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Active information sampling varies across the cardiac cycle

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25 **Abstract**

26 Perception and cognition oscillate with fluctuating bodily states. For example, visual pro-
27 cessing has been shown to change with alternating cardiac phases. Here, we study the
28 heartbeat's role for active information sampling—testing whether humans implicitly act upon
29 their environment so that relevant signals appear during preferred cardiac phases.

30 During the encoding period of a visual memory experiment, participants clicked
31 through a set of emotional pictures to memorize them for a later recognition test. By self-
32 paced key press, they actively prompted the onset of shortly (100-ms) presented pictures.
33 Simultaneously recorded electrocardiograms allowed us to analyse the self-initiated picture
34 onsets relative to the heartbeat. We find that self-initiated picture onsets vary across the car-
35 diac cycle, showing an increase during cardiac systole, while memory performance was not
36 affected by the heartbeat. We conclude that active information sampling integrates heart-
37 related signals, thereby extending previous findings on the association between body-brain
38 interactions and behaviour.

39 **Introduction**

40 We perceive and act upon the world while our brain continuously integrates exteroceptive
41 and interoceptive information, that is, information received from external (e.g., through vision
42 and touch) and internal sources (e.g., through viscerosensation and proprioception), respec-
43 tively (Barrett & Simmons, 2015; Kleckner et al., 2017). Through the fine-tuned interplay of
44 brain and body, we are able to react to changes in the external and the internal environment
45 to maintain or restore our bodily integrity and well-being. Via feedback loops, the brain there-
46 by receives afferent information about bodily states to regulate and adjust bodily activity ac-
47 cordingly (Craig, 2002; Critchley & Harrison, 2013; Mayer, 2011; Saper, 2002). To fully cap-
48 ture the bi-directionality of brain-body interactions and their association with mental process-
49 es, it is essential to investigate if and how such afferent bodily information modulates our
50 thoughts, feelings, and behaviour.

51 One approach to study bodily influences on cognition and behaviour exploits natural
52 physiological fluctuations. Such fluctuations occur at multiple time scales—ranging from milli-
53 seconds to weeks (e.g., brain oscillations, heartbeats, the circadian rhythm, or the menstrual
54 cycle)—and they dynamically interact with each other as well as with the environment (Glass,
55 2001). How such natural physiological variability is processed in the brain remains poorly
56 understood. However, it has been shown that brain and beyond-brain organ systems (e.g.,
57 the cardiorespiratory or the gastrointestinal system) co-vary in their oscillatory activity (Fan et
58 al., 2012; Luft & Bhattacharya, 2015; Richter, Babo-Rebelo, Schwartz, & Tallon-Baudry,
59 2017; Thayer, Åhs, Fredrikson, Sollers, & Wager, 2012).

60 Particularly the heart, as a fundamental internal oscillator, has been the target of a
61 growing body of research that investigates how cardiac fluctuations are integrated with the
62 processing of external stimuli (Critchley & Garfinkel, 2018). Cardiac activity occurs in a cycle
63 of two phases: During diastole, the ventricles relax to be filled with blood; during systole, the
64 ventricles contract and eject blood into the arteries, while visceral pathways send information
65 about each heartbeat to the brain (Critchley & Harrison, 2013). Such natural phasic changes
66 of the cardiovascular state have been mainly associated with variations in perception: For

67 sensory processing, which is typically measured with detection tasks or reaction time tasks,
68 response to passively presented stimuli has been shown to be attenuated during early cardi-
69 ac phases (i.e., during systole) or relatively enhanced at later time points in the cardiac cycle
70 (i.e., at diastole) (Birren, Cardon, & Phillips, 1963; Callaway & Layne, 1964; Edwards, Ring,
71 McIntyre, Carroll, & Martin, 2007; Lacey & Lacey, 1974; McIntyre, Ring, Edwards, & Carroll,
72 2008; Réquin & Brouchon, 1964; Saari & Pappas, 1976; Sandman, McCanne, Kaiser, &
73 Diamond, 1977; Wilkinson, McIntyre, & Edwards, 2013).

74 A growing number of more recent findings, however, suggests *facilitated* processing
75 during systole, specifically for task- or context-relevant stimuli. While enhanced processing
76 during systole was also reported for non-emotional visual stimuli (Pramme, Larra,
77 Schächinger, & Frings, 2014, 2016), an emotional specificity of this effect was observed
78 when testing neutral stimuli vs. valenced stimuli like emotional faces—particularly for emo-
79 tionally arousing fear or threat stimuli (Azevedo, Badoud, & Tsakiris, 2018; Azevedo,
80 Garfinkel, Critchley, & Tsakiris, 2017; Garfinkel et al., 2014). Thus pointing towards an in-
81 crease in emotional salience through interoceptive channels (Critchley & Harrison, 2013),
82 these findings correspond with evidence for preferential stimulus processing (e.g., enhanced
83 perception and memory) fostered by states of general psychophysiological arousal (Cahill &
84 McGaugh, 1998; Mather, Clewett, Sakaki, & Harley, 2016; Mather & Sutherland, 2011;
85 McGaugh, 2015; Tambini, Rimmele, Phelps, & Davachi, 2017). At the same time, phasic
86 cardiac modulation of stimulus processing has been associated with altered memory for-
87 mation and retrieval (Fiacconi, Peter, Owais, & Köhler, 2016; Garfinkel et al., 2013)—also in
88 the context of respiratory oscillations (Zelano et al., 2016). Taken together, sensory pro-
89 cessing is differentially modulated during early cardiac phases, indicating a selective pro-
90 cessing benefit for relevant (e.g., emotionally arousing) stimuli, while other perceptual pro-
91 cesses are attenuated (Garfinkel & Critchley, 2016). This suggests that cardiac (or cardio-
92 respiratory) fluctuations not only are an important target of efferent arousal regulation but
93 contribute to afferent signalling of bodily arousal states to the brain (Critchley & Harrison,
94 2013).

95 However, these studies investigating cardiac influences on perception and cognition
96 have only employed passive stimulus presentation, which ignores *self-initiated action* as a
97 crucial dimension of sensory and particularly visual processing. Mediating our engagement
98 with a visual scene, motor actions dynamically orchestrate incoming sensory data and thus
99 strongly influence visual perception—selecting what information is preferentially processed
100 (Benedetto, Spinelli, & Morrone, 2016; Tomassini, Spinelli, Jacono, Sandini, & Morrone,
101 2015). Sensorimotor coupling has also been linked to periodic attentional fluctuations
102 (Hogendoorn, 2016; Morillon, Schroeder, & Wyart, 2014). For example in the visual domain,
103 saccadic eye movements are preceded by a shift of attention to the saccade target resulting
104 in strongly improved visual performance (Deubel & Schneider, 1996; Kowler, Anderson,
105 Doshier, & Blaser, 1995; Li, Barbot, & Carrasco, 2016; Ohl, Kuper, & Rolfs, 2017) and
106 memory performance at the saccade target location (Hanning, Jonikaitis, Deubel, & Szinte,
107 2016; Ohl & Rolfs, 2017) with corresponding neural enhancement in early visual cortex
108 (Merrikhi et al., 2017; Moore, Tolia, & Schiller, 1998). There is sparse evidence that con-
109 nects the heartbeat to general action generation and the few studies that investigated if
110 movements are modulated across the cardiac cycle indicate that systole provides a facilitat-
111 ing time window for spontaneous motor activity—both in the somatomotor (Mets, Konttinen,
112 & Lyytinen, 2007) as well as in the oculomotor domain (Ohl, Wohltat, Kliegl, Pollatos, &
113 Engbert, 2016).

114 Based on findings of facilitated processing for visual stimuli (Azevedo et al., 2018,
115 2017; Garfinkel et al., 2014; Pramme et al., 2014, 2016) and increased oculomotor activity
116 (Ohl et al., 2016) during early phases of the cardiac cycle, we here hypothesized that active
117 information sampling (i.e., self-initiated action towards a visual stimulus) shows periodic vari-
118 ations with the phase of our heartbeat. To investigate perception and action within a compre-
119 hensive framework of mind-brain-body interactions, we here studied cardiac-related sen-
120 sorimotor processing in a self-paced visual sampling paradigm, in which participants decide
121 when to press a key to see a task-relevant visual stimulus. Extending studies that emphasize
122 a selectivity of this effect for motivationally salient, passively presented stimuli (Azevedo et

123 al., 2018, 2017; Garfinkel et al., 2014), we predicted that observers implicitly act upon a rele-
124 vant visual stimulus such that it is received (and perceived) during preferred cardiac phases.
125 More specifically, we hypothesized that visual sampling would be biased towards processing
126 task-relevant pictures during systole.

