



## t4 Workshop Report\*

# Biology-Inspired Microphysiological System Approaches to Solve the Prediction Dilemma of Substance Testing

Uwe Marx<sup>1</sup>, Tommy B. Andersson<sup>2,3</sup>, Anthony Bahinski<sup>4</sup>, Mario Beilmann<sup>5</sup>, Sonja Beken<sup>6</sup>, Flemming R. Cassee<sup>7,8</sup>, Murat Cirit<sup>9</sup>, Mardas Daneshian<sup>10</sup>, Susan Fitzpatrick<sup>11</sup>, Olivier Frey<sup>12</sup>, Claudia Gaertner<sup>13</sup>, Christoph Giese<sup>14</sup>, Linda Griffith<sup>9</sup>, Thomas Hartung<sup>10,15</sup>, Minne B. Heringa<sup>7</sup>, Julia Hoeng<sup>16</sup>, Wim H. de Jong<sup>7</sup>, Hajime Kojima<sup>17</sup>, Jochen Kuehn<sup>18</sup>, Marcel Leist<sup>10</sup>, Andreas Luch<sup>19</sup>, Ilka Maschmeyer<sup>1</sup>, Dmitry Sakharov<sup>20</sup>, Adrienne J. A. M. Sips<sup>7</sup>, Thomas Steger-Hartmann<sup>21</sup>, Danilo A. Tagle<sup>22</sup>, Alexander Tonevitsky<sup>23</sup>, Tewes Tralau<sup>19</sup>, Sergej Tsyb<sup>24</sup>, Anja van de Stolpe<sup>25</sup>, Rob Vandebriel<sup>7</sup>, Paul Vulto<sup>26</sup>, Jufeng Wang<sup>27</sup>, Joachim Wiest<sup>28</sup>, Marleen Rodenburg<sup>7</sup> and Adrian Roth<sup>29</sup>

<sup>1</sup>TissUse GmbH, Berlin, Germany; <sup>2</sup>AstraZeneca, Cardiovascular and Metabolic Diseases, Innovative Medicines and Early Development Biotech Unit, Mölndal, Sweden; <sup>3</sup>Section of Pharmacogenetics, Department of Physiology and Pharmacology, Karolinska Institutet, Stockholm, Sweden; <sup>4</sup>Wyss Institute for Biologically Inspired Engineering at Harvard University, Boston, MA, USA; <sup>5</sup>Boehringer Ingelheim Pharma GmbH & Co. KG, Non-clinical Drug Safety, Biberach, Germany; <sup>6</sup>Federal Agency for Medicines and Health Products, Brussels, Belgium; <sup>7</sup>National Institute for Public Health & the Environment, Bilthoven, The Netherlands; <sup>8</sup>Institute for Risk Assessment Science, Utrecht University, The Netherlands; <sup>9</sup>Massachusetts Institute of Technology, Cambridge, MA, USA; <sup>10</sup>Center for Alternatives to Animal Testing-Europe, University of Konstanz, Konstanz, Germany; <sup>11</sup>US Food and Drug Administration, Center for Food Safety and Applied Nutrition, College Park, MD, USA; <sup>12</sup>ETH Zurich, Dept. Biosystems Science and Engineering, Bio Engineering Laboratory, Basel, Switzerland; <sup>13</sup>microfluidic ChipShop GmbH, Jena, Germany; <sup>14</sup>ProBioGen AG, Berlin, Germany; <sup>15</sup>Center for Alternatives to Animal Testing, Bloomberg School of Public Health, Johns Hopkins University, Baltimore, MD, USA; <sup>16</sup>Philip Morris International R&D, Neuchâtel, Switzerland; <sup>17</sup>Japanese Center for Validation of Animal Methods, Tokyo, Japan; <sup>18</sup>Beiersdorf, Hamburg, Germany; <sup>19</sup>German Federal Institute for Risk Assessment, Department of Chemicals and Product Safety, Berlin, Germany; <sup>20</sup>Scientific Research Centre Bioclinicum, Moscow, Russia; <sup>21</sup>Bayer, Investigational Toxicology, Berlin, Germany; <sup>22</sup>National Center for Advancing Translational Sciences, National Institutes of Health, Bethesda, MD, USA; <sup>23</sup>National Center of Medical Radiological Research, Moscow, Russia; <sup>24</sup>Russian Ministry of Production and Trade, Moscow, Russia; <sup>25</sup>The Institute for Human Organ and Disease Model Technologies, Leiden, The Netherlands; <sup>26</sup>MIMETAS BV, Leiden, The Netherlands; <sup>27</sup>Chinese National Center for Safety Evaluation of Drugs, Beijing, China; <sup>28</sup>cellasys GmbH, Kronburg, Germany; <sup>29</sup>F. Hoffmann-La Roche Ltd, Roche Innovation Centre Basel, Switzerland

### Summary

The recent advent of microphysiological systems – microfluidic biomimetic devices that aspire to emulate the biology of human tissues, organs and circulation *in vitro* – promises to enable a global paradigm shift in drug development. An extraordinary US government initiative and various dedicated research programs in Europe and Asia recently have led to the first cutting-edge achievements of human single-organ and multi-organ engineering based on microphysiological systems. The expectation is that test systems established on this basis will model various disease stages and predict toxicity, immunogenicity, ADME profiles and treatment efficacy prior to clinical testing. Consequently, this technology could significantly affect the way drug substances are developed in the future. Furthermore, microphysiological system-based assays may revolutionize our current global programs of prioritization of hazard characterization for any new substances to be used, for example, in agriculture, food, ecosystems or cosmetics, thus replacing the use of laboratory animal models. Here, thirty-six experts from academia, industry and regulatory bodies present the results of an intensive workshop (held in June 2015, Berlin, Germany). They review the *status quo* of microphysiological systems available today against industry needs, and assess the broad variety of approaches with fit-for-purpose potential in the drug development cycle. Feasible technical solutions to reach the next levels of human biology *in vitro* are proposed. Furthermore, key organ-on-a-chip case studies as well as various national and international programs are highlighted. Finally, a roadmap into the future towards more predictive and regulatory-accepted substance testing on a global scale is outlined.

Keywords: microphysiological systems, organ-on-a-chip, *in vitro* models, predictive toxicology, drug testing

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## 1 The prediction dilemma of substance testing using laboratory animals

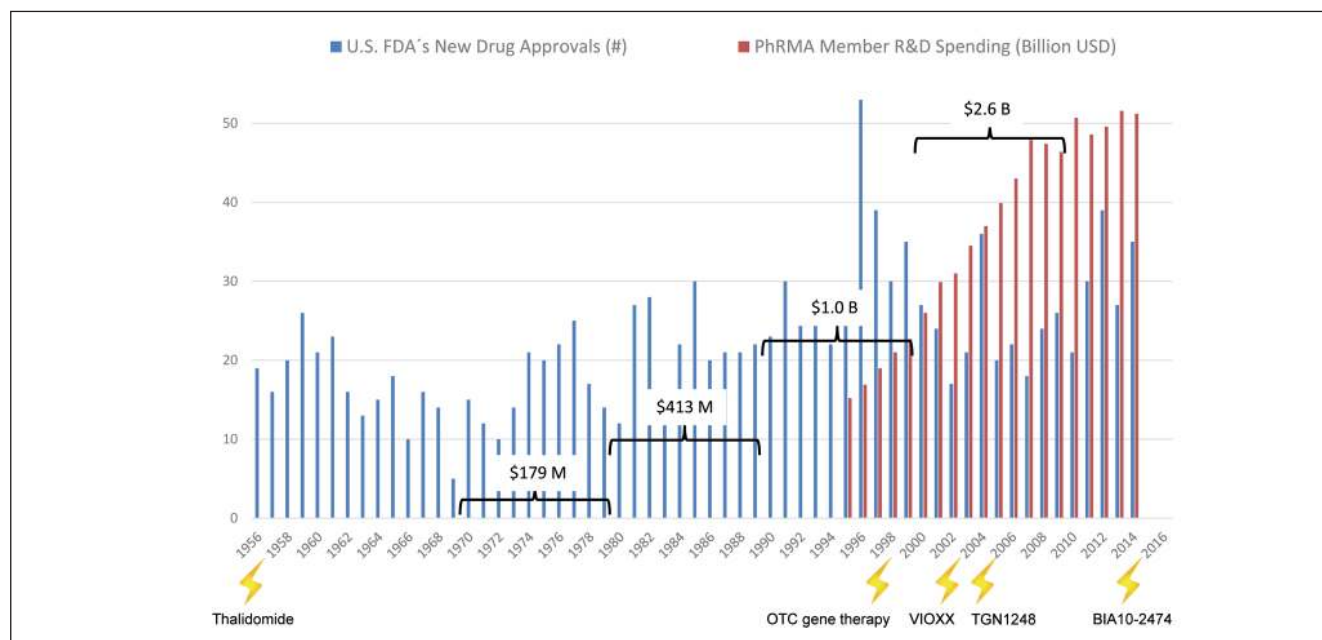
According to the most recent report from the European Commission (EC) to the Council and the European Parliament (EC, 2013), 11.5 million animals were used for experimental and other scientific purposes in the Member States of the European Union (EU) in 2011. The report stated that the number of animals used for research and development for human medicine, dentistry and veterinary medicine dropped since the last report in 2008 from 22.8 to 18.8%. The number of animals used for toxicological and other safety evaluation, amounting to 8.75% of the total, remained relatively unchanged. However, the percentage of animals used for fundamental biological research increased sharply from 38 to 46%. These three areas use by far the highest number of animals (8.7 million in 2011) for scientific purposes in the EU (Daneshian et al., 2015). Information and results generated from fundamental biological studies using animals lay the groundwork for new medicine development in the pharmaceutical and biotech industries. The EC report highlights this fact by saying that ocular research, bone metabolism, fertility studies, potency testing, immunogenicity testing, studies in the areas of neuroscience and immunology, studies on pathophysiological mechanisms of tumors and research to elucidate mechanisms of action of diseases for therapeutic purposes were the major causes for the increase in fundamental biological research.

However, the last few decades of research and development have shown clearly that data from animal studies are often poorly indicative of the human situation (Hackam and Redelmeier, 2006;

Leist and Hartung, 2013; Matthews, 2008; Olson et al., 2000; Perel et al., 2007; Hartung and Leist, 2008; Schnerch et al., 2010; Sena et al., 2010; Seok et al., 2013; van der Worp et al., 2010; Hartung, 2013). The latter is illustrated by repeated failures of drugs in clinical trials. Industry benchmarks for candidate success rates in each phase of clinical trials are 48-64% for phase I, 29-32% for phase II and 60-67% for phase III, respectively (Cook et al., 2014; Hay et al., 2014). Hence, the report presented here focuses on the drug development aspects of the substance testing dilemma.

Development of new medicines currently suffers from two major obstacles (Rovida et al., 2015a): The current approach in preclinical therapeutic drug discovery cannot safeguard against high candidate attrition before and even during clinical trials, and constantly increasing regulatory requirements regarding preclinical testing to avoid harm to human individuals reduces R&D productivity. In the last seven decades pharmaceutical drug development costs increased significantly (spending of U.S. PhRMA members) while new drug approval rates by the US Food and Drug Administration (FDA) fluctuated in response to prime drug development disasters (Fig. 1). R&D productivity has declined more than fifteen-fold, as indicated by the respective increase in inflation-adjusted average spending from \$179 million per successful drug (including the costs of failures) in the 1970s to \$2.6 billion in the twenty-first century (Scannell et al., 2012; Tufts CSDD, 2014) (Fig. 1).

The thalidomide disaster in the late 1950s and early 1960s was the first notorious drug failure resulting in extreme handicaps in over 10,000 people. This event triggered the introduction of pre-clinical teratogenicity testing. Each subsequent disaster



**Fig. 1: Changes in drug development over the last seventy years**

Number of drugs approved by the US FDA (FDA, 2013; FDA, 2014a) are plotted against the pharmaceutical research and development spending of the members of the Pharmaceutical Research and Manufacturers of America (PhRMA, 2015). Drug or substance failures with detrimental outcome for humans (lightening) (see Tab. 1) and average costs to develop one new drug including costs of failures within the corresponding decade (brackets) are given.



prompted an increase in relevant regulations for substance hazard identification, safety testing and efficacy evaluation. Some of these events, including the most recent fatty acid amide hydroxylase inhibitor failure from Bial-Portela & Ca. SA in 2016, are summarized in Table 1.

These historical drug failures with severe outcomes led to the establishment of a drug development approach spanning several years of experimentation and involving animals, *in vitro* tests and healthy volunteers or patients (Fig. 2). A pool of more than 10,000 entities needs to be fed into the drug development pipeline to finally arrive at one successful product (Kessel and Frank, 2007). A stringent regime of traditionally defined steps guides the process. The main goal of this extensive testing approach is to ensure patient safety. It has been the best approach possible to date. However, it is often inefficient and would today cause blockbuster drugs, such as aspirin or paracetamol, to fail regulatory approval (Hartung, 2009).

The smaller part of the investment during the cycle is spent on discovery and lead optimization (Paul et al., 2010), performing larger numbers of *in vitro* assays per lead identification and a significant number of laboratory animal tests per target or lead. Despite all these efforts, the phylogenetic distance between laboratory animals and humans and the discrepancy between cur-

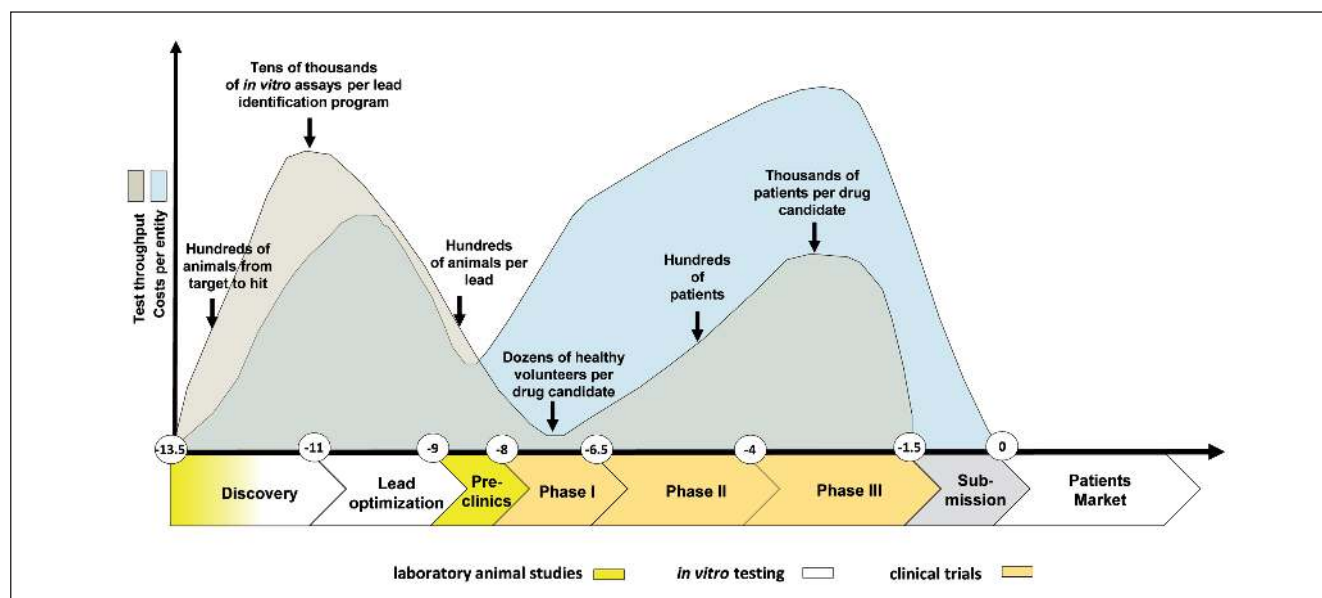
rent human *in vitro* tests and the human body have not improved attrition rates in clinical trials to a satisfactory level. Although animals represent systemic organisms, they are not human, and the *in vitro* tests on human cells are neither physiological nor systemic. Despite intense preclinical safety testing in a number of phase I trials, safety issues may arise which can lead to the termination of a program (Cook et al., 2014; Schuster et al., 2005). Failure to predict efficacy and toxicity in the preclinical phases leads to serious delays in the development of new drugs, exposure of subjects to inefficient substances and even unwanted side effects, as well as initiating unsuccessful, expensive clinical programs, which are the largest investment points in the drug development process (Ledford, 2011).

Next to the pharma industry, other industries, such as chemical and consumer product industries face similar problems regarding toxicological hazard and risk assessment of substances as they also rely on animal experiments. This situation has led to ethical concerns about the use of large numbers of laboratory animals.

New approaches are needed to bridge the translational gap and improve productivity of the drug development process. We believe that biology-inspired microphysiological *in vitro* systems (MPS) will be a cornerstone of this bridge.

**Tab. 1: Prime examples of adverse outcome effects of drugs in humans**

Date / Substance	Adverse Outcome Pathway / Mode of Action	Reference
1957-1961 / Thalidomide	It was administered as a sleeping pill and an antidote to morning sickness suitable for pregnant women. Thalidomide or its metabolic breakdown products inhibit transcription of genes which interferes with normal angiogenesis resulting in truncation of the limb.	Fabro et al., 1965; Woollam, 1965; Bauer et al., 1998; Stephens and Fillmore, 2000
1999 / experimental gene therapy	Ornithine transcarbamylase (OTC) deficiency is a genetic disease that prevents the body from breaking down ammonia, which is a metabolic waste product. The 18-year-old Jesse Gelsinger volunteered for a gene therapy experiment designed to test possible treatments for OTC. He died four days after the injection of the adenovirus, the vector being used to deliver the OTC gene.	Somia and Verma, 2000; Edwards, 2004
2004 / VIOXX	Specific genetic predisposition is one of the key reasons for the now common and highly publicized drug withdrawals. This human genetic diversity is rarely addressed in preclinical and clinical safety studies. A sound hypothesis on the correlation of the morbidity with polymorphic genotypes for 5-LOX and 5-LOX activating proteins is one of many examples.	Dieppe et al., 2004; Arbor, 2004
2006 / TGN1412	Super-agonist antibody TGN1412 was developed to direct the immune system to fight cancer cells or reduce arthritis pain. It triggered multiple organ failure in six healthy volunteers who participated in phase I clinical testing. The antibody, by binding to the CD28-receptor, overrides the basic control mechanisms of the whole immune system.	Clair, 2008; Stebbings et al., 2012
2016 / BIA 10-2474	Clinical testing on an experimental fatty acid amide hydrolase inhibitor from Bial-Portela & Ca. SA, led to six patients being hospitalized on January 10, 2016 in France. Testing was stopped on January 11. One volunteer died. The drug, aiming to treat mood and motor disorders, had previously been tested in mice, rats, dogs and monkeys with no adverse effects. Species differences in inhibitor activity have been discussed to be particularly problematic in drug discovery because <i>in vivo</i> efficacy models are largely based on rodent studies but the candidate inhibitor is ultimately developed as a human drug.	Jouan, 2016; Mileni et al., 2008



**Fig. 2: Drug development cycle: test throughput and cost profile**

The vertical axis illustrates approximate numbers of tests performed (grey) and related spending (blue). The horizontal axis illustrates the development time in years (Paul et al., 2010). Animal tests are used in early discovery for mechanistic mode of action research and for toxicity and ADME profiling in the preclinical phase, while conventional *in vitro* assays are largely used in discovery for target validation, target-to-lead translation and lead optimization steps.

## 2 Microphysiological systems – an expanding toolbox for hazard, safety, disease and efficacy prediction of particulate matter, chemicals and drug candidates

### 2.1 Definition and terminology

Microphysiological systems are microfluidic devices capable of emulating human (or any other animal species') biology *in vitro* at the smallest biologically acceptable scale, defined by purpose. The application of fluid flow (dynamic) for physiological nutrition of the tissues and for the creation of microenvironmental biomolecular gradients and relevant mechanical cues (e.g., shear stress) is a major aspect of these systems, differentiating them from conventional (static) cell and tissue cultures.

The “system” component of MPS refers to devices which support human-like physiology of tissues and organ equivalents within the devices *in vitro*. This may include the maintenance of physical factors, such as temperature (e.g., 37°C), relevant pH, and supply and control of oxygen and humidity levels. Furthermore, it comprises mechanical coupling of organs by mimicking, for example, the flow of blood, urine, air, bile, pancreatic juice or cerebral fluid; shear stress regarding blood and lymphatic vessels; physical pressure on bone and cartilage; strain on skin, lung and stomach wall; intestinal peristaltic movement and muscle contraction. For more details on how microfluidic tools can be used to study mechanobiology we refer to a comprehensive review (Polacheck et al., 2013). In addition, the term “system” may incorporate readout of electrical activity of neuronal and cardiac tissues. The implementation of miniaturized relevant actuators and sensors into the devices enables neces-

sary features for *in vivo*-like tissue-specific electro-mechano-biochemical signaling. They support expansion and compression forces especially relevant for lung, bone and cartilage, and microelectrodes for the electrical stimulation and readout of muscle tissue (Ahadian et al., 2012; Dvir et al., 2012) or stimulation of cardiac cells or neurons (Bussek et al., 2009; Gramowski et al., 2011; Himmel et al., 2012; Johnstone et al., 2010, Khoshfetrat-Pakazad 2014). Moreover, such devices could be able to apply other technical means of measurement and control, such as noninvasive optical imaging. Finally, the “system” in an MPS implies a high degree of automation, which makes it robust and scalable. It is necessary to consider all of these in order to enable reproducible high throughput repeated substance exposure protocols mimicking human drug exposure as closely as possible. Further detailed information on these features is given elsewhere (Andersson and van den Berg, 2004; Huh et al., 2011; Ingber and Whitesides, 2012; Kim et al., 2007; Park and Shuler, 2003; Wu et al., 2010).

The “physiological” component of MPS stands for the ambition to truly emulate human biology. In the current literature, the “true emulation” of human biology *in vitro* is described in different ways, depending on the background and prior experience of the author(s). Adherence as far as possible to the emulation of human organ architecture, including proper cell-to-cell, cell-to-matrix, biochemical and mechanical signaling, is one of the cornerstones of our definition of “physiological.” Glass- and silicone-based devices complemented with polymers, textiles, ceramic or biological matrix entities are individually designed to match the well reviewed requirements regarding shape, surface pattern, stiffness, and microarchitecture of each specific



organ microenvironment (Griffith and Swartz, 2006; Nelson and Gleghorn, 2011; Pexton et al., 2011). Another cornerstone encompasses the maintenance of healthy, long-term organ homeostasis. The third cornerstone covers the ability to repair and regenerate organs that have been damaged or diseased. Thus, the latter cornerstone logically introduces one pathophysiological dimension of MPS. The final crucial cornerstone is to mimic human diseased tissue in the chip, this further introduces the pathophysiological dimension.

The “micro” component of MPS stands for miniaturization to the smallest biologically acceptable scale for each application. This miniaturization is driven by four major factors: mimicking organ function at laminar fluid flow in the cultured tissue, test throughput in the different phases of the drug development cycle (fit-for-purpose), minimum use of human cells and tissues, and, along with this, cost consideration. Scaling MPS-based organ equivalents down to an organoid level, as defined below, is one of the possible scaling strategies in the field. Almost all human organs consist of multiple, identical, functionally self-reliant, structural units, realizing the most relevant functions of the respective organ. Multiplication of these structures within a given organ is nature’s risk management tool to prevent a total loss of functionality during partial organ damage or disease for the majority of body organs. During evolution, this concept has allowed the easy adjustment of organ size and shape to the needs of a given species – for example, liver size in mice and men – still using nearly the same master plan to build up single functional organoids. The term “organoid” was used as early as 1876 in different ways in life science (Bristowe, 1876, p. 73) and means “the smallest functional organ or tissue unit.” A selection of organoid histologies, all with a relevant functionality and highly variable conglomerate geometry, has been published for 15 key human organs (Marx et al. 2012). Ideally, the reactivity of organoids to drugs is representative of the reactivity of the organ. Therefore, a single organoid should reflect the smallest possible scale that can be used in MPS in order to emulate organ functionality. Selected functions may be emulated on a smaller scale, however, the investigation of disease emergence and progression, as well as tissue repair and regeneration processes requires more identical organoids to represent the organ response in an MPS. With regard to the scaling aspect of MPS, a computational methodology for design and operations for pharmacology applications was developed by Yu et al. (2015). Stokes et al. (2015) discuss on-platform scaling based on physiology and pharmacology and *in vitro-in vivo* translation of results for complex MPS technologies. These different aspects reflect the current diversity of MPS within the scientific community.

MPS devices exist in two categories: plates and chips, as illustrated in Figure 3. Plates are usually based on the microtiter plate dimensions as defined by ANSI/SLAS (SLAS, 2014) and use passive, gravity-based microfluidic flow or active on-board pumping (Ebrahimkhani et al., 2014). An advantage of plate-based systems, whether gravity-based or active flow-based, is that they can be used with standard liquid handling equipment, such as robotic pipettors, and are fully compatible with automated microscopes and plate readers.

Chips of microscope slide size and other formats are operated by an active microfluidic flow (external or on-chip pumps are used). This supports the emulation of shear stress at physiological intra-capillary or interstitial rates mandatory to maintain stable protein and oxygen gradient-based microenvironments over long time periods. Typically, the single chip format is used when more complex tissue architectures need to be mimicked, while plate-based formats are preferred when a minimal amount of data points per system are needed.

