

# 1 **Action does not enhance but attenuates predicted touch**

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## 4 **Abstract**

5 Dominant motor control theories propose that the brain uses efferent information to  
6 predict and attenuate the somatosensory consequences of actions, referred to as sensory  
7 attenuation. Support for this model comes from psychophysical and neuroimaging studies  
8 showing that touch applied on a passive hand elicits attenuated perceptual and neural  
9 responses if it is generated by actively tapping with one's other hand, compared to  
10 identical touch from an external origin. However, recent experimental findings have  
11 challenged this view by providing psychophysical evidence that the perceived intensity of  
12 touch on the passive hand is enhanced if the active hand does not receive simultaneous  
13 tactile stimulation with the passive hand (somatosensory enhancement) and by further  
14 attributing attenuation effects to the double tactile stimulation of the hands upon contact.  
15 Here, we directly contrasted the hypotheses of the attenuation and enhancement models  
16 regarding how action influences somatosensory perception by manipulating whether the  
17 active hand contacts the passive hand. In three preregistered experiments, we demonstrate  
18 that action does not enhance the perceived intensity of touch (Experiment 1), that the  
19 previously reported "enhancement" effects are driven by the baseline condition used  
20 (Experiment 2), and that self-generated touch is robustly attenuated regardless of whether  
21 the two hands make contact (Experiment 3). Our results provide conclusive evidence that  
22 action does not enhance but attenuates predicted touch. These findings prompt a  
23 reappraisal of recent experimental findings upon which theoretical frameworks proposing  
24 a perceptual enhancement by action prediction are based.

## 25 **Highlights**

- 26 • Dominant motor control theories propose that action attenuates or cancels  
27 predicted touch.
- 28 • Recent theories propose that action enhances predicted touch.
- 29 • We show that action does not enhance but attenuates predicted touch.

## 30 **Keywords**

31 somatosensory attenuation; prediction; cancellation; sharpening; enhancement

## 32 **Introduction**

33 Dominant motor control theories propose that the brain uses an internal forward model in  
34 combination with a copy of the motor command (efference copy) to predict the sensory  
35 consequences of our movements (McNamee & Wolpert, 2019; Shadmehr et al., 2008;  
36 Daniel M Wolpert & Flanagan, 2001). For example, the brain predicts the upcoming  
37 touch as one reaches towards an object. These predictions allow for the correction of  
38 motor errors without relying on sensory feedback that suffers from intrinsic delays  
39 (Shadmehr et al., 2010), thereby improving the estimation of the current state of our body  
40 by combining the predicted touch with the actual sensory input (Scott, 2004; Shadmehr et  
41 al., 2008; Todorov & Jordan, 2002). These predictions *attenuate* the perception of the  
42 self-generated input (sensory reafference) compared to that of externally generated input  
43 (Davidson & Wolpert, 2005; Franklin & Wolpert, 2011; D. M. Wolpert & Kawato, 1998)  
44 and infer whether the cause of the sensory input is the self or the environment (Brown et  
45 al., 2013; P. Corlett, 2020; Idei et al., 2022). A classic example of this attenuation is that  
46 we are unable to tickle ourselves with our own touch, yet we are easily tickled by the  
47 touch of others (S.-J. Blakemore, Wolpert, et al., 2000). The attenuation of sensory  
48 reafference – also referred to as sensory cancelation – is thought to be necessary to  
49 compensate for the limited capacity of the sensory systems by optimally prioritising the  
50 perception of more informative externally generated stimuli (Bays & Wolpert, 2012;  
51 McNamee & Wolpert, 2019). Thus, the attenuation model proposes that we dampen  
52 perceptual representations of expected self-generated stimuli to reduce redundancy and to  
53 highlight behaviourally relevant unexpected externally generated stimuli.

54 In contrast, an alternative theoretical framework proposes that predictions, including  
55 those arising from our motor commands, should not attenuate but instead enhance  
56 sensory signals, thereby allowing for sharper (*i.e.*, more accurate) representations of  
57 predicted compared to unpredicted sensory events (Press et al., 2020; Press & Yon, 2019;  
58 Yon et al., 2020a). This *enhancement* account – also referred to as the sharpening account  
59 – posits that predictions based on our motor commands are equivalent to expectations  
60 formed by statistical regularities in sensory input or from prior knowledge (*e.g.*, at the  
61 North Pole, one expects to see a polar bear rather than an elephant) and that these  
62 predictions should bias our perception towards our expectations. The proposal mainly  
63 stems from experimental research outside the domain of action and argues that weak,  
64 noisy, or ambiguous sensory input that is in line with prior expectations should be  
65 enhanced to achieve, on average, more accurate representations. For example, we are  
66 more biased to report the presence of visual events that are statistically likely to occur  
67 rather than unlikely events (Chalk et al., 2010; Wyart et al., 2012), more sensitive to low-  
68 level visual features that are in line with prior expectations (Stein & Peelen, 2015; Teufel  
69 et al., 2018), and show greater biases when perceiving visual events that are congruent  
70 with our expectations (Hudson, Nicholson, Ellis, et al., 2016; Hudson, Nicholson,  
71 Simpson, et al., 2016). Such effects are thought to result from mechanisms that increase  
72 the “gain” of expected information by altering the weights of different sensory signals  
73 (Summerfield & de Lange, 2014). Thus, the enhancement model proposes that we  
74 amplify the perceptual representations of expected compared to unexpected sensory  
75 input.

76 In the somatosensory domain, evidence supporting the attenuation model has repeatedly  
77 shown that touch delivered to one (passive) hand by the other (active) hand (*i.e.*, self-  
78 generated touch) is perceived as weaker or less ticklish (Asimakidou et al., 2022; Bays et  
79 al., 2005, 2006; Sarah J. Blakemore et al., 1999; Kilteni et al., 2018, 2019, 2020, 2021;  
80 Kilteni & Ehrsson, 2017a, 2017b, 2022; Knoetsch & Zimmermann, 2021; McNaughton  
81 et al., 2022; Weiskrantz et al., 1971; Wolpe et al., 2016) and evokes attenuated  
82 somatosensory cortical activation (Sarah J. Blakemore et al., 1998; Hesse et al., 2010;  
83 Kilteni & Ehrsson, 2020; Shergill et al., 2013, 2014) compared to touch of identical  
84 intensity applied on the passive hand that is externally generated. In contrast, one study  
85 supporting the enhancement model has shown that the action of the active hand results in  
86 an increase in the perceived intensity of touch on the passive hand, provided that the  
87 active hand never receives touch simultaneously with the passive hand (*i.e.*, hands do not  
88 make contact) (Thomas et al., 2022). This enhancement finding has been recently used to  
89 support the sharpening model and to argue that attenuation effects are due to unspecific  
90 gating processes caused by the simultaneous double tactile stimulation of the two hands  
91 (Press et al., 2022).

92 The attenuation (or cancellation) and enhancement (or sharpening) models present  
93 strikingly different hypotheses regarding how action influences the perception of sensory  
94 input and are supported by contradictory experimental evidence, leading to debates  
95 between researchers (P. Corlett, 2020; Führer et al., 2022; Kilteni & Ehrsson, 2022; Press  
96 et al., 2020, 2022). The present study aimed to contribute to this debate by revisiting the  
97 enhancement findings (Thomas et al., 2022) and directly contrasting them with earlier  
98 attenuation findings (Bays et al., 2006) which used similar experimental manipulations  
99 with respect to the contact between the hands. To this end, the same force discrimination  
100 task employed in earlier studies reporting attenuation (Asimakidou et al., 2022; Bays et  
101 al., 2005, 2006; Kilteni et al., 2019, 2020, 2021, 2022; Kilteni & Ehrsson, 2022) and  
102 enhancement (Thomas et al., 2022) was used to determine (a) whether movement of the  
103 right hand enhances or attenuates the perceived magnitude of touch applied on the left  
104 hand when the two hands do not make contact (Experiments 1 and 2) and (b) whether  
105 attenuation effects are due to double tactile stimulation caused by the contact of the two  
106 hands or action prediction (Experiment 3). Capitalizing on the fact that *any* conclusion  
107 about whether action prediction “attenuates” or “enhances” the perception of the  
108 somatosensory input needs to be made with a comparison to one’s somatosensory  
109 perception in the absence of action, we also included a condition in which participants  
110 passively received externally generated touch, with which we compared the participants’  
111 perception in all experimental conditions. Consequently, if participants perceive a touch  
112 as less or more intense during action than in the absence of action, we can infer that the  
113 received touch was attenuated or enhanced, respectively. This is a critical methodological  
114 detail compared to previous studies (Bays et al., 2006; Thomas et al., 2022) because if  
115 such baseline conditions are missing, the same patterns of results can be incorrectly  
116 attributed to “attenuation” or “enhancement”: for example, if one condition produces less  
117 attenuation than another, it may be interpreted as enhancement, and vice versa. All  
118 studies and analysis plans were preregistered on the Open Science Framework prior to  
119 data collection (**STAR Methods**).

## 120 **Results**

### 121 **Experiment 1. Action does not enhance predicted touch.**

122 Thirty naïve participants moved their right index finger towards their left index finger to  
123 generate the touch on their left index finger with (*contact* condition) or without (*no-*  
124 *contact* condition) simultaneous stimulation on their active finger. A *baseline* condition  
125 in which the participants did not move their right index finger and received touch on the  
126 left index finger passively (externally generated touch) was included in order to  
127 distinguish between effects of attenuation or enhancement (**Figure 1A**).

