



THE UNIVERSITY *of* EDINBURGH

Edinburgh Research Explorer

## Analysis of Photon Detection Efficiency and Dynamic Range in SPAD based Visible Light Receivers

**Citation for published version:**

Gnecchi, S, Dutton, N, Luca, P, Rae, BR, Pellegrini, S, McLeod, SJ, Grant, LA & Henderson, R 2016, 'Analysis of Photon Detection Efficiency and Dynamic Range in SPAD based Visible Light Receivers', *Journal of Lightwave Technology*, vol. 34, no. 11, pp. 2774-2781. <https://doi.org/10.1109/JLT.2016.2550497>

**Digital Object Identifier (DOI):**

[10.1109/JLT.2016.2550497](https://doi.org/10.1109/JLT.2016.2550497)

**Link:**

[Link to publication record in Edinburgh Research Explorer](#)

**Document Version:**

Peer reviewed version

**Published In:**

Journal of Lightwave Technology

**General rights**

Copyright for the publications made accessible via the Edinburgh Research Explorer is retained by the author(s) and / or other copyright owners and it is a condition of accessing these publications that users recognise and abide by the legal requirements associated with these rights.

**Take down policy**

The University of Edinburgh has made every reasonable effort to ensure that Edinburgh Research Explorer content complies with UK legislation. If you believe that the public display of this file breaches copyright please contact [openaccess@ed.ac.uk](mailto:openaccess@ed.ac.uk) providing details, and we will remove access to the work immediately and investigate your claim.



# Analysis of Photon Detection Efficiency and Dynamic Range in SPAD based Visible Light Receivers

Salvatore Gnecci<sup>\*†</sup>, Neale A.W. Dutton<sup>\*†</sup>, Luca Parmesan<sup>\*†</sup>

Bruce R. Rae<sup>\*</sup>, Sara Pellegrini<sup>\*</sup>, Stuart J. McLeod<sup>\*</sup>, Lindsay A. Grant<sup>\*</sup>, Robert K. Henderson<sup>†</sup>

<sup>\*</sup>ST Microelectronics Imaging Division, Edinburgh, United Kingdom

<sup>†</sup>The University of Edinburgh, Edinburgh, United Kingdom

**Abstract**—We investigate the photon detection efficiency and the dynamic range for digital silicon photomultipliers (dSiPMs) over a selection of design parameters: dSiPM unit cell dead time, photon detection efficiency, unit cell area and fill factor, number of cells and total dSiPM active area. Two receiver scaling scenarios are considered: varying the number of cells for (1) a fixed unit cell area or (2) a fixed total dSiPM area. Theoretical and simulated results are confirmed with experimental data from a selection of dSiPMs realised on a test chip in 130nm CMOS process.

**Index Terms**—Single Photon Avalanche Diodes, SPAD, dSiPM, digital Silicon Photomultiplier, Visible Light Communication, VLC

## I. INTRODUCTION

CMOS single photon avalanche diodes (SPADs) are finding commercial application in positron emission tomography (PET), time-of-flight ranging and advanced microscopy thanks to their high timing resolution, integration in array formats with fast digital signal processing at low cost [1], [2], [3], [4], [5], [6].

Recent interest has been shown in applying these detectors in guided wave or free space visible light communications (VLC) where they promise high sensitivity and photon shot noise limited links [7], [8]. Although only modest data rates have been so far obtained [9], [10], evidence of optical communications operating at the quantum limit is already emerging [11], [12], [13], [14]. Enhancements of data rates towards the Gb/s rates competitive with state of the art visible communications, [15], [16], [17], [18], rely on advances in the architectures of SPAD receivers. Two key areas are being investigated (1) architectures for combining multiple SPAD outputs into a single sampled data stream (2) optimisation of the physical characteristics of the SPAD array itself. Analogue circuit approaches to the latter problem include commercial analogue silicon photomultipliers (SiPMs) [19] as well as custom CMOS active analogue SiPM achieving 200Mb/s [20]. Digital silicon photomultipliers (dSiPMs) [21] first proposed for PET have also been applied to VLC providing direct integration of a “light to digital” electronic receiver with advantages of low power, circuit area and compatibility with existing DSP.

In this paper, we investigate theoretically and experimentally the trade-offs in selection of the number, dead time, fill-factor and area of unit cells in a dSiPM receiver approach in order to achieve certain sensitivity, dynamic

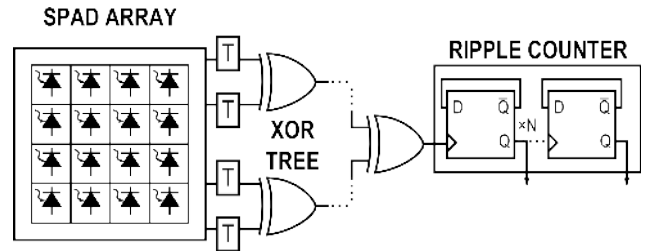


Figure 1. XOR-based dSiPM example - SPAD cells are digitally combined through a Toggle+XOR Tree sharing a common counting circuit.

range (DR), linearity and signal to noise ratio (SNR) properties. The results are relevant to future analogue and digital dSiPM VLC receiver architectures, particularly the case of bandwidth limited links such as found in free-space GaN LED [22] or polymer optical fibre (POF) [23]. In these cases, the potential SNR improvement offered by dSiPM receivers over APD or PIN solutions [8] requires use of higher order of modulation schemes (e.g. OFDM, PAM [10], [13]) and linear transmitter and receiver characteristics.

Our study focusses on a recently proposed technique to combine multiple cell outputs into a data stream; the XOR tree (Fig. 1). This approach has been shown to be effective in recent PET dSiPMs and proof-of-concept VLC receivers [11], [24]. A series of experimental XOR dSiPMs has been constructed in 130nm CMOS test chip allowing the number, diameter, dead time and dark count rate (DCR) of the SPAD cells in XOR dSiPM receiver front-ends to be varied. Measurements of important properties for communication system designers are provided allowing linearity, DR, SNR and photon detection efficiency (PDE) (or sensitivity) to be directly derived. In addition, non-linearity and saturation limits are studied allowing practical requirements to be set on received signal power. Although an XOR dSiPM has been used as the basis of this study, many results are valid for analogue SiPMs and other pulse-combining readouts, [21], [25], [26].

