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A Power-Efficient Continuous-Time Incremental Sigma-Delta ADC for Neural Recording Systems

Sha Tao, *Student Member, IEEE*, and Ana Rusu, *Member, IEEE*

Abstract—This paper presents an analog-to-digital converter (ADC) dedicated to neural recording systems. By using two continuous-time incremental sigma-delta ADCs in a pipeline configuration, the proposed ADC can achieve high-resolution without sacrificing the conversion rate. This two-step architecture is also power-efficient, as the resolution requirement for the incremental sigma-delta ADC in each step is significantly relaxed. To further enhance the power efficiency, a class-AB output stage and a dynamic summing comparator are used to implement the sigma-delta modulators. A prototype chip, designed and fabricated in a standard 0.18 μm CMOS process, validates the proposed ADC architecture. Measurement results show that the ADC achieves a peak signal-to-noise-plus-distortion ratio of 75.9 dB over a 4 kHz bandwidth; the power consumption is 34.8 μW , which corresponds to a figure-of-merit of 0.85 pJ/conv.

Index Terms—Analog-to-digital converter (ADC), incremental sigma-delta ADC, two-step ADC, continuous-time.

I. INTRODUCTION

OVER the past decade, recordings of neuropotentials using multi-electrode arrays (MEAs) have emerged as an effective solution for brain-computer interface (BCI) research and applications [1], [2]. Consequently, there is growing interest in the development of integrated circuits for multi-channel neural recording systems, which demand low power consumption and small chip area. In such systems, the Analog-to-Digital Converter (ADC) is an important building block that has a dominant impact on the speed and resolution of the entire system. A successive-approximation-register (SAR) ADC, which features medium-resolution and excellent power-efficiency, is usually adopted in state-of-the-art neural recording systems [2]–[4]. Such an SAR ADC based signal chain, however, imposes stringent requirements on front-end circuitries [5]. By employing a high-resolution ADC, these requirements can be much relaxed, and several power hungry signal conditioning blocks (e.g., additional gain stages and active anti-aliasing filters) can be simplified or even eliminated. The significant reduction of front-end circuit complexity, on the other hand, is traded with the challenge of designing a high-resolution ADC with high power-efficiency.

Sigma-delta ($\Sigma\Delta$) ADCs achieve high-resolution with relaxed matching requirements comparing to their Nyquist counterparts. Traditional $\Sigma\Delta$ ADCs capture a band-limited stream of inputs and produce the corresponding outputs as average. Without one-to-one mapping between input and output samples, they can hardly be multiplexed between channels,

with the exception of applying special techniques [6], [7]. Incremental $\Sigma\Delta$ ($\text{I}\Sigma\Delta$) ADCs, on the contrary, reset their modulators and digital filters after each conversion, and thus are well suited to process multiplexed signals. The first-order $\text{I}\Sigma\Delta$ ADC [8] can achieve high resolution, but at the cost of very long conversion time, thus resulting in poor power-efficiency. Higher-order and multi-bit $\text{I}\Sigma\Delta$ ADCs have been developed to speed up the conversion rate of $\text{I}\Sigma\Delta$ ADCs [9]–[12]. Alternatively, ADC architectures that combine the $\text{I}\Sigma\Delta$ with a Nyquist ADC, such as extended counting (EC) [13] or extended range (ER) ADCs [14], have been proposed to effectively improve the resolution of $\text{I}\Sigma\Delta$ ADCs.

$\text{I}\Sigma\Delta$ ADCs developed up to now, almost exclusively employ discrete-time (DT) loop filters. So far, the only continuous-time (CT) $\text{I}\Sigma\Delta$ prototypes existing in the literature include the first-order CT $\text{I}\Sigma\Delta$ ADCs [15], [16] presented as parts of an integrated system, and a higher-order CT $\text{I}\Sigma\Delta$ ADC [17] reported recently. $\text{I}\Sigma\Delta$ ADCs implemented with CT loop filters have relaxed settling and bandwidth requirements on the active blocks compared with their DT counterparts, thus leading to potential power reduction. This advantage still holds even with the existence of a sample-and-hold (S/H) preceding the ADC, as the loop filter processes each input in a continuous fashion. The front-end S/H, however, would induce considerable power and noise penalties. Therefore, implementations without a front-end S/H are preferred.

In this paper, we take a step further by proposing a more power-efficient CT $\text{I}\Sigma\Delta$ alternative for high-resolution multi-channel A/D conversion. The proposed architecture combines the speed of pipelined ADCs and the resolution of $\Sigma\Delta$ ADCs. By pipelining CT $\text{I}\Sigma\Delta$ stages, high-resolution can be achieved without sacrificing the conversion rate [18]. This feature would be important in the next generation neural recording systems, in which the high-density MEAs will be scaling to thousands of electrodes [19]. Compared to higher-order single-loop $\text{I}\Sigma\Delta$ ADCs, the 2nd-order loop filter in each stage requires less coefficient scaling and is thus more power-efficient. Compared to EC/ER architectures, which require extra cycles for EC/ER conversion, this architecture can operate faster when achieving the same resolution. The paper is organized as follows. Section II describes design considerations of the target neural recording system and derives ADC specifications. Section III presents operation principle and design methodology of the proposed CT $\text{I}\Sigma\Delta$ ADC. The circuit implementation of the ADC is detailed in Section IV. Measurement results of the prototype ADC and comparison with state-of-the-art are given in Section V. Finally, Section VI concludes the paper.

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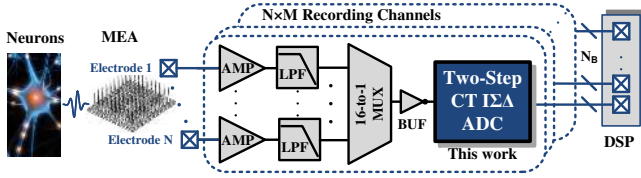


Fig. 1: Simplified architecture of a multi-channel neural recording system based on a high-resolution ADC.

II. SYSTEM ARCHITECTURE AND ADC SPECIFICATIONS

The electrocorticography (ECoG), which records the neuron activity from the surface of the brain [1], is the target neural signal. ECoG-based BCI systems are more invasive than the traditional electroencephalography (EEG)-based systems, and thus can provide better spatial resolution and record higher-frequency content of the signal. Clinical studies using ECoG recordings in humans show that the functional activation of a cortex is associated with an increase in power in the high-gamma frequency range (60-200 Hz) [20]. It has been also shown that at least a 64-electrode setup is needed for achieving useful and reliable results [21].

The simplified architecture of a multi-channel ECoG-based neural recording system is shown in Fig. 1, where the proposed two-step CT $\Sigma\Delta$ ADC is shared among multiple recording channels. In $\Sigma\Delta$ ADCs, to achieve ideal behavior, the input signal is held constant for the entire conversion, which requires a S/H preceding the ADC. In the proposed system architecture, the S/H is removed from the front-end circuitry. As it is illustrated later, removing the S/H alters the ideal signal transfer function of the loop filter, and marginally attenuates the signal amplitude. This might be a good trade-off since it eliminates the need for implementing both a high-resolution S/H, and a low-noise high-order anti-aliasing filter. By this means, further reduction in both power and area can be achieved for the entire integrated neural recording system.

In a multi-channel system, signals from all channels should be fed into a single ADC to save chip area. However, this demands a high sampling rate ADC, which leads to excessive power consumption. A practical approach is to find the optimal number of channels per ADC so as to obtain a better trade-off between power and area. For the targeted 64-channel system, 16 channels are shared by one ADC, to achieve the minimum power-area product for the entire system [22]. Without utilizing a variable-gain amplifier as in many conventional ECoG systems, such as [23], a 80 dB dynamic range (DR) is typically required for the ADC to resolve ECoG signals [24]. So, the proposed ADC should achieve a 13-14 bits resolution and handle inputs from 16 channels with 60-200 Hz per channel.