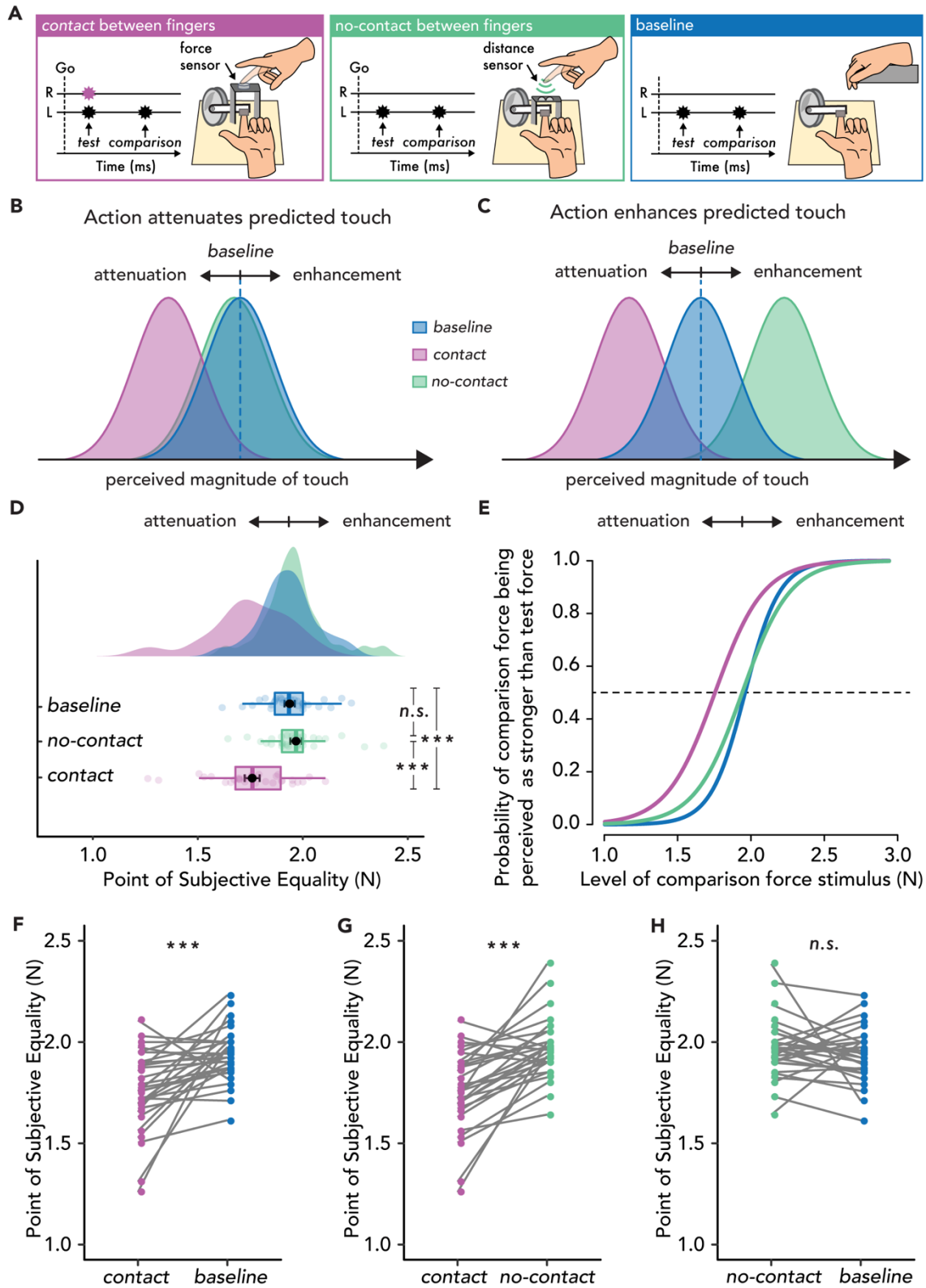
128 During the force-discrimination task, participants judged the intensity of a ‘*test*’ force and  
129 a ‘*comparison*’ force (100 ms duration each) separated by a random interval ranging from  
130 800 ms to 1200 ms. The forces were delivered to the pulp of the left index finger by a  
131 cylindrical probe attached to a lever driven by a DC electric motor. In each trial,  
132 participants reported which force they felt was stronger (the *test* or the *comparison*). The  
133 intensity of the *test* force was fixed at 2 N, while the intensity of the *comparison* force  
134 was systematically varied among seven force levels (1, 1.5, 1.75, 2, 2.25, 2.5 or 3 N). In  
135 the *contact* condition, participants moved their right index finger towards their left index  
136 finger after an auditory cue and actively tapped on a force sensor placed on top of, but not  
137 in direct contact with, the probe. The participant’s active tap on the force sensor triggered  
138 the *test* force on their left index finger, thereby producing simultaneous stimulation of  
139 both fingers in the *contact* condition and the sensation of pressing with the right index  
140 finger against the left index finger through a rigid object. Participants were told that they  
141 would always make contact between their fingers (through the probe) in this condition. In  
142 the *no-contact* condition, following the same auditory cue, participants moved their right  
143 index finger towards their left index finger. At the beginning of the condition, the force  
144 sensor was removed and replaced with a distance sensor that detected the relative  
145 distance of their active finger as it approached their left index finger to trigger the *test*  
146 force, similar to (Bays et al., 2006; Thomas et al., 2022). The distance threshold was set  
147 such that the position of the right index finger when triggering the *test* force was  
148 equivalent to that in the *contact* condition. Participants were told that they would never  
149 make contact between their fingers. Before the experiment, participants were trained to  
150 make similar movements with their right index finger in the *contact* and *no-contact*  
151 conditions. Finally, in the *baseline* condition (externally generated touch), participants  
152 were told to relax their right hand, and each trial began with the same auditory cue  
153 followed by the *test* force delivered to the participants’ left index finger 800 ms after the  
154 cue. In all trials, the *comparison* force was delivered after the *test* force, and participants  
155 verbally reported their judgement (**STAR Methods**).

156 Participants’ responses were fitted with logistic psychophysics curves, and we extracted  
157 the point of subjective equality (PSE), which represents the intensity of the comparison  
158 force at which the test force feels equally as strong. Consequently, a PSE in a movement  
159 condition (*contact* or *no-contact*) that is lower than the PSE of the *baseline* condition  
160 indicates attenuation, while a PSE that is higher than the PSE of the *baseline* condition  
161 indicates enhancement (**STAR Methods**). According to the attenuation model (**Figure**

162 **1B**), attenuation of the somatosensory input on the left hand in the *contact* condition  
163 compared to the *baseline* condition should be observed (*i.e.*, lower PSEs) due to the *test*  
164 force being predicted from the action of the right hand. Moreover, earlier studies have  
165 shown that the mere movement of one hand is not sufficient to produce predictions of  
166 somatosensory input simultaneously applied on the other hand (Bays et al., 2005; Kilteni  
167 et al., 2018; Kilteni & Ehrsson, 2017a, 2017b, 2020; Shergill et al., 2003; Wolpe et al.,  
168 2018). Instead, a bimanual sensorimotor context is needed such as during bimanual object  
169 manipulation and bimanual contact of the hands (Blakemore et al., 1998). Based on this,  
170 neither attenuation nor enhancement should be observed in the *no-contact* condition (*i.e.*,  
171 no change in PSEs from *baseline*). In contrast, according to the enhancement model, if  
172 action enhances the received sensation (Thomas et al., 2022), then higher PSEs in the *no-*  
173 *contact* condition compared to the *baseline* condition should be observed (**Figure 1C**).  
174 Finally, since the enhancement model proposes that attenuation effects are attributed to  
175 unspecific (nonpredictive) gating effects caused by the simultaneous tactile stimulation of  
176 the two hands, touch in the *contact* condition should also be perceived as weaker, albeit  
177 not due to action prediction. In summary, Experiment 1 explicitly assessed whether  
178 action enhances the received touch when the index fingers of the two hands do not make  
179 contact.

180 The results showed a robust attenuation of the perceived touch when the two fingers  
181 made contact (*contact* condition) (**Figure 1D, E, F**): the PSEs were significantly lower in  
182 the *contact* condition than in the *baseline* condition ( $W = 422.00$ ,  $p < 0.001$ ,  $rrb = 0.82$ ,  
183  $CI^{95} = [0.08\ 0.25]$ ,  $BF_{01} < 0.005$ ). Similarly, the PSEs were significantly lower in the  
184 *contact* condition than in the *no-contact* condition ( $W = 441.00$ ,  $p < 0.001$ ,  $rrb = 0.90$ ,  
185  $CI^{95} = [0.13\ 0.26]$ ,  $BF_{01} < .001$ ) (**Figure 1D, E, G**). Critically, however, in the comparison  
186 that contrasts the hypotheses of the two models, the *no-contact* condition did not produce  
187 any significant change in the perceived magnitude of the touch compared to the *baseline*  
188 condition ( $W = 187.00$ ,  $p = 0.360$ ,  $rrb = -0.20$ ,  $CI^{95} = [-0.08\ 0.030]$ ) (**Figure 1D, E, H**). A  
189 Bayesian factor analysis provided strong support for the absence of any difference  
190 ( $BF_{01}=3.58$ ). (See also **Supplementary Material** for individual fits and additional  
191 analyses).

192 In summary, we used both frequentist and Bayesian statistics and found no evidence that  
193 action of the right index finger produces an enhancement of the touch received on the left  
194 index finger when the fingers did not make contact. Thus, Experiment 1 does not support  
195 the hypothesis of the enhancement model that action enhances predicted touch but  
196 supports the hypothesis of the attenuation model.



198 **Figure 1. Experimental methods, hypotheses, and results of Experiment 1.** **A.** In the *contact*  
199 condition (magenta), participants tapped with their right index finger (R) on a force sensor placed  
200 above the probe that delivered a *test* force of 2 N to their left index finger (L), followed by a  
201 *comparison* force randomly varying between 1 and 3 N. In the *no-contact* condition (green),  
202 participants approached a distance sensor with their right index finger, which triggered the test  
203 force on their left index finger, thus receiving no touch on their active finger. In the *baseline*  
204 condition (blue), participants relaxed both hands and passively received the forces on their left  
205 index finger. **B.** Hypotheses based on the attenuation model. Touch in the *contact* condition  
206 (magenta) should be perceived as weaker than in the *baseline* (blue), but touch in the *no-contact*  
207 condition (green) should be perceived similarly to that in the *baseline* (blue). **C.** Hypotheses  
208 based on the enhancement model. Touch in the *no-contact* condition (green) should be perceived  
209 as stronger than in the *baseline* (i.e., enhanced) (blue), but touch in the *contact* condition  
210 (magenta) should be perceived weaker than the *baseline* (blue). Note that attenuation effects in  
211 the *contact* condition are predicted both by the attenuation and the enhancement model with the  
212 difference that the attenuation model attributes these effects to action prediction, while the  
213 enhancement model attributes these effects to the simultaneous touch on the active hand. **D-H.**  
214 Data are colour-coded per condition. **D.** Box plots show the median and interquartile ranges for  
215 the PSE values per condition, black circles and error bars show the mean PSE  $\pm$  s.e.m, and the  
216 raincloud plots show the individual PSE values and their distributions. No enhancement effects  
217 were observed in the *no-contact* condition. **E.** Group psychometric functions for each condition.  
218 The leftward shift of the curves in the *contact* condition indicates attenuated PSE values  
219 compared to the other two conditions. **F-H.** Line plots for individual participant PSE values  
220 illustrating significantly lower PSEs for the *contact* versus *baseline* (**F**) and *no-contact* (**G**)  
221 conditions, but no significant differences in the PSE values between *no-contact* and *baseline* (**H**).  
222 (\*\*\*) $p < .001$ )

## 223 **Experiment 2. Previous ‘enhancement’ effects are driven by the baseline used.**

224 Having found no evidence for somatosensory enhancement in Experiment 1, Experiment  
225 2 aimed to understand the potential source of the previously reported enhancement effects  
226 (Thomas et al., 2022). One critical methodological difference between Experiment 1 and  
227 the experiment of Thomas et al. (Thomas et al., 2022) concerns the *baseline* condition, as  
228 Thomas et al. (Thomas et al., 2022) compared the participants’ perception in the *no-*  
229 *contact* condition to a condition where the participants prepared their right index  
230 movement but received a NOGO cue to inhibit the movement, and it was that comparison  
231 that revealed enhancement effects. However, motor inhibition (i.e. planning the hand  
232 movement but not executing it) can lead to suppression of somatosensory input both on  
233 the hand that is planned to move (Hoshiyama & Sheean, 1998; Voss et al., 2008; Walsh  
234 & Haggard, 2007) and the hand that would receive touch if the movement was executed  
235 (Kilteni et al., 2018); moreover, such conditions result in a competition for attentional  
236 resources to inhibit the motor response with processes that encode sensory stimuli into  
237 memory (Chiu & Egner, 2015b, 2015a; Yebra et al., 2019) (e.g., the *test* force in this  
238 paradigm). Therefore, if the motor inhibition condition used by Thomas et al. (Thomas et  
239 al., 2022) results in a suppression of the perceived touch, a comparison of the *no-contact*  
240 condition with such a baseline would produce an apparent enhancement effect.

