

De novo design of highly selective miniprotein inhibitors of integrins $\alpha\beta6$ and $\alpha\beta8$

Anindya Roy^{1,*}, Lei Shi^{1,2,*}, Ashley Chang^{3,*}, Xianchi Dong^{4,5}, Andres Fernandez⁶, John C. Kraft¹, Jing Li⁴, Viet Q. Le⁴, Rebecca Viazzo Winegar³, Gerald Maxwell Cherf^{8,9}, Dean Slocum³, P. Daniel Poulson³, Garrett E. Casper³, Mary L. Vallecillo-Zúniga³, Jonard Corpuz Valdoz³, Marcos C. Miranda^{1,19}, Hua Bai¹, Yakov Kipnis^{1,16}, Audrey Olshefsky^{1,20}, Tanu Priya^{10,11}, Lauren Carter¹, Rashmi Ravichandran¹, Cameron M. Chow¹, Max R. Johnson¹, Suna Cheng¹, McKaela Smith¹, Catherine Overed-Sayer^{12,21}, Donna K. Finch^{12,13}, David Lowe^{12,14}, Asim K. Bera¹, Gustavo Matute-Bello¹⁵, Timothy P Birkland¹⁶, Frank DiMaio¹, Ganesh Raghu¹⁶, Jennifer R. Cochran⁸, Lance J. Stewart¹, Melody G. Campbell^{6,#}, Pam M. Van Ry^{3,#}, Timothy Springer^{4,#}, David Baker^{1,18,#}

Author affiliations

¹Department of Biochemistry and Institute for Protein Design, University of Washington, Seattle, WA 98195, USA.

²Current Address: Encodia Inc, 5785 Oberlin Drive, San Diego, CA 92121.

³Department of Chemistry and Biochemistry, Brigham Young University, Provo, UT 84602, USA.

⁴Program in Cellular and Molecular Medicine, Children's Hospital Boston, and Departments of Biological Chemistry and Molecular Pharmacology and of Medicine, Harvard Medical School, Boston, United States.

⁵Current address: State Key Laboratory of Pharmaceutical Biotechnology, School of Life Sciences, Nanjing University, Nanjing, China; Engineering Research Center of Protein and Peptide Medicine, Ministry of Education.

⁶Division of Basic Sciences, Fred Hutchinson Cancer Center, Seattle, WA 98109, USA.

⁸Department of Bioengineering, Stanford University, Stanford CA 94305.

⁹Current Address: Denali Therapeutics, South San Francisco, CA, USA.

¹⁰Department of Materials Science and Engineering, University of Washington, Seattle, WA 98195, USA.

¹¹Current Address: Department of Pharmacology, Northwestern University Feinberg School of Medicine; Chicago, IL 60611, USA

¹²Research and Early Development, Respiratory and Immunology, BioPharmaceuticals R&D, AstraZeneca, Cambridge, United Kingdom.

¹³Current Address: Alchemab Therapeutics Ltd, Cambridge, United Kingdom.

¹⁴Current Address: Evox Therapeutics Limited, Oxford Science Park, Medawar Centre, East Building, Robert Robinson Avenue, Oxford, OX4 4HG.

¹⁵Center for Lung Biology, Division of Pulmonary, Critical Care and Sleep Medicine, University of Washington.

¹⁶Division of Pulmonary, Critical Care and Sleep Medicine, Department of Medicine, University of Washington, Seattle, Washington.

¹⁷Dept of Medicine, University of Washington, Seattle WA, USA.

¹⁸Howard Hughes Medical Institute, University of Washington, Seattle, WA 98195, USA.

¹⁹Current Address: Department of Medicine Solna, Division of Immunology and Allergy, Karolinska Institutet and Karolinska University Hospital, Stockholm, Sweden

²⁰Department of Bioengineering, University of Washington, Seattle, WA 98195, USA.

²¹Current Address: Bioscience COPD/IPF, Research and Early Development, Respiratory and Immunology, BioPharmaceuticals R&D, AstraZeneca, Cambridge, UK

*These authors contributed equally to this manuscript.

#correspondence to melody@fredhutch.org, pvanry@chem.byu.edu, springer@crystal.harvard.edu, and dabaker@uw.edu

Abstract

The RGD (Arg-Gly-Asp)-binding integrins $\alpha\beta6$ and $\alpha\beta8$ are clinically validated cancer and fibrosis targets of considerable therapeutic importance. Compounds that can discriminate between the two closely related integrin proteins and other RGD integrins, stabilize specific conformational states, and have sufficient stability enabling tissue restricted administration could have considerable therapeutic utility. Existing small molecules and antibody inhibitors do not have all of these properties, and hence there is a need for new approaches. Here we describe a method for computationally designing hyperstable RGD-containing miniproteins that are highly selective for a single RGD integrin heterodimer and conformational state, and use this strategy to design inhibitors of $\alpha\beta6$ and $\alpha\beta8$ with high selectivity. The $\alpha\beta6$ and $\alpha\beta8$ inhibitors have picomolar affinities for their targets, and >1000-fold selectivity over other RGD integrins. CryoEM structures are within 0.6-0.7Å root-mean-square deviation (RMSD) to the computational design models; the designed $\alpha\beta6$ inhibitor and native ligand stabilize the open conformation in contrast to the therapeutic anti- $\alpha\beta6$ antibody BG00011 that stabilizes the bent-closed conformation and caused on-target toxicity in patients with lung fibrosis, and the $\alpha\beta8$ inhibitor maintains the constitutively fixed extended-closed $\alpha\beta8$ conformation. In a mouse model of bleomycin-induced lung fibrosis, the $\alpha\beta6$ inhibitor potently reduced fibrotic burden and improved overall lung mechanics when delivered via oropharyngeal administration mimicking inhalation, demonstrating the therapeutic potential of *de novo* designed integrin binding proteins with high selectivity.

Introduction

The highly homologous integrins $\alpha\beta6$ and $\alpha\beta8$ bind to latent transforming growth factor- $\beta1$ and $\beta3$ (L-TGF- $\beta1$ and L-TGF- $\beta3$) leading to release of active TGF- $\beta1$ and - $\beta3$.¹⁻³ Upregulation of $\alpha\beta6$ - and/or $\alpha\beta8$ -mediated TGF- β activation is a driver of multiple diseases, including idiopathic pulmonary fibrosis (IPF)⁴⁻⁶, primary sclerosing cholangitis (PSC),⁷ and several solid tumors⁸⁻¹⁰, but deconvoluting the contribution of $\alpha\beta6$ and $\alpha\beta8$ to the etiology of these diseases has been challenging due to limitations in current interventions. Selective antibodies targeting RGD integrins have been generated by immunizing mice,¹¹⁻¹³ but this approach lacks precise control over the target binding site on the integrin. Control over the target site is important because differential modulation of $\alpha\beta6$ integrin conformations (bent-closed, extended-closed, and extended-open) by orthosteric and allosteric inhibitors has dramatically different outcomes on receptor internalization^{11,14,15} and led to different safety signals in preclinical and clinical studies.¹⁶ For example, the mAb BG00011 and small molecule MORF-720 both target the non-internalized, bent-closed $\alpha\beta6$ conformation^{11,15} and have on-target/ $\alpha\beta6$ -mediated toxicity,¹⁷⁻¹⁹ while the small molecules PLN-74809²⁰ and GSK3008348²¹ stabilize the extended-open $\alpha\beta6$ conformation that induces $\alpha\beta6$ internalization, and have not shown any drug-related serious adverse events in clinical trials.^{22,23} Since eight integrin heterodimers, including $\alpha\beta6$ and $\alpha\beta8$, share the conserved RGD binding sequence, it has not been possible to generate selective RGD-mimetic small molecules for individual integrins, making it challenging to dissect the role a single integrin plays in a particular disease.²⁴ Therefore, there is a need for a new integrin therapeutic modality with (i) high selectivity for a single RGD integrin heterodimer, (ii) atomic-level control over the precise location of the target binding site and the protein-protein interaction interfaces to control the evoked integrin conformation, (iii) hyperstability to enable tissue restricted administration (inhaled and oral), and (iv) a smaller hydrodynamic size than IgG antibodies to enable better tissue penetration.