127 We assessed the emotional specificity of cardiac-phase effects (Garfinkel et al., 2014;
128 Garfinkel & Critchley, 2016) by presenting negative, positive, and neutral pictures (cf. **Meth-**
129 **ods**). To further induce stimulus relevance, participants were instructed to memorize the pic-
130 tures during sampling and their recognition memory was tested after a delay of several
131 minutes. This enabled us to also address the previously reported link between memory per-
132 formance and the cardiac cycle: Based on the abovementioned systolic modulation of
133 memory formation (Garfinkel et al., 2013), we expected recognition performance to be modu-
134 lated by the cardiac timing of memory probes during encoding. Specifically, we hypothesized
135 that memory performance for pictures encoded at different time points of the cardiac cycle is
136 not equally distributed, but varies across the cardiac cycle.

137

138 **Methods**

139 **Preregistration.** The protocol and the hypotheses of our study were pre-registered prior to
140 the data acquisition using the Open Science Framework (<https://osf.io/5z8rx/>).

141 **Participants.** 47 (23 female) healthy, young, right-handed subjects (age: 18 – 34 years, $M =$
142 25.8 years, $SD = 4.31$) with normal or corrected-to-normal vision participated in this study.
143 Four subjects were excluded due to deviant cardiovascular parameters: two subjects with
144 tachycardic mean resting heart rates (> 100 bpm), parallel to previous studies (Edwards,
145 McIntyre, Carroll, Ring, & Martin, 2002; Garfinkel et al., 2014; Wilkinson et al., 2013); one
146 subject with hypertonic blood pressure (171/89 mmHg), based on Tukey's (1977) criterion of
147 1.5 times the interquartile range (IQR) above the third quartile ($Q3 = 122$ mmHg, $IQR = 20.5$
148 mmHg); one subject with numerous ventricular extrasystoles during the experimental period
149 (> 10 per minute). The sample size was based on previous cardiac cycle studies (mainly
150 Fiacconi et al., 2016): We aimed for a net sample size of 40 to enter the analyses (cf.

151 <https://osf.io/5z8rx/>) expecting 10% participant exclusions. Participants were recruited
152 through the ORSEE-based (Greiner, 2015) participant database of the Berlin School of Mind
153 and Brain and received a monetary compensation of 9 €/h for their participation. All partici-
154 pants were naïve regarding the purpose of the study and signed informed consent before
155 participation. The study followed the Declaration of Helsinki and was approved by the Ethics
156 Committee of the Department of Psychology at the Humboldt-Universität zu Berlin.

157 **Setup and experimental task.** (cf. **Fig. 1a**) Participants were seated in a dimly lit room in
158 front of a gamma-linearized 19-inch Cathode ray tube (CRT) monitor (Samsung Syncmaster
159 959NF, Suwong, Korea) with a refresh rate of 100 Hz and a spatial resolution of 1280x1024
160 pixels. Their head was positioned on a chin rest at a distance of 50 cm from the screen. The
161 participants' task comprised two parts: During the *encoding* period, participants were asked
162 to click through a picture set (800x600 pixels) in self-paced speed and to memorize the pic-
163 tures for a subsequent memory test. By button press, they prompted the immediate onset of
164 the next picture, which appeared for 100 ms. In between self-chosen key presses (i.e., pic-
165 ture onsets), a central fixation cross was presented. After a break of five minutes, they com-
166 pleted the *recognition* period, during which they indicated for each picture whether or not
167 they had seen it before. Here, pictures were passively presented for 100 ms, followed by a
168 centrally presented fixation cross until participants entered their recognition response ("old",
169 "new") via key press.

170 **Stimuli.** The picture set consisted of 180 coloured photographs (60 pictures with positive, 60
171 with negative, and 60 with neutral content) of humans in various life situations, selected from
172 a collection of standardized and validated affective picture material (EmoPicS) (Wessa et al.,
173 2010). For the index numbers of the selected photographs cf. **Table S1 (Supplementary**
174 **Methods)**. To correct for potential stimulus-intrinsic influences on visual processing, the
175 three picture sets were largely matched for physical image statistics (Wessa et al., 2010):
176 Contrast and visual complexity did not differ (all $p > .21$); positive images had significantly
177 higher luminance values than negative images ($t(118) = 3.75$, $p < .001$, Cohen's $d = 0.68$),
178 while both did not differ from neutral images. In addition, two independent observers

179 matched the three sets for more high-level stimulus features: (1) number of people shown,
180 (2) number of images with social interactions, (3) number of images with close-ups, (4) num-
181 ber of images showing eye contact with the observer. Notably, positive and negative images
182 were matched for (normative) arousal ratings and did not significantly differ ($t(78.6) = 1.20$, p
183 $= .23$, Cohen's $d = 0.22$). Stimuli were displayed using MATLAB version 7.8.0.347 (The
184 MathWorks Inc., Natick, MA, USA) with the Psychophysics Toolbox 3 (Brainard, 1997;
185 Kleiner et al., 2007; Pelli, 1997).

186 For each participant, stimuli were randomly selected and presented in randomized
187 order: For encoding, a subset of 120 pictures with 40 pictures of each picture valence (posi-
188 tive, neutral, negative) was sampled from the whole set of 180. The second picture set,
189 shown during the recognition period, consisted of the 60 yet unused pictures (20 per picture
190 valence)—serving as distractors—as well as 60 memory probes (20 per picture valence) that
191 were sampled from the encoded picture set.

192 **ECG recording.** ECG was recorded at 2048 Hz using an ActiveTwo AD amplifier (Biosemi,
193 Amsterdam, Netherlands). Three electrodes were attached according to an adapted limb
194 lead configuration at the right and left lower coastal arch as well as the left medial ankle. Par-
195 ticipants were told that the ECG is to measure their general bodily state without mentioning
196 details regarding the experimental conditions (Fiacconi et al., 2016). The ECG lead most
197 clearly displaying the onset of ventricular depolarisation (lead II) was used for analysis.

198 **Additional measures of inter-individual differences.** Previous studies suggest that the
199 influence of cardiac signals on perception and behaviour varies with interoceptive accuracy,
200 that is, the ability to consciously perceive signals originating in the body (Dunn et al., 2010;
201 Garfinkel et al., 2013). We determined inter-individual differences in interoceptive accuracy
202 with a heartbeat perception task (Schandry, 1981), in which participants were asked to esti-
203 mate the number of their heartbeats in five intervals of different length (25, 45, 15, 55, and 35
204 s). As inter-individual differences in anxiety have been proposed to moderate the behavioural
205 effect of autonomic signalling (Garfinkel et al., 2014; Pollatos, Schandry, Auer, & Kaufmann,
206 2007), we also acquired participants' trait anxiety using the State-Trait Anxiety Inventory

207 (STAI-T; Laux, Glanzmann, Schaffner, & Spielberger, 1981; Spielberger, Gorsuch, Lushene,
208 Vagg, & Jacobs, 1983). Resting heart rate variability (HRV) measures inter-individual differ-
209 ences in brain-heart interaction and particularly in parasympathetic cardioregulation (Task
210 Force, 1996). HRV can be quantified through changes in the beat-to-beat intervals of the
211 ECG (Task Force, 1996). We calculated the root mean square of successive differences
212 (rMSSD) during the 7-minute baseline ECG.

213 **Procedure.** Upon arrival in the lab, participants were equipped with the ECG. Comfortably
214 seated, they were asked to relax for seven minutes and breathe normally. Then, blood pres-
215 sure was measured (twice, if elevated) using a standard sphygmomanometer (OMRON M8
216 Comfort). After a brief training session to familiarize participants with the task, they per-
217 formed the two experimental periods (i.e., encoding and recognition). During a 5-minute
218 break between the two parts, participants completed the Trait Anxiety Inventory (STAI-T)
219 (Laux et al., 1981; Spielberger et al., 1983). To assess subjective perception in our sample
220 and compare it to the EmoPicS' normative ratings, all 180 photos were rated after the recog-
221 nition period similarly to the original EmoPicS normative ratings (Wessa et al., 2010): "How
222 do you feel looking at the picture?" was answered for valence (1: sad – 9: happy) and arous-
223 al (1: calm – 9: excited) on a 9-level Likert-type scale. For each trial, both rating scales were
224 displayed successively, one above and one below each picture, followed by a 500-ms fixa-
225 tion cross (between trials). Finally, subjects performed the heartbeat perception task
226 (Schandry, 1981) that was presented acoustically.

