

Published in final edited form as:

Crit Rev Biomed Eng. 2014 ; 42(1): 85–93.

Approaches for modeling magnetic nanoparticle dynamics

Daniel B Reeves^{a)} and John B Weaver^{b)}

Dept. Physics and Astronomy, Dartmouth College, Hanover NH 03755

Abstract

Magnetic nanoparticles are useful biological probes as well as therapeutic agents. There have been several approaches used to model nanoparticle magnetization dynamics for both Brownian as well as Néel rotation. The magnetizations are often of interest and can be compared with experimental results. Here we summarize these approaches including the Stoner-Wohlfarth approach, and stochastic approaches including thermal fluctuations. Non-equilibrium related temperature effects can be described by a distribution function approach (Fokker-Planck equation) or a stochastic differential equation (Langevin equation). Approximate models in several regimes can be derived from these general approaches to simplify implementation.

Keywords

Stochastic modeling; magnetic nanoparticles; Fokker-Planck; Langevin equation

I. INTRODUCTION AND NANOPARTICLE APPLICATIONS

Magnetic nanoparticles (MNPs) are useful in many biophysical and medical applications because they can be remotely controlled and monitored with magnetic fields. For these applications, it is important to model the dynamics of the particles; and many approaches have been used previously to do so. In this case ‘modeling’ means simulating the magnetizations of the particles over time to study how different variables (e.g., field strength, anisotropy) affect their dynamics. In this review, we outline the major advances in MNP modeling including state-of-the-art techniques requiring numerical simulations and accounting for many experimentally verified phenomena. We also include approximate theories that admit analytical solutions, formulations that are easier to implement and other expressions that are more transparent.

A. Sensing and imaging

Magnetic nanoparticles can be used as sensors to detect properties of their local micro-environments when rotations couple MNP dynamics to the environmental parameters¹⁻³. For example, the concentration of specific molecules can be detected because their dynamics can be noticeably different when bound and unbound⁴. This is depicted in Fig. 1(a). Nanoparticle sensing is sensitive (down to 100pM of analyte and nanogram amounts of iron) and could potentially be used *in vivo* to detect changing concentrations over time. Aside

^{a)}dbr@dartmouth.edu..

^{b)}Also at Dept. of Radiology, Dartmouth Hitchcock Medical Center, Hanover NH 03755

from molecular sensing, MNPs have been used as probes to measure local temperatures⁵, viscosities⁶, and local environment rigidity⁷. MNPs have been used as MRI contrast agents⁸, and the developing technology of magnetic particle imaging (MPI). MPI uses the particles themselves as high-contrast imaging agents which hold the possibility for time-domain tracers⁹⁻¹¹.

B. MNP hyperthermia

Magnetic nanoparticle (MNP) hyperthermia is considered a potentially useful addition to current cancer treatment modalities^{12,13}. Nanoparticles can be directly injected¹⁴ or targeted biologically¹⁵ to achieve specific localized therapy. Furthermore, it appears cells ingest the MNPs, so cellular distribution may be possible¹⁶. If oscillating magnetic fields are applied to the sample, diverse physical mechanisms prevent the particles from following the field exactly, and thus energy is dissipated locally. This energy can be thought of as heat, and it has been shown that cytotoxic heating is possible^{17,18}. The principle of MNP hyperthermia can be conceptualized as in Fig. 1(b). It is important to design efficient heating agents and much work has been done to characterize MNPs and improve properties such as magnetic moment magnitude and anisotropy energy^{17,19}.

II. NANOPARTICLE ROTATIONS AND RELAXATION TIMES

There are two mechanisms for nanoparticles to rotate their magnetic moment μ . This is visualized in Fig. 2. The whole particle can rotate, as in so-called Brownian rotation, named for Robert Brown. The moment can rotate internally due to restructuring of electronic states. This so-called Néel rotation is named for Louis Néel, who first described the phenomenon while studying magnetic remanence in geological samples²⁰. The timescale for a perturbed system to return to equilibrium is called the ‘relaxation time’. This expression is different for each mechanism and depends on the parameters of interest.