Alternatively, microphysiological systems can be broken down into three distinct types: Single-organ systems, multi-organ systems and more complex systems that are often termed human “body-on-a-chip” systems (see Fig. 3).

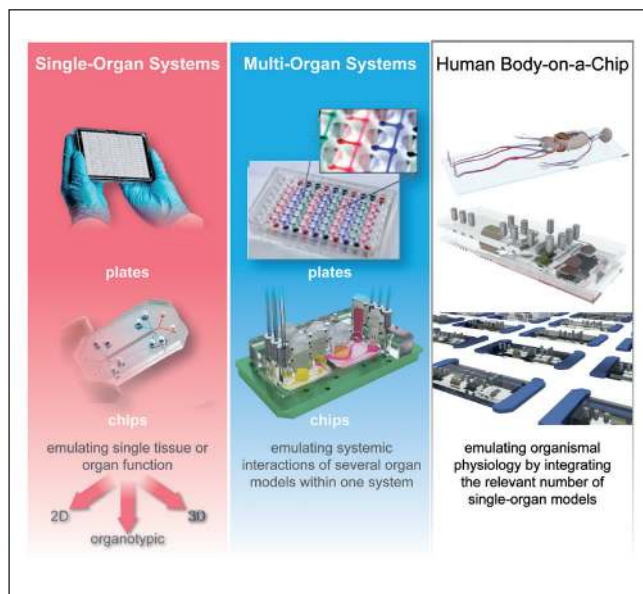
Single-organ systems are plates or chips emulating single tissue or organ function and are designed to improve early predictivity of human single-organ toxicity of a particulate matter, a chemical or a drug candidate. These tissues or organs can be modeled at a two-dimensional (2D), three dimensional (3D) or organotypic complexity: 2D stands for suspension or monolayer cell cultures; 3D involves multilayer cultures of different geometry, e.g., spheroids, strata and irregular tissue formations; and organotypic differs from 3D by capturing as many desirable features of the *in vivo* architecture as necessary to gain the appropriate organ function (Hartung, 2014). Single-organ formats range from those employing passive gravity-based flow in plates adapted from standard cell culture plates to a variety of plate-based and microfluidic chip-type approaches using active flow from on-board or external pumps. These approaches allow the generation of various flow profiles, different fluid-to-tissue ratios and other physiologically relevant characteristics. Multi-organ systems emulate systemic interactions of two or more organ models within one system to enable adverse outcome pathway (AOP) and mode of action (MoA) data generation from their crosstalk. In contrast, human-on-a-chip (or body-on-a-chip) systems are envisioned to mimic the physiological interaction of a number of organs capable of emulating entire organismal functionality. A minimum of ten organs has been set as a goal by the Defense Advanced Research Projects Agency (DARPA)/National Institutes of Health (NIH) MPS program (Hartung and Zurlo, 2012), for example, as a means to identify the field of technical challenges for such organ combinations. This number has yet to be defined by the scientific community and regulatory bodies.

The current literature on MPS describes different culture times: short-term cultures last hours or days, supporting single exposure acute substance testing, and long-term cultures last weeks and months, enabling disease modeling and repeated dose substance exposure.

## 2.2 Human cell supply for MPS

Human beings are the source for human cells and tissues used today in *in vitro* research and industrial applications (Fig. 4).

Historically, human cell lines derived from adult donors (blue arrow, Fig. 4) have been the source of first choice for industrial *in vitro* assays due to their unlimited expansion potential, relative stability and the amenability to long-term cryostorage. The first human cell line – HeLa – was derived from the cervical adeno-



**Fig. 3: Types of MPS used for emulation of human biology *in vitro***

The MIMETAS OrganoPlate for 3D perfused cell culture in microtiter format (top left), the lung-on-a-chip developed by the Wyss Institute (middle left), the hanging drop microtiter plate with microfluidic channel connecting multiple spheroids developed by ETH Basel (top center), an artist's impression of the four organ system developed by TissUse (center bottom), and artist's impressions of a human body-on-a-chip platform (right) (courtesy of MIMETAS, The Netherlands; Wyss Institute, USA; ETH, Switzerland; and TissUse GmbH, Germany, respectively).

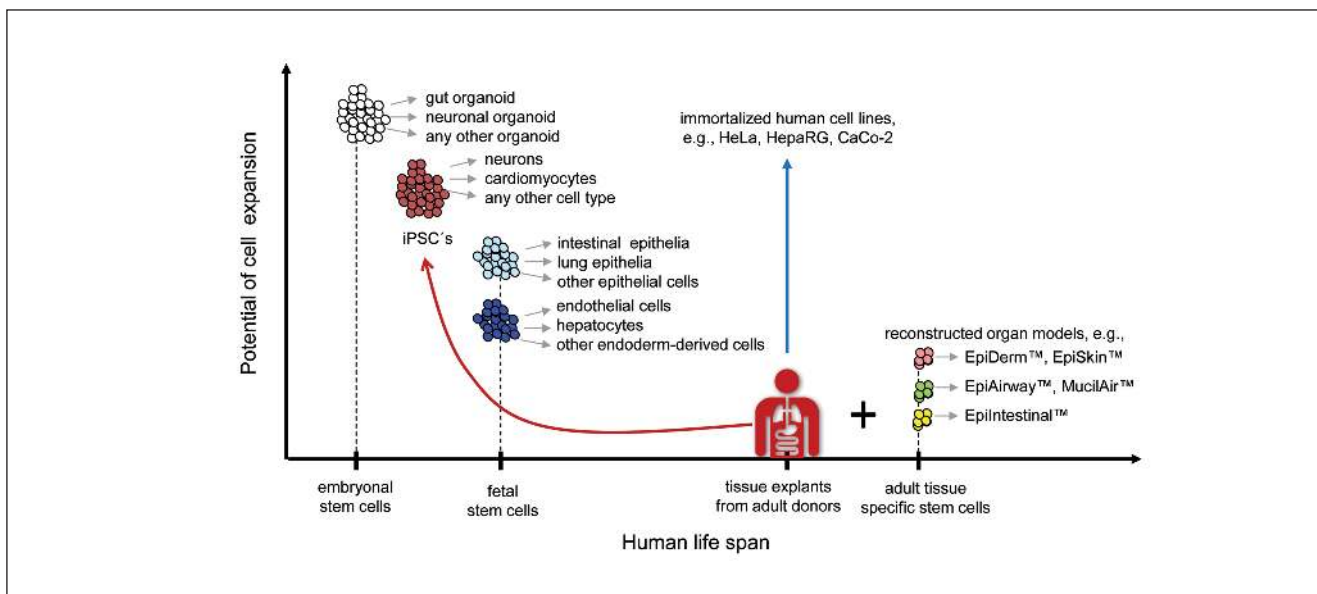
carcinoma of Henrietta Lacks as early as 1951. Today, thousands of human cell lines more or less representative of different organ/tissue cell types are available, for example, patient-derived human cell lines like HepaRG, used in a number of toxicity assays, and the CaCo-2 cell line used for intestinal permeation assays. With increasing knowledge on the genetic engineering of mammalian cells, an ever growing panel of designed human cell lines has been integrated into industrial and research applications (Sandig and Jordan, 2007). Well established human cell lines are a common cell source for MPS-based cell culture. The drawbacks of cell lines are the partial loss of or gain of functionality due to their cancer background in addition to an inability to form complex heterogenic tissue architecture. Primary tissue explants and biopsies from healthy donors are the most complex and *in vivo*-like human tissue sources. These sources are used primarily in basic research and tissue engineering. Regarding use in MPS, the respective microsystem needs to be adapted for direct integration of such human explants and biopsies into the fluid flow. The drawback of tissue explants is their limited availability.

Another common approach to generate human tissue architecture *in vitro* is the *de novo* assembly or reconstruction of human organoids. All primary tissues and/or their necessary adult tissue-specific stem cells are harvested from a donor or patient (Fig. 4) (Clevers and Bender, 2015; Rookmaaker et al., 2015; Sato and

Clevers, 2015). Then single cells are isolated from the tissues, expanded and reassembled *in vitro*. Prime targets for such reconstruction are the human barrier organs of skin, lung and intestine: EpiDerm™ from MatTek, EpiSkin™ from EpiSkin, EpiAirway™ and MucilAir™ from Epithelix and EpiIntestinal™ from MatTek are prime reconstruction examples, see Gordon et al. (2015) for a comprehensive overview of non-animal models of epithelial skin, lung and intestinal barriers. In order to integrate such models into MPS devices, the latter need to be adapted to the standard architecture of the respective reconstructed model. Optimized manufacturing procedures and a pool of standardized donors at the vendor site support a certain robustness of such reconstructed human tissue models. The drawbacks are limited architectural complexity, short-term stability and costs.

There are three further human cell sources for organoid engineering in MPS. All three are stem cell-based – embryonic, fetal and induced pluripotent – but only the induced pluripotent stem cell (iPSC) approach works with primary cells from an adult donor (red arrow, Fig. 4). Since the inception of the induced pluripotent stem cell technology by Takahashi and Yamanaka (2006), induction of pluripotency in primary human cells from patients or healthy donors has become an experimental routine. An impressive panel of companies, such as AxioGenesis, Axol, BioTalentum, Cellular Dynamics International, Plurionics, Lonza, Takara Bio Europe AB, Viagene Biotech, iXCells Biotechnologies, Applied StemCell, Applied Biological Materials, Centre for Commercialization of Regenerative Medicine and Cedars-Sinai provide reprogramming and/or differentiation services. While reprogramming has become a professional industrial standard, leading to more than 1,500 cryopreserved and well characterized iPSC lines, differentiation into organ-specific human cells still remains a big challenge, see Bellin et al. (2012) for a comprehensive review. Within the last three years there has been an unprecedented increase of experimental research into differentiation protocols, starting from induced pluripotency. Here we list a number of papers trying to differentiate cell types relevant for MPS-based organoid engineering and subsequent assay development: hepatocytes (Szkolnicka et al., 2014), cardiomyocytes (Burrige et al., 2014), small intestine (Kauffman et al., 2013), neurons (Hoelting et al., 2013; Lippmann et al., 2014; Lancaster and Knoblich, 2014; Terrasso et al., 2015; Simão et al., 2016), lung (Ghaedi et al., 2013), gallbladder (Kauffman et al., 2013), pancreas (Pagliuca et al., 2014), kidney (Song et al., 2012), skin (Itoh et al., 2013), biliary ducts (Ogawa et al., 2015), bone-marrow (Hynes et al., 2014), ovaries (Leng et al., 2015) and vasculature (Patsch et al., 2015). To the best of our knowledge, none of the protocols or procedures have yet been adopted by pharmaceutical industry for robust reproducible assay establishment, but there are first data indicating that MPS might be the right approach to drive the differentiation of pre-differentiated iPSC cells toward a final stage by supplying the physiological environment of the respective organoid (Moreno et al., 2015).

Fetal cells are rarely used in the engineering of human adult tissue, but recently, mesenchymal stem cells derived from fetal tissues could be differentiated into neuronal (Zhang et al., 2011) and osteoblastic lineages (Zhang et al., 2010). The main advantage with fetal cells is that they retain



**Fig. 4: Human cell sources for *in vitro* formation of organoids**

The expansion potential of different human cell and tissue sources used in MPS are plotted against their appearance in the human life-span. (Grey arrows) – indicate Differentiation potential of the respective stem cell pool (grey arrows); induction of pluripotency using primary cells (red arrow); unlimited expansion potential of immortalized cell lines (blue arrow).

their proliferative capacity while being committed to an endpoint, and are not teratogenic in nature. However, their source is controversial.

Embryonic stem cells (ESC) are derived early after fertilization from the inner cell mass of human blastocysts. A variety of human embryonic stem cell lines has been created over the last few decades (Mummery, 2011). These pluripotent progenitor cells lack the epigenetic modifications that may sometimes be seen in iPSC. Therefore, ESC might provide the broadest background for differentiation into any human organoid. The disadvantages of human embryonic cells or cell lines are the ethical debate surrounding their use and their propensity to give rise to teratomas, as shown in transplantation experiments (Lees et al., 2007; Leist et al., 2008)

Pluripotent stem cells of the origin described above have been used for the *de novo* assembly of human gastric (McCracken et al., 2011), cerebral (Lancaster et al., 2013), kidney (Xia et al., 2014) and lung organoids (Dye et al., 2015) in static culture systems. Physiological, mechanical and electrical coupling of such human organoids using MPS seems to be an attractive approach for their further differentiation into *in vivo*-like functional organ units. See Huch and Koo (2015) and Li et al. (2014a) for a review on organoid cultures based on pluripotent human stem cells.

## 2.3 Current state of the art of MPS

### 2.3.1 Introduction

Technical drawbacks of any static cell culture-based assay include the limitation of oxygen and nutrient supply to a given 3D tissue size or monolayer, and the lack of dynamic protein gradients. Oxygen restriction in cultures of primary human

hepatocytes in static culture flasks, for example, was described as early as 1968 (McLimans et al., 1968). Microfabrication and microfluidics technologies, initiated as a scientific discipline in its own right as early as 1990 (Manz et al., 1990) delivered commercially available lab-on-a-chip platforms at the end of the 20<sup>th</sup> century (see El-Ali et al., 2006 and Whitesides, 2006 for reviews), and advances in bioengineering related to materials science enabled the appearance of first plate- and chip-based microfluidic tissue culture systems aiming to solve the two aforementioned limitations of static cultures and to replicate the spatiotemporal, mechanical and biochemical cues that drive the physiological behavior inherent in those tissues. MPS developers approached their goal from two different angles, some of them aiming to integrate microfluidic principles of nutrient supply into well-established industrial high throughput compliant static cell culture microtiter well formats and some trying to miniaturize well established industrial tissue culture bioreactor systems.

Plate-based MPS developments accommodated conventional static cell culture microtiter plates with arrays of 96, 384, 1536 and 3,456 wells, which have become the standard of choice in any biological laboratory (SLAS, 2014). These platforms appeared on the grounds that the sheer nature of experiments and inherent variability in biology requires a vast amount of control experiments, repetitions and dilutions. In addition, the trend in molecular and cell biological sciences has progressed to ever higher throughput approaches, testing more conditions in one experimental session. It is for these reasons that manual and automated liquid handling and readout equipment has been designed in accordance with this standard. Moreover, the high number of wells in a plate offers the additional advantage of



**Fig. 5: Single-organ microcassette bioreactor device with hollow-fiber-based perfusion**

(A) Integration of electromechanically controlled peristaltic pumps; (B) controller for ten microcassettes; (C) micro-bioreactor in operation in an incubator for temperature, humidity and CO<sub>2</sub> control (courtesy of ProBioGen AG, Germany).

reduced volumes of cells and reagents, leading to a reduction of cost per assay.

Chip-based microphysiological systems for tissue and organ modeling have usually been designed by downscaling the fluidic and tissue culture compartments and miniaturizing the sensors and actuators of conventional industrial cell-culture bioreactors. Automated dynamic bioreactors, such as hollow-fiber bioreactors, invented in the early-1970s, solved the problem of large scale oxygen and nutrient supply— up to one liter tissue culture — by the introduction of artificial capillaries for medium perfusion (Knazek, 1972). These dynamic perfusion tissue culture systems later were advanced into functional long-term *in vitro* organ equivalents introduced into medical practice as extracorporeal bioartificial liver devices in the late-1990s (Catapano and Gerlach, 2007; Gerlach, 1996; Wang et al., 2010). Following from this, numerous dynamic tissue-specific bioreactor devices, such as human artificial lymph nodes for immunogenicity testing, were miniaturized for *in vitro* testing purposes towards the lower ml per tissue culture scale (Giese et al., 2006). Figure 5 illustrates a miniaturized incubator-dependent dynamic bioreactor prototype for the simultaneous culture of human immune tissues at 0.5 ml each in operation.

Unfortunately, it became obvious in the first decade of this century that the lower ml scale still required too many cells and was still far too large to enable simultaneous high content testing at reasonable costs. This triggered the advent of chip-based MPS, which adopted lab-on-a-chip platforms to decrease tissue culture volumes down from micro- to nanoliter scale per tissue culture compartment. These aim to apply automated pumping systems and electrical, optical and mechanical transduction to monitor and control complex minute tissue cultures in automat-

ed incubator-independent systems at relevant throughput.

In summary, plate- and chip-based MPS aim to reflect physiologically relevant parameters, including proper cell-to-cell, cell-to-matrix, and biochemical and mechanical signaling. These capabilities present unprecedented opportunities to create MPS with the potential of capturing the dynamics of disease appearance, of repair and regeneration processes and of drug effects in the human body. Recent advances in MPS development have made it possible to initiate the engineering of cellular environments and/or functional units of lung, heart, blood vessels, muscles, bones, liver, reproductive system, nervous system (including eye), gut, skin, intestine and kidney.

In this chapter, we report the status of the development of biology-inspired microphysiological single- and multi-organ systems and their use for substance testing. Furthermore, we introduce achievements in modeling diseases using MPS. Recent initiatives to advance multi-organ systems into human body-on-a-chip solutions are outlined in Chapter 4.

### 2.3.2 State of the art of microphysiological single-organ systems

Early microtiter plate-based microfluidic cell culture formats with passive gravity-based microfluidic flow approaches to *in vitro* tissue regeneration with application in human disease modeling and drug development were developed by CellAsic (Lee et al., 2007a). Inspired by the work of Luke Lee's group (Lee et al., 2007b; Hung et al., 2005b), they developed a microtiter plate with eight independent flow units that did not require tubing for perfusion flow, but relied on passive leveling instead. The device consists of a polydimethylsiloxane (PDMS) molded microfluidic layer that is bonded to a glass bottom and an acrylic user interface. Cells were introduced with the help of a vacuum manifold and positioned by a filter consisting of densely packed micropillars. Perfusion flow was induced by gravity leveling in conjunction with a carefully tuned fluid resistance of the microfluidic channels. HP Medizintechnik GmbH's (Oberschleißheim, Germany) intelligent microplate reader is an advanced 24-well-based microphysiological system incorporating an automated microscope, pipetting robot and microsensors for pH, dissolved oxygen and impedance, and is premounted in an incubator (Demmel et al., 2015). It was successfully used to monitor the viability of various cell types and primary tissue (Kleinhaus et al., 2012) and to develop new toxicological endpoints (Wolf et al., 2011). The relatively high grade of parallelization and the automation of the pipetting robot and the microscope allow autonomous, label-free long-term experiments in the field of MPS. The PDMS material used, however, displays high unspecific binding of drug candidates.

Dave Beebe's group at the University of Wisconsin, Madison, WI, US, developed a series of microtiter plate-based cell culture devices, including a 3D culture plate and a chemotaxis plate (Berthier et al., 2010). A total of 192 single channels on a microtiter plate were filled with cell-loaded gels (Meyvantsson et al., 2008). An interstitial flow through the gel was applied, making use of differential meniscus pressure between two droplets of different size at the in- and outlet, respectively. A similar pumping concept was used for a 49-channel network chemotaxis de-



vice consisting of a source and a sink channel that are connected to a very thin gradient channel.

The OrganoPlate was recently introduced by the company MIMETAS, Leiden, The Netherlands, consisting of 40 to 96 individually addressable microfluidic networks (Jang et al., 2015; Moreno et al., 2015; Trietsch et al., 2013). The OrganoPlate makes use of PhaseGuide technology to stratify extracellular matrix (ECM) gels in orderly layers, one next to the other. This enables a co-culture approach that is fully free of artificial membranes, while still enabling the engineering of tissues. The OrganoPlate is fully devoid of high absorbance materials, such as PDMS, does not require any other handling equipment apart from standard pipettes for operation, and provides continuous perfusion flow through passive leveling.

Plate-based microfluidic cell culture formats with active on-board pumping were introduced for liver models by the group of Linda Griffith at MIT, Cambridge, MA, US and commercialized by CN Bio Innovations, London, UK. The Liverchip™ system, such a plate-based system, is described in more detail below.

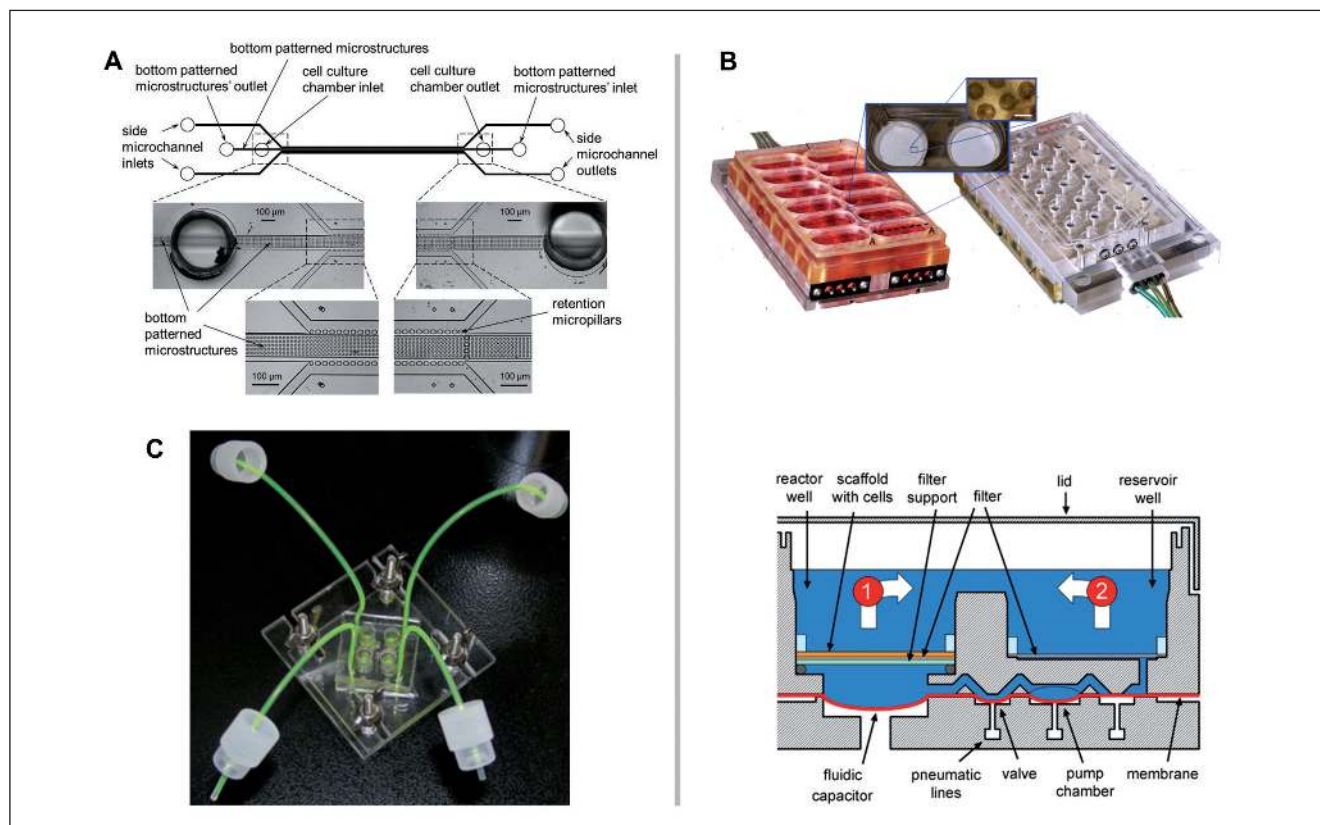
Many single-organ chip concepts covering a wide range of tissues were proposed during the last decade and were actively introduced into biological research. They began with single cell type cultures of different organ specificity, such as endothelial cells (Young and Simmons, 2010), myoblasts (Gu et al., 2004),

hepatocytes (Carraro et al., 2008; Goral et al., 2010; Ho et al., 2006; Leclerc et al., 2004; Lee et al., 2007b; Park et al., 2008; Powers et al., 2002; Toh et al., 2007, 2009), neurons (Rhee et al., 2005), mammary epithelial cells (Grafton et al., 2011), adipose cells (Nakayama et al., 2008), and human embryo cells (Chung et al., 2005; Hung et al., 2005a; Smith et al., 2012; Villa-Diaz et al., 2009).

In a next phase, heterotypic microfluidic single-organ co-culture systems combining crucial cell types of a specific organoid into artificial functional units reflected aspects of the individual organs more realistically.

Scientific activities in the field of organ-on-a-chip models have increased dramatically in the last five years (van de Stolpe et al., 2013). Therefore, we decided to exemplarily highlight the single-organ MPS developments for human liver and lung modeling whilst referring readers to the original MPS literature for other organs and systems.

MPS-based liver cultures have matured from dynamic, random cell culture towards systems of higher tissue complexity. The unique importance of liver for organismal homeostasis (e.g., plasma protein synthesis, glucose biotransformation) and blood detoxification (e.g., urea, xenobiotic drug metabolism) has led to an evolutionary optimization of the human liver architecture at the scale of its smallest functional unit – the liver lobule. A



**Fig. 6: Increasing complexity of MPS-based liver models**

Inspired by the lobulus architecture of human liver lobules, MPS have evolved from bile canaliculi forming cord-like liver cultures (A) through sinusoid-like arrangements supporting functional space Disse structures (B) towards tissue slice cultures maintaining functional organoid liver structures (C).

precise zonal division of labor along a 500  $\mu\text{m}$  long stretch of about 25 hepatocytes arranged in cords allows the management of blood detoxification at a blood contact time of only a few seconds. Not much is known about the fluid dynamics of plasma-hepatocyte contact. The nature of the plasma flow in the space of Disse and the mechanics applied to hepatocytes at the basolateral surfaces are under dispute. The high degree of fenestration may result in transmission of fluid shear stress to hepatocytes. Furthermore, the sinusoids in the periportal zone are of a very small diameter, i.e., the size of an erythrocyte. Blood cell passage through these tight sinusoids may additionally modulate shear stress. Four types of MPS-based liver equivalents have been developed so far: random dynamic hepatocyte monocultures, cord-like liver equivalents, endothelial sinusoid models and hepatic lobule “equivalents” (Materne et al., 2015). Figure 6 highlights prominent examples for the latter three types.