227 **Data analysis.** The timing of behavioural responses was analysed relative to the heartbeats:
228 electrical events indicating the beginning of each cardiac cycle (R peaks) were extracted
229 from the ECG signal with Kubios 2.2 (Tarvainen, Niskanen, Lipponen, Ranta-aho, &
230 Karjalainen, 2014, <http://kubios.uef.fi/>). Two complementary analytic approaches—circular
231 and binary analysis—were performed to exploit the oscillatory (repeating cycle of cardiac
232 events) as well as the phasic (two distinct cardiac phases: systole and diastole) nature of
233 cardiac activity, respectively.

234 **Encoding period—cardiac modulation of self-paced visual sampling.**

235 *Circular analysis:* For the circular analysis, we computed the relative onset of each key press
236 (prompting picture onset) within the cardiac cycle, which was indicated in the ECG as the
237 interval between the previous and the following R peak (**Fig. 1b**). According to its relative
238 timing within this R-R interval, radian values between 0 and 2π were assigned to each stimu-
239 lus (Ohl et al., 2016; Pikovsky, Rosenblum, & Kurths, 2001; Schäfer, Rosenblum, Kurths, &
240 Abel, 1998). For each participant, we computed the mean of the circular distribution for the
241 120 picture onsets. In a second step, a mean vector of all participants was computed via
242 vector addition of individual means divided by their number, showing the average self-paced
243 picture onset in the cardiac cycle across the group, and weighted by its length (mean result-
244 ant length ρ) to reflect the spread of individual means around the circle. As a measure of
245 concentration of circular data, ρ was integrated in a subsequent Rayleigh test for uniformity
246 (Pewsey, Neuhäuser, & Ruxton, 2013): if ρ gets sufficiently high to exceed a threshold value
247 (i.e., the set of individual means is not spread evenly across the cardiac cycle), the data can
248 be interpreted as too locally clustered to be consistent with a uniform distribution that served
249 as null hypothesis (Pewsey et al., 2013). The code for individual and group-level circular
250 analysis can be found on GitHub (https://github.com/SKunzendorf/0303_INCAS1). Confi-
251 dence intervals and significance were non-parametrically calculated through bootstrapping
252 based on analyses from a previous study (Ohl et al., 2016): From the original pool of 43 par-
253 ticipants, we drew a random bootstrap sample of 43 participants with replacement. For each
254 participant in the bootstrap sample, we first computed a circular density (bandwidth = 20) of
255 picture onsets, and then computed the mean circular density across the 43 participants in the
256 bootstrap sample. Confidence intervals (95%) were determined as 2.5% and 97.5% percen-
257 tiles from the distribution of mean circular densities obtained by repeating the bootstrap pro-
258 cedure 10000 times. Deviation from the circular uniform was considered as significant when
259 the 95% confidence interval determined by the bootstrapping is outside the circular density of
260 a uniform distribution.

261 *Binary analysis:* To account for the phasic nature of cardiac activity and to increase
262 comparability to previous cardiac cycle studies, we segmented the cardiac cycle into systole

263 and diastole (**Fig. 1b**). It needs to be noted that systolic phases vary inversely with heart rate
264 (Fridericia, 1920; Lewis, Rittogers, Froester, & Boudoulas, 1977; Lombard & Cope, 1926;
265 Wallace, Mitchell, Skinner, & Sarnoff, 1963; Weissler, Harris, & Schoenfield, 1968): Although
266 the absolute length of systole decreases with a faster heartbeat, its proportionate share of
267 the entire cardiac cycle increases. Between-subject variation of cardiac phase length (e.g.,
268 through differences in heart rate) supports the need to adapt analytical approaches in cardiac
269 cycle studies. With the ECG waveform as physiological reference of cardiac activity, we did
270 not use absolute systole and diastole lengths (e.g., defining systole as the 300 ms following
271 an R peak) but computed participant-specific cardiac phases. Cardiac modulation of percep-
272 tion and cognition has often been attributed to baroreceptor signalling (e.g., Garfinkel &
273 Critchley, 2016; Lacey & Lacey, 1974), which occurs in response to transient pressure rises
274 (i.e., with the systolic upstroke) at each blood ejection (Angell James, 1971). In our ap-
275 proach, phases of high baroafferent feedback were approximated by determining each par-
276 ticipant's systolic ejection phase (in the following referred to as "systole"). For the detailed
277 binning procedure, the time ranges of individualized cardiac phases, and the association
278 between heart rate and cardiac phase length cf. **Supplementary Methods, Supplementary**
279 **Results, Fig. S1, and Fig. S2**. The (self-paced) picture onsets were then assigned to the
280 respective cardiac phase (i.e., individual systole or diastole). To take into account between-
281 subject differences in heart rate (and thus cardiac phase lengths), the sum of picture onsets
282 per phase (as ratio of all 120 trials) was normalized to the proportion of the subject-specific
283 phase length in the total cardiac cycle, resulting in a value of (picture onsets per cardiac
284 phase / 120) / (individual cardiac phase length / individual mean R-R length) for each cardiac
285 phase. With no cardiac effect, button presses (triggering picture onsets) would be randomly
286 distributed across both cardiac phases. That is, the rate of systolic (diastolic) picture onsets
287 should correspond to the proportion of systole (diastole) in the total R-R length, thereby re-
288 sulting in a ratio of 1. A ratio >1 thus reflects an over-proportional accumulation of picture
289 onsets in the respective cardiac phase. In the group-level analysis, normalized systolic and
290 diastolic ratios were tested against each other with a two-sided paired t-test.

291 **Recognition period—cardiac modulation of recognition memory.**

292 *Circular analysis:* To relate memory performance in the recognition period and stimulus onset
293 in the encoding period, we analysed—for each participant—the stimulus subset of memory
294 probes (i.e., pictures in the recognition period that had already been shown during the encod-
295 ing phase) with respect to their cardiac onset during encoding. Parallel to the circular analy-
296 sis regarding visual sampling during encoding (see above), we computed the self-paced on-
297 set of memory probes during encoding across the participant's cardiac cycle (**Fig. 1b**). To
298 correct for a possible bias due to self-paced memory probe distributions, three subjects with
299 non-uniform circular distributions of memory probes (indicated by significant Rayleigh tests)
300 were excluded from further analysis. At the group level, we then analysed circular distribu-
301 tions of onset times for memory probes that were correctly remembered (hits) or erroneously
302 identified as new pictures (misses). To that aim, sets of individual mean onsets for hits and
303 misses were tested against the circular uniform distribution using Rayleigh tests.

