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A Synergistic Workspace for Human Consciousness Revealed by Integrated Information Decomposition — [Source link](#)

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1 A Synergistic Workspace for Human Consciousness Revealed
2 by Integrated Information Decomposition
3

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34

35

Abstract

36

37 A central goal of neuroscience is to understand how the brain synthesises information from
38 multiple inputs to give rise to a unified conscious experience. This process is widely believed
39 to require integration of information. Here, we combine information theory and network
40 science to address two fundamental questions: how is the human information-processing
41 architecture functionally organised? And how does this organisation support human
42 consciousness? To address these questions, we leverage the mathematical framework of
43 Integrated Information Decomposition to delineate a cognitive architecture wherein
44 specialised modules interact with a “synergistic global workspace,” comprising functionally
45 distinct gateways and broadcasters. Gateway regions gather information from the specialised
46 modules for processing in the synergistic workspace, whose contents are then further
47 integrated to later be made widely available by broadcasters. Through data-driven analysis of
48 resting-state functional MRI, we reveal that gateway regions correspond to the brain’s well-
49 known default mode network, whereas broadcasters of information coincide with the
50 executive control network. Demonstrating that this synergistic workspace supports human
51 consciousness, we further apply Integrated Information Decomposition to BOLD signals to
52 compute integrated information across the brain. By comparing changes due to propofol
53 anaesthesia and severe brain injury, we demonstrate that most changes in integrated
54 information happen within the synergistic workspace. Furthermore, it was found that loss of
55 consciousness corresponds to reduced integrated information between gateway, but not
56 broadcaster, regions of the synergistic workspace. Thus, loss of consciousness may coincide
57 with breakdown of information integration by this synergistic workspace of the human brain.
58 Together, these findings demonstrate that refining our understanding of information-
59 processing in the human brain through Integrated Information Decomposition can provide
60 powerful insights into the human neurocognitive architecture, and its role in supporting
61 consciousness.

62

Introduction

63 Humans and other vertebrates rely on a centralised nervous system to process information
64 from the environment, obtained from a wide array of sensory sources. However, information
65 from different sensory sources must eventually be combined and integrated with the
66 organism's memories and goals, in order to guide adaptive behaviour effectively (Varela et
67 al., 2001). Indeed, theoretical and empirical work in cognitive neuroscience indicates that
68 information processed in parallel by domain-specific sensory modules (Taylor et al., 2009)
69 needs to be integrated within a multimodal “central executive” (Fodor, 1985)

70 Furthermore, influential theories in computational neuroscience have also proposed that
71 global integration of information from diverse sources plays a fundamental role in relation to
72 human consciousness. The influential Global Neuronal Workspace Theory (GNWT) focuses
73 on the process by which specific neural information becomes available for conscious access,
74 as occurring through the global integration induced by a “global workspace” (Baars, 2005;
75 Dehaene and Changeux, 2011; Dehaene et al., 2011; Mashour et al., 2020). The contents of
76 the global workspace are thought to be widely broadcast back to localised processors, thereby
77 providing “experiential integration” of distributed cortical modules into a coherent whole
78 (Mashour et al., 2020). Also highlighting the importance of integration, the prominent
79 Integrated Information Theory (IIT) posits that the degree of consciousness in a system is
80 determined by its “integrated information”: the amount of intrinsic information generated by
81 the dynamics of the system considered as a whole, over and above the information generated
82 by the dynamics of its individual constituent parts (Tononi, 2004; Tononi et al., 2016). Thus,
83 this notion of integrated information corresponds to the extent to which “the whole is greater
84 than the sum of its parts” (Balduzzi and Tononi, 2008)

85 Therefore, leading theoretical accounts of consciousness converge on this point:
86 consciousness critically depends on the capability for global integration across a network of
87 differentiated modules (Cavanna et al., 2018). However, despite this partial agreement, it is
88 important to note that the role GNWT and IIT assign to integration with respect to
89 consciousness is functionally distinct. On the one hand, GNWT builds on the premise that
90 conscious information is globally available for further cognitive processing, contrasting with
91 unconscious information that is only available within local modules. Thus, information
92 becomes consciously accessible only upon being broadcasted to the rest of the brain, and
93 integration is viewed as a necessary - but not sufficient - prerequisite step on the way to

94 broadcasting. In contrast, IIT proposes a more fundamental identity between the system's
95 integrated information and subjective experience, but without specifying a formal
96 architecture for this process: that is, according to IIT any system that integrates information
97 will thereby be conscious, regardless of its specific organisation. Seen under this light, it
98 becomes apparent that IIT and GWT are actually addressing different aspects of
99 consciousness, and their views of integration are different but potentially complementary.

100 A crucial step for carrying these approaches forward is to deepen our understanding of how
101 the brain's information-processing architecture enables the integration of information.
102 Crucially, our ability to make sense of any information-processing architecture is limited by
103 our understanding of the information that is being processed. An elegant framework to
104 account for information in distributed systems is provided by *Partial Information*
105 *Decomposition* (PID) (Williams and Beer, 2010), which posits that not all information is the
106 same: two sources can possess information about a given target that is either unique (each
107 source provides independent information), redundant (the same information is provided by
108 both sources) or synergistic (complementary information, available only when both sources
109 are considered together). As an example, humans have two sources of visual information
110 about the world i.e. two eyes. The information that is lost when one eye is closed is called the
111 "unique information" of that source - information that cannot be obtained from the remaining
112 eye. The information that one still has when one eye is closed is called "redundant
113 information" - because it is information that is carried equally by both sources. This provides
114 robustness and resilience: i.e. you can still see even after losing one eye. However, losing one
115 eye also deprives you of stereoscopic information about depth. This information does not
116 come from either eye alone: you need both, in order to perceive the third dimension.
117 Therefore, this is called the "synergistic information" between the sources - the extra
118 advantage that is derived from combining them.

119 By applying a generalisation of PID to timeseries data - known as Integrated Information
120 Decomposition (Φ ID) (Mediano et al., 2019a) - to functional and diffusion MRI data, our
121 previous work identified a set of brain regions that constitute a "synergistic core" supporting
122 higher-level cognitive functions in the human brain - which we believe may play the role of
123 the brain's global workspace (Luppi et al., 2020a). This "synergistic global workspace"
124 mainly comprises high-level prefrontal and parietal cortical regions whose network
125 organisation is especially well-suited for global integration of information across the brain,

126 which contrast with the modular and redundant interactions observed in sensorimotor areas
127 (Luppi et al., 2020a). Building on these findings, it is natural to ask whether this synergistic
128 workspace is related to human consciousness. Furthermore, given that the views on
129 information integration put forward by GNWT and IIT are potentially complementary, an
130 important challenge to move the field forward is to leverage both accounts into a unified
131 architecture that could explain empirical effects observed in neuroimaging data.

132 Therefore, in this paper we set out to address two fundamental questions of contemporary
133 neuroscience:

- 134 1. How is the human information-processing workspace functionally organised?
135 Specifically: What brain regions does it involve, and what are the roles of the two
136 types of information integration proposed by GNWT and IIT within the workspace?
- 137 2. How are these information-processing roles related to human consciousness?

138 To address these questions, we study three resting-state fMRI datasets: (i) data from the
139 Human Connectome Project (Van Essen et al., 2013); (ii) N=15 healthy volunteers who were
140 scanned before and after general anaesthesia with the intravenous propofol as well as during
141 post-anaesthetic recovery (Luppi et al., 2019); (iii) N=22 patients suffering from chronic
142 disorders of consciousness (DOC) as a result of severe brain injury (Luppi et al., 2019).

143 **Results**

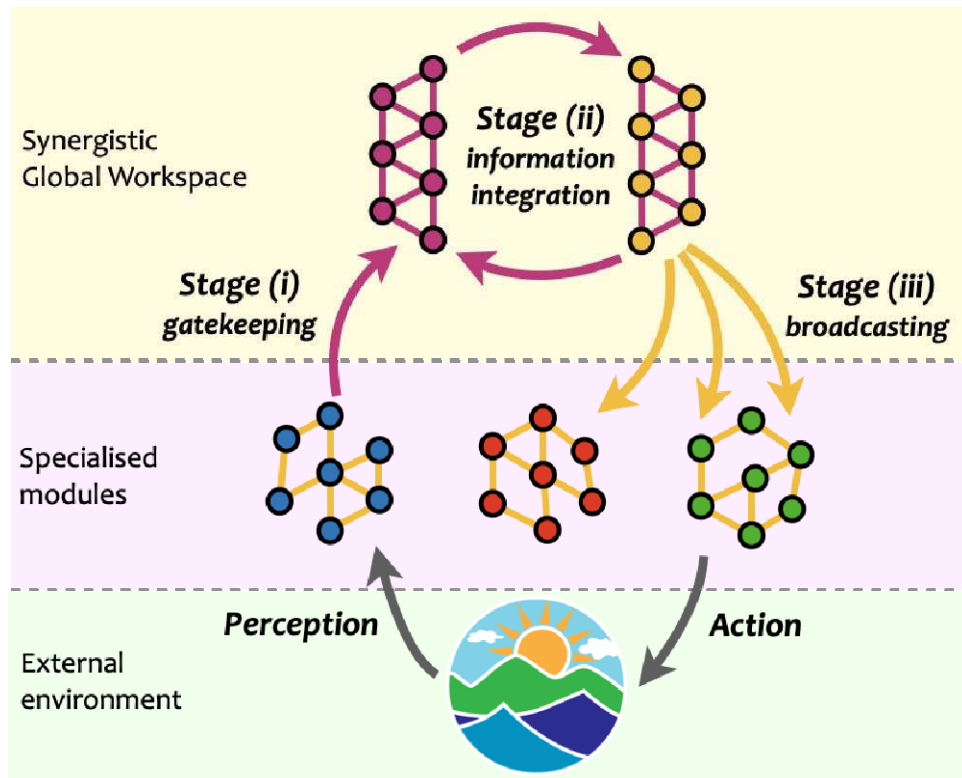
144

145 **Identification of workspace gateways and broadcasters**

146 By considering principles of distributed information-processing, one can introduce a
147 functional taxonomy to differentiate the constituent elements of the global workspace
148 according to their function. Specifically, we propose to divide the information-processing
149 stream within a distributed system (such as the human brain) in three key stages: (i) gathering
150 of information from multiple distinct modules into a workspace; (ii) integration of the
151 gathered information within the workspace; and (iii) global information broadcasting to the
152 rest of the brain. Furthermore, we propose that while all workspace regions are involved in
153 stage (ii), they are differentially involved in stages (i) and (iii).