A. Brownian relaxation time

The Brownian relaxation time, sometimes called the Einstein relaxation time²¹ based on Einstein’s original work to derive the timescale from Brownian motion arguments is written

$$\tau_B = \frac{3\eta V_h}{kT} \quad (1)$$

in terms of the suspension viscosity η , the hydrodynamic volume of the particle V_h and the thermal energy introduced with Boltzmann’s constant k and local temperature T .

B. Néel relaxation time

The Néel relaxation time derives from the thermal movements between two potential energy minima that arise from postulating a single anisotropy axis n (see Fig. 2). The anisotropy energy is written in terms of the anisotropy constant K and the magnetic core volume V_c ; the unitless ratio of this energy to the thermal energy is defined σ . Thus, the relaxation time can be expressed

$$\tau_N = \tau_0 e^{KV_c/kT} = \tau_0 e^\sigma \quad (2)$$

where the ‘event time’ τ_0 is often quoted as 10^{-10} s but is defined

$$\tau_0 = \frac{\mu}{2\gamma kT} \frac{(1+\alpha^2)}{\alpha} \quad (3)$$

in terms of the electron gyromagnetic ratio $\gamma = 1.76 \cdot 10^{11}$ Hz/T, a dimensionless magnetic damping parameter α , and the magnetic moment—calculated using M_s , the material dependent saturation magnetization as $\mu = M_s V_c$. More precise forms of the Néel relaxation time including additional factors of σ can be found in Ref.²².

C. WF relaxation time

W F Brown developed a more general characteristic time including applied fields²³. Letting $\sigma \gg 1$ he approximated this time to be

$$\tau_{WF} = \frac{\tau_N}{1 - \epsilon^2} \frac{e^{\sigma \epsilon^2}}{\cosh \xi + \epsilon \sinh \xi} \quad (4)$$

where the applied magnetic field H is accounted for with the unitless $\xi = \mu H/kT$. The ratio of anisotropic to magnetic energy is defined $E = \xi/2\sigma$ and the expression reduces to the equilibrium Néel time in the absence of an applied field.

D. Relaxation time considerations

An assumption found frequently in the literature is that the more prevalent relaxation mechanism is the one with the shorter relaxation time. The process is then approximated as parallel so the effective relaxation time is

$$\frac{1}{\tau_{eff}} = \frac{1}{\tau_N} + \frac{1}{\tau_B}. \quad (5)$$

To the best of our knowledge there has been no theoretical work that deals with Néel and Brownian relaxation simultaneously, so currently this expression is not derived from first principle and does not incorporate the fact that the processes could be coupled^{24,25}. Another consideration is that these relaxation times only hold for equilibrium conditions, and should not be applied without awareness of this constraint.

III. ANISOTROPIC HYSTERESIS LOOPS

The energy of a magnetic particle with a single anisotropy direction \mathbf{n} immersed in a magnetic field \mathbf{H} can be written

$$E = KV_c(\mathbf{n} \cdot \boldsymbol{\mu})^2 - \boldsymbol{\mu} \cdot \mathbf{H} \quad (6)$$

so that if the field is applied in the \hat{z} direction, we define the angle from the polar to be θ and the angle between the moment and the easy axis to be ϕ . Thus

$$E(\theta, \phi) = KV_c \sin^2(\theta - \phi) - \mu H \cos\theta. \quad (7)$$

To find the minimum energy, the equilibrium state of the particle, with respect to the moment direction θ we write

$$0 = \frac{\partial E(\theta, \phi)}{\partial \theta} = \mu H \sin\theta - 2KV_c \sin(\theta - \phi) \cos(\theta - \phi) \quad (8)$$

or

$$\epsilon = \frac{\sin[2(\theta - \phi)]}{2\sin\theta} \quad (9)$$

To ensure a minima we also require $\frac{\partial^2 E(\theta, \phi)}{\partial \theta^2} > 0$. Solving for the magnetization $M = \cos\theta$ and plotting this with respect to the normalized field E we find that the so-called Stoner-Wohlfarth hysteresis loop emerges²⁶.

This model is useful because the area of the loop indicates the energy dissipated when the particle is forced to change its orientation from one potential minima to another. This can then be used as a model for hyperthermic heating given particles with specific sizes, saturation magnetizations, and anisotropy constants. The weakness of the model is that it assumes no relaxational timescale for the process, thus neglecting that any phenomena depend on the frequency of the applied field. Still, models based on the theory have been extended to model heating more realistically²⁷.