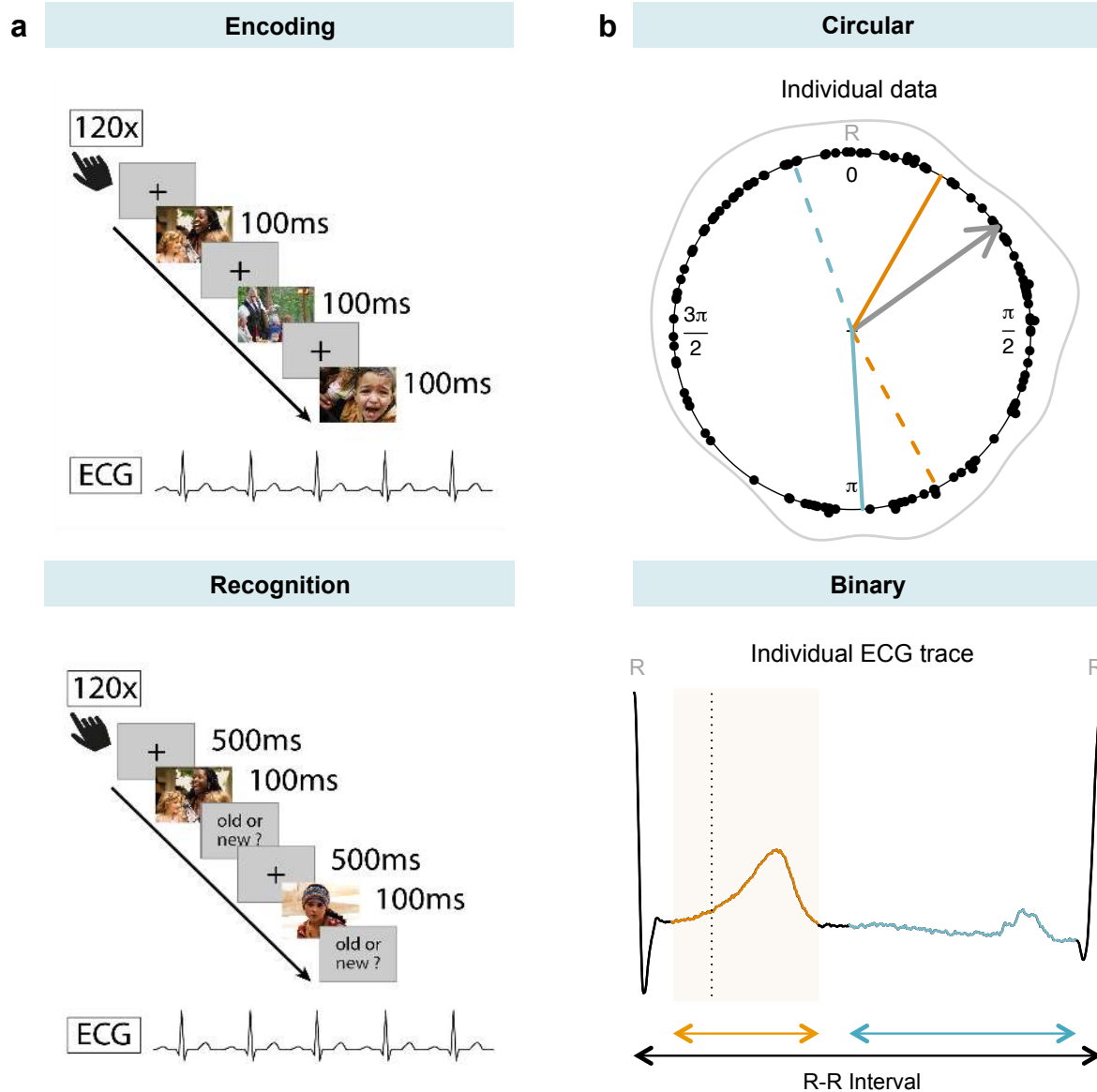
304 *Binary analysis:* The hypothesized association between cardiac phase and memory
305 performance was further analysed by determining the stimulus' phasic timing during encod-
306 ing, that is, whether it had been presented in individual systole or diastole (for detailed bin-
307 ning procedure cf. **Supplementary Methods**), relative to its recognition performance. To
308 predict the binary recognition outcome (miss = 0, hit = 1), we computed general linear mixed
309 regression models (GLMM) for binomial data, with subjects as random factor. The first model
310 (m1) was fitted for the overall fixed effect of valence with the three levels of picture valence
311 (positive, negative, neutral) contrast-coded against neutral picture valence as baseline condi-
312 tion. The second model (m2) included picture valence (negative-neutral, positive-neutral),
313 cardiac phase (diastole = 0, systole = 1), and their interaction as fixed effects. Significance
314 was obtained by likelihood ratio tests to compare the full model, which included the effect in
315 question (i.e., valence, cardiac phase), with the reduced model, which did not include the
316 effect in question (i.e., m1 vs. m0 and m2 vs. m1). NB: For m1, the data included only pic-
317 tures encoded in individual systole or diastole (i.e., pictures encoded in non-defined cardiac
318 intervals were excluded from analysis). An advantage of GLMMs (Jaeger, 2008) is that they

319 can simultaneously test for random effects of subject and item (i.e., picture). To assess addi-
320 tional variance explained by individual pictures, we added picture as a random factor to our
321 models. For the regression analysis, we used the lme4 package (Bates, Mächler, Bolker, &
322 Walker, 2015) in the R Statistical Environment.

323 **Exploratory analysis of visual sampling and recognition memory relative to inter-**
324 **individual differences.** In an additional exploratory analysis, participants' individual (i.e.,
325 systolic and diastolic) ratios of self-paced picture onsets as well as their overall mean recog-
326 nition performance (i.e., the percentage of correctly recognised pictures) were correlated with
327 variables of inter-individual differences: Interoceptive accuracy (centred via z-transformation),
328 trait anxiety (centred via z-transformation), and resting heart rate variability/ rMSSD (log-
329 transformed to mitigate skewedness and centred to the mean). For measures of interocep-
330 tive accuracy, two participants with lacking information in the heartbeat perception task were
331 excluded from the analysis (n = 41).

332 **Code availability.** The code of our analysis, computed in the R Statistical Environment
333 (v3.4.3) with RStudio version 1.0.136 (RStudio Team, 2016) is available on GitHub
334 (https://github.com/SKunzendorf/0303_INCAS1). Graphics were obtained with the circular
335 package (Agostinelli & Lund, 2013) and the ggplot2 package (Wickham, 2009).

336 **Data availability.** The data that support the findings of this study are available on GitHub
337 (https://github.com/SKunzendorf/0303_INCAS1). Data for preprocessing are available from
338 the corresponding author upon request.



339

340 **Figure 1. Experimental setup and data analysis.** **a**, During encoding (top), participants prompted by
341 button press the onset of the next picture, which could be positive, neutral, or negative. In the recogni-
342 tion period (bottom), they indicated for each picture (60 old, 60 new) whether or not they had seen it
343 before. Simultaneous ECG was recorded to analyse behaviour relative to the cardiac cycle: **b**, For
344 circular analysis (top), values between 0 and 2π were assigned to each stimulus onset (black dots),
345 corresponding to its appearance within the cardiac cycle (from the previous to the next R peak in the
346 ECG). Mean (grey arrow) and circular density (grey line) of stimulus onsets were calculated per sub-
347 ject. Individual cardiac phases from the binary analysis (see below) are visualised as circular seg-
348 ments (start: solid, end: dashed): systole (orange) and diastole (blue). For binary analysis (bottom),
349 stimulus onsets (dashed line) were binned into participant-specific systole (orange) and diastole (blue)

350 using a template approach (cf. **Supplementary Methods, Supplementary Results, Fig. S1, and Fig.**
351 **S2**).

352

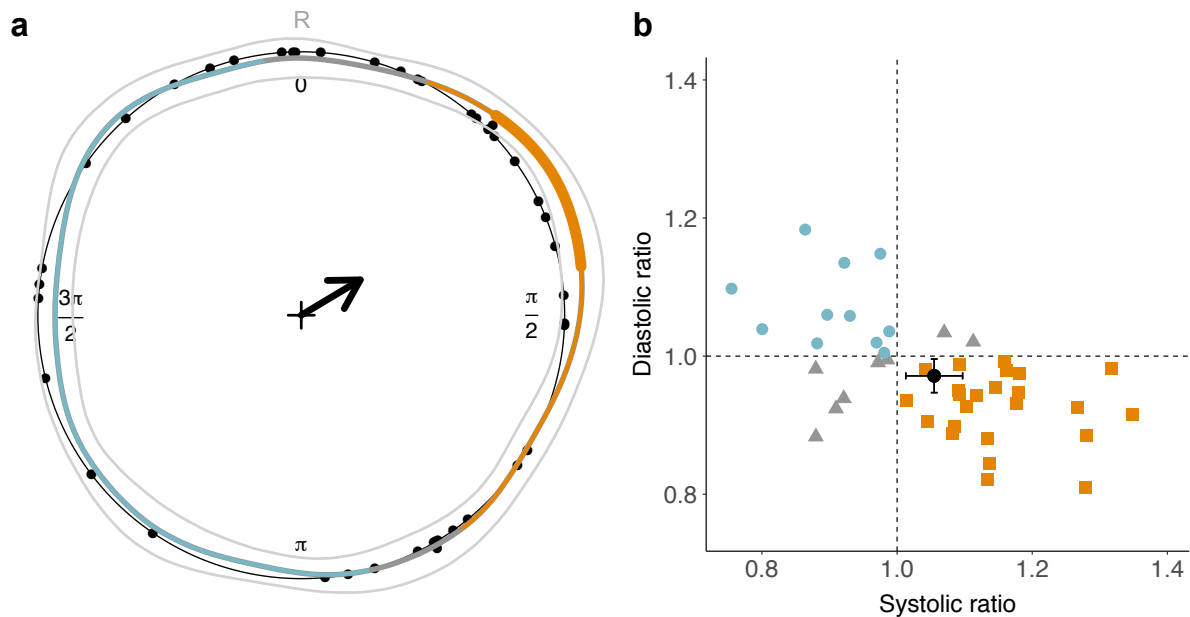
353 **Results**

354 We tested whether self-paced visual sampling and visual memory encoding fluctuate across
355 the cardiac cycle. Based on previous studies that demonstrated facilitated visual processing
356 (Pramme et al., 2014, 2016) and increased oculomotor activity (Ohl et al., 2016) during the
357 early phase of the cardiac cycle, we hypothesized that participants prefer to prompt a visual
358 stimulus during early phases of the cardiac cycle. In addition, we hypothesized memory per-
359 formance to be influenced by the cardiac time point of memory probes during encoding
360 (Garfinkel et al., 2013).

