_j \approx f(\mathbf{x}_j) = \sum_{\mathbf{r} \in I_N^d} \hat{f}_{\mathbf{r}} e^{2\pi i \mathbf{r} \mathbf{x}_j}, \quad j = 0, \dots, M-1. \quad (6.3)$$

In matrix vector notation this reads as  $\mathbf{A}\hat{\mathbf{f}} \approx \mathbf{y}$ . We propose to solve this system of linear equations by the method of least squares with sampling density compensation weights  $w_j > 0$ , i.e.,

$$\min_{\hat{\mathbf{f}}} \left\| \mathbf{y} - \mathbf{A}\hat{\mathbf{f}} \right\|_{\mathbf{W}}^2 = \min_{\hat{\mathbf{f}}} \sum_{j=0}^{M-1} w_j |y_j - f(\mathbf{x}_j)|^2, \quad (6.4)$$

where  $\mathbf{W} := \text{diag}(w_j)_{j=0, \dots, M-1}$ . The iterative solution of this problem is addressed in [2, 9] by solving the explicitly formed Toeplitz system  $\mathbf{A}^H \mathbf{W} \mathbf{A} \hat{\mathbf{f}} = \mathbf{A}^H \mathbf{W} \mathbf{y}$ . This method is known as ACT (Adaptive weights, Conjugate gradients, Toeplitz) and has been proven to be superior to previous established methods like POCS (projection onto convex sets) or the Landweber iteration, cf. [9]. The inverse NFFT applies the conjugate gradient method as well, but uses the NFFT instead of methods for Toeplitz matrices.

**Acknowledgement.** The second author is grateful for partial support of this work by the German Academic Exchange Service (DAAD). We would like to thank the referees for their valuable suggestions. Moreover, we would like to thank Michael Schacht Hansen, Steffen Ringgaard (MR Research Centre, University of Aarhus, Denmark), and Holger Eggers (Philips Research, Sector Technical Systems, Hamburg, Germany) for numerous fruitful discussions and for provided datasets.

## References

- [1] C. B. Barber and H. Huhdanpaa. Qhull, Softwarepackage. <http://www.qhull.org>.
- [2] R. F. Bass and K. Gröchenig. Random sampling of multivariate trigonometric polynomials. *SIAM J. Math. Anal.*, 36:773 – 795, 2004.
- [3] G. Beylkin. On the fast Fourier transform of functions with singularities. *Appl. Comput. Harmon. Anal.*, 2:363 – 381, 1995.
- [4] Å. Björck. *Numerical Methods for Least Squares Problems*. SIAM, Philadelphia, 1996.
- [5] B. Desplanques, R. van de Walle, and I. Lemahieu. Iterative reconstruction of magnetic resonance images from arbitrary samples in k-space. *IEEE Trans. Nucl. Sci.*, 49:2268 – 2273, 2002.