154 The existence of a synergistic workspace and these three processing stages can be seen as
155 emerging from a trade-off between performance and robustness that is inherent to distributed
156 systems. Theoretical work in cognitive science (Baars, 2005; Fodor, 1985) and the field of
157 distributed signal processing (Tsitsiklis, 1989; Veeravalli and Varshney, 2012) has long
158 recognised the computational benefits of combining multiple distinct processing streams.
159 However, having a single source of inputs to and outputs from the workspace introduces what
160 is known as a “single point of failure,” which can lead to catastrophic failure in case of
161 damage or malfunction (Lever et al., 2013). Therefore, a natural solution is to have not a
162 single but multiple units dedicated to gathering and broadcasting information, respectively,
163 thereby forming a workspace that can be in charge of synthesising the results of peripheral
164 processing (Rosas et al., 2017).

165 Focusing on Stage (ii), our previous work (Luppi et al., 2020a) identified which regions of
166 the human brain are predominantly synergistic, and thus are most reliant on combining
167 information from other brain regions. The key signature of workspace regions is to have a
168 high prevalence of synergistic (compared to redundant) connections, and therefore the
169 synergy-rich regions reported in (Luppi et al., 2020a) are ideally poised as GNW candidates.
170 Here, we consider the architecture of the global workspace more broadly, and combine
171 Integrated Information Decomposition with graph-theoretical principles to bring insights
172 about processing stages (i) and (iii) (Figure 1). We term this proposal the “Synergy- Φ -
173 Redundancy” neurocognitive architecture (SAPHIRE).



174

175 **Figure 1. Schematic of the proposed SAPHIRE neurocognitive architecture.** Below, specialised
176 modules characterised by robust redundant interactions (Luppi et al., 2020a) process information
177 about the environment. Information is then collected by workspace gateways through synergistic
178 interactions [Step (i)]; synergistic interactions integrate information within the synergistic global
179 workspace [Step (ii)]; workspace broadcasters spread the integrated information back to the
180 specialised modules, through redundant interactions [Step (iii)], for further processing and to guide
181 behaviour. Orange connections represent redundant interactions, and violet connections represent
182 synergistic interactions. Grey connections represent interactions between the system and its
183 environment.

184

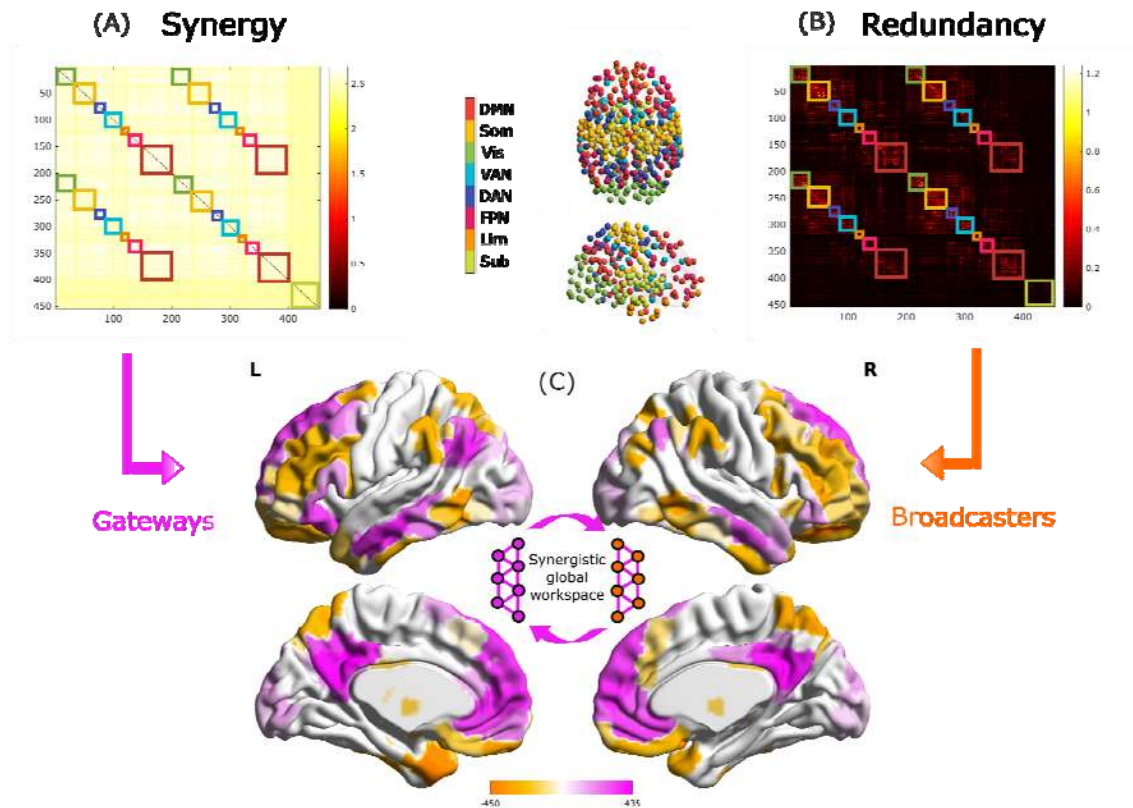
185 We reasoned that brain regions through which information gains access to the workspace
186 should exhibit synergistic connections that are widely distributed across the brain, as - by
187 definition - the workspace gathers and synthesises information from a multiplicity of diverse
188 brain modules. Thus, we postulate that regions that mediate the access to the synergistic
189 workspace are connected with multiple modules within networks of synergistic interactions,
190 synthesising incoming inputs from diverse sources (Sneve et al., 2019). We refer to such
191 regions as *gateways* (Figure 1, violet nodes). In contrast, the process of broadcasting
192 information corresponds to disseminating multiple copies of the same information from the
193 workspace to many functionally adjacent brain regions. Therefore, broadcaster regions also
194 have connections with many different modules, but of non-synergistic, redundant

195 connections: “redundancy” accounts for the fact that multiple copies of the same information
196 are being distributed. These regions are designated as *broadcasters* (Figure 1, orange nodes).

197 One approach to operationalise these ideas is by leveraging well-established graph-theoretical
198 tools. In this work, we assess the diversity of intermodular connections using the
199 *participation coefficient* (Rubinov and Sporns, 2010), which captures to what extent a given
200 node connects to modules beyond its own (Methods). Note that this is different from the node
201 *strength*, which captures a region’s total amount of connectivity, and which we used to
202 identify which regions belong to the synergistic workspace (Luppi et al., 2020a); the
203 participation coefficient instead quantifies the diversity of modules that a region is connected
204 to. Therefore, gateways are identified as brain regions that (a) belong to the workspace, and
205 (b) have a highly-ranked participation coefficient in terms of synergistic connections.
206 Conversely, broadcasters are global workspace regions that have a higher participation
207 coefficient rank over redundant connections.

208 To explore these hypotheses, we computed synergistic and redundant interactions between
209 454 cortical and subcortical brain regions (Luppi and Stamatakis, 2020) based on resting-
210 state functional MRI data from 100 subjects of the Human Connectome Project (following
211 the same procedure as in Luppi *et al.*, 2020 (Luppi et al., 2020a)). We then subdivided the
212 brain into the well-established resting-state networks identified by Yeo and colleagues (Yeo
213 et al., 2011), plus an additional subcortical module (Tian et al., 2020). Based on this partition
214 into modules, we identified gateways and broadcasters by comparing the participation
215 coefficients of synergistic versus redundant connections, for brain regions belonging to the
216 synergistic workspace previously identified by Luppi *et al.*, (2020) (Luppi et al., 2020a)
217 (Figure 2Ai,ii).

218



219

220 **Figure 2. Gateways and broadcaster regions identified by their network connectivity profiles.**
221 (A) Group-average matrices of synergistic interactions between regions of the 454-ROI augmented
222 Schaefer atlas (Luppi and Stamatakis, 2020; Schaefer et al., 2018). (B) Group-average matrices of
223 redundant interactions. We highlighted modular allegiance to the canonical resting-state networks by
224 using the colour scheme shown in between A and B. (C) Regions are identified as gateways (violet) or
225 broadcasters (orange) based on the difference between rank of participation coefficient for synergy
226 and redundancy, (only shown for brain regions identified as belonging to the synergistic global
227 workspace by Luppi *et al* (Luppi et al., 2020a)). Violet indicates synergy rank > redundancy rank,
228 corresponding to workspace regions that combine information of many brain modules (gateways);
229 orange indicates the opposite, identifying workspace regions that broadcast information to many
230 modules. Inset: illustration of the synergistic workspace. Legend: DMN, default mode network. Som,
231 somatomotor network. Vis, visual network. VAN, ventral attention network. DAN, dorsal attention
232 network. FPN, fronto-parietal control network. Lim, limbic network. Sub, subcortical network
233 (comprised of 54 regions of the Tian 2020 atlas (Tian et al., 2020)). These results were also replicated
234 using an alternative parcellation with 232 cortical and subcortical nodes (Supplementary Figure 1).