IV. DIFFERENTIAL EQUATIONS FOR THE MAGNETIZATIONS

There exist more general methods to model the behaviors of the magnetic moments in various applied fields. This can be accomplished by describing the time dynamics of the magnetization using differential equations. Then the varying rotation methods as well as the specific conditions the particles experience in various applications can be simulated.

A. Brownian dynamics

A Brownian particle can be modeled phenomenologically with a balance of torques²⁸:

$$\tau = \underbrace{-\mu \mathbf{m} \times \mathbf{H}}_{\text{magnetic}} + \underbrace{6\eta V_h \mathbf{m} \times \frac{\partial \mathbf{m}}{\partial t}}_{\text{viscous}}. \quad (10)$$

We have neglected the acceleration term because the nanoparticles have a very small Reynold's number. Balancing this equation admits a differential equation for the magnetization which can be rewritten in terms of a unitless field $\alpha = \mu \mathbf{H} / kT$ and the Brownian relaxation time τ_B as

$$\frac{d\mathbf{m}}{dt} = \frac{(\mathbf{m} \times \alpha) \times \mathbf{m}}{2\tau_B} \quad (11)$$

This magnetization equation can be enhanced by including thermal fluctuations of the magnetization of the particles. There is no one general way to do this, and we will see the prescription for Néel particles is slightly different. Here we supplement the torques with the stochastic term $T_s = N / \tau_B$. The magnitude of this term depends on the relaxation time so that larger torques occur at higher temperatures and lower viscosities. We have also introduced the random variable N which we define to have

$$\langle N(x, t) \rangle = 0, \langle N(x, t) N(x', t') \rangle = \phi_{xx'} \phi(t - t') \quad (12)$$

This is a white frequency spectrum—so that in the time domain, it is controlled by a Dirac delta function—and the term only contributes if the correlation function is taken in the same spatial direction, a property encoded by the Kronecker delta²⁹. The noise is not truly white but provides the simplest inclusion of stochastic effects. We write the stochastic differential equation, called a Langevin equation³⁰ as

$$\frac{d\mathbf{m}}{dt} = \frac{(\mathbf{m} \times \alpha) \times \mathbf{m}}{2\tau_B} + \frac{N \times \mathbf{m}}{\sqrt{\tau_B}} \quad (13)$$

This equation is used to model Brownian particles and is amenable to changing local variables like fluid viscosity and temperature as well as externally applied fields.

B. Néel dynamics

The equation for the change in the magnetization of a Néel particle is the phenomenological Landau-Lifshitz-Gilbert (LLG) equation. This can be derived from the Larmor precession of a spin in a magnetic field with an added velocity-dependent damping term³¹. The normalized internal moment then rotates with

$$\frac{d\mathbf{m}}{dt} = \frac{\gamma}{1+\alpha^2} [\mathbf{H} \times \mathbf{m} + \alpha \mathbf{m} \times (\mathbf{H} \times \mathbf{m})]. \quad (14)$$

The effective field \mathbf{H} is used to include additional dynamics beyond the applied field³². For example we include an externally applied field with amplitude H_o and frequency ω , a field from the anisotropy axis \mathbf{n} ³³, and a stochastic field \mathbf{h} , so that

$$\mathbf{H} = \underbrace{H_o \hat{z} \cos \omega t}_{\text{applied}} + \underbrace{\frac{2\tilde{n}KV_a}{\mu} \mathbf{m} \cdot \mathbf{n}}_{\text{anisotropy}} + \underbrace{\mathbf{h}(t)}_{\text{stochastic}}. \quad (15)$$

In this case, the fluctuations are added to the model with an additional stochastic field, a white noise field with zero-mean and standard deviation parameterized by the nanoparticle variables

$$\langle \mathbf{h}(x, t) \rangle = 0, \langle \mathbf{h}(x, t) \mathbf{h}(x', t') \rangle = \frac{2kT\alpha}{\mu\gamma} \phi_{xx'} \phi(t - t'). \quad (16)$$

Some work has been attempted to describe the effects of dipole fields, which can also be added to the effective field³² or treated as a mean field³⁴. But because it seems the effects are actually of detriment to the effectiveness of hyperthermia, we do not discuss them here.

