



Color Stability of Ceramic Veneers Luted With Resin Cements and Pre-Heated Composites: 12 Months Follow-Up

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The objective was to evaluate the color stability of ceramic veneers luted with resin cements and pre-heated composite resins (60 °C) for 12 months, and determine the degree of conversion (DC) of the luting agents. Two resin cements (AllCem Veneer, light-cured (LRC) and AllCem, dual-cured (DRC)] and three composite resins [Z100 (MNCR-minifilled), Herculite Classic (MHCR-micro-hybrid) and Durafill (MCCR-microfilled)] were used for cementing 0.8-mm-thick lithium-silicate glass-ceramic laminates (Suprinity, shade B2-HT, Vita) on bovine enamel (n=10). The specimens were stored at 37 °C in distilled water. CIELab parameters were determined at 24h after luting (baseline), 7, 30, 90, 180 days and 12 months. Three specimens were prepared for DC evaluation, performed by micro-Raman spectroscopy. Data were analyzed by ANOVA and Tukey's test ($\alpha=5\%$). For ΔE_{ab} and ΔE_{00} , there were significant differences for luting material ($p<0.001$), time ($p<0.001$), and double interaction ($p<0.001$). The groups cemented with MHCR (1 year), MCCR (90 days and 1 year) and MCCR-PH (1 year) were the ones with ΔE values greater than the acceptability threshold. All other groups maintained their ΔE lower than the acceptability threshold after 1 year in distilled water. Regarding DC, there were no significant differences ($p=0.127$) among the materials. Non-significant negative correlations were observed between the mean ΔE_{ab} and DC ($R=-0.65$) and ΔE_{00} and DC ($R=-0.64$). A significant positive correlation was observed mean ΔE_{ab} and ΔE_{00} ($R=0.99$). It was concluded that the different luting agents influenced the final color of the restorations. The heating of the composite resins did not affect their DC.

Key Words: color stability, degree of conversion, ceramic veneers, resin cements, pre-heated composites.

Introduction

One of the major challenges for modern dentistry is to achieve the perfect optical properties of natural teeth with artificial materials (1). In general, the optical behavior of a ceramic restoration is determined by the combination of the underlying tooth structure color, the thickness of the ceramic layers, and the color of the cement (2). In clinical situations, it is essential to understand how the color of a cemented ceramic restoration may change after aging in the oral cavity. Cement layer discoloration is an important aspect to be considered when luting ceramic restorations. When compared to ceramic materials, the cement layer is chemically less stable and may undergo color changes over time. Nonetheless, the perception of color alteration due to resin cement aging may be different according to the ceramics' translucency. Therefore, clinicians should understand the factors affecting final result of indirect restorations and carefully choose restorative materials in order to achieve optimal aesthetic results (3).

Resin cements are often used for the cementation of all-ceramic restorations, as they have good esthetic and mechanical properties, low solubility in the oral environment and can be adhesively bonded to dental tissues

(4). Among luting agents, light-cured cements are widely recommended for cementation of ceramic veneers. The major advantages of these cements are color stability and longer working time, as compared to chemically activated or dual-cured resin cements (5,6).

Dual-cured resin cements can also be used for cementation of ceramic veneers. These cements have better mechanical properties than light-cured or chemically activated cements, such as flexural strength, modulus of elasticity, hardness, and degree of conversion (DC) (7). However, these cements have a shorter working time, and oxidation of reactive groups of tertiary amines and inhibitors may cause changes in their color over time, especially yellowing of the cement (8). It is important to note that these compounds, amines and inhibitors, may also be found in light-cured materials, but in a smaller amount (9).

Ceramic veneers can be cemented with resin cements and with composite resins. There is a growing interest in making composite resins with higher filler content less viscous by using pre-heating, without affecting the properties of the polymerized material (10). Some of the possible advantages of pre-heating composite resins include

better adaptation of the material to the cavity walls, lower potential for the formation of defects at the margins, increase in the DC and, consequently, better physical and mechanical properties (11). As the cost of pre-heated composite resins is lower than that of resin cements and as the range of colors is maximized, they can be used as an alternative for the adhesive cementation of ceramic veneers (12). The success of ceramic restorations depends on good polymerization of resin-based materials used for cementation. Thus, understanding how the pre-heating of different composite resins used for cementation of ceramic veneers influences the DC could help in the clinical decision for the luting agent, aiming for long-term esthetic and functional outcomes (13).