235

236 Intriguingly, our results reveal that gateways reside primarily in the brain's default mode
237 network (Figure 2B, violet). In contrast, broadcasters are mainly located in the executive
238 control network, especially lateral prefrontal cortex (Figure 2B, orange). Remarkably, the
239 latter results are in line with Global Neuronal Workspace Theory, which consistently
240 identifies lateral prefrontal cortex as a major broadcaster of information (Bor and Seth, 2012;
241 Mashour et al., 2020).

242

243 **Information decomposition identifies a synergistic core supporting human**
244 **consciousness**

245

246 Having introduced a taxonomy within the synergistic global workspace based on the distinct
247 information-processing roles of different brain regions, we then sought to investigate their
248 role in supporting human consciousness. Given the importance attributed to integration of
249 information by both GNWT and IIT, we expected to observe reductions in integrated
250 information within the areas of the synergistic workspace associated with loss of
251 consciousness. Furthermore, we also reasoned that any brain regions that are specifically
252 involved in supporting consciousness should “track” the presence of consciousness: the
253 reductions should occur regardless of how loss of consciousness came about, and they should
254 be restored when consciousness is regained.

255

256 We tested these hypotheses with resting-state fMRI from 15 healthy volunteers who were
257 scanned before, during, and after anaesthesia with the intravenous agent propofol, as well as
258 22 patients with chronic disorders of consciousness (DOC) (Luppi et al., 2019). Resting-state
259 fMRI data were parcellated into 400 cortical and 54 subcortical brain regions (Luppi and
260 Stamatakis, 2020). Building on the IIT literature, which provides a formal definition of
261 integrated information, we assessed integration corresponding to conscious activity via two
262 alternative metrics: the well-known whole-minus-sum Φ measure introduced in (Balduzzi and
263 Tononi, 2008), and the “revised Φ ” (Φ -R) measure recently introduced in (Mediano et al.,
264 2019a) (see Methods). Being demonstrably non-negative, this revised measure overcomes a
265 major conceptual limitation of the original formulation of integrated information (Mediano et
266 al., 2019a). For each subject, we computed the integrated information between each pair of
267 BOLD signal timeseries, resulting in a 454-by-454 matrix of integrated information between
268 brain regions. Treating this matrix as an (undirected) network enabled us to study
269 consciousness-related changes in integrated information across conditions, which were
270 analysed using the Network Based Statistic correction for multiple comparisons (Zalesky et
271 al., 2010). Importantly, since we are interested in changes that are shared between the DOC
272 and propofol datasets, we computed edge-level statistics using a composite null hypothesis
273 test designed to detect such shared effects (see Methods).

274

275 Analysis based on Φ -R revealed a widespread reorganisation of integrated information
276 throughout the brain when comparing awake volunteers against DOC patients, with both
277 increases and decreases being observed ($p < 0.001$; Figure 3A). Likewise, propofol
278 anaesthesia was also characterised by significant changes in integrated information between
279 brain regions, both when compared with pre-anaesthetic wakefulness ($p < 0.001$; Figure 3B)
280 and post-anaesthetic recovery ($p < 0.001$; Figure 3C).

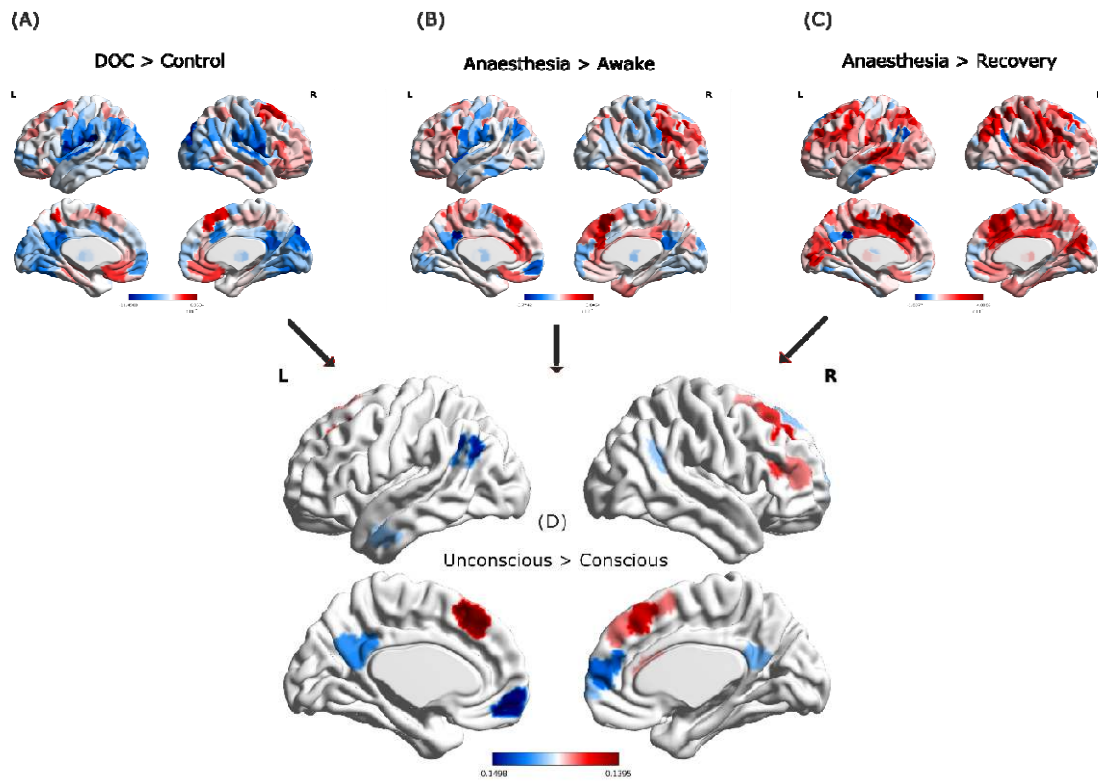
281 Our analysis identified a number of the Φ -R connections that were reduced when
282 consciousness was lost due to both anaesthesia and brain injury, and were restored during
283 post-anaesthetic recovery - as we had hypothesised (Figure 3D). Remarkably, almost all
284 regions showing consistent decreases in Φ -R when consciousness was lost were members of
285 the global synergistic workspace, and specifically located in the default mode network
286 (bilateral precuneus and medial prefrontal cortex) - and bilateral inferior parietal cortex -
287 although left temporal cortices were also involved (Figure 3D). Additionally, some
288 connections exhibited increases in Φ -R during loss of consciousness, and were restored upon
289 recovery (Figure 3D), including areas in frontal cortex - especially lateral prefrontal cortex.
290 Nevertheless, the overall balance was in favour of reduced integrated information: sum of F-
291 scores associated with significant edges = -25.37 (Supplementary Figure 2). This was in
292 contrast with the analysis based on the original formulation of Φ introduced by (Balduzzi and
293 Tononi, 2008), which did not identify any reductions in integrated information that were
294 common across anaesthesia and disorders of consciousness, instead only identifying common
295 increases (Supplementary Figure 3A).

296

297

298

299



300

301 **Figure 3. Loss of consciousness induces similar reorganisation of cortical integrated information**
302 **across anaesthesia and disorders of consciousness.** Top: Brain regions exhibiting overall NBS-
303 corrected increases (red) and decreases (blue) in integrated information exchange when consciousness
304 is lost. (A) DOC patients minus awake healthy volunteers; (B), propofol anaesthesia minus pre-
305 induction wakefulness; (C) propofol-anaesthesia minus post-anaesthetic recovery. (D) Overlaps
306 between the three contrasts in (A-C), showing increases and decreases that are common across
307 anaesthesia and disorders of consciousness.

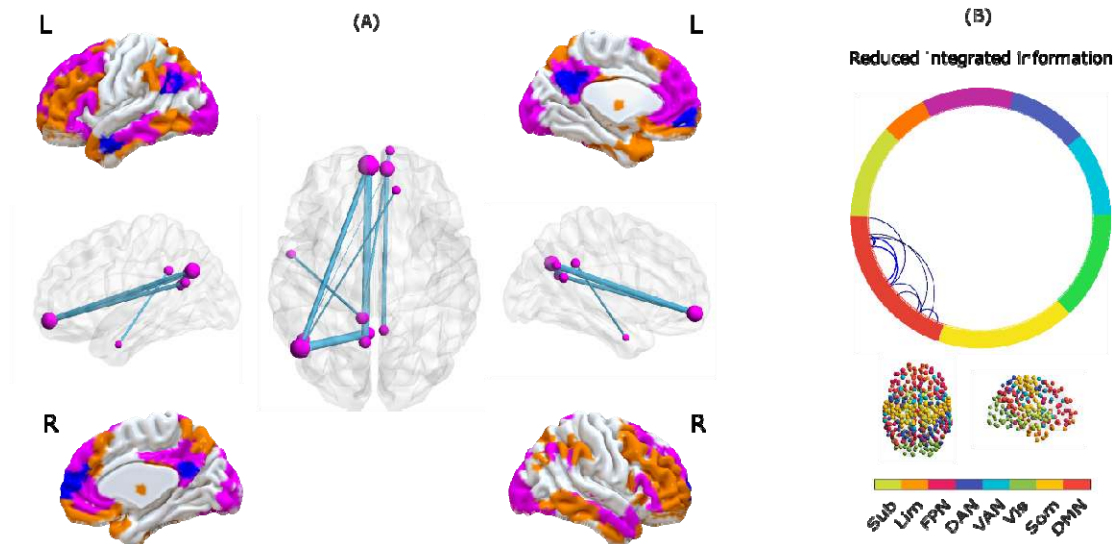
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309 Having identified the subset of brain regions that are reliably associated with supporting
310 human consciousness in terms of their integrated information, the last step of our analysis
311 was to leverage the architecture proposed above to understand their role in the information
312 processing stream within the brain. Since IIT predicts that loss of consciousness corresponds
313 to reductions in integrated information, we focused on regions exhibiting reliable reductions
314 in Φ -R when consciousness is lost (whether due to anaesthesia or DOC), which were restored
315 upon recovery (shown in blue in Figure 3D).