III. ADC ARCHITECTURE

A. Operation Principle

The block diagram of the proposed two-step CT $\Sigma\Delta$ ADC and the associated timing diagram are shown in Fig. 2. At the beginning of each conversion, one of the input channels is selected by the MUX. Then, two CT $\Sigma\Delta$ ADCs are initially

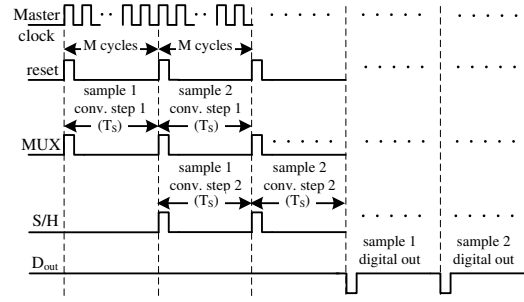
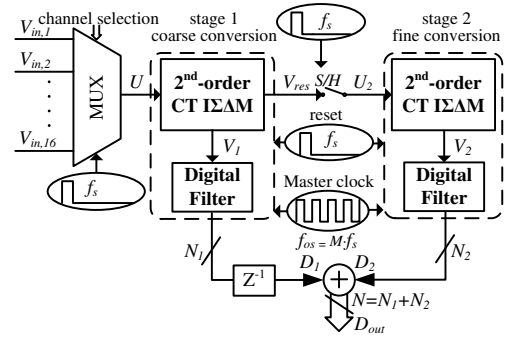


Fig. 2: Block diagram of the proposed two-step CT $\Sigma\Delta$ ADC.

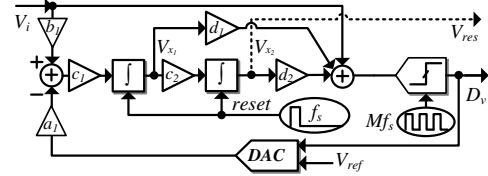


Fig. 3: The 2nd-order CT $\Sigma\Delta$ M with CIFF+IFF topology.

reset and process the sample in a pipeline fashion: stage 1 for coarse conversion and stage 2 for fine conversion. The CT $\Sigma\Delta$ modulator in stage 1 processes the input sample, U , with an oversampling clock, $f_{OS} = Mf_S$, where M is the number of clock cycles per conversion and f_S is the frequency of the periodical resetting. After M cycles, the most significant bits (MSBs), N_1 , are extracted by the digital filter. The modulator and digital filter are then reset, and an analog residue V_{res} is captured by the S/H. Note that V_{res} can fit directly the input range of the second stage ADC. So, this architecture does not require the inter-stage amplification needed in conventional pipelined ADCs. The sampled residue voltage, U_2 , is passed to the CT $\Sigma\Delta$ modulator in stage 2, and oversampled again with f_{OS} . After M cycles, the least significant bits (LSBs), N_2 , are extracted, and the modulator and digital filter are reset. By digitally combining the MSBs and LSBs from the two conversion stages, a resolution of $N_1 + N_2$ can be ideally achieved. Due to the two-step pipelining operation, the coarse conversion can process the next sample immediately after the fine conversion starts. Therefore, the effective conversion rate is determined by the conversion time of only one stage while the conversion resolution is doubled.

As shown in Fig. 3, for each 2nd-order $\Sigma\Delta$ modulator, the cascaded integrators in feed-forward (CIFF) configuration with input signal feed-forward (IFF) topology is used to reduce the

signal swing in the integrators and minimize the performance degradation due to coefficient variations. The use of a single-bit quantizer minimizes the digital filter complexity and avoids the need of linearization techniques in the feedback digital-to-analog converter (DAC). For the feedback DAC, a non-return-to-zero (NRZ) scheme is employed considering the best trade-off between jitter sensitivity and power consumption [25].

B. Design Methodology

Given the specifications described in Section II, the system level design of the proposed ADC follows these steps.

1) *Effective conversion rate*: In this work, the multi-channel system consists of 16 channels, and each channel carries a signal bandwidth of 200 Hz. Due to time multiplexing, the effective sampling rate for each channel is given by the ADC's conversion rate divided by the number of channels. By selecting a sampling rate that is slightly higher than the Nyquist rate, the maximum time slot devoted to each channel is: $T_{S,max} = 1/(200 \text{ Hz} \times 2.5 \times 16) = 125 \mu\text{s}$. This corresponds to an effective conversion rate of $f_S = 8 \text{ kHz}$.

2) *Resolution of each step*: In traditional pipelined ADCs, a range overlap is usually introduced between adjacent conversion stages to make sure that the residue voltage will not exceed the input range of the following stage. In an $\text{I}\Sigma\Delta$ modulator based conversion stage, on the other hand, the output of the last integrator, where the residue voltage is sampled, is theoretically bounded assuming constant input [26]. In addition, even considering the circuit non-idealities, the voltage swing at the last integrator's output can still be limited within a practical bound (i.e., $\pm V_{ref}$) by applying proper coefficient scaling. Therefore, range overlap is not necessary for the proposed ADC architecture. As the two-step ADC targets a resolution of 14-bit, 8-bit is allocated for each conversion step to account for circuit non-idealities.

3) *Time-domain analysis*: Assuming that each conversion requires n cycles, the two integrators' outputs $V_{x_1}(t)$ and $V_{x_2}(t)$ can be expressed in the time domain as [9]:

$$V_{x_1}(n) = c_1 b_1 n V_i - c_1 a_1 V_{ref} \sum_{i=0}^{n-1} D_v(i) \quad (1)$$

$$V_{x_2}(n) = c_2 c_1 b_1 \frac{n(n-1)}{2} V_i - c_2 c_1 a_1 V_{ref} \sum_{j=0}^{n-1} \sum_{i=0}^{j-1} D_v(i) \quad (2)$$

where V_i is the input from one channel that is assumed to change very slowly during each conversion; $V_{x_1}(n)$ and $V_{x_2}(n)$ are the analog voltages at the two integrators' outputs after n clock cycles; $D_v(i) = \pm 1$ is the modulator output in the i^{th} cycle. Note that through coefficient scaling, $V_{x_2}(n)$ can be bounded between the DAC references as:

$$\begin{aligned} -V_{ref} &\leq c_2 c_1 b_1 \frac{n(n-1)}{2} V_i \\ &- c_2 c_1 a_1 V_{ref} \sum_{j=0}^{n-1} \sum_{i=0}^{j-1} D_v(i) \leq +V_{ref} \end{aligned} \quad (3)$$

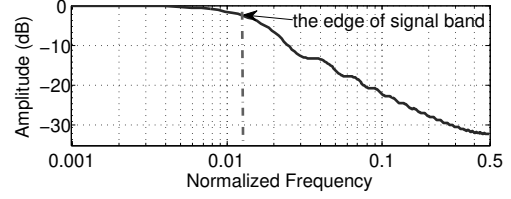


Fig. 4: STF of a 2nd-order $\text{I}\Sigma\Delta$ ADC when S/H is removed.