It should be highlighted that the assessment of color stability of different luting materials plays an important role in thin translucent ceramic veneers, fabricated mainly of feldspathic ceramics and glass-ceramics, with thicknesses ranging from 0.3 to 0.9 mm, possibly affecting their long-term success (14). Therefore, the objective of the present study was to evaluate the color stability of thin ceramic veneers luted with resin composites and pre-heated composite resins (60 °C) for 12 months, and determine the degree of conversion (DC) of the luting agents. The null hypotheses were as follows: i) the different luting agents would not influence the final color of cemented thin ceramic veneers; ii) storage time would not influence the color of thin ceramic veneers, regardless of the luting material used; and iii) there would not be any difference in the DC of the evaluated luting materials.

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Material and Methods

Forty pigmentation-free bovine incisors with intact crowns without visually detectable enamel cracks were selected. The shades of all teeth were determined prior to the experiments with a Vita Classical shade guide (Vita Zahnfabrik, Bad Säckingen, Baden-Württemberg, Germany), and were classified as A1, B2 or A2. Two flat surfaces were obtained using a semiautomatic polisher (Buehler MetaServ 250, Lake Bluff, IL, USA) with silicon carbide sandpapers (grit sizes 320, and 600) for 1 min under water cooling. The surfaces had at least 6 mm of flat area and were located only on the enamel.

After preparation of the surfaces, the specimens were randomly distributed into eight groups (n=10) according to the luting agent used: LRC – light-cured resin cement; DRC – dual-cure resin cement; MNCR – minifilled composite resin; MNCR-PH – pre-heated minifilled composite resin; MHCR – micro-hybrid composite resin; MHCR-PH – pre-heated micro-hybrid composite resin; MCCR – microfilled composite resin; and MCCR-PH – pre-heated microfilled composite resin. The composition of materials is described in Table 1. All resin cements and composite resins used were shade A1 (Vita Classic shade guide, Vita Zahnfabrik, Bad Säckingen, Baden-Württemberg, Germany).

Five blocks of lithium silicate-based glass-ceramics (Suprinity, shade B2-HT, Vita Zahnfabrik, Bad Säckingen, Baden-Württemberg, Germany) were cut using a low speed diamond saw (IsoMet 1000, Buehler, Lake Bluff, USA) under cooling to obtain 0.8-mm thick ceramic veneers. The veneers were subjected to thermal treatment under vacuum at 840 °C for 8 min, according to the manufacturer's

Table 1. Composition of resin cements and composite resins

Luting material	Classification	Composition
AllCem Veneer (FGM)	Light-cured resin cement	Methacrylate monomers, camphorquinone, co-initiators, stabilizers, pigments, silanized barium, aluminum, and silicate glass particles, and silicon dioxide 63% of filler content
AllCem (FGM)	Dual-cured resin cement	Cement base: methacrylate monomers, camphorquinone, co-initiators, stabilizers, pigments, barium, aluminum, and silicate glass microparticles, silicon dioxide nanoparticles, inorganic pigments, preservatives Catalyst paste: methacrylate monomers, dibenzoyl peroxide and stabilizers, barium, aluminum, and silicate glass microparticles 67% of filler content
Z100 (3M)	Minifilled composite resin	Bis-GMA, TEGDMA, zirconia/silica 81% of filler content
Herculite Classic (Kerr)	Micro-hybrid composite resin	Bis-GMA, TEGDMA, camphorquinone, amine, iron oxide pigments, aluminum borosilicate glass, colloidal silica (SiO ₂) 79% of filler content
Durafill (Kulzer)	Microfilled composite resin	UDMA, highly dispersive silicon dioxide, prepolymerized filler particles 54% of filler content

Bis-GMA: Bisphenol-A glycidyl methacrylate; TEGDMA: Tetraethylene glycol dimethacrylate; UDMA: Urethane dimethacrylate.

recommendations.