C. Numerical integration of Langevin equations

With the addition of the stochastic terms, the differential equations cannot be integrated as a normal Riemann integral³⁵. In general we see that the dimensions of the stochastic terms are actually the square-root of time, so in fact it is more precise to instead write these equations as integral equations of the form

$$d\mathbf{m} = \mathbf{f}dt + \mathbf{b}dW \quad (17)$$

where the W represents the Wiener process, the continuous analogue to the random walk. Additional information on the various types of stochastic differential equations can be found in Ref.^{35,36}. The usual method is to integrate the differential equation to first or second order, using the Euler-Maruyama or the Heun integration scheme, respectively^{28,37}. Then, magnetization moments are found from successive solving

$$\langle \mathbf{m}^j \rangle = \frac{1}{N} \sum_i^N \mathbf{m}_i^j \quad (18)$$

so that the average magnetization is when $j = 1$.

V. DISTRIBUTION FUNCTION APPROACH LEADING TO APPROXIMATE MODELS

We saw in the Langevin equation formulation that it is possible to include thermal effects to models of nanoparticles. This is particularly useful when the particles are expected to be at room temperature (as in biological and medical applications). The finite temperature will cause magnetization fluctuations and thus the nanoparticles are accurately described as a distribution of states. Instead of repeatedly solving a stochastic differential equation, we can use a distribution function approach where the distribution of states evolves over time.

A. The Fokker-Planck equation

We can represent a single nanoparticle's magnetization as a point on the unit sphere, so that the surface density of many magnetizations is determined by a function $f(\theta, \phi, t)$. As the particles rotate in space, the magnetization surface density changes, leading to a surface current J . The total number of nanoparticles is conserved, i.e., $\int f d\Omega = 1$, defining the surface density function as a probability distribution. The normalization also implies the continuity equation

$$\frac{\partial f}{\partial t} = -\nabla \cdot J \quad (19)$$

The probability current depends on the probability itself; this is the key to understanding the dynamics. At temperature $T = 0$ the current density J depends only on the velocity

$\left(v = \frac{dm}{dt}\right)$ of the points on the sphere. However, when the temperature is not zero, the system evolves towards equilibrium. A postulated phenomenological ‘diffusion’ of the distribution function²³ accounts for the approach to equilibrium. This is represented by a new term in the continuity equation proportional to a diffusion constant D and the gradient of the distribution function. We write the Fokker-Planck (FP) equation for the distribution function $f(\theta, \phi, t)$ as

$$\frac{\partial f}{\partial t} = -\nabla \cdot \left[\frac{d\mathbf{m}}{dt} - D\nabla \right] f. \quad (20)$$

From this distribution, magnetization statistics can be determined using the definition of the probability moments

$$\int \mathbf{m}^j f(\theta, \phi, t) d\Omega = \langle \mathbf{m}^j(t) \rangle \quad (21)$$

What remains is to define the change in the magnetization and the diffusion constant. The magnetization dynamics are controlled by the zero temperature differential equations Eq. 11 and Eq. 14. The diffusion constant is determined by the parameters at equilibrium

conditions, when there is no applied field and $\frac{\partial f}{\partial t} = 0$. In general, solutions to the Fokker-Planck equation are not possible, so approximation methods are used in practice.

B. Néel rotation and hyperthermia

If the expression for the magnetization dynamics of Néel rotation is inserted, this FP equation can be used to describe the rotations of small particles that are fixed spatially. These are the expected conditions for nanoparticles during hyperthermia³². It is also possible to develop an analytical approximation based on the assumption that the distribution function is linear in the magnetization. This approximation has been used to model hyperthermia because the imaginary response indicates heat deposition³⁸. Though these expressions are commonly used, we do not describe them here because recent work has shown that they are inadequate to fully model heating^{25,27}. The methods are accurate but care is necessary to assure that they are applied in the correct range of validity: when magnetizations are indeed linear as when applied fields are weak, magnetic moments are small and/or frequencies are high³⁹.