The paper examines two dSiPM receiver design scenarios (1) a chosen fixed unit cell area with no limitation on total area (hence number of cells) combined by one XOR tree or (2) a fixed total dSiPM area with the possibility of fitting more (but smaller) cells in the chosen area at the cost of fill-factor and sensitivity. Section II and

III develop theoretical models for the *DR* and linearity based on these two scenarios, respectively. A 130 nm CMOS dSiPM test chip is presented in Section IV and provides a comparison between modelled and measured optical characteristics including *DR*, sensitivity and *SNR* (Section V). Considerations on general dSiPM design and conclusions are given in Section VI and VII.

## II. DIGITAL SiPM WITH FIXED UNIT CELL AREA

To realise high count rate detectors, arrays of SPAD cells are manufactured together with timing or counting circuits in so-called silicon photomultipliers (SiPMs) [27], [28], [29]. As suggested by Mandai et al. [2], the structure of a SiPM can be optimised by designing arrays with outputs combined into a common pulse-combining readout channel. This technique allows timing or counting circuitry to be shared thus reducing the required silicon area and simplifying the read-out. The many advantages of digital aggregation of SPAD cells has led to the increasing popularity of digital silicon photon multipliers (dSiPMs) [21]. A typical way to digitally combine SPAD cells is represented by the use of an OR-tree preceded by a monostable pulse-shortener cell per cell [25], [26]. The limitation on the count rate due to the latter has been overcome by the replacement of monostables and OR tree respectively with toggle cells and XOR tree [11], [24], see Fig. 1, promising high count rates in optimised dSiPMs. To investigate the optimisation process, we analyse the performance of such detectors in terms of photon detection efficiency and dynamic range. Together with the estimation of such figures of merit under a selection of assumptions, we provide a comparison with experimental data to verify the effectiveness of the two approaches.

One typical option in dSiPM design is to aggregate a certain number of unit cells with the same active area  $A_{\text{cell}}$ <sup>1</sup> and dead time  $\tau_d$ . It is of interest to understand how the dynamic range changes when different number cells are aggregated into a common pulse-combining readout receiver.

### A. SiPM Photon Detection Efficiency

For an individual dSiPM unit cell, the photon detection efficiency ( $PDE_1$ ) is calculated as the ratio between the count rate  $m$  and the rate  $n$  of the incident photons on the total area of the SPAD cell including any per-SPAD circuitry such as guard rings, well isolation, quench circuits, memory, buffering or pulse combining electronics. The fill-factor ( $FF$ ) is the ratio of photosensitive area to SPAD unit cell area. For an SiPM made of identical cells, the total  $PDE$  is the same as a single cell since both the count rate  $m_{\text{TOT}}$ , assuming no loss of counts (low light level), and the incident photons  $n(N)$  scale linearly with the number of diodes:

$$PDE(N) = \frac{m_{\text{TOT}}}{n(N)} = PDE_1 \quad (1)$$

While at moderate light level the total count rate of a dSiPM is proportional to the incident photon rate (dSiPM

<sup>1</sup>The active area of each proposed cell can be calculated from the pitch and the fill factor as:  $A_{\text{cell}} = \text{pitch}^2 \times FF$

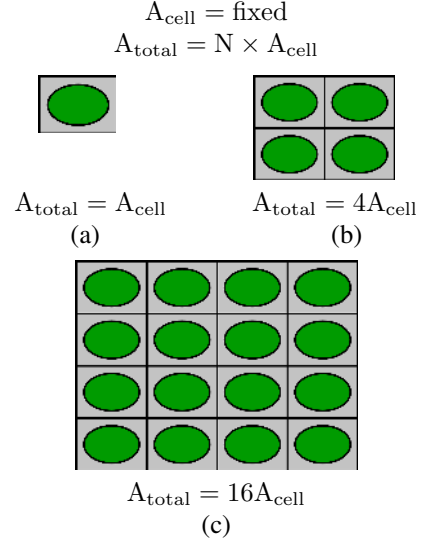


Figure 2. **Fixed unit cell area for dSiPM design** - A different number of cells with fixed area can be integrated into arrays. The total area of the dSiPM scales linearly with the number of cells:  $A_{\text{total}} = N \times A_{\text{cell}}$ .

*linear region*), at high light levels, due to detector saturation a loss of registered counts is observed. This region will be referred to as *saturation region*.

### B. Dynamic Range

We define as dynamic range *DR* the ratio between the maximum registered count rate and the noise level known as the dark count rate (*DCR*) of the dSiPM:

$$DR(\text{dB}) = 20 \cdot \log_{10} \frac{m_{\text{MAX}}}{DCR} \quad (2)$$

For a dSiPM made of  $N$  identical unit cells, the *DCR* is linear with the number of cells, hence we write:

$$DCR(N) = N \cdot DCR_1 \quad (3)$$

At high incident photon rates, a dSiPM enters its saturation regime where, due to count loss, the count rate is not proportional to the incident photon rate. The count loss can be caused by either the saturation of the single diodes, or the bandwidth limitation imposed by the pulse-combining readout channel. The former is described by the dSiPM unit cell dead time  $\tau_d$  while the latter can be described by an equivalent maximum frequency  $f_{\text{BW}}$  limiting the recorded count rate. The maximum count rate  $m_{\text{MAX}}$  for a dSiPM is modelled as:

$$m_{\text{MAX}}(N) = f_{\text{BW}} \left( 1 - e^{-N \cdot m_1 / f_{\text{BW}}} \right) \quad (4)$$

where  $m_1$  is the maximum detection rate of an individual cell equal to  $1/(e \cdot \tau_d)$  for a passive recharge SPAD cell [30]. This expression fits experimental data, see Section IV, with a level of confidence described by a reduced chi-squared  $\tilde{\chi}^2 \sim 0.9$ .

