

Connectivity-Based Parcellation: Critique and Implications

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Abstract: Regional specialization and functional integration are often viewed as two fundamental principles of human brain organization. They are closely intertwined because each functionally specialized brain region is probably characterized by a distinct set of long-range connections. This notion has prompted the quickly developing family of connectivity-based parcellation (CBP) methods in neuroimaging research. CBP assumes that there is a latent structure of parcels in a region of interest (ROI). First, connectivity strengths are computed to other parts of the brain for each voxel/vertex within the ROI. These features are then used to identify functionally distinct groups of ROI voxels/vertices. CBP enjoys increasing popularity for the in-vivo mapping of regional specialization in the human brain. Due to the requirements of different applications and datasets, CBP has diverged into a heterogeneous family of methods. This broad overview critically discusses the current state as well as the commonalities and idiosyncrasies of the main CBP methods. We target frequent concerns faced by novices and veterans to provide a reference for the investigation and review of CBP studies. *Hum Brain Mapp* 36:4771–4792, 2015. © 2015 Wiley Periodicals, Inc.

Key words: brain parcellation; clustering; resting-state correlations; diffusion MRI; data-driven; statistical learning; statistical inference; double dipping

INTRODUCTION

The human brain is commonly assumed to be organized in distinct modules [Brodman, 1909; Vogt and Vogt, 1919]. These could be described according to structure,

connectivity, and function. Cortical areas can be conceptualized as patches of the brain that differ from their neighbors in terms of their microarchitecture (e.g., cyto-, myelo-, and receptorarchitecture), connectivity (i.e., set of input and output connections), and function (e.g., lesion-induced behavior or electrophysiological responses) [Felleman and Van Essen, 1991; Van Essen, 1985]. The conjunction of (i) input and output connectivity of a cortical area and (ii) its local infrastructure is thought to crucially determine what classes of computational problems (i.e., function) it can solve [Scannell et al., 1995; Mesulam 1998; Passingham et al., 2002; Saygin et al., 2012].

The correspondence between a cortical area and its axonal connectivity fingerprint has prompted connectivity-based parcellation (CBP) approaches [Behrens and Johansen-Berg,

Correction added on 01 October 2015, after first online publication.

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Received for publication 7 June 2015; Revised 22 July 2015; Accepted 30 July 2015.

DOI: 10.1002/hbm.22933

Published online 27 September 2015 in Wiley Online Library (wileyonlinelibrary.com).

2005; Wiegell et al., 2003]. Capitalizing on the distinct connections of each area [Passingham et al., 2002], CBP divides a region of interest (ROI, i.e., a volume- or surface-based topographical definition) into distinct subregions. The key idea is to first compute a connectivity profile for each individual voxel or vertex in the ROI. The voxel/vertex-wise connectivity profiles are then used to group the ROI voxels/vertices such that connectivity is similar for the voxels/vertex within a group and different between groups. That is, distinct clusters are identified in the ROI by differences between long-range interaction patterns of the voxels/vertices in the ROI. Historically, CBP has first been performed based on whole-brain structural (fiber) connectivity profiles as derived from diffusion magnetic resonance imaging (dMRI) [Behrens et al., 2003; Wiegell et al., 2003]. Later, analogous approaches based on resting-state functional connectivity (RSFC) [Kim et al., 2010] and, most recently, meta-analytic connectivity modeling (MACM) [Eickhoff et al., 2011] have been introduced. On the one hand, previous investigations have demonstrated that CBP can reveal clusters that recover known histological parcellations [e.g., Bzdok et al., 2012; Johansen-Berg et al., 2005]. On the other hand, there are also reports showing that CBP may yield more fine-grained subdivisions than classical cytoarchitectonic mapping [e.g., Clos et al., 2013]. Hence, CBP-derived modules may be viewed as “functional areas,” although these are outlined by connectivity differences rather than function.

The ability of CBP methods to map functional areas led to rapid adoption by neuroimaging investigators [cf. Smith et al., 2013a]. Yet, several circumstances encourage heterogeneity in this nascent field. Methodologically, the CBP procedure is based on practical choices inconsistent across laboratories. Importantly, no single package permitting CBP is, to the best of our knowledge, openly distributed at the moment. Rather, it seems that different research groups perform CBP analyses based on their own script library, in-house databases, and laboratory setups. However, sharing of code implementations and international collaboration on its successive improvement will hopefully contribute towards a widely accepted software infrastructure [cf. Pradal and Varoquaux, 2013].

Challenges that typically arise in CBP studies will be discussed in different sections. We will start out with the purpose of CBP and the neurobiological conclusions that can be drawn from it. The subsequent sections deal with the initial, interrelated decision on the ROI definition and the connectivity aspect to be investigated. We will then outline the main clustering approaches and corresponding cluster-selection criteria. The ensuing CBP results frequently raise questions around statistical inference and double dipping, discussed in later parts of the manuscript. We finally reflect possible ways to capitalize on CBP results as a starting point for multi-modal studies. All these issues are discussed below by providing overview, potential pitfalls, and possible solutions aimed at neuroimaging novices and experts. We

hope that these considerations may ultimately help unify the dynamically developing spectrum of CBP methods.

MOTIVATION

Aim

The principle of brain segregation guided by long-distance connections can be attractive from different perspectives, including the investigation of local functional differentiation, the creation of data-driven brain atlases, and catalyzing the inception of unprecedented hypotheses.

Location mapping

Comparing to other current neuroimaging approaches, CBP has the key strength to actually map distinct brain areas. This can be opposed to either localizing a particular (dys)function or characterizing a particular region. Most whole-brain association studies, be it functional MRI, voxel-based morphometry, lesion mapping, or most resting-state connectivity analyses, primarily elucidate the location in the brain of a particular effect such as the recruitment by a particular task, a differential response between two conditions, a difference between two groups, or the association with a particular phenotype. They are mapping cognitive, behavioral, and clinical aspects onto the brain. They do however not allow constructing a map from the brain itself (cf. Amunts et al., 2014). Put differently, most neuroscientific methods associating behavior with aspects of neurobiology are naïve to underlying neurobiological compartments. While observing mappings between behavior and the brain, these methods are not well suited to establish or question the architecture of the brain itself [Frackowiak and Markram, 2015]. That is, rather than providing a map of the brain, they provide a map of a particular functional or structural feature (such as recruitment by a particular task or aberrations in a particular group of patients) in brain space. The potency of brain-behavior interpretations can however be increased when constrained by knowledge of brain organization units [Devlin and Poldrack, 2007]. CBP can propose such organizational units.

Atlas mapping

CBP methods are capable of automatically compartmentalizing the human brain into topographically delineated, functionally distinct regions [Behrens and Johansen-Berg, 2005]. That is, 3D brain atlases can be obtained as quantitative models of brain segregation. In that context, an atlas represents a map of (parts of) the brain that assigns each location (voxel/vertex) to a particular structure and hence provides a segregation of the assessed volume into distinct modules. In whole-brain CBP, the ROI to be segregated covers the entire gray matter. By evaluating connectivity strengths from each gray-matter voxel/vertex to every other gray-matter voxel/vertex, a compartmental model of

functional organization in the cerebral cortex can be derived. In local CBP, the ROI to be segregated covers a circumscribed part of gray matter. It can thus be evaluated whether that brain patch contains functionally distinct modules. As another important CBP variant, a-priori hypotheses can be introduced by measuring connectivity only to preselected brain regions, instead of the whole brain [e.g., Bach et al., 2011; Behrens et al., 2003; Sallet et al., 2013]. In sum, CBP can readily propose 3D models of brain organization for use as reference atlases.

Hypothesis generation

Many currently employed neuroimaging methods test spatial hypotheses by either localizing effects or characterizing a region, instead of providing explicit hints that encourage novel research hypotheses [cf. Biswal et al., 2010]. CBP may be seen as an approach towards the generation of novel hypotheses on regional differentiation. These can subsequently be tested in hypothesis-driven experimental studies. For instance, exploratory CBP evidence supported existence of distinct subregions in the right temporo-parietal junction [Mars et al., 2012]. This was subsequently confirmed by targeted neuroimaging studies based on cognitive fMRI experiments [Silani et al., 2013], ICA-based experiments [Igelstrom et al., 2015], hypothesis-driven meta-analysis [Krall et al., 2015], quantitative reviews [Schurz et al., 2014], as well as multivariate pattern analysis in clinical populations [Koster-Hale et al., 2013].

Neurobiological Meaning

What does it actually mean to divide the brain based on differences in connectivity profiles? CBP performs a systematic summary of the Cortex cerebri by combining same tissue and separating different tissue according to an organizational criterion, namely, brain connectivity. Analogous to cytoarchitectonic mapping by microanatomical criteria [cf. Brodmann, 1909, pages 5 and 288-290], functional mapping by connective criteria critically depends on the certainty that we have about the divisive criterion.

Cortical areas

From an anatomical perspective of brain segregation [Amunts et al., 2013], cortical areas are believed to be distinguishable from their neighbors by featuring a distinct (micro)structure, distinct connectivity, and distinct function. In fact, function may follow naturally given that structure and connectivity are thought to conjointly enable locally specific neuronal computations [Passingham et al., 2002]. As CBP is based on connectivity (true in a strict sense only for dMRI-CBP, cf. below), the defined clusters are not directly interpretable as cortical areas. Note that the current concepts of what constitutes a cortical area are mainly derived from studies of early sensory [Van Essen et al., 1992] and motor [Rizzolatti et al., 1988] brain sys-

tems. They may not be readily applicable to higher-level associative brain areas [Yeo et al., 2011], such as the dorso-medial prefrontal cortex [cf. Eickhoff et al., 2014]. Indeed, with increasing distance from sensory input processing, it is more and more difficult to relate the connectivity pattern of an area to its functional roles [Bzdok et al., 2013; Bzdok et al., in press; Mesulam 1998; Yeo et al., 2011]. Claims about cortical areas based on CBP results may therefore become more and more delicate with increasing level in the cerebral processing hierarchy.

One single versus multiple parallel subdivisions

From a more methodological perspective of brain segregation, CBP does not address the neurobiological question whether there is a “true” parcellation. It is employed to identify the “optimal” clustering solution, in the sense of best describing the data. It is about the question whether different parcellation results for the same ROI capture different resolutions or dimensions of an underlying neurobiological organization [cf. Amunts et al., 2014; Eickhoff and Grefkes, 2011; Kelly et al., 2012]. The answer depends on the region of interest. For instance, previous CBP work on the insula [Kelly et al., 2012; Nanetti et al., 2009] and the right temporo-parietal junction [Bzdok et al., 2013b; Mars et al., 2012] have indicated close agreement between the parcellations based on different connectivity modalities. In contrast, parcellations of the posteromedial cortex diverged more strongly between dMRI- and RSFC-CBP studies [Cauda et al., 2010; Zhang and Li, 2012; Zhang et al., 2014]. These observations corroborate the relevance of the conceptual differences between aspects of connectivity, such as dMRI, RSFC, and structural covariance. Moreover, there is probably no such thing as “the connectivity” for a particular location. There may neither be “the CBP parcellation”. Rather, brain segregation across connectivity modalities can possibly feature both similarity and dissimilarity.

Multi-modal comparison

Unfortunately, there are yet very few studies that address this fundamental question of brain organization. Such a comparison across connectivity modalities is currently impeded by two key factors. On the one hand, results from previous CBP studies are rather inconsistently available to the community as image files, which renders most attempts to compare findings purely qualitative [Gorgolewski et al., 2015]. On the other hand, there appears to be a sentiment that a new CBP study in an already analyzed brain region is primarily a replication and hence lacking novelty. This discourages additional work on previously parcellated brain regions.

Meaning of CBP clusters

Given the biological and methodological characteristics of the most frequently used anatomical and functional

connectivity measures, we would suggest the following tentative distinction. For dMRI-CBP, the delineated clusters most likely reflect truly connectivity-defined modules, even in light of known artifacts (cf. below). In contrast, MACM-CBP reveals clusters that are probably functionally distinct modules even though the spectrum of brain functions is likely to be larger than what can be probed by neuroimaging techniques [cf. Mennes et al., 2013; Smith et al., 2009]. That is, task-based functional connectivity might be limited by real-world behavior being richer than in-scanner behavior. The neurobiological nature of RSFC-CBP derived clusters might remain most uncertain. This is because the relation of resting-state correlations to anatomical connectivity, function, and the brain's housekeeping physiology is currently only incompletely understood [Biswal et al., 1995; Bzdok and Eickhoff, 2015; Zhang and Raichle, 2010].

The insula

To take a concrete example, previous CBP results match some neurobiological dimensions of the insula, but certainly not all of them (Fig. 1). On a microanatomical scale, investigations classically divided the insula into a rostroventral (agranular), rostradorsal (dysgranular), and caudal (granular) portions in macaque monkeys [Mesulam and Mufson, 1982a]. On a macroanatomical scale, the more rostral insula is preferentially connected to frontal regions, whereas the more caudal insula is preferentially connected to primary and secondary sensory as well as motor regions [Mesulam and Mufson, 1982a,b]. On a developmental scale, anterior-posterior segregation in the human insula becomes observable within the first two years of life, as indicated by RSFC-CBP in infants [Alcauter et al., 2015]. From the perspective of sensory input channels, the insula contains primary gustatory, primary auditory, as well as associative somato- and viscerosensory cortices. On a functional scale, along the caudo-rostral insula, primary interoceptive representation gradually shifts over environmental input representation into highly abstract cognitive representations of self and time [Craig, 2009]. These observations exemplify that an identical ROI may be segmented along diverging features and notions of brain organization.

