

# Behavioral Paradigm for the Evaluation of Stimulation-Evoked Somatosensory Perception Thresholds in Rats

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## 19 Abstract

20 Intracortical microstimulation (ICMS) of the somatosensory cortex via penetrating microelectrode  
21 arrays (MEAs) can evoke cutaneous and proprioceptive sensations for restoration of perception in  
22 individuals with spinal cord injuries. However, ICMS current amplitudes needed to evoke these  
23 sensory percepts tend to change over time following implantation. Animal models have been used to  
24 investigate the mechanisms by which these changes occur and aid in the development of new  
25 engineering strategies to mitigate such changes. Non-human primates are commonly the animal of  
26 choice for investigating ICMS, but ethical concerns exist regarding their use. Rodents are a preferred  
27 animal model due to their availability, affordability, and ease of handling, but there are limited choices  
28 of behavioral tasks for investigating ICMS. In this study, we investigated the application of an  
29 innovative behavioral go/no-go paradigm capable of estimating ICMS-evoked sensory perception  
30 thresholds in freely moving rats. We divided animals into two groups, one receiving ICMS and a  
31 control group receiving auditory tones. Then, we trained the animals to nose-poke – a well-established  
32 behavioral task for rats – following either a suprathreshold ICMS current-controlled pulse train or  
33 frequency-controlled auditory tone. Animals received a sugar pellet reward when nose-poking  
34 correctly. When nose-poking incorrectly, animals received a mild air puff. After animals became  
35 proficient in this task, as defined by accuracy, precision, and other performance metrics, they continued  
36 to the next phase for perception threshold detection, where we varied the ICMS amplitude using a  
37 modified staircase method. Finally, we used non-linear regression to estimate perception thresholds.

38 Results indicated that our behavioral protocol could estimate ICMS perception thresholds based on  
39 ~95% accuracy of rat nose-poke responses to the conditioned stimulus. This behavioral paradigm  
40 provides a robust methodology for evaluating stimulation-evoked somatosensory percepts in rats  
41 comparable to the evaluation of auditory percepts. In future studies, this validated methodology can be  
42 used to study the performance of novel MEA device technologies on ICMS-evoked perception  
43 threshold stability using freely moving rats or to investigate information processing principles in neural  
44 circuits related to sensory perception discrimination.

## 45 **Introduction**

46 Intracortical microstimulation (ICMS) of the somatosensory cortex via microelectrode arrays (MEAs)  
47 has been successfully used to evoke cutaneous and proprioceptive sensations in amputees and  
48 individuals with spinal cord injuries (Armenta Salas et al., 2018; Bjånes et al., 2022; Christie et al.,  
49 2022; Page et al., 2021). These sensations can provide somatosensory feedback for closed-loop brain-  
50 machine interfaces and neuroprosthetics (Carè et al., 2022), which has been demonstrated to improve  
51 the control of robotic arms (Flesher et al., 2021). However, once implanted into the brain, achieving  
52 long-term stability of perception thresholds with these devices has been challenging (Callier et al.,  
53 2015; Hughes et al., 2021; Urdaneta et al., 2022) due to multifactorial failure of the interface. These  
54 failures include surpassing the safety limits of electrical microstimulation (Kramer et al., 2019;  
55 Pancrazio et al., 2017; Shannon, 1992), foreign body response that can isolate the MEAs from the  
56 surrounding neural tissue (Rajan et al., 2015), neuroinflammation that leads to neuronal loss (Ereifej  
57 et al., 2018; Potter et al., 2012), and material cracking and delamination (Barrese et al., 2013). Despite  
58 the promises of using ICMS to restore sensation, these failure modes pose a barrier for more  
59 widespread use. Because of this, research to improve the long-term reliability of ICMS is needed. The  
60 majority of pre-clinical studies investigating ICMS involve non-human primates; however, ethical  
61 concerns and costs limit their use (Bailey & Taylor, 2016; Carvalho et al., 2019; Pankevich, 2012).  
62 Rodents have been widely used to investigate the recording performance of MEAs due to their  
63 availability, affordability, and ease of handling (El-Ayache & Galligan, 2020; A. S. Koivuniemi et al.,  
64 2011). However, the use of this model organism for evaluating ICMS-induced somatosensory  
65 perceptions has been hindered by the limited behavioral paradigms available for this purpose.

66 To our knowledge, three behavioral paradigms have been described in the literature for assessing ICMS  
67 in the primary somatosensory cortex of rodents (A. Koivuniemi et al., 2011; Lycke et al., 2023; Öztürk  
68 et al., 2019; Urdaneta et al., 2021). These behavioral tasks use either a freely moving passive avoidance  
69 psychophysical detection task, a freely moving active avoidance conditioning paradigm, or a head-  
70 fixed go/no-go task. All were successful at detecting thresholds for up to 33 weeks with 70-95%  
71 accuracy; however, all three paradigms involve water deprivation for up to 36 hours prior to behavioral  
72 testing (A. Koivuniemi et al., 2011; Öztürk et al., 2019) which can produce stress (Vasilev et al., 2021)  
73 and confound chronic assessments. Alternative behavioral paradigms that use food-restriction have  
74 been described for the testing of auditory thresholds. An example of this is the well-established nose-  
75 poke behavioral paradigm (Abolafia et al., 2011; Riley et al., 2021; Schindler et al., 1993), a behavioral  
76 paradigm where a food-deprived rat is introduced into an operant conditioning chamber and trained to  
77 nose-poke through a hole on a side wall upon presentation of an auditory tone followed by a sugar  
78 pellet reward. While this behavioral task has been shown to be highly accurate with ~90%  
79 discrimination accuracy scores (Riley et al., 2021; Sloan et al., 2009) and effective for auditory  
80 psychophysical testing, it has not been used to assess ICMS-induced somatosensory perceptions  
81 because no adaptations of the task have been made to suit this need.

82 Here we describe an innovative operant conditioning behavioral task to effectively assess ICMS-  
83 evoked sensory perception thresholds. We adapted the well-established and validated nose-poke  
84 auditory task into a food positive reinforcement go/no-go behavioral paradigm in food-deprived, freely  
85 moving rats with a mild passive avoidance positive-punishment air-puff. We implanted MEAs into  
86 Sprague-Dawley rats, targeting the forelimb area of the left primary somatosensory cortex (S1FL) and  
87 delivered electrical stimulation to modulate the neural activity and evoke artificial sensory percepts.  
88 We compared the accuracy of this task for ICMS perception thresholds with the accuracy of auditory  
89 tone discrimination for validation of the novel behavioral paradigm. Our results show that this  
90 behavioral protocol could estimate ICMS perception thresholds based on ~95% accuracy of all rat  
91 nose-poke responses to the conditioned stimulus, validating its use for future ICMS perception  
92 threshold investigations.

## 93 **Material and Methods**

### 94 **Ethics Statement**

95 All animal handling, housing and procedures were approved by The University of Texas at Dallas  
96 IACUC (protocol #21-15) and in accordance with ARRIVE guidelines.

### 97 **Animal Use**

98 We used six (N=6) male Sprague-Dawley rats (Charles River Laboratories Inc., Houston, TX, US) that  
99 were single-housed in standard home cages under a reverse 12-hour day/night cycle. We food-deprived  
100 the animals four consecutive days per week to a 90% free-feeding level that was redefined weekly to  
101 promote consistent performance during the behavioral task (Schindler et al., 1993) and given ad libitum  
102 access to food three consecutive days per week. Their weight was recorded on the last day of the week  
103 with ad libitum access to food, and before every behavioral session during the four consecutive days  
104 of food deprivation to assess welfare of the animal. If the weight before the behavioral session was  
105 below 90% of its recorded control weight, we provided supplemental rodent feed pellets to provide  
106 additional nourishment and excluded the animal from behavioral experimentation until the 90% free-  
107 feeding control weight was restored. Animals were given dustless reward pellets (F0021, Bio-Serv,  
108 Flemington, NJ, US) as positive reinforcement for the behavioral paradigm. These pellets contain a  
109 balanced caloric profile enriched with amino acids, carbohydrates, fatty acids, vitamin, and mineral  
110 mix to ensure the nutritional wellbeing of the animals despite food deprivation. In addition, we  
111 provided rats with supplemental regular food pellets (5LL2 - Prolab® RMH 1800, LabDiet, St. Louis,  
112 MO, US) after each behavioral session to maintain weight. This supplemental feed was calculated  
113 based on the number of reward pellets eaten during each behavioral session. Animals had ad libitum  
114 access to water at all times while in their standard home cages.

115 Rats were randomized and divided into two groups. The first was the experimental group, which  
116 received implantation with a multi-shank MEA (MEA-PI-A3-00-12-0.01-[1-2]-3-0.25-0.25-1-1SS;  
117 Microprobes for Life Science, Gaithersburg, MD, US) consisting of 12 Pt/Ir (70% Pt, 30% Ir, 0.01  
118 MΩ) microwires of 75 μm diameter, insulated with polyamide. The tips of each microwire had an  
119 exposed geometric surface area ranging between 6000 and 9000 μm<sup>2</sup>. The MEA design has two rows  
120 of six microwires each, which slant in opposing directions ranging in length between 0.5 - 2 mm (Figure  
121 1A). Each MEA includes an additional 2 mm microwire that serves as the reference electrode. The  
122 experimental group received ICMS (n=3) during the behavioral task. The second group was a control  
123 group (n=3), which underwent a sham surgery and received auditory tones during the behavioral task.  
124 The sham surgery consisted of a craniotomy and durotomy procedure comparable with the  
125 experimental group without implantation of the MEA. The goal of the control group was to compare

126 the accuracy of the behavioral paradigm presented here. The operant chamber apparatus was  
127 thoroughly cleaned with a 70% ethanol solution between each session to help eliminate any distracting  
128 scents between animal subjects. After completing the behavioral testing, the animals in the ICMS group  
129 were subjected to the same behavioral task without electrical stimulation. This was done to act as an  
130 intragroup negative control to validate ICMS as the only interpreted conditioning cue by verifying  
131 changes in accuracy during the absence of a stimulus.

## 132 **Surgical Procedure**

133 Rats underwent a surgical procedure for sham and MEA implantation as previously described (Sturgill  
134 et al., 2022). Briefly, animals were anesthetized using vaporized isoflurane (1.8-2.5%) mixture with  
135 medical grade oxygen (500 mL/min; SomnoSuite® for Mice & Rats, Kent Scientific Corporation,  
136 Torrington, CT, US). The surgical team monitored vital signs throughout the surgical procedure while  
137 body temperature was maintained using a controlled far-infrared warming pad (PhysioSuite® for Mice  
138 & Rats, Kent Scientific Corporation, Torrington, CT, US). The scalp was shaved and animals were  
139 mounted onto a digital stereotaxic frame (David Kopf Instruments, Tujunga, CA, US). The skin at the  
140 surgical site was cleaned using three alternating applications of betadine and alcohol wipes. A  
141 subcutaneous injection of 0.5% bupivacaine hydrochloride (Marcaine, Hospira, Lake Forest, IL, US)  
142 was given at the intended incision site. An incision was made through the midline of the scalp, muscles,  
143 and connective tissue. Next, the skull was leveled and centered in the stereotaxic frame using bregma,  
144 lambda, and the sagittal suture as references ( $\pm 0.1$  mm). Three holes were then drilled into the skull  
145 to insert stainless-steel bone screws (Stoelting Co., Wood Dale, IL, USA) (Figure 1B). Then, a 2 mm  
146 x 3 mm craniotomy was made targeting the S1FL (AP: -0.5 mm, ML: 4 mm), followed by a durotomy  
147 (Figure 1B). The surgeon secured the ground wire to one of the mounted bone screws and implanted  
148 the MEA to a cortical depth of ~1.6 mm using a precision-controlled inserter (NeuralGlider, Actuated  
149 Medical, Inc., Ann Arbor, MI, US) (Figure 1B). Implantation within the cranial window was done to  
150 avoid disruption of major surface blood vessels (He et al., 2022; Kozai et al., 2010). The implant site  
151 was then sealed with a biocompatible, transparent silicone elastomer adhesive (Kwik-Sil, World  
152 Precision Instruments, Sarasota, FL, US), followed by a dental cement head cap to tether the MEA to  
153 the skull while also reducing the likelihood of contamination and infection. Then, the incision was  
154 closed using surgical staples and tissue adhesive (GLUture, World Precision Instruments, Sarasota, FL,  
155 US). At the end of the surgical procedure, we injected each animal with 0.05 mL/kg intramuscular  
156 cefazolin (Med-Vet International, Mettawa, IL, US) for antibiotic prophylaxis together with topical  
157 application triple-antibiotic ointment around the incision site. For analgesia, we administered either  
158 0.15 mL/kg of subcutaneous slow-release (Buprenorphine SR-LAB, ZooPharm, LLC., Laramie, WY,  
159 US) or 0.5 mL/kg of extended-release (Ethiqa XR, Fidelis Animal Health, North Brunswick, NJ, US)  
160 buprenorphine depending on availability of the substance. When necessary, we administered a dose of  
161 buprenorphine after 72 hours post-surgery if the animal showed signs of pain. Lastly, we provided  
162 sulfamethoxazole and trimethoprim oral suspension (200 mg/40 mg/5 mL, Aurobindo Pharma, Dayton,  
163 NJ, US) in the animals' drinking water (1 mL/100 mL drinking water) as an additional antibiotic for 7  
164 days post-surgery.