C. Brownian Fokker-Planck with cylindrically symmetric applied field

Replacing the velocity of the magnetization in Eq. 20 with Eq. 13, simplified slightly we have the FP for Brownian rotation

$$\frac{\partial f}{\partial t} = -\nabla \cdot \left[\frac{\alpha - \mathbf{m}(\mathbf{m} \cdot \alpha)}{2\tau} - D\nabla \right] f. \quad (22)$$

A general solution is not currently analytically possible, but if the applied magnetic field is in the z_2 -direction only, the FP equation can be simplified. This involves writing out all the components and unit vectors of \mathbf{m} in spherical coordinates,

$$\mathbf{m} = \sin \theta \cos \phi \hat{x} + \sin \theta \sin \phi \hat{y} + \cos \theta \hat{z}$$

and each unit vector is expressed e.g.,

$$\hat{x} = \nabla x = \left(\hat{\theta} \frac{\partial}{\partial \theta} + \hat{\phi} \frac{1}{\sin \theta} \frac{\partial}{\partial \phi} \right) \sin \theta \cos \phi$$

eventually we find

$$\hat{z} - \mathbf{m} \cos \theta = -\sin \theta \hat{\theta}$$

where the second term completely cancels. Thus, we arrive at the intuitive result that the distribution function does not depend on the azimuthal angle $f = f(\theta, t)$ only. We now have the FP equation

$$\frac{\partial f}{\partial t} = -\nabla \cdot \left[-\frac{\alpha}{2\tau} \sin \theta f - D \frac{\partial f}{\partial \theta} \right] \quad (23)$$

where by using the definition of the spherical gradient over only the polar angle we write

$$\frac{\partial f}{\partial t} = -\frac{1}{\sin \theta} \frac{\partial}{\partial \theta} \left[\sin \theta \left(-\frac{\alpha}{2\tau} \sin \theta f - D \frac{\partial f}{\partial \theta} \right) \right] \quad (24)$$

and lastly with the change of variables $x = \cos \theta$ we have $-\frac{1}{\sin \theta} \frac{\partial}{\partial \theta} = \frac{\partial}{\partial x}$ and with $D = 1/2 \tau$ we can write the 1-D FP equation,

$$2\tau \frac{\partial f}{\partial t} = \frac{\partial}{\partial x} \left[(1-x^2) \left(\frac{\partial f}{\partial x} - \alpha f \right) \right]. \quad (25)$$

This equation has solutions in a Legendre polynomial expansion^{34,40}. But it is of interest to demonstrate a further approximation method, the so-called ‘effective field’ method or ‘macroscopic relaxation equation’.

D. Effective field model for low-frequency Brownian relaxation

If we set the applied field to be a constant α_0 and let $\frac{\partial f}{\partial t} = 0$ we find the normalized distribution function

$$f(x) = \frac{\alpha_0}{4\pi} \frac{e^{\alpha x}}{\sinh \alpha}. \quad (26)$$

This is the same result as we get from Boltzmann statistics (remembering $x = \cos \theta$ in terms of the polar angle because the field is applied in the \hat{z} direction). We write the average magnetization in the direction of the field as M . Using this distribution function and

integrating to get the first moment, we find, as we should, that the Langevin function $L(x)$ describes the equilibrium dynamics of an ensemble of particles in an applied field:

$$M=L(\alpha_0)=\coth \alpha_0 - 1/\alpha_0. \quad (27)$$

The valuable approximation is to assume the particles are always at equilibrium so that the distribution function retains the same functional form, but with a time varying field $a \rightarrow \alpha(t)$. This ‘effective field’ approach turns out to be very useful to model low frequency oscillating fields where the relaxation time of the particles is shorter than the period of the applied field^{28,34}. Multiplying by x and integrating Eq. 25 with the effective distribution and definitions of the probability moments leads to an equation for the second moment in terms of the first. We have then a differential equation for the magnetizations at near-equilibrium conditions:

$$\frac{dM}{dt} = -\frac{M}{\tau_B} \left(1 - \frac{\alpha(t)}{\alpha_{eff}} \right) \quad (28)$$

where α_{eff} is found from inverting the Langevin function at every step³⁴. An inverse Langevin function can be used as in Ref.⁴¹. The effective field equation is useful for quicker analyses because it is much less computationally challenging than the full stochastic models.