Computational design strategy

We set out to overcome the limitations of integrin-targeted small molecules and antibodies by developing a computational approach that generates small (<75 amino acids) hyperstable *de novo* integrin binding proteins that have high integrin selectivity and specific receptor binding interfaces optimal for treating disease. Integrin $\alpha\beta6$ and $\alpha\beta8$ both bind to a RGD_{LXX(L/I)} motif in the pro-domains of L-TGF- $\beta1$ and $\beta3$ with low nM affinity (Fig. 1a).^{1,25} As in other structures of RGD-containing peptides bound to integrins, the arginine and aspartate side chains make multiple hydrogen bond and salt-bridge interactions to residues at the interface between the integrin alpha and beta subunits (Fig. 1b, 1c). For both $\alpha\beta6$ and $\alpha\beta8$, C-terminal to the RGD, the peptide adopts an alpha-helix-like turn with two leucines (or Ile for $\beta8$) fitting into a hydrophobic pocket formed by a $\beta6/\beta8$ subunit specificity determining loop 2 (SDL2, Figure 1d, 1e).^{1,2,25} In the unliganded state, SDL2 of $\alpha\beta6$ is ordered with multiple backbone hydrogen bonds (PDB ID 4UM8), whereas SDL2 of unliganded $\alpha\beta8$ is mainly flexible.^{1,2,25} To engineer selectivity, we focused on two main areas on the β subunit that differ between the

two targets: the region that contacts the LXX(L/I) motif in the L-TGF- β 3 peptide (Fig. 1d, 1e) and a charge reversal on the β subunit (Fig. 1f). There are several key differences in the hydrophobic packing pattern of LXX(L/I) motif and SDL2 of β 6 compared to β 8 (Fig. 1d, 1e, 1k). Y185 from SDL2 of $\alpha\beta$ 6 packs optimally with Leu (LXX(L/I), L247) of the L-TGF- β 3 peptide (PDB ID 4UM9, Fig. 1d), while the equivalent position on the SDL2 of $\alpha\beta$ 8 (L174) packs much less tightly with Ile (LXX(L/I), I221) of L-TGF- β 1 (PDB ID 6OM2, Fig. 1e). There is also a key charge reversal on the β subunit; β 8 contains K304 whereas the equivalent position on β 6 is E316 (Fig. 1f). We hypothesized that minibinders interacting with the Y185/L174 and E316/K304 regions of $\alpha\beta$ 6 and $\alpha\beta$ 8, respectively, might be able to achieve selectivity between the two proteins.

To implement this design strategy, we sought to generate small proteins that incorporate the central RGD affinity loop, make favorable contacts with both α and β subunits, and interact closely with the two structurally diverging regions described above. We started from the crystal structure of human $\alpha\beta$ 6 in complex with an RGD-containing L-TGF- β 3 peptide (PDB ID 4UM9),¹ and screened the PDB database *in silico* for topologies and structure segments capable of hosting the 8 residue extended turn conformation of the peptide (RGDLGALA, Fig. 1g). Low RMSD matches to the peptide backbone conformation, along with the five flanking residues on both the N- and C-termini, were superimposed on the bound peptide conformation in the complex structure, and those making backbone level clashes with the integrin were discarded (Fig. 1h). We found small α/β ferredoxin folds (Fig. 1i) were able to scaffold the RGD(LXX(L/I)) binding loop without clashing with the integrin while making additional contacts with both α and β subunit (α - and β -loop respectively, Fig. 1i). Structures were assembled from fragments following rules for constructing ideal proteins,²⁶ sampling different alpha helix, beta sheet, and loop lengths, while constraining torsion angles in the region corresponding to the RGD peptide to those observed in the co-crystal structure using Rosetta (Fig. 1g). Following two rounds of design and optimization (see supplementary info for details), two high affinity variants were selected for further characterization: B6B8_BP (av6_3_E13T) and B6_BP (av6_3_A39KG64R) (Extended Data Figs. 5, 6). Any mutation to the LXX(L/I) motif was depleted during affinity maturation, confirming the importance of this motif for selectivity towards $\alpha\beta$ 6 (Extended Data Fig. 5b). Additionally, the A39K mutation makes a salt bridge interaction with E316 of the β 6 subunit (Extended Data Fig. 5f) where there is a charge reversal for the β 8 subunit (K304) (Fig. 1f).

To achieve selectivity for the β 8 subunit, we redesigned the β -loop to take advantage of the K304 charge reversal on the β subunit (Fig. 1f). We generated 200 models with different lengths and conformations of the β -loop using RosettaRemodel²⁷ and the resulting models were superimposed on the L-TGF- β 1 / $\alpha\beta$ 8 complex structure (PDB ID 6OM2) by superposition on the RGD peptide (Fig. 1j). As packing of the L-TGF- β 1 LXX(L/I) motif with SDL2 of $\alpha\beta$ 8 integrin is suboptimal (Fig. 1e), we hypothesized that a minibinder mimicking this interaction would be able to accommodate bulkier residues at these positions, giving additional selectivity. Both the β -loop and LXX(L/I) motif were redesigned using Rosetta and a total of 9 designs with lowest predicted binding energy were selected following structure prediction using AlphaFold.²⁸ Four out of 9 designs showed preferential binding to $\alpha\beta$ 8 integrin with B8_BP_dslf showing the highest affinity and selectivity towards $\alpha\beta$ 8 (Extended Data Fig. 7). Mutations from the B8_BP_dslf sequence (MAVY) to LATI (avb8_#12, which corresponds to the L-TGF- β 1 peptide sequence) completely abrogated selectivity towards $\alpha\beta$ 8 on the yeast surface displayed design (Extended Data Fig. 7b), indicating these residues are critical for selectivity against $\alpha\beta$ 8 vs. $\alpha\beta$ 6. B8_BP_dslf is a monomeric and hyperstable protein when expressed in *E. coli* and binds to human $\alpha\beta$ 8 with 1.9 nM affinity, with no appreciable binding to human $\alpha\beta$ 6 up to 1 μ M (Extended Data Fig. 6b). In agreement with yeast surface display data, purified avb8_12 with the reversion mutations loses selectivity towards $\alpha\beta$ 8 and binds to $\alpha\beta$ 6 with a Kd of 1.13 nM (Extended Data Table 1, Extended Data Fig. 6), confirming the importance of the LXX(L/I) motif for selectivity. B8_BP_dslf has a MAVY motif that packs against SDL2 of $\alpha\beta$ 8. We systematically varied each position within the LATI motif to determine which residue plays a critical role in determining selectivity (Fig. 2e). We found a single mutation containing the LATY (B8_BP-LATY) motif binds to $\alpha\beta$ 8 with an affinity of 500 pM with no appreciable binding to $\alpha\beta$ 6 at 500 nM concentration (Fig. 2e, Extended Data Fig. 6b).

Selectivity profiles of $\alpha\beta6$ and $\alpha\beta8$ binders towards other RGD binding integrins

B6_BP and B8_BP_dslf are highly selective to $\alpha\beta6$ and $\alpha\beta8$, respectively. We investigated the selectivity of the designed binders against seven other RGD-binding integrins. B6B8_BP and B6_BP do not cross-react with RGD-binding integrins $\alpha\beta1$, $\alpha\beta3$, $\alpha\beta5$, $\alpha5\beta1$, $\alpha8\beta1$, and $\alpha11\beta3$ at concentrations up to 200 nM in cell surface binding experiments using K562 cells stably transfected with different RGD-binding integrins, corresponding to >1000-fold selectivity (Extended Data Fig. 8a, 8c). In B6_BP, the β -loop is positioned to confer selectivity between the two integrins, where residue K39 faces E316 on the $\beta6$ subunit and K304 on $\beta8$ (Fig. 2a). As intended, B6_BP is more selective for $\alpha\beta6$ than B6B8_BP. B6_BP binds $\alpha\beta6$ with a higher affinity than $\alpha\beta8$ on the surface of K562 cells, with a K_d of 0.11 (\pm .09) and 580 (\pm 40) nM, respectively (Fig. 2b, Extended Data Fig. 8b). B6B8_BP, which has an alanine at this position (A39), is less selective for $\alpha\beta6$, and binds to $\alpha\beta6$ and $\alpha\beta8$ with a K_d of 1.7 (\pm 0.2) and 7.3 (\pm 1.2) nM, respectively (Fig. 2b, Extended Data Fig. 8b). We generated fluorescently labeled B6B8_BP and B6_BP by conjugating AlexaFluor-488 to an engineered C-terminal cysteine via maleimide chemistry. The fluorescently labeled proteins were titrated against $\alpha\beta6$ (+) human epidermoid carcinoma A431 cells. B6B8_BP and B6_BP bind to A431 cells with K_d values of 167 (\pm .028) pM and 30 (\pm .004) pM, respectively (Fig. 2c).

