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Deterministic scRNA-seq of individual intestinal organoids reveals new subtypes and coexisting distinct stem cell pools

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1 **Abstract**

2 Single-cell RNA-sequencing (scRNA-seq) has transformed our ability to resolve cellular
3 properties across systems. However, current scRNA-seq platforms are one-size-fits-all
4 approaches that are tailored toward large cell inputs (> 1,000 cells), rendering them inefficient
5 and costly when processing small, individual tissue samples. This important drawback tends to
6 be resolved by loading bulk samples, but this yields confounded mosaic cell population read-outs.
7 To overcome these technological limitations, we developed a deterministic, mRNA-capture bead
8 and cell co-encapsulation dropletting system, DisCo. We demonstrate that DisCo enables precise
9 particle and cell positioning and droplet sorting control through combined machine-vision and
10 multilayer microfluidics. In comparison to other microfluidics systems, the active flow control
11 driving DisCo, enables continuous operation and processing of low-input samples (< 100 cells) at
12 high capture efficiency (> 70%). To underscore the unique capabilities of our approach, we
13 analyzed intestinal organoid development by “DisCo-ing” 31 individual organoids at varying
14 developmental stages. This revealed extensive organoid heterogeneity, identifying distinct
15 subtypes including a regenerative fetal-like *Ly6a*⁺ stem cell population which persists as
16 symmetrical cysts even under differentiation conditions. Furthermore, we uncovered a so far
17 uncharacterized “gobloid” subtype consisting predominantly of precursor and mature (*Muc2*⁺)
18 goblet cells. These findings demonstrate the unique power of DisCo in providing high-resolution
19 snapshots of cellular heterogeneity among small, individual tissues.

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27 **Introduction**

28 Single-cell RNA sequencing (scRNA-seq)¹ induced a paradigm shift in biomedical sciences, since
29 it allows the dissection of cellular heterogeneity by high-dimensional data. Recent technological
30 developments, particularly for cell capture and reaction compartmentalization²⁻⁶, have led to a
31 substantial increase in experimental throughput, enabling massive mapping efforts such as the
32 mouse and human cell-atlas studies^{5,7,8}. These developments were accompanied by biochemical
33 advances, for instance for targeted transcript detection or library multiplexing^{9,10}, which present a
34 rich toolbox for large-scale scRNA-seq studies. However, since the majority of methods rely on
35 stochastic cell capture, entailing large sample inputs, efficient processing of small samples (<
36 1,000 cells) remains challenging. The three main reasons for this are: 1) high fixed run costs,
37 which lead to a large expense per cell at low inputs. For instance, a 10X Chromium run on 100
38 cells would cost \$44 per sequenced cell. 2) Requirements of minimum cell inputs. For example
39 index-sorting FACS or 10X Chromium require minimum cellular inputs ranging between 10,000
40 and 500 cells, respectively^{11,12}. 3) Reduced effectiveness at low inputs because of limited cell
41 capture efficiencies or cell size-selective biases¹³ when processing small heterogeneous
42 samples. To illustrate these limitations, we summarized the performance of various scRNA-seq
43 technologies on low input samples in **Supplementary Table 1**. Consequently, small samples,
44 involving for instance zebrafish embryos¹⁴, organisms like *C. elegans*¹⁵, or intestinal organoids¹⁶⁻
45 ¹⁸, are still pooled to obtain cell numbers that are compatible with stochastic microfluidic and well-
46 based technologies. Thus, it is rather paradoxical that limitations overcome by single cell methods
47 are nevertheless reintroduced at the sample level: artificial averages across samples, resulting in
48 an inability to resolve cell type distributions of individual systems or tissues. This particularly
49 hampers research on emergent and self-organizing multicellular systems, such as organoids, that
50 are heterogeneous and small at critical development stages.