The ceramic veneers were etched with 5% hydrofluoric acid (Condac Porcelana, FGM, Joinville, SC, Brazil) for 20 s, washed under running water for 20 s, and air-dried. Silane (Prosil, FGM, Joinville, SC, Brazil) was applied for 60 s followed by a layer of adhesive (ScotchBond Multi-Purpose, 3M, St. Paul, MN, USA). The enamel surface was etched with 37% phosphoric acid (Condac 37, FGM, Joinville, SC, Brazil) for 30 s, washed for 30 s under running water, and air-dried. A layer of adhesive (ScotchBond Multi-Purpose, 3M, St. Paul, MN, USA) was applied. The luting material was placed on the treated surface of the ceramic veneer. In the pre-heated composite resin groups, the luting material was placed in an oven and pre-heated at 60°C for 3 min in a dappen dish. After the heating period, the dappen dish was removed from the oven when the surfaces of the ceramic veneers and enamel were already treated. The luting material was promptly placed over the surface of the ceramic veneers. The veneers were cemented on the flat surface of the middle third of the dental enamel, with finger pressure for 10 s repeated until the flow of excess material was completely ceased and the veneer was fully seated onto the enamel, simulating a clinical cementation procedure. A pilot study was conducted (sixteen specimens) for standardization of the cementation procedure. These specimens were sectioned and evaluated at 40x magnification under a stereomicroscope (SZX9, Olympus, Tokyo, Japan) to determine the thickness of the luting material. The cement line was considered uniform and clinically acceptable, with thickness of $133.4 \pm 29.0 \mu\text{m}$ (coefficient of variation of 22%). The mean cementation time for each veneer was approximately 1 min (from placing the luting material into the veneer until complete excess removal). Cementations were carried out in controlled temperature (23 °C) and humidity (30 to 50%). Light-curing of adhesive layers and of the luting agent occurred simultaneously for each veneer with a LED curing unit (Radii-Cal, SDI, Bayswater, Australia) with 1200 mW/cm² irradiance for 40 s. The light-curing unit was fully charged before the luting procedures and the irradiance of the light-curing unit was checked using a radiometer (LED Demetron, Kerr, Middleton, WI, USA) before use. Ten minutes after light-curing, the specimens were stored in an oven, immersed in distilled water at 37 °C. The distilled water was replaced every week throughout the whole evaluation period.

Color stability after cementation was evaluated using a spectrophotometer (EasyShade Advance, Vita Zahnfabrik, Bad Säckingen, Baden-Württemberg, Germany). The specimens were dried with absorbent paper, and placed on a flat surface with a standardized white background. The spectrophotometer was calibrated before the readings. The spectrophotometer was always positioned in the

center of the specimen, at a 90° angle to the surface. The measurements were always made in the same environment with the same lighting conditions and at similar times of the day, to minimize the interference of the environment in the color measurements.

Color parameters were assessed 24 h after cementation (baseline), and subsequently at 7, 30, 90, and 180 days, and at 12 months. After each reading, the specimens were stored in distilled water at 37 °C. Color stability was assessed by determining the color difference between color measurements and baseline, using L, a and b coordinates from the CIELab (ΔE_{ab}) and CIEDE2000 (ΔE_{00}) system, where L indicates luminosity, a represents the green (-a) and red color (+a) and b represents the blue (-b) and yellow (+b) color. ΔE_{ab} was calculated using the formula (15,16):

$$\Delta E_{ab} = [(\Delta L)^2 + (\Delta a)^2 + (\Delta b)^2]^{1/2}$$

where ΔL , Δa and Δb indicates difference between the final and baseline measurements for different periods for each parameter.

ΔE_{00} was calculated according to the CIEDE2000 formula (16,17):

$$\Delta E_{00} = \{ [(\Delta L' / (k_{SL}))^2 + [\Delta C' / (k_{SC})]^2 + [\Delta H' / (k_{SH})]^2 + RT[\Delta C' / (k_{SC})] \times [\Delta H' / (k_{SH})] \}^{1/2}$$

where ΔL , ΔC and ΔH are the differences in lightness, chroma, and hue for a pair of samples in CIEDE2000, and RT is a rotation function that accounts for the interaction between chroma and hue differences in the blue region. The weighting functions SL, SC, and SH adjust the total color difference for variation in the location of the color difference pair at the L, a, and b coordinates, and the parametric factors kL, kC, and kH are correction terms for experimental conditions. In the present study, kL, kC, and kH were set to 1.

The 50:50% acceptability thresholds for CIELab (ΔE_{ab}) and CIEDE2000 (ΔE_{00}) were 2.66 and 1.77, respectively (18).

For DC measurements, disc (1 mm in height and 5 mm in diameter) specimens were prepared for the luting materials using a Teflon mold. The material was inserted in one increment and light-cured for 40 s. The internal diameter tip of the light-curing unit was 6 mm, and the specimen was fully positioned and centered below the tip of the curing unit during light activation. One reading per specimen was performed, with the discs carefully positioned so that the readings were made in the central area of the specimen.