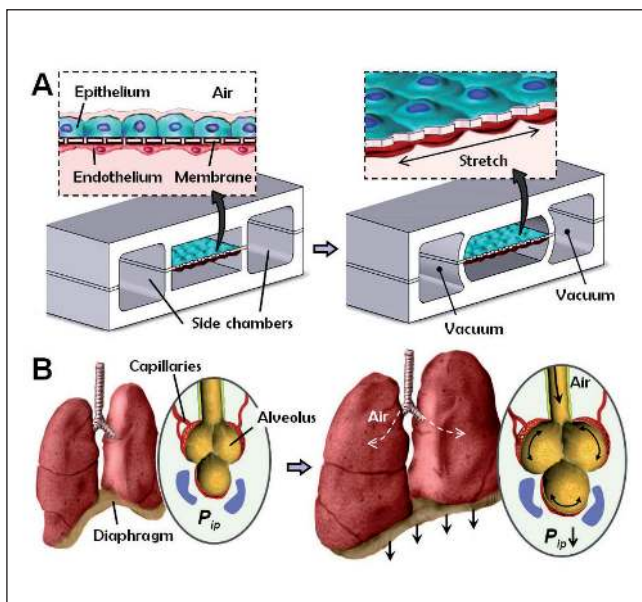
In contrast to random dynamic hepatocyte cultures, the formation of 3D cord-like structures composed of polarized cells that form extended bile canalicular structures was presented by Goral and colleagues (2010). A series of retention pillars formed a microchannel centered between two side-channels (Fig. 6a). However, unlike other perfusion-based microdevices, the bottom of the cell culture chamber was patterned with microstructures, which provided additional control of hepatocyte polarity. After two weeks of perfusion culture, the cells remained viable and had formed a cord-like structure. An extended bile canalicular structure and the formation of gap junctions between the 3D structured cells could be shown. The system thus allowed the arrangement of hepatocytes into an artificial but cord-like assembly, control of hepatocyte polarity and sporadic bile segregation. Co-culture of hepatocytes with non-parenchymal cells in a spatially arranged 3D environment under constant perfusion might lead to the formation of a next level of architectural resemblance to the *in vivo* situation. A very interesting approach to modeling sinusoid-like structures in a microfluidic system was developed by Linda Griffith's group at MIT (Domansky et al., 2010). An array of multiple bioreactors was built into a multiwell plate comprising 12 autonomous microfluidic systems (Fig. 6b), each perfused by an integrated pneumatic micropump circulating a total volume of 3 ml. Each tissue culture scaffold contains 769 multichannels (0.24 mm deep, 0.34 mm diameter) and is seeded with 106 rat hepatocytes and endothelial cells at a 1:1 ratio. A continuous adjustable oxygen gradient can be established over long operating times. The scaffold supports near physiological tissue densities and the functional zonation of hepatocytes can be stipulated. The large channels of the scaffold support self-assembly of the two cell types in dynamic conditions. Liver sinusoid endothelial cells, known to lose their differentiated phenotype *in vitro*, maintained the expression of the functional marker SE-1 throughout the culture. The important features of adjustable flow rates on the basis of an oxygen consumption model, long-term steady gradient maintenance and the amenability to co-culture of hepatocytes with different types of non-parenchymal cells made the system an interesting approach for toxicity testing. It is one of the still rare cases where a research MPS has been transferred into industrial application. The scaffold size of the LiverChip™ system commercialized by

CN Bio Innovations can be scaled for 10,000 - 1,000,000 cells, and plates are similarly scaled in 12- or 36-well formats. Active pumping allows flow rates through the tissue to be uncoupled from the morphology of the tissue. The system provides high-content data for drug metabolism and pharmacokinetics, toxicology and disease biology applications (Sarkar et al., 2015; Vivares et al., 2015). It has been applied in preclinical development (Dash et al., 2009; Vivares et al., 2015). Furthermore, a model of micrometastasis of cancer cells in liver has been developed on the platform and a demonstration of dormancy of the aggressive MDA-MB-231 cell line has been established in the model (Wheeler et al., 2014). A model of hepatitis B virus infection has also been developed using the same 3D perfused liver model. Infection of cryopreserved primary human hepatocytes is achieved through incubation with patient serum. The full viral life cycle is recapitulated, making the model of utility in exploring both the basic biology of hepatitis B virus and evaluating novel treatments (Wai et al., 2014).

The highest level of architecture – the entire liver lobule – has not yet been reached, but a chip-based microfluidic approach to containing a major part of a liver lobule has been made by van Midwoud and colleagues (van Midwoud et al., 2010a), who cultivated 3 mg of liver slice tissue in a microfluidic chip (Fig. 6c). The precision-cut liver slice (100  $\mu\text{m}$  thick, 4 mm diameter) was perfused with a flow of 10  $\mu\text{l}/\text{min}$  in an incubator chamber with constant pH and dissolved oxygen. Biotransformation activity was shown to be equal in control slices in static culture over three days. The system does not demonstrate any advantage with regard to metabolic functionality over the 3 d measurement time. The authors highlight the advantage of continuous media perfusion at low tissue-to-fluid volume ratios in contrast to steady metabolite accumulation in static culture. Unfortunately, data on the culture performance over times longer than 72 hours are not yet presented (van Midwoud et al., 2011a).

In addition to the examples described above, MPS-based single-organ liver modeling has led to a large variety of liver-on-a-chip devices (Baudoin et al., 2014a; Hwa et al., 2007; Kane et al., 2006; Khetani and Bhatia, 2008; Leclerc et al., 2014, 2015; Legendre et al., 2013, 2014; Pasirayi et al., 2014; Snouber et al., 2013). Research tools and assays have been developed to investigate liver metabolism and toxicity in single-organ chips (Baudoin et al., 2014b; Leclerc et al., 2014, 2015; Legendre et al., 2013, 2014; Pasirayi et al., 2014; Snouber et al., 2013a). For further details on the development of liver-on-a-chip models readers are referred to respective reviews (Materne et al., 2013; van Midwoud et al., 2011b).

Another complex organ where MPS-based models are already making a difference regarding the understanding of human organ functionality, testing safety and disease modeling is the human lung. Human *in vitro* models of small lung airways and alveoli were developed historically in static air-liquid interface cultures on cell culture inserts. For a comprehensive overview on such models, readers are referred to Gordon and colleagues (2015). Until recently, only a few MPS trying to emulate functional parts of the lung had been developed (Nalayanda et al., 2007, 2010), but in 2010, a microphysiological lung-on-a-chip system developed by Donald Ingber's group at the Wyss Insti-



**Fig. 7: Biology-inspired microfluidic alveolar models applying mechanical stretch**

Design of a lung-on-a-chip system. (A) Cross-sectional view of the device in the native and stretched state. Human alveolar epithelial cells are cultivated on the top of the membrane and human pulmonary microvascular endothelial cells are cultivated on the bottom of the membrane. (B) View of the lung showing the stretch and resulting distribution of air during inhalation. Applying a cyclic vacuum through the side chambers causes the cell layer to stretch, mimicking natural stretching during inhalation (reprinted from Huh et al., 2010).

tute for Biologically Inspired Engineering at Harvard University Boston, MA, USA, made it for the first time into *Science* (Huh et al., 2010). Figure 7a shows the design and principles of this system, which mimics the function of a lung alveolus. The system is prepared by microfabricating a chamber with two microchannels separated by a thin (10  $\mu\text{m}$ ) porous PDMS membrane coated with an ECM (fibronectin or collagen). Human alveolar epithelial cells are cultivated on top of the membrane (in the upper channel) and human pulmonary microvascular endothelial cells are cultivated on the lower side of the membrane (in the lower channel). Air is pumped through the top channel and a culture fluid is pumped through the lower channel as a blood substitute. Thus, the system mimics the alveolar-capillary barrier. By applying a vacuum to the side channels, it is possible to stretch the culture layer; release of vacuum causes elastic recoil of the membrane, returning it to its natural state, mimicking the stretching of the alveoli during breathing (Fig. 7b). Molecules present in the air cross the culture layer through a combination of passive diffusion and active transport, as in the alveoli in the lung. Huh and colleagues (2012) used their lung-on-a-chip system to develop a model of pulmonary edema. Pulmonary edema is a life-threatening disease associated with increased hydrostatic pressure or microvascular permeability caused by various diseases or dose-limiting drug toxicities (Willett, 2014). Huh

and colleagues (2012) confirmed that administration of high doses of interleukin-2 (IL-2) caused a state consistent with pulmonary edema in their lung-on-a-chip system, similar to the effects of administering IL-2 to human cancer patients. They also found that angiopoietin-1 and GSK2193874, an inhibitor of the transient receptor potential vanilloid 4 ion channel, attenuated edema *in vitro* and may prevent this dose-limiting toxicity of IL-2 in clinical settings. The authors concluded that the system could be used to model diseases in other organs and predict the efficacies and toxicities of other drugs in humans. Emulate Inc. (Boston, USA) is commercializing tools based on this platform. The system has also been used to examine the production of intracellular reactive oxygen species (ROS) in response to nanoparticles (Huh, 2015; Huh et al., 2010). In these studies, silica nanoparticles with a diameter of 12 nm induced and amplified the acute toxic responses measured in terms of ROS generation. Cyclic stretching and relaxation of the porous membrane to mimic breathing further enhanced the absorption and translocation of the silica nanoparticles from the upper air channel to the lower fluid channel. Similar findings were observed in a ventilation-perfusion model using whole mouse lung.

Other research groups have developed lung-on-a-chip systems using human primary pulmonary alveolar epithelial cells from patients who had undergone partial lung resection (Stucki et al., 2015) or primary airway epithelia (Bol et al., 2014; Sellgren et al., 2014) for selection of candidate drugs to treat pulmonary pathologies.

Finally, a model of chemotherapy-induced pulmonary edema has been developed on the basis of a small-airway-on-a-chip model (Benam et al., 2015b). The main biology-inspired aspect of the systems is the application of physiological cyclic strain placed on the cells, which not only closely mimics normal respiratory movements, but also influences the permeability of the cell layers. *In vivo* studies have shown that distention of the lung, as in inhalation, increases the permeability of the lung to hydrophilic molecules (Marks et al., 1985). This is probably due to the stretching of the intercellular junctions, which increases the size of the pores and allows larger hydrophilic molecules to cross the junctions (Mason et al., 2001). Innovative approaches to develop microfluidic systems for the culture of other types of epithelia could potentially also be adapted to establish new lung-on-a-chip systems. For further information on MPS-based lung model development readers are referred to a recent review (Nichols et al., 2014). Although the consensus is that lung-on-a-chip systems are useful tools for toxicological research, very few toxicology studies have been performed using these systems.

Other organs models in single-organ MPS include the small artery (Günter et al., 2010), the nervous system (Booth and Kim, 2012; Brown et al., 2014; Kerman et al., 2015; Nery et al., 2015; Park et al., 2009; Taylor et al., 2005), the pancreas (Silva et al., 2013; Jun et al., 2013; Lee et al., 2012), the kidney (Snouber et al., 2011, 2012; Jang et al., 2013; Ferrell et al., 2012; Kim and Takayama, 2015; Huang et al., 2013; Mu et al., 2013), the bone-marrow (Cui et al., 2007), the skin and hair (Ataç et al., 2013) and the intestine (Esch et al., 2012; Kim and Ingber, 2013; Kim et al., 2012, 2013a; Kimura et al., 2008; Lahar et al., 2011; Mahler et al., 2009a; McAuliffe et al., 2008; Ootani et al., 2010;

Sato et al., 2009; Sung et al., 2011; Yu et al., 2012) at different levels of biological complexity. Gao and colleagues (2013) designed an integrated microfluidic device directly coupled to a mass spectrometer, for instance, to characterize drug permeability of the intestinal barrier in a real-time manner. They were able to measure the permeation of curcumin through a Caco-2 cell monolayer in real-time and obtained results consistent with published *in vivo* data. Another integrated microfluidic platform, called the “NutriChip,” was set up to investigate the potential of the immune-modulatory function of dairy food (Ramadan et al., 2013). Ramadan and colleagues quantified the variation of pro-inflammatory cytokine expression directly online using magnetic beads and an optical detection device in their epithelial/immune cell co-culture model. These techniques offer useful tools for substance permeability studies or physiological response measurement. Finally, the lung-on-a-chip platform of the Wyss Institute at Harvard, Boston, USA, has recently been used for a gut-on-a-chip model of inflammatory bowel disease (Kim et al., 2016). This single-organ chip was used to co-culture multiple commensal microbes in contact with living human intestinal epithelial cells and to analyze how gut microbiome, inflammatory cells and peristalsis-associated mechanical deformations contribute independently to intestinal bacterial overgrowth and inflammation. This *in vitro* model replicated results from past animal and human studies, including a demonstration that probiotic and antibiotic therapies can suppress villus injury induced by pathogenic bacteria. By ceasing peristalsis-like motions while maintaining luminal flow, lack of epithelial deformation was shown to trigger bacterial overgrowth similar to that observed in patients with ileus and inflammatory bowel disease. Thus, this human gut-on-a-chip can be used to analyze contributions of the microbiome to intestinal pathophysiology and dissect disease mechanisms in a controlled manner that is not possible using existing *in vitro* systems or animal models.

For further information on single-organ systems modeling tissues of the respiratory, nervous, digestive and excretory systems, we refer readers to a recent systematic review by Prestrelo and co-authors (2015), whilst the use of single-organ MPS to model diseases has been reviewed elsewhere (Benam et al., 2015a).

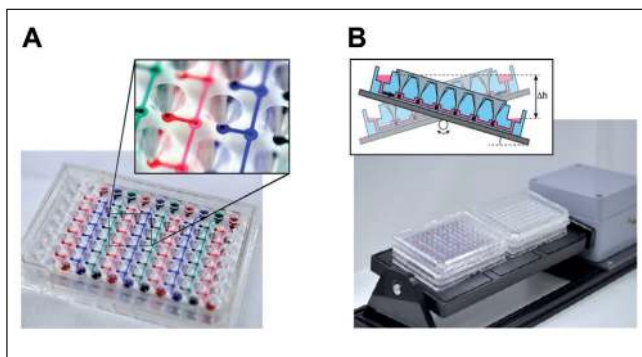
A recent survey of microfluidic and microengineered 3D cell culture systems conducted by Hankemeier and colleagues (van Duinen et al., 2015) at Leiden University, The Netherlands, found that most tissue modeling efforts published between 2012 and early-2015 in the field of MPS were focused on the vasculature. Authors explained the striking dominance of efforts in vascular modeling by the fact that MPS is the only platform capable of perfusing such vessels, thereby including the vitally important flow and accompanying shear stress. MPS emulating microvessels to study angiogenesis (Bischel et al., 2013; Zheng et al., 2012), permeability (Lee et al., 2014), pattern diffusive gradients (Baker et al., 2013), micro-vascular environments (Hasenberg et al., 2015; Kim et al., 2013b; Park et al., 2014; Tourovskaia et al., 2014; Wang et al., 2014a) and vascular response to vessel geometries (Ye et al., 2014) have been developed within the last few years. Finally, vascular MPS are used as models for arterial thrombosis (Huh et al., 2007; Westein et al., 2013).

Another important finding of the survey of Hankemeier and colleagues (van Duinen et al., 2015) was the fact that microfluidic cancer models published between 2012 and early 2015 hold approximately the same numeric share as the aforementioned microfluidic tissue models. Breast and lung cancer models comprise half of the cancer models published and many of the cancer models developed recently include a vascular component. Here again, MPS technologies provide the only platform to model tumor cell intravasation into a surrogate blood stream or immune cell extravasation into the tumor by combining human microperfused 3D tumor models with human vasculature. These systems add to our understanding of tumor progression. Migration (Haessler et al., 2012; Hockemeyer et al., 2014), intravasation (Zervantonakis et al., 2012) extravasation (Bersini et al., 2014; Jeon et al., 2013) and metastasis (Griep et al., 2013) have been studied in such MPS-based cancer models.

### 2.3.3 Microphysiological multi-organ system developments

Combining single-organ models towards integrated multi-organ configurations lifts the degree of complexity to a systemic level of organ interaction. Emulation of human organ-to-organ cross-talk, ADME pathways and systemic regulatory circuits between organs by such multi-organ systems is envisioned. Their development poses significant challenges both for plate- and chip-based formats. Different organ models have to be handled in the same device, remain fully functional at the same time and interact through the same circulating liquid phase. These challenges raise the qualification requirements for tools and approaches using multi-organ MPS to generate results that are reproducible and predictive of humans. Any technological plate- or chip-based MPS approaches chosen for these systemic models are a trade-off between complexity and *in vivo* resemblance on the one hand, and ease of use, reproducibility and potential for parallelization on the other hand (van Midwoud et al., 2011b). Olivier Frey's group at the ETH Zurich and InSphero AG, Switzerland, and collaborators pioneered the development of multi-organ plate concepts using 3D micro-tissue spheroids as a 3D tissue model (Kim et al., 2015a,b). The microfluidic platform is built in a way that micro-tissue development is completely uncoupled from microfluidic culturing and the loading of the spheroids is realized in a modular way (Fig. 8A).

The plate consists of straight channels connecting up to 10 identical compartments into which spheroids can be loaded using simple pipetting. The medium is perfused between two lateral medium reservoirs using gravity-based flow through tilting the platform periodically. A single plate comprises up to 10 channels so that up to 60 multi-organ conditions can be tested on a single tilting device (Fig. 8B). Human tissue spheroids generally possess inherent organotypic functionality and biomimetic morphology and can be manufactured precisely, reliably and flexibly in off-line automated systems. Their spherical shape makes them easy to handle and has enabled the development of plate- or chip-based MPS that are simple to handle and robust to operate. Multi-organ arrangements using spheroids can be built up in a very flexible way regarding the large variety of cell types with which spheroids can be formed so as to represent differ-



**Fig. 8: A prime example of a plate-based multi-organ system**

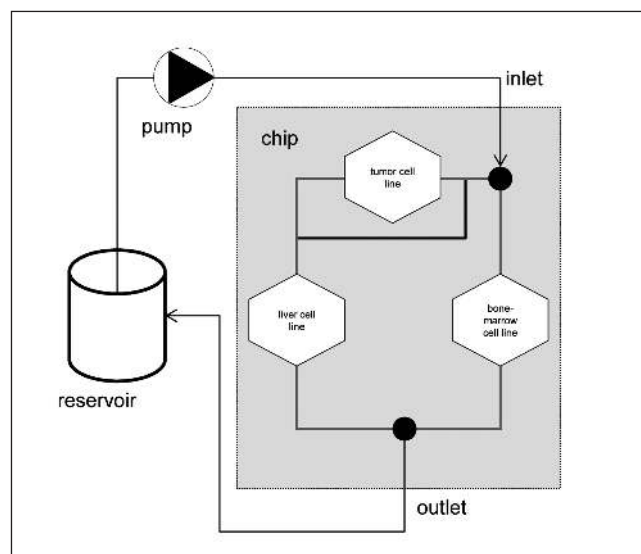
(A) A 96-well format multi-tissue interaction testing chip (close-up shows spheroid compartment with loading port). Ten parallel microfluidic channels interconnect six culturing compartments, in which spheroids of different types can be loaded.

(B) Platform operated in a standard incubator tilting the chips back and forth producing a gravity-induced flow between the different culturing compartments (courtesy of ETH, Switzerland).

ent organ models and fluidically interconnected systems of many spheroid compartments. The spheroid model can, thereby, be improved and further developed continuously without the need to redesign the microfluidic test platform itself. While offering a large amount of flexibility in arranging different organ models in physiological order as well as tuning the different tissue volumes and ratios over the number of spheroids introduced into the system, the limitation of this approach lies within the spheroid model itself. Spheroids are frequently considered as the smallest functional tissue unit. However, it is clear that spheroids do not include mechanical cues (dynamic forces such as breathing strains) nor are they vascularized. Multi-organ models based on spheroids will, therefore, focus predominantly on biochemical and metabolic interactions between different tissue types (e.g., adding metabolic liver functionality to bioactivation applications). For proof of concept (Kim et al., 2015a,b) primary rat liver tissues were cultured over eight days in combination with colorectal tumor micro-tissues (HCT-116). Interestingly, albumin secretion of the rat liver micro-tissues increased over the first few days in the fluidic devices compared to static culture conditions, which indicates further tissue maturation under flow conditions in the chip. The importance of interconnecting liver and tumor tissues was demonstrated by applying cyclophosphamide, a pro-drug which requires activation by the liver metabolism (mainly CYP2B6) to become effective. The impact of cyclophosphamide on tumor growth was simultaneously assessed under static culture conditions by discrete liquid transfer using a pipetting protocol and under perfusion conditions on the chip. Remarkably, hardly any effect on tumor growth was observed under static culture conditions, whereas a clear size decrease of the microtumor was detected after treatment with cyclophosphamide in the case of direct and continuous fluidic coupling in the chip. These findings illustrate the importance of continuous liquid and metabolite transfer between the different tissues or tissue compartments. In isolated spheroid configurations such transfer could only be

achieved with frequent discrete media exchanges. Suitable transfer timing and incubation times that are long enough to obtain the desired metabolic compounds are, however, difficult to estimate and optimize. Furthermore, the comparably large well volumes of conventional setups may result in the active metabolites being diluted too much. Increasing the cell-to-medium volume ratio by co-culturing spheroids in the same well would lead to uncontrolled tissue fusion. The findings further demonstrate that the use of well formats with an already labor-intensive pipetting protocol cannot reproduce the results obtained with continuous media exchange, as has been exemplified for a setup including only two different tissue types. Pipetting approaches are no longer an option for experimental scenarios requiring more than two different tissue types, as the respective protocols become very complex, whereas microfluidic networks offer viable solutions. This plate-based MPS technology is being developed for commercialization by InSphero AG, Switzerland.

Another approach of the same group includes the use of the hanging drop itself – the primary technique to form spheroids – as an on-chip culturing compartment (Frey et al., 2014). Arrays of hanging drops are linked to functional hanging-drop networks, in which the medium can be perfused between the drops and interconnects different spheroid types. The platform combines formation and culturing of spheroids of different cell types without any risk of adhesion or functional loss, as spheroids are located on the liquid-air interface. The array-based format enables parallel multi-tissue experiments and reproduced the cyclophosphamide bioactivation study described above. The integration of an on-chip pulsatile micropump, with its stroke



**Fig. 9: Scheme of the flow diagram of a  $\mu$ CCA**

The chip is 25 by 25 mm and flow channels are 20-100  $\mu$ m wide. Flow is laminar and typically more than 10,000 cells populate each tissue culture compartment. The design is based on the Hagen Poiseuille Law, which allows matching human-like fluid velocity in each channel and liquid residence time in each compartment with the respective PKPD model *in silico* (modified from Marx et al., 2012).

rate synchronized to the beating of a human iPS-derived cardiac spheroid, recently “added the heart” to the hanging-drop network technology (Rismani et al., 2015).

Another plate-based system has been used to investigate intestinal first pass metabolism coupled with secondary liver metabolism of paracetamol using a co-culture of CaCo-2 and HepG2/C3A cells over 24 h (Prot et al., 2014). The results demonstrated paracetamol transport through the intestinal unit followed by synergistic metabolism via the production of paracetamol sulfate in both the liver and intestinal units. Glucuronide paracetamol was detected in the liver co-culture.

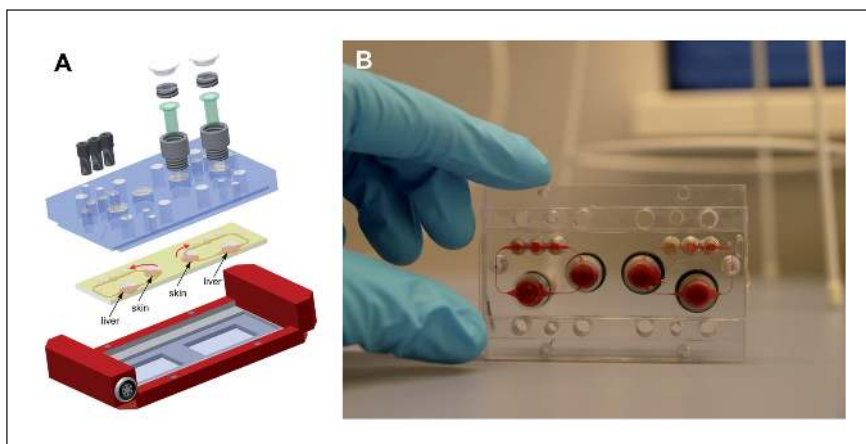
Michaels Shuler's group at Cornell University, Ithaca, NY, US, pioneered the development of human multi-organ chips (MOCs). They developed a chip-based miniaturized micro-cell culture analog ( $\mu$ CCA) which was used for pharmacokinetic/pharmacodynamic (PK/PD) modeling as early as 2004 (Sin et al., 2004). The system supports physiologically based pharmacokinetic, quantitative structure-activity relationship (QSAR) studies and quantitative *in vitro* to *in vivo* extrapolation (QIVIVE) modeling. It combines different human tissue cultures into a common media flow for the prediction of the time-dependent concentration of a parental compound and its metabolites. The principle design of the system is schematically illustrated in Figure 9. It relies on the recirculation of a common culture medium with around 10,000 cells per culture compartment and substance exposure times of up to four days.