As B6_BP starts unfolding close to $\sim 90^\circ\text{C}$ (data not shown), we sought to further increase the stability of the engineered inhibitors.^{29,30} Four variants with additional disulfide bonds stapling the N and C terminus had considerably increased thermostability (Extended Data Fig. 9), and bound to $\alpha\beta6$ with subnanomolar affinity; mutation of the RGD to KGE abrogated binding to $\alpha\beta6$ confirming that the RGD loop is necessary for binding (Extended Data Fig. 6a). We further characterized one variant, B6_BP_dslf, and found that it selectively inhibited $\alpha\beta6$ -mediated TGF- β activation (IC_{50} 32.8 \pm 3.4 nM) using CAGA reporter cells³¹ and GARP/TGF- β 1 transfectants, and had marginal effect on $\alpha\beta8$ -mediated TGF- β activation in the tested concentration range, confirming the selectivity towards $\alpha\beta6$ (Fig. 2d, Extended Data Fig. 10d, 10e). $\alpha\beta8$ -selective B8_BP_dslf does not bind to any other RGD binding integrins as confirmed by BLI (Extended Data Fig. 6b).

We compared the potency and selectivity of our designed $\alpha\beta6$ and $\alpha\beta8$ minibinders to the small-molecule dual $\alpha\beta6/\alpha\beta1$ inhibitor (PLN-74809) currently in clinical trials as an oral IPF therapy,²⁰ by assessing their ability to outcompete binding of hLAP₁, the endogenous ligand of $\alpha\beta6$ and $\alpha\beta8$. For $\alpha\beta6$ integrin, B6_BP_dslf had the lowest IC_{50} (1.84 nM), followed by B6B8_BP_dslf (3.79 nM), PLN-74809 (4.36 nM), and no significant binding of B8_BP_dslf to $\alpha\beta6$ integrin was detected (Fig. 2f, 2h). For $\alpha\beta8$, B8_BP_dslf outcompeted hLAP₁ with the lowest IC_{50} (2.68 nM), followed in order of potency by B6B8_BP_dslf (8.48 nM), PLN-74809, and B6_BP_dslf (Fig. 2g, 2h). Taken together, these data confirm that B6_BP_dslf and B8_BP_dslf have exquisite selectivity and affinity for their respective integrin targets, with considerably greater RGD integrin selectivity than the small molecules PLN-74809 and GSK3008348 (Fig. 2i).

Negative stain EM reveals B6_BP_dslf stabilizes the $\alpha\beta6$ open headpiece conformation

Integrin $\alpha\beta6$ adopts the well-characterized range of integrin conformations including bent-closed, extended-closed, and extended-open, which have been linked to activation and binding site accessibility.³ However, $\alpha\beta8$ has not been observed in this range of conformations and instead has been shown to bind and activate L-TGF- β while exclusively occupying the extended-closed conformation.² To confirm the conformational effects of minibinder binding on global $\alpha\beta6$ conformations, we used single-particle negative stain electron microscopy to image complexes of minibinder binding on glycosylated soluble construct of the $\alpha\beta6$ headpiece. All minibinder-integrin complexes were formed in a buffer containing excess Mn^{2+} ions to push the conformational equilibrium towards extended-open and to ensure the availability of the MIDAS cation, which is known to be crucial for ligand binding. As expected, the 2D class averages showed that both B6_BP_dslf and B8_BP_dslf bind at the canonical ligand binding site at the alpha / beta subunit cleft in $\alpha\beta6$ and $\alpha\beta8$, respectively (Fig. 3a). Furthermore, B6_BP_dslf induces $\alpha\beta6$ headpiece opening whereas B8_BP_dslf does not have an effect on the global conformation of $\alpha\beta8$ and the headpiece remains closed (Fig. 3a, Extended Data Fig. 18).

cryoEM structure characterization

To investigate the accuracy of our designed structures, we used single-particle cryoelectron microscopy (cryoEM) to determine structures of a stable complex of human $\alpha\beta6$ ectodomain bound to B6_BP_dslf and human $\alpha\beta8$ ectodomain bound to B8_BP_dslf. Using focused refinement, the nominal overall resolution is 3.4Å for the $\alpha\beta6$ - B6_BP_dslf complex and 2.9Å for the $\alpha\beta8$ - B8_BP_dslf complex, although the resolution varies considerably due to the intrinsic flexibility of both integrins (Supplementary Table 7, Extended Data Fig. 19).² Both integrin-minibinder complexes have extensive binding interfaces (Extended Data Table 3). The structure of the $\alpha\beta6$ - B6_BP_dslf complex identifies several glycosylation sites that had not previously been observed structurally. Despite extensive 3D classification of the $\alpha\beta6$ - B6_BP_dslf complex (Extended Data Fig. 19), we did not observe any subclasses of the integrin-minibinder complex in a closed headpiece conformation. As expected based on the negative stain class averages, the $\alpha\beta8$ - B8_BP_dslf was found to be exclusively in the extended-closed conformation.

The secondary structural elements of the designed B6_BP_dslf minibinder model are in close agreement with the cryoEM map (complex RMSD 0.6 Å vs design, Fig. 3b, 3c, 3d) and the three minibinder loops make contact with the alpha, the beta, or both subunits of integrin, although some interactions vary slightly from the initial design (Extended Data Table 3). B6_BP_dslf was designed using a closed integrin headpiece (PDB ID 4UM9),¹ however, our cryoEM map revealed that, when bound to minibinder, the $\beta1$ domain of the $\beta6$ subunit rearranges to the same open conformation as when bound to ligand (Fig. 3b). In the cryoEM map, the overall orientation of the minibinder is shifted relative to initial design, but the RGD loop positioning is as predicted (Fig. 3c, 3d). As expected, the RGD loop spans the subunit binding interface with RGD-Arg10 forming a hydrogen bond with D218 of the α -subunit and RGD-Asp12 of the minibinder in a position to coordinate with the MIDAS cation. The engineered positively charged, affinity-enhancing point mutation in B6_BP_dslf, A41K (A39K in B6_BP), interacts with negatively charged E316 of the $\beta2$ subunit to form a salt bridge (Fig. 3h). Although the second charge reversal mutation (G64R in B6_BP, G66R in B6_BP_dslf) does not form the anticipated salt bridge with D148 in our structure, we note that this binding surface has a strong negative charge and speculate that this stabilizes the positively charged Arg. As predicted, we observe hydrophobic packing of LXX(L/I) L16 with Y185 of the $\beta6$ subunit (Fig. 3j). Of the 13 interacting pairs of residues present in the cryoEM model, 11 are present in the computational design model, including all three salt bridges. The two unanticipated interactions were backbone interactions with integrin: minibinder R10 and α A21 and minibinder RGD-Asp12 and $\beta6$ S127 (Extended Data Table 3).

The cryoEM model of $\alpha\beta8$ - B8_BP_dslf complex is also very close to the computational design model (Fig. 3e, 3f, 3g, complex RMSD 0.7 Å). In the cryoEM model of the $\alpha\beta8$ - B8_BP_dslf complex, there are 12 interacting pairs of residues between integrin and the minibinder (Extended Data Table 3); as in the design model, the α -loop interacts with α , β -loop with $\beta8$, and the RGD loop spans the two subunits (Fig. 3f). Y172 of the $\beta8$ -SDL2 loops bends inward to form a hydrophobic patch similar to the conformation in L-TGF- β -bound structures (Fig. 3k).² We showed above that altering the known binding motif LXX(L/I) to LATY confers selectivity for $\alpha\beta8$ (Fig. 2e) and the cryoEM structure reveals the molecular basis for this selectivity: we find that Y16 forms stabilizing interactions with A115 of the $\beta8$ subunit and interacts with the less bulky L174 in the $\beta8$ -SDL2 loop (Fig. 3k). The equivalent position in the $\beta6$ -SDL2 loop, Y185, is too bulky and we hypothesize that the steric clash would interfere with binding.