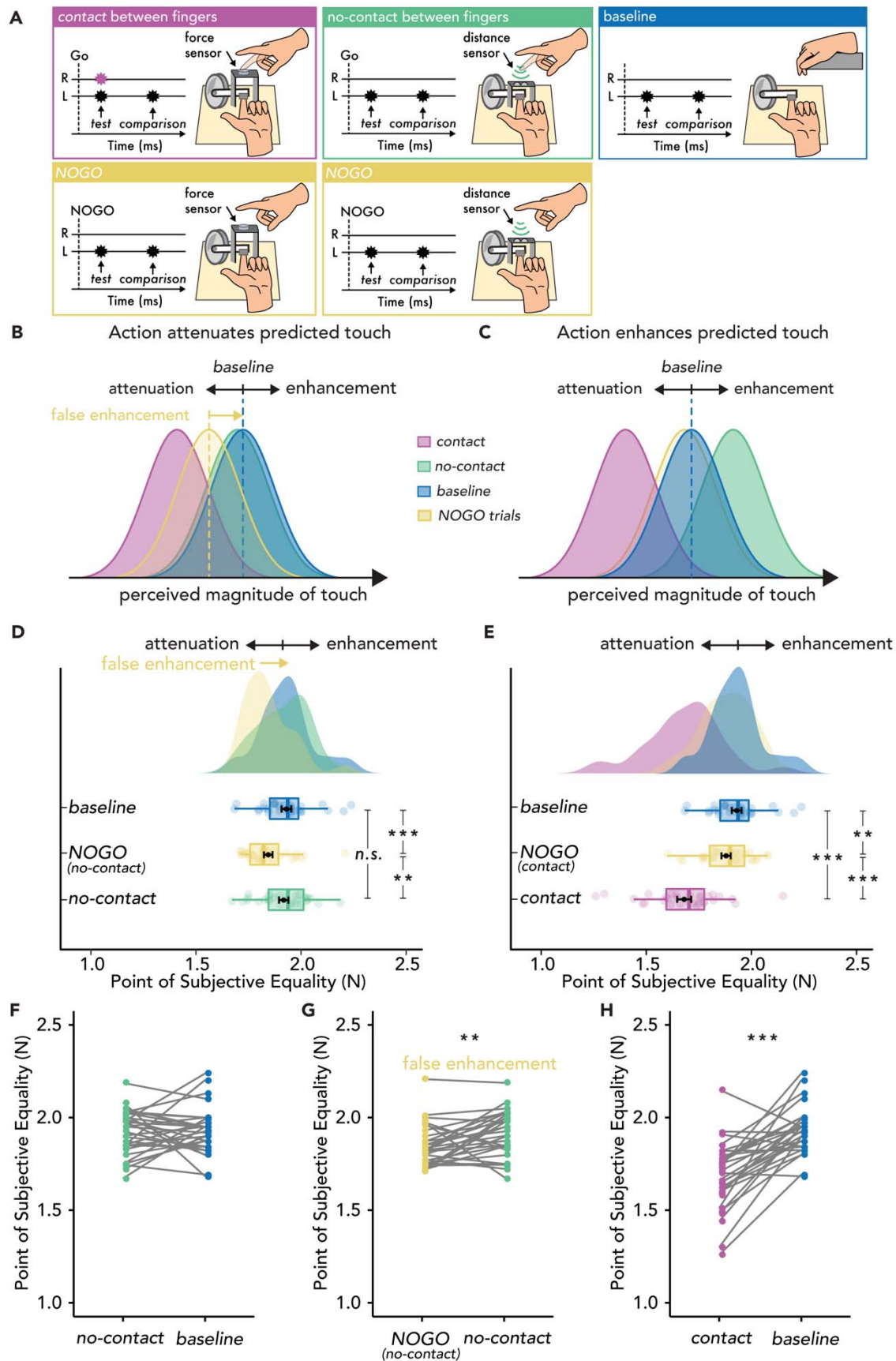
241 Thirty new naïve participants participated in Experiment 2, which included a block of  
242 *contact* trials and a block of *no-contact* trials in which participants moved their right

243 index finger, but each block also contained randomly intermixed NOGO trials where  
244 participants were cued to withhold their movement, identical to the design of Thomas et  
245 al. (Thomas et al., 2022) (**Figure 2A**). Participants were trained to make similar  
246 movements with their right index finger in the *contact* and *no-contact* trials. An  
247 externally generated touch condition was also included as an action-free *baseline*  
248 condition (*i.e.*, no action execution or inhibition). If the previously reported enhancement  
249 effects are due to the baseline used, attenuated perception of touch during the motor  
250 inhibition condition (*i.e.*, NOGO trials) should be found compared to the *baseline*, which  
251 would then lead to apparent enhancement effects upon comparison with the *no-contact*  
252 trials (**Figure 2B, C**) (**STAR Methods**).

253 This hypothesis (**Figure 2B**) was confirmed. First, all the effects of Experiment 1 were  
254 replicated in the new sample (**Figure 2D, E, F & H**). The *contact* trials yielded  
255 significant attenuation (*i.e.*, lower PSEs) compared to the *baseline* condition ( $t(29) =$   
256  $6.79, p < 0.001, d = 1.24, CI^{95} = [0.18\ 0.33], BF_{01} < 0.001$ ) (**Figure 2E & H**). Once  
257 again, there was no enhancement in the *no-contact* trials compared to the *baseline*  
258 condition ( $t(29) = 0.45, p = 0.658, d = 0.08, CI^{95} = [-0.05\ 0.07]$ ) (**Figure 2D & F**), and  
259 the Bayesian analysis again yielded strong evidence for the absence of any effects ( $BF_{01} =$   
260  $4.69$ ). Importantly, the PSEs in the *NOGO* (motor inhibition) trials were significantly  
261 lower than the *baseline* condition both for the *contact NOGO* ( $t(29) = 2.99, p = 0.006, d$   
262  $= -0.55, CI^{95} = [0.02\ 0.09], BF_{01} = 0.136$ ) and the *no-contact NOGO* trials ( $t(29) = 4.44, p$   
263  $< 0.001, d = 0.81, CI^{95} = [0.05\ 0.13], BF_{01} = 0.005$ ) (**Figure 2D, E & G**). This  
264 demonstrates that NOGO trials resulted in a suppression of perceived touch on the left  
265 hand. Critically, this led to an apparent increase in the PSE from the *no-contact* trials to  
266 the NOGO trials in the no-contact block ( $t(29) = -2.98, p = 0.006, d = -0.54, CI^{95} = [-0.12$   
267  $-0.02], BF_{01} = 0.139$ ), mimicking an ‘enhancement’ effect. Finally, PSEs were  
268 significantly lower in the *contact* trials than in the NOGO trials ( $t(29) = 5.91, p < 0.001, d$   
269  $= 1.08, CI^{95} = [0.13\ 0.27], BF_{01} < 0.001$ ), while the NOGO trials in the *contact* and *no-*  
270 *contact* blocks did not significantly differ ( $t(29) = 1.58, p = 0.126, d = 0.29, CI^{95} = [-0.01,$   
271  $0.08], BF_{01} = 1.697$ ). (See also **Supplementary Material** for individual fits and  
272 additional analyses).

273 In summary, identical to Experiment 1, we used both frequentist and Bayesian statistics  
274 and did not find any evidence that action of the right index finger produces an  
275 enhancement of the touch received on the left index finger when the fingers do not make  
276 contact. Moreover, we showed that the purported “enhancement” effect (Thomas et al.,  
277 2022) is driven by a suppression of the perceived intensity of touch following a cue to  
278 inhibit the planned movement. Thus, Experiment 2 does not support the hypothesis that  
279 action enhances predicted touch.





281 **Figure 2. Experimental methods, hypotheses, and results of Experiment 2.** **A.** The *contact*  
282 (magenta) and *no-contact* (green) trials were identical to those of Experiment 1, with the only  
283 difference that in 50% of the trials, the participants had to inhibit their movement (*NOGO* trials -  
284 yellow), and the test force was delivered automatically. The *baseline* condition (blue) was  
285 identical to that of Experiment 1. **B.** Hypotheses based on the attenuation model. Touch in the  
286 *contact* condition (magenta) should be perceived as weaker than in the *baseline* (blue), but touch  
287 in the *no-contact* condition (green) should be perceived similarly to that in the *baseline* (blue).  
288 Critically, touch may also be perceived as weaker than *baseline* in the *NOGO* trials, resulting in a  
289 ‘false enhancement’ of the *no-contact* trials. **C.** Hypotheses based on the enhancement model.  
290 Touch in the *no-contact* condition (green) should be perceived as stronger than in the *baseline*  
291 (*i.e.*, enhanced) (blue), but touch in the *contact* condition (magenta) should be perceived weaker  
292 than the *baseline* (blue). **D-H.** Data are colour-coded per condition. **D-E.** Box plots show the  
293 median and interquartile ranges for the PSE values in the *baseline* and *no-contact* blocks (**D**) and  
294 in the *baseline* and *contact* blocks (**E**). Black circles and error bars show the mean PSE  $\pm$  s.e.m,  
295 and the raincloud plots show the individual PSE values and their distributions. **F-H.** Line plots for  
296 individual participant PSE values illustrating no significant differences in the PSE values between  
297 *no-contact* and *baseline* (**F**), significantly higher PSEs for the *no-contact* versus *NOGO* trials in  
298 the same block (**G**) and significantly lower PSEs in the *contact* versus *baseline* trials (**H**). (\*\* $p <$   
299  $0.01$ , \*\*\* $p < 0.001$ )

### 300 **Experiment 3. Action attenuates predicted touch, even without simultaneous** 301 **stimulation of the active hand.**

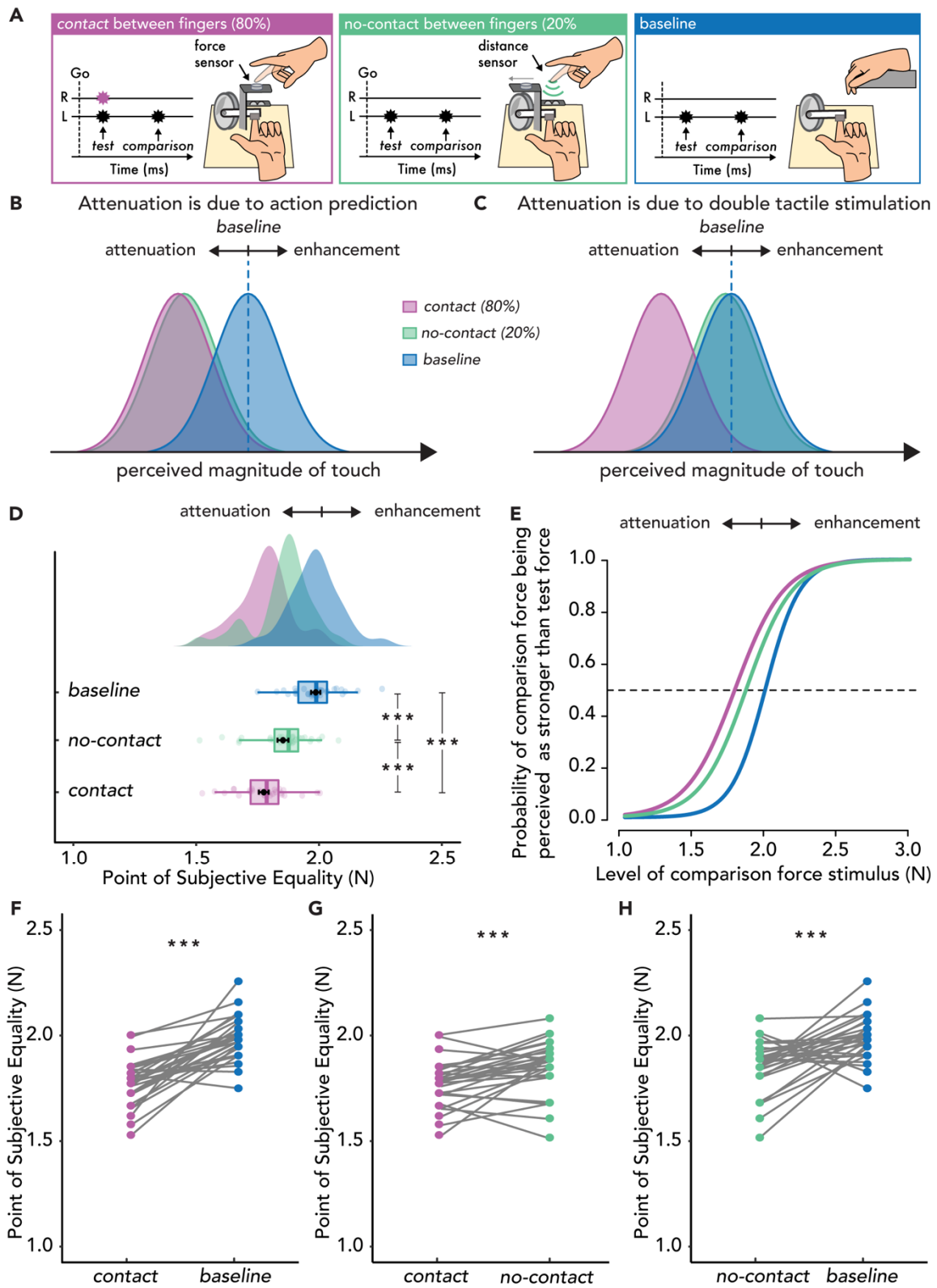
302 Within the framework of internal forward models, the absence of attenuation in the *no-*  
303 *contact* conditions of Experiments 1 and 2 is expected, given the lack of a sensorimotor  
304 context conducive to perceiving the touch as self-generated: when contact is never made,  
305 the forces applied on the passive left hand are only arbitrarily, and not causally,  
306 associated with the movement of the active right hand. Alternatively, it could be argued  
307 that the absence of attenuation in the *no-contact* conditions is caused by the lack of  
308 simultaneous tactile stimulation of the active hand rather than by predictive mechanisms.