More globally, it appears that agreement across connectivity modalities decreases when the parcellation becomes more fine-grained. In this context, it is important to appreciate that many brain regions may be described at multiple scales and by multiple notions. It is hence likely that there are several correct answers to the question of a neurobiologically valid parcellation, even when based on a single approach. This has probably best been demonstrated for the insula, subject to repeated CBP analyses [Cauda et al., 2011; Chang et al., 2013; Deen et al., 2011; Jakab et al., 2012; Kelly et al., 2012; Nanetti et al., 2009; cf. also Kurth et al., 2010]. This previous work has shown that the insula may be described by a primary rostral-caudal distinction [cf. Alcauter et al., 2015] as well as a repeatedly reported a triplet of rostroventral, rostradorsal, and caudal portions.

Diverse functional recruitments and more fine-grained parcellation schemes, such as described by Kelly et al. [2012] and Nanetti et al. [2009], should then reflect additional differentiation within these.

Hierarchical level, functional gradients, and completeness

Three further aspects that need to be considered in any neurobiological interpretation of CBP results are hierarchical level, functional gradients, and completeness. (i) Generally, boundaries between brain regions become less clear with increasing abstraction level in the neural processing hierarchy. This is reflected by the fact that the more similar the connectivity patterns of two areas are, the more difficult it is to demonstrate a functional double dissociation by lesion studies [Young et al., 2000]. In a CBP context, particular care and modesty is therefore recommended when investigators interpret functional borders in highly associative brain regions. (ii) Both high- and low-level processing regions in the brain may feature dedicated functional gradients. For instance, the left inferior parietal lobe (i.e., a high-level region) might contain a functional gradient from more person-state- to more person-trait-related processing facets in social judgments [Hensel et al., 2013], while V1 (i.e., a low-level region) contains functional gradients related to retinotopy [Wandell et al., 2007]. Whenever there is previous evidence for functional gradients in a ROI, investigators should be careful not to overstretch the discovered functional mapping. This is because the commonly used clustering algorithms (e.g., *k*-means, spectral, and hierarchical clustering) will impose clear-cut boundaries somewhere along such gradual transition zones. (iii) It is moreover noteworthy that the distinct functional modules identified in a locally circumscribed ROI might extend beyond the boundaries of that ROI (cf. next section).

Taken together, convergence and divergence across parcellation schemes should raise the attention of CBP investigators. It is conceivable that discussing CBP results exclusively by a single parcellation solution of the ROI might entail loss of neurobiological insight. Investigators should treat diverging parcellation solutions (at same and different cluster numbers) as potentially complementary rather than strictly exclusive. Indeed, the insula did feature several stable parcellation solutions in a dMRI-CBP study [Nanetti et al., 2009]. To facilitate more comparison across modalities and CBP approaches, however, the neuroimaging field probably needs increased sharing of CBP parcellations (cf. Poldrack and Gorgolewski, 2014) and more complementary investigations of already examined regions using different connectivity measures and approaches. Put differently, connectivity-derived clusters are primarily descriptions of the data. Meaning of clusters can only arise in the adoption of a neurobiological viewpoint. They do not, however, simply represent 'cortical areas'. Hence, this term should probably be avoided until

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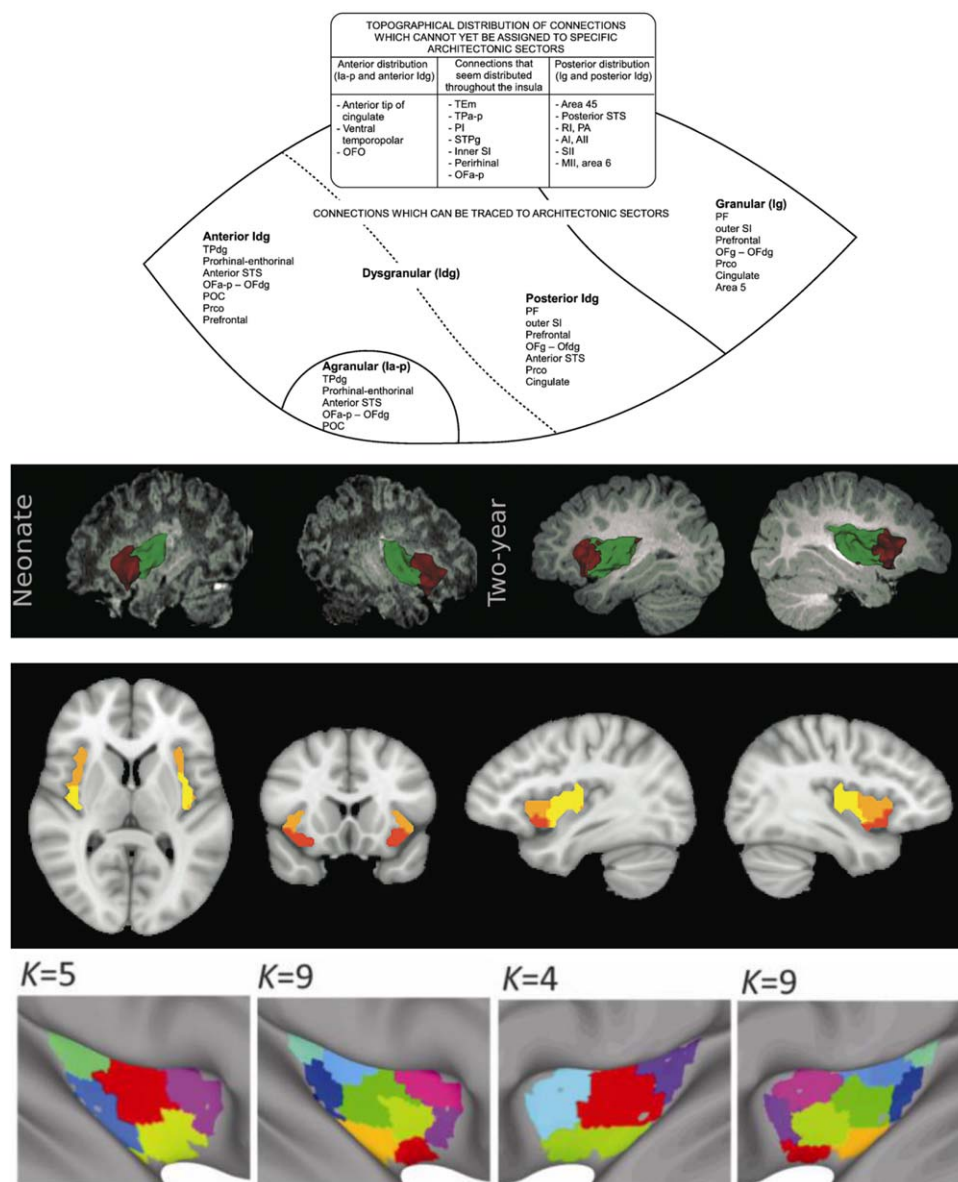


Figure 1.

Different functional segregation models of the insula. From upper to lower panel: (a) depicts a concept of functional segregation in the insula as inferred from connectivity studies by axonal tracing in monkeys [Mesulam and Mufson, 1982b], (b) two-cluster solution of the maturing insula from connectivity-based parcellation of newborn and two-year-old humans based on longitudinal resting-state measurements [Alcauter et al., 2015], (c)

three-cluster solution of the insula of human adults based on resting-state correlations [Deen et al., 2011], and (d) different consensus-cluster solutions of the right and left insula in human adults based on the three connectivity modalities resting-state correlations, task-derived coactivations, and structural covariance [Kelly et al., 2012].

sufficient evidence has been gathered on distinctions from neighboring areas in terms of structural, functional and connectivity-related features. Moreover, clusters in the

associative cortices and those identified in regions with evidence for functional or structural gradients need to be interpreted with particular caution.

PROCEDURE

ROI Definition

The first decision in CBP analyses is on the part of the brain to analyze. The ROI outlines the set of target gray-matter voxels/vertices that the investigator wishes to segregate into subregions. This important step operationalizes the investigation, which strongly impacts the overall outcome and interpretation of the study.

Whole-brain CBP

As the perhaps most intuitive choice, the ROI may comprise the entire gray matter in the aim of whole-brain parcellation [e.g., Craddock et al., 2012; Shen et al., 2013; Thirion et al., 2006b; Thirion et al., 2014; Yeo et al., 2011]. A ROI with all voxels/vertices in gray matter can for instance be drawn from the ICBM tissue map (International Consortium on Brain Mapping) at a gray-matter probability of choice [e.g., Bzdok et al., 2013b], from gray-matter segmentation [Fischl et al., 2004], as well as from the MNI [Evans et al., 1992] or Talairach and Tournoux [1988] template spaces. Importantly, it might not always be the most attractive option to group the brain in voxel or vertex units. Single voxels/vertices can hardly be interpreted by themselves [cf. Chumbley and Friston, 2009]. Additionally, operating in a voxel/vertex space can make clustering procedures computationally expensive. Rather than voxel/vertex-level clustering, whole-brain parcellation lends itself to node-level clustering. That is, not individual voxels/vertices but predefined groups of voxels/vertices (i.e., nodes) are the units that are grouped as a function of connective similarity [Smith et al., 2013b]. Note that the nodes represent voxel/vertex combinations based on previous knowledge that can, for instance, be derived from ICA or structural atlases. Constructing nodes as an alternative unit of observation is therefore not itself an instance of clustering. An advantage of performing a connectivity-based grouping of nodes covering the brain's gray matter relies in the increased neurobiologically interpretability. This is because these nodes are often created based on neurobiological features, whereas a single voxel/vertex does usually not allow a one-to-one mapping of salient neurobiological properties. For instance, using each region of the default-mode network as nodes allows finding node clusters that represent functionally distinct subnetworks (Amft et al., 2014; Andrews-Hanna et al., 2010). Such node definitions can be called hard (i.e., one single shape) or soft (i.e., several slightly different shapes dependent on occurrence likelihood) (Varoquaux et al., 2013). Concretely, subregions from hard ROI clustering are typically nonoverlapping, whereas subregions from soft clusterings can typically be overlapping. Frequently used hard brain nodes include cytoarchitecture (Brodman, 1909) and AAL (Tzourio-Mazoyer et al., 2002), while frequently used soft brain nodes include the probabilistic

atlases from Jülich (microanatomical) and from Harvard-Oxford (macroanatomical). As a more data-driven variant of whole-brain parcellation, sets of coherent functional nodes can be obtained by (spatial) independent component analysis (ICA; Beckmann et al., 2005; Malherbe et al., 2014; cf. below). Yet, note that the optimal conceptualization of a "node" is unclear and the practical choice is a matter of debate (Zalesky et al., 2010). A whole-brain atlas of functional nodes can also be learned directly from RSFC data of multiple subjects in a probabilistic hierarchical model [Varoquaux et al., 2011]. Among whole-brain CBP approaches, one might further distinguish 3D-volume-based parcellation (most studies cited in this paper) and surface-based parcellation [e.g., Blumensath et al., 2013; Gordon et al., 2014; Yeo et al., 2011]. Further, whole-brain parcellations, be it based on individual gray-matter voxels/vertices or preset voxel/vertex groups as nodes, enjoy increasing popularity. Whole-brain CBP might be particularly important for current and future high-throughput projects in neuroscience (e.g., the European Human Brain Project [HBP], the international Human Connectome Project [HCP], the American Brain Research through Advancing Innovative Neurotechnologies [BRAIN]) [a very good overview is given in Poldrack and Gorgolewski, 2014].

Regional CBP

In contrast to whole-brain CBP, the majority of existing CBP studies used a ROI that outlines a circumscribed part of the brain. The underlying motivation typically relates to a test of functional heterogeneity. Note however that whole-brain CBP provides individual clusters that can each be used as circumscribed ROI. Practically, cluster from whole-brain CBP studies can subsequently serve as targets for local regional CBP studies. One can distinguish between anatomical and functional ROIs. An anatomical ROI can be constructed in a straightforward fashion by manually outlining macroanatomical landmarks guided by gyri, sulci, ventricle borders, or white matter [e.g., Anwander et al., 2007; Beckmann et al., 2009; Mars et al., 2011; Solano-Castiella et al., 2010]. One might note three relevant aspects. First, this type of ROI definition may be limited by the fact that sulcal/gyral boundaries do not always coincide with functional boundaries [Amunts et al., 1999; Zilles et al., 1997; in contrast to Weiner et al., 2014]. Intentionally extending the ROI may therefore be an attractive option (cf. below). Second, these gross anatomical features can be subject to considerable inter-individual variability [Kochunov et al., 2010]. This encourages region delineation on a single-subject basis. The presence or absence of the paracingulate sulcus may, for instance, not be captured by an automated group-level procedure [cf. Beckmann et al., 2009]. Third, manually defined ROIs might be thought of as more subjective by some authors. While the ensuing CBP studies could suffer from poor reproducibility, a completely automatic method is however no guarantee for better results (cf. below). Note that all three presented caveats

are controversial in the literature. As a frequently used alternative, macroanatomical ROIs may be based on probabilistic maps such as, e.g., provided by the Harvard-Oxford atlas (<http://fmrib.ox.ac.uk/fsl/>) or constructed by automatic segmentation [Fischl et al., 2004]. Both strategies have frequently been employed in previous CBP studies [e.g., Bach et al., 2011]. Such maps provide objective and reliable masks reflecting the location of a particular structure in a group of subjects that contrast investigator-guided or hand-drawn ROI definitions. Microanatomical ROIs, in turn, represent an attractive alternative because regional heterogeneity of histological features, such as cytoarchitecture (Zilles and Amunts, 2010), is a likely indicator of regional specialization. Such probabilistic cytoarchitectonic ROIs have already been used for CBP studies [e.g., Bzdok et al., 2012; Johansen-Berg et al., 2005]. It is however important to appreciate that cytoarchitectonic areas exhibit often marked inter-individual variability and hence may not map well to the corresponding regions of an individual subject following standard-space alignment. Consequently, the resolution of any CBP analysis can only be as accurate as permitted by the preceding realignment procedures. In summary, when using an anatomical ROI, the ensuing CBP analysis addresses the question whether a particular (macro- or microanatomical) structure contains subregions featuring distinct connectivity. More specifically, CBP performed on microstructural ROIs then yields modules that are defined by a particular structure (due to the ROI definition) and connectivity (due to the CBP logic) and may therefore be more likely to represent actual functional units in the brain.