***In vivo* tumor targeting using fluorescently labeled B6_BP**

As B6_BP binds to A431 cells with higher affinity and is more selective than B6B8_BP for $\alpha\beta6$, we selected B6_BP for further *in vivo* experiments. We prepared tumor bearing rodents by injecting 6-8 week old female athymic nude mice with A431 cells ($\alpha\beta6$ (+)) and HEK 293T ($\alpha\beta6$ (-)) into the left and right shoulders, respectively. When the tumors reached 5-10 mm in diameter, mice were injected via the tail vein with 1.5 nmols of AlexaFluor-680 labeled B6_BP (AF680-B6_BP). AF680-B6_BP rapidly accumulated in the $\alpha\beta6$ positive tumors and reached a high tumor-to-muscle fluorescence contrast ratio within 3 hours post-injection (Fig. 4a, Extended Data Fig. 11). There was no detectable fluorescence at the $\alpha\beta6$ negative HEK-293T tumors (Fig. 4a). We also performed a semiquantitative *ex vivo* biodistribution analysis of AF680-B6_BP at 6 hours post-tail vein injection. Analysis of fluorescence intensities of different tissues revealed accumulation of

AF680-B6_BP to $\alpha\beta6$ positive tumors and kidney (tumor-to-kidney ratio 1:1.04) with no significant off-target binding including $\alpha\beta6$ negative tumors (Fig. 4b). Quantification of whole body imaging data for AF680-B6_BP (Fig. 4b) suggests glomerular filtration through the kidneys into the urine is the primary route of elimination.³² We also characterized the pharmacokinetics of B6_BP_dslf in the lungs and serum of healthy male C57BL/6 mice following a single dose via different routes of administration. B6_BP_dslf was rapidly cleared from the blood following IV and IP administration with a half-life of ~10 min, and following inhaled administration, B6_BP_dslf had a half-life in the lungs of ~1 hr (Extended Data Fig. 12).

***In vivo* efficacy of B6_BP_dslf in bleomycin-induced IPF**

We investigated the therapeutic efficacy of B6_BP_dslf using the bleomycin-induced pulmonary fibrosis (PF) mouse model. 12-week-old C57BL/6 male mice were administered bleomycin intratracheally at 1 U/kg body weight to induce fibrosis in a “mild” and “severe” manner (see Methods for details) to mirror the progressive stages of PF. Therapeutic dosing was confirmed by first showing fibrotic development at day 7 in our longitudinal High-Resolution micro-Computed Tomography (HR- μ CT) renders (Extended Data Fig. 13c, 15a) and therefore the data described here verifies treatment began after the development of fibrosis. As proof-of-principle, we administered B6_BP_dslf intraperitoneally at 100 μ g/kg in the mild bleomycin model and at 1 mg/kg in the severe bleomycin model starting on day 7 after bleomycin instillation and found significant improvement in lung health and function through HR- μ CT and lung function measurements (Extended Data Figs. 13-15). For both doses, B6_BP_dslf halted fibrotic progression as evident by the reduced Ashcroft scores and improved respiratory mechanics such as static compliance and forced vital capacity (FVC) (Extended Data Figs. 13-15).

A clinical trial involving an antibody targeting $\alpha\beta6$ (BG00011) from Biogen has been discontinued because it exacerbated disease at higher doses among other serious adverse effects (SAE) including mortality.¹⁷ The SAEs were attributed to increased alveolar inflammation, increased MMP12 generation, and emphysema due to the long half-life of BG00011.^{33,34} An inhaled, tissue-restricted therapy delivered directly to the site of action of fibrosis in the lung could result in a considerably safer and more effective option than systemic inhibition of $\alpha\beta6$ -mediated TGF- β activation; therefore, we pursued a respiratory system delivery. To mimic inhalation³⁵, mice were administered B6_BP_dslf via oropharyngeal administration (OA, 43.6 and 185.2 μ g/kg) every-other-day starting at day 7 post-bleomycin instillation (using the severe bleomycin application method), ending on day 19, for a total of 7 treatments. Non-treated mice were given neither bleomycin nor B6_BP_dslf and serve as a healthy lung control to identify B6_BP_dslf efficacy. Three-dimensional renders and representative slices of the HR- μ CT scans show increased healthy lung tissue available for segmentation in the 185.2 μ g/kg B6_BP_dslf group compared to bleomycin controls (Fig. 5a, upper and middle panels). Quantification of HR- μ CT scans shows a significant rescue of healthy lung volume following 185.2 μ g/kg OA treatment and a shift away from fibrotic intensities (Extended Data Figs. 16a,b). Ashcroft scoring of Masson-trichrome stained lung sections by a blinded veterinary pathologist was significantly reduced in the 185.2 μ g/kg B6_BP-disulf treatment group compared to the BLM and 43.62 μ g/kg B6_BP-disulf treatment group (Fig. 5b). Western blot analysis of the whole lung homogenate lysates shows a reduction in TGF- β mechanistic biomarkers: collagen 1, pSMAD2, and fibronectin (Figs. 4e, f; Extended Data Figs. 16e, f). Further analysis of fibrosis using the Sircol™ Collagen Assay shows the 185.2 μ g/kg OA treatment significantly attenuates both soluble and insoluble collagen deposition, indicative of newly synthesized collagen and more mature crosslinked collagen, respectively (Figs. 4g, h). FVC (Fig. 5c) and static compliance (Extended Data Fig. 16c) were significantly improved with 185.2 μ g/kg OA treatment, and respiratory mechanics show a less restrictive nature (Fig. 5d). We investigated the 185.2 μ g/kg dose further through recovered bronchoalveolar lavage fluid (BALF) using cytokine array analysis, histological immunofluorescence and Sirius Red staining. Commonly implicated cytokines in the progression and severity of PF noted in patients and upregulated in the bleomycin model of PF including IL-6, TNF- α , and TIMP-1, were significantly reduced in 185.2 μ g/kg treated BALF samples (Fig. 5i)³⁶⁻³⁹. Immunofluorescence imaging shows a marked reduction in TGF- β -related fibrotic markers collagen type I and α -smooth muscle actin (α -SMA) (Extended Data Fig. 16d). Sirius Red staining corroborates a reduction of histological total collagen levels (Extended Data Fig. 16g).

With no significant changes in the total number of cells (Extended Data Figs. 16h-k) and reduction of inflammatory cytokines in BALF (Fig. 5i), inhaled B6_BP_dslf has potential to inhibit TGF- β induced fibrosis without exacerbating inflammation as compared to a systemically delivered antibody with a longer *in vivo* half-life⁴. A median mass aerodynamic diameter (MMAD) of ~1-5 μm is necessary to reach the lower respiratory tract⁴⁰ for an inhaled nebulized drug. To confirm the aerosol formulability, we nebulized B6_BP_dslf using an Aeroneb nebulizer and collected aerosols of two different MMADs: 2.5-4 μm and 4-6 μm . For both of these particle sizes, B6_BP_dslf is monomeric, hyperstable, and binds to $\alpha\text{v}\beta\text{6}$ with similar affinity pre-nebulization (Extended Data Fig. 17), paving the way for the development of this molecule as an inhaled nebulized therapy for IPF.

Evidence of human efficacy using lung organotypic model

To assess the viability of B6_BP_dslf in a human organoid-based bleomycin system, we used the human fluorescent lung alveolar organoid (hFLO) triculture model as described previously⁴¹. hFLO organoids were allowed to self-pattern for 7 days after which fibrosis was induced using bleomycin for 3 days prior to treatment with 10 nM B6_BP_dslf for 4 days. Upon immunofluorescent analysis, we observed increased pro-fibrotic markers α -SMA, fibronectin, and PDGFR α in bleomycin-treated organoids. Among these, we observed a statistically significant reduction in α -SMA and fibronectin levels in the organoids treated with B6_BP_dslf showing the efficacy of the treatment in lowering pro-fibrotic markers in human organoids (Fig. 5k-n).

Discussion

The limited effectiveness of current treatments has renewed interest in developing inhaled therapeutics for IPF.^{35,42} To the best of our knowledge, the designed $\alpha\text{v}\beta\text{6}$ inhibitor described here (B6_BP_dslf) binds to its target with higher affinity and selectivity than any previously reported linear or cyclic peptide, or disulfide cross-linked knottin inhibitors of $\alpha\text{v}\beta\text{6}$,⁴³⁻⁴⁷ and is comparable to the leading antibody BG00011, which is no longer under development for IPF (Extended Data Table 2) due to exacerbation of the disease and death.^{17,19} While inhaled tissue-restricted delivery of drugs at the site of action minimizes overall toxicity, dose, and adverse effects, a challenge in development of inhaled biologics is instability or aggregation at the liquid-air interface. The properties of B6_BP_dslf are unchanged following aerosolization: the protein is monomeric, thermostable, has the same CD spectrum, and binds to $\alpha\text{v}\beta\text{6}$ with similar affinity. In addition to the highly potent anti-fibrotic effects demonstrated here in the bleomycin-induced lung fibrosis model, the reduced systemic exposure due to the short serum half-life (~10 min), high selectivity and affinity for $\alpha\text{v}\beta\text{6}$, stabilization of the open $\alpha\text{v}\beta\text{6}$ conformation, ease of production using *E. coli*, hyper-thermostability, and aerosol formulability give B6_BP_dslf an improved target product profile as a therapeutic candidate for IPF. Our designed $\alpha\text{v}\beta\text{6}$ inhibitor could also help combat progressive respiratory disease associated with current and future coronavirus infections.⁴⁸⁻⁵¹ Further improvement in the pharmacokinetic/pharmacodynamic properties of these molecules can be achieved by site-selective chemical PEGylation or fusion to an immunoglobulin Fc domain for immune-oncology indications.^{8,9} More generally, a frequent challenge in drug development is the targeting of a single member within a large family of closely related proteins. This can be difficult to achieve with small molecules that share a conserved binding site, and the development of antibody panels capable of fine discrimination require considerable amounts of negative selection. Our structure-based *de novo* design strategy has high accuracy, as demonstrated by the cryoEM structures and achieves high selectivity by integrating both previously known binding motifs and introducing completely new interactions in a hyperstable small scaffold. As exemplified by our successful design of a potent and selective $\alpha\text{v}\beta\text{8}$ minibinder, this approach should be widely applicable to developing binders with high selectivity and affinity to individual members of the many therapeutically important families of cell surface receptors. Taken together, B6_BP_dslf, with its exquisite RGD integrin selectivity, hyperstability, *in vivo* efficacy in the bleomycin mouse model of lung fibrosis, and the potential for the inhaled route to deliver high drug concentrations to the lungs with minimal systemic exposure and thus provide an effective and safer treatment option for IPF patients than oral $\alpha\text{v}\beta\text{6}$ inhibitors, warrants further clinical investigation.