We then substitute (4) and (3) in (2):

$$DR(\text{dB}) = 20 \cdot \log_{10} \frac{f_{\text{BW}} \left( 1 - e^{-N / (e \cdot \tau_d \cdot f_{\text{BW}})} \right)}{N \cdot DCR_1} \quad (5)$$

For  $N \ll e \cdot \tau_d \cdot f_{\text{BW}}$  the maximum count rate is:

$$m_{\text{MAX}}(N) \sim \frac{N}{e \cdot \tau_d} \quad (6)$$

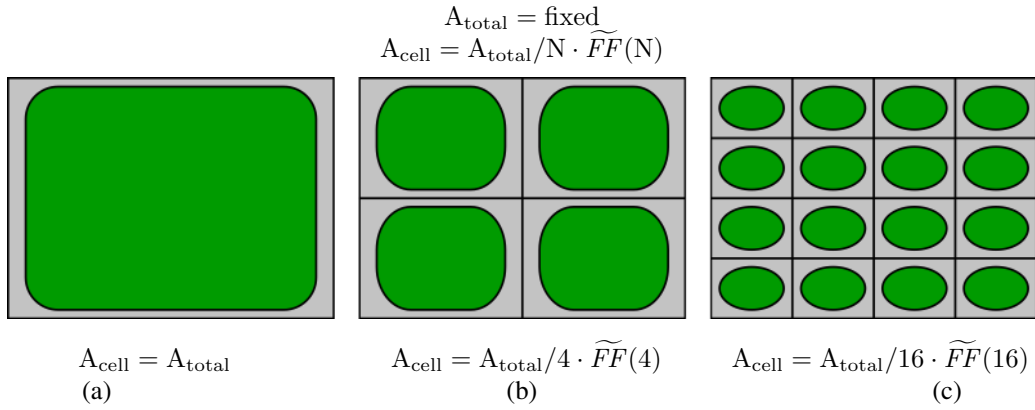


Figure 3. **Fixed area for dSiPM design** - In a total given area, a different size and number of cells can be fitted. Shrinking the dSiPM unit cells causes lower fill factor but lower dark count rates.

Therefore (2) becomes:

$$DR(\text{dB}) \sim 20 \cdot \log_{10} \frac{1}{e \cdot DCR_1 \cdot \tau_d}, \text{ for } N \ll e \cdot \tau_d \cdot f_{\text{BW}} \quad (7)$$

For a high number of dSiPM cells  $N \gg e \cdot \tau_d \cdot f_{\text{BW}}$  the dSiPM enters the saturation region, i.e. presents count loss due to too many cells being aggregated into a common pulse-combining readout. The dynamic range is therefore:

$$DR(\text{dB}) \sim 20 \cdot \log_{10} \frac{f_{\text{BW}}}{DCR_1 \cdot N}, \text{ for } N \gg e \cdot \tau_d \cdot f_{\text{BW}} \quad (8)$$

We conclude that the dynamic range is constant as long as the number of aggregated cells is below a limit depending on the unit cell dead time and the bandwidth limitation of the pulse-combining readout channel:

$$N \ll e \cdot \tau_d \cdot f_{\text{BW}} \quad (9)$$

Although aggregating a higher number of cells allows a larger area to be covered while not affecting the photon detection efficiency according to (1), the dynamic range is compromised according to (8).

### III. DIGITAL SiPM WITH FIXED TOTAL AREA

If a dSiPM has to be designed to cover a total active area  $A_{\text{total}}$ , it is relevant to understand how dividing the available area into  $N$  cells influences the photon detection efficiency and the dynamic range of the resulting dSiPM. Fig. 3 shows an example of such a scenario where a different number of cells can be designed in the given available area. Note that smaller unit cells have lower fill factor due to the surrounding electronics. We therefore analyse the counting performance of the dSiPM under this possible scenario.

#### A. SiPM Photon Detection Efficiency

To calculate the photon detection efficiency of a dSiPM under such an assumption, we need to consider one important effect of shrinking the dSiPM unit cells: the decreasing fill factor due to the in-pixel electronics. When  $N$  cells are fabricated in the given area, each will have a fill factor of  $FF(N)$ , therefore:

$$PDE(N) = PDE_1 \cdot \widetilde{FF}(N) \quad (10)$$

where  $PDE_1$  is the  $PDE$  of the detector when only one cell (of  $FF_1$  fill factor) is fitted in the available area, and  $\widetilde{FF}(N)$  is the reduction of fill factor when the area is populated by  $N$  cells:

$$\widetilde{FF}(N) = \frac{FF(N)}{FF_1} \quad (11)$$

Such term is highly dependent on the dSiPM unit cell design and will not be modelled in this work and will be left as a factor to be plugged in for final calculations.

#### B. Dynamic Range

We now calculate the  $DCR$  and the maximum signal rate of the dSiPM for a fixed total area. It is well known that the  $DCR$  scales with the active area of the dSiPM [31], therefore in the scenario of  $N$  cells fitted into a constant total area, we can approximate the  $DCR$  over the dSiPM as:

$$DCR(N) = DCR_1 \cdot \widetilde{FF}(N) \quad (12)$$

where  $DCR_1$  is the  $DCR$  of the device when only one cell is fitted into the total available area.