## 165 **Behavioral Operant Chamber, Equipment and Software**

166 Figure 1C&D illustrates the behavioral operant chamber used for this study. The go/no-go behavioral  
167 paradigm was conducted within a commercially available operant conditioning chamber (OmniTrak,  
168 Vulintus, Inc., Lafayette, CO, US). This chamber had two holes in one of the side walls, one containing  
169 an infrared break-beam sensor (nose-poke sensor) and a second hole connected to a precision pellet  
170 dispenser. In addition, the nose-poke hole had the capability of delivering a mild air-puff from a

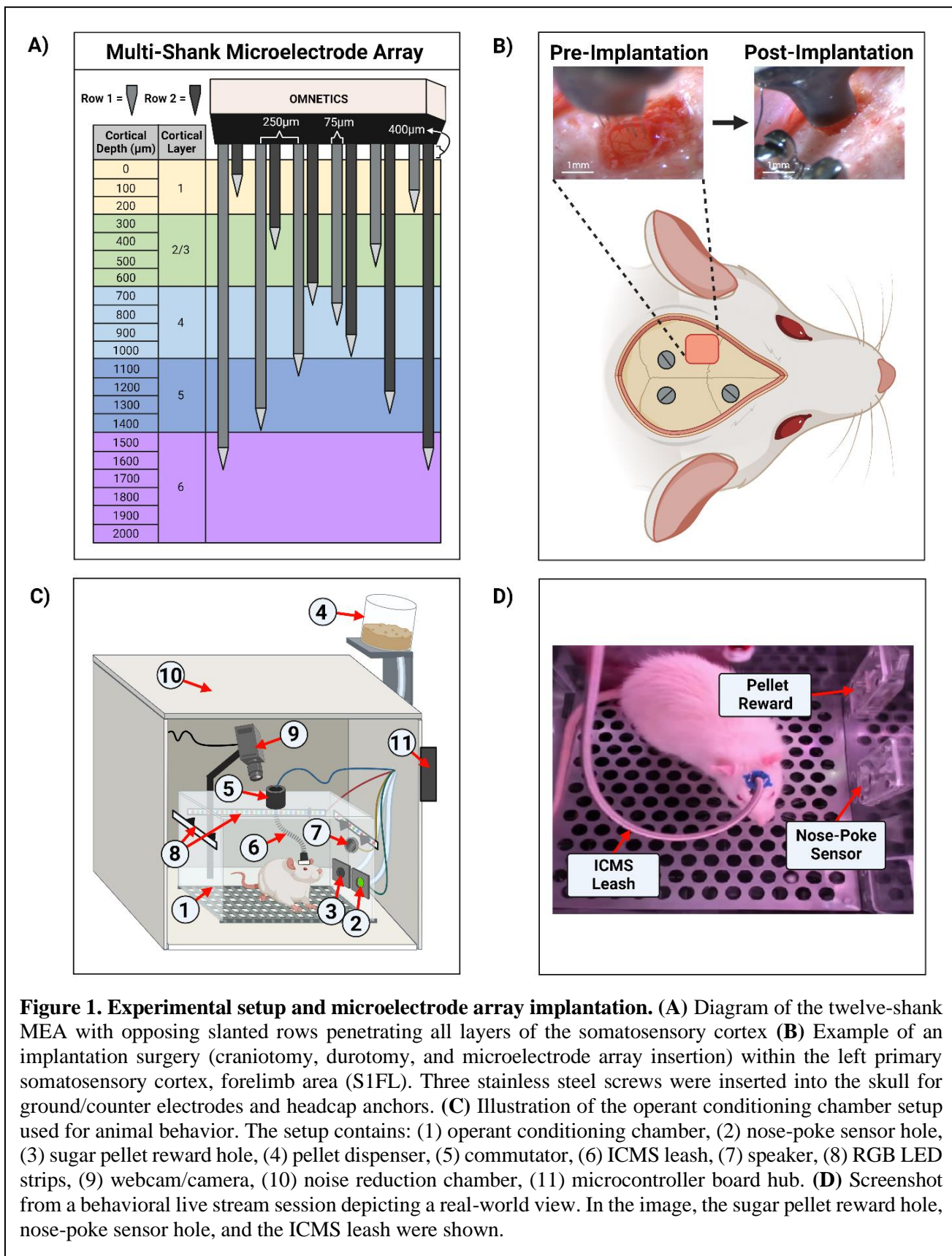


171 medical-grade compressed air cylinder tube as positive punishment. This air-puff was controlled via a  
172 pneumatic solenoid (SKUSKD1384729, AOMAG) connected to an Inland Nano microcontroller  
173 through a relay switch to deliver air to the nose-poke sensor hole. A rotating commutator (76-SR-12,  
174 NTE Electronics, Bloomfield, NJ, US) was bolted at the top of the operant chamber to allow the  
175 animals to roam free while connected to an external stimulator (PlexStim, Plexon Inc., Dallas, TX, US)  
176 for ICMS. A custom cord was designed to connect the animal to the commutator for ICMS,  
177 incorporating an Omnetics (A79021-001, Omnetics Connector Corporation, Minneapolis, MN, US)  
178 adapter and surrounded with a stainless-steel spring cable shielding (#6Y000123101F, Protech  
179 International Inc., Boerne, TX, US) to protect the wires against biting. For the auditory control group,  
180 auditory tones were presented through a mini speaker (Product ID: 3923, Adafruit Industries, New  
181 York City, NY, US) that was placed inside the chamber and connected to a PC's headphone auxiliary  
182 port. The chamber was illuminated via an RGB LED strip controlled by the Inland Nano  
183 microcontroller. A webcam (960-001105, Logitech, Lausanne, CH, US) was mounted to the chamber  
184 to record a live video stream of the animal during behavioral sessions. Finally, the chamber was  
185 enclosed inside a sound-reduction chamber equipped with a fan for cooling and air circulation. All  
186 modules were connected and controlled by an ATMEGA2560 microcontroller board hub (OmniTrak  
187 Controller V3.0, Vulintus Inc., Lafayette, CO, US), interfaced using custom MATLAB (R2022b,  
188 Mathworks, Natick, MA, US) software. The RGB LED strip and solenoid valve required a  
189 supplemental 12V 2A DC power supply to power the devices.

190 In addition, we developed a custom MATLAB GUI application (Supplementary Figure 1) that  
191 simultaneously controls and displays the behavioral task parameters, monitors animal performance,  
192 and records session data. While a behavioral session is active, the application feeds the session video  
193 live stream from the operant chamber to the researcher, as shown in Supplementary Figure 1.  
194 Furthermore, this GUI included specialized buttons for the researcher to annotate instances during each  
195 session where we deemed the animals distracted (e.g., grooming or turning away from the  
196 sensors/modules for the entire trial duration) for exclusion from analysis. After each session, a second  
197 researcher validated the annotations offline to reduce bias. Additional features of the GUI application  
198 include a button for manually dispensing sugar pellets, the ability to record voltage transients  
199 throughout the session, and the capability to choose which electrode channels are delivered ICMS. This  
200 custom MATLAB and UI/UX behavior software is available as an open-source package on GitHub  
201 ([https://github.com/Neuronal-Networks-and-Interfaces-Lab/Stimulation-](https://github.com/Neuronal-Networks-and-Interfaces-Lab/Stimulation-Evoked_Perception_Behavioral_Software.git)  
202 [Evoked\\_Perception\\_Behavioral\\_Software.git](https://github.com/Neuronal-Networks-and-Interfaces-Lab/Stimulation-Evoked_Perception_Behavioral_Software.git)).

## 203 **Electrical Stimulation and Auditory Parameters**

204 Electrical stimulation for ICMS was delivered to 10 electrode sites simultaneously per implanted MEA.  
205 The stimulation parameters selected for this work were previously established by another group and  
206 validated to evoke somatosensory percepts in rats (Urdaneta et al., 2021). We used current-controlled,  
207 charge-balanced symmetric biphasic waveforms with a cathodal-leading phase, a frequency of 320 Hz,  
208 pulse width of 200  $\mu$ s per phase, 40  $\mu$ s interphase interval, with a 650 ms train duration (PlexStim,  
209 Plexon Inc., Dallas, TX, US). Current amplitudes used in this work ranged from 0-25  $\mu$ A corresponding  
210 to a charge of 0-5 nC/ph. The maximum charge limit set for all experiments was 5 nC/ph per electrode  
211 stimulated simultaneously across ten channels. Seven to twelve days after implantation but before  
212 operant conditioning training, we estimated a provisional ICMS naïve perception threshold for each  
213 animal by slowly increasing the charge/phase across all 10 individually pulsed channels simultaneously  
214 from 0 to 5 nC/ph until a physical response (e.g., paw withdrawal) was observed. Once this provisional  
215 perception threshold was determined, we confirmed that the

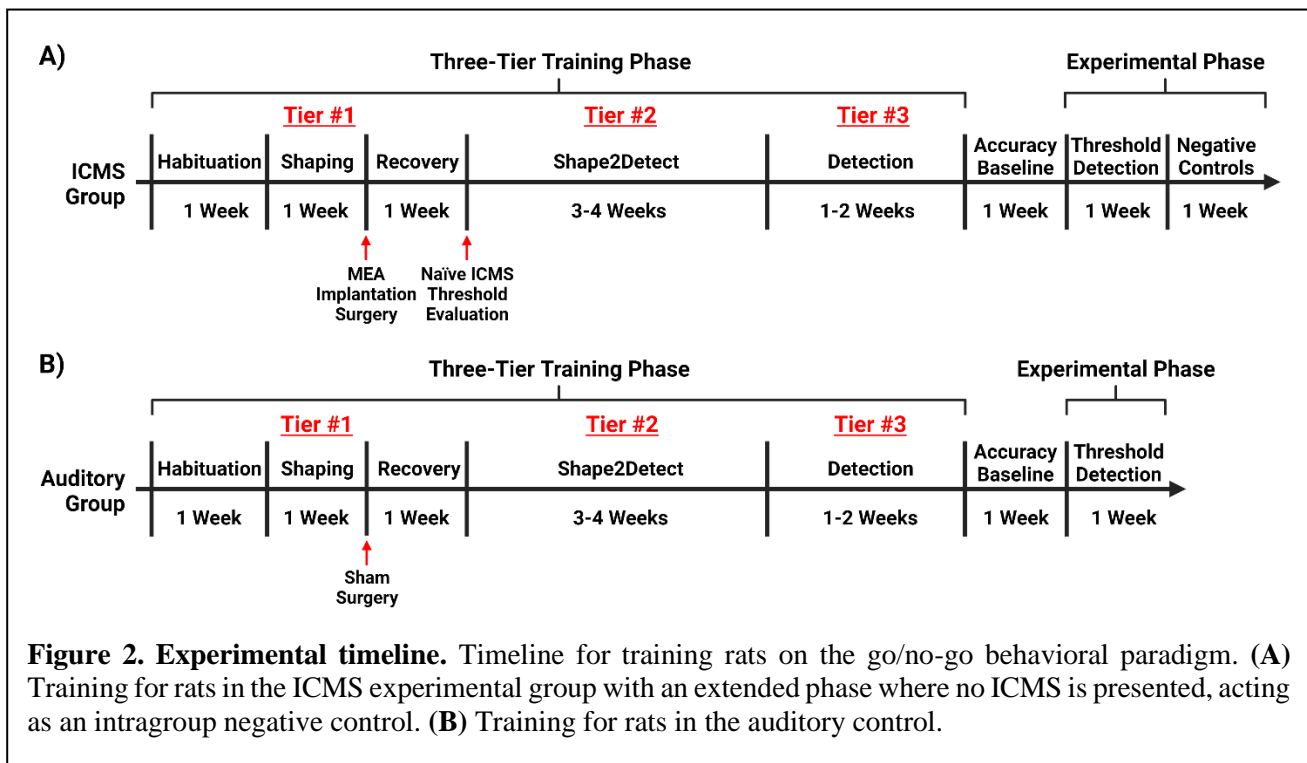


216 physical response was driven primarily by somatosensory ICMS and not motor activation by presenting  
 217 the stimulus at the same charge intensity while the animal was anesthetized (1.8-2.0% isoflurane). This  
 218 naïve perception threshold was subsequently used as the starting known threshold for the go/no-go  
 219 behavioral paradigm. Voltage transients during ICMS were recorded by connecting the external  
 220 stimulator to an oscilloscope (TBS1052B, Tektronix, Beaverton, OR, US).