361 **Encoding:** The distribution of self-paced picture onsets relative to the cardiac R-R
362 interval showed an overall increase in early phases of the cardiac cycle ($M = 0.33\pi$, $SD =$
363 0.52π , $\rho = 0.26$, cf. **Fig. 2a**). This observation was supported by inferential circular statistics
364 indicating a non-significant trend that the self-paced key presses in the present experiment
365 are unlikely to be uniformly distributed (Rayleigh test statistics $R_0 = 0.26$, $p = .053$). Of note,
366 the same analysis with our preregistered sample size (i.e., the first 40 healthy subjects of $N =$
367 43 ; cf. <https://osf.io/5z8rx/>) showed a significant deviation from a uniform distribution ($R_0 =$
368 0.28 , $p = .039$), that is due to a significant increase in self-paced key presses in the interval
369 from 0.24 to 0.44π (**Fig. 2a**) as revealed by nonparametric bootstrapping (performed on the
370 original participant pool, $N = 43$). Although this circular statistics can infer that the distribution
371 of relative picture onsets deviates from a uniform distribution, it cannot pinpoint the transition
372 from systole to diastole – particularly in the presence of varying heartbeat lengths, for which
373 the same section of the circular distribution can be associated with different cardiac phases.

374 Accounting for the bi-phasic nature of cardiac activity in the binary analysis, we com-
375 puted the number of key presses during cardiac systole and diastole, normalised by the pro-
376 portion of the systole vs. diastole in the whole cardiac cycle. We found a significantly larger
377 ($t(42) = 2.76$, $p = .009$, Cohen's $d = 0.42$) ratio of picture onsets in the systole ($M = 1.05$, SD

378 = 0.14) as compared to diastole ($M = 0.97$, $SD = 0.081$), corroborating our finding of an
379 increase in self-paced visual sampling during cardiac systole (cf. **Fig. 2b**). Similar results were
380 obtained for the preregistered sample size ($n = 40$), showing a significantly larger ($t(39) =$
381 2.70 , $p = .010$, Cohen's $d = 0.43$) systolic ($M = 1.05$, $SD = 0.14$) than diastolic ratio ($M =$
382 0.97 , $SD = 0.079$).



383
384 **Figure 2. Circular and binary analysis of visual sampling relative to the heartbeat.** **a**, Circular
385 distribution of individual mean picture onsets (black dots, $N = 43$) across the cardiac cycle (from R
386 peak to R peak). We observed a trend for increased self-prompted stimulus presentations (weighted
387 overall mean as black arrow) in early phases of the cardiac cycle. Based on a bootstrapping proce-
388 dure, we computed the mean circular density of picture onsets (middle thicker line), as well as a 95%
389 confidence interval (CI, within inner and outer thin grey lines). Segments of the cardiac cycle are de-
390 termined as statistically significant (thick orange segment) when the circular density significantly differs
391 from the circular uniform (i.e., the lower bound of the CI is outside of the black uniform circle). To re-
392 late segments of the cardiac cycle to the two cardiac phases (systole = orange, diastole = blue, non-
393 defined = grey), overall mean systole and diastole lengths were obtained, showing, that the significant
394 density segment falls into systole. **b**, Most subjects ($24/43$) preferred to prompt pictures during their
395 systole (orange/square). Fewer subjects ($11/43$) chose to prompt them during their diastole (blue/dot)
396 or did not show a preference in any of the two defined phases ($8/43$; grey/triangle). The phase-specific
397 proportion of key presses (relative to all 120 trials) was normalized by the proportion of the cardiac
398 phase (systole, diastole) in the entire R-R interval. A ratio >1 thus indicates that the number of

399 prompted picture onsets during systole or diastole exceeds the number that would be expected if they
400 were uniformly distributed (resulting in a ratio = 1, dashed line). The group-level mean (black dot with
401 standard error bars) shows an over-proportional accumulation of picture onsets during individual sys-
402 tole relative to individual diastole.

403

404 **Recognition:** We also investigated the association between the cardiac cycle and
405 memory processing: In a circular analysis, we tested whether the distribution of onset times
406 during stimulus encoding differed for pictures that were correctly remembered (hits) or erro-
407 neously identified as new pictures (misses). Overall, picture onset times during the encoding
408 period did not significantly deviate from a uniform distribution over the cardiac cycle for hits
409 ($R_0 = 0.20$, $p = .21$) and misses ($R_0 = 0.16$, $p = .36$).

410 We further investigated the influence of cardiac phase (systole, diastole) and picture
411 valence on recognition memory. The results of the GLMM (cf. **Table 1**) with contrast-coded
412 picture valence (m1), that is, negative-neutral and positive-neutral, showed a significant
413 memory benefit for negative vs. neutral and for positive vs. neutral stimuli. More specifically,
414 memory performance for negative pictures ($M = 0.80$, $SD = 0.13$) and for positive pictures (M
415 $= 0.78$, $SD = 0.16$) significantly exceeded memory performance for neutral pictures ($M =$
416 0.73 , $SD = 0.18$). Comparison of m1 against the null model (without the fixed effect of va-
417 lence) showed that valence significantly increased the model fit. Critically, adding cardiac
418 phase (i.e., systole, diastole) to the model (m2) did not improve the model fit (cf. **Table 1**):
419 Neither phase nor its interaction with picture valence significantly accounted for variation in
420 recognition memory. Compared to m1, cardiac phase did not significantly improve the model
421 fit. Adding picture as additional random effect only slightly changed parameter estimates but,
422 critically, did not account for additional variance in the association between memory perfor-
423 mance and the cardiac cycle (detailed results not reported).

424

a.	Coefficient	SE	Z-Value	P-Value
m1 (~ picture valence)				
Intercept	1.17	0.15	7.71	< .001

negative vs. neutral (neg-neu)	0.37	0.12	3.11	.002
positive vs. neutral (pos-neu)	0.29	0.12	2.43	.015
m2 (~ picture valence X cardiac phase)				
Intercept	1.24	0.17	7.14	< .001
cardiac phase (0 = diastole, 1 = systole)	-0.17	0.19	-0.89	.37
phase X neg-neu	0.30	0.27	1.11	.27
phase X pos-neu	0.16	0.27	0.61	.54

b.	Model Fitting Criteria			Likelihood Ratio Tests		
	AIC	BIC	LogLikelihood	Chi-Square	Df	P-value
m1	2626	2650	-1309	10.71	2	.005
m2	2171	2211	-1079	1.24	3	.74

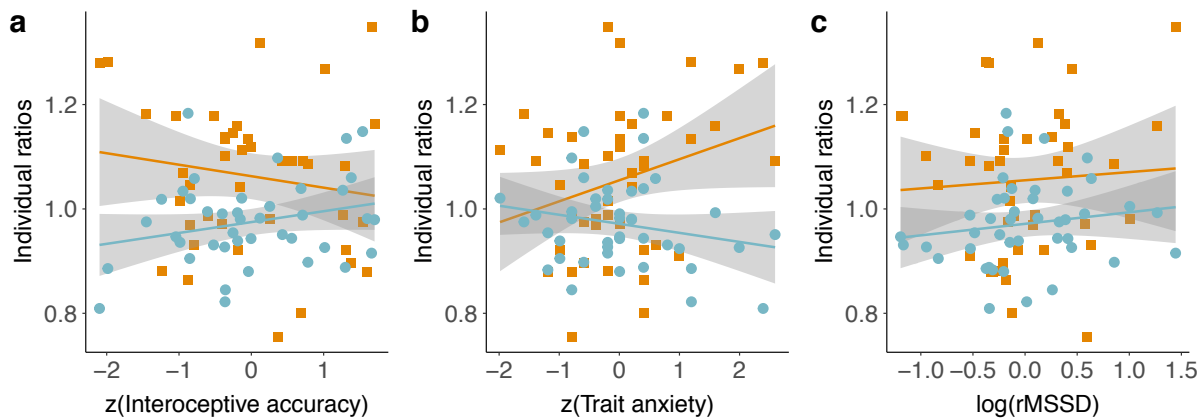
425 **Table 1. a**, General linear mixed model (GLMM) with recognition memory (hit = 1, miss = 0) relative to
426 picture valence (negative-neutral, positive-neutral) (m1 = memory ~ picture valence + (1|vp)), cardiac
427 phase, and their interaction (m2 = memory ~ picture valence X cardiac phase + (1|vp)). Valenced pic-
428 tures (negative and positive) showed a significant memory benefit compared to neutral pictures. Nei-
429 ther cardiac phase nor its interaction with picture valence significantly accounted for variation in visual
430 memory performance. **b**, Likelihood ratio tests of m1 and m2 against the reduced model (i.e., m0 and
431 m1, respectively) show that picture valence significantly increased the model fit while cardiac phase
432 did not account for variation in memory performance.