316 Remarkably, our whole-brain results show that Φ -R disconnections induced by loss of
317 consciousness play the role of gateway nodes (Figure 4A, violet) rather than broadcaster
318 nodes (Figure 4A, orange) according to our previous identification (see Figure 2B, violet
319 regions). Indeed, all reductions occur specifically within the default mode network (Figure

320 4B). Thus, these results suggest that loss of consciousness across anaesthesia and disorders of
321 consciousness would correspond to anterior-posterior disconnection - in terms of integrated
322 information - between DMN nodes that act as gateways into the synergistic workspace.

323



324

325 **Figure 4. Synergistic core of human consciousness.** (A) Surface projections indicate brain regions
326 that play the role of broadcasters (orange) or gateways (violet) in the synergistic workspace, and
327 regions that exhibit an overall significant reduction in integrated information across anaesthesia and
328 disorders of consciousness (blue). Network representation: edges indicate reduced integrated
329 information during both propofol anaesthesia and disorders of consciousness, between gateway
330 (violet) and broadcaster (orange) nodes of the workspace. (B) Circular graph representation of
331 significant reductions in integrated information (Φ -R) between brain regions, observed in all three
332 contrasts, divided into canonical resting-state networks. Legend: DMN, default mode network. Som,
333 somatomotor network. Vis, visual network. VAN, ventral attention network. DAN, dorsal attention
334 network. FPN, fronto-parietal control network. Lim, limbic network. Sub, subcortical network
335 (comprised of 54 regions of the Tian 2020 atlas (Tian et al., 2020)).

336

337 **Replication with alternative parcellation**

338 To ensure the robustness of our results to analytic choices, we also replicated them using an
339 alternative cortical parcellation of lower dimensionality: we used the Schaefer scale-200
340 cortical parcellation (Schaefer et al., 2018), complemented with the scale-32 subcortical ROIs
341 from the Tian subcortical atlas (Luppi and Stamatakis, 2020; Tian et al., 2020)

342 (Supplementary Figure 3B). Additionally, we also show that our results are not dependent on
343 the choice of parameters in the NBS analysis, and are replicated using an alternative
344 threshold definition for the connected component (extent rather than intensity) or a more
345 stringent value for the cluster threshold ($F > 12$) (Supplementary Figure 3C-D). Importantly,
346 whereas the increases in Φ -R are not the same across different analytic approaches,
347 reductions of Φ -R in medial prefrontal and posterior cingulate/precuneus are reliably
348 observed, attesting to their robustness.

349

350

Discussion

351 **Architecture of the synergistic global workspace**

352 This paper proposes a functional architecture for the brain's macroscale information
353 processing flow, which leverages insights from network science and a refined understanding
354 of neural information exchange. The synergy- Φ -redundancy (SAPHIRE) architecture posits
355 the existence of a "synergistic workspace" of brain regions characterised by highly
356 synergistic global interactions, which our previous work had shown to be composed by
357 prefrontal and parietal cortices that are critical for higher cognitive functions (Luppi et al.,
358 2020a). This workspace is further functionally decomposed by distinguishing gateways,
359 which bring information from localised modules into the workspace, and broadcasters, which
360 disseminate multiple copies of workspace information back to low-level regions.

361 Remarkably, our results on the HCP dataset show that the proposed operationalisation of
362 gateways and broadcasters corresponds to the distinction between the brain's default mode
363 network and executive control network, respectively. This data-driven identification of
364 workspace gateways and broadcasters with the DMN and FPN provides a new framework to
365 explain well-known functional differences between DMN and FPN, based on their distinct
366 and complementary roles within the brain's synergistic global workspace, which is discussed
367 below.

368 The fronto-parietal executive control network (FPN) mainly comprises lateral prefrontal and
369 parietal cortices, and it is associated with performance of a variety of complex, cognitively
370 demanding tasks (Barbey, 2018; Duncan and Owen, 2000; Fedorenko et al., 2013). A key

371 component of this network is lateral prefrontal cortex (LPFC). Based on theoretical and
372 empirical evidence, as summarised in a recent review of GNWT (Mashour et al., 2020), this
373 region is posited to play a major role in the global workspace, as a global broadcaster of
374 information. Remarkably, this is precisely the role that our results assigned to LPFC, based
375 on its combined information-theoretic and network properties. These results are also
376 consistent with recent insights from network neuroscience, which indicate that the FPN is
377 ideally poised to steer whole-brain dynamics through novel trajectories, in response to
378 complex task demands (Barbey, 2018; Gu et al., 2015). Specifically, by broadcasting to the
379 rest of the brain information that has been integrated within the workspace, the FPN may act
380 as global coordinator of subsequent whole-brain dynamics.

381 On the other hand, the default mode network comprises posterior cingulate and precuneus,
382 medial prefrontal cortex, and inferior parietal cortices (Fox et al., 2005; Raichle et al., 2001).
383 Far from being merely a “task-negative network”, as initially believed, the DMN is
384 prominently involved in self-referential processing (Cavanna and Trimble, 2006; Qin and
385 Northoff, 2011), and ‘mental-time-travel’ (Karapanagiotidis et al., 2017) or episodic memory
386 and future-oriented cognition (Buckner and DiNicola, 2019; Buckner et al., 2008; Schacter et
387 al., 2007; Szpunar et al., 2014). Its posterior regions in particular, act as relays between the
388 neocortex and the hippocampal memory system (Buckner and DiNicola, 2019). This network
389 was found to occupy a crucial position at the convergence of functional gradients of
390 macroscale cortical organisation (Margulies et al., 2016), supporting its recently observed
391 involvement in broader cognitive tasks (Vatansever et al., 2015b, 2015a, 2017). Thus, in
392 terms of both neuroanatomical connectivity and functional engagement, the DMN is uniquely
393 positioned to integrate and contextualise information coming into the global workspace (e.g.
394 from sensory streams) by combining it with rich information pertaining to one’s past
395 experiences and high-level mental models about ‘self’ and world (Hassabis and Maguire,
396 2009) .

397

398 **Integrated Information Decomposition of human consciousness**

399 After identifying the neuroanatomical-functional mapping of the synergistic workspace in
400 terms of gateways and broadcasters, we sought to identify their role in supporting human
401 consciousness. Considering integrated information as a measure of consciousness, we

402 focused on identifying regions where information integration is reduced when consciousness
403 is lost (regardless of its cause, be it propofol anaesthesia or severe brain injury), and restored
404 upon its recovery. Our results indicate that brain regions exhibiting consciousness-specific
405 reductions in integrated information coincide with major nodes of the synergistic global
406 workspace.

407 Intriguingly, we found that the main disruptions of information integration were localised in
408 gateway nodes, rather than broadcasters. Thus, loss of consciousness in both anaesthesia and
409 disorders of consciousness could be understood as a breakdown of the entry points to the
410 “synergistic core” (Figure 4), which becomes unable to properly integrate inputs for the
411 workspace. Importantly, the original “whole-minus-sum” Φ introduced by Balduzzi and
412 Tononi (Balduzzi and Tononi, 2008) did not show consistent reductions during loss of
413 consciousness. Thus, the present results demonstrate the empirical validity of the “revised”
414 measure, Φ -R, in addition to its theoretical soundness (Mediano et al., 2019a).

415 Since workspace gateway regions coincide with the brain’s default mode network, these
416 results are also in line with recent evidence that information content and integrative capacity
417 of the DMN are compromised during loss of consciousness induced by both anaesthesia and
418 severe brain injury (Boveroux et al., 2010; Hannawi et al., 2015; Luppi et al., 2019;
419 MacDonald et al., 2015; Di Perri et al., 2018; Vanhaudenhuyse et al., 2010). Due to its
420 prominent role in self-referential processing (Qin and Northoff, 2011), breakdown of DMN
421 connectivity within the synergistic workspace may be seen as a failure to integrate one’s self-
422 narrative into the “stream of consciousness”, in the words of Willam James.

423 This notion is further supported by focusing on reductions of integrated information during
424 anaesthesia compared with wakefulness. In addition to the synergistic core, overall reductions
425 are also observed in a set of thalamic, auditory and somatomotor regions, largely resembling
426 the brain regions that stop responding to sensory (auditory and noxious) stimuli once the
427 brain reaches propofol-induced saturation of EEG slow-wave activity (SWAS (Ní
428 Mhuirheartaigh et al., 2013)). Although there was no EEG data available to confirm this,
429 the doses of propofol employed in the present study are compatible with the doses of
430 propofol at which SWAS has been shown to arise (Warnaby et al., 2017), and therefore it is
431 plausible that our participants also reached SWAS and the loss of brain responsiveness it
432 indicates.

433 Thus, both resting-state integration of information between brain regions, as well as stimulus-
434 evoked responses within each region (Ní Mhuirheartaigh et al., 2013), converge to indicate
435 that propofol disrupts further processing of thalamocortical sensory information – a
436 phenomenon termed “thalamocortical isolation” (Ní Mhuirheartaigh et al., 2013). We
437 propose that as the thalamus and sensory cortices lose their ability to respond to stimuli, they
438 cease to provide information to the synergistic core of the global workspace, resulting in a
439 disconnection from the external world and presumably loss of consciousness.