221 For the auditory control group, auditory tone parameters were derived from prior go/no-go paradigms  
 222 (Engineer et al., 2008; Green et al., 1979; Sloan et al., 2009). In our experiment, we used a carrier  
 223 frequency of 6 kHz pure tone sinusoidal wave with a 100 kHz sampling rate, 500 ms tone duration,  
 224 and a 50 ms beginning/end tone ramp duration. Using a sound level meter (Extech Instruments, Nashua,  
 225 NH, US), the produced output intensity of this auditory training tone was measured to be ~90 dB in  
 226 reference to the sound pressure level (SPL) of 0 dB, which is the intensity of sound waves relative to  
 227 the minimum threshold of human hearing.

## 228 Go/No-Go Behavioral Training

229 We trained rats on the go/no-go behavioral paradigm following a three-tier protocol. Namely, Shaping,  
 230 Shape2Detect, and Detection, as shown in Figure 2. Each tier is designed to gradually train every  
 231 animal to nose-poke following a presented stimulus (ICMS or auditory tone) to receive a reward pellet  
 232 in the go/no-go paradigm as shown in Figure 3A. Before training began, animals were habituated for  
 233 a minimum of 10 hours until the animal tolerated handling and head restraint for at least two  
 234 consecutive minutes. This habituation allowed for manipulation of the animals and connection of the  
 235 implanted MEA to the rotating commutator hardware before each behavioral session. During the  
 236 habituation period, the animals were fed reward pellets to incentivize the reward-seeking behavior.



## 237 **First Tier: Shaping**

238 Shaping was the first tier for the go/no-go training, which consisted of one-hour sessions, five days per  
239 week. The goal of this phase was to train the animal on the nose-poke behavior task via positive  
240 reinforcement. First, the animal was introduced into the operant chamber and allowed to freely roam.  
241 The chamber was illuminated with white light via the RGB LED strip. After three seconds, the RGB  
242 LED strip was configured to illuminate with green light for an indefinite amount of time, indicating a  
243 trial had begun. A pellet reward was dispensed when the animal nose-poked through the nose-poke  
244 hole as a positive-reinforcement to promote this behavior unless the animal poked within the first 150  
245 ms of the trial. This delay was incorporated to prevent accidental nose-pokes from occurring at the start  
246 of a trial. After the animal nose-poked, the green light turned back to white light for an inter-trial period  
247 of three seconds. If the animal nose-poked during the inter-trial period, no reward pellet was dispensed.  
248 When needed, we manually dispensed pellets when animals approached the nose-poke hole, even if  
249 the animal did not poke to encourage exploration. Animals were considered proficient in the Shaping  
250 task when they received 100+ reward pellets for two consecutive sessions without manual pellets  
251 dispensed. After passing this tier, they received either surgery for MEA implantation, or sham surgery.  
252 If a rat did not meet the 100+ pellet reward within 10 sessions, the animal was excluded from the study.

## 253 **Second Tier: Shape2Detect**

254 Shape2Detect was the second tier for the go/no-go task training, as shown in Figure 2. During this  
255 phase, animals were trained to nose-poke only upon presentation of either the ICMS at their pre-  
256 established naïve threshold or the auditory training tone at ~90 dB SPL, depending on their group  
257 allocation. We began each session by placing the animal into the apparatus once per day, four days per  
258 week for 60-minute-long sessions. At the start of the session, the operant chamber was illuminated by  
259 white light from the RGB LED strip. When each trial began, the RGB LED strip changed to green light  
260 to indicate the beginning of a trial (Figure 3B). During this phase, animals were presented with two  
261 types of trials: stimulus trials or catch trials as outlined in Figure 3A&B. A stimulus trial was defined  
262 as the presentation of the ICMS or auditory tone; whereas a catch trial consisted of an absence of  
263 stimulation or sound. Positive punishment was tied to the catch trial to reinforce the rat's ability to  
264 ignore trials in the absence of stimulus and discourage nose-poking freely. Stimulus and catch trials  
265 were presented sequentially in trial windows followed by a 3 second inter-trial period of white light.  
266 The trial window duration varied as time progressed throughout the session, as shown in Table I. For  
267 the first 20 minutes, the trial window duration was set to 3 seconds. The next ten minutes had trial  
268 durations of 4 seconds, the following ten minutes durations of 5 seconds, and the final ten minutes  
269 durations of 6 seconds. Throughout the session, the likelihood of a stimulus trial being presented versus  
270 a catch trial was varied. The first ten minutes had an 83.3% probability of presenting a stimulus trial  
271 (with a 16.7% probability of catch trials) and then changed until the last ten minutes had a 50%  
272 probability of presenting a stimulus trial (50% probability of catch trials). The rationale for varying  
273 this probability was to increase the frequency of stimulus exposure at the beginning of the session,  
274 providing the animal ample opportunities to associate the stimulus presentation with a reward. Then,  
275 we decreased the frequency of the stimulus exposure as the session progressed to avert continuous  
276 poking and encourage discriminatory decision making. Finally, the hit window and timeouts were also  
277 varied throughout the session (see Table I). The hit window was defined as the duration of time after  
278 the presentation of a stimulus during which the animal can nose-poke and receive a pellet reward  
279 (Figure 3B). A hit was determined if an animal nose-poked during this hit window. If an animal nose-  
280 poked after the hit window (trial remainder) or during a catch trial, it received a mild-air puff as a  
281 punishment and triggered a timeout period, characterized by red light illumination. The first instance  
282 was classified as a miss for quantification purposes; the latter as a false alarm. If the animal poked  
283 during the timeout period, it received an air-puff and additional time was added to the timeout. The



284 pressure of the air-puff was adjusted as needed so that it was enough to prevent timeouts but not to  
285 completely deter the animal from nose-poking. Furthermore, if the animal failed to nose-poke for ten  
286 stimulus trials in a row, the session would be paused and resumed only after the animal nose-poked  
287 again. Finally, a correct rejection was defined as the animal refraining from nose-poking during a catch  
288 trial.

**Table I.** Shape2Detect behavioral training task parameters

Session Time (min)	Trial Window Duration (s)	Stimulus Trial Probability (%)	Hit Window (s)	Timeout (s)
0-9	3	83.3	3	2
10-19	3	71.4	3	3
20-29	4	66.7	4	3
30-39	5	60.0	5	5
40-60	6	50.0	3	8

289 In the context of this study, hits and correct rejections were considered true responses, whereas misses  
290 and false alarms were considered false responses. Animals were considered proficient in the  
291 Shape2Detect task if they met four conditions for two consecutive sessions: 1) at least a 75% accuracy  
292 (Equation 1), 2) 75% precision (Equation 2), 3) 75% hit rate (Equation 3) score, and 4) received at least  
293 100 reward pellets.

$$\text{Accuracy} = \frac{\text{Hits} + \text{Correct Rejections}}{\text{Hits} + \text{Misses} + \text{False Alarms} + \text{Correct Rejections}} \quad (1)$$

$$\text{Precision} = \frac{\text{Hits}}{\text{Hits} + \text{False Alarms}} \quad (2)$$

$$\text{Hit Rate} = \frac{\text{Hits}}{\text{Hits} + \text{Misses}} \quad (3)$$

### 294 **Third Tier: Detection**

295 Detection was the third tier for the go/no-go task training (Figure 2). The goal of this phase was to  
296 maximize animal accuracy during consistently paced trials with invariable parameters. This phase of  
297 training was similar to the Shape2Detect task but used fixed behavioral parameters throughout the 60-  
298 minute-long sessions. These parameters outlined in Figure 3B were the same as those used during the  
299 last 20 minutes of the Shape2Detect sessions (i.e., 6 second trial window duration, 3 second hit  
300 window, 50% probability of presenting a stimulus trial, and 8 second timeouts). Animals were  
301 considered proficient when they showed at least 75% accuracy, 75% precision, 75% hit rate, 75%  
302 correct rejection rate (Equation 4), and 75% F1-score (Equation 5) with at least a 1.5 d-prime ( $d'$ ) score  
303 (Equation 6) in three total sessions. The F1-score is a measure of performance in binary classification  
304 that considers the harmonic mean, in this case, of an animal's precision and hit rate scores. The  $d'$   
305 metric is another performance indicator and common statistical measure used in psychophysical

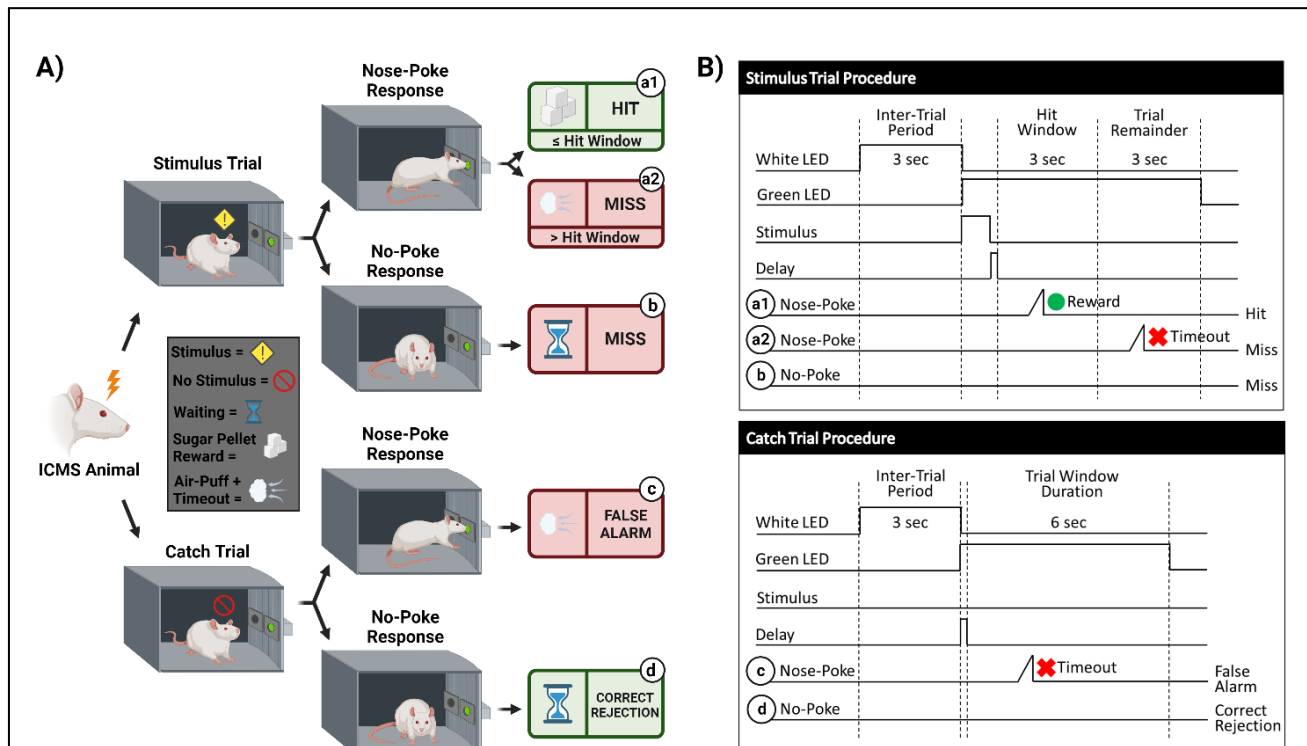
306 detection tasks and signal detection theory to quantify a subject's ability to accurately distinguish  
 307 between a signal and noise within a given task.

$$\text{Correct Rejection Rate} = \frac{\text{Correct Rejections}}{\text{Correct Rejections} + \text{False Alarms}} \quad (4)$$

$$F1 \text{ Score} = 2 \left( \frac{\text{Precision} * \text{Hit Rate}}{\text{Precision} + \text{Hit Rate}} \right) \quad (5)$$

$$d' = z(\text{Hit Rate}) - z\left(\frac{\text{False Alarms}}{\text{False Alarms} + \text{Correct Rejections}}\right) \quad (6)$$

308 After the training on the go/no-go paradigm was completed, animals underwent five additional  
 309 Detection sessions to assess baseline accuracy and subject consistency before proceeding to the go/no-  
 310 go perception threshold detection task.