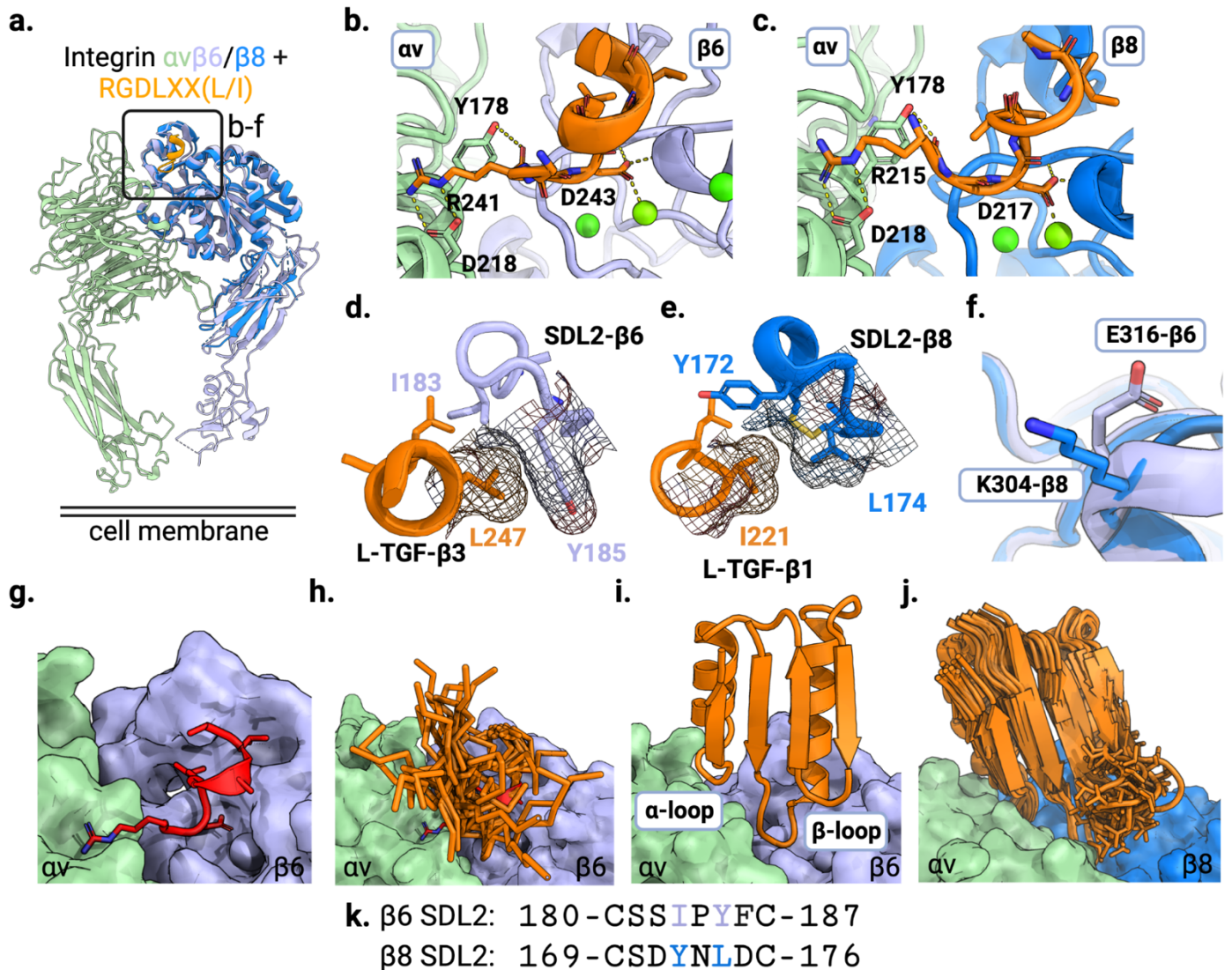


Figure 1. Computational design of $\alpha v\beta 6$ and $\alpha v\beta 8$ selective minibinders. **a)** Crystal structure of $\beta 8$ (PDB ID 6OM2) overlaid on the structure of $\alpha v\beta 6$ integrin in complex with the L-TGF- $\beta 3$ peptide RGD $LXX(L/I)$ (PDB ID 4UM9). Inset highlights the zoomed-in regions shown in panels b-f. The αv subunit is shown in green, $\beta 6$ is in lavender, $\beta 8$ is in blue, and the RGD $LXX(L/I)$ peptide is in orange. **b,c)** Shared polar interactions between the RGD motif and (b) $\alpha v\beta 6$ and (c) $\alpha v\beta 8$ integrin (L-TGF- $\beta 3/\alpha v\beta 6$ complex PDB ID 4UM9, L-TGF- $\beta 1/\alpha v\beta 8$ PDB ID 6OM2). **d)** Hydrophobic packing of LXX(L/I) motif of L-TGF- $\beta 3$ peptide with SDL2 of $\alpha v\beta 6$ (PDB ID 4UM9). Leu247 packs optimally against Y185 from SDL2 of $\beta 6$. **e)** Hydrophobic packing of LXX(L/I) of L-TGF- $\beta 1$ peptide with SDL2 of $\alpha v\beta 8$ (PDB ID 6OM2). I221 of L-TGF- $\beta 1$ peptide packs less tightly against L174 on SDL2 of $\beta 8$ compared to the homologous interactions in panel d. **f)** Charge reversal on β subunit: $\beta 8$ contains K304 whereas the equivalent position on $\beta 6$ is E316. **g)** Surface structure of the $\alpha v\beta 6$ integrin in complex with L-TGF- $\beta 3$ peptide (red cartoon representation, PDB ID 4UM9). **h)** Low RMSD matches to the L-TGF- $\beta 3$ peptide bound to $\alpha v\beta 6$ were harvested from the PDB database (orange stick representations). **i)** Non-clashing fragments with $\alpha v\beta 6$ were then incorporated in the α/β ferredoxin folds (orange ribbon representation) using Rosetta. **j)** Loop extension strategy to design an $\alpha v\beta 8$ selective minibinder: to make more extensive contacts to the $\beta 8$ subunit the β -loop was resampled by one residue insertion (blue surface representation for $\beta 8$ subunit, PDB ID 6OM2). In addition to the loop extension, the LXX(L/I) motif was allowed to be redesigned using Rosetta. **k)** Partial sequence alignment of SDL2 of the $\beta 6/\beta 8$ subunits is shown highlighting two key positions packing against the LXX(L/I) motif of the L-TGF- β ligand (I183 and Y185 in SLD2- $\beta 6$, and Y172 and L174 in SDL2- $\beta 8$).