For the uncured specimens, the same amount of material was used. All specimens were subjected to micro-Raman spectroscopy (Senterra Bruker, Ettlingen, Baden-Württemberg, Germany), with a resolution of 4 cm⁻¹ and 32 readings at 4,000 to 800 cm⁻¹. Peak absorbance of aromatic bonds was recorded at 1,608 cm⁻¹ (Abs 1608) and the peak absorbance of double-bond aliphatic compounds (C=C) was

recorded at 1,636 cm⁻¹ (Abs 1636). Three specimens were assessed in each material.

The readings for the cured materials were performed 10 min after light-curing. During these 10 min, the specimens were stored in dark canisters, at room temperature. The ratio between Abs 1636 and Abs 1608 was calculated for both cured and uncured materials. The percentage of remaining double bonds (RDB) was determined according to the formula:

$$\%RDB = (\text{Abs 1636} / \text{Abs 1608 for cured material}) \times 100 / (\text{Abs 1636} / \text{Abs 1608 for uncured material}).$$

The % degree of conversion (%DC) of double bonds was then calculated using the formula:

$$\%DC = 100 - \%RDB$$

The color change data were analyzed by repeated-measures two-way ANOVA and Tukey's test. The DC data were analyzed by one-way ANOVA. All analyses were performed with a 5% significance level. All correlations (mean ΔE_{ab} or ΔE_{00} in the evaluated period and the DC; and between mean ΔE_{ab} and ΔE_{00} in the evaluated period) were

determined by Pearson's correlation coefficient.

Results

The means and standard deviations for ΔE_{ab} and ΔE_{00} are shown in Tables 2 and 3, respectively. There were statistically significant differences for the luting material ($p < 0.001$) and time ($p < 0.001$). Double interaction was statistically significant ($p < 0.001$).

All groups had a ΔE (both ΔE_{ab} and ΔE_{00}) lower than the acceptability threshold at 7, 30, and 180 days. The groups cemented with MHCR (1 year), MCCR (90 days and 1 year) and MCCR-PH (1 year) were the only ones with ΔE values greater than the acceptability threshold. All other groups maintained their ΔE lower than the acceptability threshold at the end of 1 year of storage in distilled water.

The DCs obtained for the luting materials are shown in Table 3. There were no statistically significant differences among the materials ($p = 0.127$). The DC ranged from 64.0% (MCCR-PH) to 85.1% (DRC).

Non-significant moderate to strong negative

B. P. Gugelmin et al. Table 2. Means and standard deviations of ΔE_{ab} for the different materials and time periods after cementation

Luting material	Temperature	ΔE_{ab}				
		7 days	30 days	90 days	180 days	1 year
LRC	Room temperature	1.0 ± 0.5 Aa	1.5 ± 0.5 Aa	1.6 ± 0.6 Aa	1.7 ± 0.5 Aa	2.0 ± 0.5 Aa
DRC	Room temperature	1.4 ± 0.7 Aa	1.3 ± 0.6 Aa	1.1 ± 0.5 Aa	1.3 ± 0.6 Aa	2.3 ± 0.8 Aab
MNCR	Room temperature	2.3 ± 0.2 Aa	1.6 ± 0.5 Aa	2.3 ± 0.9 Aab	2.0 ± 0.8 Aa	2.4 ± 0.2 Aab
	Pre-heated (PH)	1.5 ± 0.5 Aa	1.9 ± 0.7 Aa	2.4 ± 0.6 Aab	2.1 ± 0.6 Aa	2.1 ± 0.6 Aab
MHCR	Room temperature	1.8 ± 0.8 Aa	1.9 ± 0.9 Aa	2.1 ± 1.3 Aa	2.2 ± 1.3 Aa	2.7 ± 1.4 Aab
	Pre-heated (PH)	1.5 ± 0.6 Aa	1.6 ± 0.6 Aa	1.4 ± 0.8 Aa	1.5 ± 0.5 Aa	2.0 ± 0.7 Aa
MCCR	Room temperature	2.1 ± 0.7 Aa	1.7 ± 0.9 Aa	2.7 ± 1.7 Ab	2.4 ± 1.2 ABa	3.6 ± 1.0 Bab
	Pre-heated (PH)	1.5 ± 0.8 Aa	1.6 ± 0.7 Aa	2.6 ± 1.1 ABb	2.4 ± 1.3 ABa	3.6 ± 1.6 Bb

Values followed by the same uppercase letters in the row are statistically similar ($p > 0.05$). Values followed by the same lower case letters in the columns are statistically similar ($p > 0.05$).