VI. SUMMARY

We have seen that there are two mechanism for a magnetic particle to reorient its moment. The energy changes for particles to relax internally over energy barriers are also discussed in the framework of localized heating as is used in magnetic nanoparticle hyperthermia. The dynamics of these magnetic moments undergoing each relaxation mechanism separately are explored. The two most general approaches (the Langevin equation, or stochastic differential equation approach, and the Fokker-Planck, or distribution function approach) are illustrated. These include full variability of nanoparticle parameters as well as thermal fluctuations induced in a realistic setting. The methods for numerical integration are highlighted, and readers are directed to valuable sources. However, these equations are difficult and time consuming to solve, so we also introduce a macroscopic relaxation equation that is useful for low-frequency Brownian simulations.

Acknowledgments

The authors gratefully acknowledge the support of the Neukom Graduate Fellowship and NIH grant NIH-NCI 1U54CA151662-01 for funding.

REFERENCES

1. Koh I, Josephson L. Magnetic nanoparticle sensors. *Sensors*. 2009; 9(10):8130–8145. [PubMed: 22408498]
2. Haun JB, Yoon TJ, Lee H, Weissleder R. Magnetic nanoparticle biosensors. *Wiley Interdisciplinary Reviews: Nanomedicine and Nanobiotechnology*. 2010; 2(3):291–304. [PubMed: 20336708]
3. Chung SH, Hoffmann A, Bader SD, Liu C, Kay B, Makowski L, Chen L. Biological sensors based on brownian relaxation of magnetic nanoparticles. *Applied physics letters*. 2004; 85(14):2971–2973.

4. Zhang X, Reeves DB, Perreard IM, Kett WC, Griswold KE, Gimi B, Weaver JB. Molecular sensing with magnetic nanoparticles using magnetic spectroscopy of nanoparticle brownian motion. *Biosensors and Bioelectronics*. 2013; 50:441–446. [PubMed: 23896525]
5. Weaver JB, Rauwerdink AM, Hansen EW. Magnetic nanoparticle temperature estimation. *Medical physics*. 2009; 36:1822. [PubMed: 19544801]
6. Rauwerdink AM, Weaver JB. Viscous effects on nanoparticle magnetization harmonics. *Journal of Magnetism and Magnetic Materials*. 2010; 322(6):609–613.
7. Weaver JB, Rauwerdink KM, Rauwerdink AM, Perreard IM. Magnetic spectroscopy of nanoparticle brownian motion measurement of microenvironment matrix rigidity. *Biomedizinische Technik/ Biomedical Engineering*. 2013; 58(6):547–550.
8. Sun C, Lee JSH, Zhang M. Magnetic nanoparticles in MR imaging and drug delivery. *Advanced drug delivery reviews*. 2008; 60(11):1252–1265. [PubMed: 18558452]
9. Gleich B, Weizenecker J. Tomographic imaging using the nonlinear response of magnetic particles. *Nature*. 2005; 435(7046):1214–1217. [PubMed: 15988521]
10. MH, Publico-Lansigan; Situ, SF.; Samia, ACS. Magnetic particle imaging: advancements and perspectives for real-time in vivo monitoring and image-guided therapy. *Nanoscale*. 2013
11. Weizenecker J, Gleich B, Rahmer J, Dahnke H, Borgert J. Three-dimensional real-time in vivo magnetic particle imaging. *Physics in medicine and biology*. 2009; 54(5):L1. [PubMed: 19204385]
12. Hergt R, Dutz S, Müller R, Zeisberger M. Magnetic particle hyperthermia: nanoparticle magnetism and materials development for cancer therapy. *Journal of Physics: Condensed Matter*. 2006; 18(38):S2919.
13. Jordan A, P Wust, Fühling H, John W, Hinz A, Felix R. Inductive heating of ferrimagnetic particles and magnetic fluids: physical evaluation of their potential for hyperthermia. *International Journal of Hyperthermia*. 2009; 25(7):499–511. [PubMed: 19848612]
14. Giustini AJ, Petryk AA, Cassim SM, Tate JA, Baker I, Hoopes PJ. Magnetic nanoparticle hyperthermia in cancer treatment. *Nano LIFE*. 2010; 1(01n02):17–32.
15. Veiseh O, Gunn JW, Zhang M. Design and fabrication of magnetic nanoparticles for targeted drug delivery and imaging. *Advanced drug delivery reviews*. 2010; 62(3):284–304. [PubMed: 19909778]
16. Giustini AJ, Perreard IM, Rauwerdink AM, Hoopes PJ, Weaver JB. Noninvasive assessment of magnetic nanoparticle–cancer cell interactions. *Integrative Biology*. 2012; 4(10):1283–1288. [PubMed: 22945022]
17. Khandhar AP, Ferguson RM, Krishnan KM. Monodispersed magnetite nanoparticles optimized for magnetic fluid hyperthermia: Implications in biological systems. *Journal of applied physics*. 2011; 109:07B310.
18. Latorre M, Rinaldi C. Applications of magnetic nanoparticles in medicine: magnetic fluid hyperthermia. *PR Health Sciences Journal*. 28(3):2009.
19. Goya GF, Berquo TS, Fonseca FC, Morales MP. Static and dynamic magnetic properties of spherical magnetite nanoparticles. *Journal of Applied Physics*. 2003; 94:3520.
20. Néel L. Théorie du traînage magnétique des ferromagnétiques en grains fins avec applications aux terres cuites. *Annals Gèophysics*. 1949; 5(2):99–136.
21. Einstein, Albert. *Investigations on the Theory of the Brownian Movement*. Dover. 1956
22. Fannin PC, Charles SW. On the calculation of the neel relaxation time in uniaxial single-domain ferromagnetic particles. *Journal of Physics D: Applied Physics*. 1994; 27(2):185.
23. Brown WF. Thermal fluctuations of a single-domain particle. *Physical Review*. 1963; 130(5):1677.
24. Mamiya H, Jeyadevan B. Hyperthermic effects of dissipative structures of magnetic nanoparticles in large alternating magnetic fields. *Scientific reports*. 2011; 1
25. Dennis CL, Ivkov R. Physics of heat generation using magnetic nanoparticles for hyperthermia. *International Journal of Hyperthermia*. 2013; 29(8):715–729. [PubMed: 24131317]
26. Stoner EC, Wohlfarth EP. A mechanism of magnetic hysteresis in heterogeneous alloys. *Philosophical Transactions of the Royal Society of London. Series A. Mathematical and Physical Sciences*. 1948:599–642.