309 In Experiment 3, this hypothesis was explicitly tested with thirty new naïve participants.  
310 The same *contact* and *no-contact* conditions were included as in Experiment 1, but their  
311 relative frequency was manipulated within the same block (*contact* trials: 80%, *no-*  
312 *contact* trials: 20%) (**Figure 3A**). The force sensor the participants tapped in the *contact*  
313 trials was now attached to a platform that could be automatically retracted. In the *contact*  
314 trials, participants tapped the force sensor to trigger the *test* force identically to  
315 Experiments 1 and 2, but in the *no-contact* trials, the platform automatically retracted  
316 before trial onset, unbeknownst to the participants, leading them to unexpectedly miss the  
317 contact with the sensor but still trigger the *test* force only by the position of their right  
318 index finger. Participants’ vision was occluded so that they could not know whether the  
319 next trial would be a *contact* or a *no-contact* trial. According to the attenuation model,  
320 providing a bimanual sensorimotor context in 80% of the trials should lead participants to  
321 form predictions about the somatosensory consequences of their movement in most of the  
322 trials and thus attenuate the received touch on their passive left hand compared to the  
323 *baseline*, even if the touch of their active hand was unexpectedly missed (**Figure 3B**). In  
324 contrast, if attenuation is a nonpredictive process caused by the mere simultaneous tactile

325 stimulation of the active finger, no attenuation effects in the *no-contact* trials should be  
326 observed with respect to the *baseline* (**Figure 3C**).

327 The results showed a robust attenuation in both *contact* and *no-contact* trials with respect  
328 to the *baseline* condition, regardless of whether contact was made (**Figure 3D, E, F &**  
329 **H**): the PSEs were significantly lower in the *contact* condition than in the *baseline*  
330 condition ( $t(29) = 8.06, p < 0.001, d = 1.47, CI^{95} = [0.16\ 0.27], BF_{01} < 0.001$ ) and lower in  
331 the *no-contact* condition than in the *baseline* condition ( $t(29) = 4.45, p < 0.001, d = 0.81,$   
332  $CI^{95} = [0.07\ 0.20], BF_{01} = 0.004$ ). The magnitude of attenuation was larger in the *contact*  
333 condition than in the *no-contact* condition, with significantly lower PSEs in the *contact*  
334 condition than in the *no-contact* condition ( $t(29) = 3.94, p < 0.001, d = 0.72, CI^{95} = [0.04$   
335  $0.12], BF_{01} = 0.016$ ) (**Figure 3G**) (see also **Supplementary Material** for individual fits  
336 and additional analyses). It should be mentioned however that the difference in the  
337 attenuation magnitudes was modest ( $\cong 35\%$ ). These findings indicate that the perceived  
338 intensity of touch on the passive left hand was significantly attenuated both when the  
339 active hand received touch or not, thereby ruling out the possibility that attenuation is  
340 merely due to simultaneous tactile stimulation (Thomas et al., 2022).

341 The results of Experiment 3 emphasise the predictive nature of somatosensory  
342 attenuation, which is observed only when the sensorimotor context allows the formation  
343 of such predictions. To further strength our interpretation we performed an ANOVA on  
344 the difference in the PSEs between the *contact* and *no-contact* conditions across all three  
345 experiments. The ANOVA revealed a significant main effect of Experiment ( $F(2, 87) =$   
346  $8.05, p < 0.001, \eta p^2 = 0.156$ ), with Bonferroni corrected post hoc comparisons indicating  
347 significant differences between Experiments 1 and 3 ( $t(2, 87) = 3.10, p = 0.008, d = 0.80,$   
348  $CI [0.03\ 0.23], BF_{01} = 0.085$ ) as well as Experiments 2 and 3 ( $t(2, 87) = 3.76, p < 0.001, d$   
349  $= 0.97, CI [0.06\ 0.26], BF_{01} = 0.002$ ), but no significant differences between Experiments  
350 1 and 2 ( $t(2, 87) = -0.66, p = 1.000, d = -0.17, CI [-0.13\ 0.07], BF_{01} = 3.308$ ). Thus, *no-*  
351 *contact* trials elicited attenuated perception only when the sensorimotor context allowed  
352 for a prediction of self-touch (Experiment 3) and not when the action was only arbitrarily  
353 associated with the touch (Experiments 1 and 2).



355 **Figure 3. Experimental methods, hypotheses, and results of Experiment 3.** **A.** The *contact*  
356 (magenta) and *no-contact* (green) conditions were identical to those of Experiment 1, with the  
357 only difference being their relative proportion (*contact* trials 80%, *no-contact* trials 20%). In the  
358 *no-contact* trials, the force sensor was automatically retracted, unbeknownst to the participant,  
359 revealing the distance sensor placed below. The *baseline* condition (blue) was identical to that of  
360 Experiments 1 and 2. **B.** Hypotheses based on the attenuation model. If attenuation is due to  
361 action prediction, then the perceived magnitude of touch should be reduced in both the *contact*  
362 (magenta) and *no-contact* conditions (green) compared to the *baseline* (blue). **C.** Hypotheses  
363 based on the enhancement model. If attenuation effects are driven by simultaneous touch on the  
364 active hand, then the perceived magnitude of touch should be reduced only in the *contact*  
365 condition (magenta) compared to the *baseline* (blue) and not in the *no-contact* condition (green)  
366 which should be similar to the *baseline* (blue). **D-H.** Data are colour-coded per condition. **D.** Box  
367 plots show the median and interquartile ranges for the PSE values per condition, black circles and  
368 error bars show the mean PSE  $\pm$  s.e.m, and the raincloud plots show the individual PSE values  
369 and their distributions. **E.** Group psychometric functions for each condition. The leftward shift of  
370 the curves in the *contact* and *no-contact* conditions indicates attenuated PSE values compared to  
371 the *baseline*. **F.** Line plots for individual participant PSE values illustrating significantly lower  
372 PSEs for the *contact* versus *baseline* condition, **G.** significantly lower PSEs in the *contact* versus  
373 *no-contact* condition and **H.** significantly lower PSEs in the *no-contact* versus *baseline*. (\*\* $p <$   
374 0.001)

## 375 Discussion

376 Clarifying how predictions about the sensory consequences of our movements affect our  
377 perception is fundamental to understanding the interaction between perception and action  
378 (McNamee & Wolpert, 2019; Shadmehr et al., 2008; Daniel M Wolpert & Flanagan,  
379 2001) but also for clinical and neurobiological theories of psychosis spectrum disorders,  
380 such as schizophrenia (S.-J. Blakemore, Smith, et al., 2000; P. R. Corlett et al., 2019; C.  
381 Frith, 2005a, 2005b; Chris D. Frith et al., 2000; Christopher D. Frith, 2019; Shergill et al.,  
382 2005, 2014) and schizotypy (Asimakidou et al., 2022), as well as functional movement  
383 disorders (Parees et al., 2014), Parkinson's disease (Wolpe et al., 2018) and ageing  
384 (Wolpe et al., 2016). In the present study, two opposing hypotheses regarding how action  
385 influences somatosensory perception were contrasted: the attenuation model and the  
386 enhancement model. Our findings demonstrate that action does not enhance (Experiments  
387 1 and 2) but attenuates the predicted touch (Experiment 3).

388 Before discussing the findings, it is important to emphasise that to draw conclusions  
389 about whether perception is attenuated or enhanced in an experimental condition  
390 including action, it is necessary to include a baseline condition without action. Only  
391 comparing conditions that include action prevents differentiating a genuine effect of  
392 enhancement (or attenuation) from an effect of reduced attenuation (or enhancement) in  
393 one of the two conditions. This also applies to experimental manipulations that contrast  
394 predicted with unpredicted somatosensory stimuli during action (see (Thomas et al.,  
395 2022) for such comparisons). To this end, a *baseline* condition of pure somatosensory  
396 exafference (*i.e.*, externally generated touch) was included in all of the present  
397 experiments that allowed us to distinguish the direction of the effects.

398 The results of Experiment 1 showed a robust attenuation of the touch applied on the  
399 passive left hand when the two hands made contact (*contact* condition), but neither  
400 attenuation nor enhancement was caused by the mere movement of the right hand (*no-*  
401 *contact* condition). In contrast, the perceived intensity of touch in the *no-contact*  
402 condition was similar to that of the *baseline* (*i.e.*, externally generated touch). These  
403 findings are in line with the results of Bays et al. (Bays et al., 2006), who found no  
404 change in the participants' somatosensory perception when the two hands did not make  
405 contact, but do not replicate those of Thomas et al. (Thomas et al., 2022), who observed  
406 enhancement of touch in a *no-contact* condition. Experiment 2 further investigated the  
407 source of the previously reported enhancement effects and showed that they are in fact  
408 driven by the baseline condition used: enhancement was observed only relative to a  
409 condition in which the touch was applied rapidly following a cue to inhibit the movement  
410 (*i.e.*, a “do not move” cue), as in previous research (Thomas et al., 2022), but not relative  
411 to an externally generated touch condition (our baseline). In support of this claim,  
412 Experiment 2 showed that a cue to inhibit the movement results in a significant reduction  
413 in the perceived intensity of the imperative stimulus (*i.e.*, touch on the passive hand)  
414 compared to baseline perception. This is in line with previous evidence showing reduced  
415 amplitude of somatosensory evoked potentials for tactile stimuli presented shortly  
416 following a cue to inhibit a movement (Hoshiyama & Sheean, 1998), reduced perceived  
417 amplitude for tactile stimuli under the mere expectation to move (Voss et al., 2006,  
418 2008), and reduced encoding of sensory stimuli following motor inhibition (Chiu &  
419 Egner, 2015b, 2015a; Yebra et al., 2019). Therefore, rather than participants' perception  
420 being enhanced in the *no-contact* condition, it is a reduction of the perceived intensity  
421 following the cue to inhibit the movement that leads to an apparent enhancement. In  
422 contrast, by including a novel externally generated touch condition as a *baseline* that  
423 involved neither motor planning nor response inhibition, it became clear that there were  
424 no enhancement effects.