By rearranging (3), it gives the following equation:

$$\begin{aligned} -\frac{V_{ref}}{c_2 c_1 b_1 \frac{n(n-1)}{2}} &\leq V_i - \frac{a_1}{b_1 \frac{n(n-1)}{2}} V_{ref} \sum_{j=0}^{n-1} \sum_{i=0}^{j-1} D_v(i) \\ &\leq +\frac{V_{ref}}{c_2 c_1 b_1 \frac{n(n-1)}{2}} \end{aligned} \quad (4)$$

4) *Required number of clock cycles*: The middle term of (4) denotes the difference between the input V_i , and the measurable modulator output D_v , after n clock cycles. It is then possible to estimate the input as:

$$\hat{V}_i = \frac{a_1}{b_1 \frac{n(n-1)}{2}} V_{ref} \sum_{j=0}^{n-1} \sum_{i=0}^{j-1} D_v(i) \quad (5)$$

The difference between V_i and \hat{V}_i is the quantization error, which is bounded within $\pm \frac{1}{2} V_{LSB}$ in an ideal ADC. According to (4), the V_{LSB} can be expressed by:

$$V_{LSB} = 2 \times \frac{V_{ref}}{c_2 c_1 b_1 \frac{n(n-1)}{2}} \quad (6)$$

After n clock cycles, the conversion resolution is given by:

$$\begin{aligned} n_{bit} &= \log_2 \left(\frac{2 \times V_{i,max}}{V_{LSB}} \right) = \log_2 \left(\frac{u_{max} V_{ref}}{V_{ref}} c_2 c_1 b_1 \frac{n(n-1)}{2} \right) \\ &= \log_2 (n(n-1)) + \log_2 (c_2 c_1 b_1) + \log_2 \left(\frac{u_{max}}{2} \right) \end{aligned} \quad (7)$$

where $u_{max} = \frac{V_{i,max}}{V_{ref}}$ is the normalized maximum input, which limits the peak input amplitude to a fraction of the DAC reference, V_{ref} . Accordingly, the number of clock cycles, M , for achieving the desired resolution, n_{bit} , can be found as:

$$M = 2^{[n_{bit} + \log_2(b_1 c_1 c_2) + \log_2(0.5 u_{max})]/2} \quad (8)$$

5) *Modulator design*: For the 2nd-order modulator, the DT noise transfer function $NTF(z)$ is designed with the Schreier's Toolbox [27]. The DT loop filter is derived as $LF(z) = 1/NTF(z) - 1$. The signal transfer function of the CIFF+IFF topology is unity. However, removing the S/H block in front of an $\text{I}\Sigma\Delta$ results in a modified STF as [28]:

$$STF(z) = \frac{1 + 2z^{-1} + 3z^{-2} + \dots + Mz^{-(M-1)}}{M(M+1)/2} \quad (9)$$

The frequency response of the modified $STF(z)$ is plotted in Fig. 4 for $M = 40$. It shows that the signal is attenuated approximately 2.55 dB at the edge of the signal band.

TABLE I: Coefficient values of the modulator shown in Fig. 3

a_1	b_1	c_1	c_2	d_1	d_2
1	1	0.4	0.8	3.1251	1.5625

6) *CT loop filter coefficients*: The CT loop filter is determined by the impulse invariant transformation [29] as:

$$LF(z) = \mathcal{Z} \left\{ \mathcal{L}^{-1} [LF(s)R_{DAC,NRZ}(s)]|_{t=nT_{OS}} \right\} \quad (10)$$

Transient simulations are used to assure that the second integrator's output is bounded between $\pm V_{ref}$. The resulting modulator's coefficients, assuming a normalized sampling rate of 1 (i.e., $f_{OS} = 1$), are listed in Table I.

7) *Residue voltage generation*: In the proposed two-step architecture, the input of the fine conversion stage is the sampled residue voltage of the coarse conversion stage. As aforementioned, because of the CIFF+IFF loop filter topology and the incremental operation, the quantization error of the coarse conversion stage can be readily obtained in analog form. Following the analysis in steps 3) and 4), the relative quantization error (with respect to 1 LSB) can be found by:

$$q = \frac{\hat{V}_i - V_i}{V_{LSB}} = \frac{c_2 c_1 a_1}{2} \sum_{j=0}^{n-1} \sum_{i=0}^{j-1} D_v(i) - \frac{c_2 c_1 b_1}{2} \frac{n(n-1)}{2} \frac{V_i}{V_{ref}} \quad (11)$$

By combining (11) and (2), the second integrator's output is determined as $V_{x_2}(n) = -2V_{ref} \cdot q$. Then, at the end of each conversion, i.e., after M clock cycles, the residue voltage can be found as $V_{res} = V_{x_2}(M) = -2V_{ref} \cdot q$. So far, a constant input, V_i , has been assumed in deriving the equations. By removing this assumption, the analog representation of the residue, V_{res} , will not be affected. A time-varying input, $V_i(i)$, however, would lead to in-band amplitude attenuation, as illustrated in Fig. 4, which can be compensated in the digital domain if needed [14].

8) *Digital filter design*: The digital filter is designed to make sure that the quantization error of the $\Sigma\Delta$ ADC in each stage, given by (11), can be derived from the second integrator's output, as $-V_{x_2}(M)/(2V_{ref})$, after M clock cycles. Following the method in [17], the digital filter transfer function, $H_{DF}(z)$, can be derived as:

$$H_{DF}(z) = \left[\frac{z^{-2}}{(1-z^{-1})^2} + \frac{1}{2} \frac{z^{-1}}{1-z^{-1}} \right] \frac{2}{M(M-1)} \quad (12)$$

9) *Theoretical resolution*: Considering only the quantization noise, the theoretical signal-to-quantization-noise-ratio (SQNR) of the two-step ADC can be estimated as:

$$\text{SQNR}_{2\text{step}} [\text{dB}] \approx 20 \log_{10} \left[\frac{2V_{ref}}{u_{max} V_{ref}} \frac{1}{M(M-1)} \right] + 20 \log_{10} \left[\frac{2V_{ref}}{V_{res,peak}} \frac{1}{M(M-1)} \right] \quad (13)$$

where $V_{res,peak}$ is the peak amplitude of the residue voltage. The theoretical SQNR estimated by (14) is compared against system-level simulation results, when the number of cycles in each conversion, M , is swept, as shown in Fig. 5. Good

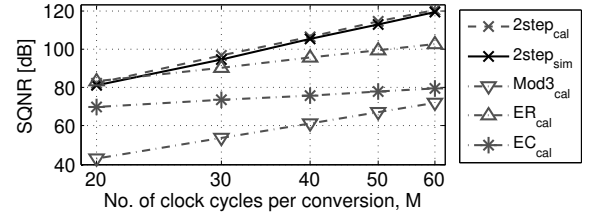


Fig. 5: Simulated ($2\text{step}_{\text{sim}}$) and theoretical ($2\text{step}_{\text{cal}}$) SQNR of the two-step CT $\Sigma\Delta$ ADC. Theoretical results of the 3rd-order $\Sigma\Delta$ (Mod3_{cal}) [17], ER $\Sigma\Delta$ ADC (ER_{cal}) [14] and the EC $\Sigma\Delta$ ADC (EC_{cal}) [13] are also included in this plot.

matching between the simulated and estimated SQNRs is achieved. For the sake of comparison, the theoretical results of the EC $\Sigma\Delta$ ADC [13], the ER $\Sigma\Delta$ ADC [14] (8-bit is used for the extended conversion in both cases) and the 3rd-order $\Sigma\Delta$ ADC [17] are included in this plot. As it can be appreciated from the figure, the proposed two-step ADC requires the lowest M to achieve a high theoretical resolution.

It is also interesting to compare the proposed ADC to a 2-2 MASH CT $\Sigma\Delta$ ADC, as both architectures have similar analog complexity and benefit from processing the residue of a 2nd-order $\Sigma\Delta$ stage. Under ideal conditions, the resolution of the proposed architecture is the sum of two 2nd-order $\Sigma\Delta$ ADCs, while the 2-2 MASH architecture achieves a resolution equivalent to 4th-order noise shaping. Thus, for a given M , the SQNR of the 2-2 MASH architecture is not as good as the one achieved by the proposed two-step ADC. In addition, the effectiveness of the noise shaping in MASH architectures relies on the perfect cancellation of the quantization noise of the first stage. This indicates that the non-idealities of all integrators in the first stage are equally important in determining the noise leakage to the overall output. As it is shown later, in the proposed architecture, only the non-idealities of the first integrator limits the overall performance.

10) *Circuit non-idealities*: Prior to circuit implementation, extensive simulations were performed at system-level in Matlab/Simulink and at behavioral-level in Cadence using Verilog-A models. Circuit non-idealities that are critical for the CT implementations have been examined to derive the specifications of circuit blocks and clock signals. Simulation results show that the 1st integrator in stage 1 limits the overall performance and the specifications for the 2nd integrator as well as the integrators in stage 2, e.g., circuit noise, amplifier's gain, integrator's coefficient variation, clock jitter and excess loop delay, are greatly relaxed. In addition, since both the noise and the accuracy of the inter-stage S/H block are set only by the DR of stage 2, the requirements for the inter-stage S/H block are also very relaxed.