The proof of concept was provided in studies with naphthalene as a model toxicant (Viravaidya et al., 2004). Furthermore, two combination therapies using doxorubicin (Tatosian and Shuler, 2009) and tegafur (Sung and Shuler, 2009) have been tested on human cancer cell lines in  $\mu$ CCA layouts specifically developed for substance testing applications. The system at its selected scale provides *in vivo*-like tissue mass ratios among the culture compartments, a media inflow split equivalent to the respective blood flow split in humans, and relevant residence times in tissue compartments. Furthermore, the microfluidic chip design is claimed to support physiological shear stress and liquid to cell ratios, mimicking those of the respective organ. It can be operated over periods of up to four days. The platform is commercialized by Hurel Corporation, North Brunswick, NJ, US. The layout of the  $\mu$ CCA has progressed over the years (Mahler et al., 2009a,b, 2012; Sung et al., 2010; Sung and Shuler, 2010). The following goals to advance the  $\mu$ CCA technology into a routine test assay platform were summarized in 2012 (Shuler, 2012):

- Avoidance of any pump system by design of a “pumpless” chip with a gravity-based media flow;
- improvement of the monitoring and control periphery;
- maintenance of mechanical forces or electrical coupling, where relevant;
- improvement of the common culture medium into a more realistic blood surrogate; and
- improvement of organotypicness of cell culture compartments from 3D human cell line constructs towards primary human organoids, addressing their specific ECM architecture, epithelial barriers, stromal tissue impact, physiological absorption, and secretion or evaporation kinetics of water where relevant.

A  $\mu$ CCA platform-based two-organ chip mimicking the gastrointestinal tract by a co-culture of CaCo-2 cells and the mucin producing cell line TH29-MTX, and the liver by a HepG2/C3A cell line culture has recently been described by Shuler's team (Esch et al., 2014). This intestine-liver chip was exposed to nanoparticles over a period of 24 h. The results suggest that ingested carboxylated polystyrene nanoparticles have the potential to cause liver injury in the system. In a next step, the group developed a four-organ chip for toxicity testing (Oleago et al., 2016). A low-cost, pumpless gravity driven flow system for maintaining viable and functional human cardiac, liver, skeletal muscle and neuronal cultures within a common defined medium for two weeks has been recently described. These cell types were chosen to provide insight into important metabolic and functional changes in human tissues in response to challenge with doxorubicin, atorvastatin, valproic acid, acetaminophen and N-acetyl-aminophenol with well-defined toxicological properties. The presented data demonstrates the survival and continued functionality of all four human cell types over a 14-day culture period under flow and their response to a 48 h single dose exposure to the drugs. The results of all drug treatments were in general agreement with published toxicity results from human and animal data. The presented phenotypic culture model exhibits a multi-organ toxicity response and constitutes a step towards an *in vitro* “human-on-a-chip” assay for systemic toxicity screening. The latest prototype of the development in Shuler's lab is a 10-organ prototype illustrated in Chapter 4 of this report.

A range of other MOCs targeting systemic arrangements of different human tissues on a chip have emerged. A customizable Lego<sup>®</sup>-like plug & play system,  $\mu$ Organo, which enables initial individual culture of single organ-on-a-chip systems and subsequent connection to create integrated multi-organ microphysiological systems has been constructed by Loskill and colleagues (2015). As a proof of concept, the  $\mu$ Organo system was used to connect multiple heart chips in series with excellent cell viability and spontaneously physiological beat rates. Experiments with multi-tissue arrangements are ongoing. Zhang and co-workers from the Institute of Bioengineering and Nanotechnology, Singapore, have developed a multichannel 3D micro-fluidic cell culture system providing four separate channel-based cell culture spaces which can be loaded with tens of thousands of cells each (Zhang et al., 2009). Human liver, lung and kidney cell lines and primary human adipose cells were arranged in micro-channels shielded from direct shear stress to mimic *in vivo* shear stress protection by endothelial walls. Recirculation at flow rates of 0.2 ml/min and exposure times of two days for transforming growth factor  $\beta$ 1 led to a discrete biological response of the human lung cells, whilst other compartments remained uncompromised. Another integrated systemic solution for the emulation of intestinal absorption, hepatic metabolism and toxic responsiveness of human breast carcinoma cells applying four commonly used drugs has been reported by Imura and co-workers from the Department of Applied Biological Chemistry, School of Agricultural and Life Sciences of the University of Tokyo (Imura et al., 2010). Their system provides a unidirectional flow in a chip format the area of a microscope slide. It supports the constant perfusion of tens of thousands of human HEPG2 cell line-based



**Fig. 10: Multi-organ chip platform**

(A) A PDMS chip (yellow), 3 mm high, bonded onto a microscopic slide hosts two independent microcircuits with a circulation channel of  $100 \times 500 \mu\text{m}$ . Each channel connects two tissue culture compartments, supporting the integration of 3D tissues, such as cell spheroids, and standard 96-well inserts for reconstructed barrier organ models. A peristaltic on-chip micropump (black) enables pulsatile unidirectional fluid flow at physiological frequencies. (B) Represents a worm's-eye view of two blood-perfused circuits (reprinted from Marx et al., 2012).

hepatocytes and human MCF-7 cell line-based human breast carcinoma cells, consecutively arranged in a single microchannel. Drugs are provided through a tightly closed monolayer of human CaCo2 cell line-based intestinal epithelial cells into the media flow of the channel before the liver compartment, emulating the absorptive properties of the human intestine. Exposure time reached two days at a flow rate of  $0.4 \mu\text{l}/\text{min}$  and led to discrete biological effects on the human breast carcinoma cells. Ifosfamide nephrotoxicity has been investigated over 72 h in a liver-kidney co-culture MPS in comparison to static conditions (Snouber et al., 2013b). The results suggest that ifosfamide nephrotoxicity in a liver-kidney microfluidic co-culture model using HepaRG-MDCK cells is induced by the metabolism of ifosfamide into chloroacetaldehyde. This study demonstrated the capability of multi-organ systems to detect secondary metabolite toxicity, combining a human cell line-based liver model with a second target organ, in this case, kidney.

Gordana Vunjak-Novakovic and her colleagues are developing a HeLiVa multi-organ platform with functionally connected vascular, liver and cardiac microtissues derived from a single line of human pluripotent stem cells (Vunjak-Novakovic et al., 2013). The ability to derive all necessary cell types for multi-organ systems from one donor source is a very important prerequisite for advancement into immunocompetent multi-organ systems to avoid organ rejection due to donor incompatibility. The platform enables functional representation of human physiology in conjunction with real-time biological readouts (via imaging and homologous reporters for all three cell phenotypes) and compatibility with high-throughput/high-content analysis. The first prototypes of microfluidic platforms for the formation and cultivation of vascular, cardiac and hepatic microtissues are currently under evaluation to demonstrate utility of human iPS cell derived microtissues for physiological and pharmacological studies.

In order to overcome the non-physiological fluid-to-tissue ratio caused by the use of external pumps and reservoirs in all pump-based aforementioned MOCs, the group of Uwe Marx at the University of Technology Berlin and their collaborators designed and prototyped a MOC platform (Fig. 10) in a standardized chip format of the area of a microscopic slide, equipped with a robust peristaltic on-chip micropump, modified from Wu

and colleagues (2008). It supports pulsatile recirculation of medium flow through one, two or more tissue culture compartments at near *in vivo*-like rates and pulse frequencies. Furthermore, the organ culture compartments of this MOC platform universally support the culture of 3D cell spheroids, reconstructed tissue equivalents, such as insert-based skin or intestine, and donor-derived tissue explants or biopsies. The platform aims at homeostatic long-term performance of co-cultured human organ models over at least 28 days to enable repeated dose systemic substance exposure. A robust and reproducible 28-day co-culture process of human HepaRG-stellate cell spheroids interconnected with insert-based human skin biopsies was established, each  $1/100,000$  of the biomass of their original human organ counterparts (Wagner et al., 2013). Functional skin could be maintained in an air-liquid interface during on-chip co-culture. Furthermore, the total fluid-to-tissue ratio in the system supports tissue crosstalk, indicated by the consumption of albumin produced by liver tissue by the skin. Finally, the co-cultures revealed a dose-dependent toxic response to a 6-day repeated dose exposure to troglitazone, a diabetes drug withdrawn from the market due to drug-induced liver injury. Another two-organ co-culture using the MOC platform combined the 3D liver model described above with a commercially available reconstructed human 3D small intestine model (Maschmeyer et al., 2015a). This aimed to increase human organotypicity of the barrier compared to the CaCo-2 barriers and to improve robustness and industrial applicability. A reproducible and easy to perform oral substance administration protocol was applied over a stretch of 11 days after a three-day administration-free adaptation period, resulting in a continuous two-week MOC performance at repeated dose testing conditions. Immunohistochemistry of transporters, transepithelial electrical resistance measurement of barrier integrity and gene expression analysis revealed stable intestinal barrier functionality, whilst the troglitazone treatment decreased albumin mRNA expression in the liver spheroids.

The same platform was used to repeatedly expose a long-term co-culture of human liver and neuronal spheroids to hexanedione (Materne et al., 2015). 14-day co-cultures of the aforementioned liver spheroids with human neuronal spheroids, preformed and differentiated in a stirred tank bioreactor using the NT2 cell



line, were exposed daily to different doses of hexanedione over an 8-day period. Sensitivity profiles of the co-culture could be compared with the responses of the single organ chips and revealed higher levels of sensitivity. Finally, a robust procedure to integrate biological vasculature into the microfluidic channels of the MOC platform was established under physiological fluid flow conditions (Schimek et al., 2013). Thus, the MOC platform is suitable for long-term repeated dose substance evaluation at homeostatic conditions combining human primary or cell line-based 3D micro-tissues. It is commercialized by TissUse GmbH, Berlin, Germany. Rapid prototyping tools allow the flexible adjustment of MOCs to any new format. Thus, 28-day four-organ co-culture has recently been established in MOC format as a human organotypic ADMET test chip (Maschmeyer et al., 2015b): Reconstructed human small intestine was interconnected with a liver spheroid model, a skin biopsy at air-liquid interface and a human proximal tubule cell monolayer barrier. All human tissues maintained a high cell viability and discrete physiological tissue architecture over the entire co-culture period of 28 days. The human small intestine epithelia formed stable 3D villi-like structures of up to 270  $\mu\text{m}$  height and expressed an apical brush border. Skin biopsies developed a stratified stratum corneum at the air-liquid interface. The human proximal tubule epithelia maintained a functional polarized monolayer barrier. Small intestine and kidney proximal tubule cell barriers were able to keep up a continuously stable glucose gradient balance between the intestinal lumen, the surrogate blood circuit and the excretory circuit of the system. Moreover, in-depth metabolic and gene analysis revealed the establishment of reproducible homeostasis between all four tissues over at least 28 days, independent of the individual human cell line or tissue donor background used for each organ equivalent. The four-organ chip has been designed to support ADME profiling of substances along with repeated dose systemic toxicity testing of drug candidates. Evaluation of physiological absorption, first pass metabolism and pharmacokinetic and pharmacodynamic parameters such as effective concentration, maximum tolerable dose, time course, and intensity of therapeutic and adverse effects are envisioned. Finally, the system might support investigation of damage and regeneration of the intestine and skin compartments due to their stable physiological turnover in the system. The next step of the MOC at Uwe Marx' lab is a 10-organ prototype illustrated in Chapter 4 of this report.

Other multi-organ systems integrating two or more organ equivalents are under development in Linda Griffith's lab at MIT and in Donald Ingber's lab at the Wyss Institute at Harvard financed by the US DARPA/NIH/FDA initiative. Both groups have successfully demonstrated several two-organ chip variations (e.g., MIT liver/immune, gut/immune, endometrium/epithelial and lung/airway MPS) to the project evaluation committee. Further, progress towards a four-organ platform with these MPS, for which two-week viability and functionality was achieved, was recently presented to DARPA/NIH/FDA by the MIT team. The DARPA/NIH/FDA initiative is described in more detail in Chapter 4 of this report in the context of the development of human body-on-a-chip platforms aiming to emulate organismal complexity of human biology *in vitro*.

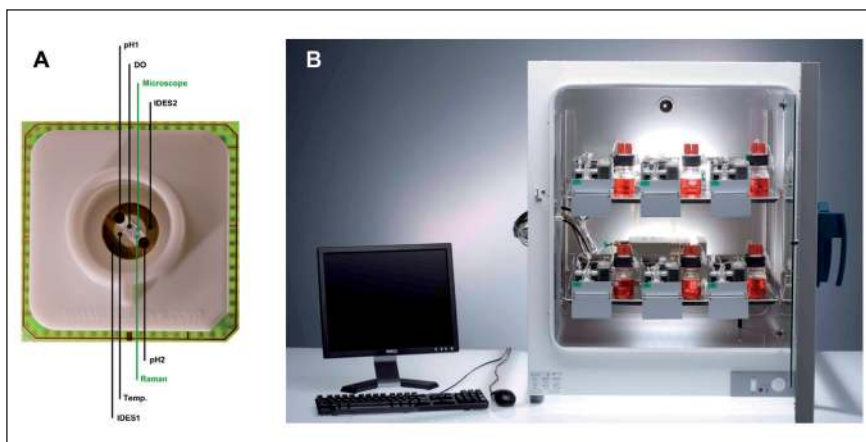
## 2.4 Computational models, in-process controls and readouts for MPS

The use of computational and experimental paradigms for single and multi-MPS is critical to build physiologically and pharmacologically relevant MPS and interactomes. On-platform scaling describes how tissue weights, media volumes and inter-MPS flow rates can be based on either allometric scaling or functional scaling (Stokes et al., 2015). Computational fluid dynamics simulations calculate flow and oxygen/drug distributions, and shear stresses (Domansky et al., 2010). Physiologically based pharmacokinetic (PBPK) models investigate platform design and data interpretation via predicting/analyzing drug concentrations and exposure for given operational parameters, such as inter-MPS flow rates and MPS volumes (Yu et al., 2015). Correlation, extrapolation and translation of results in such MPS systems only can be performed with the proper use of various computational models. *In vitro/in vivo* correlation of pharmacokinetic parameters is widely used for simpler systems (Brown et al., 2007; Obach, 1999). The superior advantage of MPS technologies comes into play when we extrapolate drug and organ interaction where the biology is less well understood. Combining systems biology and pharmacology models with high-content experimental data from MPS technologies will allow *in vitro* to *in vivo* translation, advancing clinical outcomes (Stokes et al., 2015).

MPS-based assays aim for comparability with standard tests and approaches currently in use. Process controls and endpoint analysis should at least match those required in current gold standard tests. For laboratory animal experiments – often the gold standard in the field – daily laboratory analysis of blood and urine, body temperature and visual monitoring of animal behavior are the most common in-process controls. These can be matched by daily medium analysis and viability testing in MPS-based assays. The instrumentation of MPS should be able to monitor and control tissue culture temperature, pH and oxygen consumption. This, in combination with, for example, LDH measurement and glucose consumption analyses in media, provides a good match to the visual inspection of animals' general behavior. A critical aspect of these fundamental in-process controls is the limited amount of medium (blood surrogate) available for analysis due to the miniature size of the MPS. Prime endpoints for toxicity studies in animals are dose-dependent death and histological analysis of all relevant organs after necropsy. Viability assessment in MPS has already been discussed. Organ histology in animals, to a certain degree, can be matched with histological analysis of the MPS tissues similarly fixed, paraffin-embedded and stained, including immunofluorescent staining for proteins and other markers. Disease modeling and efficacy testing in animals applies disease-specific in-process controls (e.g., serum biomarkers, leukocyte monitoring, biopsies, neuronal electrodes, EEG, ECG) and endpoint analysis (e.g., pathohistology, restoration of organ function). Not all of these are easily applicable to MPS-based disease models. However, MPS offer analysis opportunities that cannot be performed in laboratory animals and patients.

Due to their minute size, real-time optical access at high spatial resolution, and the tight instrumentation-based control of their environment, biological events that cannot be monitored in





**Fig. 11: A prime example of MPS instrumentation**

(A) BioChip-D (24 x 24 mm<sup>2</sup>) with microsensors for pH, dissolved oxygen, impedance and temperature. (B) The sensors are manufactured on a transparent substrate allowing additional optoanalytical methods. Computer-controlled 6xIMOLA-IVD arrangement with six measurement units and an automated fluidic system pre-mounted in an incubator (courtesy of cellasys GmbH, Germany).

animals or patients can be followed in MPS-based organ models. In principle, all modern tissue and cell analysis methods, such as PCR, (methylated) DNA and RNA sequencing, mRNA expression profiling, proteomics, metabolomics and multiplex protein analysis (e.g., Luminex), can be used on (single) cells, tissue slices or flow through solutions to characterize cells, intracellular processes and tissue architecture. Model-specific assays also can be developed, including electrical monitoring by microelectrode arrays, for example, for MPS-based heart or brain models. Optical access to the micro-tissues of MPS allows the use of 3D microscopic imaging of cell morphology and ECM architecture, as well as fluorescent imaging, both at sufficiently high resolution (at least around 1 micron) to distinguish nuclear or cytoplasmic localization in a cell. The main challenge is to combine sufficient focus depth with high resolution. Optical coherence tomography to a depth of 1-2 mm into the tissue, with space- and time-resolutions of micrometers and tenths of a second, respectively, is an attractive option. Other imaging techniques, such as confocal laser scanning microscopy, dual or multi-photon fluorescent microscopy, Raman spectroscopy or fluorescence-lifetime imaging microscopy, can be applied.

Numerous label-free, nonoptical methods have proven to be valuable tools for the monitoring of living systems (Fang, 2015; Wang and Liu, 2010). Extracellular acidification can be monitored with pH sensors, such as light addressable potentiometric sensors, ion sensitive field effect transistors, opto-chemically or with simple potentiometric sensors (Brischwein et al., 2009). Dissolved oxygen can be measured with amperometric sensors or optochemically. Impedance sensors, quartz crystal microbalance systems, surface plasmon resonance systems and surface acoustic wave systems are used to monitor morphological changes. The activity of electrophysiologically active cells (e.g., cardiomyocytes or nerves) is monitored with microelectrode arrays (Liu et al., 2014). These label-free methods allow real-time, time-resolved monitoring of cellular parameters which may be a great advantage in the field of MPS, since automated label-free monitoring of the living system for hours and days is achievable. However, the use of, for example, fluorescent markers, bears the risk of activating receptors and altering the behavior of the MPS (Shinawi et al., 2013)

## 2.5 Instrumentation, prototyping and manufacturing of MPS

MPS are composed of a cell culture part – a plate or a chip – and the instrumentation used to control and operate the cell culture part: incubators, pumps, tilting devices, control units with sensors and actuators, optical imaging devices and automated pipettors. The challenges of developing instrumentation for MPS have been reviewed elsewhere (Wikswow et al., 2013).

On-chip pumps have been one of the most challenging hurdles. Electromechanical or gas pressure controlled peristaltic micropumps are integrated into the microchannel circuits for a maximum of autonomous operation and to ensure low perfusion rates for circulation and exchange of culture media (Busek et al., 2013; Schimek et al., 2013). Miniaturized sensors based on thin-film or microbead-based fluorescent indicators (Liebsch et al., 2000; Schmäzlin et al., 2005) are increasingly implemented into MPS to monitor and control dO<sub>2</sub>, dCO<sub>2</sub> or pH. Several reviews have summarized the current status of technologies for electrical coupling of neuronal and cardiac cell cultures to record physiological signals and stimulate the cells (Gosselin, 2011; Hierlemann et al., 2011; Simmons et al., 2012; Spira and Hai, 2013). Electrical coupling of neuronal cells in a dynamic microfluidic environment using microelectrodes was described as early as 2005 (Pearce et al., 2005a,b). Electrical coupling of muscle cells cultured in MPS has also been described (Agarwal et al., 2013; Ahadian et al., 2012; Cheng et al., 2006; Dvir et al., 2012; Grosberg et al., 2012; Klauke et al., 2003, 2006, 2007; Werdich et al., 2004). A prime example for feasible instrumentation for MPS is the cellasys (Kronburg, Germany) technology (Fig. 11), which employs BioChips with label-free microsensors for pH, dissolved oxygen, impedance and temperature, and was used to monitor living cells in suspension, adherent monolayers, primary tissue and 3D spheroids for more than a month (Weiss et al., 2013; Wiest, 2015). The 6xIMOLA-IVD consists of six measurement modules which can be operated in parallel or serial mode. A computer-controlled fluidic system with peristaltic pump, valves and air bubble detectors allows a flexible arrangement of the MPS with 24 channels. This modular approach can be used to select different units out of a toolbox to build various organ-on-a-chip setups.

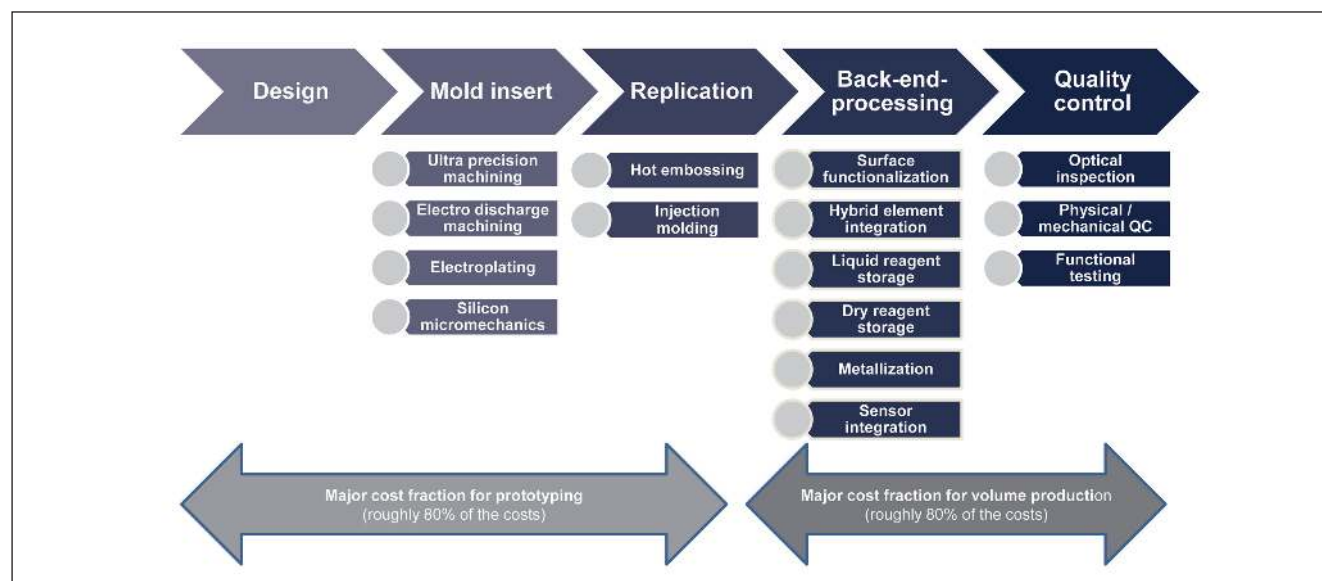
Prototyping and manufacturing of the (mostly disposable) cell culture part of MPS is another challenge in the field. Affordable, easy to handle, reliable and scalable manufacturing approaches applicable for volume fabrication in an aseptic environment are required to meet the demand in ready-to-use chips, combining the desired polymers, metallic sensors and immobilized biological molecules, cells or tissues. For these reasons, fabrication of MPS requires a multidisciplinary approach combining the engineering aspect with biological functionality. General principles of microsystems relevant for biological applications have been described in detail (Ziaie et al., 2004). Polymer devices are used for most applications in the life sciences. Thermoplastic materials dominate for industrial applications since this is a scalable fabrication technology, whilst the soft polymer PDMS is a widely used material in the academic world. The challenges of fabrication of microfluidic cell culture systems and the pros and cons of soft PDMS-based systems versus thermoplastic polymer systems in the field of MPS have been reviewed elsewhere (Alrifaiy et al., 2012; Andersson and van den Berg 2004; Berthier et al., 2012; Huh et al., 2013; Kim et al. 2007; Park et al. 2003; Wu et al. 2010). A replication-based technology, such as injection molding or injection compression molding, is a valid option for scalable industrial fabrication with a long track record in the industry of life science consumables (Becker and Gaertner, 2008, 2012). The technology chain for the realization of MPS in thermoplastic polymers is summarized in Figure 12.