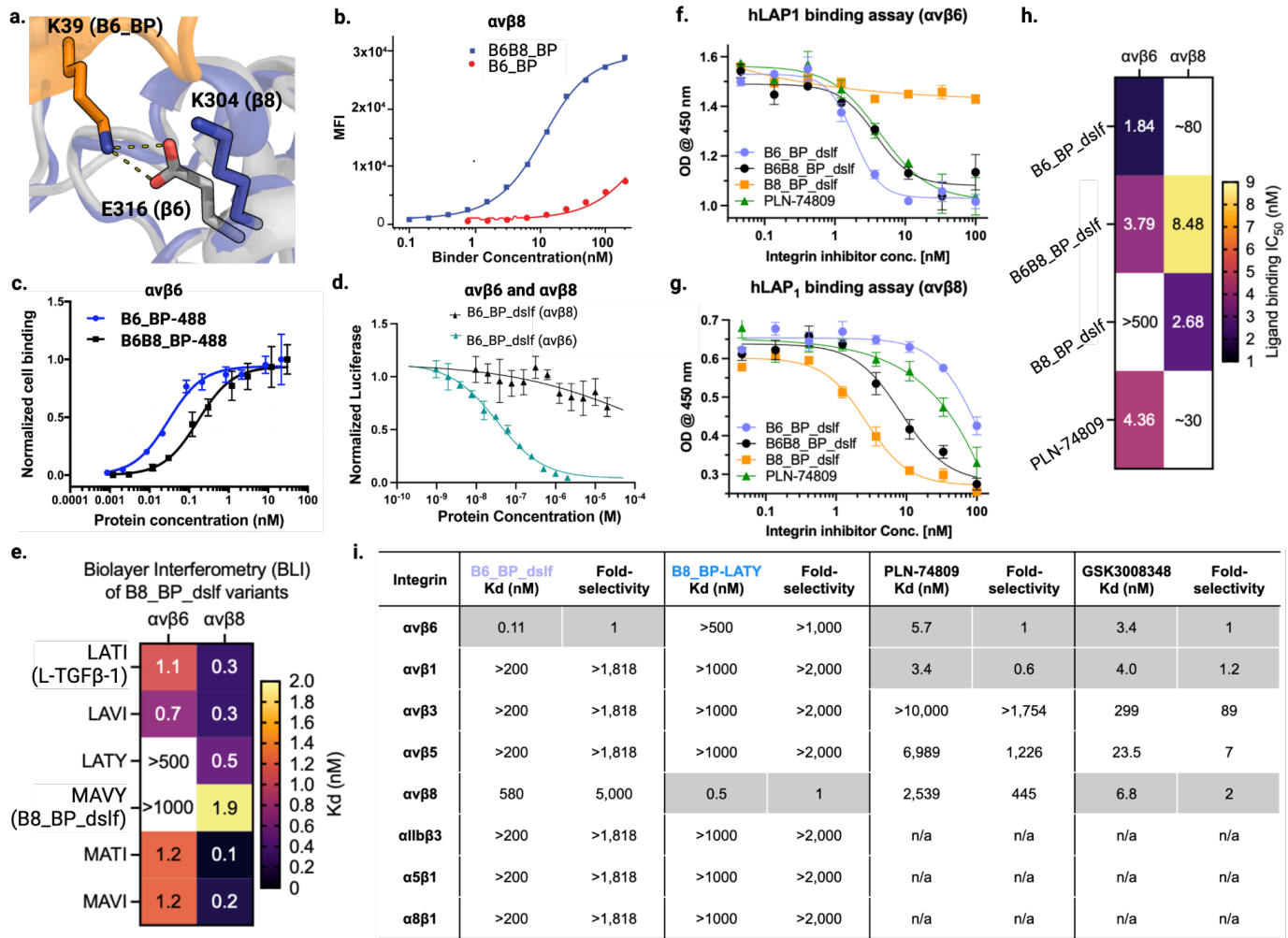


Figure 2. Selectivity of designed binders for $\alpha\text{v}\beta\text{6}$ and $\alpha\text{v}\beta\text{8}$. **a)** The A39K mutation confers selectivity towards $\alpha\text{v}\beta\text{6}$ compared to $\alpha\text{v}\beta\text{8}$ where there is a charge reversal (Glu316 for β6 shown as a gray stick, Lys304 for β8 shown as a blue stick). **b)** Cell surface titration of B6B8_BP and B6_BP against K562 cells stably transfected with $\alpha\text{v}\beta\text{8}$. B6B8_BP lacking the A39K mutation binds to $\alpha\text{v}\beta\text{8}$ with a Kd of ~7.3 nM whereas B6_BP containing the A39K mutation binds to $\alpha\text{v}\beta\text{8}$ >500 nM. **c)** Cell surface titration of AlexaFluor-488-labelled B6B8_BP and B6_BP using $\alpha\text{v}\beta\text{6}$ (+) human epidermoid A431 carcinoma cells. B6_BP binds to A431 cells with higher potency than B6B8_BP (30 pM vs 167 pM). **d)** B6_BP_dslf selectively inhibits $\alpha\text{v}\beta\text{6}$ -mediated TGF- β1 activation. $\alpha\text{v}\beta\text{6}$ and $\alpha\text{v}\beta\text{8}$ transfectants were co-incubated with CAGA-reporter cells and GARP/TGF- β1 transfectants and inhibitors. B6_BP_dslf inhibits TGF- β activation with an IC₅₀ of 32.8 nM. **e)** Binding affinities (Kd) of B8_BP_dslf (MAVY) point mutants to integrins $\alpha\text{v}\beta\text{6}$ and $\alpha\text{v}\beta\text{8}$, determined by BLI. The LATI motif is in native L-TGF- β1 . **f, g)** Competitive inhibition of h-LAP₁ binding to **(f)** $\alpha\text{v}\beta\text{6}$ and **(g)** $\alpha\text{v}\beta\text{8}$ by designed inhibitors and control small molecule PLN-74809.²⁰ **h)** Heatmap of IC₅₀ values for h-LAP₁ binding assays in **f** and **g**. **i)** Binding affinities (Kd) and fold-selectivity values of B6_BP_dslf and B8_BP-LATY to all eight RGD integrins compared to small molecules PLN-74809²⁰ and GSK3008348.²¹ Binding data for PLN-74809 and GSK3008348 are taken from Decaris et al. 2021.²⁰ Rows shaded in gray indicate the RGD integrin(s) for which each molecule is selective (i.e., B6_BP_dslf and B8_BP-LATY are both mono-selective whereas PLN-74809 and GSK3008348 are dual- and tri-selective, respectively). n/a, not available.