Contrary to anatomical ROIs, neuroimaging researcher sometimes use alleged neuroanatomical terms to predominantly denote a certain function rather than a certain location. Examples for such “pseudo-anatomical” regions that often have a rather coarsely defined or even disputed relationship to structural anatomy would be the “fusiform face area” [cf. Kanwisher et al., 1997], “frontal eye field” [cf. Grosbras et al., 2002], and “temporo-parietal junction” [cf. Mars et al., 2012]. When interested in such region, a functionally defined ROI might be the preferred approach. It is possible to use the results of a single fMRI study. In its simplest form, it could be defined by voxels/vertices activated by one or more fMRI tasks. Yet, the functional definition would be highly specific to the respective experimental setup. A principled approach to create a functional ROI from experimental fMRI that acknowledges inter-subject variability is known as functional localizers [Friston et al., 2006; Fox et al., 2009; Saxe et al., 2006]. Originally, this approach used a separate neuroimaging experiment performed to constrain both analysis (i.e., increasing sensitivity) and interpretation of the actual study. If inter-subject variability is not of interest, it can be an attractive option to consolidate the location of the functional process of interest by means of quantitative image-based [i.e., using whole-brain activation maps; Dehaene

et al., 2003; Schilbach et al., 2008] or coordinate-based [i.e., using peak activation information; Eickhoff et al., 2009; Radua and Mataix-Cols, 2009; Wager et al., 2007] meta-analysis. The resulting ROI would then statistically constrain the most robust location of activation convergence underlying the process of interest across various subjects, study designs, and laboratories. In either case, CBP will address the heterogeneity of connectivity patterns within this functionally defined region. This becomes particularly interesting when ROIs are defined by (partially) overlapping activation blobs from experimental neuroimaging studies [Cieslik et al., 2013] or meta-analyses summarizing different functions [Bzdok et al., 2013b] that are located in closely neighboring yet potentially different locations. In cases where a ‘composite’ functional ROI is used, CBP allows answering a new type of question: ‘Are the different cognitive processes reflected by the different activations or meta-analyses related to the same or different connectivity-defined modules in the human brain?’ Note that this is not circular even if CBP always locates subregions in the ROI. This is because cluster validity criteria may provide evidence that all obtained cluster solutions are instable and therefore not neurobiologically meaningful. Such judgments should be weighed against external knowledge. CBP with composite ROIs has hence the potential to reconcile controversies in cognitive neuroscience. For instance, the one-module versus mosaic-modules debate for the temporo-parietal junction [Decety and Lamm, 2007; Mitchell, 2008] has probably been resolved by repeated demonstration of functionally distinct subregions using CBP [Bzdok et al., 2013b; Mars et al., 2012].

ROI borders

As an important consideration in CBP studies, the outside borders of the nonwhole-brain ROI are not tested or validated. They will hence be taken as borders of the ensuing clusters. A thorough motivation of why and how these outside boundaries are defined is pertinent to any CBP study. In turn, if the localization of a particular module is the primary interest of an investigation, it is advisable to dilate the ROI to include sufficient coverage of the neighboring cortex, allowing for additional clusters around the volume of primary interest. That is, CBP may find all borders of the main regions of interest by including neighboring regions of no or limited interest [cf. Muhle-Karbe et al., 2015; Sallet et al., 2013]. In principle, if the ROI extends only a little beyond the ground-truth area(s), only a neglectable amount of noise should be introduced into the cluster estimation. If the ROI extends beyond the ground-truth area(s) to extended parts of areas of no interest, then new clusters (of no interest) emerge that delineate the cluster(s) of interest. As an extreme scenario, if the ROI is incorrectly defined, interpretation of the clustering results becomes challenging to impossible.

In sum, different ways for anatomical or functional definitions of a ROI for CBP have been used and are legitimate. This choice and its operationalization should be well motivated. Generally, population or meta-analysis based ROIs are an alternative to hand-drawn ones or those that are based on a single-subject data (e.g., AAL). In principle, microanatomical ROI definitions can be preferable to macroanatomical ones. In case of lacking neuroanatomical consensus for the target region in the literature of interest, a functionally motivated ROI suggests itself. A functional ROI can be constructed from neuroimaging studies or activation convergence quantified by meta-analytic methods. Finally, “composite” ROIs allow answering the specific question how a particular set of findings relate to regional specialization. Apart from that, if the aim is whole-brain parcellation, voxel/vertex-level CBP does less crucially depend on the ROI definition, while node-level CBP currently suffers from uncertainty about the most biologically valid reduction to network nodes and about methodological biases incurred by node choice [Zalesky et al., 2010]. As a consequence, the motivation of the CBP study should be consolidated before selecting the preferred ROI. This is because the location and type of ROI explicitly frame the scientific question and motivation underlying a CBP study. Consequently, the initially selected ROI constrains the spectrum of permissible conclusions from the later CBP results. Critically, the decision on the ROI should be taken hand-in-hand with the connectivity data of interest. This is because the underlying neurobiological question should guide methodological choices.

Measures of Brain Connectivity

Note that the concepts underlying CBP are not bound to a particular connectivity approach. Any method can be employed that yields a connectivity profile for each voxel/vertex in the ROI. In general, the anatomical connectivity modality most frequently used for CBP-analyses is dMRI [e.g., Anwender et al., 2007; Behrens et al., 2003; Johansen-Berg et al., 2004]. The functional connectivity modality in most frequent use is RSFC [e.g., Cauda et al., 2010; Kim et al., 2010; Zhang and Li, 2012]. It has recently been complemented by MACM [e.g., Bzdok et al., 2012; Eickhoff et al., 2011], which is rapidly gaining usage in the field. As an alternative to anatomical and functional connectivity, structural covariance [Evans, 2013] has been used in a small number of CBP studies [e.g., Kelly et al., 2012; Wang et al., 2015]. We do not cover the latter in the interest of simplicity and space. It is important to appreciate that all these measures of connectivity strength reflect drastically different ways to conceive and quantify interneuronal communication between brain regions. Choosing one of them is as important as the ROI selection and has far-reaching implications for the interpretation of the identified clusters. At this point it might be helpful to reiterate that it is not the individual connectivity profiles of the

voxels/vertices that drive the parcellation but only the differences between those.

Diffusion MRI

Anatomical connectivity between brain regions can be measured (or rather approximated) using diffusion magnetic resonance imaging. It delineates the likelihood of white-matter fiber bundles traced to link brain regions [Johansen-Berg and Rushworth, 2009; Jones, 2008]. The number of samples reaching any voxel/vertex in the gray matter or, more frequently, the likelihood of passing through brain white matter then provides the connectivity profile of a particular voxel/vertex or node in the ROI. In fact, in whole-brain CBP dMRI is seeded from every gray-matter voxel/vertex. In local CBP every voxel/vertex in the circumscribed ROI is a seed, while in node-level CBP voxel/vertex groups are seeds (goes for all three connectivity modalities). DMRI tractography is evidently closest to the notion of structural connections. Yet, it does not actually capture axonal connections as classically identified by axonal tracing studies in monkeys (cf. Mesulam, 1978). Caveats of tractography include (i) the dominance of large fiber bundles, thus omitting sharply curved or very long fiber bundles, which precludes exhaustive assessment of all connections [Ng et al., 2013; Jbabdi and Behrens, 2013] as well as impaired detection of (ii) poorly myelinated or (iii) closely neighboring (“kissing”) connections. Finally, dMRI can neither precisely delineate cortical origin nor cortical termination of fiber bundles [Petrides et al., 2012].

Resting-state functional connectivity

Alternatively, functional connectivity can be measured by resting-state correlations under the assumption that the coupling strengths between distant brain regions is measurable by correlation between time series of BOLD signal fluctuations outside of an experimental context [Biswal et al., 1995; Buckner et al., 2013; Zhang and Raichle, 2010]. It quantifies the correlative relationships between distant brain regions in subjects idling in the MRI scanner. This is possible because interneuronal communication continues and is reflected by ongoing physiological fluctuations in the absence of an experimentally imposed cognitive set, i.e., during natural mind wandering, which can be measured using fMRI [Bzdok and Eickhoff, 2015]. While RSFC signals have been shown to recover well-documented axonal connections and functional networks, there is an increasing awareness that much of the observed signal may be influenced, if not distorted, by physiological sources (but see Hipp and Siegel, 2015). The ensuing conundrum may challenge the interpretation of brain-behavior relationships discovered by RSFC. Despite initial skepticism, the consistency of RSFC results has been demonstrated repeatedly across subjects, brain scans, time points, and other factors [Damoiseaux et al., 2006; Shehzad et al., 2009]. RSFC thus provides proxies of dynamic neuronal

interactions that might reflect mixtures of various cognitive processes and physiological factors [Smith et al., 2009; contrasted by Mennes et al., 2013].

Meta-analytic connectivity modelling

Meta-analytic connectivity-modeling, in turn, operates under the assumption that functional connectivity between brain regions should entail reliable coactivation [Robinson et al., 2010; Toro et al., 2008]. It quantifies correlative increase/decrease of neural activity in distant brain regions throughout various experimental paradigms. This connectivity modality capitalizes on the increasing trend for large-scale data aggregation, exemplified by Neurosynth [Yarkoni et al., 2011], BrainMap [Fox and Lancaster, 2002], and NeuroVault [Gorgolewski et al., 2014]. Caveats of MACM include (i) reliance on very sparse activation information (i.e., peak coordinates of significant activation), which might entail missing information and biased sampling, (ii) inability of subject-specific connectivity analysis, and (iii) inheritance of the limitations from experimental neuroimaging studies. In spite of these limitations, the analysis of coactivation likelihoods represents a complementary approach by focusing on the interactions during the performance of externally purported tasks.

Commonalities and differences

Several aspects are of note when choosing between anatomical and functional connectivity modalities in a CBP study. None of the three introduced connectivity modalities provides axonal connectivity in stricto sensu (as gleaned from tracing studies in monkeys). dMRI and RSFC are task-unconstrained (i.e., task-independent) as opposed to task-constrained (i.e., task-dependent) MACM. While dMRI is a measure of anatomical or structural connectivity by assessing white-matter trajectories, RSFC and MACM identify temporal coincidence of neural signals in gray matter, that is, functional connectivity. MACM builds on experimental fMRI and PET studies motivated by cognitive theory (i.e., interventional, capturing metabolic changes in the brain caused by manipulation of environmental variables), whereas participants simply lie still during RSFC and dMRI measurements (i.e., observational, capturing baseline brain features without controlled environmental modulation). It may also be noted that none of these methods can distinguish between involved neurotransmitters (i.e., excitatory versus inhibitory neuronal modulations) or ask whether a connection is stronger in one direction (i.e., “undirected” connectivity). Moreover, we also need to point out that functional connectivity between two regions may be mediated by a third region. That is, RSFC and MACM (but not dMRI) may be driven by indirect connections. This could however be alleviated by computing partial correlations, which is closer to direct interaction by summarizing conditional independences [Marrelec et al., 2006]. In fact, regression-based estimators,

such as dictionary learning [Lee et al., 2011], instead of standard clustering approaches, may be more robust to the issue of third-party influences. Additionally, RSFC and MACM are generally more sensitive in delineating existing connections but more prone to false positives, whereas dMRI is generally less sensitive with frequent false negative results [cf. Jbabdi and Behrens, 2013]. Contrarily to RSFC and MACM, the accuracy of dMRI tract tracings decreases with the distance between the considered regions. Only dMRI- and RSFC-CBP can be conducted in individual subjects [Anwander et al., 2007; Kim et al., 2010]. dMRI- and RSFC-CBP thus enable detecting inter-individual differences in regional functional organization, while MACM-CBP inevitably generalizes across various inter-individual variability sources in the sampled subject population. As an important consequence, dMRI and RSFC can readily parcellate individual brains and infer group aggregates based on between-subject variance. Contrarily, MACM is constrained to aggregating group-level statistics from meta-analytic experiment databases. Hence, MACM-CBP may provide information on the functional parcellation of a region of interest across many experiments, which often shows remarkable congruency with parcellations derived from other modalities, but does not allow any individual, subject-specific parcellation. Taken together, dMRI, RSFC, and MACM grasp different features of connectional brain organization and imply different limitations and promises.

Anatomical and functional connectivity measures are all equally valid for assessing connectivity strengths to perform CBP. dMRI, RSFC, and MACM all lend themselves to whole-brain, node-level, and local CBP. It is important, however, to remember that they are based on fundamentally different concepts of “brain connectivity”. Roughly, dMRI is most “structural/physiological” in nature, whereas MACM is exclusively “functional/psychological”. RSFC, in turn, most likely reflects a mixture of both (with a different set of physiological confounds). These considerations may guide the choice of the employed method when the motivation particularly relates to either functional or anatomical questions. Their different limitations and promises might yield conflicting views on the organization of the ROI, even though first comparative studies show a fairly close convergence [Kelly et al., 2012; Wang et al., 2015]. Nevertheless, exploiting distinct connectivity modalities is likely to extend the space of questions that we can ask about functional brain organization.