425 Experiment 3 demonstrated that action attenuates the predicted touch even if the active  
426 hand does not receive simultaneous tactile stimulation with the passive hand. When  
427 participants simply moved their right hand to trigger the touch on their left hand (*no-*  
428 *contact* trials in Experiments 1 & 2), no change in their somatosensory perception was  
429 found. This suggests that an arbitrary mapping between the movement of the right hand  
430 and the delivery of touch on the left hand is insufficient to elicit attenuation. In contrast,  
431 when participants expected to touch their own hand (Experiment 3), significant  
432 attenuation was observed, even when the active hand unexpectedly missed the contact  
433 (*no-contact* trials, 20%). Thus, a sensorimotor context that closely resembles tapping  
434 directly on the left index finger with the right (self-touch) was critical (Bays et al., 2006).  
435 This finding contradicts the suggestion that attenuation on a passive hand reflects a  
436 nonpredictive gating of tactile input during movement of the active hand (Thomas et al.,  
437 2022). Indeed, several earlier studies showed gating effects only on the moving limb  
438 (movement effector) and not on the passive limb (Chapman et al., 1987; Cohen & Starr,  
439 1987; Colino et al., 2014; Papakostopoulos et al., 1975; Pertovaara et al., 1992; Rushton  
440 et al., 1981), and we also recently showed that experimental paradigms identical to the

441 one used in the present study produce attenuation effects but not gating effects on the  
442 passive hand (Kilteni & Ehrsson, 2022).

443 It is interesting to note that the magnitude of attenuation was greater in the *contact*  
444 compared to the *no-contact* condition by approximately 35% in Experiment 3. We  
445 speculate that the decrease of attenuation in the *no-contact* trials is due to the unexpected  
446 omission of contact influencing the perceived magnitude of touch in a postdictive  
447 manner. Specifically, the unexpected omission of contact on the minority of trials (20%)  
448 could be seen as a form of stimulus omission akin to so called ‘silent oddballs’ that are  
449 known to generate prediction errors (Busse & Woldorff, 2003; Karamürsel, 2000;  
450 SanMiguel, Saupe, et al., 2013; SanMiguel, Widmann, et al., 2013). Although  
451 participants clearly attenuated the touch predicted by their movement in the *no-contact*  
452 trials, their expectation of contact was necessarily violated. This violation could be  
453 considered a novel event, given its infrequency. Novel events can have several  
454 consequences for cognition, including transient enhancements of perception (Schomaker  
455 & Meeter, 2012), facilitated encoding of information into working memory (Mayer et al.,  
456 2011) as well as changes in the allocation of attentional resources in a postdictive manner  
457 (for a review of effects of novelty on cognition see (Schomaker & Meeter, 2015)).  
458

459 Some authors have criticised the comparison of perceived intensity of sensory stimuli in  
460 self-generated and externally generated conditions (Press et al., 2020; Yon et al., 2018,  
461 2020b), as tactile input may be “predicted” in self-generated conditions through action  
462 and “unpredicted” in externally generated (passive) conditions that do not involve action.  
463 This concern can be ruled out since in all three experiments, the stimulus in the *baseline*  
464 (*i.e.*, externally generated touch) condition was delivered at a fixed timepoint (800 ms  
465 after the cue); therefore, participants could predict it in the absence of motor-based  
466 predictions. Moreover, it has been argued that somatosensory attenuation findings may be  
467 driven by dual-task requirements (Press et al., 2020) present only in self-generated  
468 conditions that could increase the working memory load or result in a shift of attention  
469 towards the active hand. This explanation can also be ruled out, given that dual-task  
470 requirements were present in the *contact* and *no-contact* conditions of all three  
471 experiments without concomitant attenuation effects. Finally, alternative explanations  
472 based on differences in other psychophysical parameters, movement kinematics or  
473 timings between experiments can also be ruled out (see **Supplementary Material** for  
474 additional analyses).

475 Overall, the results suggest that attenuation effects are driven by action prediction and not  
476 the double tactile stimulation of the two hands. Somatosensory attenuation has been  
477 previously observed in the absence of double tactile stimulation, for example, when  
478 imagining but not executing the right hand movement (Kilteni et al., 2018) or just before  
479 the hands make contact (Bays et al., 2005). Similarly, no somatosensory attenuation is  
480 observed in the absence of action prediction, even if the two hands received double tactile  
481 stimulation; for example, the passive displacement of the right hand towards the left hand  
482 that is accompanied by double touch (Kilteni et al., 2020) or the mere delivery of double  
483 tactile stimulation on both hands (Bays et al., 2005) does not produce attenuation. From  
484 an ecological point of view, in every self-touch behaviour, we necessarily receive

485 somatosensory input on the active hand and the body part that passively receives touch  
486 (“touchant-touche” (Schütz-Bosbach et al., 2009)), and it is within these sensorimotor  
487 contexts that the brain forms predictions about the somatosensory consequences on  
488 multiple body parts (S J Blakemore et al., 1998).

489 How can the findings that action prediction attenuates touch be reconciled with those  
490 showing that expectations outside the domain of action improve sensory perception  
491 (Press et al., 2020)? While it is difficult to directly compare these lines of research  
492 because of differences in the sensory modality investigated, the task designs used and the  
493 perceptual measures employed, we speculate that there are numerous possible reasons  
494 why action prediction may not have the same effect on perception as prediction  
495 mechanisms outside the domain of action. First, research on action-based predictions  
496 concerns ubiquitous associations between actions and their sensory consequences that we  
497 are continually exposed to throughout the lifespan. For example, we are constantly  
498 exposed to associations between our motor behaviours and their tactile consequences  
499 during self-touch, even as early as 13 weeks *in utero* (Kurjak et al., 2003). In contrast,  
500 research on sensory expectations outside the domain of action primarily concerns  
501 arbitrary associations between stimuli that are typically learned only during the time  
502 course of a given task. It is therefore conceivable that separable mechanisms may operate  
503 to predict action effects versus stimulus-stimulus associations (see (Dogge, Custers, &  
504 Aarts, 2019; Dogge, Custers, Gayet, et al., 2019) for discussion). Second, higher-level  
505 expectations, such as explicit prior knowledge that a specific sensory event is likely,  
506 might not operate in the same way as lower-level action predictions; for example, it has  
507 been proposed that action-based predictions inhibit expected stimuli, while sensory  
508 expectations potentiate the expected sensory inputs (de Lange et al., 2018). Most  
509 importantly, from a theoretical perspective, attenuating the predicted sensory  
510 consequences of actions does not necessarily mean that the brain forms inaccurate  
511 representations of the world but instead indicates a flexible strategy that prioritises more  
512 informative externally generated events.

513 Debates between researchers supporting attenuation or enhancement are useful and  
514 fruitful for scientific dialogue and advancement. The present study revisited recent  
515 findings on somatosensory enhancement during action and showed that when the  
516 requirement to inhibit the action is removed from the baseline, action predictions do not  
517 enhance but attenuate the received somatosensory input. Our results are in strong  
518 alignment with animal studies showing that action attenuates the predicted sensory  
519 consequences (for reviews, see (Brooks & Cullen, 2019; Crapse & Sommer, 2008;  
520 Cullen, 2004; Schneider & Mooney, 2018; Straka et al., 2018)). For example, crickets  
521 and mice suppress auditory reafferent signals but maintain their sensitivity to external  
522 sounds (Audette et al., 2021; J. F. A. A. Poulet & Hedwig, 2006; J. F. A. Poulet &  
523 Hedwig, 2003; Schneider et al., 2018), the weakly electric fish attenuates its  
524 electrosensory reafference to respond to externally generated electrical signals (Cullen,  
525 2004; Sawtell, 2017), and primates attenuate their vestibular reafference and activate  
526 vestibular-related reflexes only when the vestibular input is exafferent (Brooks et al.,  
527 2015; Cullen, 2012; Roy, 2004). To this end, the results of the present study prompt a



528 reappraisal of recent experimental findings upon which theoretical frameworks proposing  
529 a perceptual enhancement by action prediction are based.

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## 535 **Author Contributions**

536 K.K. and X.J. designed the experiments; X.J. collected the data; X.J. analysed the data;  
537 X.J. and K.K. wrote the manuscript.

## 538 **Declaration of interests**

539 The authors declare no competing interests.

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853 **STAR Methods**

854 **KEY RESOURCES TABLE**

855 **Key resources table**

RESOURCE	SOURCE	IDENTIFIER
<b><i>Preregistered studies</i></b>		
Pre-registered experimental designs, methods and analyses	Open Science Framework (OSF)	Experiment 1: <a href="https://osf.io/9jkqt">https://osf.io/9jkqt</a> Experiment 2: <a href="https://osf.io/hs8au">https://osf.io/hs8au</a> Experiment 3: <a href="https://osf.io/gkwu7">https://osf.io/gkwu7</a>
<b><i>Deposited Data</i></b>		
Extracted PSEs and JNDs for analysis	This paper	Supplementary material
<b><i>Software and algorithms</i></b>		
R Studio Version 1.4.1717	R Studio Team (2021)	<a href="https://www.rstudio.com/">https://www.rstudio.com/</a>
JASP Version 0.13.1	JASP Team (2020)	<a href="https://jasp-stats.org/">https://jasp-stats.org/</a>
MATLAB 2020b	MATLAB	<a href="https://www.mathworks.com/products/new_products/release2021b.html">https://www.mathworks.com/products/new_products/release2021b.html</a>
<b><i>Other</i></b>		
Motor	Maxon Group	<a href="https://www.maxongroup.com/">https://www.maxongroup.com/</a>
Servo	Hitec	<a href="https://hitecrd.com/products/servos/analog/micromini/hs-81/product">https://hitecrd.com/products/servos/analog/micromini/hs-81/product</a>
Force sensor	Honeywell Inc	<a href="https://buildings.honeywell.com/us/en">https://buildings.honeywell.com/us/en</a>
Motion tracking device	Polhemus Liberty	<a href="https://polhemus.com/motion-tracking/all-trackers/liberty">https://polhemus.com/motion-tracking/all-trackers/liberty</a>
Distance sensor	Distance sensor	Ultrasonic Distance Sensor HC-SR04 5V Version
Arduino	Arduino DUE	<a href="https://store.arduino.cc/products/arduino-due">https://store.arduino.cc/products/arduino-due</a>

856

857 **RESOURCE AVAILABILITY**

858 **Lead contact**

859 Further information and requests for resources should be directed to and will be fulfilled  
860 by the lead contact, Konstantina Kilteni (konstantina.kilteni@ki.se).

861 **Materials availability**

862 This study did not generate new unique material.

863 **Data and code availability**

864 All data (PSEs and JNDs) have been deposited at Open Science Framework and are  
865 publicly available as of the date of publication. DOIs are listed in the key resources table.

866 This paper does not report original code.  
867 Any additional information is available from the lead contact upon request.

## 868 **EXPERIMENTAL MODEL AND SUBJECT DETAILS**

### 869 **Participants**

870 Thirty naive adults participated in Experiment 1 (18 female, aged 18-36, 28 right-handed  
871 and 2 ambidextrous), thirty naive adults participated in Experiment 2 (17 female, aged  
872 20-37, 29 right-handed and 1 left-handed) and thirty naive adults participated in  
873 Experiment 3 (12 female, aged 21-40, 29 right-handed, 1 ambidextrous, 1 left-handed).  
874 Current or history of psychological or neurological conditions, as well as the use of any  
875 psychoactive drugs or medication to treat such conditions, were criteria for exclusion.  
876 The sample size of each Experiment was decided prior to data collection based on our  
877 previous studies using the same task (Kilteni et al., 2019; Kilteni & Ehrsson, 2022).  
878 Handedness was assessed using the Edinburgh Handedness Inventory (Oldfield, 1971).  
879 All experiments were approved by the Swedish Ethical Review Authority (registration  
880 no. 2021-03790) and participants were compensated for their time.