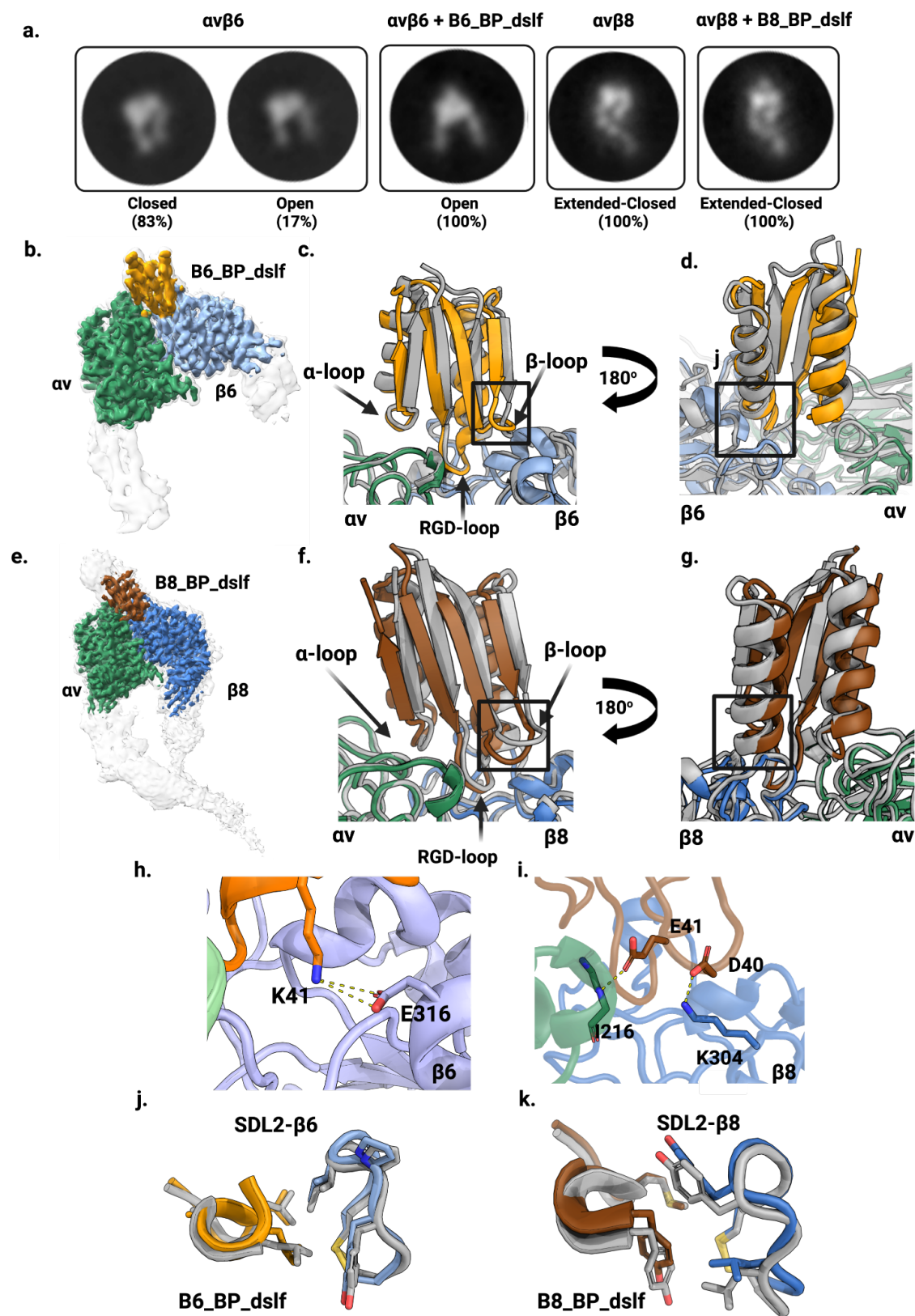


Figure 3. Structural characterization. **a)** Representative 2D class averages of integrin with and without minibinder. For $\alpha\beta 6$, both closed and open headpiece conformations are present in the unbound state, but in the presence of the minibinder the open conformation is dominant. For $\alpha\beta 8$, no open headpieces were observed, with or without minibinder. **b)** CryoEM density map of $\alpha\beta 6$ bound to

minibinder B6_BP_dslf. B6_BP_dslf (goldenrod) binds the integrin ligand binding cleft between the αv (green) and $\beta 6$ (light blue) subunits and induces or stabilizes the open conformation. The sharpened, locally refined cryoEM map is shown in color, superimposed with the unsharpened map showing all domains of the $\alpha v\beta 6$ headpiece in semi-transparent white. **c,d**) Overlay of the designed $\alpha v\beta 6$ + B6_BP_dslf model (gray) and the experimentally determined cryoEM model (colors). Although the overall angle of the minibinder is shifted, the RGD loop positioning is as predicted. Insets in c) and d) are magnified in panels h) and i), respectively. **e**) CryoEM density map of $\alpha v\beta 8$ bound to minibinder B8_BP_dslf. Similar to B6_BP_dslf, B8_BP_dslf (brown) binds the integrin ligand binding cleft between the αv (green) and $\beta 8$ (blue) subunits, however the conformation of $\alpha v\beta 8$ remains in the closed headpiece conformation. The sharpened, locally refined cryoEM map is shown in color, superimposed with the unsharpened map showing all domains in the $\alpha v\beta 8$ ectodomain construct in semi-transparent white. **f,g**) An overlay of the designed $\alpha v\beta 8$ + B8_BP_dslf model (gray) and the experimentally determined model. Although the overall angle of the minibinder is shifted, the RGD loop positioning is as predicted. Insets in f) and g) are magnified in panels i) and k), respectively. **h,i**) Key designed interactions between β -loop and $\beta 6/\beta 8$ subunit are observed in the cryoEM structure: K41 from B6_BP_dslf forms a salt bridge with E316 from the $\beta 6$ subunit (panel h). E41 from β -loop makes backbone level hydrogen bond with I216 from $\beta 8$ subunit and D40 makes salt bridge interaction with K304 from $\beta 8$ subunit (panel i). **j**) Experimental vs designed (gray) packing pattern of the LXXL motif and SDL2 of $\alpha v\beta 6$. **k**) Experimental vs designed (gray) packing pattern of the MAVY motif and SDL2 of $\alpha v\beta 8$.

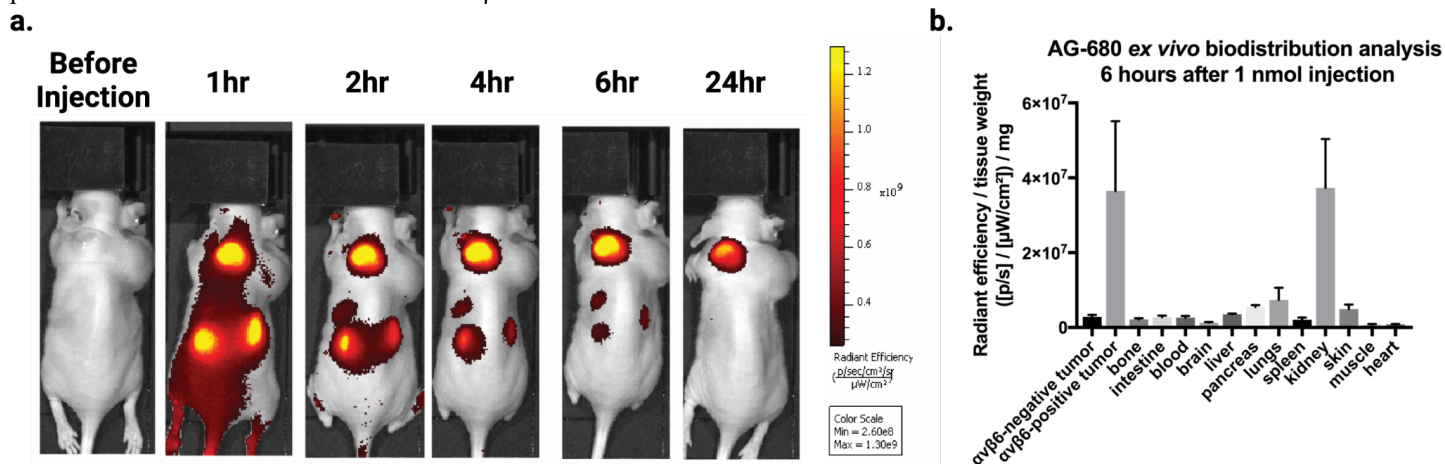


Figure 4: *In vivo* imaging of $\alpha v\beta 6$ (+) A431 tumors using fluorescently-labeled B6_BP. a) Athymic nude mice were injected with $\alpha v\beta 6$ (+) A431 cells on the left shoulder and $\alpha v\beta 6$ (-) HEK293T cells on the right shoulder. AlexaFluor-680-labelled B6_BP (AF680-B6_BP) was injected via the tail vein to image the tumors over time as indicated (see Extended Data for additional images, n=5). b) Semiquantitative *ex vivo* biodistribution assay of AF-680-B6_BP at 6 hours post-tail vein injection. B6_BP selectively accumulates in $\alpha v\beta 6$ (+) tumors and primarily clears via glomerular filtration in the kidneys.