Table 3. Means and standard deviations of ΔE_{00} for the different materials and time periods after cementation and degree of conversion

Luting material	Temperature	ΔE_{00}					Degree of conversion (%)
		7 days	30 days	90 days	180 days	1 year	
LRC	Room temperature	0.6 ± 0.2 Aa	0.9 ± 0.3 Aa	0.9 ± 0.3 Aab	1.1 ± 0.3 Aa	1.3 ± 0.3 Aa	78.5 ± 4.3
DRC	Room temperature	0.8 ± 0.4 Aa	0.8 ± 0.3 Aa	0.7 ± 0.3 Aa	0.9 ± 0.4 Aa	1.6 ± 0.5 Aab	85.1 ± 11.3
MNCR	Room temperature	1.6 ± 0.2 Ab	0.9 ± 0.3 Aa	1.2 ± 0.5 Aab	1.2 ± 0.5 Aa	1.4 ± 0.1 Aa	66.5 ± 14.6
	Pre-heated (PH)	1.0 ± 0.3 Aab	1.2 ± 0.3 Aa	1.5 ± 0.5 Aab	1.3 ± 0.4 Aa	1.3 ± 0.4 Aa	64.0 ± 9.0
MHCR	Room temperature	1.2 ± 0.5 Aab	1.2 ± 0.6 Aa	1.4 ± 0.8 Aab	1.4 ± 0.9 Aa	1.8 ± 1.0 Aab	72.9 ± 7.7
	Pre-heated (PH)	1.0 ± 0.3 Aab	1.0 ± 0.3 Aa	0.9 ± 0.5 Aab	0.9 ± 0.3 Aa	1.3 ± 0.5 Aa	72.6 ± 8.4
MCCR	Room temperature	1.6 ± 0.5 ABb	1.1 ± 0.6 Aa	1.8 ± 1.1 ABb	1.6 ± 0.8 ABa	2.4 ± 0.7 Bb	65.8 ± 3.6
	Pre-heated (PH)	1.2 ± 0.6 Aab	1.0 ± 0.5 Aa	1.8 ± 0.7 ABb	1.5 ± 0.8 ABa	2.4 ± 1.1 Bb	74.1 ± 5.6

Values followed by the same uppercase letters in the row are statistically similar ($p > 0.05$). Values followed by the same lower case letters in the columns are statistically similar ($p > 0.05$).

correlations were observed between the mean ΔE_{ab} and DC, and ΔE_{00} and DC, with a Pearson's correlation coefficient of -0.65 ($p=0.083$) and -0.64 ($p=0.089$), respectively; indicating that the higher the DC, the lower the color change and the higher the color stability (Fig. 1). Significant strong positive correlations were observed between ΔE_{ab} and ΔE_{00} for all evaluated times (7 and 30 days=0.96; 90 days=0.97; 180 days=0.98; and 1 year=0.99) and also considering the mean ΔE_{ab} and ΔE_{00} values (Pearson's correlation coefficient of 0.99, $p<0.001$) (Fig. 2).

Discussion

Luting material is a determinant factor that influences the final color of thin ceramic veneers (19). In this study, the results for luting materials are in accordance with those described in the literature, rejecting the first hypothesis, since the different luting agents influenced the final color

of thin ceramic veneers. The mean ΔE values were significantly different, considering the luting material, with a lower ΔE values for DRC, LRC and MHCR-PH, when compared with MCCR. A possible explanation could be the larger amount of organic matrix in relation to filler particles in microfilled resins, resulting in high water and pigment sorption rates (20).

Some studies report lower color stability in dual-cured resin cements (12,21) caused by the oxidation of initiators, as well as of unreactive tertiary amines, and by the presence of unreactive benzoyl peroxide during photoactivation, leading to yellowing of the material and compromising long-term esthetics. In this study, however, the DRC had a statistically similar result to that of LRC and of some composite resins (minifilled and micro-hybrid, at room temperature and pre-heated). A