**Figure 3. Behavioral paradigm for go/no-go task. (A)** Visualization of the go/no-go behavioral paradigm with possible responses to ICMS. **(B)** Illustration of the go/no-go behavioral paradigm outlining trial types. Schematic shows differences between the stimulus trials (top) and the catch trials (bottom). Depending on the response to the presented trial type, the animal can either receive a sugar pellet reward (hit) symbolized by the green circle, an 8 s timeout sequence + air puff (false alarm) symbolized by the red x, or nothing (miss/correct rejection). A 150 ms delay immediately following a stimulus presentation is used, where the nose-poke sensor does not trigger.

## 311 **Go/No-Go Perception Threshold Detection Task**

312 After rats were fully trained in the go/no-go behavioral paradigm, they were introduced to a dynamic  
313 perception threshold detection task that implemented a modified version of the up/down staircase  
314 method (A. Koivuniemi et al., 2011; Levitt, 1971), as shown in Supplementary Figure 2. The goal of  
315 this task was to approximate an estimation of an animal's perception threshold value. The first 20  
316 minutes of every perception threshold detection task began with all ICMS stimulus trials presented at  
317 the naïve threshold intensity and with 50% probability (catch trials were presented as the alternative).  
318 For the remainder of the session, the naïve threshold intensity was presented with a 33.3% probability,  
319 while a dynamic charge intensity was also presented with 33.3% probability (the remainder probability  
320 presented a catch trial). The dynamic charge intensities were presented following the modified staircase  
321 method (Figure 4A). First, we presented the dynamic charge intensity value at the maximum naïve  
322 threshold intensity. If the rat perceived the dynamic charge intensity value and nose-poked, the  
323 dynamic charge intensity value was decreased by the step size variation outlined in Table II. If the rat  
324 did not nose-poke, the dynamic charge intensity value was increased. This up/down staircase  
325 methodology was followed throughout the session.

326 For the auditory stimulus trials, dynamic tone intensity values were determined by modulating the  
327 sinusoidal wave amplitude of the training tone. Increases in sinusoidal wave amplitude resulted in a  
328 louder and more intensely perceived tone, while decreases produced a quieter and less intense tone. To  
329 create a scale for estimating auditory tone thresholds, the amplitude of the training tone was normalized  
330 to a range of 0-100%, where 0% represented silence (0 dB SPL) and 100% represented the maximum  
331 intensity of the training tone (~90 dB SPL). Similar to the ICMS variation, initial trials in the perception  
332 threshold detection task were presented at the maximum training tone intensity of 100% amplitude  
333 with a 50% probability. The remaining trials followed the modified staircase method where changes in  
334 dynamic tone intensity values were presented to the rats based on their response behavior. Step size  
335 variations of auditory tone intensity in percent amplitude are outlined in Table II.

**Table II.** Dynamic stimulus step size variation throughout a one-hour session

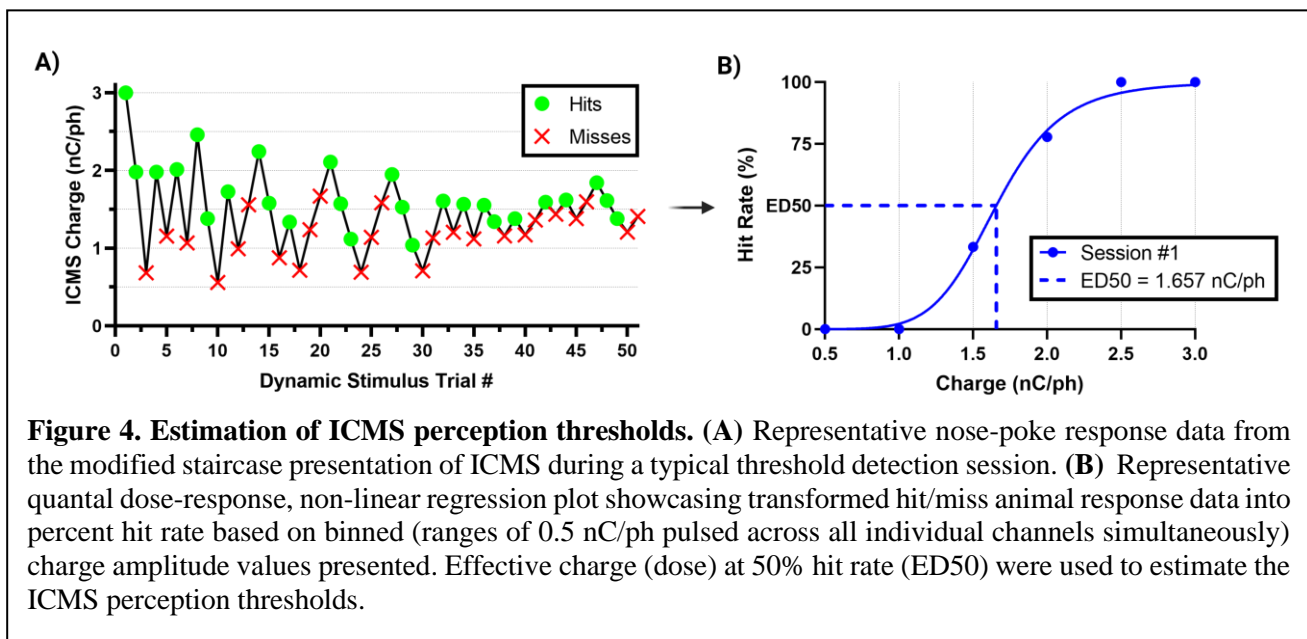
Session Time (min)	Step size variation	
	Charge Intensity (nC/ph)	Tone Intensity (% amplitude)
0-19	No variation	No variation
20-29	1.00 ± 0.40	20.00 ± 5.00
30-39	0.60 ± 0.20	10.00 ± 3.00
40-49	0.40 ± 0.10	1.00 ± 0.30
50-60	0.20 ± 0.05	0.10 ± 0.03

## 336 **Estimation of Threshold Perception**

337 We estimated perception thresholds using non-linear regression (Equation 7) in a quantal dose-  
338 response non-linear regression (Liu et al., 2022; Müller & Schmitt, 1990) in the GraphPad Prism  
339 Software ([Agonist] vs. normalized response -- Variable slope, Prism, v9.5.1). In Equation 7,  $x$

340 represents the linear dose in charge/phase or percent amplitude,  $y$  denotes the normalized response of  
 341 the percent hit rate from 0-100%, and the Hillslope represents the slope factor or steepness of the curve  
 342 shared globally between all perception threshold detection sessions per animal. We binned the dynamic  
 343 stimulus trial values into increments of 0.5 nC/ph stimulated across all individual channels  
 344 simultaneously for the ICMS group and 1% sinusoidal wave amplitude for the auditory group to  
 345 establish a quantal response (Figure 4B). We defined the effective dose in charge/phase or percent  
 346 amplitude needed to produce a 50% hit rate response (ED50) as previously demonstrated (Müller et  
 347 al., 1990). In this equation, we constrained ED50 so that it must be greater than zero. Finally, perception  
 348 threshold values were estimated individually for all animals in the ICMS and auditory groups, using  
 349 the ED50 data collected across five go/no-go perception threshold detection task sessions.

$$y = 100 * (x^{Hillslope}) / (ED50^{Hillslope} + (x^{Hillslope})) \quad (7)$$



## Data Analysis and Statistics

350 All data analysis was conducted through custom MATLAB (R2022b) scripts, GraphPad Prism (v9.5.1,  
 351 GraphPad Software, Boston, MA, US), or Statgraphics Centurion 19 (v19.4.04, Statgraphics  
 352 Technologies, Inc., The Plains, VA, US). In MATLAB, we evaluated signal detection theory  
 353 parameters (Macmillan & Creelman, 2005) for all behavioral sessions, including: accuracy, precision,  
 354 hit rate, correct rejection rate, F1-score, and  $d'$  (equations 1-6). If a session contained either zero hits,  
 355 misses, false alarms, or correct rejection responses – all of which are denominators in equations (1-6)  
 356 – then their values were adjusted in order to prevent behavioral performance scores of infinities using  
 357 a commonly accepted approach (Macmillan & Creelman, 2005). An arbitrary value of 0.5 was added  
 358 to the metric that had a score of zero (e.g., hits, misses, false alarms, or correct rejections), meanwhile  
 359 this arbitrary value of 0.5 was subtracted from its non-zero counterpart. For example, if a session  
 360 contained 119 hits and zero misses, then the adjusted values would be 118.5 hits and 0.5 misses. Then,  
 361 we generated confusion matrices based on these calculations for each group to highlight the overall  
 362 accuracies, hit rates, and correct rejection rates during the accuracy baseline Detection task sessions.



363 GraphPad Prism was used to calculate the perception threshold values. Furthermore, we calculated the  
364 average training time for each group. For statistical analysis, unpaired two-sample t-tests were used to  
365 determine significant differences between the ICMS and auditory groups. We conducted a one-tailed  
366 paired sample t-test between the ICMS results and the intragroup negative control for further validation  
367 of this methodology. We analyzed tests of normality in the data using the Shapiro-Wilk test and  
368 confirmed results by examination of their respective QQ plots. Lastly, we performed an equivalence  
369 test using Statgraphics Centurion 19 to further investigate if the average ICMS group accuracy was  
370 statistically similar or different than the average auditory group accuracy. The upper and lower  
371 differential limits were determined from the 95% CI range of the difference between means (Hazra,  
372 2017). All results are reported as the mean  $\pm$  SEM. We defined statistical significance as  $p < 0.05$ .

## 373 Results

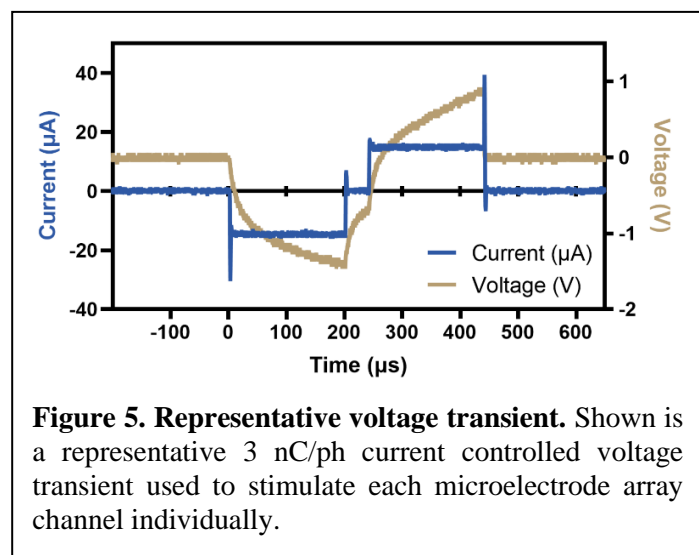
374 All animals remained above the 90% weekly weight limit for the entire duration of this study,  
375 demonstrating that food restriction did not affect their weight. Furthermore, 70% of animals completed  
376 the study with at least a 20% increase in overall weight compared to their first shaping session; the  
377 remaining animals showed less than 5% weight loss (Supplementary Table I). All animals passed the  
378 Shaping task in less than 10 sessions, resulting in no exclusions from the study due to poor  
379 performance.