The chain starts with the design of the system, followed by the realization of a mold insert with the respective microstructures that will, subsequently, be replicated. The mold insert fabrication is the critical process, since all follow-up fabrication steps rely on the quality of the template generated at this point. After mold insert generation, the master will be replicated in polymers by injection or injection-compression molding allowing for high volume fabrication. Keeping in mind that these first fabrication steps consume 80% of the cost of prototyping or

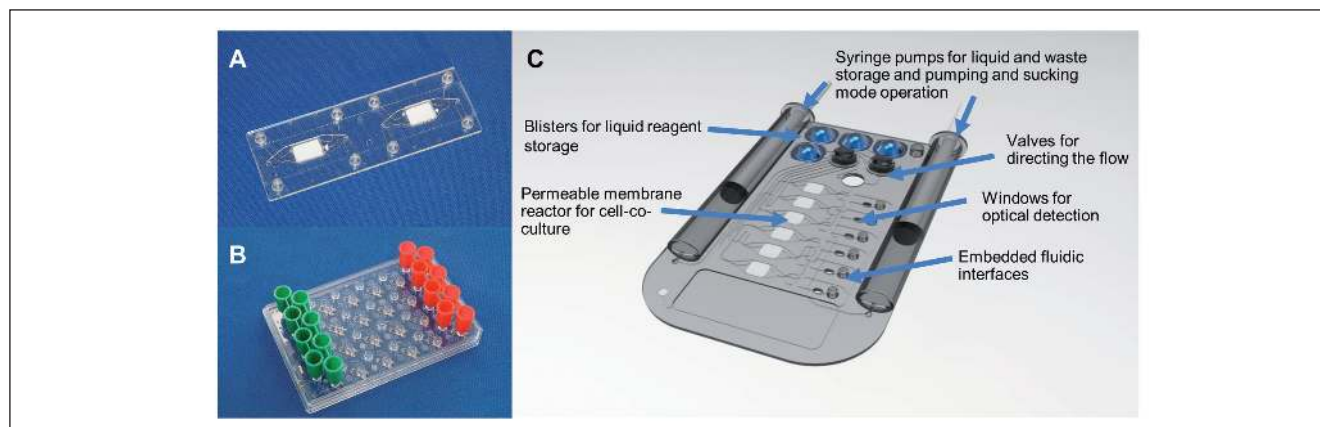
low-volume manufacturing, the back-end processes consume up to 80% of the overall cost at a higher-volume fabrication scale. Back-end processes summarize steps such as surface functionalization, bonding, assembly, integration of hybrid elements, e.g., membranes, sensors, valves, and dry and liquid reagents. The final step is quality control, which requires, in addition to physical inspection, technologies such as optical evaluation, in particular a functional control in the case of biological reagents, and finally, cells or pre-assembled tissues can be shipped. Taking the cost-structure into account, a design for manufacturing is a crucial step towards later commercial success and the penetration of the new technology into standard laboratory life.

It is beneficial for any product development to start directly with the material that is intended to be used for the later product. When envisioning using thermoplastic polymers, such as cyclo-olefinic polymers (trade name “Zeonor”), cyclo-olefinic co-polymers (tradename “Topas”) or, in particular, polystyrene, which is a standard material for cell culture petri dishes or microtiter plates, these materials should also be used for prototyping. As in the microfluidic area of the life science world, from which the MPS approach originates, standard formats are used: the format of a microscopy slide (75.5 x 25.5 mm) and that of a microtiter plate. This has two major benefits: family tools for fabrication can be used for a large variety of application-specific designs, therefore not requiring larger investments even at medium scale production. Also, the same fabrication chain for the back-end processes can be applied, making the realization of MPS affordable from the start through scalable fabrication technologies. The standardization of MPS formats allows the use of the complete instrumentation for lab automation and screening, namely pipetting robots, imaging systems, incubation and storage elements and standard microscope setups.

Figure 13 illustrates two different MPS formats from microfluidic ChipShop – a chip and a plate – fabricated using the technology chain outlined above. The chip in the format of a



**Fig. 12: Technology chain for scalable industrial manufacturing of polymer-based MPS**



**Fig. 13: Hard micro-machining of microfluidic plates and chips**

MPS examples of a chip and a plate manufactured using thermoplastic polymers. (A) Microscopy slide format chip with integrated fluidic interfaces with cross-flow operating membranes for on-chip co-culture of cells. (B) A microtiter plate-sized platform with on-plate reservoirs for passive hydrodynamic driven fluid flow (design HepaChip project, FKZ 031A121D). (C) Animation of an integrated MPS with parallel on-chip co-culture of different organ equivalents and on-chip liquid supply, including windows optical imaging of metabolites (courtesy of Microfluidic ChipShop, Germany).

microscopic slide requires a microstructured molded part, integration of a membrane, assembly of top and bottom with a cover lid and surface functionalization. With this straightforward scalable fabrication technology simple devices for cell co-cultures can be realized on-chip. The lower left picture illustrates a microtiter plate-sized device combining fabrication steps such as injection molding, thin film technology for electrode integration, surface functionalization, biological reagent patterning and assembly with a cover film. The design of an integrated device fulfilling multiple tasks is shown on the right-hand side: Injection molding, integration of membranes and valves, liquid reagent implementation and pressure driven flow through embedded syringe pumps are some of the challenges towards the illustrated fully integrated MPS.

### 3 Industry test standards, unmet needs and potential for MPS adoption

Although there are only a small number of young companies, e.g., AIM Biotech, Bionas, cellasys, CN Bio Innovations, Emulate, Hesperos, Hurel, InSphero, Kirkstall, micronit, Mimetas and TissUse, providing MPS devices, they are already advanced enough to provide exploratory platforms for feasibility studies. Certain members of the pharma and cosmetics industries have already been investigating the use of MPS for hazard potential identification, and safety and efficacy testing; however, to the knowledge of the workshop experts none of the current MPS-based approaches and tools has been adopted by these industries to date. In this chapter, we report the results of the workshop discussions and subsequent surveys with regard to current standards of substance testing in the pharmaceutical, chemical/cosmetics and tobacco industries. On the basis of this information experts from each industry segment summarize the unmet needs in the field. Finally, potential directions for demand-driven

an industrial adoption of relevant MPS-based approaches in the industries are highlighted.

#### 3.1 Pharmaceutical industry – test standards and potential for MPS adoption

##### 3.1.1 Aspects of pharmaceutical safety assessment

Drug safety assessment is an ever evolving process which takes account of both historical data and newer findings, together with changing regulations from authorities and new experimental and technical capabilities. Drug safety assessment today spans a large battery of *in silico*, *in vitro* and *in vivo* tools, which aim to select and optimize the best candidates for safe dosing in humans. A portion of the tests are required to gain approval by regulatory authorities, while other tests are used for internal decision-making and for mechanistic understanding of adverse effects. Required tests include, for example, assessment of the genotoxic potential by MNT (micronucleus test) or AMES (Bruce Ames' test), an indication of risk of cardiac arrhythmias (torsades de pointes, assessed by measuring the inhibition of the human ether-a-go-go-related gene channel) or the estimation of drug-drug interaction potential in liver using *in vitro* assays. On an *in vivo* level, the indication of target organs of toxicity, types of toxicities, plasma exposure, and distribution and excretion patterns on a quantitative basis in both a rodent and a non-rodent species, taking into account comparable treatment duration, are expected as part of a package for entry into human trials. These are just a few examples and the requirements vary depending on the drug modality (small molecule, peptide, large molecule, other), drug administration route (orally, by inhalation), disease indication, and existing knowledge in a particular area.

Despite continuous improvements, there are failures in drug programs, both in preclinical and in clinical stages (e.g., Arrow-smith and Miller, 2013). Drug programs stopped at preclinical stages usually face issues with unacceptable, acute or severe toxicities, exposure incompatibility or similar types of effects,



which would make successful development of a drug unlikely. As highlighted in Chapter 1 of this report, industry benchmarks for candidate success rates in phase I clinical trials are 48-64% (Cook et al., 2014; Hay et al., 2014). Cardiac and liver toxicity are the prime contributors to these withdrawals, followed by kidney toxicity. Thus, there is still an unmet need to develop *in vitro* systems mimicking these human organs in a near to *in vivo* environment. Here, MPS-based single-organ systems might contribute with long-term *in vitro* stability for repeated dose substance testing over weeks. A significant improvement of existing MPS-based liver, neuronal, cardiac or kidney systems would be desirable. For easier industrial adoption, we recommend the generation of a biological baseline for each chip-based single organ equivalent. Exemplarily, it is necessary for MPS-based liver systems to determine the architectural and functional correlation of the chip-based liver equivalent with the *in vivo* liver based on histology, analysis of gene expression, protein levels, such as albumin secretion, CYP450 (particularly selected protein activities such as CYPs 1A, CYP2C and CYP3A), ATP, GSH, LDH, AST, ALT and metabolite analysis. We further recommend the generation of an extensive time course of both early and late time points and to compare it with data of standard hepatocyte cultures. In a next step, well-known hepatotoxicants should be assessed by the chip-based liver equivalents to prove that additional data can be derived at tissue level in contrast to static hepatocyte models. We would advise the use of early and late time points and, if possible, pharmacologically relevant doses for assessment. Improvements of the MPS-based liver models reported would be a segregation of bile from long-term cultures and the integration of immunocompetent cells, e.g., Kupffer cells. This scheme of improvement of single organ MPS can be universally applied to the other human organ models.

Another important added value for pharma safety testing could be the qualification and validation of the liver+X two-organ systems presented in Chapter 2.3.3. Such organ arrangements might lead to assays reliably allowing the elimination of candidates that are not toxic *per se* but through their liver metabolites from nonclinical pipelines. Finally, immunogenicity evaluation of biopharmaceuticals is another unmet safety need. Most large biomolecules in the pipeline are of human origin. This makes immunogenicity testing of such candidates in animals obsolete. Human immune organ cultures that can predict immunogenicity of candidates are under development (Giese and Marx, 2014).

Drug-induced idiosyncratic injuries of individual organs, e.g., liver, based on a genetic predisposition of a tiny subpopulation of patients and the properties of a given drug pose a big unmet challenge in the pharmaceutical safety assessment space. Drugs inducing this type of toxicity often fail only in late clinical stages or after market approval. In many cases, the program is terminated if the mechanism cannot be fully elucidated. These effects usually arise from a potential liability of the drug combined with a patient-derived factor (genetic predisposition, disease-specific). Toxicity arises only when these two aspects occur together. Some of the idiosyncratic drug-induced liver mechanisms are dependent on specific HLA types and possibly on specific factors of the adaptive immune system. For these cases, MPS-based

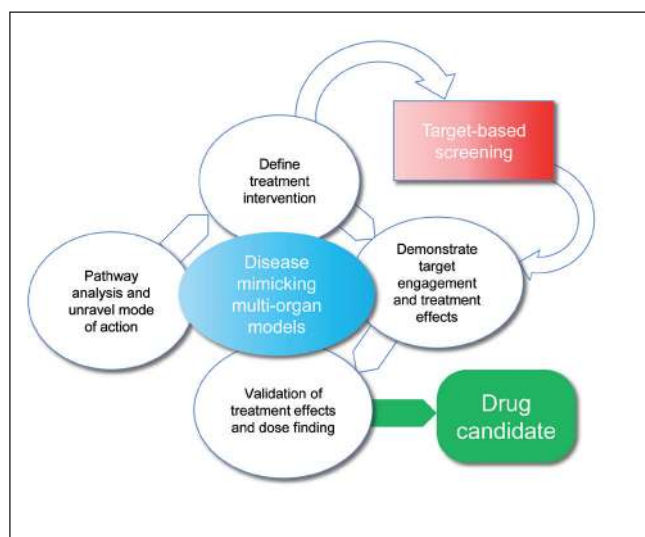
screening platforms might be worth trying. Furthermore, the extension of the multi-tissue systems towards systems physiologically arranging an intestine and a kidney equivalent with a liver equivalent on a chip may enable the generation of ADME data and PK/PD analysis within one experimental setting, provided quantitative aspects of drug uptake, distribution and excretion can be recapitulated *in vitro*. All the desirable MPS developments mentioned previously can be implemented both in screening strategies and in mechanistic investigations.

There are other major fundamental challenges when working *in vitro*, one being the quantitative translation from an *in vitro* to an *in vivo* effect. The concept of investigating AOPs, for example, which has arisen from the cosmetics and chemical industry in their effort to seek alternatives to systemic toxicity studies, cannot really be linked to the concept of defining a “No Observed Adverse Effect Level” established for clinical drug development: What does a toxic effect at 10  $\mu\text{M}$  influencing an AOP mean for the clinic if we do not know the kinetic parameters, the exposures, metabolism, distribution and elimination of the drug, in humans? Information on AOPs may not be directly translatable to the *in vivo* situation where doses have to be defined. In addition, such quantitative estimates are generally not available in the early stages of drug development when *in vitro* tests are applied, and this makes firm statements on the relevance of an *in vitro* flag difficult. Historical data can be employed to validate some but not all of these endpoints, and a drawback of historical datasets is that the chemical space of, for example, 1970 drug development may be very different from that in 2016. Therefore, MPS-based assays mimicking human multi-organ arrangements with physiological blood flow at scaled down parameters matching basic physiological principles in patients are highly desirable for pharmaceutical safety testing.

### 3.1.2 Test standards, unmet needs and new approaches in efficacy testing

Efficacy of drug candidates is assessed along the drug development cycle. Drugs no longer fail in the clinic because of undesirable physicochemical or pharmacokinetic properties. Instead, a major reason for failure is lack of efficacy. *In vivo* efficacy and activity testing in laboratory animals are a major cornerstone of and requirement in preclinical phases. These tests are accompanied by *in vitro* bioassays, such as target binding and potency assays. A compilation for oral small molecules from four large pharmaceutical companies revealed an attrition rate of 35% in phase II due to efficacy concerns (Waring et al., 2015). This high late stage attrition rate demonstrates the limits of knowledge on the efficacy and MoA of a drug candidate gained in preclinical studies.

The clinical relevance of most targets pursued in drug discovery is often not completely understood. Since the advent of the rational design concept in the late 1970s, the focus of most screening programs in pharmaceutical R&D has been on single drug targets, which are typically proteins that appear to play a role in disease pathogenesis. Such target-based screening platforms also fit well into high throughput screening strategies, very potent and selective compounds can often be found and specific chemical and molecular knowledge can be applied to modify the



**Fig. 14: Impact of MPS-based models on drug discovery screening strategies**

A model of how to transform drug discovery screening strategies by including disease mimicking multi-organ system approaches and tools. The model can be used to analyze and unravel disease mechanisms and define treatment interventions.

chemical entities. However, the low success rates in clinical trials indicate that different preclinical strategies are needed that focus on clinically relevant biological pathways. Swinney and Anthony (2011) analyzed R&D productivity, especially for innovative medicines including new molecular entities and new biologics approved by the US FDA between 1999 and 2008. The majority of approved *first-in-class* small molecules came primarily from phenotypic screening in animal models and not from target-based approaches. One major reason why the reductionist screening strategies using a single receptor/protein often fail could be that most diseases are multifactorial events with a systemic impact on many organs and, consequently, a response needs to be observed at the level of an intact organ and its interaction with the other organs in the pathophysiological context.

There is, thus, an urgent need to develop preclinical assays that translate more effectively into clinical effects in patients with a specific disease. Metabolic syndrome is a good example of a multi-factorial and multi-organ disease collecting a number of risks associated with cardiovascular disease and diabetes. Metabolic syndrome is becoming increasingly common, largely as a result of the increased prevalence of obesity. It is an insidious and progressive disorder that can culminate in type 2 diabetes, which carries a high risk of cardiovascular disorders and is also prevalent in patients with chronic kidney diseases. There are no approved drugs that can reliably reduce all the metabolic risk factors. To avoid the problem of polypharmacy, these patients would be helped with drugs that target several or all risk factors with single therapies. A human relevant preclinical MPS-based multi-organ model useful for a disease such as metabolic syndrome is urgently needed due to the low predictive power of animal models in the field (Aleixandre de Artinino and

Miguel Castro, 2009). It needs to incorporate the key organs, such as pancreas, liver, adipose tissue, muscle vasculature and the kidney. In such a model, the key steps in the progression of the disease from abdominal obesity and insulin resistance to type 2 diabetes and diabetic complications could be investigated. The model could be built up using healthy tissues from which the progression of metabolic disorder can be studied by, for example, medium, nutritional or hormonal manipulation. Another strategy would be to use tissues or cells from diseased subjects. Such a model could be used to unravel new biological pathways and targets and their clinical relevance at various stages of disease progression in the model. The ultimate aim for MPS in drug development is to recapitulate the various stages of a disease and understand the stages before the disease is clinically manifested, which may open the way to new treatment paradigms.

The optimization of drug candidates can include target-based screening if a specific target has been selected. The optimized compound can then be investigated in the disease model for treatment effects. Eventually the selected compounds can be evaluated in the disease model and an *in vitro* dose-finding study to guide the clinical program. This strategy integrates early drug discovery and translational discovery. In addition to treatment effects in a disease-relevant model, the MPS-based model can also be used to investigate useful *in vivo* treatment biomarkers.

The multi-organ model can use either material from diseased individuals or the disease can be induced in the system. The disease pathogenesis can be investigated and biological networks unraveled by using the latest multi-parameter read-out technologies and bioinformatics. The insight into the disease pathology at the molecular level can indicate whether a single target approach or a more complex strategy pursuing multiple targets is warranted. Bioinformatics and conventional structural biology tools combined with cheminformatics and computational analysis can guide the choice of intervention and aid in identifying the types of chemistry needed for pathway perturbation. A schematic overview of a possible patient-centered drug discovery model using the MOC as a focal point to evaluate intervention strategies, evaluate targets and for dose setting is described in Figure 14.

Another important opportunity for advanced multi-organ MPS in current pharmaceutical new drug candidate assessment is combined toxicity and efficacy testing in the oncology space. After the identification of a valuable cancer target, compound libraries are screened for inhibitors (or sometimes activators) of this target. Subsequently, compounds which have passed this first step are tested for *in vitro* efficacy by determining the inhibitory effect of these so-called hits on tumor cell lines. In a next step, compounds with promising *in vitro* inhibitory potential and an acceptable pharmacokinetic profile are administered to tumor-bearing rodents. During these early phases, safety aspects can be investigated in non-cancer cell lines or primary cell cultures (Tab. 2). The endpoints in these *in vitro* toxicity assays are rather simple and determine the inhibition of proliferation in short-term assays lasting from 24 to 72 h, for example, in cultures of proliferating keratinocytes (HaCaT(p)) or overt cytotoxicity in non-proliferating cells (HaCaT(q)). Primary rat hepatocytes are frequently used

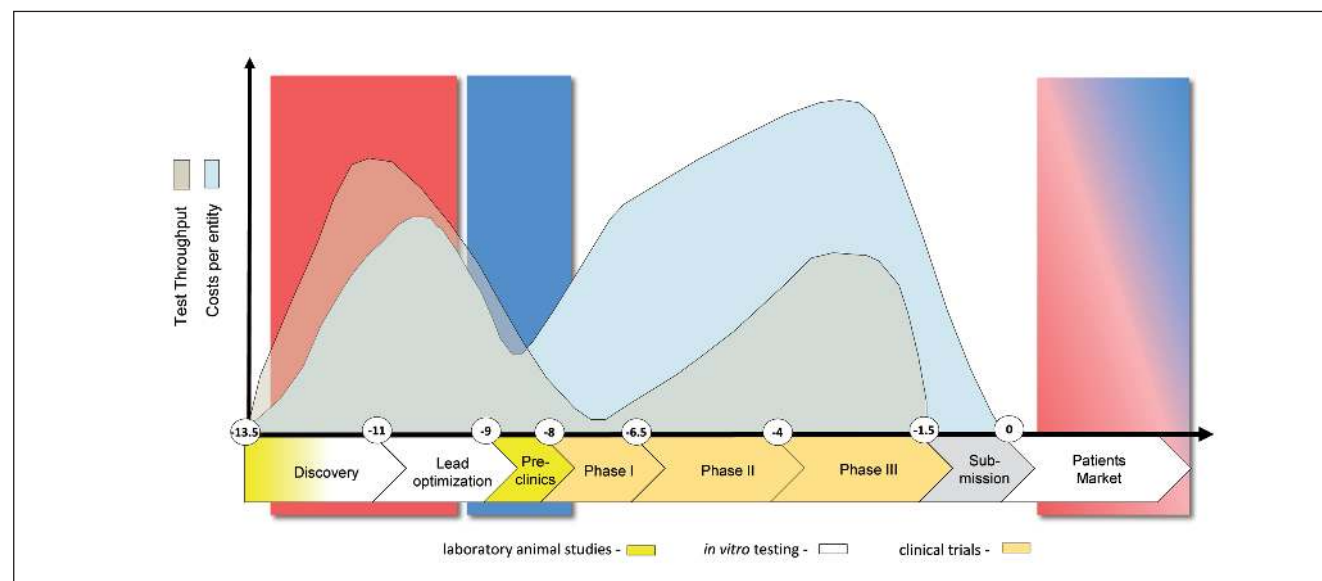
**Tab. 2: Illustration of a conventional early *in vitro* safety assessment of oncology drug candidates**

The test compounds are tested in three different safety screens and the results are compared to the results of the tumor cell line inhibition (Hepas: primary rat hepatocytes; HaCaT: human keratinocytes, non-proliferating quiescent (q) or proliferating (p)). Efficacy of both compounds is in the same range; compound 2 is ranked as critical (category 2) because of its cytotoxicity in a non-proliferating cell at concentrations less than 10-fold above the effective concentrations.

Assay	HaCaT(p) 4 h, MTT IC <sub>50</sub> (μM)	HaCaT(p) 72 h, MTT IC <sub>50</sub> (μM)	HaCaT(q) 72 h, MTT IC <sub>50</sub> (μM)	Hepas 24 h, MTT IC <sub>50</sub> (μM)	HeLa growth inhibition EC <sub>50</sub> (μM)	Category
Compound 1	~87	<1	~74	>100	2.8	1
Compound 2	10	<1	4.3	6.1	3.0	2
Endpoint	Acute cytotoxicity	Anti-proliferative	Cytotoxicity (resting cells)	Cytotoxicity (metabolically competent cells)	Effect on tumor cells (efficacy)	

in order to reflect the potential metabolism of a compound. Such an isolated *in vitro* test battery is able to identify those compounds which lack specificity towards the tumor target by comparing the EC<sub>50</sub> obtained in the tumor cell line test with the cytotoxic concentrations in the quiescent culture or the IC<sub>50</sub> in the proliferating non-cancer cell. An IC<sub>50</sub> in the range of the EC<sub>50</sub> clearly indicates that the specificity to the tumor target is too low and adverse effects on healthy, particularly on proliferating tissues have to be expected in patients. In Table 2, Compound 2 shows cytotoxicity in a non-proliferating cell at concentrations less than 10x above the effective concentrations, as determined in HeLa cells, and is, therefore, regarded

as problematic. Compound 1 is less toxic towards non-proliferating cells, but still shows anti-proliferative effects at a concentration lower than the EC<sub>50</sub>, and HeLa cells are also inhibited, i.e., the anti-proliferative specificity of this compound is questionable. However, this comparative approach is not able to reflect effects which might be caused by the interaction between the tumor and healthy tissues, as it occurs in the whole organism. In addition, effects which are elicited only upon chronic exposure cannot be depicted due to the short-term nature of the test systems described. It would, therefore, be desirable to obtain an MPS where cancer cells could be cultivated over several days or even weeks as spheroids and co-cultured


**Fig. 15: Target segments of various categories of MPS along the drug development cycle**

Single-organ systems are envisioned to add significant value from target selection toward lead optimization (red box) with plate-based systems serving primarily the high throughput demand of earlier discovery and chip-based systems serving primarily the demand of lead identification and early lead optimization. Multi-organ systems are intended to enable predictive measurements in the late lead optimization phase and early preclinical evaluation (blue box). All categories of MPS might add relevant data to the post-approval extension or restriction of indication to specific genotypic subpopulations (red-blue box). The vertical axis illustrates approximate numbers of tests performed (grey) and related spending (blue). The horizontal axis illustrates the development time in years.



with a panel of non-cancer organoids, such as liver, heart, skin and/or kidney, raised from human cells or tissue explants. Such a model would allow determining both efficacy and first safety parameters in just one system. In addition, it would be able to reflect changes in the microenvironment and display the effect of drug metabolites on both healthy and cancerous tissue. In theory, such a model residing on human material should also offer a better translatability of the effects observed to the clinical situation both in terms of safety and efficacy.

In summary, MPS could be used in the pharma industry as screening tools for both efficacy and toxicity testing of new chemical or biological molecules. The resulting test information can contribute to the selection of targets and lead structures, as well as to prioritize and select drug candidates for further development. Scientific information or data arising from such assays may also be used for internal decision-making and guidance in the course of the development process. In addition, as part of mechanistic investigations, it may also be attached as supplementary state-of-the-art scientific information to Investigational Medicinal Product Dossier and/or Investigational New Drug Application documentation. Figure 15 illustrates the potential application segments for single- or multi-organ systems within the drug development life cycle.

Single-organ systems are envisioned to add significant value in earlier phases at higher throughput, whilst multi-organ systems would enable predictive measurements at a later preclinical stage. The latter could provide more systemic *in vivo*-like assays where the therapeutic impact is more readily translated. However, a disadvantage is the challenge to optimize the molecular properties of candidate drugs without the design parameters provided by the exact knowledge of the target(s) and the lower throughput. Although preclinical discovery and qualitative clinical data generation will become the prime application of MPS-based tools, their use for post-approval evaluation could be of further added value. MPS-based tools bear the potential to compete with animal models in early discovery and the preclinical stage in the future. It may also be possible to use information from MPS testing throughout the entire drug development process, even during clinical development. Finally, during this process, mechanistic information on findings may support clinical use. Notably, the pharmaceutical industry will only adopt such systems when compelling data has shown that MPS-based tools provide a clear added value, for example, in the areas of unmet needs. Subsequent validation of MPS-based tools will be essential for complete adoption within the entire pharmaceutical industry. Information on a validation strategy for MPS-based tools is provided in Chapter 6 of this report.