For the calculation of the maximum count rate, two aspects need to be considered: when smaller dSiPM unit cells are fabricated, they typically exhibit lower dead times compared to bigger cells due to the size of the device capacitance. Therefore the maximum count rate can be written as a variation of (4):

$$m_{\text{MAX}}(N) = f_{\text{BW}} \left( 1 - e^{-N \cdot m_1(N)/f_{\text{BW}}} \right) \quad (13)$$

where  $m_1(N) = 1/(e \cdot \tau_d(N))$ . However, when the number  $N$  increases, the maximum count rate is no longer dominated by the individual dSiPM unit cell dead time  $\tau_d(N)$ , instead it is limited by the term  $f_{\text{BW}}$  describing the bandwidth of the pulse-combining readout. In this work, we concentrate on this behaviour rather than well known saturation due to dead time. Therefore, for simplicity, let us consider the variation on the dead time as second order effect so that we can replace the term  $\tau_d(N)$  with a constant  $\tau_d$  and use (4) instead of the more generic (13). We can now estimate the dynamic range as:

$$DR(\text{dB}) = 20 \cdot \log_{10} \frac{f_{\text{BW}} \left( 1 - e^{-N \cdot m_1/f_{\text{BW}}} \right)}{DCR_1 \cdot \widetilde{FF}(N)} \quad (14)$$

Table I  
DYNAMIC RANGE AND PHOTON DETECTION EFFICIENCY - DEFINITION AND THEORETICAL EXPRESSIONS UNDER THE TWO SCENARIOS OF SECTIONS II AND III

	Definition	Fixed Total dSiPM Area	Fixed dSiPM Area
<b>Linear Dynamic Range</b>	$DR(\text{dB}) = 20 \cdot \log_{10} \frac{m_{\text{MAX}}}{m_{\text{MIN}}}$	$DR(\text{dB}) = 20 \cdot \log_{10} \frac{f_{\text{BW}} \left( 1 - e^{-N/(e \cdot \tau_d \cdot f_{\text{BW}})} \right)}{N \cdot DCR_1}$	$20 \cdot \log_{10} \frac{f_{\text{BW}} \left( 1 - e^{-N \cdot m_1 / f_{\text{BW}}} \right)}{DCR_1 \cdot \widetilde{FF}(N)}$
<b>Photon Detection Efficiency</b>	$PDE(N) = \frac{m_{\text{TOT}}}{n}$	$PDE(N) = PDE_1$	$PDE(N) = PDE_1 \cdot \widetilde{FF}(N)$

The two limits regarding the number of unit cells and the minimum dead time are here presented:

$$DR(\text{dB}) \sim 20 \cdot \log_{10} \frac{N}{e \cdot \tau_d \cdot DCR_1 \cdot \widetilde{FF}(N)}, \text{ for } N \ll e \cdot \tau_d \cdot f_{\text{BW}} \quad (15)$$

$$DR(\text{dB}) = 20 \cdot \log_{10} \frac{f_{\text{BW}}}{DCR_1 \cdot \widetilde{FF}(N)}, \text{ for } N \gg e \cdot \tau_d \cdot f_{\text{BW}} \quad (16)$$

Results from both analyses are summarised in Table I and will be compared to experimental data in the next section.

#### IV. TEST CHIP

We present now a test chip manufactured in STMicroelectronics 130nm imaging process as shown in Fig. 4. Two sets of dSiPMs of previously published SPAD structures have been designed, [31], [32]. The crosstalk, less than 1%, has not been included in the analysis since considered a second order effect. The first set is composed by a  $16 \times 16$  XOR-combined with  $7\mu\text{m}$  pitch shared-well passively quenched SPAD cells. The second set consists of five pitch variants of  $4 \times 4$  arrays of the same structure, with external combination logic. The 16 cell outputs from each dSiPM are multiplexed onto selectable XOR and OR trees. Table II summarises the properties of the designed dSiPM. In our test dSiPMs, the unit cells contain only SPADs wired to readout electronics placed at the exterior of the arrays. This has been done to avoid interactions between SPADs and neighbouring electronics. The fill-factor is therefore higher than practically achievable in larger dSiPM arrays but there is no loss of generality in our model. A 16bit on-chip ripple counter provides the counts  $M$  of the selected dSiPM (and relative enabled cells) for a controlled exposure time  $T_{\text{exp}}$  from which the average count rate  $m$  is calculated as  $m = M/T_{\text{exp}}$ .

The SPAD cells were biased to the same average dead time of  $\tau_d \simeq 5\text{ns}$  in order to fulfil the assumption useful for calculations. The bandwidth of the pulse-combining readout consisting of the XOR tree and the on-chip counters is measured as  $f_{\text{BW}} = 1.01\text{GHz}$ .

For the experiments, we illuminate the detector with an LED with dominant wavelength  $\lambda = 470\text{nm}$ . For each light intensity we record the average count rate. The exposure time has been set to a range from  $2\mu\text{s}$  to  $0.6\text{ms}$  in order to have significant number of counts in the 8bit on-chip ripple counter and to avoid its saturation over all

Table II  
DSiPM - PROPERTIES AND PARAMETERS OF UNIT CELLS.

dSiPM	Unit Cell Pitch ( $\mu\text{m}$ )	Number of Cells	Fill Factor (%)	Dead Time
D1	7	$16 \times 16$	6.4	$\tau_d \simeq 5\text{ns}$
D2	9	$4 \times 4$	18.7	
D3	13	$4 \times 4$	37.4	
D4	18.62	$4 \times 4$	73.6	
D5	34.62	$4 \times 4$	85.4	

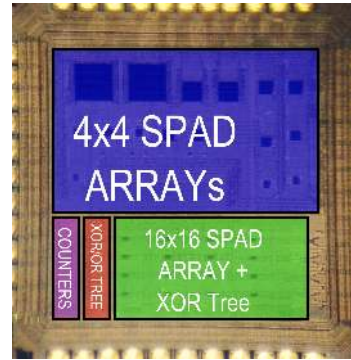


Figure 4. **Test Chip** - A selected samples of dSiPMs has been manufactured on the same test chip. All the varieties of dSiPMs have been combined through toggle cells and a common XOR tree outside the cells.

the desired light levels. To improve the statistics, each exposure is repeated for 500 iterations taking advantage of the off-chip memory (PC) to store larger and therefore more statistically significant data. For all the obtained count rates, we report the mean value and the standard deviation in error bar plots.