51

52 In this study, we develop a novel deterministic, mRNA-capture bead and cell co-encapsulation
53 dropletting system (DisCo) for low input scRNA-seq. In contrast to established methods that rely
54 on passive cell capture strategies, we utilize machine-vision to actively detect cells and coordinate
55 their capture in droplets. This active flow control approach allows for continuous operation,
56 enabling free per run scaling and serial processing of samples. We demonstrate that DisCo can
57 efficiently process samples of 100 cells and below, making this platform well suited to handle
58 small, individual tissues. Here, we exploit DisCo's unique capabilities to explore the
59 heterogeneous early development of single intestinal organoids at the single cell level. Grown
60 from single stem cells, organoids of vastly different morphologies and cell type compositions form
61 under seemingly identical *in vitro* conditions¹⁶. These unpredictable developmental patterns
62 represent one of the major limitations of this model system, preventing their widespread
63 implementation e.g. in drug screens¹⁹. Thus, efforts to advance our understanding of the extent
64 of organoid heterogeneity, how it arises, and how it can be controlled, for instance with synthetic
65 growth matrices^{20,21}, are of essence. In depth mapping of individual organoid heterogeneity by
66 scRNA-seq has so far been prevented by the minute cell numbers contained in a single intestinal
67 organoid at critical developmental stages, such as post symmetry breaking at the 16-32 cell
68 stage¹⁶. In total, we "DisCo'd" 31 single organoids at four developmental time points post
69 symmetry breaking, and identified striking differences in cell type composition between individual
70 organoids. Among these subtypes, we detected "spheroids" that are composed of regenerative
71 fetal-like stem cells marked by Stem Cell Antigen-1 (*Sca1/Ly6a*)²²⁻²⁵ and that persist under
72 differentiation conditions. In addition, we uncovered a rare subtype that is predominantly
73 comprised of precursor- and mature goblet cells, which we term "gobloids".

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77

78 **Results**

79 To develop our Deterministic Co-encapsulation (DisCo) system, we engineered a three inlet
80 (cells, beads, oil) multilayer dropletting device with two outlet ports (sample, waste) (Schematic
81 **Figure 1A**, full design **Supplementary Figure 1A**). On this device, each inlet and outlet was
82 augmented with a Quake-style microvalve²⁶, to facilitate flow control during operation. In addition,
83 one common valve spanning both the cell and bead channel, termed the dropletting valve, was
84 integrated to allow for on-demand droplet generation. To operate the device, we developed a
85 three-stage process (**Figure 1B**): 1. Stop two particles at the encapsulation site, 2. Eject particles
86 into one droplet, 3. Selectively extract the droplet in a sample channel (Microscopy images of the
87 process are depicted in **Figure 1C**). To enable precise coordination of particles in microchannels,
88 we developed a machine-vision-based approach utilizing subsequent image subtraction for blob
89 detection (**Supplementary Figure 1B**), and on-chip valves for flow-control. Deterministic
90 displacement patterns were induced by opening and closing the cell and bead valves (depicted
91 in **Supplementary Figure 1C**), which moved particles according to discrete jumps into the target
92 region of interest (ROI) with 95.9% of particles placed in an approximately ~200 μm wide region
93 (**Supplementary Figure 1D**). Upon placement, the stopped particles were ejected by
94 pressurizing the dropletting valve, displacing an equal volume of liquid from both channels. The
95 ejected liquid phase was then sheared into a droplet by activating the oil stream. We found that
96 precise pressurization of the dropletting valve allowed for accurate control of droplet volume
97 (**Supplementary Figure 1E**, **Supplementary Video 1**). Post droplet formation, the outlet valves
98 were actuated to separate the formed droplet from the excess waste liquids (**Figure 1D**). With all
99 components operating in tight orchestration, we were able to generate monodisperse emulsions
100 with high co-encapsulation purity (**Figure 1E**, **Supplementary Video 2**).

101
102 As a first benchmarking experiment, we set out to determine the encapsulation performance of
103 DisCo for scRNA-seq-related applications, involving co-encapsulation of single cells with

104 microspheres. Specifically, we aimed to reconfigure the Drop-seq² approach as it only requires
105 coordination of two channels, as compared to three channels for inDrop³. Since co-encapsulation
106 purity and cell capture efficiency are critical system parameters for droplet scRNA-seq systems,
107 we quantified the system's processing speed and encapsulation performance in a free-run
108 configuration, i.e. without cell number limitations at varying cell densities. We found that on
109 average, 91.4% of all droplets contain a cell and a bead, and 1.7% contain an independent cell
110 doublet (**Figure 1F**). Overall, the system provided high cell capture efficiencies of 90% at around
111 200 cells per hour for a 2 cells/ μ L cell concentration (**Figure 1G**). At higher cell concentrations of
112 20 cells/ μ L, the processing speed could be increased to 350 cells per hour, yet with decreased
113 capture efficiencies of approximately 75%.