### 3.2 Chemical and cosmetics industries – how MPS can make a difference

Substance testing in chemical and consumer products, e.g., the cosmetics industry, aims at the identification of any hazard potential a substance might entail for humans. In contrast to the pharmaceutical industry, where a risk-benefit analysis may lead to the acceptance of a certain drug toxicity level of a candidate drug if its efficacy benefit for the patient outweighs the safety downsides, the regulatory requirements for chemicals and con-

sumer products do not accept any meaningful hazard potential of substances used for humans.

Often it is skin that these substances are exposed to. Contact with the skin is either wanted or inevitable for many daily life products, such as cosmetics, household products, perfumes, volatile organic compounds and fertilizers. Tests and strategies have been developed and validated for the *in vitro* assessment of skin irritation, corrosion and penetration. The risk of skin sensitization towards specific components and, consequently, allergic responses to products is another important toxicological concern. Allergic responses to consumer products can be explained by occupational skin sensitization, cross-reactivity towards structurally similar antigens, interindustry use of ingredients and sensitization of customers by the product itself.

Animal test methods, such as the Local Lymph Node Assay (LLNA, Gerberick et al., 2007a) and the Guinea Pig Maximization Test (Basketter and Scholes, 1992), have been the gold standards and enabled risk assessors to identify both the hazard potential and the potency of a compound, the latter parameter referring to the concentration range sufficient to evoke skin sensitization. The respective OECD guideline for skin sensitization testing is number 406 (OECD, 1992). By complementing this information with additional read-across information and exposure scenarios, risk assessors were able to make judgments on safe concentrations of specific compounds in the final product. In order to minimize risk, default safety factors are applied to give consideration to the interspecies differences in penetration, metabolism and immunology, as well as the inherent fallibility of toxicity testing (Basketter et al., 2015; Dean et al., 2001).

The cosmetics and fragrance industry is particularly challenged due to European Commission Regulation (EU) 1223/2009 (EC, 2009), also called the European cosmetics directive (Hartung, 2008) and, consequently, is very active in the field of non-animal skin sensitization assessment. The chemical industry is also actively working on strategies for *in vitro* skin sensitization testing, aiming to avoid unnecessary reassessment of chemicals due to the Registration, Evaluation, Authorisation and Restrictions of Chemicals (REACH) regulation (Rovida and Hartung, 2009; Hartung and Rovida, 2009). The legal framework for human risk assessment for chemicals in the EU is detailed in Chapter 5.5 of this report (Hartung, 2010a). Here, we focus on test standards for hazard potential identification in skin.

In the field of skin sensitization, the European animal testing ban for cosmetic products and ingredients spurred the development of a multitude of *in vitro* assays and, in parallel, strategies to facilitate the development and validation of such methods for regulatory acceptance (Basketter et al., 2012, 2015; Leist et al., 2014). Activities in this field are intellectually and financially supported by associations such as Cosmetics Europe and the Research Institute for Fragrance Materials (RIFM), as well as institutions such as the European Centre for the Validation of Alternative Methods (EURL-ECVAM), the Interagency Coordinating Committee on the Validation of Alternative Methods (IC-CVAM), the Centre for Alternatives to Animal Testing (CAAT) and the European Partnership for Alternative Approaches to Animal Testing (EPAA).

**Tab. 3: Examples for Integrated Testing Strategies and Integrated Approaches to Testing and Assessment**

Current *in vitro* skin sensitization assessment follows a pathophysiology-inspired chain of adverse effects from covalent binding to proteins to the immunogenic activation of dendritic cells. Several methods are used to integrate and interpret the corresponding complex *in vitro* information in combination with (Q)SAR methods for subsequent risk assessment.

IATA	(Q)SAR / <i>in silico</i> methods	Covalent binding to proteins	Keratinocyte response	Dendritic cell activation	Prediction model	Reference
P&G	TIMES-M, Bioavailability variables	DPRA	KeratinoSens	h-CLAT	Bayesian Network	Jaworska et al., 2013
Kao		DPRA	KeratinoSens	h-CLAT	Tiered system	Nukada et al., 2013
Shiseido	Molecular-orbital descriptors	DPRA	AREc32-cell-based assay	h-CLAT	artificial neural network (iSENS)	Tsujita-Inoue et al., 2014
BASF	OECD QSAR Toolbox	DPRA, SH Test	ARE/Nrf2-based cell activation assays (KeratinoSens, LuSens)	h-CLAT or mMUSST	2 of 3 approach	Bauch et al., 2012; Natsch et al., 2013
RIVM, Givaudan	DEREK, CAESAR, MultiCASE, OECD toolbox	DPRA	KeratinoSens or Gene signature assay	h-CLAT	Tiered strategy	van der Veen, 2013

The development of non-animal *in vitro* methods for skin sensitization benefited from extensive data gathered by academic and clinical research, enabling scientific insights into the complex mechanisms of sensitization. Four key steps in an adverse outcome pathway (AOP) for skin sensitization were identified and published by the OECD in 2012 (EC, 2012b): 1) covalent binding of compound to skin proteins, 2) activation of keratinocytes, 3) activation and migration of skin-residing dendritic cells (DCs) to the draining lymph nodes, and 4) DC-dependent, allergen-specific priming of naïve T-cells in the lymph node, resulting in T-cell proliferation and T-memory cell formation. These insights specified appropriate targets for *in vitro* methods and, in addition, suggested AOP-based testing strategies.

To date, EURL-ECVAM lists 18 skin sensitization testing options in different formal validation phases, most of them addressing single AOP events (<https://eurl-ecvam.jrc.ec.europa.eu/test-submission/ecvam-test-method-submissions-2008-2015>). Strategic approaches to systematically evaluate different non-animal testing options by comparing different assays also have been reported from the cosmetics industry (Reisinger et al., 2015). A recent major breakthrough for *in vitro* testing was the formal validation and regulatory acceptance of the direct peptide reactivity assay (DPRA; Gerberick et al., 2004, 2007b) and the KeratinoSens™ (Emter et al., 2010; Natsch et al., 2013) in 2015. Following endorsement by EURL ECVAM, OECD test guidelines were published for both assays (OECD TG 442C and OECD TG 442D, respectively). A third assay, the human cell line activation test (h-CLAT; Ashikaga et al., 2006), is currently rated as provisionally accepted by the OECD. The three assays conveniently encompass the first three AOP events; i) the DPRA assesses the haptenization of cysteine or lysine-containing artificial peptides; ii) the KeratinoSens™ analyzes the Nrf2-dependent stress response based on ARE promoter-driven

luciferase reporter gene expression in HaCat cells, and, iii) the hCLAT analyzes the activation of the dendritic-like cell line THP-1 based on the induction of CD54 and CD86 co-stimulatory cell surface markers. Examples for integrated testing strategies are provided in Table 3.

Though the DPRA, KeratinoSens™ and h-CLAT may be ahead in terms of validation, other alternative assays addressing similar endpoints are being actively advanced by method developers. The PPRA may introduce partial metabolism to peptide reactivity assessment to improve *in chemico* evaluation of pro-haptens (Gerberick et al., 2009), whereas the LuSens assay (Ramirez et al., 2014) and other Nrf-2-reporter cell line-based assays present alternatives to KeratinoSens™ testing. Regarding DC activation, several tests besides the h-CLAT exist, most prominently the Myeloid U937 Skin Sensitization Test (U-SENS, formerly known as “MUSST” assay, Ade et al., 2006), the Modified Myeloid U937 Skin Sensitisation Test (modified MUSST assay) and the Peripheral Blood Monocyte-derived Dendritic Cell assay (PBMDc, Reuter et al., 2011). Despite substantial efforts, the development of assays for the fourth AOP key event has not yet been successful. First promising steps towards a T cell-based assay were published recently (Richter et al., 2013). However, the complex “organ response” in the lymph node, where activated dendritic cells from the periphery present haptenized peptides to naïve T cells, thereby priming the biologically important proliferation of antigen-specific and skin-homing T effector and T memory cells, is difficult to emulate *in vitro* using suspension cell-based test designs.

There is general agreement that the results of the AOP-aligned tests are more complementary than exclusive (Basketter et al., 2015). However, the interpretation of testing results is challenging and the need for transparent and reproducible decision frameworks stimulated the generation of Integrated Testing





Strategies (ITS, Hartung et al., 2013b) and Integrated Approaches to Testing and Assessment (IATA, Tollefsen et al., 2014; Bal-Price et al., 2015). These strategies have been recently reviewed in a t<sup>4</sup> report on ITS for safety assessment (Rovida et al., 2015b). ITS, according to a perspicuous explanation by Jaworska and Hoffmann, represent a guiding framework for the generation of comprehensive, non-redundant *in vitro* data by means of a reasonable and logical combination of tests that cover relevant mechanistic steps (Jaworska and Hoffmann, 2010; Jaworska et al., 2010; Luechtefeld et al., 2015). For optimized risk assessment the comprehensive data generated by individual approaches should be interpreted according to thoroughly evaluated decision schemes and should consider applicability domains of individual assays as well as the consistency of assay results, especially if the ITS contains assays with partial mechanistic overlap.

The IATAs extend the ITS concept by strategically integrating and weighing all relevant data to inform regulatory decision on potential hazard and/or risk and/or the need for further targeted and, thus, minimal testing (Barroso, 2014). Information sources for IATAs are not restricted to *in vitro* results, but include physico-chemical data, *in silico* predictions and weight of evidence considerations. Several skin sensitization IATAs have been developed, often based on combinations of AOP-key event assays enriched by additional assays, e.g., for surface thiol concentration and toxicogenomics. Six IATAs were presented and discussed in a recent workshop organized by the EPAA and Cosmetics Europe. The ITS and IATA approaches generate highly complex data. Pragmatic approaches, such as the 2-of-3 concept (Bauch et al., 2012) are delivering promising results. Machine learning systems, such as Bayesian models, artificial neural networks and support vector machines have become valuable tools for establishing prediction models for hazard (and partially potency) information for specific compounds (Hirota et al., 2013; Jaworska et al., 2015; Tsujita-Inoue et al., 2015). Furthermore, those systems are able to refine and improve predictive parameters easily by virtue of extended training sets. However, it should be noted that the “black box” character of hidden layers in the computational models does not provide mechanistic insights for the ensuing risk assessment.

Though current IATA case studies for prediction of skin sensitization look promising, quantitative approaches for potency prediction have only recently begun to gain traction. Potency determination is a keystone in risk assessment and is still a major gap for most non-animal skin sensitization assessment strategies. While singular assays exist that aim to provide potency information, for example, the toxicogenomic-based Genomic Allergen Rapid Detection test (GARD; Johansson et al., 2013) and Sens-Is assay (Cottrez et al., 2015), IATA approaches are now also closing in to categorizing the potency of test compounds.

Three-dimensional skin models, such as MatTek's EpiDerm™, Henkel's Phenion® and SkinEthic's EpiSkin™, have proven to be valuable tools for toxicity testing and have been extensively reviewed in a recent t<sup>4</sup> report (Gordon et al., 2015). Characterization of skin models showed, in some cases, high similarity to skin metabolism *in vivo*. Though difficult, progress has been made in the creation of immune-competent skin models. In parallel, skin sensitization assays based on co-cultures

of HaCat cells and DCs were reported to show increased sensitivity towards pro-haptens, explained by increased metabolic capacity. Recent publications report on successful integration of dendritic-like Mutz-3 cells into skin models (Ouweland et al., 2011) and showed responsiveness towards irritants and sensitizers (Kosten et al., 2015).

In summary, promising advances have been made over the last few years in the field of skin sensitization assessment *in vitro*. The predictive parameters of current ITS and IATAs for hazard are comparable to, or even superior to, the gold standard LLNA. The AOP-based ITS and IATA strategies split the biological complexity of animal testing into practicable pieces. However, the corresponding pieces of information need to be assembled by complex computational models. In addition, the applicability of cell culture-based assays often can be restricted by compound solubility and application form. Only a few skin sensitization assays are based on skin models that can deal with water-insoluble compounds or formulations. Moreover, the metabolic capacity of the test system is important for the detection of pro-haptens and needs to be considered for the interpretation of results.

The potential of MPS for hazard identification and toxicity testing in this area has been recognized by consumer product industries and first feasibility studies are ongoing to evaluate the potential avenues of adoption of MPS by the industry segments. MPS may facilitate a comprehensive testing approach by integrating the four aforementioned biologically and AOP-relevant key events and multiple readouts in a single immunocompetent skin MPS. Skin explants or 3D skin models are suitable for topical application of compounds and, for example, cosmetic formulations. In addition, they would (partially) add bioavailability parameters that directly influence the skin sensitizing effect of a compound. Skin penetration of sensitizing compounds is probably not only determined by molecular weight and solubility, but also by chemical reactivity, which may result in absorption of a compound by, for example, stratum corneum proteins. First approaches to combine primary DCs and epidermal models in the microfluidic MOC platform described in Chapter 2.3 were carried out and revealed parameters that need to be adjusted for future successful integration of both cell types (unpublished data).

A further step towards MPS approaches integrating all relevant parameters would be the combination of immunocompetent human skin models with human lymph nodes in a two-organ chip. Such systems might allow the detection and quantification of lymph node responses towards topically applied chemicals, which in a way mirrors the readouts of the LLNA. Such MPS approaches have another advantage over testing strategies comprising several assays: Combinations of assays increase the overall sensitivity at the expense of false positive results. False positive results complicate not only the interpretation of inconsistent results, but also the previous generation of computational prediction models.

Apart from skin sensitization testing, the chemical testing landscape uses a broad repertoire of toxicity tests, again, historically primarily based on laboratory animal tests. There are possibilities to apply *in vitro* methods, but no accepted alternative methods are available yet for studies on systemic toxicity



(e.g., acute toxicity, repeated dose toxicity and reproduction toxicity). This is another unmet need in the domain of cosmetics in Europe, for which animal tests have been banned. As of yet, there have not been any applications for market admittance for cosmetics that are based entirely on alternative methods. Needless to say, there is a great demand for alternative methods for systemic toxicity testing for regulatory use.

Acute toxicity tests focus on organism death, an effect that cannot be easily mimicked with conventional static *in vitro* tests, as it can involve single-organ failure or interplay between organs. Current efforts to replace acute toxicity tests involve *in vitro* cytotoxicity tests with cell lines, such as the 3T3 NRU cytotoxicity assay, which need complementation with kinetic data and *in vitro* target organ assays (Prieto et al., 2013). Improved target organ models, such as the MPS models, in which cytotoxicity may also be analyzed, could improve the predictive value of these *in vitro* tests for acute toxicity. The potential of MPS to substantially improve kinetic measurement and systemic toxicity testing, described in Chapter 3.1 for pharmaceutical safety assessment, is generally equally applicable for chemicals and cosmetics testing of hazard potential. Thus, MPS tools described in Chapter 2.3 for kinetics (e.g., gut-on-a-chip; gut+liver-on-a-chip and gut+liver+skin+kidney-on-a-chip) are envisaged to add value for kinetic endpoints, as the different kinetic processes are reasonably separated with a different organ for each process. While the regulatory need for kinetic data does not seem large, according to Table 3 of this report, when using *in vitro* tests for hazard endpoints, the addition of kinetic data becomes essential in combination with *in vitro* tests or strategies. The reason is that kinetics are included in whole animal tests, but not in tests with only a small part of the organism, such as *in vitro* tests. Thus, kinetic data must be added to the result of an *in vitro* hazard test to make this result more predictive of an *in vivo* response. As outlined above, coupling MPS-based testing systems to physiologically based toxicokinetic modeling would be advisable. These models ideally allow an estimation of local substance and metabolite concentrations in different tissues and organs. Together with a given exposure, they can, thus, potentially identify target organs together with the relevant organ doses for subsequent testing *in vitro*. However, there is little experience with regard to the applicability and reliability of such a “tox-test dummy” (Tralau et al., 2012). In addition, the required data concerning substance absorption, distribution and metabolism is often not available (Caldwell et al., 2012). It would, thus, be warranted to conduct blinded pilot studies with established and already assessed substances before any routine use.

Finally, the achievement of stable functional homeostasis in MOCs combining human intestine, liver, skin and kidney equivalents over time frames of at least four weeks (Maschmeyer et al., 2015b) opens possibilities for MPS-based 28-day repeated dose testing, which, after improvement and validation, might become competitive with animal testing performed according to OECD guidelines 407, 410, 412 and 419 where appropriate. The human origin of MPS provides additional competitive advantages versus animal testing. When combined with AOPs, which connect early biochemical effects with clinical outcomes, and kinetic models, which can extrapolate accumulating doses,

responses seen in MPS could become predictive of ultimate toxicological endpoints after prolonged exposure. However, the difference between four weeks of culture and 90-day repeated dose testing or 1- or 2-year animal tests, which are required for certain toxicity evaluations in animals according to OECD guidelines 408, 411, 413 and 453, respectively, in geographies and segments where there is no ban, will still remain a significant technical challenge for MPS to overcome.

In summary, MPS-based advanced immunocompetent human skin models and their combination with human lymph nodes can have an extraordinary added value for hazard potential identification and potency assessment in the chemical and cosmetics industries. Moreover, human MOCs enabling stable physiological organ homeostasis and crosstalk of universal combinations of human organs over periods of 28 days and longer can mature towards valuable approaches for predictive systemic acute and repeated dose toxicity testing. In contrast to the pharmaceutical industry, where qualified assays can immediately improve the drug development process and internal decision-making, MPS-based assay adoption in the chemical and cosmetics industries requires much more formal validation effort prior to full industrial adoption. Information on a validation strategy for MPS-based tools is given in Chapter 6 of this report.

### 3.3 The tobacco industry, the human respiratory system and MPS approaches

The tobacco industry is under immense pressure to increase the safety of their product portfolio due to the proven high hazard potential of tobacco smoke for the human respiratory system. The US FDA Center for Tobacco Products (CTP) was set up in 2009 when the FDA was authorized to regulate the manufacture, marketing and distribution of cigarettes and smokeless tobacco products in the Family Smoking Prevention and Tobacco Control Act. The FDA recommends that applicants conduct nonclinical studies to address the known clinical toxicities of tobacco products and evaluate a range of potential toxicities of the product compared to other tobacco products on the market. Nonclinical toxicology studies should use methods that are sufficiently sensitive to assess the actual differences between the use of the product and the use of other tobacco products, or between the use of the product and the nonuse of tobacco products. Animal models are the industry standard to assess the effects of tobacco smoke on the respiratory system. Limitations associated with human or animal studies require alternative tools to align with the goals of the 21<sup>st</sup> century toxicology framework, and develop a “systems approach that fully integrates exposure and toxicity information in a holistic framework for improved public health decision-making” (Sheldon and Cohen Hubel, 2009). The FDA noted commitment to the three Rs and the inclusion of “modernizing toxicology” as one of the priority areas to address (FDA, 2011a) and, thus, has expressed interest in learning of current assays that could meet their goals (IMNA, 2012).

In addition to the regulatory aspects, the industry’s efforts to develop new approaches and tools for assessment of smoke-related adverse effects on the human respiratory system are driven by ethical considerations and the aim of developing safer products. Tobacco smoke primarily targets airways and alveoli in the lung.



Gordon et al. (2015) provide a comprehensive recent review on *in vitro* lung models. Another recent review by Manuppello and Sullivan (2015) specifically emphasizes the technological advances in the *in vitro* assessment of tobacco products, including reconstituted human lung tissue cultures that allow exposure at the air-liquid interface (ALI) to test the toxicity of tobacco smoke, E-cigarette aerosols, constituents and particulates. The community of experts from industry and academia together with regulatory stakeholders are currently working on addressing the challenges pertaining to the standardization of methods and endpoints for the new *in vitro* toxicity testing approaches.

Existing *in vitro* models to study the biological impact of inhaled toxicants on cells of the human airway epithelia are currently based on 2D or 3D cell culture systems. Some of the drawbacks of using epithelial cell lines for *in vitro* toxicity studies include a limited metabolic competency, which may affect their responsiveness to toxic stimuli (Garcia-Canton et al., 2013), and an absence or reduced formation of tight junctions or refractoriness to differentiation (Stewart et al., 2012). One of the most suitable *in vitro* models to characterize the impact of inhaled toxicants in current use is the 3D culture system, where fully differentiated primary epithelial cells grow at the ALI. This model system features the full cellular complexity of a pseudo-stratified epithelium found in human airways, containing ciliated/non-ciliated epithelial cells and basal (progenitor) cells (Prytherch et al., 2011). Furthermore, it resembles epithelial functionality most closely by apical mucus secretion, expression of ion channels and the presence of tight junctions, which warrant biological barrier function (BéruBé et al., 2009). Despite the fact that 3D cell cultures resemble the native tissue closely, they usually lack cellular components of the immune system; a gap that is being addressed by a number of systems which combine the co-culturing of immune cells with epithelial cell layers as well as utilizing ALI conditions (Klein et al., 2013). A static system comprising three cell types: epithelial cells, human blood monocyte-derived macrophages and DCs was designed as an *in vitro* model of the alveolar wall to examine the physiological responses of these cells to environmental particles (Lehmann et al., 2011; Rothen-Rutishauser et al., 2008). It was used to examine the role of surfactant protein D in modulating allergen particle uptake and inflammatory responses (Schleh et al., 2012), and the physiological effects and uptake of gold nanoparticles (Brandenberger et al., 2010). In these systems, the investigators used A549 cells, a lung adenocarcinoma cell line that may not be representative of healthy epithelial cells.

An urgent unmet need for the tobacco industry is an approach to investigate the onset of lung diseases. Smoking induces chronic obstructive pulmonary disease (COPD) and accounts for as many as 8 out of 10 COPD-related deaths in the US (DHHS, 2014). The title COPD refers to a group of diseases that cause airflow blockage and breathing-related problems: COPD includes emphysema, chronic bronchitis and, in some cases, asthma. With COPD, less air flows through the airways because of the destruction of alveoli, inflammation of airways, increased excretion of mucus in the airways and loss of the ability of the lung tissue to stretch and shrink. Modeling such complex behavior of the human lungs is impossible in the static *in vitro*

lung models described above. The MPS-based lung-on-a-chip model systems, outlined in detail in Chapter 2.2 of this report, resemble additional aspects of the human respiratory tract, such as the mechanobiology of breathing (Huh et al., 2010; Stucki et al., 2015) and, therefore, provide great opportunities to model aspects of COPD, investigating toxicity-induced lung injury and repair following exposure to smoke. As outlined in Chapter 2.2, a model for chemotherapy-induced pulmonary edema has already been developed on the basis of a small-airway-on-a-chip model (Benam et al., 2015b), which contains a differentiated, mucociliary bronchiolar epithelium and an underlying microvascular endothelium that experiences fluid flow. This allows the analysis of organ-level lung pathophysiology *in vitro* with culture times of 4 to 6 weeks. Exposure of the epithelium to interleukin 13 reconstituted the goblet cell hyperplasia, cytokine hypersecretion and decreased ciliary function of asthmatics. Small airway chips lined with epithelial cells from individuals with COPD recapitulated features of the disease, such as selective cytokine hypersecretion, increased neutrophil recruitment and clinical exacerbation by exposure to viral and bacterial infections. The improvement of such a model towards smoke-induced pulmonary edema might be one avenue for MPS-based assay adoption by the tobacco industry.

Another aspect of smoke-induced disease onset is malignant transformation. First single-organ MPS developments are focusing on the malignant transformation of bronchial epithelial cells due to tobacco (Li et al., 2014b). A single-organ MPS has been applied to investigate the role of macrophages in promoting benzopyrene (BaP)-induced malignant transformation of human bronchial epithelial cells in comparison to animal models. The MPS data showed that macrophages promote BaP-induced malignant transformation of human bronchial epithelial cells, which was mediated by nuclear factor (NF)- $\kappa$ B and STAT3 pathways to induce cell proliferation, colony formation in chip culture and tumorigenicity in nude mice. Blockage of interleukin 6 or tumor necrosis factor  $\alpha$  signaling or inhibition of NF- $\kappa$ B, STAT3 or cyclinD1 expression abrogated the effect of macrophages on malignant transformation in the lung airway chip, which was in line with results obtained in comparable induction experiments in animals. This indicates that MPS-based lung models are capable of modeling key molecular events involved in COPD progression in humans and makes MPS-based lung models an attractive target for industrial adoption by the tobacco industry.

Finally, onset of both chronic obstructive and malignant disease in human lung is intimately related to the entire organismal homeostasis. Uptake of smoke-induced substances by the liver, lymph node-based immunological responses toward the induced tumor cells and interactions of the diseased lung with the cardiovascular system requires more complex multi-organ systems. The potential of MOCs to provide tools for systemic lung+X (e.g., X = liver or lymph node) on-chip assays is of high interest to the industry. Adoption of MPS-based assays by the tobacco industry needs robust qualification, but does not need regulatory acceptance yet. Value-adding MPS-based tools and approaches, once qualified, can immediately be used for internal decision-making in product development.