Clustering Techniques

Clustering uses a similarity measure to group a set of elements into subsets according to their measured similarity. In CBP, the clustering algorithm groups the voxels/vertices/nodes in the ROI into subsets according to similarity of their connectivity profiles, the heart of any CBP approach. As a result of the so-called ‘no free lunch’

theorem [Wolpert, 1996], no clustering algorithm performs optimally for all ROIs, types of connectivity information, and study motivations. Rather, methods such as k -means, spectral, and hierarchical clustering have all been frequently employed in CBP studies. While these three clustering algorithms have been used for voxel/vertices-, node-, and whole-brain-level CBP, ICA and boundary detection are popular alternatives for brain parcellation. We will detail in this section how these algorithms behave in theory and in neuroimaging practice.

K-means

The probably most popular choice in neuroimaging is *K-means clustering* [Lloyd, 1957; Forgy, 1965; Jain, 2010], a *partitional* approach. It divides a ROI into a preselected number of k nonoverlapping clusters [Nanetti et al., 2009]. In neuroimaging practice, k -means seems to perform best when the subregions in the ROI are expected to be (i) few in number, (ii) of similar size, and (iii) featuring a roughly spherical shape on spatially correlated voxel/vertex/node-wise connectivity [cf. Jain, 2010]. Additionally, k -means clustering will converge in the majority of the cases (i.e., seldom early stopping by the tolerance parameter). In a CBP context, the same connectivity data can describe not only one but several stable solutions in ROI parcellation at the *same* preset k (i.e., low reproducibility), such as observed in the human insula [Nanetti et al., 2009]. Consequently, the algorithm is conventionally applied many times since k -means fits idiosyncracies in data that may generalize poorly across subjects. As a first practical consequence, the initialization of the cluster centers (cf. Box 1) can be random [Hartigan and Wong, 1979] or based on prior knowledge (e.g., anatomical properties). As a second practical consequence, the ‘final’ solution can be obtained by an averaging procedure or by selecting the centroids from the best solution [cf. Nanetti et al., 2009]. Further, the solutions for different selections of k (i.e., different number of clusters) are independent of each other. Repeating the clustering at different k ’s does not emulate a hierarchical approach (contrary to hierarchical clustering). That is, the solutions for ROI parcellation at each level (k) are independent of the others, which makes parent-children stratifications possible but by no means necessary. As an attractive k -means variant that addresses the multi-scale nature of brain organization, investigators can first identify the best fitting k clusters and then test for further separability of each obtained cluster individually [Neubert et al., 2014].

Spectral clustering

One of the first clustering methods in the context of CBP [Johansen-Berg et al., 2004] has been spectral clustering [Donath and Hoffman, 1973; von Luxburg, 2007]. It can be useful to semi-quantitatively obtain a possible number of clusters by inspection [e.g., Bzdok et al., 2012; Johansen-Berg et al., 2004]. Alternatively, when applying an ordinary clustering algorithm, spectral clustering is able to

capture clusters that have complicated shape and are discontinuous, yet that are enforced to be roughly equally sized [Craddock et al., 2012; von Luxburg, 2007]. Note that the clustering solutions for different cluster numbers are not hierarchically consistent (analogous to k -means, contrary to hierarchical clustering). That is, nestedness of the resulting partitions of the ROI are not methodologically enforced but might still appear as a biological property of the ROI under study. Spatially constrained spectral clustering appears to be stable in capturing connectional similarity features between ROI voxels/vertices/nodes (i.e., high reproducibility). It might however not accurately represent those [i.e., poor model fit, Thirion et al., 2014]. In CBP, spectral clustering might be disfavored by some investigators because it strives to enforce simple structure not naturally present in the brain. In particular, as the potentially biggest drawback of spatially constrained spectral clustering, it imposes a strong spatial structure on the data, which thus precludes capturing such structure in the data [Craddock et al., 2012]. As a practical consequence, the more difficult one expects the clusters to separate (e.g., high-level associative brain regions), the more other clustering algorithms should be preferred.

Hierarchical clustering

In contrast to the above-mentioned partitional algorithms, hierarchical clustering [Johnson, 1967] represents an agglomerative (i.e., bottom-up) approach that may reveal connectional similarities at various coarseness levels [Eickhoff et al., 2011]. Here, each individual voxel initially represents a separate cluster. These are then progressively merged into a hierarchy by always combining the two most similar clusters. Divisive (i.e., top-down) hierarchical clustering operates in the opposite direction (start with one cluster, end with one cluster per voxel/vertex/node), but is seldom used in neuroimaging CBP. The investigator does not need to specify a cluster number because an organizational hierarchy is generated that allows for a functional-connectional multi-level stratification of the ROI. This introduces the advantage of a nested hierarchical solution of ROI parcellations (i.e., enforced parent-children relationships between clustering solutions with different cluster numbers) at the price of large result quantities. There are, however, at least three important drawbacks associated with hierarchical clustering. First, hierarchical clustering is very sensitive to effects in local neighborhoods, which can have a substantial effect on the higher-level solutions in noisy data such as in neuroimaging. Second, the output evidently depends on the investigator-chosen linkage algorithm, i.e., the rules how clusters are combined. This can be remedied by imposing the additional constraint of merging only spatially neighboring clusters, which tends to be better behaved [Thirion et al., 2014]. More specifically, as a both biologically plausible and greedy (i.e., exploiting computationally convenient simplification) variant, spatially constrained hierarchical clustering merges/divides only

Box 1**Synopsis of clustering algorithms used for CBP****K-means Clustering**

This clustering approach depends on free parameters, including (i) the cluster initialization, (ii) the cluster number k , and (iii) the tolerance for iteration stopping. Initially k voxels/vertices in the ROI are randomly chosen to represent the centers of the k desired clusters. Two steps are then iterated multiple times. First, the ROI voxels/vertices/nodes are assigned to the closest cluster center (i.e., “centroid”), which equates with partitioning the ROI into k clusters. Second, the k cluster centers are recomputed. As soon as the center needs to be shifted by less than the preset distance threshold, the iterative process stops. Note that the final assignments of ROI voxels/vertices/nodes to particular clusters may vary with different cluster initializations and yield nonoptimal solutions at local minima. The same connectivity data may thus result in several stable solutions for the ROI parcellation at the same preset k (i.e., low reproducibility), as shown, for instance, in the human insula [Nanetti et al., 2009]. Consequently, the algorithm is usually repeated many times.

Spectral Clustering

It is based on a similarity matrix quantifying the similarity of the connectivity profiles between any pair of voxels/vertices/nodes within the ROI. The first eigenvectors of the (normalized) Laplacian of the similarity matrix are computed. Those then enable transformation into an alternative data representation in a space with reduced dimensionality as the eigenvectors “summarize” features of the similarity matrix. The output of this data transformation can then be used for either (i) spectral reordering or (ii) an ordinary clustering algorithm. Spectral reordering uses the reduced similarity information to reorder the similarity matrix in such manner that voxels/vertices/nodes that are similar to each other are grouped together [Barnard et al., 1995]. This can be useful to semi-quantitatively obtain a possible number of clusters by eye inspection [e.g., Bzdok et al., 2012; Johansen-Berg et al., 2004]. Note that hierarchical consistency across solutions for different cluster numbers is not methodologically enforced. That is, voxels/vertices/nodes may be assigned to a different cluster when looking for instance at the clustering solutions with 3 or 4 clusters.

Hierarchical Clustering

Each individual voxel/vertex/node initially represents a separate cluster. These are then progressively merged into a hierarchy by (a) always combining the two most similar clusters (i.e., bottom-up) or (b) always dividing the least homogenous cluster (i.e., top-down) in every step. The algorithm implicitly walks through different choices of cluster numbers as these approaches generate a hierarchy that allows for a nested multi-level parcellation of the ROI, even if only few of those are interpreted in practice. Such successive clustering trees introduce the advantage of a nested hierarchical solution of ROI parcellations (i.e., enforced parent–children relationships between clustering solutions with different cluster numbers) at the price of large result quantities. Even if this clustering model reflects current views on the hierarchical organization of the brain, a given hierarchical clustering result is not necessarily neurobiologically valid.

immediately neighboring clusters. Unfortunately, different linkage algorithms tend to yield different solutions. Finally, there is a tendency for (nonspatially constrained) hierarchical clustering to yield very imbalanced cluster sizes. In the extreme case, one after one voxel/vertex/node is added to a group containing all other ones. This clustering algorithm should be preferred when expecting many clusters (contrarily to k -means). Depending on the merging heuristic, it can however be quite computationally expensive (e.g., complete clustering). Hierarchical clustering captures well the proper-

ties of the connectivity differences (i.e., high accuracy) but its solutions may be inconsistent (i.e., low reproducibility, like k -means). As a rule of thumb, accuracy and reproducibility tend to be mutually exclusive across clustering algorithms.

Distance measures and linkage algorithms

We would like to emphasize that neuroimaging data are typically noisy (due to intersubject variability, technical

limits, etc.) and smooth (due to Gaussian filtering). Consequently, standard *k*-means, spectral, and hierarchical clustering often find spatially contiguous clusters, although this is not immanent in the respective algorithms. While these considerations take place in the *brain space*, it is important not to confuse it with the *feature space*. Distance in brain space pertains to the spatial spacing (in, e.g., mm or voxels) between the units to be clustered, whereas distance in feature space pertains to abstract similarity metrics between connectivity measurements. The process of combining voxels/vertices/nodes in the ROI to connectionally homogeneous clusters (i.e., operating in brain space) is strongly influenced by the employed distance measure and linkage algorithm (i.e., operating in feature space) [Hastie et al., 2011]. On the one hand, distance measures represent the similarity criterion for pairs of connectivity profiles [cf. Handl et al., 2005; Jain, 2010]. These include the (a) Euclidean distance (i.e., squared difference between respective connectivity values; a special case of Minkowski metric at $P = 2$), (b) correlation distance (i.e., Pearson's correlation of the connectivity profile vectors), and (c) cosine distance (i.e., one minus the cosine of the included angle between connectivity profile items, acts as normalization). For cosine distance, subtraction of the coefficient from 1 yields a proper distance metric. It can be advantageous in the presence of outliers. If the connectivity data are known to be particularly noisy. It can be advantageous to use cosine/correlation distances or ranked variants of the above distances (i.e., by using Spearman's rather than Pearson's correlation) to improve resistance to outliers. On the other hand, the linkage algorithm guides how the measured distances are used to evolve clusters [cf. Stanberry et al., 2003; Timm 2002]. The linkage dictates how voxels are combined to clusters based on the computed distance measures. It can be a) "weighted" (weighting average distances, defined in various ways in the literature), (b) "average" (not weighting average distances; mean between all connectivity values in a first cluster to all connectivity values in a second cluster), and (c) "ward" (replaces distance measures to the minimization of intra-cluster variance) as well as d) "single" (i.e., shortest distance, often produces skewed solutions, i.e., "chaining phenomenon by always adding the respective next closest element with heterogeneous overall clusters), and (e) "complete" (maximum distance, tends towards compact clusters, less preferred for noisy data). The best linkage method obviously depends on the data properties. Some combinations of distance measure and linkage seem to be better than others. For instance, when using Euclidean distance the ward linkage seems robust to outliers in noisy data. For different distance/linkage choices, the hierarchical clusters can also find spatially contiguous clusters at a similar rate as *k*-means.

Alternative clustering procedures

While *k*-means, spectral, and hierarchical clustering algorithms are used in various parcellation scenarios, ICA and

boundary detection serve very similar goals in whole-brain parcellation. ICA is an iterative, nonclosed-form solution to blind source separation [Hyvarinen, 1999]. Applied to fMRI data, it is known to separate out stable, statistically independent, and possibly overlapping spatial activation patterns. Note that the time courses of the nodes of each extracted brain "network" are identical [Beckmann et al., 2005; Smith et al., 2009]. As a first conceptual point, this makes ICA a viable instance of connectivity-based parcellation of functional brain imaging data. As a second conceptual point, ICA is an instance of soft clustering by allowing solutions of spatially overlapping clusters (contrarily to the three clustering algorithms above). ICA is special in computing generative models of the signal, it may be more noise-sensitive than the above hard clustering algorithms [Smith et al., 2013a], and allows extraction of artifactual patterns from the data (assuming additivity), not possible with the above clustering algorithms or border detection. Such continuous and probabilistic, rather than discrete and binary, clusters also result from different alternative clustering methods in neuroimaging, including multi-subject dictionary learning [Varoquaux et al., 2013], fuzzy C-means clustering [e.g., Cauda et al., 2010], deep neural networks [Bengio, 2009; Plis et al., 2014], and Gaussian mixture models [e.g., Shen et al., 2010]. They share the advantage of extracting stratifications of overlapping patterns. This has limited gain in parcellating ROIs that cover one or very few cortical areas but will be particularly relevant in whole-brain CBP. Indeed, the neurobiological justification for CBP is the connective homogeneity of individual cortical areas. Yet, soft clustering approaches can flexibly represent overlapping neurobiological clusters with more expressive parcellation models [cf. Passingham et al., 2002]. Boundary mapping, on the other hand, reconceptualizes clustering as the identification of transitions between territories of adjacent brain areas [Cohen et al., 2008; Wig et al., 2013; Wig et al., 2014]. High confidence in boundaries (i.e., high "edge probability") indicates good cluster separability, and vice versa. Detected boundaries are interpreted as localized, abrupt changes in connectivity profiles. Boundary mapping has been instrumental in segregating both circumscribed brain regions [e.g., frontal cortex, Cohen et al., 2008; lateral parietal cortex, Nelson et al., 2010] and the entire brain [e.g., Wig et al., 2014]. Given the possibility of generating probability boundary maps (e.g., by Canny edge detection algorithm), edge modeling qualifies as a mixture between hard and soft clustering. All clustering procedures mentioned up to this point can be applied in single-subject and group analysis.