##### A. DSiPM D1

We first select the dSiPM D1 to perform light intensity sweeps for an increasing number of activated cells from 1 to the maximum 256 available on chip. This mimics the assumptions of Section II.

We start by enabling an increasing number of activated cells. We show three cases in Fig. 5. With only one cell activated (purple line), the dSiPM shows a low  $DCR$  level but a limited maximum count rate. The middle green line represents the intermediate case of number of cells  $N = 16$ . In this configuration, the maximum count rate has significantly risen and the dynamic range is not affected. The extreme case of all 256 cells activated, shown as a light blue line, confirms the model employed in Section

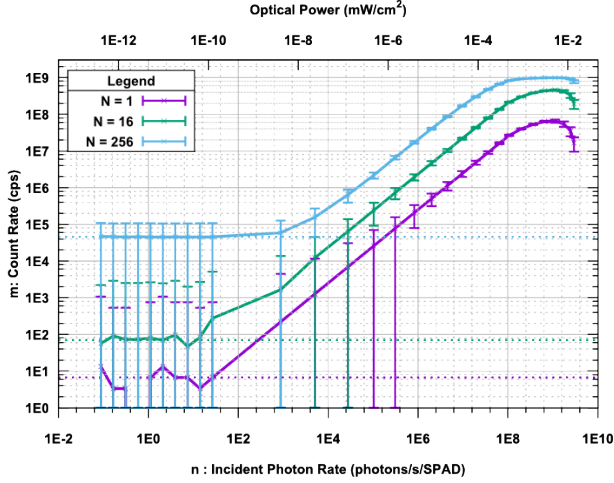


Figure 5. **Fixed dSiPM unit cell area** - Three examples of dSiPMs are shown. Aggregating more identical cells increases the photon detection efficiency but limits the dynamic range over an optimal number of cells  $N_{\text{best}}$ .

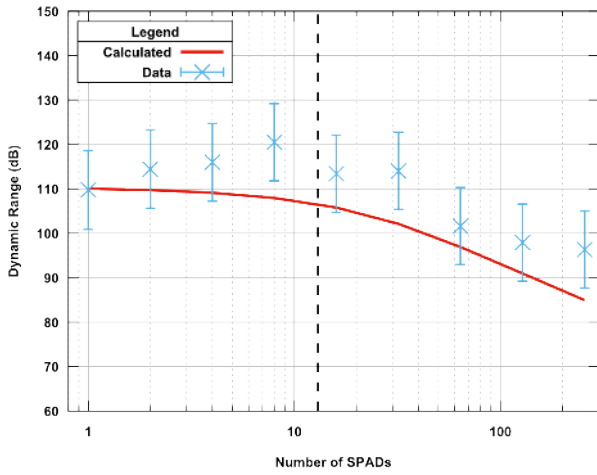


Figure 6. **dSiPM** - The dynamic range is measured activating a crescent number of unit cells in the  $16 \times 16$  array. The solid lines show the estimation from the obtained equations. The dashed vertical lines highlight the limit case expressed by (9).

II: aggregating too many unit cells does not increase the maximum count rate, due to detector saturation, but highly affects the dynamic range by increasing the *DCR* level. Fig. 6 shows the measured dynamic range over a different number of enabled cells. The deviation from the model has to be ascribed to the non-uniformity of the dSiPMs which is assumed in the modelling. However, the closeness of the error bar to the predicted line confirms (5). The experiment shows the importance of keeping the number of aggregated cells low enough in order to avoid the pulse-combining readout channel saturation. In large dSiPM design, this implies that a multi-channel approach is more efficient in terms of higher dynamic range, such as the use of an array of mini-dSiPMs, [2], [26].

### B. DSiPM D2-D5

The second set of dSiPMs (D2-D5) allows the assumptions of Section III to be experimentally validated. We choose the area occupied by a single cell of the dSiPM D5 in Table II as the reference total area. In the

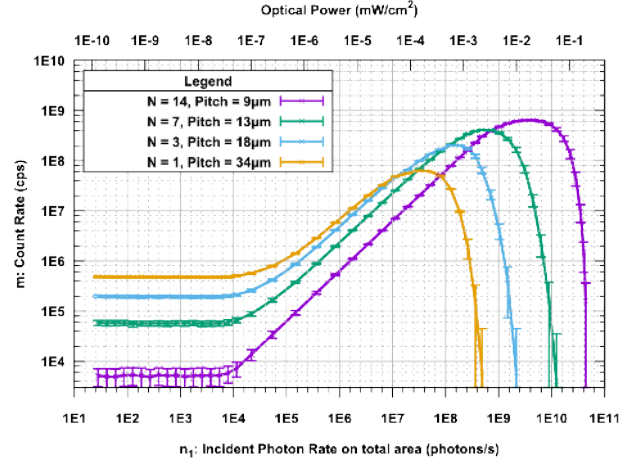


Figure 7. **Fixed total area photon transfer curve** - Different configurations possible for a fixed total area of the detector are compared in terms of count rate.

chosen area, one can then fit:

- 1 cell from D5
- 3 cells from D4
- 7 cells from D3
- 14 cells from D2

Therefore, we perform the light intensity sweeps choosing the desired dSiPM and the number of activated cells. The photon transfer curve for each configuration is shown in Fig. 7. Moreover, we provide direct measurements of the photon detection efficiency and the dynamic range in Fig. 8 to compare the data to the proposed equation model, respectively (10) and (14). As expected, having a larger number of smaller cells highly increases the DR, due to lower DCRs and higher maximum count rates, while the photon detection efficiency is negatively affected by the reduction of fill factor.