440 These results testify to the power of the Integrated Information Decomposition framework:
441 by identifying the information-theoretic components of integrated information, we have been
442 able to obtain insights about human consciousness that remained elusive with alternative
443 formulations, and could not be captured via standard functional connectivity or related
444 methods. Thus, our findings support the notion that the global workspace is highly relevant
445 for supporting consciousness in the human brain, in line with the proposal that “[...]”
446 *unconsciousness is not necessarily a complete suppression of information processing but*
447 *rather a network dysfunction that could create inhospitable conditions for global information*
448 *exchange and broadcasting*” (Mashour et al., 2020). GNWT postulates a key role for the
449 global workspace in supporting consciousness: consistent with this theory, we find that
450 several nodes of the synergistic global workspace become disconnected from each other in
451 terms of integrated information when consciousness is lost, especially between anterior and
452 posterior regions (Figure 4, brain networks). Thus, these are brain regions that (i) belong to
453 the synergistic global workspace; (ii) exhibit overall reductions of integrated information
454 when consciousness is lost; and (iii) are disconnected from other regions of the synergistic
455 workspace when consciousness is lost. The brain regions satisfying these three conditions
456 therefore constitute an interconnected “synergistic core” of workspace regions supporting
457 human consciousness.

458

459 **Limitations and future directions**

460 Intriguingly, although we have focused on anaesthetic-induced decreases in integrated
461 information, due to IIT’s prediction that this is what should occur during loss of
462 consciousness, our results also indicate concomitant increases of integrated information –
463 possibly reflecting compensatory attempts (Figure 3). Interestingly, increases appear to

464 coincide with broadcaster nodes of the synergistic workspace. In particular, even though
465 lateral prefrontal cortices are among the regions most closely associated with the global
466 neuronal workspace in the literature (Bor and Seth, 2012; Mashour et al., 2020), our results
467 indicate a paradoxical net increase in lateral prefrontal integrated information during
468 anaesthesia and DOC. We interpret this qualitatively different behaviour as indicating that
469 different subsets of the global workspace may be differentially involved in supporting
470 consciousness. However, we note that, whereas the decreases in integrated information were
471 robust to the use of different analytic approaches (e.g. use of a different parcellation or
472 different NBS threshold), the increases that we observed were less robust, with no region
473 consistently showing increases in integrated information (Supplementary Figure 3B-D).
474 Nevertheless, both this phenomenon and the meaning of increased integrated information
475 between brain regions deserve further investigation. Indeed, dreaming during anaesthesia has
476 been reported to occur in up to 27% of cases (Leslie et al., 2007), and behaviourally
477 unresponsive participants have been shown to perform mental imagery tasks during
478 anaesthesia, both of which constitute cases of disconnected consciousness (Huang et al.,
479 2018). Thus, although our doses of propofol were consistent with the presence of SWAS, we
480 cannot exclude that some of our participants may have been merely disconnected but still
481 conscious, possibly driving the increases we observed.

482 Therefore, in future work the use of independent measures to assess loss of consciousness,
483 such as SWAS (Ní Mhuirheartaigh et al., 2013), the Perturbational Complexity Index
484 (Casali et al., 2013), or quantification of the complexity of brain signals (Varley et al., 2020a)
485 could provide stronger evidence that the brain changes we observed were actually due to
486 unconsciousness rather than mere unresponsiveness. Additionally, it will be important to
487 extend these results to other perturbations of consciousness: not only loss of consciousness
488 induced by natural sleep or anaesthetics with different molecular mechanisms of action, such
489 as the dissociative anaesthetic ketamine (Colombo et al., 2019; Li and Mashour, 2019;
490 Mashour, 2014, 2016; Sarasso et al., 2015). More broadly, future research may also benefit
491 from characterising the role of the synergistic workspace in the states of altered
492 consciousness induced e.g. by psychedelics (Atasoy et al., 2018; Carhart-Harris, 2018; Luppi
493 et al., 2020b), especially since prominent involvement of the DMN has already been
494 identified (Carhart-Harris et al., 2014, 2016). Likewise, the use of paradigms different from
495 resting-state, such as measuring the brain's spontaneous responses to engaging stimuli (e.g.

496 suspenseful narratives (Naci et al., 2017) or engaging movies (Naci et al., 2014)) may provide
497 evidence for a more comprehensive understanding of brain changes during unconsciousness.

498 Additionally, the reliance here on ‘resting-state’ data without external stimuli may have
499 resulted in an overestimation of the DMN’s role in consciousness, and an under-estimation of
500 the FPN (including lateral PFC), given their known different recruitment during no-task
501 conditions (Fox et al., 2005). Indeed, recent efforts have been carried out to obtain a data-
502 driven characterisation of the brain’s global workspace based on regions’ involvement across
503 multiple different tasks (Deco et al., 2019). This work is complementary to ours in two
504 aspects: first, the focus of (Deco et al., 2019) is on the role of the workspace related to
505 cognition, whereas here we focus primarily on consciousness. Second, by using transfer
506 entropy as a measure of functional connectivity, (Deco et al., 2019) assessed the
507 directionality of information exchange – whereas our measure of integrated information is
508 undirected, but are able to distinguish between different kinds of information being
509 exchanged. Thus, different ways of defining and characterising a global workspace in the
510 human brain are possible, and can provide complementary insights about distinct aspects of
511 the human neurocognitive architecture.

512 It is also worth bearing in mind is that our measure of integrated information between pairs of
513 regions does not amount to measuring the integrated information of the brain as a whole, as
514 formally specified in the context of Integrated Information Theory (Balduzzi and Tononi,
515 2008; Tononi, 2004) - although we do show that the average integrated information between
516 pairs of regions is overall reduced across the whole brain. We also note that our revised
517 measure of integrated information is based on IIT 2.0 (Balduzzi and Tononi, 2008), which
518 relies on a conceptually distinct understanding of integrated information from the most recent
519 IIT 3.0 (Oizumi et al., 2014), whose computation requires perturbing the system and all of its
520 subsets, making it computationally intractable. Thus, these limitations should be borne in
521 mind when seeking to interpret the present results in the context of IIT.

522 We also acknowledge that our analyses did not include the cerebellum and brainstem, and
523 future work may gain additional insights into their relevance for consciousness and cognition
524 by extending our results to such regions. Finally, in order to obtain high spatial resolution, we
525 relied here on brain signals based on the BOLD signal from functional MRI, which is only an
526 indirect proxy of underlying neuronal activity, with limited temporal resolution. We sought to
527 alleviate potential confounds of the hemodynamic response function by deconvolving it from

528 our data with a state-of-the-art toolbox (Wu et al., 2013) (Methods), which has been
529 previously applied both in the context of anaesthesia (Wu et al., 2019), and of applying
530 measures of integrated information to functional MRI data. Nevertheless, future applications
531 of our analytic framework to M/EEG data may provide further insights.

532

533 **Conclusion**

534 Overall, we have shown that powerful insights about human neurocognitive architecture can
535 be obtained through a more nuanced understanding of information exchange in the human
536 brain, afforded by the framework of Integrated Information Decomposition.

537 Importantly, the proposed criteria to identify gateways, broadcasters, and the synergistic
538 workspace itself, are based on practical network and information-theoretic tools, which are
539 applicable to a broad range of neuroimaging datasets.

540 By refining and combining both the Global Neuronal Workspace Theory and Integrated
541 Information Theory of consciousness, these findings bring us closer to a unified theoretical
542 understanding of consciousness and its neuronal underpinnings - how mind arises from
543 matter.

544

545

546

547

Materials and Methods

548

549 **Anaesthesia Data**

550 The propofol data employed in this study have been published before (Luppi et al., 2019;
551 Naci et al., 2018; Varley et al., 2020a). For clarity and consistency of reporting, where
552 applicable we use the same wording as our previous study (Luppi et al., 2019).

553 **Recruitment**

554 As previously reported (Luppi et al., 2019), “The propofol data were collected at the Robarts
555 Research Institute in London, Ontario (Canada) between May and November 2014. A total of
556 19 (18–40 years; 13 males) healthy, right- handed, native English speakers, with no history of
557 neurological disorders were recruited. Each volunteer provided written informed consent,
558 following relevant ethical guidelines, and received monetary compensation for their time.
559 The Health Sciences Research Ethics Board and Psychology Research Ethics Board of
560 Western University (Ontario, Canada) ethically approved this study. Due to equipment
561 malfunction or physiological impediments to anaesthesia in the scanner, data from three
562 participants (1 male) were excluded from analyses, leaving 16” (Luppi et al., 2019).

563

564 **Procedure**

565 Resting-state fMRI data were acquired at no sedation (Awake), and Deep sedation
566 (anaesthetised: Ramsay score of 5), and also during post-anaesthetic recovery. As previously
567 reported (Luppi et al., 2019): “Ramsay level was independently assessed by two
568 anaesthesiologists and one anaesthesia nurse in the scanning room before fMRI acquisition
569 began, in each condition. Additionally, participants performed two tests: a computerised
570 auditory target-detection task and a memory test of verbal recall, to evaluate their level of
571 wakefulness independently of the assessors. For the Awake condition, participants did not
572 receive a Ramsey score, as this scale is designed for patients in critical care. Instead, they had
573 to be fully awake, alert and communicating appropriately. An infrared camera located inside
574 the scanner was used to monitor wakefulness. For the Deep sedation condition, propofol was