433

434 Beyond our preregistered hypotheses, additional results were obtained by further exploratory
435 analyses.

436 **Systole-associated visual sampling and inter-individual differences.** Individual
437 systolic ratios of self-paced picture onsets were neither significantly correlated with inter-
438 individual differences in interoceptive accuracy ($r(39) = -.16$, $p = .32$) nor in heart rate varia-
439 bility (i.e., resting rMSSD; $r(41) = .064$, $p = .69$). There was a non-significant (and not hy-
440 pothesized) trend (**Fig. 3b**) for individual systolic ratios to increase with higher trait anxiety
441 ($r(41) = .29$, $p = .062$). Neither interoceptive accuracy ($r(39) = .25$, $p = .11$) nor trait anxiety
442 ($r(41) = -.21$, $p = .17$) nor heart rate variability ($r(41) = .16$, $p = .32$) significantly modulated
443 individual diastolic ratios of picture onsets (**Fig. 3**).

444



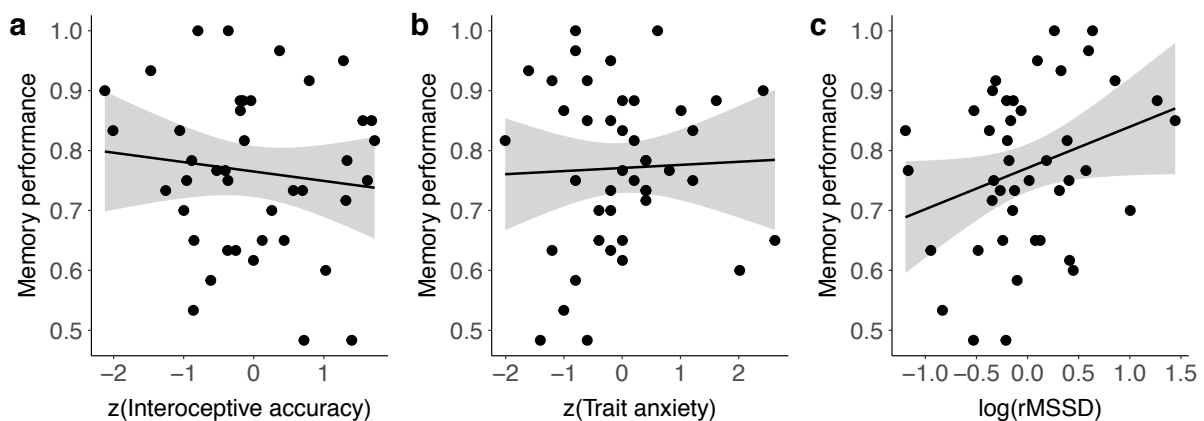
445

446 **Figure 3. Correlation of systolic (orange squares) and diastolic (blue circles) ratios of picture**
447 **onsets with inter-individual differences in a, Interceptive accuracy, b, trait anxiety, and c, resting**
448 **heart rate variability (root mean square of successive differences, rMSSD). Grey areas are the 95%**
449 **confidence intervals of the respective linear models (orange / blue lines).**

450

451 **Recognition memory varies and inter-individual differences.** We furthermore in-
452 vestigated the role of inter-individual variables (i.e., interoceptive accuracy, trait anxiety, rest-
453 ing heart rate variability) for memory performance with correlation analyses. Neither differ-
454 ences in interoceptive accuracy ($r(39) = -.12, p = .46$), nor in trait anxiety ($r(41) = .039, p =$
455 $.80$) were associated with mean recognition performance (**Fig. 4**). However, there was a non-
456 significant trend of resting heart rate variability (i.e., resting rMSSD) to be positively correlat-
457 ed with mean recognition performance ($r(41) = .29, p = .056$), that is, recognition memory
458 increased with higher resting heart rate variability (**Fig. 4c**).

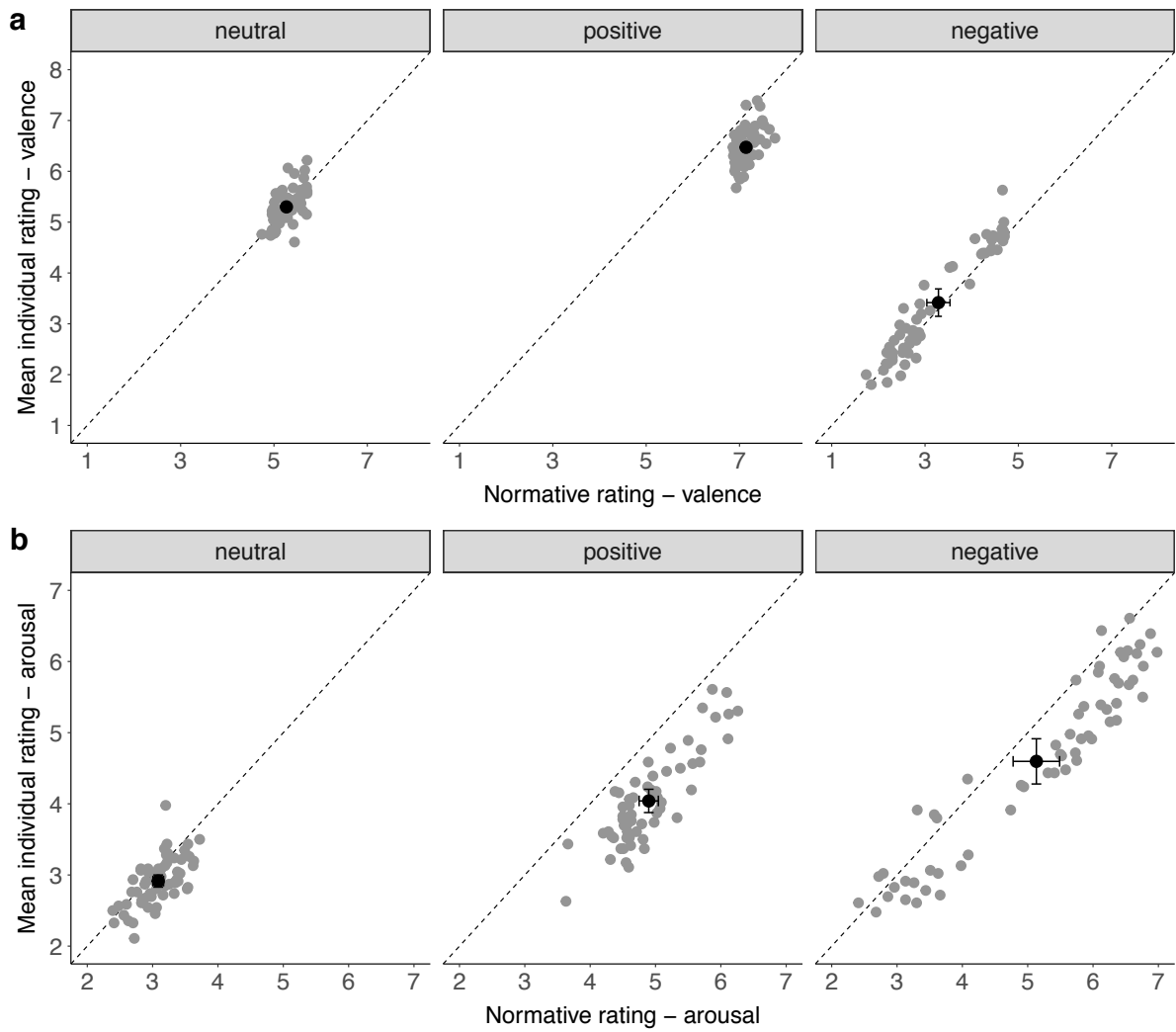
459



460 **Figure 4. Correlation of mean recognition performance with inter-individual differences.** **a**, in-
461 teroceptive accuracy, **b**, trait anxiety, and **c**, resting heart rate variability (root mean square of succes-
462 sive differences, rMSSD). Grey areas are the 95% confidence intervals of the linear model (black line).