114
115 Next, we benchmarked the performance of DisCo for scRNA-seq. With drastically reduced bead
116 amounts contained in the generated sample emulsion, we utilized a previously developed chip-
117 based cDNA generation protocol²⁷. Initially, as a library quality measure, we performed a species-
118 mixing experiment of human HEK 293T and murine brown pre-adipocyte IBA cells. We observed
119 clear species separation (**Figure 1H**), consistent with the limited number of previously detected
120 doublets (**Figure 1F**), and increased read-utilization rate compared to conventional Drop-seq
121 experiments (**Supplementary Figure 1F**). As previously reported²⁸, we found that our data
122 displayed a skewed barcode sequence editing distance distribution compared to a true random
123 distribution (**Supplementary Figure 1G**). Since the uniquely low number of beads in DisCo
124 samples (< 500) renders the random occurrence of barcode sequences with an editing distance
125 < 3 rare, we developed a graph-based approach to identify and merge closely related barcodes
126 (described in **Material and Methods**). We found that this approach did not compromise the single
127 cell purity (**Supplementary Figure 1H**) and improved the detectable number of transcripts per
128 cell as compared to published Drop-seq datasets on HEK 293T cells^{2,27} (**Figure 1I**).

129

130 Since DisCo actively controls fluid flow on the microfluidic device, we observed that the system
131 requires negligible run-in time, and is capable of efficiently processing cells from the first cell on.
132 Given this observation, and the high-capture efficiency of DisCo in free-run mode, we
133 hypothesized that the system should provide reliable performance on small samples of 100 cells
134 and below. To determine the overall cell capture efficiency of DisCo, we precisely quantified the
135 number of input cells using impedance measurements. Specifically, we utilized custom pipette
136 tips augmented with a DISPENCELL gold-plated electrode, which allowed accurate counting of
137 the number of input cells as validated by microscopy (**Supplementary Figure 1I**). Utilizing the
138 DISPENCELL approach, we processed cell numbers between 50 - 200 cells, of which on average
139 86.4% (SD \pm 8.1%) were visible on the chip. Of all input cells, 79.1% (SD \pm 7.4%) were
140 successfully co-encapsulated, which corresponds to a co-encapsulation efficiency of 91.6% (SD
141 \pm 1.6%) of all visible cells, while 74.9% (SD \pm 10.7%) of input cells were found as barcodes over
142 500 UMIs per cell (**Figure 1J**).

143
144 As a real-world application, we used DisCo to explore the developmental heterogeneity of
145 intestinal organoids²⁹. These polarized epithelial tissues are generated by intestinal stem cells in
146 3D matrices through a stochastic self-organization process, and mimic key geometric,
147 architectural and cellular hallmarks of the adult intestinal mucosa (e.g. a striking crypt-villus-like
148 axis)²⁹. When grown from single stem cells, organoids of very different morphologies form under
149 seemingly identical *in vitro* conditions (**Figure 2A**, overview image in **Supplementary Figure 2A**).
150 Pooled tissue scRNA-seq data has shed light on the *in vivo*-like cell type composition of these
151 organoids^{16-18,30}, but cannot resolve inter-organoid heterogeneity. Critical for organoid
152 development is an early symmetry breaking event at Day 2 (16-32 cell stage) that is triggered by
153 cell-to-cell variability and results in the generation of the first Paneth cell responsible for crypt
154 formation¹⁶. Here, we were particularly interested in examining the emergence of heterogeneity
155 between individual organoids subsequent to the symmetry breaking timepoints. To do so, we

156 isolated single LGR5⁺ cells by FACS, and maintained them in a stem cell state using CHIR99021
157 and valproic acid (CV)³¹. On Day 3 of culture, CV was removed to induce differentiation. In total,
158 we sampled 31 single intestinal organoids across four timepoints (Day 3 - 6) (**Figure 2A**). These
159 organoids were selected based on differences in morphology, and may thus not constitute an
160 unbiased sample of the population. Since Day 3 represents both differentiation Day 0 and the first
161 sampling time point, we re-annotated the data accordingly (S0 – S3 replacing Day 3 – Day 6).
162 During the co-encapsulation run, the number of encapsulated cells was noted and correlated to
163 the number of barcodes retrieved, which was in approximate accordance (**Supplementary**
164 **Figure 2B**). The even distribution of the number of reads mapping to ribosomal protein transcripts
165 and the observed low expression of heat shock protein-coding genes indicates that most cells
166 were not affected by dissociation and on-chip processing (**Supplementary Figure 2C**).