Taken together, spectral clustering, *k*-means, and hierarchical clustering are three multivariate data exploration techniques with frequent use in neuroimaging (cf. Abraham et al., 2014). More globally, each time the investigator chooses a clustering algorithm to be applied on the ROI, he or she accepts a number of implicit or explicit assumptions [Hastie et al., 2011]. Therefore, any clustering algorithm

unavoidably biases the resulting clustering solution with respect to the number, shape, relative sizes, hierarchy, and contiguity of the clusters. Consequently, investigators should resist the temptation to promote their CBP study as “completely model-free,” “purely data-driven,” or “without any assumptions.” Rather, it is important to realize the inevitable assumptions and biases of a clustering algorithm and motivate the choice of a particular one based on the aim of the study, the ROI, and the employed connectivity data [Handl et al., 2005]. Moreover, using different connectional modalities and other imaging modalities, the investigator can provide a valuable cross-confirmation of the clusters’ biological relevance. Cross-species evidence in favor of a parcellation solution might be especially important [cf. Neubert et al., 2014; Ramnani et al., 2006; Sallet et al., 2013].

Statistical Inference and Cluster Number Selection

Inferential versus exploratory statistics

In short, assessing the significance of brain parcellation results is hard. This is particularly true if significant is employed in the strict sense of inferential statistics and not employed in its broader sense of “interesting” or “relevant.” The key problem in wanting to assess statistical significance of CBP results is the requirement of a null hypothesis to test against. Conceptually, a ROI clustering solution would hence be deemed statistically significant if it has a very low probability of being true under the null hypothesis that the investigator seeks to reject. Yet, such a null hypothesis is often difficult to formulate in clustering applications. Instead of inferential statistics, which test for a particular structure in the clustering results, investigators need to resort to exploratory statistics, which discover and assess structure in the data [Efron and Tibshirani, 1991; Hastie et al., 2011; Tukey, 1962;]. While it is true that statistical methods span a continuum between the two poles of inferential and exploratory statistics, comparing the “importance” or “pertinence” of clustering results from a CBP analysis is naturally situated more towards the latter. CBP hence represents an unsupervised statistical learning problem that is conventionally addressed by quantitatively comparing model fit using cluster validity criteria (Table 1). It may therefore be seen as one instance of a current shift in neuroimaging away from classical inferential towards exploratory approaches, put differently, from voxel/vertex-level mappings to more global assessment of model fit or predictive power [cf. Brodersen, 2009; Cox and Savoy, 2003; Naselaris et al., 2011].

Cluster validity problem

From a broader perspective, the “true” shape and number of clusters is unknown for most real-world clustering problems, including brain research. Finding an “optimal”

number of clusters represents an unresolved issue (cluster validity problem) in computer science, pattern recognition, and machine learning [Handl et al., 2005; Jain et al., 1999; Tibshirani, 2001]. This has prompted the development of diverse heuristics (cluster validity criteria) to weigh the quality of the obtained clustering solutions. These are necessary because clustering algorithms will always find sub-regions in the investigator’s ROI, whether these truly exist in nature or not.

Cluster separation criteria

Criteria can be based on the separation between clusters such as the silhouette value (which for each element measures how similar that element is to the other ones in its own cluster, when compared to the nearest clusters) or the inter/intra-cluster distance (which compares the distance between the cluster-centers to the distance between the elements within each cluster). Such criteria reflect the goal of CBP, i.e., to form groups such that voxels/vertices/nodes within a group show similar connectivity, while the connectivity is different between groups. Note however that successively segregating brain connectivity data into clusters tends to result in lower within-cluster and higher between-cluster differences in every step, regardless of the applied clustering algorithm and the chosen cluster validity criterion.

Consistence across parcellations

Criteria can also be based on the consistency across parcellations into a given number of clusters. This set of criteria comprises metrics, including variation of information (VI), the Dice coefficient, normalized (NMI) or adjusted (AMI) mutual information as well as adjusted Rand index (ARI). These kinds of criteria are often used in multi-subject, possibly also within-subject, settings. That is, when a given ROI is parcellated separately in each subject based on dMRI or RSFC information (not possible with MACM-CBP). In such studies, assessing the quality of a particular clustering solution by testing the consistency across subjects has emerged as an important standard. Nevertheless, the same concept has also been applied to test consistency across parameters such as filter size or to evaluate the stability based on procedures such as bootstrapping [i.e., summarizing statistical results across analyses of resampled data drawn with replacement from the dataset; Efron and Tibshirani, 1994].

Consistence across cluster numbers

Criteria can be based on the hierarchical consistency, such as the VI across clustering solutions (e.g., how different is the information contained in a 4-cluster as compared to a 3-cluster solution) or the hierarchy index (what is the proportion of voxels/vertices/nodes that are originating from the dominant parent cluster). These metrics are only

TABLE I. Main characteristics of cluster validity criteria in brain parcellation

Cluster validity criterion	Rationale	Used in previous brain parcellation studies
Across-subject consistency	finds the number of clusters that yields the highest similarity across independent analyses in a number of subjects; this can be done for instance in a cross-validation framework (e.g, leave-one-subject out) or by a split-group approach	Buckner et al., 2011; Liu et al., 2013; Saygin et al., 2011; Solano-Castiella et al., 2010
Across-hemisphere symmetry	computes the percentage of cluster assignments that agree in both hemispheres; can evidently only be performed in paired brain regions outside of the midline	Bzdok et al., 2012; Kahnt et al., 2012
Adjusted Mutual information (MAI)	assesses the similarity between i) the joint distribution of two sets A and B and ii) the marginal distributions of these two sets; it thus weighs how much information is shared between A and B; results in 0 if A and B are independent, in 1 if they are deterministically related; 'adjusted' implies correction for agreement between clusters out of chance (=RAI); it accounts for the fact that the MI is generally higher for two clustering solutions with a larger number of clusters, regardless of whether there is actually more information shared; related to VI	Thirion et al., 2014
Adjusted Rand index (RAI)	in analogy to mutual information, a measure from probability theory to assess the statistical dependence between two clustering solutions; Rand index is a measure of accuracy between two clusterings; 'adjusted' implies the corrected-for-chance variant of the Rand index (cf. MAI); RAI can be an order of magnitude faster than AMI	Thirion et al., 2014
Akaike's information criterion (AIC)	derived from information theory, it finds the best number of clusters by acknowledging the trade-off between goodness-of-fit and model complexity (i.e, number of clusters); it is based on a probabilistic model and a measure of complexity; this penalty for the cluster numbers is aimed at preventing overfitting, yet is independent of the sample size; as it is a relative measure, it judges the absolute quality of the finally selected model	Zalesky et al., 2010
Bayesian information criterion (BIC)	despite many similarities to AIC, BIC is motivated by a Bayesian approach to model selection; it penalizes the model complexity (i.e, number of clusters, =AIC); in comparison to AIC, BIC imposes higher costs on more complex models (i.e, small cluster numbers are privileged)	Thirion et al., 2014
Cramér's V	assesses the statistical correlation between two groups of discrete values (i.e,	Liu et al., 2013; Solano-Castiella et al., 2011

TABLE I. (continued).

Cluster validity criterion	Rationale	Used in previous brain parcellation studies
Dice coefficient	voxel/vertex/node-wise cluster assignments) based on chi-square; put differently, it measures the strength of association between two clustering solutions assesses the similarity between two samples or adjacency matrices; primarily practically justified rather than backed up theoretically; works well in heterogeneous and outlier-prone data; can be used to compare group and single-subject clusterings; can be computed in different ways; it is equivalent to the <i>Jaccard index</i> because there is a monotonic transformation between their scores	Blumensath et al., 2013; Craddock et al., 2012; Shen et al., 2013; Wang et al., 2015
Inter- versus intra-cluster distance ratio	assesses cluster separation by the ratio between the average distance of a voxel/vertex/nodes to its cluster centre and the average distance between the cluster centres; a significantly increased ratio compared to the K-1 solution would indicate a better separation of the obtained clusters	Bzdok et al., 2014; Chang et al., 2009
Percentage of misclassification	assesses cluster assignment by the amount of noise and potentially local effects in the clustering; the average percentage of voxels/vertices/nodes that were assigned to a different cluster compared to the most frequent assignment of these voxels/vertices/nodes; used to compare ways to compute a same or different number of clusters	Bzdok et al., 2014
Percentage of parent-children congruency	assesses cluster topology by how many voxels/vertices/nodes are not related to the dominant parent cluster compared to the solution with K - 1 clusters; counts voxels/vertices/nodes that do not reflect a hierarchical organization; related to hierarchy index	Clos et al., 2013; Eickhoff et al., in press; Kahnt et al., 2012
Silhouette coefficient	assesses cluster separation by measuring how similar that voxel/vertex/node is to voxels/vertices/nodes in its own cluster compared to voxels/vertices/nodes in the nearest cluster; good solutions are those with a higher silhouette value compared to the K-1 solution; this measure of cluster quality is independent of the number of clusters	Bzdok et al., 2014; Craddock et al., 2012; Eickhoff et al., in press; Kannan et al., 2010; Zhang and Li, 2012
Variation of information (VI)	assesses how much knowing the cluster assignment for an item in clustering X reduces the uncertainty about the item's cluster in clustering Y; a linear expression involving mutual information and entropy; is not adjusted for chance (contrary to AMI and ARI); used to compare ways to obtain a same or different number of clusters	Bzdok et al., 2014; Clos et al., 2013; Eickhoff et al., in press; Kahnt et al., 2012; Kelly et al., 2010

See also http://en.wikipedia.org/wiki/Cluster_analysis.

useful in the context of nonhierarchical clustering algorithms, such as spectral and in particular k -means clustering, as hierarchical clustering inevitably yields a perfect hierarchical consistency.

External knowledge

Criteria reflecting convergence of the different cluster solutions with independent, external information, such as CBP performed in other data modalities or a priori anatomical/functional knowledge, finally, represent a very distinct class of criteria [Handl et al., 2005; Jain et al., 2010]. On the one hand, they are, in contrast to the aforementioned metrics, independent from the actual data and hence provide external validity. On the other hand, they are based on the problematic assumption [cf. Amunts et al., 2014] that different sources of information should yield the same parcellation of the brain. This has repeatedly been challenged and in fact can result in a strong confirmatory bias.

In sum, the desire to test the “statistical significance” of a clustering solution is hard to fulfill [cf. Breiman, 2001; Vogelstein et al., 2014]. The wish to assess the “trueness” of clusters within (i.e., cluster comparison) or between (i.e., model comparison) a cluster number choice may be a more legitimate concern. Choosing the clustering solution with the highest model fit represents an unsupervised statistical learning problem that cannot be easily framed within the realms of inferential statistics [Jain, 2010]. Rather than trying to test whether a clustering solution reaches statistical significance, we propose assessing different cluster validity criteria to choose among CBP results. More than one single cluster validity criterion should be used because the choice of one objective cluster validity criterion is still a subjective choice by the investigator. We would therefore suggest guiding the choice of a final parcellation by majority vote across a number of complementary cluster validity criteria. These evaluate the more or less good model fit of a given clustering solution in the sense of explaining the data. Even more so, an informed and confident decision on the most pertinent ROI segregation should be justified by consistency across different clustering algorithms and cluster validity criteria [Clos et al., 2013]. More generally, the neurobiological “ground truth,” unknown to us neuroscientists, is probably hierarchical, modular, and multi-scale [Frackowiak and Markram, 2015].

INTEGRATION

Claims of Circularity

Following ROI parcellation, one of the most frequent questions is what features actually drove this distinction. In other words, “what is the difference in connectivity between the identified clusters?” Thus, the obtained clusters are frequently submitted to supplementary analyses that usually assess the same connectivity modality that

was initially used to identify the clusters. This kind of follow-up analysis has repeatedly raised the suspicion of circular analysis or double dipping.

Double dipping

In neuroimaging, this often refers to the practice of first correlating a behavioral measure with brain activity and then using a hereby identified subset of voxels/vertices for the second ‘actual’ correlation analysis with the same behavioral measure [Vul et al., 2008]. Such ‘spurious correlations’ do entail overly enthusiastic results as voxels/vertices have been selected twice for the same purpose in a nested, nonindependent fashion [Lieberman et al., 2009]. More generally, any statistical analysis has been argued to be invalid when the same data is used for selection and then for discriminative analysis if the test statistic depends on the selection criterion [Kriegeskorte et al., 2009].

Is it an instance of double dipping to use the same (connectivity) data to first identify clusters in a ROI and then compute the connectivity profile of the ensuing clusters? We would argue that it is not. While the clustering step takes place in an exploratory statistical framework, aimed at identifying groups within the ROI voxels/vertices that are similar to each other, the characterization step takes place in an inferential statistics framework, aimed at identifying which target voxels/vertices in the brain have above-chance connections to the clusters (null hypothesis: no part of the brain is connected to the current cluster more than by chance). Put differently, the first step discovers structure in the ROI according to voxel/vertex-wise connectivity, whereas the second step explicitly tests this structure by asking which parts of the brain are significantly connected to the ensuing clusters. As a remark, we can however not test whether two derived clusters have different connectivity. This is because it is connectional differences that led to emergence of these clusters. Put differently, the validity of the statistical test depends on the validity of the underlying null hypothesis. A first way to argue against circularity in this scenario would therefore be that the underlying statistical framework/question of both analyses are markedly different.

Descriptive follow-up analyses

Apart from that, there is a completely different and probably much more pragmatic line of argumentation against accusations of circular analysis. The investigator can explicitly frame the cluster connectivity analysis (i.e., second step) as a noninferential and thus descriptive follow-up analysis. This would purely serve to ‘illustrate which are the strongest connectivity differences that contributed to the cluster formation.’ They hence should be considered nothing more than a visualization of what differences caused the cluster formation. Note that this weakens the conclusions on the cluster connectivity results. Nevertheless, purely descriptive cluster characterizations

can provide very useful representations of the ROI at hand [e.g., Smith et al., 2013a; Thirion et al., 2006a].