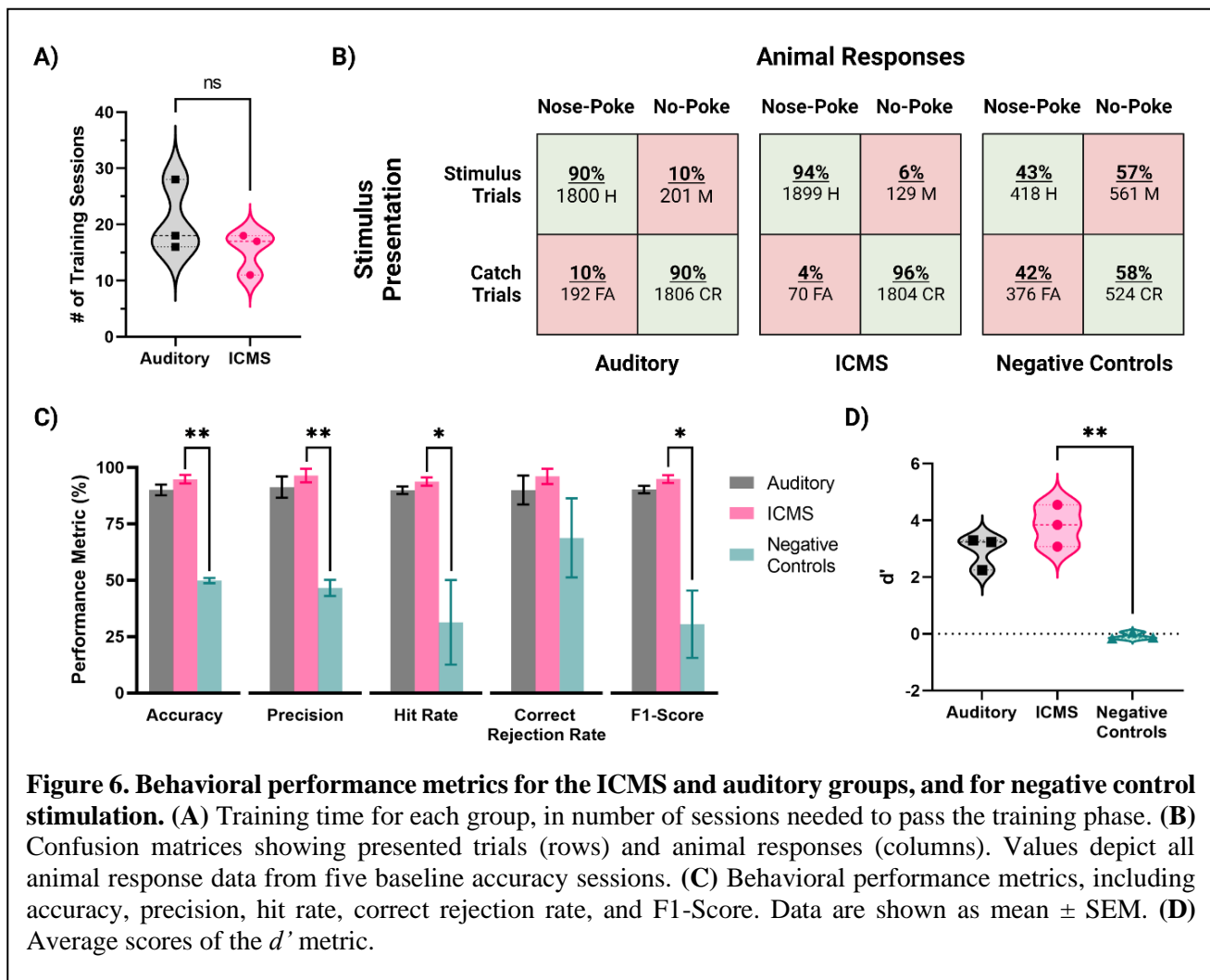
380 After implantation of the MEA into the S1FL  
381 for animals in the ICMS group, we proceeded  
382 with testing of the naïve threshold. All three  
383 animals showed a paw withdrawal in the right  
384 forepaw, corresponding to the contralateral  
385 implant location; two animals responded  
386 reliably at 3 nC/ph pulsed across all individual  
387 channels simultaneously, and one responded  
388 at 4 nC/ph. Voltage transients from each  
389 microelectrode array channel were recorded  
390 to confirm set stimulation parameters outlined  
391 within the Electrical Stimulation and  
392 Auditory Parameters subsection. Figure 5  
393 displays a representative in-vivo current-  
394 controlled voltage transient of a single  
395 channel recorded during a 3 nC/ph pulse train.

396 Voltage transients showed that the electrode delivered electrical stimulation consistently and remained  
397 unchanged throughout the sessions and validated that the applied current amplitude was delivered as  
398 set in the MATLAB custom GUI.

## 399 Go/No-Go Behavioral Training

400 Figure 6 provides the assessment of behavioral proficiency in the go/no-go task. As shown in Figure  
401 6A, animals in the ICMS group took an average of  $15.3 \pm 2.2$  sessions in total between Shaping,  
402 Shaping2Detect and Detection tasks, while animals in the auditory group took an average of  $20.7 \pm 3.7$   
403 sessions ( $p=0.28$ ). This number of sessions corresponds 4-5 weeks of training for the animal to become  
404 proficient in the go/no-go behavioral task.





**Figure 6. Behavioral performance metrics for the ICMS and auditory groups, and for negative control stimulation.** (A) Training time for each group, in number of sessions needed to pass the training phase. (B) Confusion matrices showing presented trials (rows) and animal responses (columns). Values depict all animal response data from five baseline accuracy sessions. (C) Behavioral performance metrics, including accuracy, precision, hit rate, correct rejection rate, and F1-Score. Data are shown as mean  $\pm$  SEM. (D) Average scores of the  $d'$  metric.

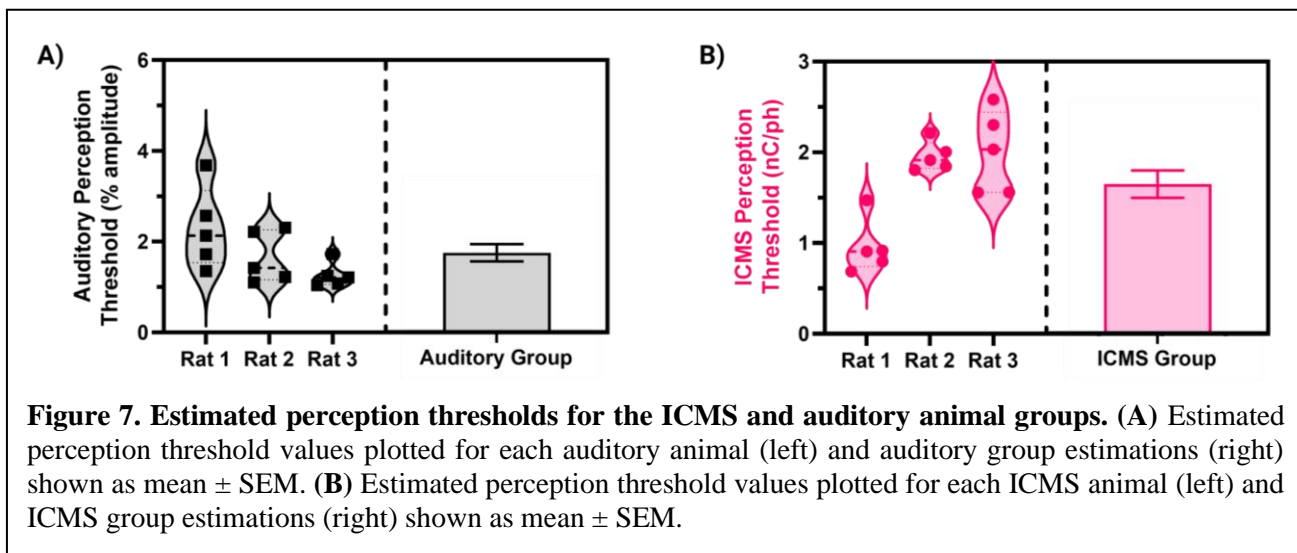
405 Then, we proceeded to assess the baseline performance on the Go/No-Go behavioral task of each  
 406 animal in five post-training sessions. Figure 6B shows the overall distribution of the total presented  
 407 trials (rows) and animal responses (columns) for each group, represented in the form of confusion  
 408 matrices. There was a total of 3,902 trials presented for the ICMS animals, including stimulus (2,028)  
 409 at the naïve threshold and catch (1,874) trials. In comparison, the auditory group received 3,999 total  
 410 trials (stimulus trials: 2,001, catch trials: 1,998). Animals in both, auditory and ICMS groups showed  
 411 similar hit rates (auditory = 90%, ICMS = 94%), showing that the animals are correctly poking upon  
 412 most stimulation trials. Similarly, animals in both groups had a high correct rejection rate (auditory =  
 413 90%, ICMS = 96%). These results indicate that both groups of animals were able to greatly recognize  
 414 a stimulus signal and respond with a nose-poke. In contrast, when the stimulation was turned off for  
 415 the ICMS group (negative control) the hit rate dropped down to only 43% and correct rejections to  
 416 only 58%, signifying random poking. Figure 6C outlines the accuracy performance metrics for all  
 417 groups. The average accuracy scores between the ICMS ( $94.7 \pm 1.9\%$ ) and auditory ( $90.0 \pm 2.4\%$ )  
 418 groups were comparable to one another ( $p = 0.19$ ). In addition, the equivalence test performed  
 419 subsequently demonstrated that the accuracy for both groups was equivalent ( $p = 0.03$ ). In contrast, the  
 420 ICMS and negative controls ( $49.8 \pm 1.2\%$ ) were significantly different ( $p=0.002$ ). The average  
 421 precision scores between the ICMS ( $96.4 \pm 3.0\%$ ) and auditory ( $91.2 \pm 4.7\%$ ) groups were comparable  
 422 ( $p = 0.41$ ); the difference between ICMS and negative controls ( $46.6 \pm 3.6\%$ ) was statistically

423 significant ( $p = 0.008$ ). The average hit rates between the ICMS ( $93.7 \pm 1.8\%$ ) and auditory ( $89.9 \pm$   
424  $1.7\%$ ) groups comparable ( $p = 0.19$ ); differences between the ICMS group and negative controls ( $31.3$   
425  $\pm 18.8\%$ ) were statistically significant ( $p = 0.04$ ). The average correct rejection rates between the ICMS  
426 ( $96.0 \pm 3.3\%$ ) and auditory ( $89.9 \pm 6.4\%$ ) groups were comparable ( $p = 0.45$ ); difference between  
427 ICMS and negative controls ( $68.7 \pm 17.6\%$ ) did not reach statistical significance ( $p = 0.10$ ). These  
428 correct rejection rates show that all animals were able to identify catch trials regardless of stimuli type.

429 The average F1-scores between the ICMS ( $94.9 \pm 1.7\%$ ) and auditory ( $90.2 \pm 1.7\%$ ) groups were  
430 comparable ( $p = 0.12$ ). The difference between the ICMS and negative controls ( $30.5 \pm 14.9\%$ ) was  
431 statistically significant ( $p = 0.03$ ), further demonstrating that animals are only poking upon stimulus  
432 presentation. In addition, the average  $d'$  scores (Figure 6D) between the ICMS ( $3.82 \pm 0.43$ ) and  
433 auditory ( $2.93 \pm 0.34$ ) groups were comparable ( $p = 0.18$ ); the difference between ICMS and negative  
434 controls ( $-0.08 \pm 0.07$ ) was found to be statistically significant ( $p = 0.008$ ), demonstrating that the  
435 animals are able to distinguish between stimulus and catch trials.

### 436 Estimated Perception Thresholds

437 Across five sessions of the go/no-go perception threshold detection task, we estimated the perception  
438 thresholds for all animals in the auditory and ICMS groups. Figure 7A (left) shows the estimated  
439 perception threshold values for individual sessions for each animal in the auditory group. The  
440 perception threshold between sessions for each animal showed a standard deviation from the mean  
441 ranging from 0.27 to 0.90% of the sinusoidal wave amplitude. Figure 7A (right) shows the summary  
442 statistics, where the perception threshold was estimated at  $1.74 \pm 0.19\%$  sinusoidal wave amplitude.  
443 Figure 7B (left) shows the estimated perception threshold values for individual sessions for each  
444 animal. Animals in the ICMS group showed a small standard deviation from the mean ranging from  
445 0.16 to 0.45 nC/ph pulsed across all individual channels simultaneously in the perception thresholds  
446 across all five sessions. Figure 7B (right) shows that the average perception threshold across all animals  
447 is  $1.64 \pm 0.15$  nC/ph pulsed across all individual channels simultaneously.



### 448 Discussion

449 In this study, we developed and validated an innovative non-pain aversive, go/no-go behavioral  
450 paradigm based on a nose-poking task to quantify rat sensory perception thresholds in response to  
451 ICMS. Our results showed that this nose-poking paradigm could reliably assess stimulation-evoked

452 sensory percepts in rats originating from ICMS in the S1FL and its accuracy was comparable to the  
453 well-established auditory discrimination task.