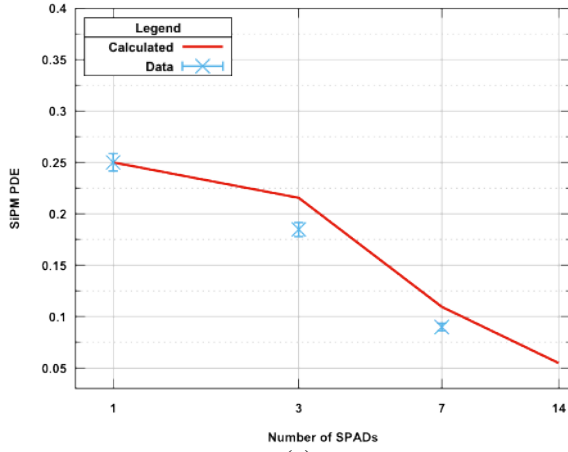
## V. NOISE AND SIGNAL-TO-NOISE RATIO

From the obtained data, additional considerations on noise can be derived. We show in Fig. 9(a) the noise as the standard deviation of the measured counts (data points) compared directly with the photon shot noise calculated as the square root of the mean counts (solid line) both normalised for a unit exposure time. These experimental data demonstrate detection rates are limited only by photon shot noise in linear regime of operation, i.e. in the region where the count rate is proportional to the incident photon rate, essential for optical communications.

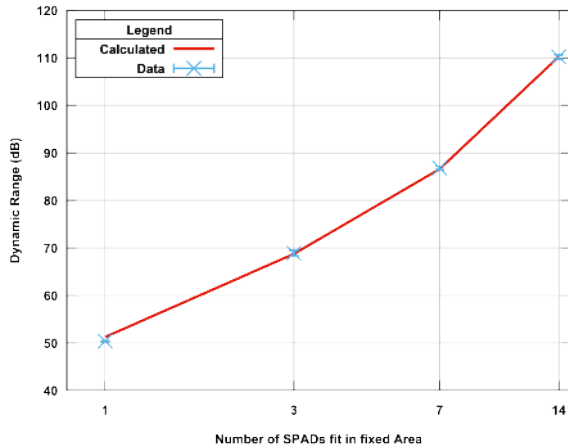
Moreover, we calculate the signal-to-noise ratio (*SNR*) for all the light intensity points as:

$$SNR = 20 \log_{10} \frac{M}{\sigma_M} \quad (17)$$

Results are shown in Fig. 9(b) where the mean value and the standard deviation of the counts have been again normalised for a unit exposure time. We confirm that the *SNR* increases linearly with the square root of the number of collected photons before the count loss due to the dSiPM saturation. Although smaller unit cells (purple line) show lower *SNR* compared to larger ones (yellow



(a)



(b)

Figure 8. **Fixed total area** - The change in the photon detection efficiency (a) and dynamic range (b) is measured for different number of unit cells fitted in a total area.

line) due to fewer collected photons, they reach a higher maximum thanks to a higher saturation threshold. The graph also shows the noise floor region: below a certain light level, the constant count rate measured from the chip is pure  $DCR$  and therefore does not contain signal information.

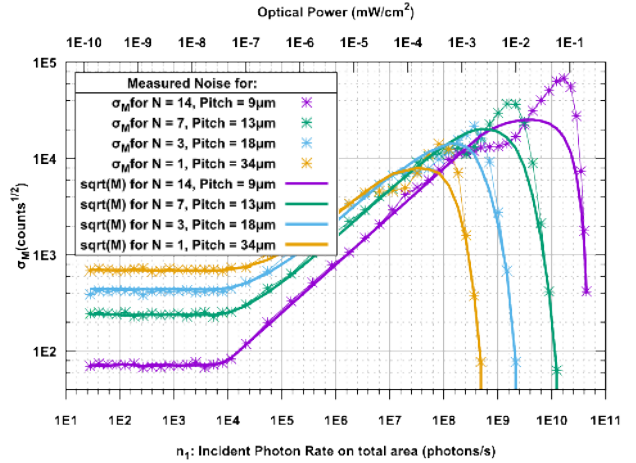
## VI. CONSIDERATIONS ON GENERAL DSiPM DESIGNS

The modelling equations here proposed have been derived under a selection of assumptions. We now discuss how to apply necessary modifications in more general SiPM designs.

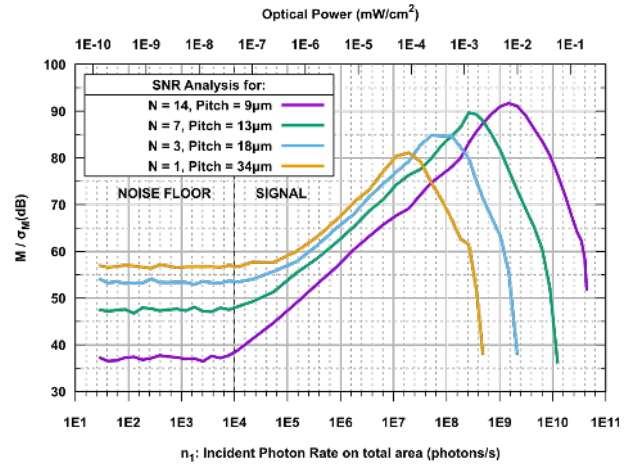
*a) Uniformity of the dSiPM:* one of the first assumptions made in the modelling is that the dSiPM consists of identical unit cells, therefore the dSiPM is supposed to have a strong uniformity in terms of fill factor and dark count rate. While the former is generally true, the latter is typically not verified especially in large dSiPMs. When more cells are enabled in a large dSiPM (case described in Section II) the calculation of the total  $DCR$  proposed in (3) can be replaced by the more general:

$$DCR(N) = \sum_{i=1}^N DCR_i \quad (18)$$

which will then replace the denominator of (5). When aggregating smaller and smaller cells, the approximation



(a)



(b)

Figure 9. **Signal-to-Noise** - For the set of dSiPMs shown in Fig. 7, (a) the measured noise (*data points*) are plotted together with the ideal photon shot noise limit (*solid line*) and (b) the normalised signal over the standard deviation data are plotted for the whole range of light levels.

proposed by (12) might not be satisfied and therefore the general term  $DCR(N)$  should replace the denominator of (14). Similarly, if smaller cells show significant lower dead times, the assumption of  $\tau_d(N) = \tau_d$  can be dropped and the general expression of the maximum count rate (13) should be used in the dynamic range calculation. As previously stated, the dependency on the dead time becomes negligible in large pulse-combining dSiPMs where the main limitation to the dynamic range is given by the common readout bandwidth.