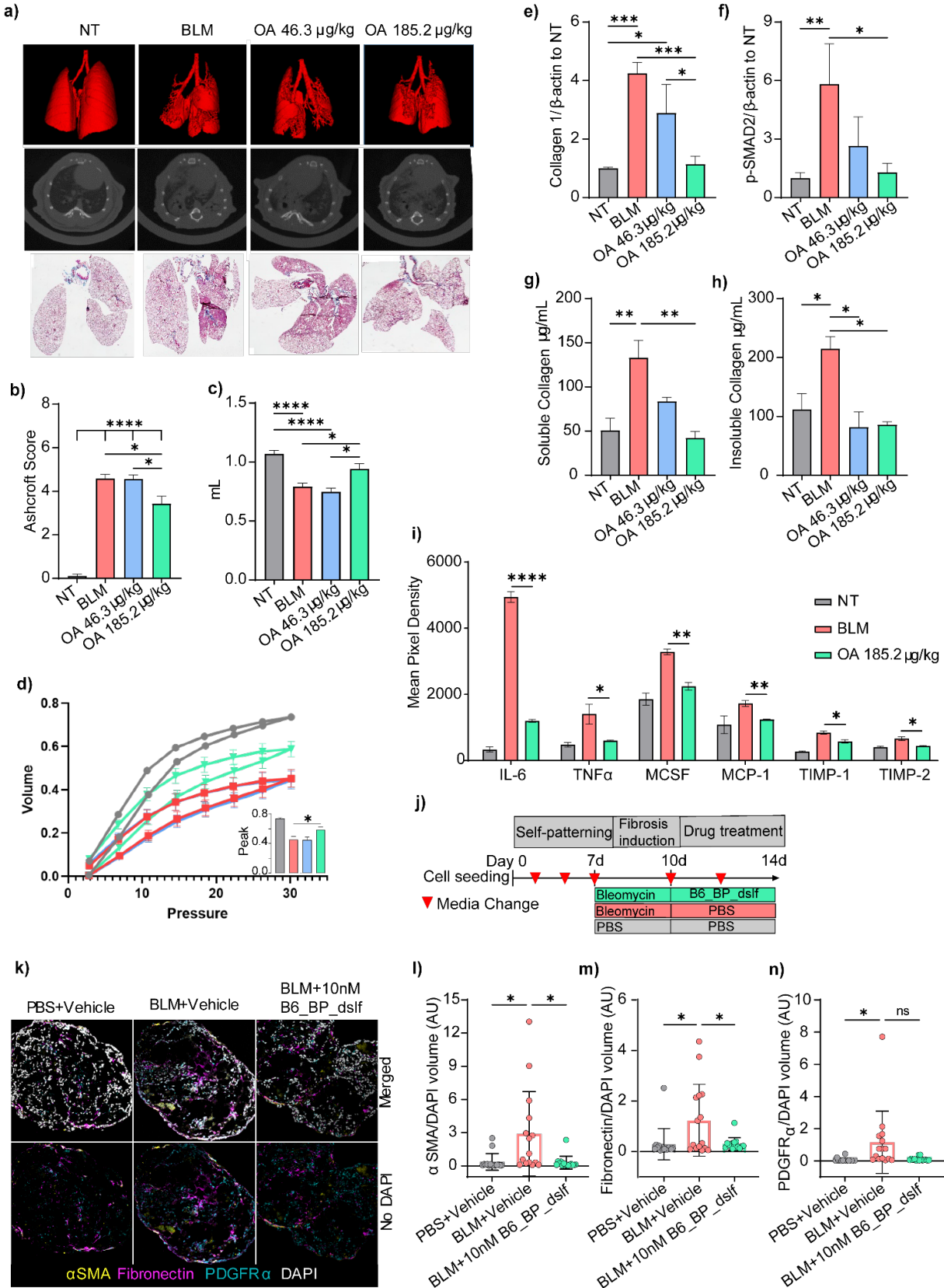


Figure 5: *In vivo* efficacy of OA-administered B6_BP_dslf in bleomycin-induced IPF. **a)** Three dimensional renderings of HR-uCT scans (top panel), representative HR-uCT scans (middle panel), and representative Masson-trichrome images for nontreated (NT), bleomycin treated (BLM) and inhaled B6_BP_dslf group show improvements in tissue health following B6_BP_dslf OA treatment. **b)** Average Ashcroft Scoring of Masson-trichrome images (mean \pm SEM, NT n=5, BLM n=3, B6_BP_dslf 46.3 ug/kg n=3, B6_BP_dslf 185.2 ug/kg n=4) **c)** Forced vital capacity as measured by SCIREQ flexiVent FX (mean \pm SEM, NT n=9, BLM n=10, B6_BP_dslf 46.3 ug/kg n=4, B6_BP_dslf 185.2 ug/kg n=6). **d)** Pressure-Volume curves measured by SCIREQ flexiVent with peak volumes in the inset graph (NT n=20, BLM n=14, B6_BP_dslf 46.3 ug/kg n=4, B6_BP_dslf 185.2 ug/kg n=7). **e)** Whole lung tissue homogenate western blot analysis of Collagen1 and **f)** p-SMAD2 show a dose-dependent reduction of these pro-fibrotic markers following B6_BP_dslf OA treatment (mean \pm SD NT n=3, BLM n=3, B6_BP_dslf 46.3 ug/kg n=3, B6_BP_dslf 185.2 ug/kg n=3). **g)** Soluble and **h)** Insoluble collagen levels are lower following B6_BP_dslf OA treatment (mean \pm SD NT n=3, BLM n=3, B6_BP_dslf 46.3 ug/kg n=3, B6_BP_dslf 185.2 ug/kg n=3). **i)** Cytokine array analysis of common cytokines implicated in inflammation and IPF (all NT vs. BLM are significant, p-value<.05, mean \pm SD, NT n=4, BLM n=4, B6_BP_dslf 46.3 ug/kg n=4, B6_BP_dslf 185.2 ug/kg n=4). **j)** Time course of hFLO organoid growth, bleomycin induction, and 10 nM B6_BP_dslf treatment. **k)** Fluorescent confocal microscopy imaging of hFLO sections immunostained with pro-fibrotic markers α SMA, fibronectin, and PDGFR α . Volumetric analysis of **l)** α SMA, **m)** fibronectin, and **n)** PDGFR α normalized to DAPI signal (mean \pm SD, N=15 cell aggregates were used per treatment, *P<0.05 determined using two-tailed Welch's t-test).

Data availability

Structures from the first round design and B6B8_BP_dslf monomer have been deposited in the Protein Data Bank with accession numbers 7LMV and 7LMX, respectively. Structures of α v β 6+B6_BP_dslf and α v β 8+B8_BP_dslf have been deposited in the Electron Microscopy Data Bank (EMDB) with the accession numbers XXXX, XXXX, XXXX, and XXXX, and Protein Data Bank with the accession numbers XXXX and XXXX. Raw data has been deposited in the Electron Microscopy Public Image Archive (EMPIR) with the accession numbers XXXX, and XXXX. Raw counts/FastQ files for two rounds of directed evolution and model of the co-complex structures for some of the mutants are also uploaded on the github account (<https://github.com/aroy10/avb6-publication>). Any additional data is available from the authors upon request.

Competing financial interests

A.R., L.S., X.D., J.L. T.S., D.B. are co-inventors on an International patent (Serial # PCT/US2020/057016) filed by University of Washington covering molecules and their uses described in this manuscript. C. O. is an employee of AstraZeneca and may own stock or stock options. M.G.C is an inventor on "Antibodies that bind integrin avb8 and uses thereof", U.S. Patent US20210277125A1. A.R., H.B., J.C.K., M.S.S., M.C. and D.B. are inventors on a provisional patent describing the sequence and usage of α v β 8 integrins binders. A.R., L.S., J.C.K, H.B. and D.B. are co-founders of Lila Biologics and own stock or stock options in the company.

Author contributions

A.R., L.S., J.C.K., L.J.S., T.S., A.C., A.F, M.G.C, P.V.R, G.R., and D.B designed the research. L.S. performed first and second round computational designs and affinity maturation of the first round design. A.R. designed the disulfide bonded version of the protein, performed directed evolution, generated material and reagents used for in vitro and in vivo experiments, performed biophysical characterization of the designed inhibitors, and wrote the manuscript. A.R., H.B. designed and characterized α v β 8 selective binders. M.S.S expressed and characterized all B8_BP_dslf variants and measured affinity and selectivity of those mutants against α v β 6 and α v β 8. X.D and T.S. provided the coordinates for human α v β 6 used for designing the inhibitor. X.D. and A.B. solved and refined the crystal structure BP and B6B8_BP_dslf. X.D. determined affinities of the inhibitors against α v β 6 and α v β 8. J.L. measured binding of the final variants against all RGD binding integrins. A.F. optimized the expression and purification of the integrin samples used for all EM studies and prepared, collected, and processed all negative stain data. A.F. and M.G.C prepared, collected, and processed all cryoEM data, built the molecular models for the integrin-minibinder complexes, and analyzed all EM data. V.Q.L. tested inhibition of α v β 6 and α v β 8 mediated TGF- β activation by B6_BP_dslf using a CAGA co-culture assay. D.F, D.L., and C.O designed and performed the TMLC assay. TMLC assay was performed by C.O at AstraZeneca following standard MTA agreement.

M.C.M. optimized expression, purification conditions and developed a one-step purification protocol for the B6B8_BP_dslf. L.C., R.R., C.M.C., T.P. performed large scale overexpression of the inhibitor. A.C. and R.V. performed the bleomycin induced PF model in mice. A.C., R.V., L.J.S., G.R., and P.V.R designed and analyzed the data for bleomycin induced PF models. P.V.R and G.R. supervised bleomycin induced PF model study. M.C. performed the binding of the designed inhibitor to A431 cells and in vivo imaging and analyzed data. J.C. designed and supervised the in vivo imaging experiments. A.R., H.B., and J.C.K. developed the sandwich ELISA bioassay for quantifying minibinders in biological samples; J.C.K. and S.C. ran the sandwich ELISA on serum and lung samples. A.R. and J.C.K. designed and analyzed the B6_BP_dslf_disulf pharmacokinetics in mice and the h-LAP₁ binding assay for integrins $\alpha\beta6$ and $\alpha\beta8$. Y.K. helped with the generation of the SSM library for the designed inhibitor. D.B. supervised, oversaw research, and coordinated research presented here. A.R., J.C.K., L.J.S., A.C., M.G.C. T.S. and D.B. wrote the paper with input from P.V.R. and G.R. Inputs from all authors were included in the manuscript as well.

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