454 The study of auditory tone discrimination tasks in animals has a long and rich history in neuroscience  
455 research. Early studies in the 1970s focused on fundamental aspects of auditory perception in rats, such  
456 as their ability to detect pure tones and discriminate between tones of different frequencies and  
457 intensities (Kelly & Masterton, 1977). These studies laid the foundation for more complex auditory  
458 tasks developed in the following decades (Hui et al., 2009; Sloan et al., 2009). One such task is the  
459 go/no-go task, which once involved training rats to press a lever in response to a specific tone (the “go”  
460 tone) and withhold their response to other tones (“no-go” tones) (Engineer et al., 2008). Then, this  
461 go/no-go task was modified from lever-pressing to nose-poking because it was found to require less  
462 experimenter intervention for a naïve rat to reliably perform the task with the addition of a higher  
463 baseline rate of responding and lower between-group variability (Mekarski, 1988; Schindler et al.,  
464 1993). This nose-poke go/no-go behavioral paradigm has been used by multiple research groups and  
465 is widely accepted because of its straightforwardness to train rats with nose-poking being an innate  
466 exploration behavior, the hardware is available off-the-shelf and does not require complex motors and  
467 controls, and it has shown high accuracy rates of up to ~90% (Riley et al., 2021; Sloan et al., 2009).  
468 Overall, the history of auditory tone discrimination tasks in rats highlights their broad utility as a model  
469 system for studying auditory perception and processing. For the development of the behavioral  
470 paradigm presented here, we built upon this nose-poke-based, go/no-go paradigm.

471 To validate the presented behavioral paradigm, we compared the ICMS group to an auditory  
472 discrimination control group. Using the auditory discrimination group as positive controls allowed us  
473 to establish an effective baseline to compare accuracy and reliability of our behavioral paradigm.  
474 Within our study, the auditory control group showed an accuracy of ~90% and demonstrated an  
475 auditory tone threshold of approximately 2% amplitude (~65 dB SPL), which is comparable to previous  
476 literature (Engineer et al., 2008; Riley et al., 2021; Sloan et al., 2009). These results validate our  
477 implementation of the nose-poke behavioral paradigm, and our method of using non-linear regression  
478 for estimating threshold perception. The ICMS group had a comparable accuracy to the auditory  
479 control group of ~95%, which validates the use of this go/no-go nose-poke task for the assessment of  
480 ICMS perception. Furthermore, animals in the ICMS group underwent a negative control phase at the  
481 end of the study to confirm that the nose-poking behavior was neither random nor were the animals  
482 nose-poking on any confounding cues. Results from this second phase of the investigation yielded a  
483 50% accuracy, which is an indication of random poking, which is consistent with the present  
484 methodology.

485 Using the validated quantal non-linear regression at the ED50 level, we established that the average  
486 electrical perception threshold across three animals was approximately 1.64 nC/ph pulsed across all 10  
487 individual channels simultaneously with the lowest animal averaging 0.96 nC/ph. Previous animal  
488 behavioral paradigms have been developed to study sensory and visual perception via ICMS, including  
489 rodents, cats, non-human primates, and humans (Fernández et al., 2021; Lycke et al., 2023; Ni &  
490 Maunsell, 2010; Rousche & Normann, 1999; Tehovnik, 1996), which have identified different  
491 thresholds of perception. Urdaneta et al. (2022) demonstrated perception thresholds ranging between  
492 6.4 and 10.7 nC/ph for rat cortex, when stimulating Ir electrode sites individually. The same group has  
493 demonstrated that delivering electrical stimulation through two or more electrode sites simultaneously  
494 can reduce the perception threshold (Kunigk et al., 2022) by at least 53% of the single site perception  
495 threshold. Other studies have shown lower perception thresholds using traditional microelectrode  
496 arrays in cat somatosensory cortex (Rousche & Normann, 1999) with an approximate threshold of 1.5  
497 nC/ph; non-human primates between 1-2 nC/ph (Callier et al., 2015; Ferroni et al., 2017; Ni &



498 Maunsell, 2010); and human studies ranging from 0.4-3 nC/ph (Fernández et al., 2021; Flesher et al.,  
499 2016; Hughes et al., 2021; Schmidt et al., 1996). A different study targeting the primary somatosensory  
500 cortex in mice (Lycke et al., 2023) found the lowest perception threshold of 0.25 nC/ph stimulating  
501 individual and multiple electrode sites simultaneously. It should be noted that stimulation parameters,  
502 MEAs, implantation targets, and number of electrode sites pulsed are not consistent between these  
503 studies. Nevertheless, results from these prior studies demonstrate broad consistency with the estimated  
504 perception thresholds in the present work.

505 Some Institutional Animal Care and Use Committees (IACUCs) require ad libitum access to water for  
506 a minimum of 1 hour for at least every 12 hours, which may further limit the deployment of previous  
507 water-restrictive behavioral paradigms to other research groups. Food restriction is preferred over  
508 water restriction by most IACUCs. In this paradigm we mildly restricted food intake, an approach  
509 ethically preferred over water deprivation, to ensure rodent engagement during the behavioral task. At  
510 the end of each session, animals were given supplemental feed to ensure appropriate nutrition.  
511 However, both water deprivation and food restriction have been associated with a stress response  
512 characterized by an upregulation of adrenal corticosterone (Dietze et al., 2016; Vasilev et al., 2021). It  
513 is unknown whether this stress response may play a role in the reliability of intracortical MEAs and  
514 stability of ICMS. Future work may consider methods to avoid food restriction while participating in  
515 the nose-poke task.

516 A final limitation of this study was the training time, resulting from having a mostly positive  
517 reinforcement behavioral task. Animals in this study underwent one week of Shaping, three to four  
518 weeks of Shape2Detect, one to two weeks of Detection and one week of the accuracy baseline  
519 Detection task assessment for a total of six to eight weeks of training. During this time, we could not  
520 assess perception thresholds, meaning that we could not assess changes during the first six to eight  
521 weeks post-implantation. Previous studies (Urdaneta et al., 2022) have reported training phases of up  
522 to eight weeks post implantation, comparable to the number of sessions required for training in the  
523 present paradigm. However, this acute phase is known for presenting changes to the MEA surrounding  
524 tissues, including myelin degeneration and glial encapsulation. Assessment during the acute phase  
525 would provide information regarding perception threshold and documented tissue response. In future  
526 studies, we will optimize the training time to assess perception thresholds as early as possible after  
527 implantation by increasing the probability of presenting a stimulus trial during the Shape2Detect and  
528 Detection phases of training and lowering the threshold to pass from one training stage to the next.

529 Despite these limitations, this study presents an effective behavioral paradigm for evaluating ICMS-  
530 evoked somatosensory percepts in rats. However, there are still known challenges associated with rat  
531 ICMS studies apart from establishing a reliable perception threshold indicator. For example, it has been  
532 well-documented that perception thresholds change over time (Bjånes et al., 2022; Callier et al., 2015;  
533 Hughes et al., 2021; A. Koivuniemi et al., 2011; Kunigk et al., 2022; Lycke et al., 2023). In the future  
534 we will employ this behavioral paradigm to study ICMS-evoked perception threshold stability of novel  
535 MEA device technologies that aim at improving the long-term reliability of the neural interface.  
536 Finally, the control software that we have developed for this paradigm is open-source and available to  
537 download at no cost. This will allow research groups who are interested in evaluating long-term  
538 stability of novel stimulating MEAs (especially those whose IACUC prefer food restriction over water  
539 deprivation in rodents) to easily adopt this go/no-go behavioral paradigm using hardware available off-  
540 the-shelf.

## 541 **Conclusion**

542 In this study we presented a new, highly accurate behavioral paradigm to assess ICMS-evoked  
543 somatosensory perception thresholds. This paradigm builds upon well-established and accepted  
544 auditory discrimination tasks with comparable results, validating the go/no-go behavioral task for  
545 assessment of ICMS-evoked percepts. Full deployment of this paradigm establishes a new platform for  
546 elucidating the information processing principles in the neural circuits related to neuroprosthetic  
547 sensory perception and for studying the performance of novel MEA device technologies using freely  
548 moving rats. Future studies will assess how MEA design and cortical circuitry impacts stimulus  
549 response-time circuitry, threshold sensitivity, and selectivity discrimination for the primary  
550 somatosensory cortex.

## 551 **Data Availability Statement**

552 The data is available upon request to the corresponding author. MATLAB custom GUI behavior  
553 software is available as an open-source package on GitHub ([https://github.com/Neuronal-Networks-  
554 and-Interfaces-Lab/Stimulation-Evoked\\_Perception\\_Behavioral\\_Software.git](https://github.com/Neuronal-Networks-and-Interfaces-Lab/Stimulation-Evoked_Perception_Behavioral_Software.git)).

## 555 **Ethics Statement**

556 All aspects of this study were conducted under our 21-15 protocol endorsed by the Institutional Animal  
557 Care and Use Committee (IACUC) at the University of Texas at Dallas and were in accordance with  
558 the ARRIVE essential 10 guidelines.

## 559 **Author Contributions**

560 **Thomas Smith:** Conceptualization, Methodology, Software, Validation, Formal Analysis,  
561 Investigation, Resources, Writing – Original Draft, Visualization, Project Administration. **Yupeng**  
562 **Wu:** Investigation. **Claire Cheon:** Investigation. **Arlin Khan:** Investigation. **Hari Srinivasan:**  
563 Investigation. **Jeffrey Capadona:** Conceptualization, Writing – Review and Editing, Funding  
564 Acquisition. **Stuart Cogan:** Conceptualization, Resources, Writing – Review and Editing, Funding  
565 Acquisition. **Joseph Pancrazio:** Conceptualization, Resources, Writing – Review and Editing, Project  
566 Administration, Funding Acquisition. **Crystal Engineer:** Methodology, Resources, Writing – Review  
567 and Editing. **Ana Hernandez-Reynoso:** Conceptualization, Methodology, Software, Formal Analysis,  
568 Writing – Review and Editing, Project Administration.

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582 Shape2Detect task used in this study.

583 **Declaration of Competing Interests**

584 Crystal Engineer is married to an employee of Microtransponder, Inc, a company that develops vagus  
585 nerve stimulation therapies. Microtransponder was not involved in the development or analysis of this  
586 research. All other authors declare that they possess no competing interests.