IV. CIRCUIT DESIGN AND IMPLEMENTATION

The block diagram of the implemented two-step CT $\Sigma\Delta$ ADC is shown in Fig. 6. The two 2nd-order CT $\Sigma\Delta$ modulators and the S/H between the two stages have been implemented in a 0.18 μm CMOS process. To achieve the target resolution, $M = 40$ is chosen for the 4 kHz signal bandwidth.

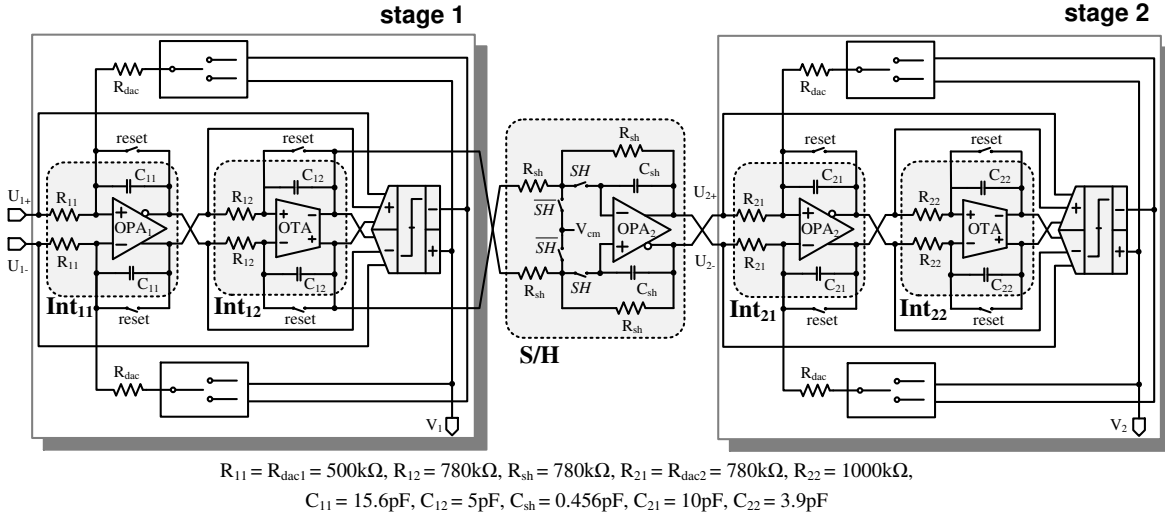


Fig. 6: Simplified circuit block diagram of the implemented two-step CT $I\Sigma\Delta$ ADC.

This corresponds to a 320 kHz oversampling clock frequency. Active-RC integrators are used to implement the loop filters for better linearity, larger signal swing and lower sensitivity to parasitics than their G_mC counterparts.

Given the coefficients specified in Table I, the values of passive components are derived with respect to the oversampling frequency, f_{OS} . In the proposed architecture, the first integrator in the first stage, Int_{11} , is the most critical block that dominates the noise performance of the entire ADC. The circuit noise at Int_{11} has five contributors: the input resistance, R_{11} , the DAC resistance, R_{dac} , the reset switch resistance, R_{rst} (kT/C noise), the input transconductance, gm , and the flicker noise of the Opamp. Considering that for a power-efficient design, the ADC's performance is limited by circuit noise rather than quantization noise [30], R_{11} , R_{dac} and C_{11} can be determined. The passive values of Int_{21} are determined in a similar way with half of the resolution specification. Due to the noise-shaping characteristics of the loop filter, linearity and noise requirements on Int_{12} and Int_{22} are further relaxed with respect to the first integrator. R_{sh} and C_{sh} in the S/H are chosen, considering the trade-off among sampling accuracy, settling time, thermal noise and loading condition.

A. Opamps and OTAs

A power-efficient, low noise Class-A/Class-AB amplifier, OPA_1 , is chosen for the Int_{11} , as shown in Fig. 7 (a). In the input stage, PMOS differential pairs M_1 and M_2 with very large gate area ($W/L = 320\mu/4\mu$) are used to achieve low flicker noise and reduced sensitivity to mismatch. Additionally, the thermal noise contribution from the current source transistors M_3 and M_4 is minimized by using source degeneration resistors R_{deg} . In the output stage, the Class-AB operation is achieved by dynamically biasing the output transistors M_5/M_6 and M_7/M_8 through the current mirrors M_9/M_{10} and M_{11}/M_{12} . The peak transient current delivered from this output stage to the integrating capacitor C_{11} can be much higher than the DC biasing current. The common-

mode voltage of the output stage can be sensed and stabilized by the common-mode feedback (CMFB) shown in Fig. 8 (a) [31]. Since the DC current in dynamic biasing current mirrors are set by the DC voltages at nodes 1 and 2, another dedicated feedback loop is usually desired for the input stage [31], [32]. Instead of employing two independent CMFB loops which may potentially lead to instability, a simple CMFB structure is used here to set the common-mode voltages for the input stage. As shown in Fig. 7 (a), two very large resistors, R , are used to sense and average the DC voltages at nodes 1 and 2, and then feed it back to the gates of M_3 and M_4 . The OPA_2 used in Int_{21} is implemented as a two-stage Class-A Opamp, as shown in Fig. 7 (b), and its CMFB circuit is shown in Fig. 8 (b). The amplifiers employed in the second integrators (Int_{12} and Int_{22}) in the loop filters have relaxed swing, GBW, slew rate and loading requirements. They have been implemented with a current-mirror OTA, as shown in Fig. 7 (c). An NMOS input differential pair is adopted to obtain better gm efficiency and consequently less current consumption. To avoid loading the OTA resistively, two differential pairs are used to sense the output voltages, as shown in Fig. 8 (c). Linearity of these differential pairs and hence the output swing of the OTA is enhanced by the linearization transistors $M_{R1} - M_{R4}$ acting as source degeneration resistances [33].

B. Summation, Quantizer, and Feedback DAC

State-of-the-art designs of CT CIFF loop filters usually employ a dedicated summing amplifier to perform the weighted addition of feed-forward coefficients [31]. An alternative solution is to integrate the weighted addition into the last integrator [34]. This solution, however, imposes tougher requirements (e.g., larger output swing) on the last integrator. For the two-step architecture, in particular, reusing the last integrator for summation is not desired, as its outputs need to be directly accessed by an inter-stage S/H. In order to save power and area, a dynamic summing comparator is designed to perform both the 1-bit quantization and the weighted addition, as shown in

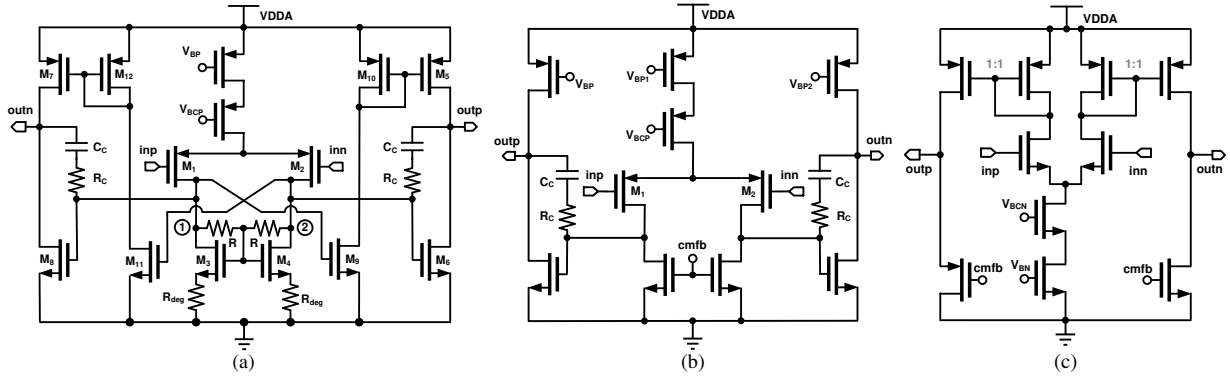


Fig. 7: Amplifier Schematics: (a) 2-stage Class-A/Class-AB Opamp, (b) 2-stage Class-A Opamp, and (c) Current-mirror OTA.