- [6] A. J. W. Duijndam and M. A. Schonewille. Nonuniform fast Fourier transform. *Geophysics*, 64:539 – 551, 1999.
- [7] A. Dutt and V. Rokhlin. Fast Fourier transforms for nonequispaced data. *SIAM J. Sci. Stat. Comput.*, 14:1368 – 1393, 1993.
- [8] H. Eggers, T. Knopp, and D. Potts. Field inhomogeneity correction based on gridding reconstruction. *IEEE Trans. Med. Imag.*, to appear.
- [9] H. G. Feichtinger, K. Gröchenig, and T. Strohmer. Efficient numerical methods in non-uniform sampling theory. *Numer. Math.*, 69:423 – 440, 1995.
- [10] J. A. Fessler and B. P. Sutton. Nonuniform fast Fourier transforms using min-max interpolation. *IEEE Trans. Signal Process.*, 51:560 – 574, 2003.
- [11] K. Fourmont. Non equispaced fast Fourier transforms with applications to tomography. *J. Fourier Anal. Appl.*, 9:431 – 450, 2003.
- [12] J. I. Jackson, C. H. Meyer, D. G. Nishimura, and A. Macovski. Selection of a convolution function for Fourier inversion using gridding. *IEEE Trans. Med. Imag.*, 10:473 – 478, 1991.
- [13] Y. Kadah, A. Fahmy, R. Gabr, K. Heberlein, and X. Hu. Progressive magnetic resonance image reconstruction based on iterative solution of a sparse linear system. *Int. J. of Biomedical Imaging*, Article ID 49378:1 – 9, 2006.
- [14] S. Kunis and D. Potts. NFFT, Softwarepackage, C subroutine library. <http://www.tu-chemnitz.de/~potts/nfft>, 2002 – 2006.
- [15] S. Kunis and D. Potts. Time and memory requirements of the nonequispaced FFT. Preprint 06-01, TU-Chemnitz, 2006.
- [16] S. Matej, J. A. Fessler, and I. G. Kazantsev. Iterative tomographic image reconstruction using Fourier-based forward and back- projectors. *IEEE Trans. Med. Imag.*, 23:401 – 412, 2004.
- [17] N. Nguyen and Q. H. Liu. The regular Fourier matrices and nonuniform fast Fourier transforms. *SIAM J. Sci. Comput.*, 21:283 – 293, 1999.
- [18] A. Nieslony and G. Steidl. Approximate factorizations of Fourier matrices with nonequispaced knots. *Linear Algebra Appl.*, 266:337 – 351, 2003.
- [19] J. D. O’Sullivan. A fast sinc function gridding algorithm for Fourier inversion in computer tomography. *IEEE Trans. Med. Imag.*, 4:200 – 207, 1985.
- [20] C. C. Paige and M. A. Saunders. LSQR: An algorithm for sparse linear equations and sparse least squares. *ACM Transactions on Mathematical Software*, 8:43 – 71, 1982.

- [21] J. Pelt. Fast computation of trigonometric sums with applications to frequency analysis of astronomical data. In D. Maoz, A. Sternberg, and E. Leibowitz, editors, *Astronomical Time Series*, pages 179 – 182, Kluwer, 1997.
- [22] J. G. Pipe. Reconstructing mr images from undersampled data: data-weighting considerations. *Magn. Reson. Med.*, 43:867 – 875, 2000.
- [23] D. Potts, G. Steidl, and M. Tasche. Fast Fourier transforms for nonequispaced data: A tutorial. In J. J. Benedetto and P. J. S. G. Ferreira, editors, *Modern Sampling Theory: Mathematics and Applications*, pages 247 – 270. Birkhäuser, Boston, 2001.
- [24] K. P. Pruessmann, M. Weiger, P. Börnert, and P. Boesiger. Advances in sensitivity encoding with arbitrary k-space trajectories. *Magn. Reson. Med.*, 46:638 – 651, 2001.
- [25] V. Rasche, R. Proksa, R. Sinkus, P. Börnert, and H. Eggers. Resampling of data between arbitrary grids using convolution interpolation. *IEEE Trans. Med. Imag.*, 18:385 – 392, 1999.
- [26] Y. Saad. *Iterative Methods for Sparse Linear Systems*. PWS Publ., Boston, 1st edition, 1996.
- [27] G. E. Sarty, R. Bennett, and R. W. Cox. Direct reconstruction of non-cartesian k-space data using a nonuniform fast Fourier transform. *Magn. Reson. Med.*, 45:908 – 915, 2001.
- [28] G. Steidl. A note on fast Fourier transforms for nonequispaced grids. *Adv. Comput. Math.*, 9:337 – 353, 1998.
- [29] B. P. Sutton, J. A. Fessler, and D. C. Noll. A min-max approach to the nonuniform  $N$ -dimensional FFT for rapid iterative reconstruction of MR images. In *Proc. ISMRM 9th Scientific Meeting*, page 763, 2001.
- [30] B. P. Sutton, D. C. Noll, and J. A. Fessler. Fast, iterative, field-corrected image reconstruction for MRI in the presence of field inhomogeneities. *IEEE Trans. Med. Imag.*, 22:178 – 188, 2003.