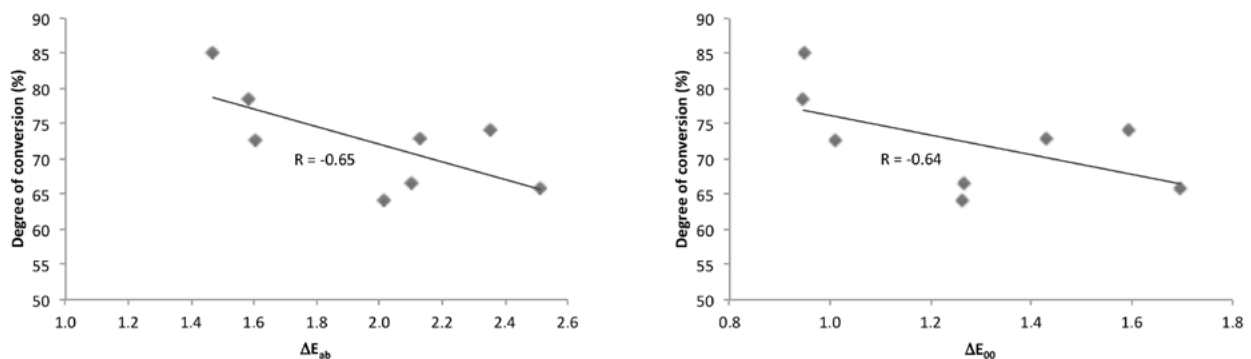


Figure 1. Correlation plots between the degree of conversion (in %) and the mean ΔE_{ab} or ΔE_{00} values in the evaluated period.

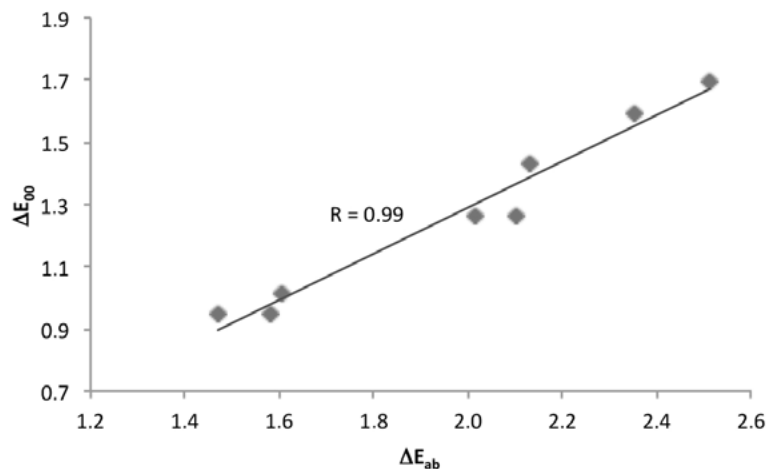


Figure 2. Correlation plot between the mean ΔE_{ab} and ΔE_{00} values in the evaluated period.

possible explanation would be the experimental design of the present study, which assessed the final color of ceramic veneers after cementation, evaluating the whole set (ceramic veneer, luting agent, and tooth substrate), rather than the resin cement only. By evaluating the set, color change tends to be minimized, when compared to studies in which cement specimens are directly exposed to degradation. In the present study, due to the cementation of laminates over the tooth substrate, with a thin layer of cement not directly exposed to the medium, only at the margins, the results tend to be closer to the ones found in clinical situations. This phenomenon is more relevant on the cervical margins of ceramic veneers. Hence, clinicians should give special attention to the proper positioning of the finishing lines, using the gingival or slightly subgingival level to minimize this phenomenon. Despite the favorable result obtained for dual-cured resin cement in the present study in terms of color stability, working time – limited by the chemical reaction – is an important clinical disadvantage, especially in cases of multiple veneers. Thus, light-cured resin cement is still the material of choice for the cementation of veneers because of its large working time and long-term color stability (5,6). The composite resins assessed, both at room temperature and pre-heated, had statistically similar ΔE values, which is in accordance with the literature (12), indicating that photoactivated materials provide good esthetic outcomes and that composite resins can also be indicated for the cementation of ceramic veneers.

During the cementation of ceramic veneers, the polymerization of light-cured luting materials may be affected if the ceramic restorations significantly attenuate the irradiance of the light-curing unit. This is a clinically relevant issue, since the properties of light-cured resin-based materials could change depending on the ceramic type and thickness (13,22). Several factors can influence the translucency of ceramic restorations, such as shade, thickness, surface roughness, polishing, volume fraction of porosity and crystalline phase (23). A recent systematic review and meta-analysis evaluated how variations in thickness of lithium disilicate restorations influenced the degree of conversion of the resin cements. It was concluded that the degree of conversion of cements was significantly decreased when ceramic thickness increased. Thicknesses greater than 1.0 mm were shown to considerably reduce the degree of

conversion of dual- or light-cured materials (24).