*b) Interconnection/Readout impact:* the maximum signal rate of the dSiPM has been shown to depend on both the dead time of the unit cells and on the pulse-combining readout bandwidth. The latter dependency becomes dominant when a large number of cells is combined onto a common readout. It is therefore useful during the design process to estimate the bandwidth of the pulse-combining readout taking into account also digital circuit switching speeds and interconnect parasitics. This will allow an estimation of the parameter  $f_{BW}$ , present in all the proposed equations, and therefore of the dynamic range.

*c) In-Pixel Electronics:* the model here proposed has been verified with a test chip containing small in-pixel electronics (only buffers and toggle cells) while the main XOR tree is shared outside the cell arrays.

However, typical dSiPMs contain additional cells, such as monostable circuits and OR cells. The impact of such design choice on the model is the following: first of all, the fill factor of the dSiPM unit cells decreases due to the occupying cells. Therefore the parameter  $FF$  present in the equations needs to take into the account such reduction. Moreover, having in-pixel electronics might impact the single-channel bandwidth, which yet again can be simulated and included in the model by estimating the proposed parameter  $f_{BW}$ . With these parameters, the model allows general conclusions to be derived as with the example test chip proposed in this work.

## VII. CONCLUSIONS

We have calculated the photon detection efficiency and dynamic range of digital silicon photomultipliers depending on typical design parameters.

We have demonstrated that a high dynamic range, exceeding 110dB, can be obtained by using an array of small SPAD cells,  $7\mu\text{m}$  pitch, with an optimal number of activated cells  $\sim 16$ . We have moreover proven single photon shot noise count rates in the linear region of operation of the dSiPM. All these results can be applied to the modelling and design of future dSiPM receiver architectures.