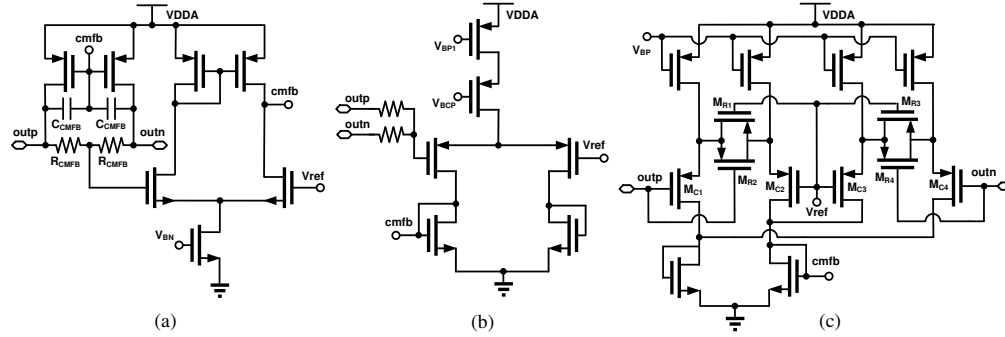


Fig. 8: CMFB circuits used in the amplifiers.

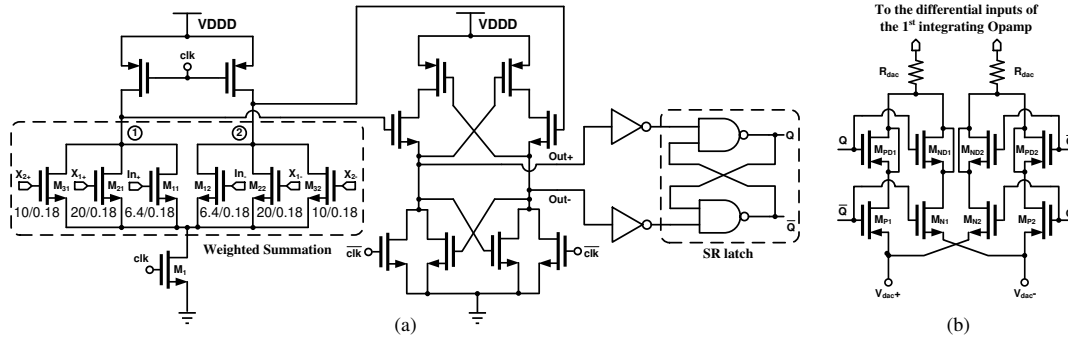


Fig. 9: Illustration of the feed-forward coefficient summation, 1-bit quantization, and feedback DAC path.

Fig. 9 (a). The 1-bit quantization is implemented by a power-efficient two-stage comparator. Compared to conventional dynamic comparators, the two-stage dynamic comparator [35] features an input amplification stage with dynamic biasing followed by a latching stage. It provides better kickback noise isolation and more freedom in optimizing the trade-off between latching speed and offset. By sizing the tail transistor, M_1 , wide enough, the speed of the comparator can be improved at the expense of the increased offset. This comparator consumes only transient current, and its averaged dynamic current consumption is proportional to the clock rate. The weighted addition is realized with virtually no additional power and area by integrating it into the comparator [36]. In this design, the 1st and 2nd integrator's outputs ($X_{1\pm}$ and $X_{2\pm}$) as well as the input signal (In_{\pm}) are tied to the comparator

through three differential pairs, as shown in Fig. 9 (a). The three differential inputs are added in current at the nodes 1 and 2, and the weights in the current addition are related to the feed-forward coefficients d_1 , d_2 and 1. When the input transistors are designed with the same length, these coefficients can be realized by sizing the widths of these input transistors.

The 1-bit NRZ DAC, as shown in Fig. 9 (b), consists of two sets of complementary switches and feedback resistors. The positive and negative DAC references V_{dac+} and V_{dac-} are switched by the differential outputs of the quantizer, Q and \bar{Q} . In addition, dummy transistors, M_{ND1} , M_{PD1} , M_{ND2} and M_{PD2} , are placed alongside with the switch transistors to reduce the glitches induced by the switching instances. Outputs of the feedback resistances R_{dac} are connected to virtual ground nodes of the first integrating Opamp.

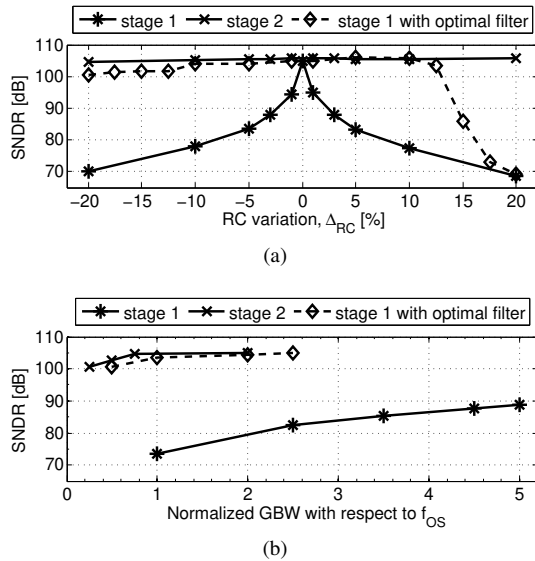


Fig. 10: SNDRs of the two-step CT $\Sigma\Delta$ ADC versus (a) integrator's coefficient variation and (b) amplifier's finite GBW.

C. Digital Filter and Combination Logic

As shown in Fig. 2, the two $\Sigma\Delta$ modulator's output bit-streams, V_1 and V_2 , are digitally filtered before the weighted combination. The ideal transfer function of the digital filter, i.e., (12) in Section III-B, is derived as a matched filter that realizes the digital filter as the exact replica of the analog loop filter. This digital filter is the sum of a cascade of integrators that processes $M = 40$ samples coming from one of the $\Sigma\Delta$ modulators. It can be treated as an M -length finite impulse response (FIR) filter with appropriate filter coefficients [26]. These coefficients can be obtained by computing the M -length impulse response of the transfer function $H_{DF}(z)$. The final outputs of the digitized results, D_1 and D_2 , are the weighted sum of the V_1 and V_2 samples with a decimation ratio of M . The digital combination logic in the two-step ADC is expressed as: $D_{out,2step} = (D_1 \times 2^8 + D_2)/2^8$.

The presence of circuit non-idealities would induce mismatch between the analog and digital transfer functions. This makes the residue, V_{res} , no longer an accurate representation of the quantization error in the coarse conversion stage. The ADC's sensitivity to the integrator's coefficient variation and amplifier's finite GBW has been evaluated by behavioral simulations, as shown in Fig. 10 (a) and Fig. 10 (b). As it can be seen in Fig. 10, without any calibration, the signal-to-noise and distortion ratio (SNDR) of the two-step ADC is sensitive to both the coefficient variation and the finite GBW in the coarse conversion stage (stage 1). Therefore, an optimal digital filter is required in stage 1 to take better advantage of the quantization error refinement of the proposed architecture. In order to maximize the SNDR of the two-step ADC, the built-in Matlab optimization algorithm, *fmincon* [37], which finds the optimal coefficients of the FIR filter, is employed. The optimization algorithm searches for a constraint minimum of an objective function of multiple variables at an initial

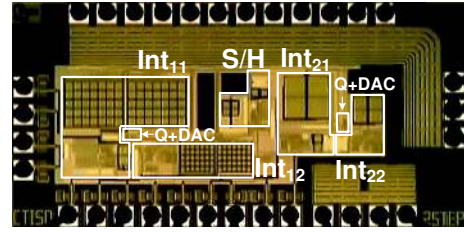


Fig. 11: Chip micrograph of the prototype ADC.

estimate. In particular, by using the coefficients calculated from (12) as the initial estimate, and the coefficients of the M -length FIR filter as the variables, this algorithm aims to minimize the inverse of the SNDR improvement of the optimized filter coefficients with respect to the original ones [17]. This digital filter optimization is a reference-free method that can operate directly with the recorded modulator's output stream. It can be run at each level of design phase to obtain a set of optimized filter coefficients taking into account circuit non-idealities. Implementation details and the benchmark of such an FIR digital filter can be found in [38]. As shown in Fig. 10, after applying the optimal filter, the requirements on both the integrator's coefficient variation and the amplifier's finite GBW are much relaxed for stage 1. Transistor-level and post-layout transient noise simulations show that the two-step CT $\Sigma\Delta$ ADC achieves SNDRs of 84.58 dB and 79.08 dB, respectively. In addition, Monte-Carlo simulations show that the SNDR is not affected significantly by process variation. Simulation results also reveal that when the analog supply goes below 1.1 V, the SNDR starts to degrade. In addition, the simulated SNDR is almost constant over the commercial temperature range (0 to 70 °C).