Even if some investigators might be inclined to reproach the post-hoc characterization of connectivity-derived clusters with circular analysis, it does not appear to hold for connectivity analyses of individual clusters. On the contrary, a comprehensive multi-modal characterization of the obtained clusters in the ROI is strongly recommended. Using the same connective modalities, connective patterns that drove the parcellation can actually be made explicit in a noncircular fashion.

Connectivity-Derived Clusters as Priors

CBP for other analyses

CBP can yield reliable cornerstones for a variety of consecutive neuroimaging analyses. Experimental methods requiring a-priori target regions can capitalize on CBP clusters to further characterize their behavioral implications by diverse viewpoints towards cross-modal functional mapping. This might include but is not exclusive to transcranial magnetic stimulation (TMS), voxel-based morphometry (VBM), structural equation models (SEM), Granger causality mapping (GCM), and seed-based experimental fMRI analyses. From a broader perspective, CBP has the potential to enhance any neuroimaging technique reliant on prospective region definitions that critically hinges on proper fit of the topographical priors.

Create atlases as references

The mentioned methods are not only suited for the creation of spatial maps, but for the characterization of known functional segregation. Connectivity-derived clusters can however be seen as novel, potentially untested hypotheses on regional differentiation. These can be tested in hypothesis-driven experimental studies (i.e., anatomical or functional hypotheses operationalized by region definitions). Asking questions on, for instance, the differences in coactivation pattern of dMRI-defined clusters, the relationship between the regional volumes of the identified regions and phenotypical traits in larger samples or the differential affection of a newly described subdivision in clinical samples are all exciting questions. The information gained from these investigations would then provide a detailed and continuously growing characterization of a brain region within the spatial framework of a particular CBP differentiation. A map of functionally distinct subregions might also serve as an independent reference to explain closely neighboring but topographically diverging activation clusters in task-based experimental neuroimaging studies [e.g., Cieslik et al., 2013; Decety and Lamm, 2007], for the characterization of hemodynamic response profiles [Ciuciu et al., 2003], as well as for functional connectome applications [Smith et al., 2013a; Varoquaux and Craddock, 2013]. CBP may thus serve as a post-hoc analysis to complement interpretation and as a preced-

ing analysis to inform the design of experimental neuroimaging investigations.

CBP may therefore fill a vacuum in the current research landscape in providing new spatial maps of brain regions (i.e., discovering structure in the brain). These can then be further characterized by a multi-modal investigation of the (differential) structure, connectivity, and function as well as their relation to various phenotypes in health and disease (i.e., testing structure in the brain). Moreover, CBP could become a crucial preliminary step to improve the potency of various seed-based neuroimaging methods.

CONCLUSIONS

Connectivity-based parcellation is currently one of the most exciting yet also one of the most fluidly evolving approaches in neuroimaging research. In contrast to most existing methods, it may yield maps of the brain that can be seen as spatial hypotheses on functional or structural segregation – a hypothesis that may and should be tested by integrative, multi-modal investigations. We hope, however, that this overview has also raised awareness for the various pitfalls that may be encountered when performing or reviewing CBP analyses; from the initial definition of the ROI (which operationalizes the motivation for that particular investigation and constrains all conclusions that can be drawn), to the choice of the clustering algorithm (with each having its specific strengths and biases), cluster number (which should be based on the examination of multiple metrics and with awareness for multi-level biological organization), and finally the difficulty to apply classical inferential statistics in the context of CBP. Brain parcellation not only serves the generation of new hypotheses. Rather, it might allow new insight into the principles of regional organization when conducting CBP based on different aspects of inter-neuronal communication. Such multi-modal comparison, hand-in-hand with results from hypothesis-testing approaches, might provide unprecedented insight into the organization of regional specialization in human brain's structure, connectivity, and function. Ultimately, connectivity-based parcellation methods offer useful simplified views on brain regions that remain complex in nature.

ACKNOWLEDGMENTS

The authors thank Olivier Grisel for very helpful discussion. The authors also thank Rogier Mars and Gesa Hartwigsen for their thoughtful comments on a previous version of this manuscript. They are indebted to two anonymous reviewers for their insightful comments.

REFERENCES

Abraham A, Pedregosa F, Eickenberg M, Gervais P, Mueller A, Kossaifi J, Gramfort A, Thirion B, Varoquaux G (2014):

- Machine learning for neuroimaging with scikit-learn. *Front Neuroinform* 8:14.
- Alcauter S, Lin W, Keith Smith JK, Gilmore JH, Gao W (2015): Consistent anterior-posterior segregation of the insula during the first 2 years of life. *Cerebral Cortex*, 25:1176–1187.
- Amft M, Bzdok D, Laird AR, Fox PT, Schilbach L, Eickhoff SB (2014): Definition and characterization of an extended social-affective default network. *Brain Structure and Function* 220: 1031–1049.
- Amunts K, Hawrylycz MJ, Van Essen DC, Van Horn JD, Harel N, Poline JB, De Martino F, Bjaalie JG, Dehaene-Lambertz G, Dehaene S (2014): Interoperable atlases of the human brain. *Neuroimage* 99:525–532.
- Amunts K, Lepage C, Borgeat L, Mohlberg H, Dickscheid T, Rousseau ME, Bludau S, Bazin PL, Lewis LB, Oros-Peusquens AM, Shah NJ, Lippert T, Zilles K, Evans AC (2013): BigBrain: An ultrahigh-resolution 3D human brain model. *Science* 340: 1472–1475.
- Amunts K, Schleicher A, Burgel U, Mohlberg H, Uylings HB, Zilles K (1999): Broca's region revisited: Cytoarchitecture and intersubject variability. *J Comp Neurol* 412:319–341.
- Andrews-Hanna JR, Reidler JS, Sepulcre J, Poulin R, Buckner RL (2010): Functional-anatomic fractionation of the brain's default network. *Neuron* 65:550–562.
- Anwander A, Tittgemeyer M, von Cramon DY, Friederici AD, Knosche TR (2007): Connectivity-based parcellation of broca's area. *Cereb Cortex* 17:816–825.
- Bach DR, Behrens TE, Garrido L, Weiskopf N, Dolan RJ (2011): Deep and superficial amygdala nuclei projections revealed in vivo by probabilistic tractography. *J Neurosci* 31:618–623.
- Barnard ST, Pothen A, Simon HD (1995): A spectral algorithm for envelope reduction of sparse matrices. *Numer Linear Algebra Appl* 2:317–334.
- Beckmann CF, DeLuca M, Devlin JT, Smith SM (2005): Investigations into resting-state connectivity using independent component analysis. *Philos Trans R Soc Lond B Biol Sci* 360:1001–1013.
- Beckmann M, Johansen-Berg H, Rushworth MF (2009): Connectivity-based parcellation of human cingulate cortex and its relation to functional specialization. *J Neurosci* 29:1175–1190.
- Behrens TE, Johansen-Berg H (2005): Relating connective architecture to grey matter function using diffusion imaging. *Phil Trans R Soc B* 360:903–911.
- Behrens TE, Johansen-Berg H, Woolrich MW, Smith SM, Wheeler-Kingshott CA, Boulby PA, Barker GJ, Sillery EL, Sheehan K, Ciccarelli O, Thompson AJ, Brady JM, Matthews PM (2003): Non-invasive mapping of connections between human thalamus and cortex using diffusion imaging. *Nat Neurosci* 6:750–757.
- Bengio Y (2009): Learning deep architectures for AI. *Foundations Trends Machine Learn* 2:1–127.
- Biswal B, Yetkin FZ, Haughton VM, Hyde JS (1995): Functional connectivity in the motor cortex of resting human brain using echo-planar MRI. *Magn Reson Med* 34:537–541.
- Biswal BB, Mennes M, Zuo XN, Gohel S, Kelly C, Smith SM, Beckmann CF, Adelstein JS, Buckner RL, Colcombe S, Dogonowski AM, Ernst M, Fair D, Hampson M, Hoptman MJ, Hyde JS, Kiviniemi VJ, Kottler R, Li SJ, Lin CP, Lowe MJ, Mackay C, Madden DJ, Madsen KH, Margulies DS, Mayberg HS, McMahon K, Monk CS, Mostofsky SH, Nagel BJ, Pekar JJ, Peltier SJ, Petersen SE, Riedl V, Rombouts SA, Rypma B, Schlaggar BL, Schmidt S, Seidler RD, Siegle GJ, Sorg C, Teng GJ, Veijola J, Villringer A, Walter M, Wang L, Weng XC, Whitfield-Gabrieli S, Williamson P, Windischberger C, Zang YF, Zhang HY, Castellanos FX, Milham MP (2010): Toward discovery science of human brain function. *Proc Natl Acad Sci USA* 107:4734–4739.
- Blumensath T, Jbabdi S, Glasser MF, Van Essen DC, Ugurbil K, Behrens TE, Smith SM (2013): Spatially constrained hierarchical parcellation of the brain with resting-state fMRI. *Neuroimage* 76:313–324.
- Breiman L (2001): Statistical modeling: The two cultures. *Stat Sci* 16:199–231.
- Broderson KH (2009): Decoding mental activity from neuroimaging data—The science behind mind-reading. *New Collection Oxford* 4:50–61.
- Brodman, K, 1909. *Vergleichende Lokalisationslehre der Großhirnrinde*. Barth, Leipzig.
- Buckner RL, Krienen FM, Castellanos A, Diaz JC, Yeo BT (2011): The organization of the human cerebellum estimated by intrinsic functional connectivity. *Journal of neurophysiology* 106: 2322–2345.
- Buckner RL, Krienen FM, Yeo BT (2013): Opportunities and limitations of intrinsic functional connectivity MRI. *Nat Neurosci* 16:832–837.
- Bzdok D, Laird A, Zilles K, Fox PT, Eickhoff SB (2012): An investigation of the structural, connective and functional specialization in the human amygdala. *Hum Brain Mapp* 34: 3247–3266.
- Bzdok D, Langner R, Schilbach L, Engemann DA, Laird AR, Fox PT, Eickhoff SB (2013): Segregation of the human medial prefrontal cortex in social cognition. *Frontiers in human neuroscience*, 7.
- Bzdok D, Langner R, Schilbach L, Jakobs O, Roski C, Caspers S, Laird A, Fox PT, Zilles K, Eickhoff SB (2013b): Characterization of the temporo-parietal junction by combining data-driven parcellation, complementary connectivity analyses, and functional decoding. *Neuroimage* 81:381–392.
- Bzdok D, Eickhoff SB (2015): The resting-state physiology of the human cerebral cortex. In: Toga AW, editor. *Brain Mapping: An Encyclopedic Reference*. Elsevier.
- Bzdok D, Heeger A, Langner R, Laird A, Fox P, Palomero-Gallagher N, Vogt B, Zilles K, Eickhoff S (2014): Subspecialization in the human posterior medial cortex. *Neuroimage* 106: 55–71.
- Cauda F, D'Agata F, Sacco K, Duca S, Geminiani G, Vercelli A (2011): Functional connectivity of the insula in the resting brain. *NeuroImage* 55:8–23.
- Cauda F, Geminiani G, D'Agata F, Sacco K, Duca S, Bagshaw AP, Cavanna AE (2010): Functional connectivity of the posteromedial cortex. *PLoS One* 5.
- Chang SE, Kenney MK, Loucks TM, Poletto CJ, Ludlow CL (2009): Common neural substrates support speech and non-speech vocal tract gestures. *NeuroImage* 47:314–325.
- Chang LJ, Yarkoni T, Khaw MW, Sanfey AG (2013): Decoding the role of the insula in human cognition: Functional parcellation and large-scale reverse inference. *Cereb Cortex* 23:739–749.
- Chumbley JR, Friston KJ (2009): False discovery rate revisited: FDR and topological inference using Gaussian random fields. *Neuroimage* 44:62–70.
- Cieslik EC, Zilles K, Caspers S, Roski C, Kellermann TS, Jakobs O, Langner R, Laird AR, Fox PT, Eickhoff SB (2013): Is there "one" DLPFC in cognitive action control? Evidence for