575 administered intravenously using an AS50 auto syringe infusion pump (Baxter Healthcare,
576 Singapore); step-wise sedation increments sedation were achieved using an effect-site/plasma
577 steering algorithm combined with the computer-controlled infusion pump. Further manual
578 adjustments were performed as required to reach target concentrations of propofol, as
579 predicted by the TIVA Trainer (European Society for Intravenous Anaesthesia, eurosiva.eu)
580 pharmacokinetic simulation program. This software also specified the blood concentrations
581 of propofol, following the Marsh 3-compartment model, which were used as targets for the
582 pharmacokinetic model providing target-controlled infusion. The initial propofol target
583 effect-site concentration was $0.6 \mu\text{g mL}^{-1}$, with oxygen titrated to maintain SpO₂ above 96%.
584 Concentration was then increased by increments of $0.3 \mu\text{g mL}^{-1}$, and Ramsay score was
585 assessed: if lower than 5, a further increment occurred. Participants were deemed to have
586 reached Ramsay level 5 once they stopped responding to verbal commands, were unable to
587 engage in conversation, and were rousable only to physical stimulation. Data acquisition
588 began once loss of behavioural responsiveness occurred for both tasks, and the three
589 assessors agreed that Ramsay sedation level 5 had been reached. The mean estimated effect-
590 site and plasma propofol concentrations were kept stable by the pharmacokinetic model
591 delivered via the TIVA Trainer infusion pump; the mean estimated effect-site propofol
592 concentration was $2.48 (1.82- 3.14) \mu\text{g mL}^{-1}$, and the mean estimated plasma propofol
593 concentration was $2.68 (1.92- 3.44) \mu\text{g mL}^{-1}$. Mean total mass of propofol administered was
594 $486.58 (373.30- 599.86)$ mg. These values of variability are typical for the pharmacokinetics
595 and pharmacodynamics of propofol. At Ramsay 5 sedation level, participants remained
596 capable of spontaneous cardiovascular function and ventilation. However, since the sedation
597 procedure did not take place in a hospital setting, airway security could not be ensured by
598 intubation during scanning, although two anaesthesiologists closely monitored each
599 participant. Consequently, scanner time was minimised to ensure return to normal breathing
600 following deep sedation. No state changes or movement were noted during the deep sedation
601 scanning for any of the participants included in the study” (Luppi et al., 2019). Propofol was
602 discontinued following the deep anaesthesia scan, and participants reached level 2 of the
603 Ramsey scale approximately 11 minutes afterwards, as indicated by clear and rapid responses
604 to verbal commands. This corresponds to the “recovery” period.

605

606

607

608 **Design**

609 As previously reported (Luppi et al., 2019): “In the scanner, subjects were instructed to relax
610 with closed eyes, without falling asleep; 8 minutes of fMRI scan without any task (“resting-
611 state”) were acquired for each participant. Additionally, a separate 5-minute long scan was
612 also acquired while a plot-driven story was presented through headphones to participants,
613 who were instructed to listen while keeping their eyes closed” (Luppi et al., 2019). The
614 present analysis focuses on the resting-state data only; the story scan data have been
615 published separately (Kandeean et al., 2020) and will not be discussed further here.

616 **Data Acquisition**

617 As previously reported (Luppi et al., 2019): “MRI scanning was performed using a 3-Tesla
618 Siemens Tim Trio scanner (32-channel coil), and 256 functional volumes (echo-planar
619 images, EPI) were collected from each participant, with the following parameters: slices = 33,
620 with 25% inter-slice gap; resolution = 3mm isotropic; TR = 2000ms; TE = 30ms; flip angle =
621 75 degrees; matrix size = 64x64. The order of acquisition was interleaved, bottom-up.
622 Anatomical scanning was also performed, acquiring a high-resolution T1- weighted volume
623 (32-channel coil, 1mm isotropic voxel size) with a 3D MPRAGE sequence, using the
624 following parameters: TA = 5min, TE = 4.25ms, 240x256 matrix size, 9 degrees FA” (Luppi
625 et al., 2019).

626

627 **Functional MRI preprocessing**

628 Following our previous work (Luppi et al., 2019), we preprocessed the functional imaging
629 data using a standard pipeline, implemented within the SPM12-based
630 (<http://www.fil.ion.ucl.ac.uk/spm>) toolbox CONN (<http://www.nitrc.org/projects/conn>),
631 version 17f(Whitfield-Gabrieli and Nieto-Castanon, 2012). As described, “The pipeline
632 comprised the following steps: removal of the first five scans, to allow magnetisation to reach
633 steady state; functional realignment and motion correction; slice-timing correction to account
634 for differences in time of acquisition between slices; identification of outlier scans for
635 subsequent regression by means of the quality assurance/artifact rejection software *Artifact*

636 *Detection Toolbox* (art; (http://www.nitrc.org/projects/artifact_detect)); spatial normalisation
637 to Montreal Neurological Institute (MNI-152) standard space with 2mm isotropic resampling
638 resolution, using the segmented grey matter image from each volunteer's high-resolution T1-
639 weighted image, together with an *a priori* grey matter template" (Luppi et al., 2019).

640

641 **Disorders of Consciousness Patient Data**

642 The DOC patient functional data employed in this study have been published before (Luppi et
643 al., 2019, 2020b; Varley et al., 2020b). For clarity and consistency of reporting, where
644 applicable we use the same wording as our previous study (Luppi et al., 2019).

645

646 **Recruitment**

647 As previously reported (Luppi et al., 2019): "A sample of 71 DOC patients was included in
648 this study. Patients were recruited from specialised long-term care centres. To be invited to
649 the study, patients must have had a DOC diagnosis, written informed consent to participation
650 from their legal representative, and were capable of being transported to Addenbrooke's
651 Hospital. The exclusion criteria included any medical condition that made it unsafe for the
652 patient to participate (decision made by clinical personnel blinded to the specific aims of the
653 study) or any reason they are unsuitable to enter the MRI scanner environment (e.g. non-
654 MRI-safe implants), significant pre-existing mental health problems, or insufficient English
655 pre injury. After admission, each patient underwent clinical and neuroimaging testing.
656 Patients spent a total of five days (including arrival and departure days) at Addenbrooke's
657 Hospital. Coma Recovery Scale-Revised (CRS-R) assessments were recorded at least daily
658 for the five days of admission. If behaviours were indicative of awareness at any time,
659 patients were classified as MCS; otherwise UWS. We assigned MCS- or MCS+ sub-
660 classification if behaviours were consistent throughout the week. The most frequent signs of
661 consciousness in MCS- patients are visual fixation and pursuit, automatic motor reactions
662 (e.g. scratching, pulling the bed sheet) and localisation to noxious stimulation whereas MCS+
663 patients may, in addition, follow simple commands, intelligibly verbalise or intentionally but
664 inaccurately communicate^{53,54}. Scanning occurred at the Wolfson Brain Imaging Centre,
665 Addenbrooke's Hospital, between January 2010 and December 2015; medication prescribed

666 to each patient was maintained during scanning. Ethical approval for testing patients was
 667 provided by the National Research Ethics Service (National Health Service, UK; LREC
 668 reference 99/391). All clinical investigations were conducted in accordance with the
 669 Declaration of Helsinki. As a focus of this study was on graph-theoretical properties of the
 670 brain, patients were systematically excluded from the final cohort analysed in this study
 671 based on the following criteria: 1) large focal brain damage (i.e. more than 1/3 of one
 672 hemisphere) as stated by an expert in neuroanatomy blinded to the patients' diagnoses; 2)
 673 excessive head motion during resting state scanning (i.e. greater than 3mm in translation
 674 and/or 3 degrees in rotation); 3) suboptimal segmentation and normalization of images. A
 675 total of 22 adults (14 males; 17 -70 years; mean time post injury: 13 months) meeting
 676 diagnostic criteria for Unresponsive Wakefulness Syndrome/Vegetative State or Minimally
 677 Conscious State due to brain injury were included in this study” (Luppi et al., 2019) (Table
 678 1).

679 Table 1: Demographic information for patients with Disorders of Consciousness.

Sex	Age	Months post injury	Aetiology	Diagnosis	CRS-R Score
M	46	23	TBI	UWS	6
M	57	14	TBI	MCS-	12
M	46	4	TBI	MCS	10
M	35	34	Anoxic	UWS	8
M	17	17	Anoxic	UWS	8
F	31	9	Anoxic	MCS-	10
F	38	13	TBI	MCS	11
M	29	68	TBI	MCS	10
M	23	4	TBI	MCS	7
F	70	11	Cerebral bleed	MCS	9
F	30	6	Anoxic	MCS-	9
F	36	6	Anoxic	UWS	8
M	22	5	Anoxic	UWS	7
M	40	14	Anoxic	UWS	7

F	62	7	Anoxic	UWS	7
M	46	10	Anoxic	UWS	5
M	21	7	TBI	MCS	11
M	67	14	TBI	MCS-	11
F	55	6	Hypoxia	UWS	12
M	28	14	TBI	MCS	8
M	22	12	TBI	MCS	10
F	28	8	ADEM	UWS	6

680 Conscious State; TBI, Traumatic Brain Injury; fMRI-, negative responders to mental imagery task;
681 fMRI+, positive responders to mental imagery task; SMA, supplementary motor area; PPA,
682 parahippocampal place area; PMC, pre-motor cortex;

683

684 **FMRI Data Acquisition**

685 As previously reported (Luppi et al., 2019): “Resting-state fMRI was acquired for 10 minutes
686 (300 volumes, TR=2000ms) using a Siemens Trio 3T scanner (Erlangen, Germany).
687 Functional images (32 slices) were acquired using an echo planar sequence, with the
688 following parameters: 3 x 3 x 3.75mm resolution, TR = 2000ms, TE = 30ms, 78 degrees FA.
689 Anatomical scanning was also performed, acquiring high-resolution T1-weighted images
690 with an MPRAGE sequence, using the following parameters: TR = 2300ms, TE = 2.47ms,
691 150 slices, resolution 1 x 1 x 1mm”.

692

693 **Functional MRI preprocessing**

694 Due to the presence of deformations caused by brain injury, rather than relying on automated
695 pipelines, patients’ brains were individually preprocessed using SPM12, with visual
696 inspections after each step. Additionally, to further reduce potential movement artifacts, data
697 underwent despiking with a hyperbolic tangent squashing function. This is the same
698 procedure followed in our previous studies (Luppi et al., 2019, 2020b).

699

700 **Human Connectome Project data**

701 We used the same functional MRI data from 100 unrelated subjects of the Human
702 Connectome Project as in our previous work (Luppi et al., 2020a), with the same
703 preprocessing and denoising procedures, which are also described below.