## REFERENCES

- [1] S. Seifert, G. van der Lei, H. T. van Dam, and D. R. Schaart, "First Characterization of a Digital SiPM Based Time-of-Flight PET Detector with 1 mm Spatial Resolution." *Phys. Med. Biol.*, vol. 58, no. 9, pp. 3061–74, 2013.
- [2] S. Mandai and E. Charbon, "Multi-channel digital SiPMs: Concept, analysis and implementation," in *IEEE Nucl. Sci. Symp. Conf. Rec.*, no. 1, 2012, pp. 1840–1844.
- [3] C. Niclass, M. Soga, H. Matsubara, M. Ogawa, and M. Kagami, "A 0.18- $\mu\text{m}$  CMOS SoC for a 100-m-Range 10-Frame/s 200 96-Pixel Time-of-Flight Depth Sensor," vol. 49, no. 1, pp. 315–330, 2014.
- [4] P. Kumar, E. Charbon, R. B. Staszewski, and A. Borowski, "Low power time-of-flight 3D imager system in standard CMOS," *2012 19th IEEE Int. Conf. Electron. Circuits, Syst. (ICECS 2012)*, pp. 941–944, dec 2012.
- [5] D. D.-U. Li, S. Ameer-Beg, J. Arlt, D. Tyndall, R. Walker, D. R. Matthews, V. Visitskul, J. Richardson, and R. K. Henderson, "Time-domain fluorescence lifetime imaging techniques suitable for solid-state imaging sensor arrays." *Sensors (Basel)*, vol. 12, no. 5, pp. 5650–69, jan 2012.
- [6] A. C. Therrien, S. Member, B.-I. Bérubé, S. A. Charlebois, R. Lecomte, R. Fontaine, and S. Member, "Modeling of Single Photon Avalanche Diode Array Detectors for PET Applications," vol. 61, no. 1, pp. 14–22, 2014.
- [7] Y. Li, S. Videv, M. Abdallah, K. Qaraq, M. Uysal, and H. Haas, "Single Photon Avalanche Diode ( SPAD ) VLC System and Application to Downhole Monitoring," in *GlobeCom*, 2014, pp. 2108–2113.
- [8] S. Chick, R. Coath, R. Sellahewa, R. Turchetta, T. Leitner, and A. Fenigstein, "Dead Time Compensation in CMOS Single Photon Avalanche Diodes with Active Quenching and External Reset," *IEEE Trans. Electron Devices*, vol. 61, no. 8, pp. 2725–2731, 2014.
- [9] E. Fisher, I. Underwood, and R. Henderson, "A reconfigurable 14-bit 60GPhoton/s Single-Photon receiver for visible light communications," *Eur. Solid-State Circuits Conf.*, pp. 85–88, 2012.
- [10] Y. Li, M. Safari, R. Henderson, and H. Haas, "Optical OFDM With Single-Photon Avalanche Diode," vol. 27, no. 9, pp. 943–946, 2015.
- [11] O. Almer, D. Tsonev, N. A. W. Dutton, T. A. Abbas, S. Videv, S. Gneccchi, H. Haas, and R. K. Henderson, "A SPAD-based Visible Light Communications Receiver Employing Higher Order Modulation Schemes," *IEEE Globecom*, 2015.
- [12] D. Chitnis and S. Collins, "A SPAD-based photon detecting system for optical communications," *J. Light. Technol.*, vol. 32, no. 10, pp. 2028–2034, 2014.
- [13] O. Almer, N. A. W. Dutton, T. A. Abbas, S. Gneccchi, and R. K. Henderson, "4-PAM Visible Light Communications with a XOR-tree Digital Silicon Photomultiplier," in *IEEE Summer Top. Meet. Ser.*, 2015, pp. 2–3.
- [14] S. Collins, R. Mulyawan, S. Rajbhandari, H. Chun, G. E. Faulkner, and D. C. O. Brien, "A Simple Wide Field of View Concentrator for Free Space Visible Light Communications," vol. 4, no. 2, 2015, pp. 43–44.
- [15] H. Elgala, R. Mesleh, and H. Haas, "Indoor optical wireless communication: Potential and state-of-the-art," *IEEE Commun. Mag.*, vol. 49, no. 9, pp. 56–62, 2011.
- [16] a. M. Khalid, G. Cossu, R. Corsini, P. Choudhury, and E. Ciaramella, "1-Gb/s transmission over a phosphorescent white LED by using rate-adaptive discrete multitone modulation," *IEEE Photonics J.*, vol. 4, no. 5, pp. 1465–1473, 2012.
- [17] D. Tsonev, H. Chun, S. Rajbhandari, J. J. D. McKendry, S. Videv, E. Gu, M. Haji, S. Watson, A. E. Kelly, G. Faulkner, M. D. Dawson, H. Haas, and D. O'Brien, "A 3-Gb/s single-LED OFDM-based wireless VLC link using a gallium nitride  $\mu$  LED," *IEEE Photonics Technol. Lett.*, vol. 26, no. 7, pp. 637–640, 2014.
- [18] G. Cossu, A. M. Khalid, P. Choudhury, R. Corsini, and E. Ciaramella, "3.4 Gbit/s visible optical wireless transmission based on RGB LED." *Opt. Express*, vol. 20, no. 26, pp. B501–6, 2012.
- [19] G. Zhang, C. Yu, C. Zhu, and L. Liu, "Feasibility study of Multi-Pixel Photon Counter serving as the detector in digital optical communications," *Optik (Stuttg.)*, vol. 124, no. 22, pp. 5781–5786, 2013.
- [20] D. Chitnis, L. Zhang, H. Chun, S. Rajbhandari, and G. Faulkner, "A 200 Mb / s VLC demonstration with a SPAD based receiver," in *IEEE Summer Top. Meet. Ser.*, vol. 3, 2015, pp. 226–227.
- [21] T. Frach, G. Prescher, C. Degenhardt, R. de Gruyter, A. Schmitz, and R. Ballizany, "The Digital Silicon Photomultiplier - Principle of Operation and Intrinsic Detector Performance," *2009 IEEE Nucl. Sci. Symp. Conf. Rec.*, pp. 1959–1965, oct 2009.
- [22] S. Zhang, S. Watson, J. J. D. McKendry, D. Massoubre, A. Cogman, E. Gu, R. K. Henderson, A. E. Kelly, and M. D. Dawson, "1.5 Gbit/s Multi-Channel Visible Light Communications Using CMOS-Controlled GaN-Based LEDs," *J. Light. Technol.*, vol. 31, no. 8, pp. 1211–1216, 2013.
- [23] I. Möllers, D. Jäger, R. Gaudino, A. Nocivelli, H. Kragl, O. Ziemann, N. Weber, T. Koonen, C. Lezzi, A. Bluschke, and S. Randel, "Plastic optical fiber technology for reliable home networking: Overview and results of the eu project pof-all - [Topics in Optical Communications]," *IEEE Commun. Mag.*, vol. 47, no. 8, pp. 58–68, 2009.
- [24] N. A. W. Dutton, S. Gneccchi, L. Parmesan, A. J. Holmes, B. Rae, L. A. Grant, and R. K. Henderson, "A Time-Correlated Single-Photon-Counting Sensor with 14GS/s Histogramming Time-to-Digital Converter," in *Solid- State Circuits Conf. - (ISSCC), 2015 IEEE Int.*, 2015, pp. 204–206.
- [25] C. Niclass, M. Soga, H. Matsubara, and S. Kato, "A 100m-range 10-frame/s 340x96-pixel time-of-flight depth sensor in 0.18 $\mu\text{m}$  CMOS," in *Eur. Solid-State Circuits Conf.*, 2011, pp. 107–110.
- [26] L. H. C. Braga, S. Member, L. Gasparini, L. Grant, R. K. Henderson, N. Massari, M. Perenzoni, D. Stoppa, S. Member, and R. Walker, "A Fully Digital 8x16 SiPM Array for PET Applications With Per-Pixel TDCs and Real-Time Energy Output," *IEEE J. Solid-State Circuits*, vol. 49, no. 1, pp. 301–314, 2014.
- [27] O. Soto, R. Rojas, S. Kuleshov, H. Hakobyan, A. Toro, and W. K. Brooks, "Characterization of novel Hamamatsu Multi Pixel Photon Counter (MPPC) arrays for the GlueX experiment," *Nucl. Instruments Methods Phys. Res. Sect. A Accel. Spectrometers, Detect. Assoc. Equip.*, vol. 732, pp. 431–436, 2013.
- [28] I. Malass and W. Uhring, "SiPM based smart pixel for photon counting integrated streak camera," *Des. Archit. Signal Image Process. (DASIP), Conf.*, pp. 135–140, 2013.
- [29] P. Buzhan, B. Dolgoshein, and A. Ilyin, "An Advanced Study of Silicon Photomultiplier," in *Proc. 7th Int. Conf. ICATPP-7*, vol. 23, Como, Italy, 2001, pp. 28–41.
- [30] A. Eisele and R. Henderson, "185 MHz Count Rate, 139 dB Dynamic Range Single-Photon Avalanche Diode with Active Quenching Circuit in 130nm CMOS Technology," in *2011 Int. Images Sens. Work.*, 2011, pp. 6–8.
- [31] J. A. Richardson, E. A. G. Webster, L. A. Grant, and R. K. Henderson, "Scaleable Single-Photon Avalanche Diode Structures in Nanometer CMOS Technology," *IEEE Trans. Electron Devices*, vol. 58, no. 7, pp. 2028–2035, jul 2011.
- [32] R. J. Walker, E. A. G. Webster, J. Li, N. Massari, and R. K. Henderson, "High Fill Factor Digital Silicon Photomultiplier Structures in 130nm CMOS Imaging Technology," *IEEE Nucl. Sci. Symp. Conf. Rec.*, pp. 1945–1948, 2012.