V. EXPERIMENTAL RESULTS

The proposed two-step CT $\Sigma\Delta$ ADC was fabricated in a standard 0.18 μm CMOS process. Fig. 11 shows the chip micrograph. The active area of the prototype, excluding the bonding pads and I/O drivers, is approximately 0.337 mm^2 . The digital filters, as well as the digital combination of MLBs and LSBs, described in Section IV-C, were implemented in Matlab. Bit-stream samples from the two $\Sigma\Delta$ modulators are captured, and fed into the optimization algorithm to get a specific set of filter coefficients that are optimal for the fabricated chip sample. The core circuit is powered by a 1.2 V analog supply and a 1.8 V digital supply with separate grounds. For further noise reduction, decoupling capacitors are placed between power supplies and grounds in the unused chip area. The prototype chip is assembled in a 44-pin plastic leaded chip carrier (PLCC) package and mounted on a customized evaluation board (EVB), as shown in Fig. 12.

A. Measurement Setup

Apart from the device under test (DUT) ADC chip, the EVB features mainly signal conditioning and voltage/current biasing circuitries. The input test signal is brought on board

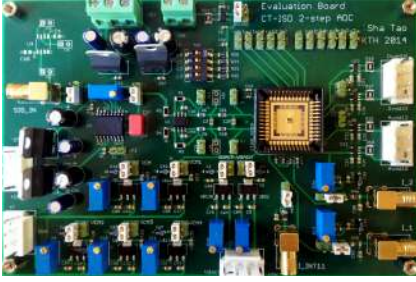


Fig. 12: Photograph of the customized evaluation board.

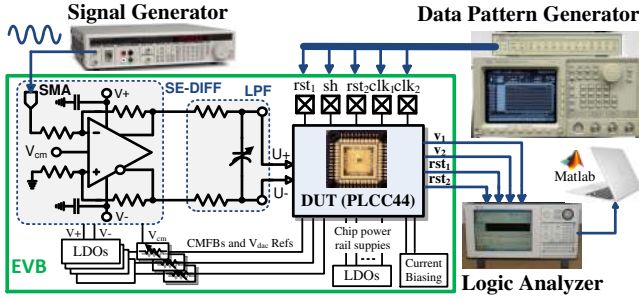


Fig. 13: Simplified block diagram of the measurement setup.

through an SMA connector and then passed through a single-ended to differential conversion (SE-DIFF) buffer. A single-pole RC filter is placed between the buffer outputs and the ADC inputs to reduce the noise contribution due to the driving circuit. To attenuate voltage ripple and noise from the external power supplies, low-dropout regulators (LDOs) are used on the EVB to generate various power supplies and voltage references required for the chip operation. The bias currents generated on board are derived from one of the power supplies using potentiometers and series resistors.

The measurement setup is depicted in Fig. 13. A sinusoidal input with the bandwidth of one channel (approximately 200 Hz), is used as the test signal, and the performance is determined by the ADC's bandwidth which covers 16 channels. An ultra-low distortion function generator (Stanford Research DS360) is used to drive the test EVB. The required synchronized signals for the chip operation are generated by a data pattern generator (Sony/Tektronix DG2020A). As shown in Fig. 13, the generated signals are used as S/H clock (sh), reset signals (rst_1 , rst_2), and oversampling clocks (clk_1 , clk_2) for the two conversion steps. The digital output data streams, i.e., the modulators outputs (v_1 , v_2) and reset signals (rst_1 , rst_2) are captured by a logic analyzer (Tektronix TLA621). These streams are then imported into Matlab where they are processed by the digital filters described in Section IV-C. A Fast-Fourier-Transform (FFT) is performed, and a Blackman-Harris window is applied to compute the performance metrics.

B. Measurement Results

The measured static power consumption of the ADC, excluding the output drivers, is $34.8 \mu\text{W}$. According to post-layout simulations, $15.1 \mu\text{A}$ is consumed in the Int_{11} , $2.5 \mu\text{A}$

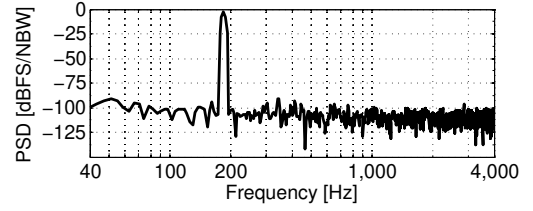
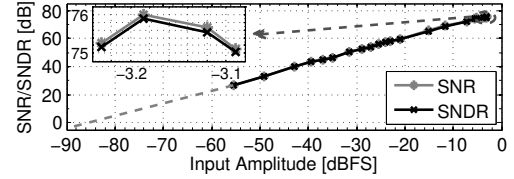
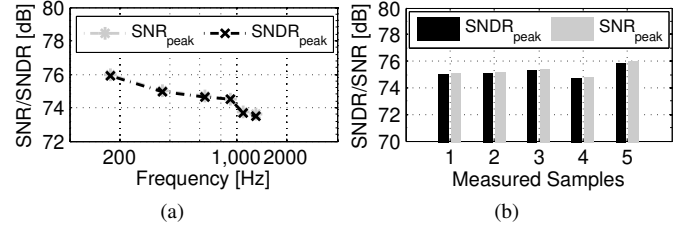

 Fig. 14: Power spectral density plot for a -3.2 dBFS input signal at 174.85 Hz. A 2048-point FFT is applied.

 Fig. 15: Measured SNR and SNDR versus the input signal amplitude. For input below -55 dBFS the curve is extrapolated.


Fig. 16: Measured SNR and SNDR: (a) over various in-band test frequencies and (b) among different samples.

in the Int_{12} , $3.2 \mu\text{A}$ in the S/H, $3.1 \mu\text{A}$ in the Int_{12} , $2.0 \mu\text{A}$ in the Int_{22} , and $3.1 \mu\text{A}$ in the biasing circuits, respectively.