27. Carrey J, Mehdaoui B, Respaud M. Simple models for dynamic hysteresis loop calculations of magnetic single-domain nanoparticles: Application to magnetic hyperthermia optimization. *Journal of Applied Physics*. 2011; 109(8):083921–083921.
28. Reeves DB, Weaver JB. Simulations of magnetic nanoparticle brownian motion. *Journal of applied physics*. 2012; 112(12):124311–124311. [PubMed: 23319830]
29. Chandrasekhar S. Stochastic problems in physics and astronomy. *Reviews of modern physics*. 1943; 15(1):1.
30. García-Palacios JL, Lázaro FJ. Langevin-dynamics study of the dynamical properties of small magnetic particles. *Physical Review B*. 1998; 58(22):14937.
31. Gilbert TL. A phenomenological theory of damping in ferromagnetic materials. *Magnetics, IEEE Transactions on*. 2004; 40(6):3443–3449.
32. Haase C, Nowak U. Role of dipole-dipole interactions for hyperthermia heating of magnetic nanoparticle ensembles. *Physical Review B*. 2012; 85(4):045435.
33. Weizenecker J, Gleich B, Rahmer J, Borgert J. Micro-magnetic simulation study on the magnetic particle imaging performance of anisotropic mono-domain particles. *Physics in medicine and biology*. 2012; 57(22):7317. [PubMed: 23079678]
34. Felderhof BU, Jones RB. Mean field theory of the nonlinear response of an interacting dipolar system with rotational diffusion to an oscillating field. *Journal of Physics: Condensed Matter*. 2003; 15(23):4011.
35. ksandal, Bernt Ø. *Stochastic differential equations: an introduction with applications*. Springer-Verlag, Berlin. 1998
36. E, Peter; and, Kloeden; Platen, Eckhard. In *Numerical Solution of Stochastic Differential Equations*. Springer; 1992. *Stochastic differential equations*; p. 103-160.
37. Gard, Thomas C. *Introduction to stochastic differential equations*. M. Dekker; New York: 1988.
38. Rosensweig RE. Heating magnetic fluid with alternating magnetic field. *Journal of Magnetism and Magnetic Materials*. 2002; 252:370–374.
39. Hergt R, Dutz S, Zeisberger M. Validity limits of the néel relaxation model of magnetic nanoparticles for hyperthermia. *Nanotechnology*. 2010; 21(1):015706. [PubMed: 19946160]
40. Deissler RJ, Wu Y, Martens MA. Dependence of brownian and néel relaxation times on magnetic field strength. *Medical physics*. 2013; 41(1):012301. [PubMed: 24387522]
41. Cohen A. A pad e approximant to the inverse langevin function. *Rheologica Acta*. 1991; 30(3): 270–273.