704 The dataset of functional and structural neuroimaging data used in this work came from the
705 Human Connectome Project (HCP, <http://www.humanconnectome.org/>), Release Q3. Per
706 HCP protocol, all subjects gave written informed consent to the HCP consortium. These data
707 contained fMRI and diffusion weighted imaging (DWI) acquisitions from 100 unrelated
708 subjects of the HCP 900 data release (Van Essen et al., 2013). All HCP scanning protocols
709 were approved by the local Institutional Review Board at Washington University in St. Louis.

710

711 **HCP: Functional data acquisition and denoising**

712 As previously reported (Luppi and Stamatakis, 2020; Luppi et al., 2020a): “The following
713 sequences were used: Structural MRI: 3D MPRAGE T1-weighted, TR= 2400 ms, TE = 2.14
714 ms, TI = 1000 ms, flip angle = 8°, FOV= 224 × 224, voxel size = 0.7 mm isotropic. Two
715 sessions of 15 min resting-state fMRI: gradient-echo EPI, TR= 720 ms, TE= 33.1 ms, flip
716 angle = 52°, FOV= 208 × 180, voxel size = 2 mm isotropic. Here, we only used functional
717 data from the first scanning session, in LR direction”.

718 We used the minimally preprocessed images made available by the HCP Consortium (Glasser
719 et al., 2013), and subsequently followed the same aCompCor denoising pipeline described
720 above, which is the same as in our previous work (Luppi and Stamatakis, 2020; Luppi et al.,
721 2020a).

722

723 **Brain Parcellation**

724 Brains were parcellated into 454 cortical and subcortical regions of interest (ROIs). The 400
725 cortical ROIs were obtained from the scale-400 version of the recent Schaefer local-global
726 functional parcellation (Schaefer et al., 2018). Since this parcellation only includes cortical
727 regions, it was augmented with 54 subcortical ROIs from the highest resolution of the recent

728 Tian 2020 parcellation (Tian et al., 2020). We refer to this 454-ROI parcellation as the
729 “augmented Schaefer” (Luppi and Stamatakis, 2020).

730 To ensure the robustness of our results to the choice of atlas, we also replicated them using an
731 alternative cortical parcellation of different dimensionality: we used the Schaefer scale-200
732 cortical parcellation, complemented with the scale-32 subcortical ROIs from the Tian
733 subcortical atlas (Luppi and Stamatakis, 2020).

734

735 **BOLD timeseries extraction and HRF deconvolution**

736 To construct matrices of functional connectivity, the timecourses of denoised BOLD signals
737 were averaged between all voxels belonging to a given atlas-derived ROI, using the CONN
738 toolbox. The resulting region-specific timecourses of each subject were then extracted for
739 further analysis in MATLAB version 2016a.

740 IN accordance with our previous work (Luppi et al., 2020a) and previous studies using of
741 information-theoretic measures in the context of functional MRI data, we used a state-of-the-
742 art toolbox (Wu et al., 2013) to deconvolve the hemodynamic response function from our
743 regional BOLD signal timeseries.

744

745 **Integrated Information Decomposition**

746 The framework of integrated information decomposition (Φ ID) unifies integrated information
747 theory (IIT) and partial information decomposition (PID) to decompose information flow into
748 interpretable, disjoint parts. In this section we provide a brief description of Φ ID and
749 formulae required to compute the results in Figures 2 and 3. For further details, see (Mediano
750 et al., 2019a).

751

752 **Partial information decomposition**

753 We begin with Shannon’s Mutual information (MI), which quantifies the interdependence
754 between two random variables X and Y . It is calculated as

$$I(X;Y) = H(X) - H(X|Y) = H(X) + H(Y) - H(X,Y) \quad (1)$$

where $H(X)$ stands for the Shannon entropy of a variable X . Above, the first equality states that the mutual information is equal to the reduction in entropy (i.e. uncertainty) about X after Y is known. Put simply, the mutual information quantifies the information that one variable provides about another (Cover and Thomas, 2005).

Crucially, Williams and Beer (Williams and Beer, 2010) observed that the information that two source variables X and Y give about a third target variable Z , $I(X,Y;Z)$, should be decomposable in terms of different *types* of information: information provided by one source but not the other (unique information), by both sources separately (redundant information), or jointly by their combination (synergistic information). Following this intuition, they developed the *Partial Information Decomposition* (PID; (Williams and Beer, 2010)) framework, which leads to the following fundamental decomposition:

$$I(X,Y;Z) = \text{Red}(X,Y;Z) + \text{Un}(X;Z|Y) + \text{Un}(Y;Z|X) + \text{Syn}(X,Y;Z). \quad (2)$$

Above, *Un* corresponds to the unique information one source but the other doesn't, *Red* is the redundancy between both sources, and *Syn* is their synergy: information that neither X nor Y alone can provide, but that can be obtained by considering X and Y together.

The simplest example of a purely synergistic system is one in which X and Y are independent fair coins, and Z is determined by the exclusive-OR function $Z = \text{XOR}(X,Y)$: i.e, $Z=0$ whenever X and Y have the same value, and $Z=1$ otherwise. It can be shown that X and Y are both statistically independent of Z , which implies that neither of them provide - by themselves - information about Z . However, X and Y together fully determine Z , hence the relationship between Z with X and Y is purely synergistic.

Recently, Mediano et al (2019) (Mediano et al., 2019a) formulated an extension of PID able to decompose the information that multiple source variables have about multiple target variables. This makes PID applicable to the dynamical systems setting, and yields a decomposition with redundant, unique, and synergistic components in the past and future that can be used as a principled method to analyse information flow in neural activity.

784 Synergy and redundancy calculation

785 As we previously observed (Luppi et al., 2020a): “While PID provides a formal framework, it
786 does not enforce how the corresponding parts ought to be calculated. While there is ongoing
787 research on the advantages of different decompositions for discrete data, most
788 decompositions converge into the same simple form for the case of continuous Gaussian
789 variables (Barrett, 2015). Known as *minimum mutual information PID* (MMI-PID), this
790 decomposition quantifies redundancy in terms of the minimum mutual information of each
791 individual source with the target; synergy, then, becomes identified with the additional
792 information provided by the weaker source once the stronger source is known. Since linear-
793 Gaussian models are sufficiently good descriptors of functional MRI timeseries (and more
794 complex, non-linear models offer no advantage (Schulz et al., 2019)), here we adopt the
795 MMI-PID decomposition, following previous applications of PID to neuroscientific data
796 (Bím et al., 2019).

797 In a dynamical system such as the brain, one can calculate the amount of information flowing
798 from the system’s past to its future, known as time-delayed mutual information (TDMI).
799 Specifically, by denoting the past of variables as $X_{t-\tau}$ and $Y_{t-\tau}$ and treating them as sources,
800 and their joint future state (X_t, Y_t) , as target, one can apply the PID framework and decompose
801 the information flowing from past to future as

$$\begin{aligned} I(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t) \\ &= Red(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t) + Un(X_{t-\tau}; X_t, Y_t | Y_{t-\tau}) \\ &+ Un(Y_{t-\tau}; X_t, Y_t | X_{t-\tau}) + Syn(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t) \end{aligned}$$

802 (3)

803 Applying Φ ID to this quantity allows us to distinguish between redundant, unique, and
804 synergistic information shared with respect to the future variables X_t, Y_t (Mediano et al.,
805 2019a). Importantly, this framework, has identified $Syn(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t)$ with the capacity
806 of the system to exhibit emergent behaviour (Rosas et al., 2020) as well as a stronger notion
807 of redundancy, in which information is shared by X and Y in both past and future.
808 Accordingly, using the MMI- Φ ID decomposition for Gaussian variables, we use

809 $Red(X, Y) = \min\{I(X_{t-\tau}; X_t), I(X_{t-\tau}; Y_t), I(Y_{t-\tau}; X_t), I(Y_{t-\tau}; Y_t)\}$

810 (4)

$$811 \text{Syn}(X, Y) = I(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t) - \max\{I(X_{t-\tau}; X_t, Y_t), I(Y_{t-\tau}; X_t, Y_t)\}.$$

812 (5)

813 Here, we used the Gaussian solver implemented in the JIDT toolbox (Lizier, 2014) to obtain
814 TDMI, synergy and redundancy between each pair of brain regions, based on their HRF-
815 deconvolved BOLD signal timeseries” (Luppi et al., 2020a).

816

817 **Revised measure of integrated information**

818 Through the framework of Integrated Information Decomposition (Φ ID) we can decompose
819 the constituent elements of Φ , the formal measure of integrated information proposed by
820 Integrated Information Theory to quantify consciousness (Balduzzi and Tononi, 2008;
821 Oizumi et al., 2014; Tononi, 2004). Note that several variants of Φ have been proposed over
822 the years, including the original formulation of Tononi (Balduzzi and Tononi, 2008), other
823 formulations based on causal perturbation (Oizumi et al., 2014) and others (see (Mediano et
824 al., 2019b; Tegmark, 2016) for recent reviews). Here, we focus on the “empirical Φ ” measure
825 of (Barrett and Seth, 2011), based on the measures by Balduzzi and Tononi (2008) (Balduzzi
826 and Tononi, 2008) and adapted to applications to experimental data. It is computed as

$$\Phi = I(X_{t-\tau}, Y_{t-\tau}; X_t, Y_t) - I(X_{t-\tau}; X_t) - I(Y_{t-\tau}; Y_t)$$

827 (6)

828 and it quantifies how much temporal information is contained in the system over and above
829 the information in its past. However, as others have pointed out (Oizumi et al., 2016), the
830 measure in Eq. (6) can be negative, which is contradictory when taken as an absolute measure
831 of integration.

832 Interestingly, with Φ ID it can be shown that Φ is composed of different information atoms: it
833 contains all the synergistic information in the system, the unique information transferred from
834 X to Y and vice versa, and, importantly, a negative redundancy contribution - which explains
835 why \square can be negative in redundancy-dominated systems.