The cement thickness obtained in this study was the result of a luting procedure carried out by a single operator, after standardization in a pilot study. In an effort to simulate clinical conditions, the cement thickness was not standardized using spacers, as reported in previous studies (25). The mean cement thickness was $133.4 \pm 29.0 \mu\text{m}$ (coefficient of variation of 22%), considering the use of various luting materials (resin cements and composite resins), and the fact that they have different viscosities. Previous *in vitro* studies also reported cement thicknesses similar to ours, varying from approximately $100 \mu\text{m}$ to $160 \mu\text{m}$ (25,26).

The second hypothesis of the present study was also rejected, since storage time influenced the final color of veneers after cementation in the case of the microfilled composite resin. The longer the storage time, the larger the change in color, which can be explained by the fact that the specimens were stored for 1 year in distilled water, after which period the luting agent went through water sorption, degradation, and plasticization, affecting its color in the long-term. Several studies that have evaluated the color stability of cemented ceramic veneers and luting materials use different artificial accelerated aging methods, with similar results to those of the present study, showing that aging and time influence color stability (12,27). Accelerated aging has been the most widely reported method for the aging of specimens and assessment of color stability in the long run, but few studies store the specimens in water for periods longer than 6 months. In this study, the specimens were stored in distilled water at 37°C for 12 months in an attempt to better simulate clinical aging in the oral environment. Regarding the outcomes after 1 year-storage, only the groups cemented with MHCR, MCCR and MCCR-PH showed a clinically significant color change with ΔE above the 50:50% acceptability thresholds.

The assessment of color differences is of great interest for dental materials and clinical situations. This study used two different color difference parameter, ΔE_{ab} and ΔE_{00} , to evaluate the color stability of different luting materials for laminate veneers over a 1 year time period. Both parameters are important, because ΔE_{ab} is well known in Dentistry and many studies over the years have used this parameter to determine color difference. However, in the last five years, the use of CIEDE2000 formula and the respective ΔE_{00}

has been encouraged as a more adequate tool for evaluation of the color of resin composites. Also, it has been shown that the CIEDE2000 formula has better match to observer responses when compared to CIELab color difference. Besides resulting in different ΔE values and with different acceptability thresholds, the literature reports significant correlations between ΔE_{ab} and ΔE_{00} for different shades of composite resins, with r^2 of 0.99 (17). The present study, also evaluating resin-based materials, corroborates this result, with a strong significant positive correlation coefficient of 0.99.

The DC can be a way to assess the mechanical properties of polymeric materials (28). The higher the DC, the better the properties and, consequently, the better the color stability in the long-term. In this study, no statistically significant difference was observed between the groups, and the hypothesis that there would not be any difference in the DC of the luting agents was accepted. Previous studies also showed that some properties, such as monomer conversion and flexural strength, were not significantly affected by composite pre-heating (29). One of the possible explanations for this fact is that, when a composite is heated to 60°C and removed from the heating device, its temperature can decrease approximately 40% in the first minute (30). Thus, considering such a decrease, it is possible that the resin temperature might not be enough to significantly increase the composite mechanical properties (29). The dual-cured resin cement had the highest DC (85.1%), since its two activation modes allowed higher monomer conversion. Dual-cured cements subjected to photo-activation usually had a better DC and better physicochemical properties when compared to light-cured materials (7). Even though no significant difference was found in the DC, there was a moderate to strong negative correlation between ΔE_{ab} and DC, and ΔE_{00} and DC. This correlation was already expected, confirming an important relationship between DC and color stability.

Pre-heating of composite resins has been used as a clinical alternative to decrease the viscosity and to improve the use of composite resins both in restorative procedures and in the cementation of ceramic veneers. There are several methods described in the literature to pre-heat resin-based materials, such as the Calset and Therma-Flo composite warmers, ovens, light of the dental unit chair, hand holding, thermocycling machines, and wax warmers (31,32). The present study used an

oven to pre-heat the composite resins, as has been previously described in the literature (12,33). This method is simple, the temperature can be easily controlled, and it is commonly available in the dental clinics. Also, it is important to mention that the cost and availability of some of the specific devices for pre-heating of composites can be a limiting factor for their use (31). The use of ovens did not have a negative effect on the properties of the assessed materials, providing a less costly alternative for clinical cementation of laminate veneers.