## 4 Initiatives to advance MPS developments into human body-on-a-chip solutions

### 4.1 Human body-on-a-chip – a courageous promise to reduce animal testing and solve unmet needs

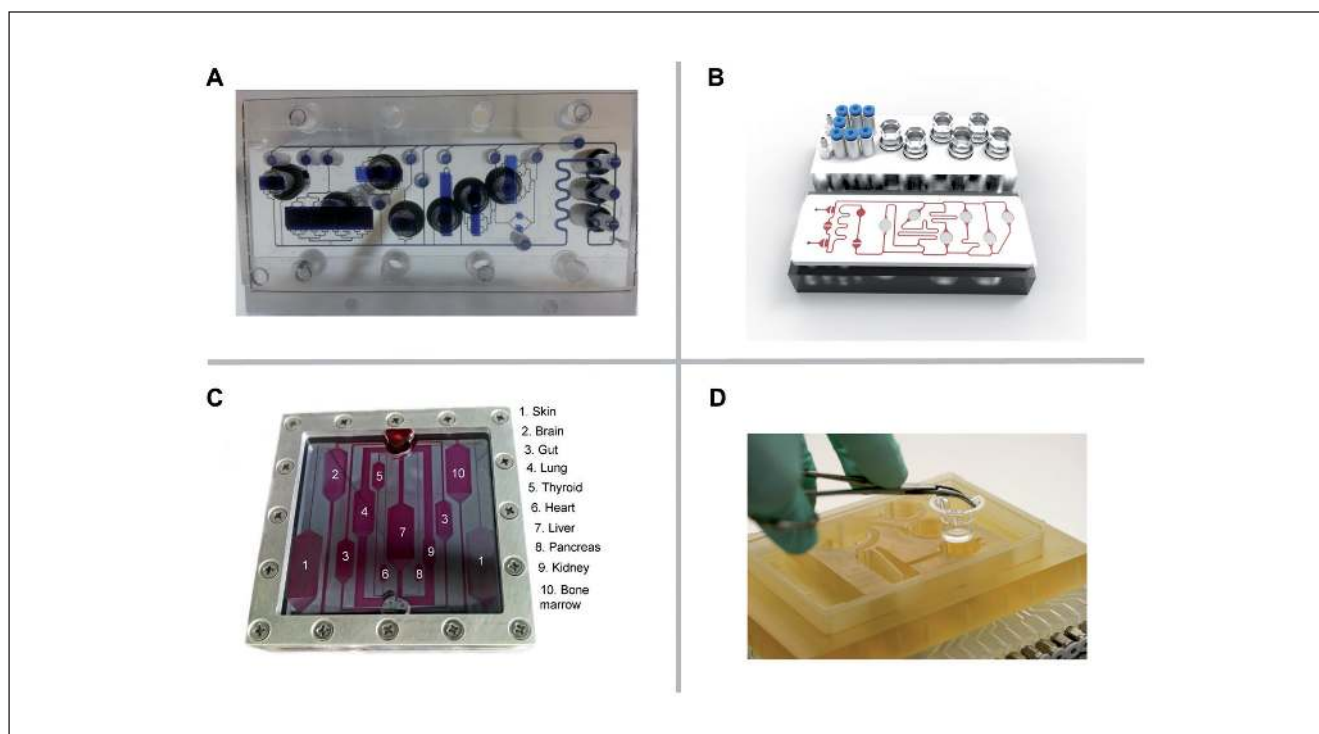
We have reported the *status quo* and potential for the adoption of MPS emulating human single- and multi-organ models in different industries. These MPS may contribute to the reduction of laboratory animal testing methods due to the early effective elimination of toxic drug candidates from further testing and better preselection of effective drugs. However, these types of MPS are incapable of emulating human biology at an entire organismal level. Some research groups have advanced their MPS platforms towards concepts to emulate a functional human-like mini-organism *in vitro* (Hartung and Zurlo, 2012), i.e., human-on-a-chip or body-on-a-chip approaches. First prototypes (Fig. 16) are in experimental evaluation. Current human body-on-a-chip developments focus on the emulation of non-pregnant adulthood, as this time span has the largest numeric relevance for safety and efficacy testing in humans. It is postulated that organs from at least the following ten systems should be interconnected in a biological manner to gain minimal human

organismal homeostasis *in vitro*: circulatory, endocrine, gastrointestinal, immune, integumentary, musculoskeletal, nervous, reproductive, respiratory and urinary.

With regard to the scale of chip-based organisms, the first approaches towards a biologically representative scale-down of human organs have been published (Marx et al., 2012; Moraes et al., 2013; Wikswow et al., 2013). In the following, we glance at the most prominent initiatives, all at a very early stage, aiming at human body-on-a-chip solutions. The initiatives are highlighted in the chronological order of their inception.

### 4.2 March 2010 – the German multi-organ chip GO-Bio initiative

The German human-on-a-chip initiative was launched under a GO-Bio grant from the German Federal Ministry of Education and Research in March 2010. The grant was awarded to Uwe Marx's group at the Technical University Berlin, in collaboration with its spinoff TissUse GmbH, and the Fraunhofer IWS in Dresden and the Fraunhofer IGB in Stuttgart. This initiative represented a reduced biphasic version of a larger VAMOS grant proposal to develop a human-on-a-chip platform under the FP7 Health 2010 Program on alternatives to laboratory animals aiming at the development of *in vitro* solutions for



**Fig. 16: First prototypes towards a human body-on-a-chip**

Images illustrate four MPS prototypes in experimental evaluation aiming to advance multi-organ systems into miniature organisms on a chip. (A) The German “GO-Bio-MOC” program-derived 10-organ prototype of TissUse GmbH, Germany (courtesy of TissUse GmbH, Germany); (B) The Russian “Homunculus” program-derived 6-organ prototype design of Bioclinicum, Russia (courtesy of Bioclinicum, Russia); (C) The US 10-organ prototype of Cornell University, USA (courtesy of Cornell University, USA); and (D) a US 4-way PhysioMimetics prototype of the Human Physiome on a Chip Program, MIT, USA (courtesy of MIT, USA), developed within the framework of the US NIH/DARPA/FDA MPS initiative.



systemic substance testing at a European level; the VAMOS proposal was not funded. The eight-year goal of the German GO-Bio program is the development of a human body-on-a-chip consisting of a relevant number of organs to allow for self-contained organismal long-term homeostasis. This includes the chip-based utilization of physiological organ functions for functional maintenance of the human body-on-a-chip: the intestine absorbing digested food, the liver supplying albumin for all organs and metabolizing xenobiotics, the bone marrow realizing adequate hematopoiesis for the mini-organism, the lung providing oxygen through red blood cells to each organ, the kidney excreting waste products from blood plasma, the immune system guarding health status, etc. The final human body-on-a-chip platform should be able to emulate the key pathophysiological behavior of patient groups in clinical trials. A first five-year period with an investment of about 6.1 million € was dedicated to establishing a MOC platform capable of hosting a relevant number of organs for such a human-on-a-chip solution; an organ miniaturization algorithm that reflects the organoid structure of a human was applied. A “man-on-a-chip” at 0.00001 scale, which fitted the format of a microscopic slide, was designed (Marx et al., 2012).

A first proof of concept milestone was reached in 2013 when a reproducible 28-day co-culture of human 3D liver and skin model equivalents and long-term repeated dose substance exposure could be established in a two-organ version of the MOC platform (Wagner et al., 2013). Subsequently, the second milestone – human two-organ chip vasculature – was reached (Schimek et al., 2013). Results and further platform improvements towards a four-organ ADMET chip for long-term testing (Maschmeyer et al., 2015b) are described in Chapter 2.3.3 of this report. Since the market launch of the two-organ chip in 2013, a number of successful industrial feasibility studies have proved the commercial viability of the concept, which was the last milestone of the first phase.

The second phase, a three-year program at TissUse GmbH under the auspices of the GO-Bio grant (031B0062) dedicated to providing the proof of concept for a human body-on-a-chip solution was initiated in 2015 and continues until 2018. The researchers’ “man-on-a-chip” design is illustrated in a video (<http://www.tissuse.com/technology.html>) and has recently been converted into a first chip prototype of a mini-organism (Fig. 16A), which is now under evaluation.

#### 4.3 October 2011 – the Russian “Homunculus” program

The Russian Ministry of Education and Science launched a program aiming at the development of an organ-on-a-chip and human-on-a-chip technology in October 2011. Dmitri Sakharov and his team at the Scientific Research Center “Bioclinicum” in Moscow were awarded a grant from the Russian Ministry of Education and Sciences and the Ministry of Production and Trade for platform development, totaling 5.7 million €. The resulting “Homunculus” microbioreactor is an MPS platform that provides prolonged cell culture viability *in vitro* and emulates physiological processes (Senyavina et

al., 2013). The system includes a control unit connected to a maximum of four microfluidic chips. The disposable microchip is designed for co-culturing of up to six cell micromodels in a single closed circuit with automatic medium exchange (Samatov et al., 2015). The system is adapted for the cultivation of cellular monolayers in standard transwell inserts, chip vascularization by seeding cells in the microchannels or work with any other cellular objects, including 3D models and human tissue samples in cell chambers. The chip contains a peristaltic micropump and cell culture wells connected by microchannels with circulating culture medium. The microfluidic channels imitate blood vessels. The control unit sustains the desired temperature of the chip and provides constant circulation of culture medium, allowing the variation of pressure on the micropump valves and their switching frequency. The chip construction allows the integration of various sensors to monitor cell culture parameters in real-time mode: cover-embedded electrodes provide the impedance-based measurement of barrier models during cultivation. The microscopic glass at the bottom of the chip allows noninvasive cell viability observation using fluorescent vital dyes and optical fibers (Sergachev et al., 2013). The microcirculation introduces convective mass transfer to the cellular microenvironment, which mimics physiological conditions, accelerating transport fluxes of nutrients and metabolites in comparison to mass transfer limited to diffusion in static culture. Thus, the predicted permeability values become more accurate. Various microcirculation regimes promote *in vivo*-like mechanical influences, including physiological values of shear stress and interstitial pressure.

The Homunculus device is commercialized by Bioclinicum and is currently passing national registration for medical use to certify the *in vitro* trials of drugs and chemical compounds with regard to bioavailability, biotransformation and drug-drug interaction on specialized cellular models. The Homunculus shall be used to determine dose-dependent and integrated toxicity of chemical compounds to target cells, given the toxicity of the metabolites produced in human liver. The danger class of hazardous chemical waste and mixtures thereof can be determined using this device applied to environmental monitoring, and sanitary and hygiene regulation. The six-organ chip prototype, as shown in Figure 16B, is currently in experimental evaluation.

#### 4.4 March 2012 – the European “Body on a chip” consortium

In March 2012, a “Body on a chip” consortium consisting of four European sites ([http://cordis.europa.eu/project/rcn/104027\\_en.html](http://cordis.europa.eu/project/rcn/104027_en.html)) was awarded 1.4 million € by the EC for a body-on-a-chip development under a 7<sup>th</sup> FP FET Open project (STREP #296257) and included InSphero AG, Switzerland, ETH Zurich, Switzerland, KU Leuven, Belgium, Technical University Dortmund, Germany, and Astra Zeneca Pharmaceuticals, UK. The “Body on a chip” consortium directive was to create a comprehensive, next-generation *in vitro* drug-testing device which interconnects multi-organ tissue models to identify toxicity and/or decreased efficacy due to metabolic activity ([300](http://www.in-</a></p>
</div>
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sphero.com/company/eu-project-the-body-on-a-chip). The partnership developed a plate-based multi-tissue device within a timeframe of three years (Kim et al., 2015a,b; Frey et al., 2014) which is described in Chapter 2.3.3.

#### **4.5 June 2012 – the US NIH/DARPA/FDA Microphysiological (Tissues-on-a-chip) Systems program**

The NIH National Center for Advancing Translational Sciences (NCATS)/DARPA/FDA Microphysiological Systems collaboration, which started in 2011, was initiated to support the development of human microsystems, or organ chips, to screen for safe and effective drugs more swiftly and efficiently than current methods. NCATS and DARPA, in coordination with the FDA, solicited proposals from industry, government labs, academic institutions and other research organizations on how best to develop the chip by bringing the latest advances in engineering, biology and toxicology to bear on this complex problem. A joint NIH/DARPA/FDA tissue-on-a-chip five-year program at a total of around \$140 million was launched in June 2012. The DARPA awarded two contracts, one to Donald Ingber's group at the Wyss Institute for Biologically Inspired Engineering at Harvard University, Boston, and one to the Human Physiome on a Chip program led by Linda Griffith at MIT, Cambridge, for the development of engineering platforms and biological proof-of-principle for a human body-on-a-chip. Each research team was required to develop a human body-on-a-chip with the following characteristics: (1) reconfigurable platform; (2) ten or more *in vitro* physiological systems; (3) ability to monitor resident tissues for up to 4 weeks; (4) uses human cells; (5) commercial availability; and (6) includes plan for validating integrated platform performance. Concurrently, NCATS awarded several grants in two complimentary areas: (1) Stem/Progenitor Cell Grants to develop stem- and progenitor-derived cell resources to seed circulatory, endocrine, gastrointestinal, immune, integumentary, musculoskeletal, nervous (including eye), reproductive, respiratory and urinary microsystems, and (2) Integrated Microphysiological Systems for Drug Efficacy and Toxicity Grants to develop *in vitro* microphysiological systems representative of major organs/tissues in the human body that will facilitate the assessment of biomarkers, bioavailability, efficacy and toxicity of therapeutic agents prior to clinical trials. Throughout the five-year research plan, NCATS, FDA and DARPA meet biannually with all the researchers to ensure progress and collaboration for all the projects. Moreover, through this program, the development of well characterized multicellular models that represent the disease pathogenesis, cellular diversity, genomic complexity, sex, microenvironment and functional output of human organ systems is being supported. Essential characteristics of advanced multicellular models of human physiology should include all of the following features:

- Multicellular architecture that represents characteristics of the target tissue;
- Functional representation of normal human physiology;
- 3D culture modeling of multicellular microenvironments;
- Reproducible and viable operation under physiological conditions maintained up to four weeks in culture;

- Representation of normal and disease phenotypes;
- Representation of population diversity; and
- Use of patient-derived cell lines where patient consent allows commercialization and broad sharing of cells and cellular derivatives with academic and industry researchers.

A critical challenge in engineering an integrated network of microsystems will be the ability to develop and assemble 3D tissue modules that are physiologically relevant, reproducible and compatible with high content screening platforms that include multiple molecular readouts, such as gene expression, proteomic, metabolomic or epigenomic analyses. The *in vitro* microsystems should provide spatial and temporal control of the cellular microenvironment, while enabling continuous monitoring (sensing), probing (direct in-cell measurements) and sampling (testing and continuous data collection and analysis) of the system in a nondestructive, real-time and label-free assay. The integrated platform should ideally support a network of microsystems that can monitor epithelial and endothelial barrier functions, exposure to environmental and infectious agents, and absorption and metabolism of drugs in real-time and at high resolution inflammatory responses. Platform challenges include: 1) ease of use and portability; 2) cost-effective designs; 3) optimization of the full range of possible physiological functions in each organ system; 4) replacement of PDMS with materials that do not absorb/bind hydrophobic molecules and exhibit physiologically relevant stiffness; 5) implementation of iPS-derived cells, when possible, to harness heterogeneities of responses in humans; 6) increase throughput with automation; 7) creation of an integrated set of organ systems with physiological flow, shear, optimal metabolic scaling between organ systems, and spatiotemporal scaling (adult male ~ 4.5 liters of blood; 4.5  $\mu$ l for  $\mu$ Human); 8) integration of dynamic mechanical, chemical and electrical cues including key contributions of missing organ systems; 9) optimization of analytical chemistry in nl to  $\mu$ l volumes for pH, O<sub>2</sub> and glucose; 10) implementation of a combination of real-time biosensors of key cell functions; 11) implementation of a universal medium with medium to cell ratios reflecting physiological values; 12) implementation of designs with minimal dead volumes in tubing and reservoirs; 13) implementation of an MPS database for integrated systems; 14) development of modeling methods to harness the rich datasets; and 15) integration of disease models. A draft summary of the human body-on-a-chip programs within the US initiative was provided recently (Dance, 2015).

Figure 16 shows the MPS-based human “body-on-a-chip” prototypes currently evaluated in the US: one of them in the lab of Michael Shuler at Cornell University (Ithaca, NY, Fig. 16C) and another one in the lab of Linda Griffith at the MIT (Cambridge, MA, Fig. 16D).

#### **4.6 February 2015 – the Netherlands Institute for Human Organ and Disease Model Technologies**

The Institute for Human Organ and Disease Model Technologies (hDMT) is a precompetitive non-profit technological R&D institute in the Netherlands. This institute, established on February 6, 2015, integrates state of the art human stem cell technologies with top level engineering and a variety of other expertise



from academia and industry to develop, implement and valorize human organ and disease models-on-a-chip. These miniature models in chip format closely mimic human tissue and organs *in vivo*. This will primarily meet the need of pharma, clinicians and society for representative human test model systems for drug development, and an active dialogue is encouraged to achieve this central aim. As an additional advantage, the use of animal experiments might be reduced. The hDMT researchers share their knowledge, expertise and facilities to develop the organ-on-chip models. A clinical expert team of medical specialists is also present. The Consortium aims at further expanding their expertise in MPS technologies. The current partners are the Leiden University and University Medical Centre, Erasmus Medical Centre in Rotterdam, the Hubrecht Institute in Utrecht, the three Universities of Technology (Twente, Eindhoven and Delft), and two companies – Genmab and Galapagos. The academic partners carry out the research and the private partners provide input on the validation and application of the models. The “scalability and manufacturability” of the MPS-technologies will also be addressed within the hDMT Institute. The hDMT will valorize the MPS-based models developed through technology and pharma companies both in The Netherlands and internationally. hDMT’s research projects fall within two research lines that reinforce and complement each other: development of innovative human organ and disease models, and development of organ-on-chip technology platforms. Four themes are currently prioritized in both healthy and disease format: vessels-on-a-chip, heart-on-a-chip, cancer-on-a-chip and brain-on-a-chip. Other models will be added in the near future, including immune system-on-a-chip, lifestyle models (skin and hair) and environmental models (nutrition and infection). All hDMT research programs are interdisciplinary programs to which each partner contributes with a specific technology focus embedded in ongoing research, clinical interest and expertise. For more information about the hDMT Institute, see <http://www.hDMT.technology>

#### 4.7 January 2016 – EU-ToxRisk – a H2020 project

EU-ToxRisk is a H2020-supported integrated European program developing new approaches for mechanism-based toxicity testing and risk assessment to achieve a paradigm shift in toxicology towards a more efficient and animal-free chemical safety assessment. An international consortium of 39 partner organizations – academia, small and medium-sized enterprises, large industry, contract research organizations and regulatory bodies – has been funded by the European Commission since January 2016 to work on the integration of new concepts for regulatory chemical safety assessment. The new approaches involve human-relevant *in vitro* non-animal methods, such as MPS-based approaches and *in silico* computational technologies, to translate molecular mechanistic understanding of toxicity into safety testing strategies. The ultimate goal is to deliver reliable, animal-free hazard and risk assessment of chemicals. The program is coordinated by Bob van de Water, Leiden University, The Netherlands. The project will integrate advancements in cell biology, omics technologies, systems biology and computational modeling to define the complex

chains of events that link chemical exposure to toxic outcome. The consortium will provide proof of concept for a new mechanism-based chemical safety testing strategy with a focus on repeated-dose systemic toxicity as well as developmental and reproductive toxicity. Importantly, novel mechanism-based test methods will be integrated in fit-for-purpose testing batteries that are in line with the regulatory framework and will meet industrial implementation.

## 5 Selected legal frameworks, regulatory science and acceptance criteria

### 5.1 General remarks

A stringent regulatory network of laws, regulations and guidelines currently covers substance development, registration and approval for all areas of potential use, such as medicine, food, agriculture, chemistry and cosmetics.

To the best of our knowledge, MPS-based test assays for the evaluation of substances have not yet been introduced into any regulatory assessment procedure in any country. This is due to the early development status at the research level and a lack of practical experience of both industry and regulatory bodies. However, experience and mutual acceptance are prerequisites for new technologies, as was experienced during the recent history of the ban of laboratory animal testing for the evaluation of cosmetics products and ingredients in the EU in 2013. The ban has thrown the global cosmetics industry into a dilemma: Cosmetics containing new ingredients tested on laboratory animals are no longer allowed to be sold in the EU, while the same cosmetics are prohibited from being sold in the rest of the world if they have not been tested on laboratory animals.

Two different approaches are being investigated to avoid a similar situation in drug development. Firstly, the FDA has launched a regulatory science-based approach, and the EU European Medicines Agency seems to be following their lead. Secondly, key academic and industrial players are actively disseminating the same approach to regulatory bodies in other countries, such as China and Russia.

At a regulatory science panel discussion at the 9<sup>th</sup> World Congress on Alternatives and Animal Use in the Life Sciences (WC9) in Prague, 2014, the representations of regulatory bodies from the US, EU, China, Russia and Japan issued a statement of intent: “*Taking into account the large-scale projects ongoing on a global scale with regard to the human-on-a-chip technologies and the potential interest for global regulatory authorities of different sectors, it is considered important that a systematic mechanism for exchange of information is being set up. The latter should take advantage of the collaborative initiatives already established for different sectors (e.g., FDA/EMA qualification exercise). Such a forum could also allow for cross-sectorial discussions on qualification criteria and performance standards in order to foster possible qualification of human-on-a-chip technologies.*”

In this chapter, some of the panel members summarize the *status quo* of substance testing regulations subject to major regulatory bodies.



## 5.2 US FDA drug regulation and regulatory science approach

Recent breakthroughs in science and technology have the potential to transform the FDA's ability to prevent, diagnose and treat disease. Recognizing this, the US FDA Advancing Regulatory Science Strategic Plan was designed to advance regulatory science to speed innovation, improve regulatory decision-making, and get safe and effective products to market in a timely manner. This strategic plan meets both today's public health needs and the challenges and opportunities of tomorrow (FDA, 2011b). One of the key elements of this plan is to improve the prediction of product safety and efficacy by developing better models of human adverse response, identifying and evaluating biomarkers and endpoints that can be used in nonclinical and clinical evaluations and developing and using computational methods and *in silico* modeling. By addressing these needs, the FDA will be better able to identify and accurately predict and reduce the magnitude and likelihood of risks associated with the products that it regulates. The FDA, the NCATS and the DARPA partnership for the development of *in vitro* microphysiological systems, described in detail in Chapter 4.5, is a groundbreaking example of the types of partnerships that are needed to bring innovative new technologies into the regulatory paradigm. The challenge is to develop an integrated microsystem platform that can incorporate several different modular organs on a chip and to incorporate it into the regulatory paradigm. The FDA's role in this partnership is to advise on regulatory requirements, validation and qualification of the organ-on-a-chip or human body-on-a-chip models. Qualification is a formal process that enables the FDA to advise product sponsors that a tool is available for use in a regulatory application. Qualification is a conclusion that, within the stated context of use, the results of assessment with a tool can be relied upon to have a specific interpretation and application in product development and regulatory decision-making.

Context of use is the key concept in the qualification process of drug development tools (DDT). It refers to a clearly articulated description delineating the manner and purpose of use for the tool including its limitations. Once qualification is granted, any product sponsor can submit data obtained with the qualified tool without being asked for further evidence in support of its suitability. Three DDT qualification programs are currently being implemented in the FDA Center for Drug Development and Research: (1) biomarkers; (2) clinical outcome assessments; and (3) animal models (FDA, 2014b). The context of use qualification concept can be applicable to any tool proposed for use in regulatory decision-making, including *in vitro* MPS.

Developing confidence in the predictive ability of *in vitro* MPS begins with identifying the critical regulatory gaps which can be addressed with these new tools, the consequences of an incorrect or incomplete answer, and an assessment of the level of confidence in each of the integral parts of an *in vitro* MPS. A determination needs to be made on the essential biological and functional features that are needed in the test organ-on-a-chip to address the context of use. The test or reference library of compounds for qualification should be tied directly to the regulatory question that is being addressed in the context of use. This

means that a different context of use may require a different set of test chemicals. Additionally, how to use the data to make/add or refine a regulatory decision should be decided up front. Combining the information above for a "context of use" evaluation of the overall predictive ability of a new tool to answer critical regulatory questions can be used as a framework for qualifying *in vitro* MPS in a transparent and scientifically defensible manner. A potential qualification and validation strategy for MPS is described in Chapter 7.

## 5.3 Chinese State Food and Drug Administration (SFDA) drug regulation and MPS

The National Institutes for Food and Drug Control (NIFDC) is a subordinate agency of the SFDA. A prime mission of the NIFDC is to organize the international collaboration and cooperation in the field of testing and analysis of drugs, medical devices, healthy food, cosmetics, and restaurant food safety. On the basis of that mission, a representative of the NIFDC actively participated in the panel discussion on regulatory science and human-on-a-chip approaches at the 9<sup>th</sup> World Congress on Alternatives and Animal Use in the Life Sciences in Prague 2014. In order to get hands-on experiences with MPS-based approaches the NIFDC signed a memorandum of understanding with the Technical University Berlin, Germany, for a joint 3-year collaboration in the field of MPS. A NIFDC team has been trained to operate MOC-based equipment. Next steps include MPS-based assay evaluation in comparison to test assays currently in use at the institute.