836

837 To address this, Mediano et al. (2019) (Mediano et al., 2019a) introduced a revised measure
838 of integrated information, Φ -R, which consists of the original Φ with the redundancy added
839 back in,

840

$$841 \quad \Phi\text{-R} = \Phi + \text{Red}(X, Y)$$

842 (7)

843 where $\text{Red}(X, Y)$ is defined in Eq. (4). This measure is computationally tractable and
844 preserves the original intuition of integrated information as measuring the extent to which
845 “the whole is greater than the sum of its parts”, since it captures only synergistic and
846 transferred information. Crucially, thanks to Integrated Information Decomposition, it can be
847 proved that the improved formulation of integrated information that we adopt here is
848 guaranteed to be non-negative (Mediano et al., 2019a) - thereby avoiding a major conceptual
849 limitation of the original formulation of Φ .

850

851 It is worth noting that more recent renditions of the theory exist (Oizumi et al., 2014). We do
852 not consider the measure of integrated information proposed in IIT 3.0 (Oizumi et al., 2014)
853 because it is computationally intractable for systems bigger than a small set of logic gates,
854 and it is not universally well-defined (Barrett and Mediano, 2019).

855

856 **Gradient of redundancy-to-synergy relative importance to identify the synergistic** 857 **workspace**

858 After building networks of synergistic and redundant interactions between each pair of
859 regions of interest (ROIs), we determined the role of each ROI in terms of its relative
860 engagement in synergistic or redundant interactions. Following the procedure previously
861 described by Luppi et al (2020) (Luppi et al., 2020a), we first calculated the nodal strength of
862 each brain region as the sum of all its connections in the group-averaged matrix. Then, we
863 ranked all 454 regions based on their nodal strength (with higher-strength regions having
864 higher ranks). This procedure was done separately for networks of synergy and redundancy.
865 Subtracting each region’s redundancy rank from its synergy rank yielded a gradient from
866 negative (i.e. ranking higher in terms of redundancy than synergy) to positive (i.e. having a
867 synergy rank higher than the corresponding redundancy rank); note that the sign is arbitrary.

868 It is important to note that the gradient is based on relative - rather than absolute - differences
869 between regional synergy and redundancy; consequently, a positive rank difference does not
870 necessarily mean that the region's synergy is greater than its redundancy; rather, it indicates
871 that the balance between its synergy and redundancy relative to the rest of the brain is in
872 favour of synergy - and *vice versa* for a negative gradient (Luppi et al., 2020a).

873

874 **Subdivision of workspace nodes into gateways and broadcasters**

875 To identify which regions within the workspace play the role of gateways or broadcasters
876 postulated in our proposed architecture, we followed a procedure analogous to the one
877 adopted to identify the gradient of redundancy-synergy relative importance (Luppi et al.,
878 2020a), but replacing the node *strength* with the node *participation coefficient*.

879 The participation coefficient P_i quantifies the degree of connection that a node entertains with
880 nodes belonging to other modules: the more of a node's connections are towards other
881 modules, the higher its participation coefficient will be⁸. Conversely, the participation
882 coefficient of a node will be zero if its connections are all with nodes belonging to its own
883 module.

$$P_i = 1 - \sum_{s=1}^M \left(\frac{\kappa_{is}}{k_i} \right)^2$$

884 (8)

885 Here, κ_{is} is the strength of positive connections between node i and other nodes in module s ,
886 k_i is the strength of all its positive connections, and M is the number of modules in the
887 network. The participation coefficient ranges between zero (no connections with other
888 modules) and one (equal connections to all other modules)⁸.

889 Here, modules were set to be the seven canonical resting-state networks identified by Yeo
890 and colleagues (Yeo et al., 2011), into which the Schaefer parcellation is already divided
891 (Schaefer et al., 2018), with the addition of an eighth subcortical network comprising all
892 ROIs of the Tian subcortical network (Tian et al., 2020). The brain's RSNs were chosen as
893 modules because of their distinct and well-established functional roles, which fit well with
894 the notion of modules as segregated and specialised processing systems interfacing with the

895 global workspace. Additionally, having the same definition of modules for synergy and
896 redundancy allowed us to compute their respective participation coefficients in an unbiased
897 way.

898 Separately for connectivity matrices of synergy and redundancy, the participation coefficient
899 of each brain region was calculated. Then, regions belonging to the synergistic workspace
900 were ranked, so that higher ranks indicated higher participation coefficient. Finally, the
901 redundancy-based participation coefficient rank of each workspace region was subtracted
902 from its corresponding synergy-based participation coefficient rank.

903 This procedure yielded a gradient over workspace regions, from negative (i.e. having a more
904 highly ranked participation coefficient based on redundancy than synergy) to positive (i.e.
905 having a more highly ranked participation coefficient based on synergy than redundancy).
906 Note that as before, the sign of this gradient is arbitrary, and it is based on relative rather than
907 absolute difference. Workspace regions with a positive gradient value were classified as
908 “gateways”, since they have synergistic connections with many brain modules. In contrast,
909 workspace regions with a negative value of the gradient - i.e. those whose redundancy rank is
910 higher than their synergy rank, in terms of participation coefficient - were labelled as
911 workspace “broadcasters”, since they possess information that is duplicated across multiple
912 modules in the brain.

913

914 **Statistical Analysis**

915 **Network Based Statistic**

916 The network-based statistic approach (Zalesky et al., 2010) was used to investigate the
917 statistical significance of propofol-induced or DOC-induced alterations on the networks of
918 synergistic and redundant connections. This nonparametric statistical method is designed to
919 control the family-wise error due to multiple comparisons, for application to graph data.
920 Connected components of the graph are identified from edges that survive an a-priori
921 statistical threshold (F-contrast; here we set the threshold to an F-value of 9). In turn, the
922 statistical significance of such connected components is estimated by comparing their
923 topology against a null distribution of the size of connected components obtained from non-
924 parametric permutation testing. This approach rejects the null hypothesis on a component-by-

925 component level, and therefore achieves superior power compared to mass-univariate
926 approaches (Zalesky et al., 2010).

927

928 **Testing for common effects across datasets**

929 Since we are interested in the neural basis of consciousness, it is crucial to find changes that
930 are common across datasets, to rule out possible propofol- or DOC-specific effects that are
931 not related to consciousness per se (Luppi et al., 2019). To this end, we employed a null
932 hypothesis significance test under the composite null hypothesis that *at least* one dataset
933 among those considered here has no effect. In other words, for the null hypothesis to be
934 rejected we demand that all comparisons exhibit non-zero effects.

935

936 As usual, the test proceeds by comparing an observed test statistic with a null distribution.
937 The test statistic is the minimum of the three F-scores obtained in the comparisons of interest
938 (DOC vs awake; anaesthesia vs awake; and anaesthesia vs recovery), and the null distribution
939 is sampled by randomly reshuffling exactly one dataset (picked at random) at a time and
940 recalculating the F-scores. By shuffling exactly one dataset (instead of all of them), we are
941 comparing the observed data against the “least altered” version of the data that is still
942 compatible with the null hypothesis. This is a type of *least favourable configuration* (LFC)
943 test (Lehmann and Romano, 2005), which is guaranteed to control the false positive rate
944 below a set threshold (here, 0.05). The details of this test will be described in a future
945 publication.

946 Common connectivity changes across the three states of consciousness were then identified
947 as edges that were either (i) increased in DOC compared with control; (ii) increased during
948 anaesthesia compared with wakefulness; and (iii) increased during anaesthesia compared with
949 post-anaesthetic recovery; or (i) decreased in DOC compared with control; (ii) decreased
950 during anaesthesia compared with wakefulness; and (iii) decreased during anaesthesia
951 compared with post-anaesthetic recovery.

952

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974

975 **Author Contributions**

976 AIL: conceived the study; analysed data; wrote first draft of the manuscript. PAM: conceived
977 the study; contributed to data analysis and interpretation of results; reviewed and edited the
978 manuscript. FR: contributed to data analysis and interpretation of results; reviewed and edited
979 the manuscript. M.M.C.: contributed to data analysis. DKM: reviewed the manuscript. RCH:
980 reviewed the manuscript and contributed to interpretation of results. DB: conceived the study
981 ; reviewed and edited the manuscript. EAS: conceived the study; reviewed and edited the
982 manuscript. P.F., G.B.W., J.A., J.D.P., A.M.O., L.N., D.K.M. and E.A.S. were involved in
983 designing the original studies for which the present data were collected. P.F., M.M.C.,
984 G.B.W., J.A., L.N. and E.A.S. all participated in data collection.

985

986 **Competing Interests**

987 The authors declare no competing interests.

988

989 **Data and Code Availability**

990 The CONN toolbox is freely available online (<http://www.nitrc.org/projects/conn>).

991 The Brain Connectivity Toolbox code used for graph-theoretical analyses is freely available
992 online (<https://sites.google.com/site/bctnet/>).

993 The Java Information Dynamics Toolbox is freely available online:

994 (<https://github.com/jlizier/jidt>).

995 The HRF deconvolution toolbox is freely available online:

996 (<https://www.nitrc.org/projects/rshrf>).

997 The Network Based Statistic code is freely available online:

998 <https://www.nitrc.org/projects/nbs/>

999 The HCP fMRI data are available online ([https://www.humanconnectome.org/study/hcp-](https://www.humanconnectome.org/study/hcp-young-adult/data-releases)
1000 [young-adult/data-releases](https://www.humanconnectome.org/study/hcp-young-adult/data-releases)).

1001 The propofol and DOC patient data that support the findings of this study are available from
1002 Dr. Emmanuel Stamatakis, University of Cambridge (email: eas46@cam.ac.uk) upon
1003 reasonable request.

1004

1005

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