## 587 **References**

- 588 Abolafia, J., Martinez-Garcia, M., Deco, G., & Sanchez-Vives, M. (2011). Slow Modulation of  
589 Ongoing Discharge in the Auditory Cortex during an Interval-Discrimination Task. *Frontiers*  
590 *in Integrative Neuroscience*, 5. <https://doi.org/10.3389/fnint.2011.00060>
- 591 Armenta Salas, M., Bashford, L., Kellis, S., Jafari, M., Jo, H., Kramer, D., Shanfield, K., Pejsa, K.,  
592 Lee, B., Liu, C. Y., & Andersen, R. A. (2018). Proprioceptive and cutaneous sensations in  
593 humans elicited by intracortical microstimulation. *eLife*, 7, e32904.  
594 <https://doi.org/10.7554/eLife.32904>
- 595 Bailey, J., & Taylor, K. (2016). Non-human Primates in Neuroscience Research: The Case against its  
596 Scientific Necessity. *Alternatives to Laboratory Animals*, 44(1), 43-69.  
597 <https://doi.org/10.1177/026119291604400101>
- 598 Barrese, J. C., Rao, N., Paroo, K., Triebwasser, C., Vargas-Irwin, C., Franquemont, L., & Donoghue,  
599 J. P. (2013). Failure mode analysis of silicon-based intracortical microelectrode arrays in non-  
600 human primates. *Journal of Neural Engineering*, 10(6), 066014. [https://doi.org/10.1088/1741-](https://doi.org/10.1088/1741-2560/10/6/066014)  
601 [2560/10/6/066014](https://doi.org/10.1088/1741-2560/10/6/066014)
- 602 Bjånes, D. A., Bashford, L., Pejsa, K., Lee, B., Liu, C. Y., & Andersen, R. A. (2022). Multi-channel  
603 intra-cortical micro-stimulation yields quick reaction times and evokes natural  
604 somatosensations in a human participant. *medRxiv*, 2022.2008.2008.22278389.  
605 <https://doi.org/10.1101/2022.08.08.22278389>
- 606 Callier, T., Schluter, E. W., Tabot, G. A., Miller, L. E., Tenore, F. V., & Bensmaia, S. J. (2015).  
607 Long-term stability of sensitivity to intracortical microstimulation of somatosensory cortex.  
608 *Journal of Neural Engineering*, 12(5). <https://doi.org/10.1088/1741-2560/12/5/056010>
- 609 Carè, M., Averna, A., Barban, F., Semprini, M., De Michieli, L., Nudo, R. J., Guggenmos, D. J., &  
610 Chiappalone, M. (2022). The impact of closed-loop intracortical stimulation on neural activity  
611 in brain-injured, anesthetized animals. *Bioelectronic Medicine*, 8(1), 4.  
612 <https://doi.org/10.1186/s42234-022-00086-y>
- 613 Carvalho, C., Gaspar, A., Knight, A., & Vicente, L. (2019). Ethical and Scientific Pitfalls Concerning  
614 Laboratory Research with Non-Human Primates, and Possible Solutions. *Animals*, 9(1).  
615 <https://doi.org/10.3390/ani9010012>
- 616 Christie, B., Osborn, L. E., McMullen, D. P., Pawar, A. S., Thomas, T. M., Bensmaia, S. J., Celnik,  
617 P. A., Fifer, M. S., & Tenore, F. V. (2022). Perceived timing of cutaneous vibration and  
618 intracortical microstimulation of human somatosensory cortex. *Brain Stimulation: Basic,*  
619 *Translational, and Clinical Research in Neuromodulation*, 15(3), 881-888.  
620 <https://doi.org/10.1016/j.brs.2022.05.015>
- 621 Dietze, S., Lees, K. R., Fink, H., Brosda, J., & Voigt, J.-P. (2016). Food Deprivation, Body Weight  
622 Loss and Anxiety-Related Behavior in Rats. *Animals*, 6(1).
- 623 El-Ayache, N., & Galligan, J. J. (2020). Chapter 28 - The Rat in Neuroscience Research. In M. A.  
624 Suckow, F. C. Hankenson, R. P. Wilson, & P. L. Foley (Eds.), *The Laboratory Rat (Third*  
625 *Edition)* (pp. 1003-1022). Academic Press. [https://doi.org/https://doi.org/10.1016/B978-0-12-](https://doi.org/10.1016/B978-0-12-814338-4.00028-3)  
626 [814338-4.00028-3](https://doi.org/10.1016/B978-0-12-814338-4.00028-3)
- 627 Engineer, C. T., Perez, C. A., Chen, Y. T. H., Carraway, R. S., Reed, A. C., Shetake, J. A.,  
628 Jakkamsetti, V., Chang, K. Q., & Kilgard, M. P. (2008). Cortical activity patterns predict  
629 speech discrimination ability. *Nature Neuroscience*, 11(5). <https://doi.org/10.1038/nn.2109>

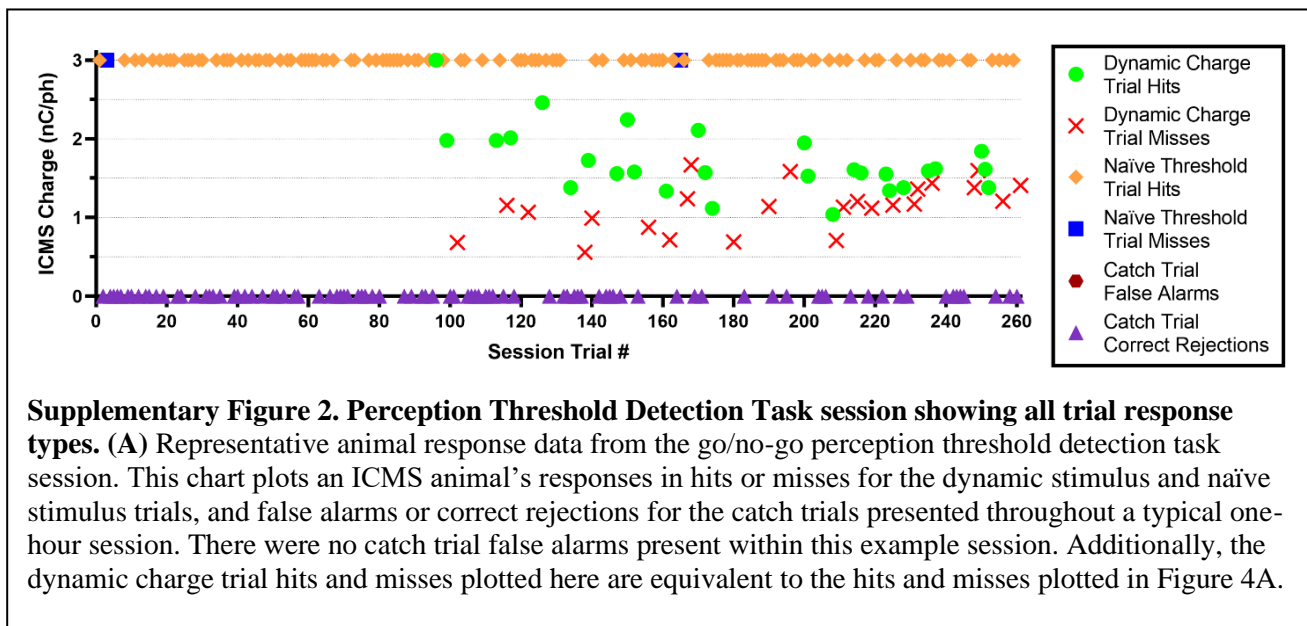
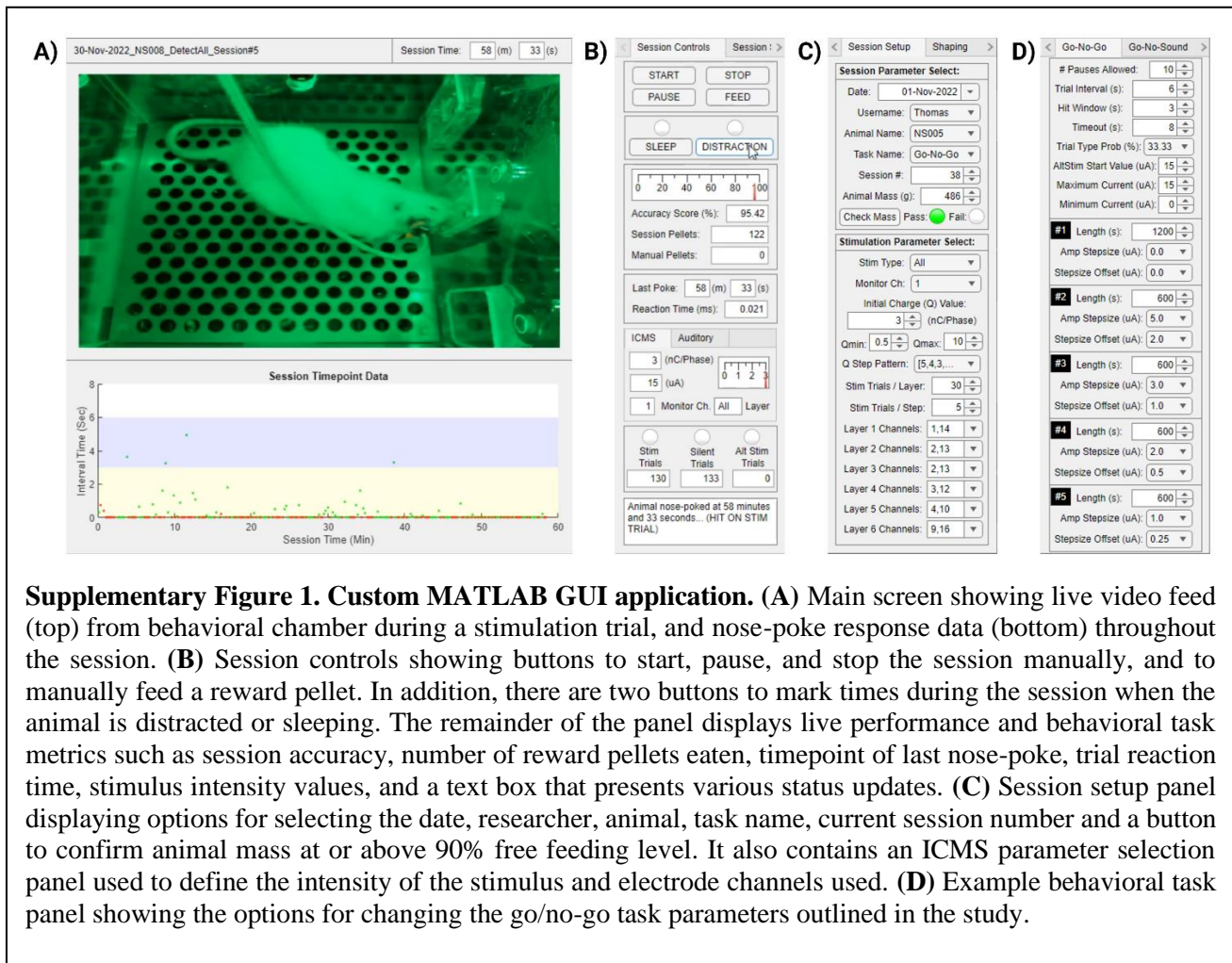


- 630 Ereifej, E. S., Rial, G. M., Hermann, J. K., Smith, C. S., Meade, S. M., Rayyan, J. M., Chen, K.,  
631 Feng, H., & Capadona, J. R. (2018). Implantation of Neural Probes in the Brain Elicits  
632 Oxidative Stress [Original Research]. *Frontiers in Bioengineering and Biotechnology*, 6.  
633 <https://doi.org/10.3389/fbioe.2018.00009>
- 634 Fernández, E., Alfaro, A., Soto-Sánchez, C., Gonzalez-Lopez, P., Lozano, A. M., Peña, S., Grima,  
635 M. D., Rodil, A., Gómez, B., Chen, X., Roelfsema, P. R., Rolston, J. D., Davis, T. S., &  
636 Normann, R. A. (2021). Visual percepts evoked with an intracortical 96-channel  
637 microelectrode array inserted in human occipital cortex. *The Journal of Clinical*  
638 *Investigation*, 131(23). <https://doi.org/10.1172/JCI151331>
- 639 Ferroni, C. G., Maranesi, M., Livi, A., Lanzilotto, M., & Bonini, L. (2017). Comparative  
640 performance of linear multielectrode probes and single-tip electrodes for intracortical  
641 microstimulation and single-neuron recording in macaque monkey. *Frontiers in Systems*  
642 *Neuroscience*, 11. <https://doi.org/10.3389/fnsys.2017.00084>
- 643 Flesher, S. N., Collinger, J. L., Foldes, S. T., Weiss, J. M., Downey, J. E., Tyler-Kabara, E. C.,  
644 Bensmaia, S. J., Schwartz, A. B., Boninger, M. L., & Gaunt, R. A. (2016). Intracortical  
645 microstimulation of human somatosensory cortex. *Science Translational Medicine*, 8(361),  
646 361ra141-361ra141. <https://doi.org/doi:10.1126/scitranslmed.aaf8083>
- 647 Flesher, S. N., Downey, J. E., Weiss, J. M., Hughes, C. L., Herrera, A. J., Tyler-Kabara, E. C.,  
648 Boninger, M. L., Collinger, J. L., & Gaunt, R. A. (2021). A brain-computer interface that  
649 evokes tactile sensations improves robotic arm control. *Science*, 372(6544), 831-836.  
650 <https://doi.org/10.1126/science.abd0380>
- 651 Green, M., Terman, M., & Terman, J. S. (1979). Comparison of yes-no and latency measures of  
652 auditory intensity discrimination. *J Exp Anal Behav*, 32(3), 363-372.  
653 <https://doi.org/10.1901/jeab.1979.32-363>
- 654 Hazra, A. (2017). Using the confidence interval confidently. *J Thorac Dis*, 9(10), 4125-4130.  
655 <https://doi.org/10.21037/jtd.2017.09.14>
- 656 He, F., Sun, Y., Jin, Y., Yin, R., Zhu, H., Rathore, H., Xie, C., & Luan, L. (2022). Longitudinal  
657 neural and vascular recovery following ultraflexible neural electrode implantation in aged  
658 mice. *Biomaterials*, 291, 121905-121905.  
659 <https://doi.org/https://doi.org/10.1016/j.biomaterials.2022.121905>
- 660 Hughes, C. L., Flesher, S. N., Weiss, J. M., Downey, J. E., Boninger, M., Collinger, J. L., & Gaunt,  
661 R. A. (2021). Neural stimulation and recording performance in human sensorimotor cortex  
662 over 1500 days. *Journal of Neural Engineering*, 18(4). [https://doi.org/10.1088/1741-](https://doi.org/10.1088/1741-2552/ac18ad)  
663 [2552/ac18ad](https://doi.org/10.1088/1741-2552/ac18ad)
- 664 Hui, G. K., Wong, K. L., Chavez, C. M., Leon, M. I., Robin, K. M., & Weinberger, N. M. (2009).  
665 Conditioned tone control of brain reward behavior produces highly specific representational  
666 gain in the primary auditory cortex. *Neurobiology of Learning and Memory*, 92(1), 27-34.  
667 <https://doi.org/https://doi.org/10.1016/j.nlm.2009.02.008>
- 668 Kelly, J. B., & Masterton, B. (1977). Auditory sensitivity of the albino rat. *J Comp Physiol Psychol*,  
669 91(4), 930-936. <https://doi.org/10.1037/h0077356>
- 670 Koivuniemi, A., Wilks, S. J., Woolley, A. J., & Otto, K. J. (2011). Chapter 10 - Multimodal,  
671 longitudinal assessment of intracortical microstimulation. In J. Schouenborg, M. Garwicz, &  
672 N. Danielsen (Eds.), *Progress in Brain Research* (Vol. 194, pp. 131-144). Elsevier.  
673 <https://doi.org/https://doi.org/10.1016/B978-0-444-53815-4.00011-X>