## 5.4 Russian drug regulation and considerations on MPS impact

The Russian Federation has been taking steps to modernize the healthcare system by stimulating the development of pharmaceutical and medical products (Russian Government, 2014). As a part of these measures, a national program "Development of pharmacological and medical industries 2013 - 2020" was approved. The program is monitored by the Ministry of Health and supported by the Ministry of Industry and the Ministry of Education and Science. The main goal of this program is the introduction of novel pharmaceutical compounds and new methods of testing them. This implies the progressive transition of Russian pharmaceutical companies and research laboratories to the international Good Manufacturing Practice (GMP), Good Laboratory Practice (GLP) and Good Clinical Practice (GCP) standards and the development of corresponding educational programs.

The Ministry of Health approved the procedure for the evaluation of medical devices, as well as the regulations for their registration for the technical testing, toxicological studies and clinical trials, in January 2014. In the meeting of the presidium of the Council for Economic Modernization and Innovative Development of Russia on 16 May, 2014, the Prime Minister Dmitry Medvedev emphasized that the introduction of innovative approaches should rely on domestic R&D programs and products, referring to the development of modern biopreparations, cell and tissue products, genomic technology, and biocompatible materials (Russian Government, 2014). New standards governing the testing of chemical impacts on the human body involving the





**Tab. 4: Overview of toxicity tests/information required for human risk assessment in the different regulations for the use of chemicals in the EU<sup>1</sup>**

Requirements based on *in vivo* tests are marked in dark blue, while requirements for which *in vitro* alternatives are included are marked in light blue, and white boxes indicate no data are required.

EU Regulation	Types of toxicity data (i.e., endpoints)								
	Kinetics	Acute toxicity	Irritation/Corrosion	Sensitization	Chronic toxicity	Mutagenicity	Carcinogenicity	Reproduction toxicity	Other
<b>Chemicals (EC, 2006)</b>									
• 1-10 t/y (Annex VII)									
• 10-100 t/y (Annex VIII) <sup>2</sup>									
• 100-1000 t/y (Annex IX) <sup>2</sup>									
• >1000 t/y (Annex X) <sup>2</sup>									
<b>Cosmetics (EC, 2009)</b>									
<b>Pesticides</b>									
• Active substances (EC, 2013a)									
• Plant protection products (EC, 2013b)									
<b>Biocides (EC, 2012)</b>									
<b>Food additives (EC, 2008)</b>									
<b>Food contact materials (EC, 2004; + SCF Guidelines)</b>									
• Migration <0.05 mg/kg food									
• Migration 0.05 – 5 mg/kg food									
• Migration >5 mg/kg food									
<b>Pharmaceuticals (EC, 2001; + ICH Guidelines)</b>									

<sup>1</sup> Many regulations include waivers and conditions for the tests required or they may be replaced by alternatives, such as QSAR predictions or *in vitro* systems, which are not included in this table for the sake of keeping a clear overview. For these waivers, conditions, and alternatives, one is referred to the specific regulation texts; optional tests, i.e., tests that are only necessary in case of certain outcomes of previous tests, are given a footnote with an explanation or are put in parentheses.

<sup>2</sup> The required tests shown for this tonnage/migration level are additional to the tests required at lower tonnage/migration levels; the tests required at the lower tonnage/migration levels are also required here.

use of an *in vitro* model of human skin (GOST 32634-2014), micronucleus test on mammalian cells (GOST 32635-2014) and the evaluation of gene mutations (GOST 32638-2014) were introduced in June, 2015.

### 5.5 Legal framework for human risk assessment for chemicals in the EU

Although animal use in biological research is much greater than that required for regulatory and chemical safety testing, the latter two are major drivers for alternative method development and testing systems. With the advent of omics, high-throughput testing, 3D cell cultures and, lately, MPS, the pressure to bring such methods into regulatory use has increased tremendously, as has the debate about the usability and application domain of such methods (Tralau et al., 2015). However, regulators continue to take a cautious stand on this matter. This is reflected not

least by the comparably modest number of validated and internationally accepted alternative methods, none of which harbors a MPS yet. The main obstacles to the implementation of any such methods are, apart from the often slow progress of legal implementation, method validation and an inherent limitation of cellular and MPS approaches to reflect established toxicological endpoints and organism plasticity (Tralau and Luch, 2015). Without changes to long established practices, this makes it difficult to readily adapt such systems for the purpose of quantifiable risk assessments or to transpose the results obtained to the classifications required by the Globally Harmonized System of Classification and Labelling of Chemicals (GHS), Classification, Labelling and Packaging (CLP) or REACH. Unsurprisingly, a lot of the regulatory testing in the EU is still carried out *in vivo*, the exceptions to the rule being skin and eye irritation, corrosion and genotoxicity.

Different legal frameworks exist for different domains of chemical substance evaluation (e.g., pesticides, cosmetics and food additives) apart from drug candidate testing in the EU. Each regulatory framework involves different requirements for information that needs to be submitted in the dossier for market acceptance, with guidelines or guidance documents usually describing which tests are acceptable to provide this information. Table 4 below gives an overview of the information required by some EU frameworks for chemicals and the OECD Test Guidelines (TGs) that can provide this information. The table shows how animal tests still predominate (in dark blue).

The highest numbers of experimental animals and resources are required for systemic and repeated dose toxicity testing (accounting for more than 65% of all experimental animals used; see ECHA, 2011; van der Jagt et al., 2004; Rovida and Hartung, 2009). The respective toxicological endpoints are challenging to address *in vivo* as well as *in vitro*, and it is in this context that MPS would ideally put their strength to the test, especially since they allow the breakdown of the species barrier by using human cells. Moreover, they could provide solutions to some of the open issues and regulatory challenges in the field of consumer protection, i.e., endocrine disruptors beyond the sex and thyroid hormone systems, low-dose effects, epigenetically active substances and the influence of background exposures. Much of this will constitute rather mid- to long-term options.

The more immediate regulatory use of MPS comprises the OECD's "adverse outcome pathways" initiative (OECD, 2013), integrated testing strategies, adverse biomarker identification and testing prioritization (e.g., similar to the Tox21-programme; Krewski et al., 2010). Concomitantly, MPS should be part of preliminary test runs for the aforementioned tox-test dummy (Tralau et al., 2012). Such blinded cross-validation trials would not only help to assess their already existing regulatory potential but help to identify shortfalls hands on.

A special situation exists with regard to cosmetics, which are subject to a ban on animal testing (EC, 2003, 2009). With effect of 2013, the ban not only prohibits live animal testing of cosmetic products, but also the marketing of products tested on animals or containing animal-tested ingredients (the only ex-

ception being chemicals that are within their scope of use also subject to REACH). Prior to that ban, significant efforts were made to develop validated *in vitro* alternatives to the animal tests with moderate success (Adler et al., 2011). No applications for market admittance for cosmetics which are based entirely on alternative methods of testing have been submitted to date. Consequently, the requirement to adapt alternative toxicity testing for cosmetics is pressing. Possible areas of adoption of MPS-based systems by the chemical and cosmetics industries are described in Chapter 3.2, whereas a potential tiered approach for qualification and validation is provided in Chapter 6.

## 6 How to qualify and validate MPS-based tools?

Qualification and validation of MPS-based assays is a major hurdle for industrial adoption and regulatory acceptance (Astshkina et al., 2012). In particular, validation of MPS-based assays requires initial qualification of the equipment and tissue sources used. Furthermore, adherence to the well-established rules of Good Cell Culture Practice (Coecke et al., 2005) and the recommendations for improving the quality and utility of organotypic models (Alépée et al., 2014) are mandatory requirements to ensure that MPS-based assays generate reliable, reproducible and robust data. Noteworthy, a concept of mechanistic validation (Hartung et al., 2013a) has been put forward out of the context of evidence-based toxicology (Hartung, 2010b) that promises to support MPS validation. As outlined in Chapter 2, only a few studies to date have sought to qualify the readouts of MPS-based assays against relevant *in vivo* models. For easier industrial adoption, we recommend the generation of a biological baseline for each MPS-based single organ equivalent, as exemplarily described for single-liver MPS in Chapter 3.1.1. We recommend a two-tiered approach for the validation of a MPS-based test assay within the current regulatory landscape in US and Europe (Fig. 17).

Validation is a process that needs to be continuously adapted to the technologies assessed for the purpose of their use (Leist et al., 2012). In a first step, we advise the voluntary "fit-for-purpose" or "context of use" qualification of an MPS-based

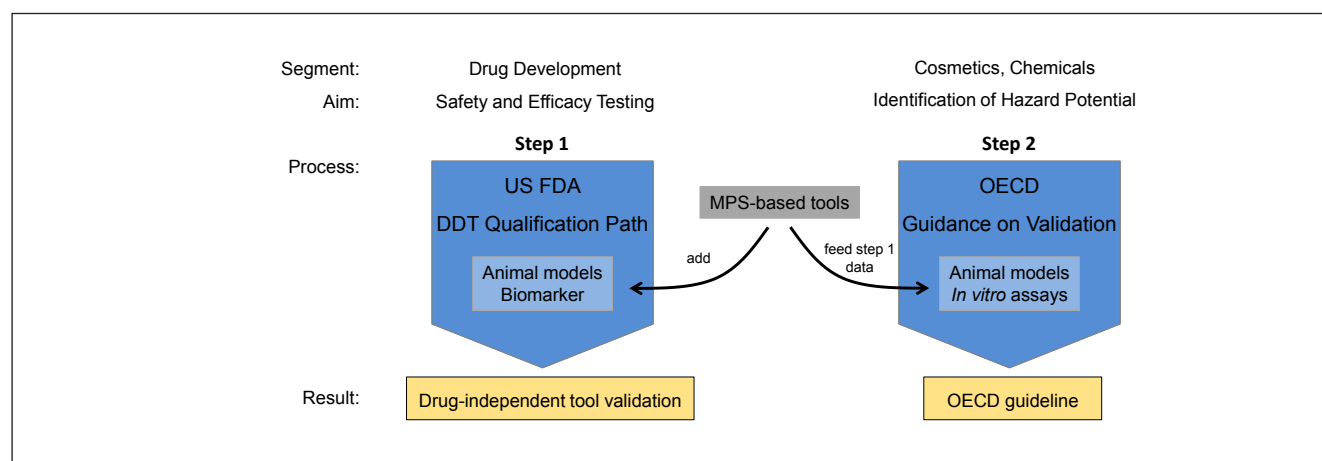


Fig. 17: A possible stepwise validation roadmap for upcoming MPS-based tools



test tool through the aforementioned FDA DDT Qualification Program. Here, collaboration between MPS-providers and pharmaceutical companies adopting the particular assay would be advisable. This qualification involves MPS providers, pharma industry and FDA officers and eventually leads to a MPS tool validation independent of the drug candidates used for validation. This, in turn, supports an easier adoption of the tool for further use in drug assessment. In addition, such a first validation step for a given MPS-based tool generates a validation algorithm and tool-specific data, which then, in a second step, can be fed into a validation program for the use of the same tool for chemical testing.

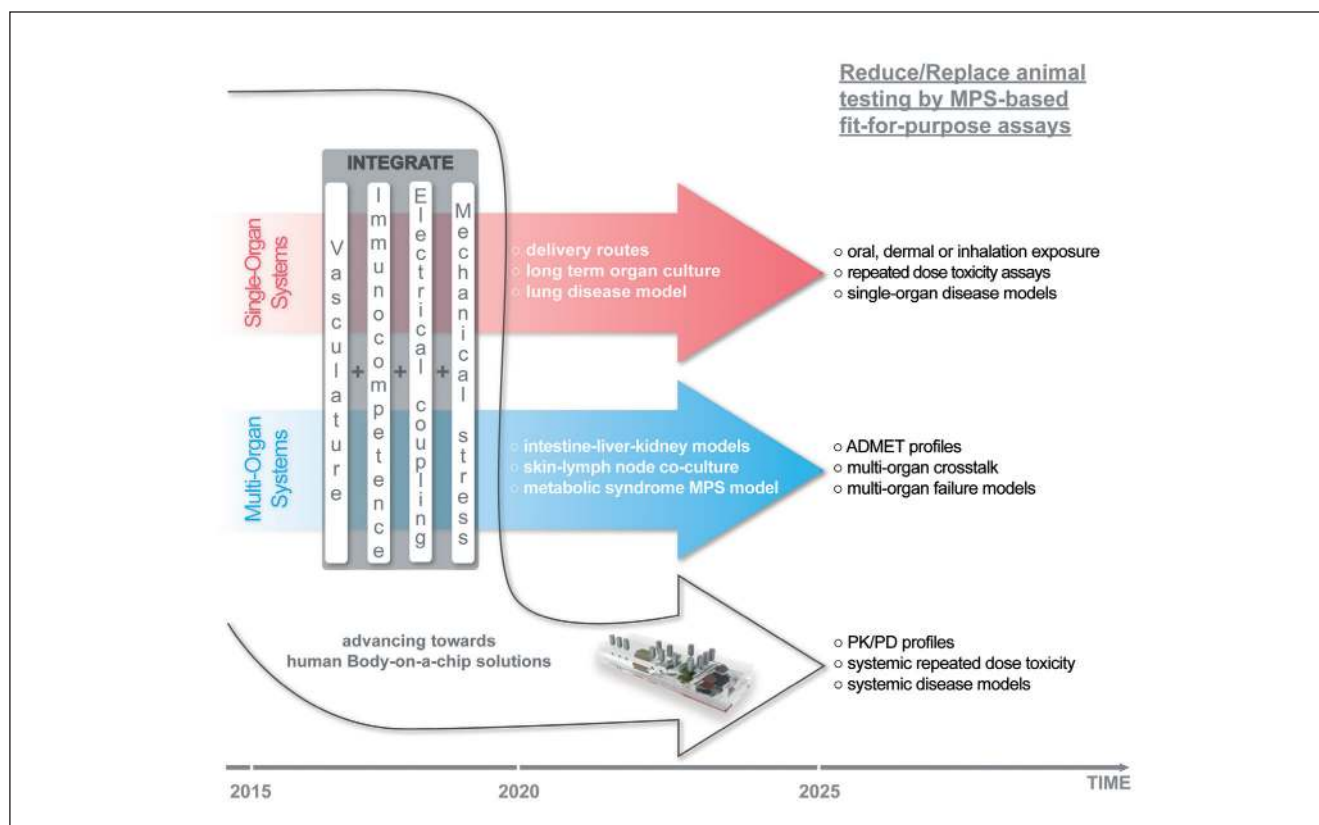
For MPS-based models aiming to replace the animal or existing *in vitro* models used in OECD guidelines in chemical safety assessment, the adherence to the existing OECD guidance document on the validation and international acceptance of new or updated test methods for hazard assessment (OECD, 2005), the EMA guideline on regulatory acceptance of 3R methods and qualification of novel methodologies for drug development (EMA/CHMP/SAWP/72894/2008 Corr1), via the EMA Scientific Advice Working Party (SAWP), and the recommendation of the ICH Safety Topic Recommendation Working Group could be instrumental.

However, given that MPS are usually based on human cell material it might be important to re-assess the suitability of animal data as the gold standard for validation.

In summary, a combination of the two qualification and validation steps, schematically illustrated in Figure 17, seems to be the most efficient road map toward validation of upcoming MPS-based drug development tools arising from single-organ, multi-organ or human body-on-a-chip developments.

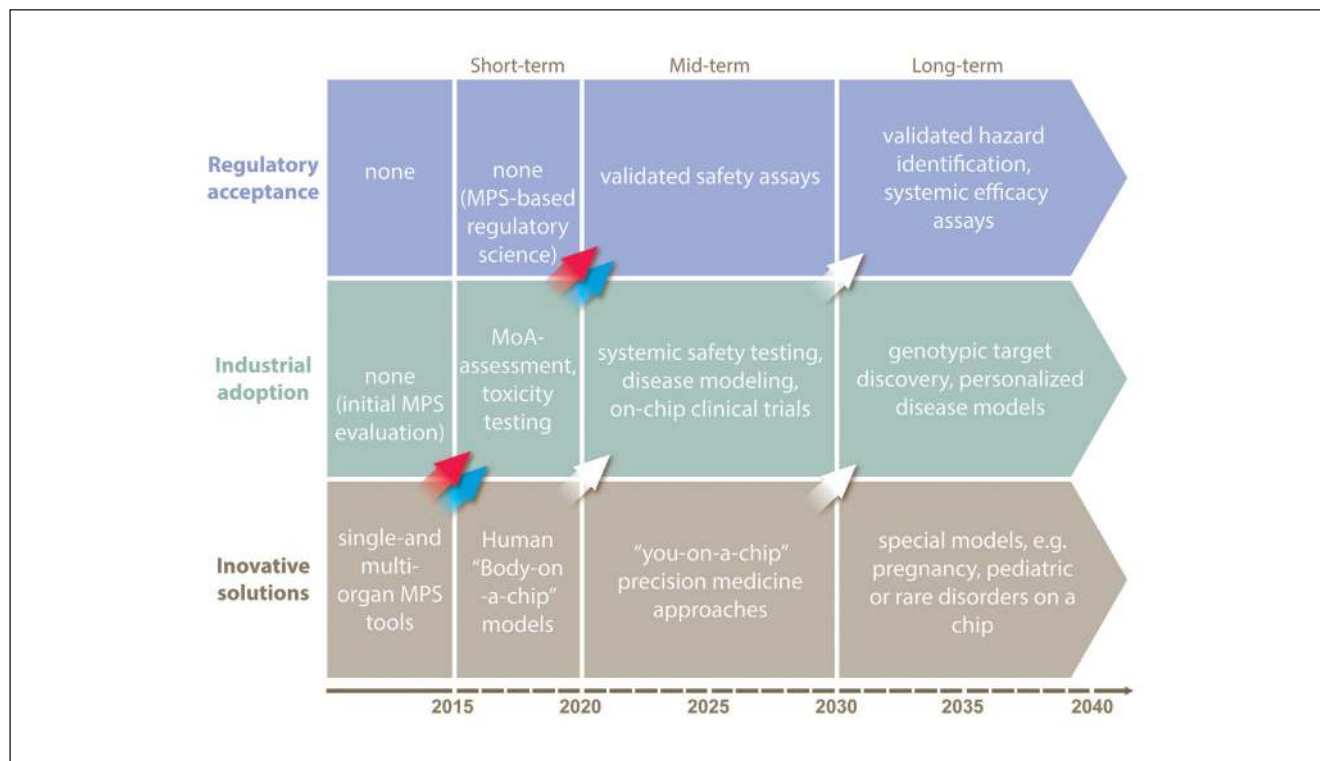
## 7 Visions are becoming reality

Single-organ MPS have been developed to establish physiological substance testing assays. Human organ models of the lung, heart, blood vessels, muscles, bones, liver, reproductive system, nervous system, gut, skin, intestine and kidney have been established and more models are to come. This development was followed by multi-organ MPS allowing the co-culture of different human organ equivalents in integrated microphysiological arrangements. First success in 28-day human intestine/liver/skin/kidney co-culture at homeostasis, for example, underlines the ability to move the technology towards systemic modeling of a human body-on-a-chip – a miniature organism.



**Fig. 18: Next MPS developments meeting industrial needs**

The next hurdles to overcome in order to achieve significant reduction and replacement of animal testing are further integration of vasculature, immunocompetence, electrical signaling and mechanical forces into the respective organ models. These developments are expected to lead to a further reduction of industrial substance testing in animals and will strongly support the development of human body-on-a-chip solutions aiming to replace systemic testing and disease modeling in laboratory animals.



**Fig. 19: A roadmap toward the reduction and replacement of animals and patients**

Red, blue and white arrows – translational impact of single-organ, multi-organ and human body-on-a-chip MPS-based approaches, respectively.

The future development of these three types of MPS will, we think, eventually lead towards the reduction and replacement of animal and human testing (Fig. 18). Prime challenges to improve single- and multi-organ systems over the next five years include the integration of biological vasculature, immunocompetence, electrical coupling and mechanical stress (where relevant). Physiological skin, intestine and lung barriers and predictive drug-induced organ toxicity assays or lung disease models may, for example, result from such single-organ improvements. Improved multi-organ systems may be suitable to enable ADMET profiling, physiological multi-organ-crosstalk and multi-organ failure models. Subsequently, the advanced knowledge and experience acquired from these successful improvements will logically enable the development of a human body-on-a-chip, providing systemic solutions to disease modeling and repeated dose toxicity assays (see Fig. 18 for overview).

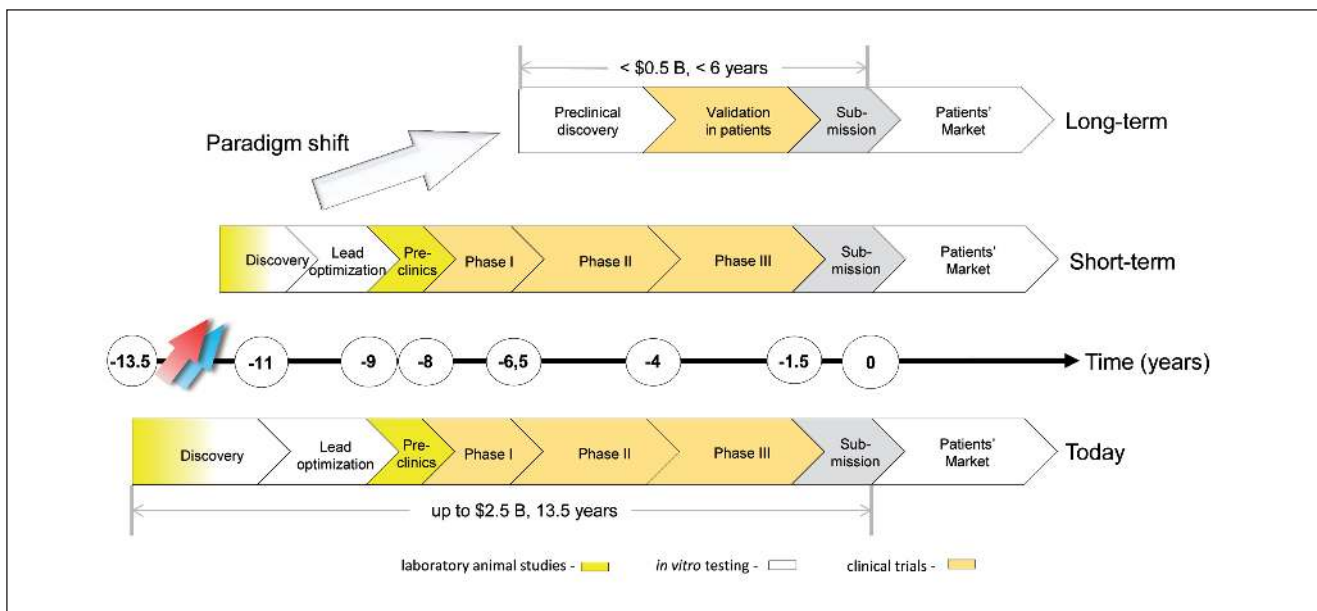
The experts at the workshop recognized a cyclic pattern of phases and levels of innovation in the field of MPS. It took the scientific community more than five years to take first single- and multi-organ systems towards initial industrial evaluation (see Fig. 19). Future development breaks down into three distinct phases: short-term, mid-term and long-term, over a total time period of more than 25 years. Each phase of innovative solutions triggers a consecutive phase of industrial adoption, which, in turn, instigates regulatory acceptance in a consecutive phase (see diagonal arrows in Fig. 19). The proof of concept of single-organ MPS, for example, may lead to their use for MoA

assessment and/or toxicity evaluation in industry within the next five years. We think that this should result in first validated regulatory safety assays between 2020 and 2030.

The individual future phases are highlighted in the roadmap (Fig. 19). The vision of the development of MPS in the long-term after 2030 could be, for example, the adoption of precision medicine tools ("You-on-a-chip") by industry for personalized disease models. Another envisioned target would be the on-chip modeling of aspects of clinical trials at an industrial level. All these developments could result in the eventual reduction and curtailing of tests on both animals and humans.

We expect MPS-based MoA assessment and toxicity testing adopted by the pharmaceutical industry in the short-term to lead to an initial reduction of the first two phases of the drug discovery life cycle (discovery and lead optimization) due to faster and more precise selection of targets and relevant leads (Fig. 20).

Once human body-on-a-chip platforms enter the pharmaceutical space with tools for predictive systemic testing and on-chip clinical trial data generation (Fig. 20) in the mid-term, this may nearly obviate the necessity of involving animals in preclinical development and healthy volunteers in phase I testing in the long-term. This, combined with expected high predictivity and, therefore, significant reduction of clinical attrition rates, may create a new drug development paradigm. The latter would change drug development from a stepwise approach to an ultra-fast discovery and validation approach with an enormous economic impact and value for society (see Fig. 20).



**Fig. 20: MPS-based approaches and tools can shift the current drug testing paradigm**

The envisioned substance testing paradigm shift (top) compares the drug development phases and related costs with the current situation (below)

The authors of this report are fully aware that this challenging roadmap, if successful, not only leads to a paradigm shift of drug development and chemical safety assessment but that it can only be successfully realized with all the parties involved (academia, industry and regulatory bodies) collaborating on a global scale.

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### Conflict of interest

Uwe Marx is a founder of TissUse GmbH which commercializes MPS platforms. Thomas Hartung is a cofounder of Organome LLC which aims to make mini-brains and other organotypic organ models commercially available.

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### Correspondence to

Uwe Marx  
TissUse GmbH  
Oudenarder Strasse 16  
13347 Berlin, Germany  
e-mail: Uwe.marx@tissuse.com