### 881 **Pre-registration of experiments**

882 The method and analysis plan for each experiment was pre-registered on the Open  
883 Science Framework (OSF) prior to data collection (Experiment 1 <https://osf.io/9jkqt>,  
884 Experiment 2 <https://osf.io/hs8au>, Experiment 3 <https://osf.io/gkwu7>).

### 885 **Modifications/additions to the pre-registered plan**

886 The only modification from the pre-registered plan was a reduction in the number of  
887 trials administered in Experiment 3. Following initial piloting, it was deemed appropriate  
888 to reduce the overall length of the task by including fewer trials (see *Methods Details*).  
889 Two additional ANOVAs were also conducted to compare the results across the three  
890 experiments (**Main Text**) and the kinematics across experiments (Supplementary  
891 Materials).

## 892 **METHODS DETAILS**

### 893 **Experimental setup**

894 Participants sat comfortably on a chair with their arms placed on a table. The left hand  
895 rested palm up, with the index finger placed on a molded support. On each trial, a motor  
896 (Maxon EC Motor EC 90 flat; Switzerland) delivered two forces (the *test* force and the  
897 *comparison* force) on the pulp of the left index finger through a cylindrical probe (25 mm  
898 height) with a flat aluminum surface (20 mm diameter) attached to a lever on the motor.  
899 A force sensor (FSG15N1A, Honeywell Inc.; diameter, 5 mm; minimum resolution, 0.01  
900 N; response time, 1 ms; measurement range, 0–15 N) within the probe recorded the  
901 forces applied on the left index finger. Following the presentation of the two forces,  
902 participants were asked to verbally report which of the two forces felt stronger – the first  
903 or the second. A second identical force sensor within an identical cylindrical probe

904 (“active force sensor”) was placed on top of, but not in contact with, the probe of the left  
905 index finger.

## 906 **Force-discrimination task**

907 Participants judged the intensity of a *test* force and a *comparison* force (100 ms duration  
908 each) separated by a random interval between 800ms and 1200ms in a two-alternative  
909 forced choice (2AFC) task. The intensity of the test force was 2 N, while the intensity of  
910 the comparison force was systematically varied among seven force levels (1, 1.5, 1.75, 2,  
911 2.25, 2.5 or 3 N). In all the conditions, the forces were delivered by the same motor, in  
912 order to precisely control their magnitude, however the source of the force was  
913 manipulated across conditions such that the force was triggered by the participants  
914 contact with a force sensor (*contact* condition), their finger movement (*no-contact*  
915 condition) or automatically by the stimulus computer (*baseline* condition).

## 916 **Experimental design and procedures**

### 917 Experiment 1

918 There were three conditions in Experiment 1 presented in three blocks separately: the  
919 *baseline* (i.e. externally generated touch) condition, the *contact* condition, and the *no-*  
920 *contact* condition.

921 In the *baseline* condition, participants did not move their limbs but passively received a  
922 *test* and the *comparison* force on the left index finger. This *baseline* condition was used  
923 to assess the participants’ somatosensory perception in the absence of any movement  
924 (Bays et al., 2005; Kiltner et al., 2019, 2020). Each trial began with an auditory cue (100  
925 ms duration, 997 Hz) followed by the *test* force delivered to the participants’ left index  
926 finger 800 ms after the cue by the motor. The *comparison* force was then delivered at a  
927 random interval between 800 ms and 1200 ms after the *test* force.

928 In the *contact* condition, participants started each trial by holding their right index finger  
929 approximately 10 cm above their left index finger. The start position was marked with a  
930 visual marker placed next to their right index finger while the final position was the probe  
931 of the active force sensor. The same auditory cue was presented as in the *baseline*  
932 condition, but participants now moved their right index finger downwards towards their  
933 left index finger and actively tapped on the active force sensor placed on top of, but not in  
934 contact with, the probe. The participant’s active tap on the force sensor triggered the  
935 motor to apply the *test* force on their left index finger (threshold 0.2 N). The tap of their  
936 right index finger triggered the test force on their left index finger with an intrinsic delay  
937 of 36 ms. The *comparison* force was then delivered at a random interval between 800ms  
938 and 1200ms after the *test* force.

939 In the *no-contact* condition, the participants started each trial by holding their right index  
940 finger 10 cm above their left index finger, identically to the *contact* condition. For this  
941 block, the active force sensor was removed and replaced by a distance sensor that  
942 detected the position of their right index finger. The distance sensor was placed on top of,

943 but not in contact with, the probe. Following the same auditory cue, participants moved  
944 their right index finger towards their left index finger. To restrict the participants' right  
945 index finger movement within similar movement ranges as in the *contact* condition and  
946 avoid contact with the distance sensor placed underneath, a second visual marker  
947 indicated the final position of the right index finger above the distance sensor (5 cm from  
948 the marker indicating the initial position). The distance sensor was connected to an  
949 Arduino microcontroller that controlled a servo motor. The servo motor and the force  
950 sensor were placed 2 meters away from the participants' hands and hidden from view.  
951 Once the distance sensor detected that the position of the right index finger became  
952 smaller than a preset threshold, it triggered the servo motor that hit the force sensor and  
953 triggered the *test* force. We accounted for the additional delay of the distance sensor by  
954 setting the position threshold for the distance sensor slightly higher than the lowest  
955 position the participants were asked to reach with their right index finger. Therefore, the  
956 test force would be delivered at a similar timing to the participants' right index finger  
957 endpoint between the *contact* and *no-contact* conditions. This position threshold was set  
958 based on significant pilot testing prior all experiments. Indeed, there was a minimal time  
959 difference between the two setups across experiments (17 ms average delay) with the *no-*  
960 *contact* condition leading, rather than lagging the *contact* one (see **Supplementary**  
961 **Materials**). The *comparison* force was delivered at a random interval between 800ms  
962 and 1200ms after the *test* force. Therefore, in the *no-contact* condition, there was no  
963 touch on the right index finger simultaneously with the *test* force on their left index  
964 finger.

965 Before the experiment, participants were trained to make similar movements with their  
966 right index finger in the *contact* and *no-contact* conditions, emphasis was placed on  
967 restricting their right index finger movements to between the two visual markers in the  
968 *no-contact* condition. The 3D position of the right index finger was recorded using a  
969 Polhemus Liberty tracker (240 Hz). Kinematic information was used to compare the  
970 movements between the *contact* and *no-contact* conditions and to reject any trials in  
971 which the participant did not trigger the test stimulus with their movement, or trials in  
972 which the participant did not move as instructed in the training (see below). Participants  
973 were administered white noise through headphones to mask any sounds made by the  
974 motor to serve as a cue for the task. The loudness of the white noise was adjusted such  
975 that participants could clearly hear the auditory tones of the trial.

976 Each block consisted of 70 trials resulting to 210 trials per participant. Thus, the  
977 proportion of *contact* and *no-contact* trials was the same (50-50%). The order of the  
978 conditions was fully counterbalanced across participants.

## 979 Experiment 2

980 The 2-AFC task was identical to that of Experiment 1. In Experiment 2, there were five  
981 conditions in total: the *baseline* condition, the *contact* condition, the *no-contact*  
982 condition, and two additional NOGO conditions (*NOGO contact* and *NOGO no-contact*).  
983 Trials of the NOGO conditions were pseudo-randomly intermixed with trials of the  
984 *contact* and *no-contact* conditions respectively (GO trials). The five conditions were

985 presented in three separate blocks: the *baseline*, *contact* (GO and NOGO trials) and *no-*  
986 *contact* (GO and NOGO trials) blocks.

987 In the *contact* block, 50% of trials began with an auditory “GO” cue (100 ms duration  
988 high tone of 2458 Hz) instructing participants to tap the active force sensor to trigger the  
989 *test* force (identically to the *contact* condition of Experiment 1). On the remaining 50% of  
990 trials an auditory “NOGO” cue (100ms duration low tone of 222 Hz) instructed  
991 participants to withhold their movement and the *test* force was then delivered 800ms  
992 following the NOGO cue. The *no-contact* block was identical to the *contact* block, except  
993 that the *test* force was triggered by the position of the right index finger without contact  
994 with the force sensor (identically to the *no-contact* condition of Experiment 1). The cue  
995 tone in the *baseline* block was the same as the cue tone in the NOGO trials (100 ms  
996 duration low tone of 222 Hz).

997 Therefore, this design replicated the experimental design of Thomas et al. (Thomas et al.,  
998 2021) with the additional inclusion of the *baseline* (i.e. externally generated touch)  
999 condition. As in Experiment 1, we recorded the 3D position of the right index finger and  
1000 the registered kinematic information was used to compare the movements between the  
1001 *contact* and *no-contact* conditions and reject any trials in which the participant did not  
1002 trigger the *test* stimulus with their movement, trials in which the participant did not move  
1003 as instructed in the training (see below), and trials in which the participants moved while  
1004 instructed not to do so by the auditory cues (NOGO trials). As in Experiment 1,  
1005 participants were administered white noise and the loudness of the white noise was  
1006 adjusted such that participants could clearly hear the GO and NOGO auditory cues of the  
1007 trial.

1008 The *baseline* block consisted of 70 trials, and the *contact* and *no-contact* blocks consisted  
1009 of 70 GO trials and 70 NOGO trials each, resulting to 350 trials in total per participant.  
1010 The order of the blocks was fully counterbalanced across participants.

### 1011 Experiment 3

1012 The 2-AFC task and the experimental conditions (*baseline*, *contact*, and *no-contact*) were  
1013 identical to those of Experiment 1, except for the following. *Contact* trials (80%) were  
1014 now pseudo-randomly intermixed with *no-contact* trials (20%) within the same block.  
1015 The force sensor was now attached to a plastic platform that could be automatically  
1016 retracted by a servo motor, depending on the trial type. Upon retraction, a distance sensor  
1017 placed underneath the platform was revealed. In the *contact* trials, participants tapped the  
1018 force sensor to trigger the *test* force identically to Experiments 1 and 2. In the *no-contact*  
1019 trials, the platform was automatically retracted before trial onset, unbeknownst to the  
1020 participant. This led participants to unexpectedly miss the active force sensor and instead  
1021 trigger the *test* force only by the position of their right index finger. In all conditions, the  
1022 participants’ vision was occluded, and white noise was administered via headphones to  
1023 prevent any visual or auditory cues indicating that the force sensor had been retracted in  
1024 *no-contact* trials. The *baseline* block was identical to that of Experiments 1 and 2.

1025 In Experiment 3, the number of trials was reduced from 70 to 56 to shorten the total  
1026 experiment time to less than 90 minutes, similar in the Experiment 2. Thus, there were 56  
1027 *no-contact* trials (20%) and 224 contact trials (80%). Similarly, there were 56 trials in the  
1028 *baseline* condition. This resulted to 336 trials per participant. The order of the two blocks  
1029 was fully counterbalanced across participants.

## 1030 **QUANTIFICATION AND STATISTICAL ANALYSIS**

### 1031 **Preprocessing of psychophysical trials.**

#### 1032 Experiment 1

1033 Experiment 1 included 6300 trials in total (30 participants \* 70 trials \* 3 conditions).  
1034 Twenty-nine (29) trials were excluded (0.5%) because of 1 missing response, 4 trials in  
1035 which the force was not applied correctly ( $1.85 \text{ N} < \textit{test force} < 2.15 \text{ N}$ ), and 24 trials  
1036 because the *test* force was not triggered when moving towards the distance sensor. All  
1037 trials excluded by the psychophysical fits were also excluded in the kinematic analysis.