- 674 Koivuniemi, A. S., Regele, O. B., Brenner, J. H., & Otto, K. J. (2011). Rat behavioral model for  
675 high-throughput parametric studies of intracortical microstimulation. *Annu Int Conf IEEE*  
676 *Eng Med Biol Soc*, 2011, 7541-7544. <https://doi.org/10.1109/iembs.2011.6091859>
- 677 Kozai, T. D. Y., Marzullo, T. C., Hooi, F., Langhals, N. B., Majewska, A. K., Brown, E. B., &  
678 Kipke, D. R. (2010). Reduction of neurovascular damage resulting from microelectrode  
679 insertion into the cerebral cortex using in vivo two-photon mapping. *Journal of Neural*  
680 *Engineering*, 7(4). <https://doi.org/10.1088/1741-2560/7/4/046011>
- 681 Kramer, D. R., Kellis, S., Barbaro, M., Salas, M. A., Nune, G., Liu, C. Y., Andersen, R. A., & Lee,  
682 B. (2019). Technical considerations for generating somatosensation via cortical stimulation in  
683 a closed-loop sensory/motor brain-computer interface system in humans. *Journal of Clinical*  
684 *Neuroscience*, 63. <https://doi.org/10.1016/j.jocn.2019.01.027>
- 685 Kunigk, N. G., Urdaneta, M. E., Malone, I. G., Delgado, F., & Otto, K. J. (2022). Reducing  
686 Behavioral Detection Thresholds per Electrode via Synchronous, Spatially-Dependent  
687 Intracortical Microstimulation. *Frontiers in Neuroscience*, 16.  
688 <https://doi.org/10.3389/fnins.2022.876142>
- 689 Levitt, H. (1971). Transformed Up-Down Methods in Psychoacoustics. *The Journal of the Acoustical*  
690 *Society of America*, 49(2B). <https://doi.org/10.1121/1.1912375>
- 691 Liu, J., Earp, J. C., Lertora, J. J. L., & Wang, Y. (2022). Chapter 19 - Dose-effect and concentration-  
692 effect analysis. In S.-M. Huang, J. J. L. Lertora, P. Vicini, & A. J. Atkinson (Eds.), *Atkinson's*  
693 *Principles of Clinical Pharmacology (Fourth Edition)* (pp. 359-376). Academic Press.  
694 <https://doi.org/https://doi.org/10.1016/B978-0-12-819869-8.00039-2>
- 695 Lycke, R., Kim, R., Zolotavin, P., Montes, J., Sun, Y., Koszeghy, A., Altun, E., Noble, B., Yin, R.,  
696 He, F., Totah, N., Xie, C., & Luan, L. (2023). Low-threshold, high-resolution, chronically  
697 stable intracortical microstimulation by ultraflexible electrodes. *bioRxiv*.  
698 <https://doi.org/10.1101/2023.02.20.529295>
- 699 Macmillan, N. A., & Creelman, C. D. (2005). *Detection theory: A user's guide, 2nd ed.* Lawrence  
700 Erlbaum Associates Publishers.
- 701 Mekarski, J. E. (1988). Main effects of current and pimozide on prepared and learned self-stimulation  
702 behaviors are on performance not reward. *Pharmacology Biochemistry and Behavior*, 31(4),  
703 845-853. [https://doi.org/https://doi.org/10.1016/0091-3057\(88\)90394-2](https://doi.org/https://doi.org/10.1016/0091-3057(88)90394-2)
- 704 Müller, H.-G., & Schmitt, T. (1990). Choice of Number of Doses for Maximum Likelihood  
705 Estimation of the ED50 for Quantal Dose-Response Data. *Biometrics*, 46(1), 117-129.  
706 <https://doi.org/10.2307/2531635>
- 707 Ni, A. M., & Maunsell, J. H. R. (2010). Microstimulation Reveals Limits in Detecting Different  
708 Signals from a Local Cortical Region. *Current Biology*, 20(9), 824-828.  
709 <https://doi.org/10.1016/j.cub.2010.02.065>
- 710 Öztürk, S., Devecioğlu, I., Beygi, M., Atasoy, A., Mutlu, Ş., Özkan, M., & Güçlü, B. (2019). Real-  
711 Time Performance of a Tactile Neuroprosthesis on Awake Behaving Rats. *IEEE Transactions*  
712 *on Neural Systems and Rehabilitation Engineering*, 27(5), 1053-1062.  
713 <https://doi.org/10.1109/TNSRE.2019.2910320>
- 714 Page, D. M., George, J. A., Wendelken, S. M., Davis, T. S., Kluger, D. T., Hutchinson, D. T., &  
715 Clark, G. A. (2021). Discriminability of multiple cutaneous and proprioceptive hand percepts  
716 evoked by intraneural stimulation with Utah slanted electrode arrays in human amputees.

- 717 *Journal of NeuroEngineering and Rehabilitation*, 18(1), 12. [https://doi.org/10.1186/s12984-](https://doi.org/10.1186/s12984-021-00808-4)  
718 021-00808-4
- 719 Pancrazio, J. J., Deku, F., Ghazavi, A., Stiller, A. M., Rihani, R., Frewin, C. L., Varner, V. D.,  
720 Gardner, T. J., & Cogan, S. F. (2017). Thinking Small: Progress on Microscale  
721 Neurostimulation Technology. *Neuromodulation*, 20. <https://doi.org/10.1111/ner.12716>
- 722 Pankevich, D. E. (2012). Animals in Neuroscience Research. In I. o. M. U. N. R. C. (US) (Ed.),  
723 *International Animal Research Regulations: Impact on Neuroscience Research: Workshop*  
724 *Summary*. Washington (DC): National Academies Press (US).  
725 <https://www.ncbi.nlm.nih.gov/books/NBK100126/>
- 726 Potter, K. A., Buck, A. C., Self, W. K., & Capadona, J. R. (2012). Stab injury and device  
727 implantation within the brain results in inversely multiphasic neuroinflammatory and  
728 neurodegenerative responses. *Journal of Neural Engineering*, 9(4), 046020.  
729 <https://doi.org/10.1088/1741-2560/9/4/046020>
- 730 Rajan, A. T., Boback, J. L., Dammann, J. F., Tenore, F. V., Wester, B. A., Otto, K. J., Gaunt, R. A.,  
731 & Bensmaia, S. J. (2015). The effects of chronic intracortical microstimulation on neural  
732 tissue and fine motor behavior. *Journal of Neural Engineering*, 12(6), 066018.  
733 <https://doi.org/10.1088/1741-2560/12/6/066018>
- 734 Riley, J. R., Borland, M. S., Tamaoki, Y., Skipton, S. K., & Engineer, C. T. (2021). Auditory  
735 Brainstem Responses Predict Behavioral Deficits in Rats with Varying Levels of Noise-  
736 Induced Hearing Loss. *Neuroscience*, 477, 63-75.  
737 <https://doi.org/https://doi.org/10.1016/j.neuroscience.2021.10.003>
- 738 Rousche, P. J., & Normann, R. A. (1999). Chronic intracortical microstimulation (ICMS) of cat  
739 sensory cortex using the utah intracortical electrode array. *IEEE Transactions on*  
740 *Rehabilitation Engineering*, 7(1). <https://doi.org/10.1109/86.750552>
- 741 Schindler, C. W., Thorndike, E. B., & Goldberg, S. R. (1993). Acquisition of a nose-poke response in  
742 rats as an operant. *Bulletin of the Psychonomic Society*, 31(4), 291-294.  
743 <https://doi.org/10.3758/BF03334932>
- 744 Schmidt, E. M., Bak, M. J., Hambrecht, F. T., Kufta, C. V., O'Rourke, D. K., & Vallabhanath, P.  
745 (1996). Feasibility of a visual prosthesis for the blind based on intracortical micro stimulation  
746 of the visual cortex. *Brain*, 119(2), 507-522. <https://doi.org/10.1093/brain/119.2.507>
- 747 Shannon, R. V. (1992). A Model of Safe Levels for Electrical Stimulation. *IEEE Transactions on*  
748 *Biomedical Engineering*, 39(4). <https://doi.org/10.1109/10.126616>
- 749 Sloan, A. M., Dodd, O. T., & Rennaker, R. L. (2009). Frequency discrimination in rats measured  
750 with tone-step stimuli and discrete pure tones. *Hearing Research*, 251(1), 60-69.  
751 <https://doi.org/https://doi.org/10.1016/j.heares.2009.02.009>
- 752 Sturgill, B., Radhakrishna, R., Thai, T. T. D., Patnaik, S. S., Capadona, J. R., & Pancrazio, J. J.  
753 (2022). Characterization of Active Electrode Yield for Intracortical Arrays: Awake versus  
754 Anesthesia. *Micromachines*, 13(3). <https://doi.org/10.3390/mi13030480>
- 755 Tehovnik, E. J. (1996). Electrical stimulation of neural tissue to evoke behavioral responses. *Journal*  
756 *of Neuroscience Methods*, 65. [https://doi.org/10.1016/0165-0270\(95\)00131-X](https://doi.org/10.1016/0165-0270(95)00131-X)
- 757 Urdaneta, M. E., Kunigk, N. G., Currllin, S., Delgado, F., Fried, S. I., & Otto, K. J. (2022). The Long-  
758 Term Stability of Intracortical Microstimulation and the Foreign Body Response Are Layer  
759 Dependent. *Frontiers in Neuroscience*, 16. <https://doi.org/10.3389/fnins.2022.908858>

- 760 Urdaneta, M. E., Kunigk, N. G., Delgado, F., Fried, S. I., & Otto, K. J. (2021). Layer-specific  
761 parameters of intracortical microstimulation of the somatosensory cortex. *Journal of Neural*  
762 *Engineering*, 18(5). <https://doi.org/10.1088/1741-2552/abedde>
- 763 Vasilev, D., Havel, D., Liebscher, S., Slesiona-Kuenzel, S., Logothetis, N. K., Schenke-Layland, K.,  
764 & Totah, N. K. (2021). Three Water Restriction Schedules Used in Rodent Behavioral Tasks  
765 Transiently Impair Growth and Differentially Evoke a Stress Hormone Response without  
766 Causing Dehydration. *eneuro*, 8(6), ENEURO.0424-0421.2021.  
767 <https://doi.org/10.1523/ENEURO.0424-21.2021>





**Supplementary Table I. Animal Weight Progression**

<b>Animal Group</b>	<b>Animal</b>	<b>Session Weight</b>		
		<b>First Session (g)</b>	<b>Last Session (g)</b>	<b>% Change</b>
ICMS	Rat 1	412	578	40.29
ICMS	Rat 2	355	517	45.63
ICMS	Rat 3	522	503	-3.64
Auditory	Rat 1	452	569	25.88
Auditory	Rat 2	550	523	-4.91
Auditory	Rat 3	362	436	20.44