463

464 **Subjective perception of picture emotionality.** As a control, we analysed if the
465 subjective valence and arousal ratings in our study differed from the EmoPicS normative
466 ratings (**Fig. 5**). For ratings of the two affective dimensions, valence and arousal, mixed-
467 design ANOVAs tested the main and interaction effects of the repeated-measures factor rat-
468 ing category (normative, individual) and the factor picture valence (positive, neutral, nega-
469 tive). We observed a significant main effect of rating category for both, valence and arousal:
470 Mean individual valence ratings ($M = 5.06$, $SD = 1.43$) were significantly lower ($F(1,352) =$
471 10.1 , $p = .002$) than normative ratings ($M = 5.23$, $SD = 1.69$), as were mean individual arous-
472 al ratings ($M = 3.85$, $SD = 1.09$) compared to normative ($M = 4.37$, $SD = 1.28$) ratings
473 ($F(1,352) = 27.0$, $p < .001$). However, while valence ratings did not show a significant interac-
474 tion for rating category X picture valence ($F(2,352) = 1.91$, $p = .15$; see **Fig. 5a**), the differ-
475 ence between individual and normative arousal ratings was influenced by picture valence
476 ($F(2,352) = 5.71$, $p = .004$; see **Fig. 5b**). To further examine this interaction, two-sided paired
477 t-tests were calculated and p-values were adjusted for multiple comparisons with Bonferroni
478 correction: positive (individual: $M=4.04$, $SD=0.65$; normative: $M=4.90$, $SD=0.58$) arousal rat-
479 ings differed significantly larger from each other ($t(59) = 20.2$, $p = < .001$, Cohen's $d = 1.39$)
480 than both neutral (individual: $M=2.91$, $SD=0.34$; normative: $M=3.09$, $SD=0.32$) ($t(59) = 4.77$,
481 $p = < .001$, Cohen's $d = 0.52$) and negative (individual: $M=4.60$, $SD=1.26$; normative:
482 $M=5.13$, $SD=1.41$) arousal ratings ($t(59) = 9.32$, $p = < .001$, Cohen's $d = 0.40$). Furthermore,
483 while normative arousal ratings did not differ significantly between positive and negative pic-
484 tures (cf. **Methods**), individual arousal ratings were significantly higher for negative com-
485 pared to positive pictures ($t(88.3) = 3.05$, $p = .003$, Cohen's $d = 0.56$).



486

487 **Figure 5. Subjective perception of picture emotionality (individual valence and arousal ratings)**

488 **compared to normative picture ratings. a, Valence ratings and b, Arousal ratings** were both signifi-

489 cantly lower for individual compared to normative ratings (overall mean in black with standard error

490 bars). For arousal but not for valence ratings there was a significant interaction effect between rating

491 category and picture valence.

492 **Discussion**

493 We studied the association between the cardiac cycle and self-paced visual sampling as well
494 as visual recognition memory for pictures of different emotional valence. We hypothesized
495 that facilitated visual processing (Pramme et al., 2014, 2016)—observed specifically for rele-
496 vant or emotionally salient stimuli (Azevedo et al., 2018, 2017; Garfinkel et al., 2014)—as
497 well as facilitated oculomotor processing during systole (Ohl et al., 2016) guides active per-
498 ception in the shape of a preference to prompt a relevant visual stimulus during early phases
499 of the cardiac cycle. We observed a significant accumulation of key presses (i.e., prompted
500 picture onsets) during systole, thereby showing for the first time a coupling between self-
501 paced visual sampling and the heartbeat. Memory performance, however, was only influ-
502 enced by picture valence, replicating a significant memory benefit for emotional content
503 (Hamann, 2001; Kensinger, 2006; Kensinger & Corkin, 2003; LaBar & Cabeza, 2006), but
504 not further modulated by the cardiac phase in which targets were encoded (Garfinkel et al.,
505 2013). The association between the cardiac cycle and self-initiated actions complements
506 findings of facilitated visual processing during systole, thereby proposing a link between the
507 heartbeat and active perception.

508 Sensorimotor processing of passively presented stimuli has been shown to be de-
509 creased during early cardiac phases (Birren et al., 1963; Callaway & Layne, 1964; Edwards
510 et al., 2007; Lacey & Lacey, 1974; McIntyre et al., 2008; Saari & Pappas, 1976), but evi-
511 dence is mixed, including some earlier null findings (Jennings & Wood, 1977; Salzman &
512 Jaques, 1976; Thompson & Botwinick, 1970). However, which processing stages are modu-
513 lated by the heartbeat has long remained unclear. More fine-grained decomposition of reac-
514 tion time into central (sensory, pre-motor) and peripheral (motor) processes has indicated
515 that the response inhibition during early cardiac phases was confined to central (pre-motor)
516 levels of stimulus processing, whereas the motor component remained unaffected (Edwards
517 et al., 2007; McIntyre et al., 2008; Saari & Pappas, 1976) or even accelerated (Schulz et al.,
518 2009). This differential effect could also underlie findings that report an increased tendency
519 to act during systole such as fire a virtual (Azevedo et al., 2017) or an actual weapon (Mets

520 et al., 2007) during early cardiac phases. Our results of facilitated spontaneous actions dur-
521 ing systole when engaging with a visual stimulus furthermore add to results from oculomotor
522 behaviour: Ohi et al. (2016) reported involuntarily occurring oculomotor activity (i.e., mi-
523 crosaccade generation) to be heightened during early cardiac phases. Hence, for both soma-
524 tomotor and oculomotor processes, our readiness to act upon an external stimulus fluctuates
525 with our (internal) cardiac rhythm, being relatively increased during the phase of systolic
526 blood ejection.

527 Although underlying heart-brain pathways remain unclear, systolic influences on per-
528 ception and cognition have often been attributed to the phasic nature of cardio-afferent sig-
529 nalling, which is triggered with the heartbeat (Koriath & Lindholm, 1986; Lacey & Lacey,
530 1974, 1978). More specifically, stretch-responsive baroreceptors located in arterial walls re-
531 spond to transient pressure rises at each blood ejection and communicate the current cardi-
532 ovascular state (i.e., the heartbeat's strength and timing) to the brain. Thus, baroreceptor-
533 transmitted cardiac signals, which are phasically registered by central processing systems,
534 have been proposed to induce a general suppression of cortical excitability, converging with
535 earlier findings of sensory inhibition (Dembowsky & Seller, 1995; Rau & Elbert, 2001). For-
536 mulated in terms of the *interoceptive predictive coding* framework (Barrett & Simmons, 2015;
537 Seth, 2013), which extends the *free-energy principle* (Friston, 2010) to interoceptive pro-
538 cesses and connects them to consciousness and emotion, this periodic—and thus predicta-
539 ble—ascending baroreceptor input to central structures is anticipatorily cancelled out by top-
540 down interoceptive predictions, thereby minimizing its influence on perception (Critchley &
541 Garfinkel, 2018; Salomon et al., 2016). Besides modulating arterial baroreceptor discharge,
542 heartbeat-related pressure fluctuations generate periodic sensory influences throughout the
543 body—affecting for example the discharge of tactile (Macefield, 2003) or muscle spindle af-
544 ferents (Birznieks, Boonstra, & Macefield, 2012)—which are predicted and normally do not
545 enter perceptual awareness. In our constant attempt to minimize sensory uncertainty (Peters,
546 McEwen, & Friston, 2017), inhibition of such predictable cardiac-induced sensory effects has
547 been argued to reduce—potentially distracting—self-related sensory noise (Salomon et al.,

548 2016) at the benefit of our processing of the outside world, for example by increasing the
549 signal-to-noise ratio of external stimuli. Correspondingly, stimuli presented simultaneously
550 with the heartbeat are interpreted as sensory consequences of the organism's own (internal)
551 cardiac activity and thus perceptually attenuated (Salomon et al., 2016). Our finding that par-
552 ticipants implicitly act upon a visual stimulus during the phase of heartbeat-related (barore-
553 ceptor-mediated) central inhibition could indicate a short-term benefit: As argued by Pramme
554 et al. (2016), the impact of baroreceptor-mediated central influences may depend on context-
555 or task-specific processing demands. In other words, extraction of behaviourally relevant
556 external stimuli from a distracting sensory scene might be facilitated during inhibition of irrel-
557 evant (e.g., cardiac-related) sensory information (Pramme et al., 2016). Accordingly, predict-
558 able phases of attenuated heartbeat-related noise might provide a short-term window to facil-
559 itate active engagement towards an external relevant stimulus.