- heterogeneity from co-activation-based parcellation. *Cereb Cortex* 23:2677–2689.
- Clos M, Amunts K, Laird AR, Fox PT, Eickhoff SB (2013): Tackling the multifunctional nature of Broca's region meta-analytically: Co-activation-based parcellation of area 44. *Neuroimage* 83C:174–188.
- Ciuciu P, Poline JB, Marrelec G, Idier J, Pallier C, Benali H (2003): Unsupervised robust non-parametric estimation of the hemodynamic response function for any fMRI experiment. *IEEE Trans Med Imaging* 22:1235–1251.
- Cohen AL, Fair DA, Dosenbach NU, Miezin FM, Dierker D, Van Essen DC, Schlaggar BL, Petersen SE (2008): Defining functional areas in individual human brains using resting functional connectivity MRI. *NeuroImage* 41:45–57.
- Cox DD, Savoy RL (2003): Functional magnetic resonance imaging (fMRI) "brain reading": Detecting and classifying distributed patterns of fMRI activity in human visual cortex. *Neuroimage* 19:261–270.
- Craddock RC, James GA, Holtzheimer PE, 3rd, Hu XP, Mayberg HS (2012): A whole brain fMRI atlas generated via spatially constrained spectral clustering. *Hum Brain Mapp* 33:1914–1928.
- Craig AD (2009): How do you feel—Now? The anterior insula and human awareness. *Nat Rev Neurosci* 10:59–70.
- Damoiseaux JS, Rombouts SA, Barkhof F, Scheltens P, Stam CJ, Smith SM, Beckmann CF (2006): Consistent resting-state networks across healthy subjects. *Proc Natl Acad Sci USA* 103:13848–13853.
- Decety J, Lamm C (2007): The role of the right temporoparietal junction in social interaction: How low-level computational processes contribute to meta-cognition. *Neuroscientist* 13:580–593.
- Deen, Ben, Naomi B. Pitskel, Kevin A. Pelphrey (2011): Three systems of insular functional connectivity identified with cluster analysis. *Cerebral Cortex* 21:1498–1506.
- Dehaene S, Piazza M, Pinel P, Cohen L (2003): Three parietal circuits for number processing. *Cogn Neuropsychol* 20:487–506.
- Devlin JT, Poldrack RA (2007): In praise of tedious anatomy. *NeuroImage* 37:1033–1041.
- Donath WE, Hoffman AJ (1973): Lower bounds for the partitioning of graphs. *IBM J Res Dev* 17:420–425.
- Efron B, Tibshirani R (1991): Statistical data analysis in the computer age. *Science* 253:390–395.
- Efron B, Tibshirani RJ (1994): *An Introduction to the Bootstrap*. CRC Press.
- Eickhoff SB, Bzdok D, Laird AR, Roski C, Caspers S, Zilles K, Fox PT (2011): Co-activation patterns distinguish cortical modules, their connectivity and functional differentiation. *Neuroimage* 57:938–949.
- Eickhoff SB, Grefkes C (2011): Approaches for the integrated analysis of structure, function and connectivity of the human brain. *Clinical EEG and neuroscience* 42:107–121.
- Eickhoff SB, Laird AR, Grefkes C, Wang LE, Zilles K, Fox PT (2009): Coordinate-based activation likelihood estimation meta-analysis of neuroimaging data: A random-effects approach based on empirical estimates of spatial uncertainty. *Hum Brain Mapp* 30:2907–2926.
- Eickhoff SB, Laird AR, Fox PT, Bzdok D, Hensel L (2014): Functional segregation of the human dorsomedial prefrontal cortex. *Cerebral cortex*.
- Evans AC, Collins DL, Milner B (1992): An MRI-based stereotactic atlas from 250 young normal subjects. *Soc Neurosci Abstr* 18.
- Evans AC (2013): Networks of anatomical covariance. *Neuroimage* 80:489–504.
- Fischl B, van der Kouwe A, Destrieux C, Halgren E, Segonne F, Salat DH, Busa E, Seidman LJ, Goldstein J, Kennedy D, Caviness V, Makris N, Rosen B, Dale AM (2004): Automatically parcellating the human cerebral cortex. *Cereb Cortex* 14:11–22.
- Felleman DJ, Van Essen DC (1991): Distributed hierarchical processing in the primate cerebral cortex. *Cereb Cortex* 1:1–47.
- Forgy EW (1965): Cluster analysis of multivariate data: Efficiency versus interpretability of classifications. *Biometrics* 21:768–769.
- Fox PT, Lancaster JL (2002): Opinion: Mapping context and content: The BrainMap model. *Nat Rev Neurosci* 3:319–321.
- Fox CJ, Iaria G, Barton JJ (2009): Defining the face processing network: Optimization of the functional localizer in fMRI. *Hum Brain Mapp* 30:1637–1651.
- Frackowiak R, Markram H (2015): The future of human cerebral cartography: A novel approach. *Phil Trans R Soc B* 370.
- Friston KJ, Rotshtein P, Geng JJ, Sterzer P, Henson RN (2006): A critique of functional localisers. *Neuroimage* 30:1077–1087.
- Gordon EM, Laumann TO, Adeyemo B, Huckins JF, Kelley WM, Petersen SE (2014): Generation and evaluation of a cortical area parcellation from resting-state correlations. *Cerebral Cortex*.
- Gorgolewski KJ, Varoquaux G, Rivera G, Schwarz Y, Ghosh SS, Maumet C, Nichols TE, Poldrack RA, Poline JP, Yarkoni Y, Margulies DS. 2014. *NeuroVault.org: A web-based repository for collecting and sharing unthresholded statistical maps of the human brain* (in press).
- Gorgolewski KJ, Varoquaux G, Rivera G, Schwarz Y, Ghosh SS, Maumet C, Sochat VV, Nichols TE, Poldrack RA, Poline J-B (2015): *NeuroVault.org: A web-based repository for collecting and sharing unthresholded statistical maps of the human brain*. *Frontiers in neuroinformatics* 9.
- Grosbras MH, Paus T (2002): Transcranial magnetic stimulation of the human frontal eye field: Effects on visual perception and attention. *Cognitive Neuroscience* 14:1109–1120.
- Handl J, Knowles J, Kell DB (2005): Computational cluster validation in post-genomic data analysis. *Bioinformatics* 21:3201–3212.
- Hartigan JA, Wong MA (1979): A k-means clustering algorithm. *Appl Stat* 28:100–108.
- Hastie T, Tibshirani R, Friedman J (2011): *The Elements of Statistical Learning*. Heidelberg, Germany: Springer Series in Statistics.
- Hensel L, Bzdok D, Müller VI, Zilles K, Eickhoff SB (2013): Neural correlates of explicit social judgments on vocal stimuli. *Cerebral Cortex* bht307.
- Hipp JF, Siegel M (2015): BOLD fMRI Correlation Reflects Frequency-Specific Neuronal Correlation. *Current biology: CB* 25:1368–1374.
- Hyvarinen A. (1999): Fast and robust fixed-point algorithms for independent component analysis. *Neural Networks IEEE Trans* 10:626–634.
- Igelström, KM, Webb, TW, Graziano, MS (2015): Neural processes in the human temporoparietal cortex separated by localized independent component analysis. *J Neurosci* 35:9432–9445.
- Jakab A, Molnár PP, Bogner P, Béres M, Berényi EL (2012): Connectivity-based parcellation reveals interhemispheric differences in the insula. *Brain topography* 25:264–271.
- Jbabdi S, Behrens TE (2013): Long-range connectomics. *Ann NY Acad Sci* 1305:83–93.

- Jain AK (2010): Data clustering: 50 years beyond K-means. *Pattern recognition letters*, 31:651–666.
- Jain AK, Murty MN, Flynn PJ (1999): Data clustering: A review. *ACN Computing Surveys* 31:264–323.
- Johansen-Berg H, Behrens TE, Robson MD, Drobnjak I, Rushworth MF, Brady JM, Smith SM, Higham DJ, Matthews PM (2004): Changes in connectivity profiles define functionally distinct regions in human medial frontal cortex. *Proc Natl Acad Sci USA* 101:13335–13340.
- Johansen-Berg H, Behrens TE, Sillery E, Ciccarelli O, Thompson AJ, Smith SM, Matthews PM (2005): Functional-anatomical validation and individual variation of diffusion tractography-based segmentation of the human thalamus. *Cereb Cortex* 15: 31–39.
- Johansen-Berg H, Rushworth MF (2009): Using diffusion imaging to study human connective anatomy. *Annu Rev Neurosci* 32: 75–94.
- Johnson SC (1967): Hierarchical clustering schemes. *Psychometrika* 32:241–254.
- Jones DK (2008): Studying connections in the living human brain with diffusion MRI. *Cortex* 44:936–952.
- Kahnt T, Chang LJ, Park SQ, Heinze J, Haynes JD (2012): Connectivity-based parcellation of the human orbitofrontal cortex. *J Neurosci* 32:6240–6250.
- Kannan SR, Ramathilagam S, Sathya A, Pandiyarajan R (2010): Effective fuzzy c-means based kernel function in segmenting medical images. *Computers in biology and medicine* 40:572–579.
- Kanwisher N, McDermott J, Chun MM (1997): The fusiform area: A module in human extrastriate cortex specialized for face perception. *J Neurosci* 17:4301–4311.
- Kelly C, Toro R, Di Martino A, Cox CL, Bellec P, Castellanos FX, Milham MP (2012): A convergent functional architecture of the insula emerges across imaging modalities. *Neuroimage* 61: 1129–1142.
- Kim JH, Lee JM, Jo HJ, Kim SH, Lee JH, Kim ST, Seo SW, Cox RW, Na DL, Kim SI, Saad ZS (2010): Defining functional SMA and pre-SMA subregions in human MFC using resting state fMRI: Functional connectivity-based parcellation method. *Neuroimage* 49:2375–2386.
- Kochunov P, Glahn DC, Fox PT, Lancaster JL, Saleem K, Shelledy W, Zilles K, Thompson PM, Coulon O, Mangin JF, Blangero J, Rogers J (2010): Genetics of primary cerebral gyrfication: Heritability of length, depth and area of primary sulci in an extended pedigree of Papio baboons. *Neuroimage* 53:1126–1134.
- Koster-Hale J, Saxe R, Dungan J, Young LL (2013): Decoding moral judgments from neural representations of intentions. *Proc Natl Acad Sci USA* 110:5648–5653.
- Krall SC, Rottschy C, Oberwelland E, Bzdok D, Fox PT, Eickhoff SB, Fink GR, Konrad K (2015): The role of the right temporo-parietal junction in attention and social interaction as revealed by ALE meta-analysis. *Brain Struct Funct* 220:587–604.
- Kriegeskorte N, Simmons WK, Bellgowan PS, Baker CI (2009): Circular analysis in systems neuroscience: the dangers of double dipping. *Nat Neurosci* 12:535–540.
- Kurth F, Zilles K, Fox PT, Laird AR, Eickhoff SB (2010): A link between the systems: functional differentiation and integration within the human insula revealed by meta-analysis. *Brain Struct Funct* 214:519–534.
- Lee K, Tak S, Ye, JC (2011): A data-driven sparse GLM for fMRI analysis using sparse dictionary learning with MDL criterion. *Med Imaging IEEE Trans* 1076–1089.
- Lieberman MD, Berkman ET, Wager TD (2009): Correlations in social neuroscience aren't voodoo: commentary on Vul et al. (2009). *Perspectives on Psychological Science* 4:299–307.
- Liu H, Qin W, Li W, Fan L, Wang J, Jiang T, Yu C (2013): Connectivity-based parcellation of the human frontal pole with diffusion tensor imaging. *The Journal of neuroscience : the official journal of the Society for Neuroscience* 33:6789–6790.
- Lloyd S (1957): published 1982 in *IEEE Transactions on Information Theory*. Least squares quantization in PCM. *Technical Report* 28:128–137.
- Malherbe C, Messé A, Bardinete E, Péligrini-Issac M, Perlberg V, Marrelec G, Worbe Y, Yelnik J, Lehericy S, Benali H (2014): Combining Spatial Independent Component Analysis with Regression to Identify the Subcortical Components of Resting-State fMRI Functional Networks. *Brain Connect* 4:181–192.
- Marrelec G, Krainik A, Duffau H, Pelegrini-Issac M, Lehericy S, Doyon J, Benali H (2006): Partial correlation for functional brain interactivity investigation in functional MRI. *Neuroimage* 32:228–237.
- Mars RB, Jbabdi S, Sallet J, O'Reilly JX, Croxson PL, Olivier E, Noonan MP, Bergmann C, Mitchell AS, Baxter MG, Behrens TE, Johansen-Berg H, Tomassini V, Miller KL, Rushworth MF (2011): Diffusion-weighted imaging tractography-based parcellation of the human parietal cortex and comparison with human and macaque resting-state functional connectivity. *J Neurosci* 31:4087–4100.
- Mars RB, Sallet J, Schuffelgen U, Jbabdi S, Toni I, Rushworth MF (2012): Connectivity-based subdivisions of the human right “temporoparietal junction area”: Evidence for different areas participating in different cortical networks. *Cereb Cortex* 22: 1894–1903.
- Mennes M, Kelly C, Colcombe S, Castellanos FX, Milham MP (2013): The extrinsic and intrinsic functional architectures of the human brain are not equivalent. *Cereb Cortex* 23:223–229.
- Mesulam MM (1978): Tetramethyl benzidine for horseradish peroxidase neurohistochemistry: a non-carcinogenic blue reaction product with superior sensitivity for visualizing neural afferents and efferents. *J Histochem Cytochem* 26:106–117.
- Mesulam MM, Mufson EJ (1982a): Insula of the old world monkey. I. Architectonics in the insulo-orbito-temporal component of the paralimbic brain. *J Comp Neurol* 212:1–22.
- Mesulam MM, Mufson EJ (1982b): Insula of the old world monkey. III. Efferent cortical output and comments on function. *J Comp Neurol* 212:38–52.
- Mesulam MM (1998): From sensation to cognition. *Brain* 121:1013–1052.
- Mitchell JP (2008): Activity in right temporo-parietal junction is not selective for theory-of-mind. *Cereb Cortex* 18:262–271.
- Mufson EJ, Mesulam MM (1982): Insula of the old world monkey. II. Afferent cortical input and comments on the claustrum. *J Comp Neurol* 212:23–37.
- Muhle-Karbe PS, Derrfuss J, Lynn MT, Neubert FX, Fox PT, Brass M, Eickhoff SB (2015): Co-Activation-Based Parcellation of the Lateral Prefrontal Cortex Delineates the Inferior Frontal Junction Area. *Cerebral Cortex*.
- Nanetti L, Cerliani L, Gazzola V, Renken R, Keysers C (2009): Group analyses of connectivity-based cortical parcellation using repeated k-means clustering. *Neuroimage* 47:1666–1677.