The measured output spectrum for a -3.2 dBFS sinusoidal input at 174.4 Hz, where 0 dBFS refers to approximately $1.0 V_{p-p}$, is shown Fig. 14. From the power spectral density plot, a spurious-free dynamic range (SFDR) of 88.1 dB has been measured. Fig. 15 presents the measured SNR and SNDR versus the input signal amplitude, demonstrating a peak SNR of 76.6 dB, a peak SNDR of 75.9 dB for an input at -3.2 dBFS and a dynamic range of 85.5 dB. Fig. 16 (a) shows the measured peak SNRs and SNDRs for various in-band test frequencies. When the test signal frequency is increased to one-third of the ADC bandwidth, there is approximately 2 dB degradation in the SNR/SNDR performance. This is mainly due to the attenuation on signal amplitude when removing the S/H in front of the $\Sigma\Delta$ ADC, as it has been explained in section III-B. The attenuation is negligible when the input signal is relatively slow compared to the ADC's conversion rate, which is the case of the target system, where the signal from one channel has a bandwidth of 60-200 Hz, while the ADC's conversion rate is 8 kHz. Fig. 16 (b) presents the performance variation among all of the five samples available for measurements. The measured samples show consistent SNR/SNDR performance. It is worth to mention that although tunable capacitive arrays have been implemented for C_{11} and

TABLE II: Performance comparison of recent CMOS Incremental $\Sigma\Delta$ ADCs

	This Work	[16] ESSCIRC	[17] TCASI	[39] JSSC	[10] CICC	[12] ESSCIRC	[14] JSSC	[40] ESSCIRC
Year	2014	2010	2013	2013	2010	2013	2010	2012
Architecture	Two-step ADC	1 st -order $\Sigma\Delta$	3 rd -order $\Sigma\Delta$	Zoom ADC	Multi-channel	Multibit $\Sigma\Delta$	ER ($\Sigma\Delta$ +SAR)	EC ADC
Implementation	CT	CT	CT	DT	DT	DT	DT	DT
Conversion Rate (kS/s)	8	0.5	4	0.025	43.48	10	1000	1000
SNDR (dB)	75.9	58.95	60	119.8 ^a	81.5	105	84.7	56
Power (μ W)	34.8	20	96	6.3	340/chann.	280	33400	1200
V _{DD} (V)	1.2/1.8	1.6	1.8	1.8	1.8	1.8	3.3/1.8	-
Technology (μ m)	0.18	0.5	0.15	0.16	0.18	0.18	0.18	0.18
FOM _{Walden} (pJ/conv)	0.85	55.2	18.5	0.31	16.1	0.19	1.98	63.7

^a SNDR measurement is not available in [39]. Instead of SNDR, a derived $SNR_{max}=20\log((\text{Max DC Input}/2\sqrt{2})/\text{Output Noise})$ is used in the FOM calculation.

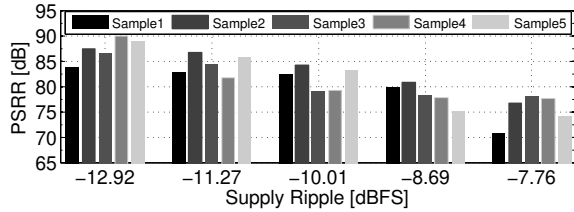


Fig. 17: Measured PSRRs versus different ripple amplitudes.

C_{12} , as shown in the chip micrograph, RC coefficient tuning was not needed for all the measured samples, due to the use of the optimal filter. To demonstrate the robustness of the prototype ADC, the measured power-supply-rejection-ratios (PSRRs) of all five samples are provided in Fig. 17, where a 918.9 Hz ripple with various amplitudes is applied to the analog power supply, when the inputs are short-circuited.

A performance comparison of this work to the state-of-the-art $\Sigma\Delta$ ADC prototypes is provided in Table II. The latest published work of each type of $\Sigma\Delta$ ADCs has been selected for the comparison. The figure-of-merit (FOM) used for comparison is given by [41]:

$$FOM_{\text{Walden}} = \frac{\text{Power}}{2 \times BW_{\text{ADC}} \times 2^{\frac{SNDR-1.76}{6.02}}} \quad (14)$$

As it can be appreciated from the table, this work improves the FOM of CT $\Sigma\Delta$ ADCs by a decade, and achieves one of the lowest FOM among the state-of-the-art $\Sigma\Delta$ ADCs, except the DT multi-bit architecture applying a Smart-DEM algorithm [12] and the DT zoom-ADC architecture targeting a very low speed sensor application [39]. It is worth mentioning that further FOM improvement of the proposed ADC architecture can be achieved by applying different enhancement techniques. From the architecture point-of-view, the two-step CT $\Sigma\Delta$ ADC can be extended to a multi-stage pipeline architecture. In this case, the number of cycles in each conversion and the modulator order in each stage, can be adjusted and optimized according to the signal bandwidth and resolution requirements. From the circuit implementation perspective, state-of-the-art power-efficient circuit techniques, such as the inverter-based integrators [39] can be employed to take better advantage of the relaxed circuit specifications in the last pipeline stages.

VI. CONCLUSION

A power-efficient incremental $\Sigma\Delta$ ADC using continuous-time implementation has been presented. To provide a flexible and power-efficient solution for the A/D conversion required in neural recording systems, a two-step ADC architecture, consisting of two second-order CT $\Sigma\Delta$ ADCs in a pipeline configuration, has been proposed. It has been shown that the ADC prototype fabricated in a standard 0.18 μ m CMOS technology, achieves a peak SNDR of 75.9 dB and a dynamic range of 85.5 dB while consuming a static power of 34.8 μ W. The proposed two-step CT $\Sigma\Delta$ ADC provides inherent flexibility, which can be better exploited if it is generalized to an architecture composed of several conversion stages. For instance, the conversion rate can be adjusted by varying the number of cycles per conversion, while maintaining the oversampling frequency; different conversion resolutions can be achieved by using different number of stages, as in pipelined ADCs. This makes the proposed ADC a promising solution for the next generation neural recording systems where both high-channel-count and high-resolution are demanded.

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REFERENCES

- [1] G. Schalk and E. C. Leuthardt, "Brain-computer interfaces using electrocorticographic signals," *IEEE Rev. Biomed. Eng.*, vol. 4, pp. 140–154, 2011.
- [2] X. Zou, L. Liu, J. Cheong, L. Yao, P. Li, M.-Y. Cheng, W. L. Goh, R. Rajkumar, G. S. Dawe, K.-W. Cheng, and M. Je, "A 100-channel 1-mW implantable neural recording IC," *IEEE Trans. Circuits Syst. I*, vol. 60, no. 10, pp. 2584–2596, 2013.
- [3] F. Shahrokhi, K. Abdelhalim, G. S. Member, D. Serletis, P. L. Carlen, and R. Genov, "The 128-Channel Fully Differential Digital Integrated Neural Recording and Stimulation Interface," *IEEE Trans. Biomed. Circuits Syst.*, vol. 4, no. 3, pp. 149–161, 2010.
- [4] W. Wattanapanitch and R. Sarpeshkar, "A Low-Power 32-Channel Digitally Programmable Neural Recording Integrated Circuit," *IEEE Trans. Biomed. Circuits Syst.*, vol. 5, no. 6, pp. 592–602, 2011.