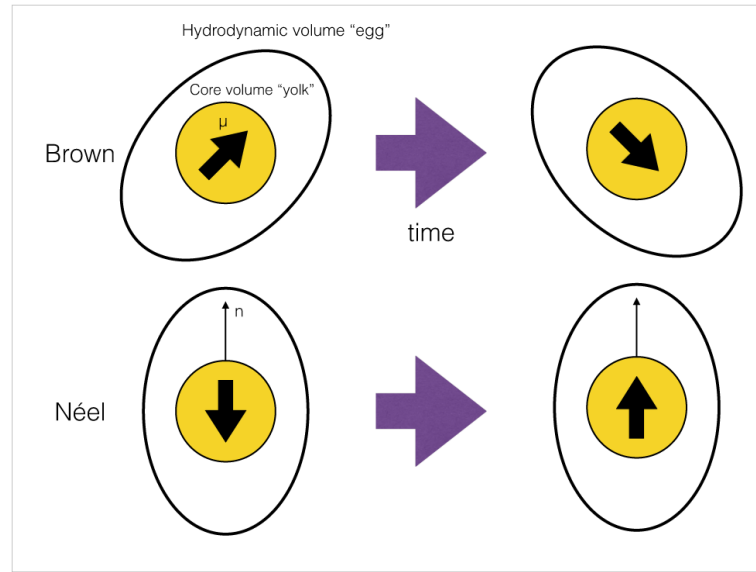


FIG. 2. Néel and Brownian particles relax differently. The moment can rotate internally to align with the anisotropy axis n , or the entire particle can rotate.

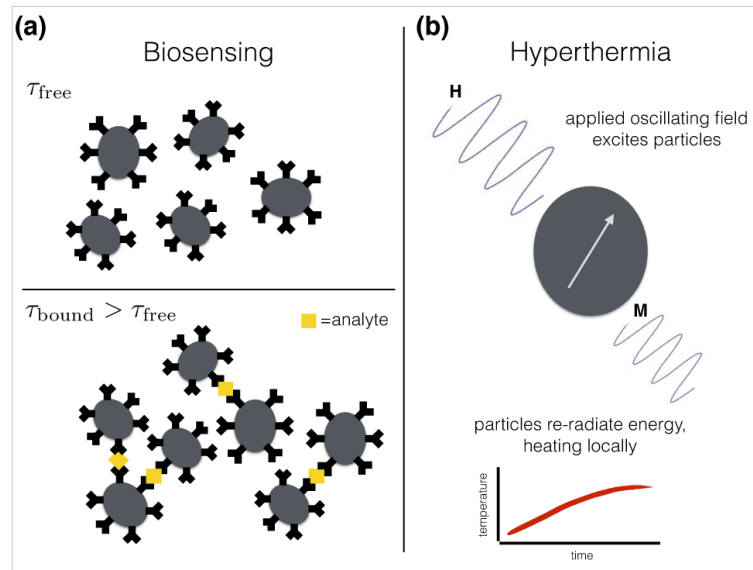


FIG. 1. Two applications for magnetic nanoparticles (a) sensing specific ‘analyte’ biomolecules, and (b) locally heating through dissipative losses from oscillating particles.