#### 1038 Experiment 2

1039 Experiment 2 included 10500 trials in total (30 participants \* 70 trials \* 5 conditions).  
1040 One-hundred fourteen (114) trials were excluded (1.1%) because of 2 missing responses,  
1041 6 trials in which the force was not applied correctly ( $1.85 \text{ N} < \textit{test force} < 2.15 \text{ N}$ ), 44  
1042 trials because the *test* force was not triggered when moving towards the distance sensor  
1043 and 62 trials because the finger moved on a NOGO trial. All trials excluded by the  
1044 psychophysical fits were also excluded in the kinematic analysis.

#### 1045 Experiment 3

1046 Experiment 3 included 10080 trials in total (30 participants \* 224 contact trials + 56 no-  
1047 contact trials + 56 baseline trials). Two-hundred twenty-four (29) trials were excluded  
1048 (2.42%) because of 29 missing responses, 86 trials in which the force was not applied  
1049 correctly ( $1.85 \text{ N} < \textit{test force} < 2.15 \text{ N}$ ), 81 because the test force was not triggered when  
1050 moving towards the distance sensor and 48 because the finger contacted the distance  
1051 sensor on *no-contact* trials. All trials excluded by the psychophysical fits were also  
1052 excluded in the kinematic analysis.

### 1053 **Preprocessing of kinematic recordings.**

1054 All kinematic trials were co-registered with the force trials through Transistor-Transistor  
1055 Logic (TTL) signals sent by the motor to both file outputs. The kinematic recordings  
1056 were corrected for any distortion in the Polhemus sensor from the force sensor and  
1057 distance sensor based on measurements made with and without the force/distance sensors  
1058 within the same space. Exclusion of trials based on the kinematics was done by assessing  
1059 whether the test force was delivered after the position of the active finger reached its  
1060 minimum value on the vertical plane. Trials in which the force was delivered after the  
1061 minimum value had been reached were rejected. For experiment 2, trials in which the  
1062 active finger moved more than 1 cm following a NOGO cue were also rejected.



## 1063 **Fitting of psychophysical responses**

1064 For each experiment and each condition, the participants' responses were fitted with a  
1065 generalized linear model using a *logit* link function (Equation 1):

$$1066 \quad p = \frac{e^{\beta_0 + \beta_1 x}}{1 + e^{\beta_0 + \beta_1 x}} \text{ (Equation 1)}$$

1067

1068 We extracted two parameters of interest: the Point of Subjective Equality (PSE) ( $PSE =$   
1069  $-\frac{\beta_0}{\beta_1}$ ), which represents the intensity at which the *test* force felt as strong as the  
1070 *comparison* force ( $p = 0.5$ ) and quantifies the perceived intensity, and the JND ( $JND =$   
1071  $\frac{\log(3)}{\beta_1}$ ), which reflects the participants' discrimination ability. Before fitting the  
1072 responses, the values of the applied comparison *forces* were binned to the closest value  
1073 with respect to their theoretical values (1, 1.5, 1.75, 2, 2.25, 2.5 or 3 N).

1074 For all participants and all conditions, the fitted logistic models were very good, with  
1075 McFadden's R squared measures ranging between 0.735 and 1.000.

## 1076 **Normality of data and statistical comparisons.**

1077 We used R (R Core Team, 2022), JASP (JASP Team, 2022) and MATLAB (2020b) to  
1078 analyze our data. The normality of the PSE and the JND data distributions, as well as the  
1079 kinematic information data distributions were assessed using Shapiro-Wilk tests.  
1080 Depending on the data normality, pairwise comparisons between conditions were  
1081 performed by using either a paired t-test or a Wilcoxon signed-rank test. We report 95%  
1082 confidence intervals ( $CI^{95}$ ) for each statistical test. Effect sizes are reported as the  
1083 Cohen's *d* for t-tests or the matched rank biserial correlation *rrb* for the Wilcoxon signed-  
1084 rank tests. In addition, a Bayesian factor analysis using default Cauchy priors with a scale  
1085 of 0.707 was performed for all statistical tests that led to not statistically significant  
1086 effects, to provide information about the level of support for the null hypothesis  
1087 compared to the alternative hypothesis ( $BF_{01}$ ) based on the data. We interpret a factor  
1088 between 1/3 and 3 as "anecdotal evidence" (Quintana & Williams, 2018; van Doorn et al.,  
1089 2021), indicating that support for either the preferred or null hypotheses is insufficient.  
1090 For the Analysis of Variance (ANOVA, see **Supplementary Material**), homogeneity of  
1091 variance was assessed using Levene's test for Equality of Variances, which did not reach  
1092 significance, and the Q-Q plot of the standardized residuals indicated approximately  
1093 normally distributed residuals. Post-hoc tests were made using Bonferroni corrections.  
1094 All tests were two-tailed.

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- 1407



## 1408 SUPPLEMENTARY MATERIAL

### 1409 **Just Noticeable Difference (JND) analysis**

1410 From the psychophysical fits, we extracted the just noticeable difference (JND), which  
1411 represents the participants' force discrimination capacity between conditions. In  
1412 Experiment 1, the JNDs did not significantly differ between any of the conditions (all  $p$   
1413 values  $> 0.05$ ). In Experiment 2, the JNDs were not significantly different between  
1414 conditions ( $p$  values  $> 0.05$ ), except in the *contact* condition, where the JNDs were  
1415 significantly higher than in the *baseline* condition ( $t(29) = -2.52$ ,  $p = 0.017$ ,  $d = -0.46$ ,  
1416  $CI^{95} = [-0.06 -0.01]$ ,  $BF_{01} = 0.355$ ). Finally, in Experiment 3, the JNDs were significantly  
1417 lower in the *baseline* condition than in the *contact* condition ( $t(29) = -3.61$ ,  $p < .001$ ,  $d = -$   
1418  $0.66$ ,  $CI^{95} = [-0.09 -0.02]$ ,  $BF_{01} = 0.034$ ) and the *no-contact* condition ( $t(29) = -2.77$ ,  $p =$   
1419  $0.010$ ,  $d = -0.51$ ,  $CI^{95} = [-0.08 -0.01]$ ,  $BF_{01} = .213$ ), but there were no significant  
1420 differences in the JNDs between the *contact* and *no-contact* conditions ( $t(29) = -0.65$ ,  $p =$   
1421  $0.521$ ,  $d = -0.12$ ,  $CI^{95} = [-0.04 0.02]$ ,  $BF_{01} = 4.233$ ). Thus, in contrast to the PSEs, there  
1422 were no significant differences in the JNDs between the *contact* and *no-contact*  
1423 conditions in any of the three experiments, demonstrating that the two conditions yielded  
1424 the same discrimination capacity.

### 1425 **Kinematic analysis**

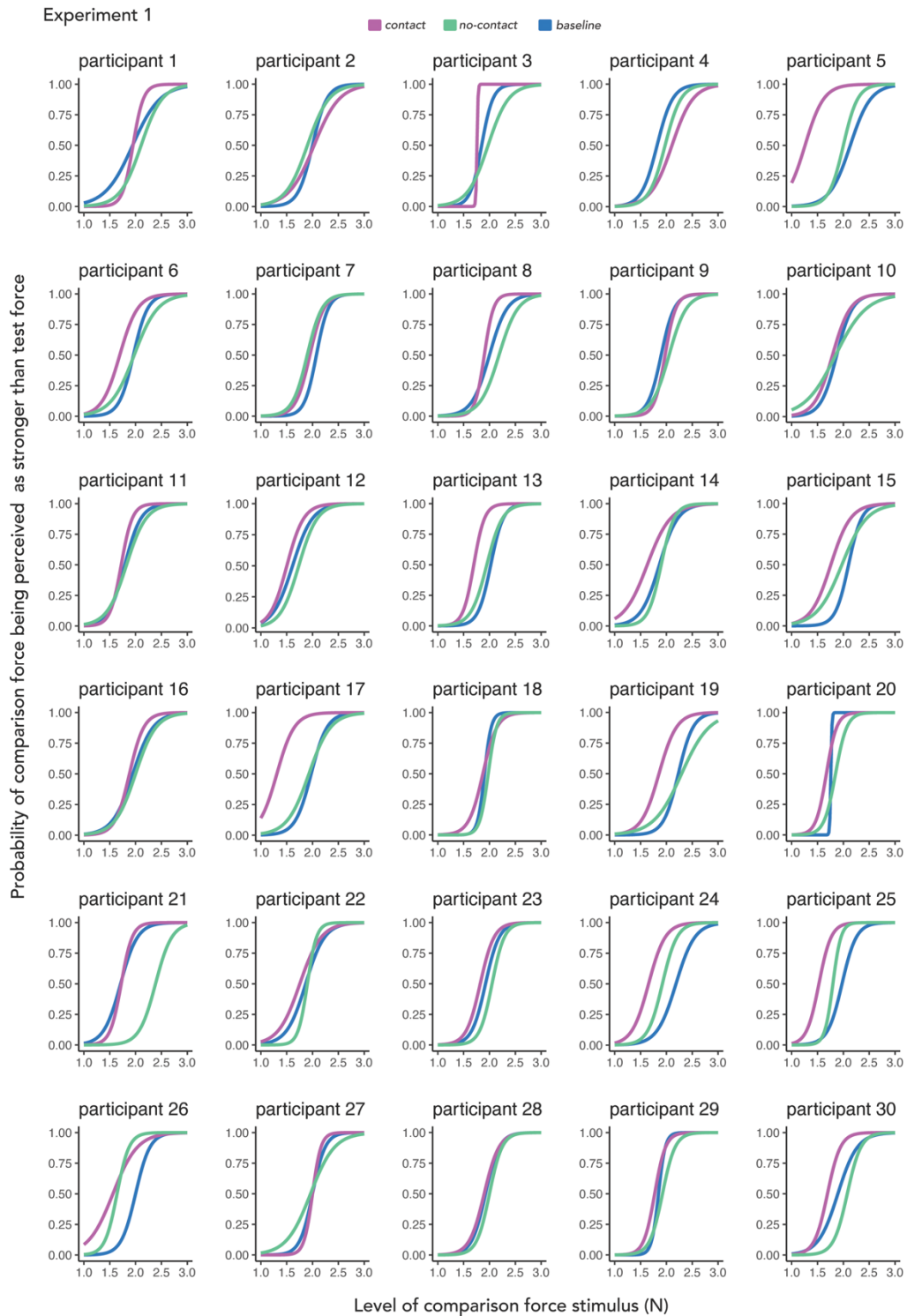
1426 To ensure that the movements in both the *contact* and *no-contact* conditions were  
1427 comparable, participants were trained to make the same movement with their right index  
1428 finger between two visual markers positioned 5 cm apart in Experiments 1 and 2. This  
1429 training was not required for Experiment 3, in which participants were blindfolded and  
1430 unaware that the distance sensor had been retracted on *no-contact* trials.