The literature reports, in some cases, an increase in DC with pre-heating of resins (33), as high temperatures increase the mobility of monomers, the collision between molecules, and the amount of bonds (34). The increase in DC would cause the polymer matrix to absorb less solvent and to lose fewer components to the external environment, slowing down its degradation (34). In another previous study on color stability and DC of pre-heated resins, pre-heating did not change color stability, but it statistically increased the DC (35). In the present study, on the other hand, pre-heating of resins did not increase the DC and also did not influence the color stability of cemented veneers.

From the clinical perspective, the results obtained in this study are favorable to the use of pre-heated composite resins for the cementation of ceramic veneers. Z100 and Durafill resins had adequate viscosity for the cementation of laminate veneers and responded well to heating, rendering their consistency even better for the cementation of veneers. It should be emphasized that not all composite resins may be indicated for pre-heating and cementation of veneers without significant interference in their physical and mechanical properties. Their composition, filler content, and photoinitiator system should be considered. Also, the thickness of the ceramic material and its fit should be considered, as more flowable materials are better indicated for thinner cement lines. Cementation with pre-heated composite resins requires higher pressure during the placement of the specimen, and in case of very thin laminates, the possibility of crack and fracture could increase.

Therefore, it is increasingly important that clinicians understand the different properties of materials for the cementation of thin ceramic veneers that are commercially available. The color stability of these materials has a crucial role, which may cause the cement film to be clinically visible

over time. The demand for esthetic treatments with ceramic veneers requires that clinicians be careful with the choice of the luting material, as this is one of the major factors that will determine long-term treatment success.

It can be concluded that the different materials used for cementation of thin ceramic veneers influenced the final color of the restorations and the light-cured and dual-cured resin cements had similar color stability. The microfilled composite resin at room temperature and pre-heated revealed clinically relevant color change after 1 year of storage. Heating did not affect the color stability of the composite resins used, as compared to materials used at room temperature. The DC of luting agents used did not show any significant difference, and pre-heating of the composite resins did not cause their DC.

Resumo

O objetivo foi avaliar a estabilidade de cor de laminados cerâmicos de fina espessura, após a cimentação com cimentos resinosos e resinas compostas em temperatura ambiente e aquecida (60 °C), durante 12 meses; bem como determinar o grau de conversão dos diferentes materiais para cimentação. Foram utilizados dois cimentos resinosos [AllCem Veneer, cimento resinoso fotoativado (LRC) e AllCem, cimento resinoso dual (DRC)] e três resinas compostas [Z100 (MNCR – resina composta de partículas finas), Herculite Classic (MHCR – resina composta micro-híbrida) e Durafill (MCCR – resina composta microparticulada)] para cimentação de laminados cerâmicos a base de silicato de lítio (Suprinity, cor B2-HT, Vita Zahnfabrik) com 0,8 mm de espessura, sobre esmalte bovino. Oitenta espécimes foram distribuídos aleatoriamente em 8 grupos de acordo com o material para cimentante (n=10). Os espécimes foram armazenados a 37 °C em água destilada. Os parâmetros do CIELab foram determinados 24h após a cimentação (baseline), 7, 30, 90, 180 dias e 12 meses. Outros três espécimes foram preparados para avaliação de grau de conversão, realizada por espectroscopia micro-Raman. Os dados foram analisados por ANOVA e teste de Tukey ($\alpha=5\%$). Para ΔE_{ab} e ΔE_{00} , houve diferenças estatisticamente significantes para o material de cimentação ($p<0,001$), tempo ($p<0,001$) e interação dupla ($p<0,001$). Os grupos cimentados com o MHCR (1 ano), MCCR (90 dias e 1 ano) e MCCR-PH (1 ano) foram os únicos com valores de ΔE maiores que o limite de aceitabilidade. Todos os demais grupos mantiveram seu ΔE menor que o limite de aceitabilidade ao final de 1 ano de armazenamento em água destilada. Em relação ao grau de conversão, não foram observadas diferenças estatisticamente significantes entre os materiais para cimentação avaliados ($p=0,127$). O grau de conversão variou entre 64,0% (MNCR-PH) e 85,1% (DRC). Correlações negativas moderadas a fortes não significativas foram observadas entre a média ΔE_{ab} e grau de conversão ($R=-0,65$) e ΔE_{00} e grau de conversão ($R=-0,64$). Observou-se uma correlação positiva forte significativa nos valores médios de ΔE_{ab} e ΔE_{00} ($R=0,99$). Pode-se concluir que os diferentes agentes cimentantes utilizados na cimentação de

laminados cerâmicos de espessura fina influenciaram na cor final das restaurações. O aquecimento das resinas compostas não implicou em alteração do grau de conversão.

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