- [5] K. Soundarapandian and M. Berarducci, "Analog Front-End Design for ECG Systems Using Delta-Sigma ADCs," *Application Report, Texas Instruments*, 2010.
- [6] F. Sebastiano and R. H. M. Van Veldhoven, "A 0.1-mm 3-Channel Area-Optimized $\Sigma\Delta$ ADC in 0.16- μm CMOS with 20-kHz BW and 86-dB DR," in *European Solid-State Circuits Conf.*, 2013, pp. 375–378.
- [7] D. Behera and N. Krishnapura, "A 2-Channel 1MHz BW, 80.5 dB DR ADC using a $\Delta\Sigma$ Modulator and Zero-ISI Filter," in *European Solid-State Circuits Conf.*, 2014, pp. 415–418.
- [8] J. Robert, G. C. Temes, V. Valencic, R. Dessoulavy, and P. Deval, "A 16-bit low-voltage cmos A/D converter," *IEEE J. Solid-State Circuits*, vol. 22, no. 2, pp. 157–163, 1987.
- [9] J. Markus, J. Silva, and G. C. Temes, "Theory and applications of incremental $\Delta\Sigma$ converters," *IEEE Trans. Circuits Syst. I*, vol. 51, no. 4, pp. 678–690, 2004.
- [10] W. Yu, M. Aslan, and G. C. Temes, "82 dB SNDR 20-channel incremental ADC with optimal decimation filter and digital correction," in *IEEE Custom Integrated Circuits Conf.*, 2010, pp. 1–4.
- [11] V. Quiquempoix, P. Deval, A. Barreto, G. Bellini, J. Markus, J. Silva, and G. C. Temes, "A low-power 22-bit incremental ADC," *IEEE J. Solid-State Circuits*, vol. 41, no. 7, pp. 1562–1571, 2006.
- [12] Y. Liu, E. Bonizzoni, A. D'Amato, and F. Maloberti, "A 105-dB SNDR, 10 kSps multi-level second-order incremental converter with smart-DEM consuming 280 μW and 3.3-V supply," in *European Solid-State Circuits Conf.*, 2013, pp. 371374.
- [13] P. Rombouts, W. De Wilde, and L. Weyten, "A 13.5-b 1.2-V micropower extended counting A/D converter," *IEEE J. Solid-State Circuits*, vol. 36, no. 2, pp. 176–183, 2001.
- [14] A. Agah, K. Vleugels, P. B. Griffin, M. Ronaghi, J. D. Plummer, and B. A. Wooley, "A high-resolution low-power incremental $\Sigma\Delta$ ADC with extended range for biosensor arrays," *IEEE J. Solid-State Circuits*, vol. 45, no. 6, pp. 1099–1110, 2010.
- [15] M. Mollazadeh, K. Murari, G. Cauwenberghs, and N. Thakor, "Micropower CMOS Integrated Low-Noise Amplification, Filtering, and Digitization of Multimodal Neuropotentials," *IEEE Trans. Biomed. Circuits Syst.*, vol. 3, no. 1, pp. 1–10, 2009.
- [16] Y. M. Chi and G. Cauwenberghs, "Micropower integrated bioamplifier and auto-ranging ADC for wireless and implantable medical instrumentation," in *European Solid-State Circuits Conf.*, 2010, pp. 334–337.
- [17] J. Garcia, S. Rodriguez, and A. Rusu, "A Low-Power CT Incremental 3rd Order Sigma-Delta ADC for Biosensor Applications," *IEEE Trans. Circuits Syst. I*, vol. 60, no. 1, pp. 25–36, 2013.
- [18] S. Tao, S. Rodriguez and A. Rusu, "Two-step continuous-time incremental sigma-delta ADC," in *IET Electron. Lett.*, vol.49, no.12, pp. 749–751, 2013.
- [19] T. Kim, N. S. Artan, J. Viventi, and H. J. Chao, "Spatiotemporal Compression for Efficient Storage and Transmission of High-Resolution Electrocardiography Data," in *Annu. Int. Conf. of the IEEE Engineering in Medicine and Biology Society*, 2012, pp. 1012–1015.
- [20] S. Ray, N. E. Crone, E. Niebur, P. J. Franaszczuk, and S. S. Hsiao, "Neural correlates of high-gamma oscillations (60-200 Hz) in macaque local field potentials and their potential implications in electrocorticography," *The Journal of Neuroscience*, vol. 28, no. 45, 11526–11536, 2008.
- [21] G. Lantz, R. Grave de Peralta, L. Spinelli, M. Seeck, and C. M. Michel, "Epileptic source localization with high density EEG: how many electrodes are needed?," *Clinical Neurophysiology*, vol. 114, no. 1, pp.63–69, 2002.
- [22] M. S. Chae, W. Liu, and M. Sivaprakasam, "Design optimization for integrated neural recording systems," *IEEE J. Solid-State Circuits*, vol. 43, no. 9, pp. 1931–1939, 2008.
- [23] F. Zhang, A. Mishra, A. G. Richardson, and B. Otis, "A low-power ECoG/EEG processing IC with integrated multiband energy extractor," *IEEE Trans. Circuits Syst. I*, vol. 58, no. 9, pp. 2069–2082, 2011.
- [24] W. Smith, B. Mogen, E. Fetz, and B. Otis, "A Spectrum-Equalizing Analog Front End for Low-Power Electrocardiography Recording," in *European Solid-State Circuits Conf.*, 2014, pp. 107–110.
- [25] S. Tao, S. Rodriguez and A. Rusu, "DAC Waveform Effects in CT Incremental $\Sigma\Delta$ ADCs for Biosensor Applications," in *IEEE Proc. Int. NEWCAS Conf.*, 2013, pp. 1–4.
- [26] J. Markus, "High-Order Incremental Delta-Sigma Analog-to-Digital Converters," Ph.D. dissertation, Budapest University of Technology and Economics, 2005.
- [27] R. Schreier, "The delta-sigma toolbox version 7.3," *On Internet: <http://www.mathworks.se/matlabcentral/fileexchange/19-delta-sigma-toolbox> [viewed 2014 08 22]*, 2011.
- [28] T. Caldwell and D. A. Johns, "Incremental data converters at low oversampling ratios," *IEEE Trans. Circuits Syst. I*, vol. 57, no. 7, pp. 1525–1537, 2010.
- [29] M. Ortmanns and F. Gerfers, *Continuous-time sigma-delta A/D conversion: fundamentals, performance limits and robust implementations*. Springer Verlag, 2006.
- [30] J. Steensgaard, Z. Zhang, W. Yu, A. Sarhegyi, L. Lucchese, D.-I. Kim, and G. C. Temes, "Noise-power optimization of incremental data converters," *IEEE Trans. Circuits Syst. I*, vol. 55, no. 5, pp. 1289–1296, 2008.
- [31] S. Pavan, N. Krishnapura, R. Pandarinathan, and P. Sankar, "A Power Optimized Continuous-Time $\Delta\Sigma$ ADC for Audio Applications," *IEEE J. Solid-State Circuits*, vol. 43, no. 2, pp. 351–360, 2008.
- [32] S. Rabii and B. Wooley, "A 1.8-V digital-audio sigma-delta modulator in 0.8- μm CMOS," *IEEE J. Solid-State Circuits*, vol. 32, no. 6, pp. 783–796, 1997.
- [33] F. Krummenacher and N. Joehl, "A 4-MHz CMOS continuous-time filter with on-chip automatic tuning," *IEEE J. Solid-State Circuits*, vol. 23, no. 3, pp. 750–758, 1988.
- [34] C. Ho, Z. Lee, M. Huang, and S. Huang, "A 75.1dB SNDR, 80.2dB DR, 4th-order Feed-forward Continuous-Time Sigma-Delta Modulator with Hybrid Integrator for Silicon TV-tuner Application," in *IEEE Asian Solid-State Circuits Conf.*, 2011, pp. 261–264.
- [35] M. Van Elzakker, E. Van Tuijl, P. Geraedts, D. Schinkel, E. A. M. Klumperink, S. Member, and B. Nauta, "A 10-bit Charge-Redistribution ADC Consuming 1.9uW at 1Ms/s," *IEEE J. Solid-State Circuits*, vol. 45, no. 5, pp. 1007–1015, 2010.
- [36] J. Zhang, Y. Lian, L. Yao, and B. Shi, "A 0.6-V 82-dB 28.6- μW Continuous-Time Audio Delta-Sigma Modulator," *IEEE J. Solid-State Circuits*, vol. 46, pp. 2326–2335, 2011.
- [37] Mathworks, "MATLAB R2013a fmincon documentation," *On Internet: <http://www.mathworks.com/help/optim/ug/fmincon.html>*, 2013.
- [38] J. Garcia, "Digitally Enhanced Continuous-Time Sigma-Delta Analog-to-Digital Converters," Ph.D. dissertation, KTH Royal Institute of Technology, 2012.
- [39] Y. Chae, K. Souri, and K. Makinwa, "A 6.3 μW 20 bit Incremental Zoom-ADC with 6 ppm INL and 1 μV Offset," *IEEE J. Solid-State Circuits*, vol. 48, no. 12, pp. 3019–3027, 2013.
- [40] P. Rombouts, P. Woestyn, M. De Bock, and J. Raman, "A very compact 1MS/s Nyquist-rate A/D-converter with 12 effective bits," in *European Solid-State Circuits Conf.*, 2012, pp. 213–216.
- [41] R. H. Walden, "Analog-to-digital converter survey and analysis," *IEEE J. Sel. Areas Commun.*, vol. 17, no. 4, pp. 539–550, 1999.



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