1431 Given that the right index finger movement ends on impact with the force sensor in the  
1432 *contact* condition but not in the *no-contact* condition, the kinematics of the finger  
1433 movements are likely to differ between conditions. The active finger was slightly closer  
1434 to the passive finger at the time of the *test* force in the *contact* compared to the *no-contact*  
1435 condition in Experiments 1 and 2 (by less than 5 mm). Specifically, in Experiment 1, the  
1436 position of the right index finger at the time of the *test* force was marginally closer to the  
1437 left index finger in the *contact* condition than in the *no-contact* condition (mean  
1438 difference = 2.32 mm, s.e.m. = 1.14:  $t(29) = -2.04$ ,  $p = 0.051$ ,  $d = 0.37$ ,  $CI^{95} = [-0.74$   
1439  $0.01]$ ,  $BF_{01} = 0.845$ ). In Experiment 2, the position of the right index finger at the time of  
1440 the *test* force was slightly closer to the left index finger in the *contact* condition than in  
1441 the *no-contact* condition (mean difference = 4 mm, s.e.m. = 1.8:  $t(29) = -2.29$ ,  $p = 0.030$ ,  
1442  $d = 0.42$ ,  $CI^{95} = [-0.79 -0.04]$ ,  $BF_{01} = 0.550$ ). In Experiment 3, participants were unaware  
1443 that they would miss the force sensor in the *no-contact* trials, so with no force sensor to  
1444 stop the movement, their right index finger continued further downwards. Here, the  
1445 position of the right index finger at the time of the *test* force was closer to the left index  
1446 finger in the *no-contact* condition than in the *contact* condition (mean difference = 25.7  
1447 mm, s.e.m. = 2.0:  $t(29) = 12.79$ ,  $p < .001$ ,  $d = 2.34$ ,  $CI^{95} = [1.63 3.03]$ ,  $BF_{01} < 0.001$ .  
1448 Critically, the closer position of the right index finger to the left index finger in the *no-*  
1449 *contact* trials compared to the *contact* trials cannot explain the attenuation findings in the

1450 *no-contact* condition since the attenuation in the *contact* trials was actually stronger  
1451 compared to that in the *no-contact* trials (**Main Text**).

1452 It could be argued that our differences between the *contact* and *no-contact* conditions  
1453 across experiments are driven by differences in the timing of the two setups. This  
1454 explanation is unlikely since we observed robust attenuation in the *no-contact* condition  
1455 of Experiment 3 but not in Experiments 1 and 2 while the setups remained the same. To  
1456 further control that the attenuation observed in the *no-contact* condition of Experiment 3  
1457 but not in the *no-contact* conditions of Experiments 1 and 2 was not driven by timing  
1458 differences in the participants' movement between experiments, we calculated the time  
1459 the *test* force was delivered in the *contact* and *no-contact* conditions with respect to their  
1460 movement end point (*i.e.*, the force sensor press in the *contact* condition and the lowest  
1461 vertical position in the *no-contact* condition). On average, the *test* force was applied 24  
1462 ms earlier in the *no-contact* compared to the *contact* condition in Experiment 1 (s.e.m. =  
1463 4.20), 11 ms earlier in the *no-contact* compared to the *contact* condition in Experiment 2  
1464 (s.e.m. = 4.53) and 15 ms earlier in the *no-contact* compared to the *contact* condition in  
1465 Experiment 3 (s.e.m. = 2.67). An ANOVA revealed a significant main effect of  
1466 Experiment ( $F(2, 87) = 3.32, p = 0.041, \eta^2 = 0.071$ ), with Bonferroni corrected post hoc  
1467 comparisons indicating significant differences between Experiment 1 and Experiment 2  
1468 ( $t(2, 87) = -2.50, p = 0.043, d = 0.65, CI [0.62\ 26.83], BF_{01} = 0.500$ ). Importantly, there  
1469 were no significant differences between neither Experiments 1 and 3 ( $t(2, 87) = -1.80, p =$   
1470  $0.226, d = 0.47, CI [-3.21\ 22.99], BF_{01} = 0.744$ ), nor Experiments 2 and 3 ( $t(2, 87) = -$   
1471  $0.69, p = 1.000, d = -0.18, CI [-16.93\ 9.27], BF_{01} = 3.051$ ) demonstrating that the  
1472 attenuation observed in Experiment 3 cannot be attributed to time differences between the  
1473 participants' movement and the received touch.

1474 **Supplemental Figure S1**



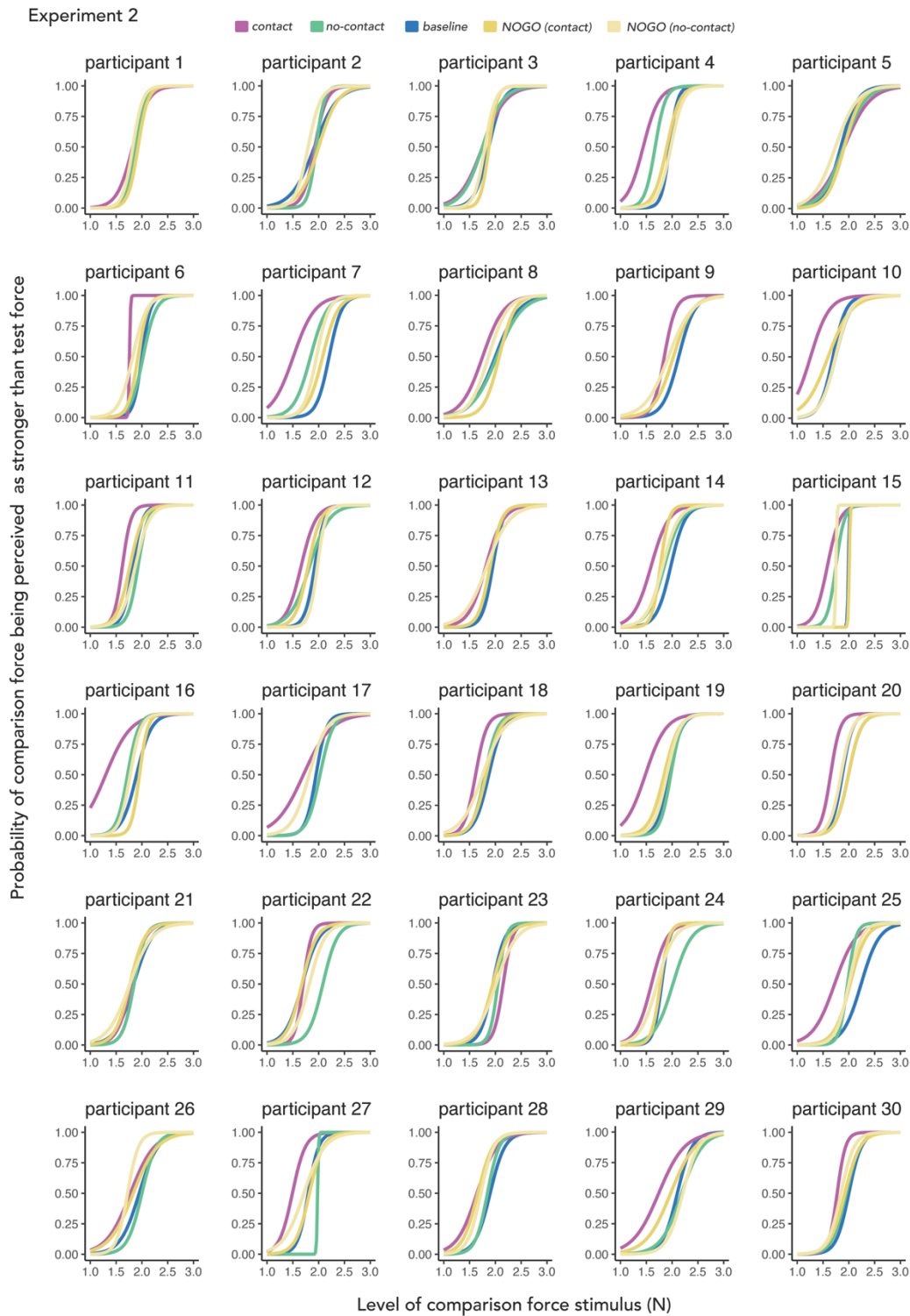
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**Figure S1. Fitted logistic models based on the participants' responses under each condition of Experiment 1.**

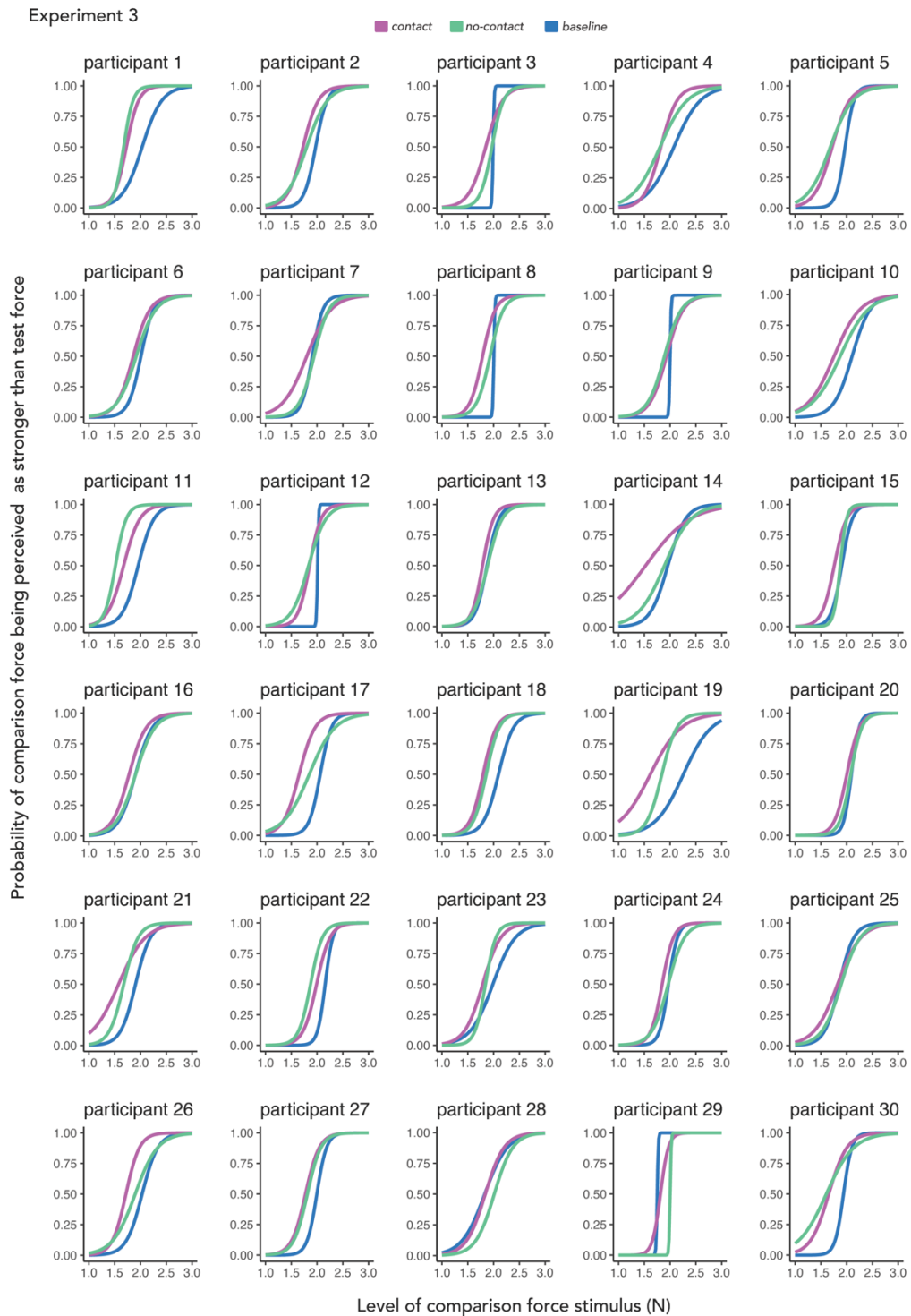
1478 **Supplemental Figure S2**



1479

1480 **Figure S2. Fitted logistic models based on the participants' responses under each condition**  
1481 **of Experiment 2.**

1482 **Supplemental Figure S3**



1483

1484 **Figure S3. Fitted logistic models based on the participants' responses under each condition**  
1485 **of Experiment 3.**