560 Such differential processing during transient cardiac signalling converges with the ob-
561 served specificity of cardiac effects when using valenced stimuli, in particular selectively facil-
562 itated processing of threat stimuli during systole (Garfinkel & Critchley, 2016). The notion that
563 cardiac signals prioritise the processing of motivationally relevant information suggests a
564 crucial role of cardiac interoceptive information in conveying bodily arousal states to the brain
565 (Critchley & Garfinkel, 2018; Garfinkel & Critchley, 2016). In other studies, states of higher
566 psychophysiological arousal have shown to bias the processing of relevant stimuli, including
567 facilitated memory formation (Cahill & McGaugh, 1998; Mather et al., 2016; Mather &
568 Sutherland, 2011; McGaugh, 2015). However, the pattern of results concerning memory
569 modulation across the cardiac cycle remains fragmented and unclear. Although perceptual
570 sensitivity for emotional stimuli is increased during systole (Garfinkel et al., 2014), affective
571 (positive, negative) and neutral words are recalled less often when they are encoded during
572 systole as compared to diastole (Garfinkel et al., 2013). Furthermore, this cardiac memory
573 effect could only be obtained in subjects with lower interoceptive accuracy, suggesting influ-
574 ences of an individual's access to interoceptive sensations (Pollatos & Schandry, 2008). On
575 the other hand, Fiacconi et al. (2016) found that fearful and neutral faces presented during

576 systole are more likely to be judged as known or old, irrespective of whether they had been
577 shown before or not. In our study, recognition memory was not influenced by the cardiac
578 phase during which a stimulus was encoded—also adding to a recent study reporting a lack
579 of cardiac influences on memory retrieval (Pfeifer et al., 2017)—but only by its valence,
580 showing a significant benefit for negative and positive pictures. This suggests that—at least
581 in our study—the influence of externally-induced emotional arousal states (e.g., by seeing an
582 upsetting negative picture) on memory formation (Tambini et al., 2017) might have exceeded
583 a transient cognitive modulation across the cardiac cycle (Garfinkel et al., 2013). Such rea-
584 soning is further supported by a recent study showing that interoceptive cardiac signals can
585 easily be overshadowed by external stimuli or other task-specific influences (Yang, Jennings,
586 & Friedman, 2017). Although in our study, stimulus content was largely matched along sev-
587 eral dimensions (physical image statistics and more high-level features), differences in stimu-
588 lus features may still account for variation in memory effects associated with the cardiac cy-
589 cle. For example, differences have been reported for different stimulus categories like words
590 (Garfinkel et al., 2013), faces (Fiacconi et al., 2016), and complex scenes (present study),
591 but also for low-level stimulus properties such as spatial frequency (Azevedo et al., 2018).
592 However, accounting for picture as random effect in our GLMM analyses did not explain ad-
593 ditional variance in memory performance across the cardiac cycle.

594 Our exploratory supplementary finding indicates that inter-individual differences in
595 recognition memory are positively associated with inter-individual differences in resting heart
596 rate variability. Considered a trait marker of autonomic or parasympathetic cardio-regulation
597 and—more generally—of heart-brain coupling (Thayer et al., 2012), variation in beat-to-beat
598 intervals at rest has been associated with cognitive capacities: participants with higher rest-
599 ing heart rate variability performed better in tests of working memory and attention (Hansen,
600 Johnsen, & Thayer, 2003; Luft, Takase, & Darby, 2009). Future studies investigating cardiac
601 influences on cognition could further examine the impact of inter-individual differences in
602 resting heart rate variability.

603 Taken together, cardiac phase effects on perception, cognition, and behaviour might
604 constitute a non-functional epiphenomenon emerging from transient physiological changes,
605 which set the context for heart-brain interactions: As baroreceptor-transmitted afferent sig-
606 nals (Critchley & Harrison, 2013) occur with every systolic pressure wave and reflect momen-
607 tary states of increased blood pressure, they constitute a fine-tuned reference of cardiovas-
608 cular arousal. Although autonomously generated, cardiac fluctuations are integrated in multi-
609 ple feedback loops to react to environmental challenges such as exercise, body position, or
610 stress (Dampney et al., 2002; Glass, 2001; Saper, 2002). Cardiovascular arousal is thus di-
611 rectly encoded via frequency (e.g., increased heart rate) and waveform (e.g., increased am-
612 plitude in elevated blood pressure) (Dampney et al., 2002; Schächinger, Weinbacher, Kiss,
613 Ritz, & Langewitz, 2001), which reciprocally affect afferent baroreceptor stimulation
614 (Chapleau, Li, Meyrelles, Ma, & Abboud, 2001). Influences of the cardiovascular state on
615 sensory processing might thus subtly emerge with heartbeat-related pressure fluctuations,
616 but are only fully expressed under a sustained shift of our bodily state beyond physiological
617 variability; for example, under stress, when the whole spectrum of adaptive brain-body re-
618 sponses is activated (e.g., elevated blood pressure and accelerated heart rate) and the af-
619 ferent cardiac signalling increases. Correspondingly, Luft and Bhattacharya (2015) found that
620 the representation of cardiac signals in the brain, as measured by EEG-derived heartbeat-
621 evoked potentials, differs between states of high vs. low emotional arousal. Besides in-
622 creased amplitudes in arterial pressure waves, it could be argued that a faster heartbeat dur-
623 ing stressful situations—next to providing metabolic support for action requirements to re-
624 stabilize our homeostatic integrity (Gianaros & Wager, 2015)—results in relatively increased
625 systolic signalling (as raises in heart rate occur mainly at the expense of diastole length) and
626 thereby generates more time windows of selectively facilitated sensory processing. Evidence
627 for this proposal comes from a recent study that associated experimentally increased heart
628 rates (Pezzulo et al., 2018) with prioritized fear processing across different measures (reac-
629 tion time, peak velocity, response acceleration, choice uncertainty). Hence, increased signal-
630 ling of cardiovascular states under conditions of higher bodily arousal and heart rates might

631 more strongly modulate cognition and behaviour (e.g., active perception and self-paced ac-
632 tion), thereby supporting what information is preferentially processed.

633 Our experiment has several limitations: While linking active perception and the cardi-
634 ac cycle, our design does not allow to decompose cardiac influences at the levels of soma-
635 tomotor, sensory, and cognitive processing. A control condition to dissociate cardiac-related
636 motor activity from visual processing could rule out a pure motor effect, for example by test-
637 ing spontaneous motor actions that are not explicitly coupled to perception of (relevant) stim-
638 ulti. The hypothesis would be that button presses that do not prompt relevant sensory input
639 would be randomly (i.e., uniformly) distributed across the cardiac cycle. An essential step to
640 investigate the role of cardiac activity as bodily reference would be to test cardiac coupling of
641 stimulus processing under conditions of altered cardiac activity (e.g., increased heart rate),
642 for example by inducing stress through increased sensory uncertainty (e.g., by manipulating
643 stimulus predictability). In addition, measurements of cardiac representations in the brain
644 (e.g., using EEG) would extend our understanding of the central integration and modulation
645 of cardiac signals, for example, in the context of self-paced visual sampling and visual
646 memory processing.

647 In conclusion, our findings imply that the heartbeat constitutes a crucial bodily signal
648 that is integrated in our active engagement with the external world. Specifically, they suggest
649 that we tend to act in a phase of inhibited cardiac- and thus self-related sensory processing
650 (namely cardiac systole) when extracting relevant information from our environment. Subtly
651 emerging under normal conditions, this influence might become functionally relevant in states
652 of high arousal (e.g., in stressful situations). Extending previous frameworks of mind-brain-
653 body interactions (Park & Tallon-Baudry, 2014), we propose that we implicitly exploit internal
654 ongoing bodily fluctuations as a predictable reference frame from which interaction with our
655 ever-changing and often unpredictable environment can arise. When initiating actions to
656 sample the noisy world around us, we relate them to the rhythm we know best—our own
657 heartbeat.

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