- Naselaris T, Kay KN, Nishimoto S, Gallant JL (2011): Encoding and decoding in fMRI. *Neuroimage* 56:400–410.
- Nelson SM, Cohen AL, Power JD, Wig GS, Miezin FM, Wheeler ME, Velanova K, Donaldson DI, Phillips JS, Schlaggar BL, Petersen SE (2010): A parcellation scheme for human left lateral parietal cortex. *Neuron* 67:156–170.
- Neubert FX, Mars RB, Thomas AG, Sallet J, Rushworth MF (2014): Comparison of human ventral frontal cortex areas for cognitive control and language with areas in monkey frontal cortex. *Neuron* 81:700–713.
- Ng B, Varoquaux G, Poline JB, Thirion B (2013): Implications of inconsistencies between fMRI and dMRI on multimodal connectivity estimation. In *Medical Image Computing and Computer-Assisted Intervention-MICCAI 2013* (pp. 652–659). Springer Berlin Heidelberg.
- Passingham RE, Stephan KE, Kötter R (2002): The anatomical basis of functional localization in the cortex. *Nat Rev Neurosci* 3:606–616.
- Petrides M, Tomaiuolo F, Yeterian EH, Pandya DN (2012): The prefrontal cortex: comparative architectonic organization in the human and the macaque monkey brains. *Cortex* 48:46–57.
- Poldrack RA, Gorgolewski KJ (2014): Making big data open: data sharing in neuroimaging. *Nature neuroscience* 17:1510–1517.
- Plis SM, Hjelm DR, Salakhutdinov R, Allen EA, Bockholt HJ, Long JD, Johnson HJ, Paulsen JS, Turner JA, Calhoun VD (2014): Deep learning for neuroimaging: A validation study. *Front Neurosci* 8:229.
- Pradal Christophe, Gaël Varoquaux, Hans Peter Langtangen. (2013): Publishing scientific software matters. *Journal of Computational Science* 4.5:311–312.
- Radua J, Mataix-Cols D (2009): Voxel-wise meta-analysis of grey matter changes in obsessive-compulsive disorder. *Br J Psychiatry* 195:393–402.
- Ramnani N, Behrens TE, Johansen-Berg H, Richter MC, Pinski MA, Andersson JL, Rudebeck P, Ciccarelli O, Richter W, Thompson AJ, Gross CG, Robson MD, Kastner S, Matthews PM (2006): The evolution of prefrontal inputs to the corticopontine system: diffusion imaging evidence from Macaque monkeys and humans. *Cereb Cortex* 16:811–818.
- Rizzolatti G, Camarda R, Fogassi L, Gentilucci M, Luppino G, Matelli M (1988): Functional organization of inferior area 6 in the macaque monkey. II. Area F5 and the control of distal movements. *Exp Brain Res* 71:491–507.
- Robinson JL, Laird AR, Glahn DC, Lovallo WR, Fox PT (2010): Metaanalytic connectivity modeling: Delineating the functional connectivity of the human amygdala. *Hum Brain Mapp* 31:173–184.
- Sallet J, Mars RB, Noonan MP, Neubert FX, Jbabdi S, O'Reilly JX, Filippini N, Thomas AG, Rushworth MF (2013): The organization of dorsal frontal cortex in humans and macaques. *J Neurosci* 33:12255–12274.
- Saxe R, Brett M, Kanwisher N (2006): Divide and conquer: A defense of functional localizers. *Neuroimage* 30:1088–1096. discussion 1097–1089.
- Saygin ZM, Osher DE, Augustinack J, Fischl B, Gabrieli JD (2011): Connectivity-based segmentation of human amygdala nuclei using probabilistic tractography. *Neuroimage* 56:1353–1361.
- Saygin ZM, Osher DE, Koldewyn K, Reynolds G, Gabrieli JD, Saxe RR (2012): Anatomical connectivity patterns predict face selectivity in the fusiform gyrus. *Nat Neurosci* 15:321–327.
- Scannell JW, Blakemore C, Young MP (1995): Analysis of connectivity in the cat cerebral cortex. *J Neurosci* 15:1463–1483.
- Schilbach L, Eickhoff SB, Rotarska-Jagiela A, Fink GR, Vogeley K (2008): Minds at rest? Social cognition as the default mode of cognizing and its putative relationship to the “default system” of the brain. *Conscious Cogn* 17:457–467.
- Schurz M, Radua J, Aichhorn M, Richlan F, Perner J (2014): Fractionating theory of mind: A meta-analysis of functional brain imaging studies. *Neurosci Biobehav Rev* 42:9–34.
- Shehzad Z, Kelly AM, Reiss PT, Gee DG, Gotimer K, Uddin LQ, Lee SH, Margulies DS, Roy AK, Biswal BB, Petkova E, Castellanos FX, Milham MP (2009): The resting brain: Unconstrained yet reliable. *Cereb Cortex* 19:2209–2229.
- Shen X, Papademetris X, Constable RT (2010): Graph-theory based parcellation of functional subunits in the brain from resting-state fMRI data. *Neuroimage* 50:1027–1035.
- Shen X, Tokoglu F, Papademetris X, Constable RT (2013): Group-wise whole-brain parcellation from resting-state fMRI data for network node identification. *Neuroimage* 82:403–415.
- Silani G, Lamm C, Ruff CC, Singer T (2013): Right supramarginal gyrus is crucial to overcome emotional egocentricity bias in social judgments. *J Neurosci* 33:15466–15476.
- Smith SM (2012): The future of FMRI connectivity. *Neuroimage* 62:1257–1266.
- Smith SM, Fox PT, Miller KL, Glahn DC, Fox PM, Mackay CE, Filippini N, Watkins KE, Toro R, Laird AR, Beckmann CF (2009): Correspondence of the brain’s functional architecture during activation and rest. *Proc Natl Acad Sci USA* 106:13040–13045.
- Smith SM, Beckmann CF, Andersson J, Auerbach EJ, Bijsterbosch J, Douaud G, Duff E, Feinberg DA, Griffanti L, Harms MP, Kelly M, Laumann T, Miller KL, Moeller S, Petersen S, Power J, Salimi-Khorshidi G, Snyder AZ, Vu AT, Woolrich MW, Xu J, Yacoub E, Ugurbil K, Van Essen DC, Glasser MF, Consortium WUMH (2013a): Resting-state fMRI in the human connectome project. *Neuroimage* 80:144–168.
- Smith SM, Vidaurre D, Beckmann CF, Glasser MF, Jenkinson M, Miller KL, Van Essen DC (2013b): Functional connectomics from resting-state fMRI. *Trends Cogn Sci* 17:666–682.
- Solano-Castiella E, Anwender A, Lohmann G, Weiss M, Docherty C, Geyer S, Reimer E, Friederici AD, Turner R (2010): Diffusion tensor imaging segments the human amygdala in vivo. *Neuroimage* 49:2958–2965.
- Solano-Castiella E, Schäfer A, Reimer E, Türke E, Pröger T, Lohmann G, Trampel R, Turner R (2011): Parcellation of human amygdala in vivo using ultra high field structural MRI. *NeuroImage* 58:741–748.
- Stanberry L, Nandy R, Cordes D (2003): Cluster analysis of fMRI data using dendrogram sharpening. *Hum Brain Mapp* 20:201–219.
- Talairach J, Tournoux P (1988): Co-planar stereotaxic atlas of the human brain. New York: Thieme.
- Thirion B, Flandin G, Pinel P, Roche A, Ciuciu P, Poline JB (2006a): Dealing with the shortcomings of spatial normalization: Multi-subject parcellation of fMRI datasets. *Human brain mapping* 27:678–693.
- Thirion B, Flandin G, Pinel P, Roche A, Ciuciu P, Poline JB (2006b): Dealing with the shortcomings of spatial normalization: Multi-subject parcellation of fMRI datasets. *Hum Brain Mapp* 27:678–693.
- Thirion B, Varoquaux G, Dohmatob E, Poline JB (2014): Which fMRI clustering gives good brain parcellations? *Front Neurosci* 8:167.

- Tibshirani R, Walther G, Hastie T (2001): Estimating the number of clusters in a data set via the gap statistic. *J Roy Stat Soc B* 411–423.
- Timm NH (2002): *Applied Multivariate Analysis*. New York: Springer.
- Toro R, Fox PT, Paus T (2008): Functional coactivation map of the human brain. *Cereb Cortex* 18:2553–2559.
- Tzourio-Mazoyer N, Landeau B, Papathanassiou D, Crivello F, Etard O, Delcroix N, Mazoyer B, Joliot M (2002): Automated anatomical labeling of activations in SPM using a macroscopic anatomical parcellation of the MNI MRI single-subject brain. *Neuroimage* 15:273–289.
- Tukey JW (1962): The future of data analysis. *Annals Stat* 33:1–67.
- Van Essen DC, Anderson CH, Felleman DJ (1992): Information processing in the primate visual system: an integrated systems perspective. *Science* 255:419–423.
- Van Essen DC (1985): Functional organization of primate visual cortex. In: Peters A, Jones EG, editors. *Cereb Cortex*. New York: Plenum Press. pp. 259–329.
- Varoquaux G, Craddock RC (2013): Learning and comparing functional connectomes across subjects. *Neuroimage* 80:405–415.
- Varoquaux G, Gramfort A, Pedregosa F, Michel V, Thirion B (2011): Multi-subject dictionary learning to segment an atlas of brain spontaneous activity. In *Information Processing in Medical Imaging* (pp. 562–573). Springer Berlin Heidelberg.
- Vogt C, Vogt O (1919): Allgemeinere Ergebnisse unserer Hirnforschung. *Journal Für Psychologie Und Neurologie* 25:279–461.
- Vogelstein JT, Park Y, Ohyama T, Kerr RA, Truman JW, Priebe CE, Zlatic M (2014): Discovery of brainwide neural-behavioral maps via multiscale unsupervised structure learning. *Science* 344:386–392.
- von Economo C (1926): Eine neue Art Spezialzellen des Lobus cinguli und Lobus insulae. *Z Ges Neurol Psychiatr* 100:706–712.
- von Luxburg U (2007): A tutorial on spectral clustering. *Stat Computing* 17:395–416.
- Vul E, Harris C, Winkielman P, Pashler H (2009): Puzzlingly high correlations in fMRI studies of emotion, personality, and social cognition. *Perspectives on Psychological Science* 4: 274–290.
- Wager TD, Lindquist M, Kaplan L (2007): Meta-analysis of functional neuroimaging data: Current and future directions. *Soc Cogn Affect Neurosci* 2:150–158.
- Wandell BA, Dumoulin SO, Brewer AA (2007): Visual field maps in human cortex. *Neuron* 56:366–383.
- Wang J, Yang Y, Fan L, Xu J, Li C, Liu Y, Fox PT, Eickhoff SB, Yu C, Jiang T (2015): Convergent functional architecture of the superior parietal lobule unraveled with multimodal neuroimaging approaches. *Human brain mapping* 36:238–257.
- Weiner KS, Golarai G, Caspers J, Chuapoco MR, Mohlberg H, Zilles K, Amunts K, Grill-Spector K (2014): The mid-fusiform sulcus: a landmark identifying both cytoarchitectonic and functional divisions of human ventral temporal cortex. *Neuroimage* 84:453–465.
- Wiegell MR, Tuch DS, Larsson HB, Wedeen VJ (2003): Automatic segmentation of thalamic nuclei from diffusion tensor magnetic resonance imaging. *Neuroimage* 19:391–401.
- Wig GS, Laumann TO, Cohen AL, Power JD, Nelson SM, Glasser MF, Miezin FM, Snyder AZ, Schlaggar BL, Petersen SE (2013): Parcellating an individual subject’s cortical and subcortical brain structures using snowball sampling of resting-state correlations. *Cerebral cortex* bht056.
- Wig GS, Laumann TO, Petersen SE (2014): An approach for parcellating human cortical areas using resting-state correlations. *Neuroimage* 93:276–291.
- Wolpert D (1996): The lack of a priori distinctions between learning algorithms. *Neural Comp* 8:1341–1390.
- Yarkoni T, Poldrack RA, Nichols TE, Van Essen DC, Wager TD (2011): Large-scale automated synthesis of human functional neuroimaging data. *Nat Methods* 8:665–670.
- Yeo BT, Krienen FM, Sepulcre J, Sabuncu MR, Lashkari D, Hollinshead M, Roffman JL, Smoller JW, Zollei L, Polimeni JR, Fischl B, Liu H, Buckner RL (2011): The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *J Neurophysiol* 106:1125–1165.
- Young MP, Hilgetag CC, Scannell JW (2000): On imputing function to structure from the behavioural effects of brain lesions. *Philos Trans R Soc Lond B Biol Sci* 355:147–161.
- Zalesky A, Fornito A, Harding IH, Cocchi L, Yucel M, Pantelis C, Bullmore ET (2010): Whole-brain anatomical networks: Does the choice of nodes matter? *Neuroimage* 50:970–983.
- Zhang D, Raichle ME (2010): Disease and the brain’s dark energy. *Nat Rev Neurol* 6:15–28.
- Zhang S, Li C (2012): Functional connectivity mapping of the human precuneus by resting state fMRI. *Neuroimage* 59:3548–3562.
- Zhang Y, Fan L, Zhang Y, Wang J, Zhu M, Zhang Y, Yu C, Jiang T (2014): Connectivity-based parcellation of the human posteromedial cortex. *Cereb Cortex* 24:719–727.
- Zilles K, Amunts K (2010): Centenary of Brodmann’s map—conception and fate. *Nat Rev Neurosci* 11:139–145.
- Zilles K, Schleicher A, Langemann C, Amunts K, Morosan P, Palomero-Gallagher N, Schormann T, Mohlberg H, Burgel U, Steinmetz H, Schlaug G, Roland PE (1997): Quantitative analysis of sulci in the human cerebral cortex: Development, regional heterogeneity, gender difference, asymmetry, inter-subject variability and cortical architecture. *Hum Brain Mapp* 5:218–221.