167
168 To retrieve a first overview of overall cellular heterogeneity, we jointly visualized all 945 cells
169 passing the quality thresholds through Uniform Manifold Approximation and Projection (UMAP).
170 We found that our data was consistent with previously published pooled organoid scRNA-seq
171 read-outs^{17,30} since it revealed expected cell types including *Fabp1*-expressing enterocytes,
172 *Muc2*-expressing goblet cells, *Reg3b*-positive Paneth cells, and *Olfm4*-expressing stem cells
173 (**Figure 2B** and **2C**). In addition, a rare subset of cells, likely too few to form clusters, showed
174 *ChgA* and *ChgB* expression, indicating the expected presence of enteroendocrine cells
175 (**Supplementary Figure 2D**). Noteworthy, we found that batch effects are correctable since no
176 batch-based clustering was observed after correction (**Supplementary Figure 2E**). We also did
177 not detect any clustering driven by cell quality, e.g. detected transcripts or mitochondrial
178 transcripts (**Supplementary Figure 2C**). These findings support the cell type-resolving power of
179 our DisCo platform (**Figure 2C**, extensive heatmap in **Supplementary Figure 2F**, and list in
180 **Supplementary Table 2**). In addition to the expected cell types, we observed a distinct cluster
181 marked by high expression of Stem cell antigen 1 (*Sca1* or *Ly6a*). In depth analysis of marker

182 genes showed high expression of *Anxa1* and *Clu* in the same cluster (**Supplementary Figure**
183 **2D**), and increased YAP-1 target gene expression (**Supplementary Figure 2G**), suggesting that
184 these cells are most likely regenerative fetal-like stem cells^{24,25,32}. Since the two remaining clusters
185 did not show a striking marker gene signature, we resolved their identity by imposing temporal
186 information on the data. This revealed that these clusters likely represent stem- and previously
187 termed potentially intermediate cells (PIC)³³, given their occurrence at early developmental time
188 points (**Figure 2D**). As expected, mature cell types were mostly present at later time points. To
189 further leverage the temporal component in the DisCo data, we used slingshot trajectory
190 analysis³⁴ to infer lineage relationships between cell types and to identify genes that may be of
191 particular significance for waypoints along differentiation (**Figure 2E**). Beyond the previously
192 utilized marker genes for cell type annotation, for example *Reg3b* and *Reg3g* for Paneth cells,
193 additional established markers³⁵ were identified, such as *Agr2* and *Spink4*, and *Fcgbp* for goblet
194 cells (**Figure 2F**). Overall, this suggests that the meta-data produced with our DisCo platform
195 aligns with and expands prior knowledge.

196
197 Intriguingly, we observed maintained presence of the *Ly6a*⁺ stem-cell population at S0, S1, and
198 S3. Since cells with similar expression signatures were previously described under alternate
199 culture conditions as belonging to a distinct organoid subtype termed spheroids²³, we next aimed
200 to verify the presence of such spheroids among our sampled organoids and study their temporal
201 behavior. To do so, we stratified our cells according to the individual organoids from which they
202 were derived by mapping this information onto the reference scaffold (**Figure 3A**). Globally, this
203 analysis revealed that the maturation seems to follow the expected pattern with early organoids
204 (S0) mainly containing stem and Paneth cells, and older organoids (S1 – S3) differentiated cells
205 like goblet cells and enterocytes. However, within single organoids, we found strong
206 heterogeneity, revealing that *Ly6a*⁺ cells were indeed present in a distinct subset of organoids,
207 predominantly comprised of these cells (S1a, S3e). Furthermore, images obtained prior to

208 dissociation showed that *Ly6a*⁺ cell-containing organoids (S3e) exhibited a larger, cystic like
209 structure (**Supplementary Figure 3A**). To confirm the presence of *Ly6a*⁺ organoids in our
210 cultures, we utilized RNAscope (**Figure 3B**, controls **Supplementary Figure 3B**) to localize *Ly6a*,
211 *Muc2*, and *Fabp1* expression in organoid sections. These analyses revealed canonical budding
212 organoids, containing few *Muc2*⁺ goblet cells and *Fabp1*⁺ enterocytes, and *Ly6a*-expressing cells
213 in spherical organoids that did not contain differentiated cell types such as enterocytes or goblet
214 cells.

215

216 The presence of *Ly6a*⁺ cells during the first day of sampling suggested that these cells constitute
217 a second, *Lgr5*-independent stem cell population in the organoid culture. Using flow cytometry,
218 we found that the majority of cells are either LGR5⁺ LY6A⁻ (24.5 %) or LGR5⁻ LY6A⁺ (3.3 %) with
219 only a minority (0.4%) being double positive (**Figure 3C**). This finding, in combination with our
220 trajectory analysis (**Figure 2E** and **2F**), suggested that *Ly6a*⁺ cells are capable of differentiating
221 into organoids. To test this, we sorted and differentiated LGR5⁻ LY6A⁺ cells, revealing that both
222 LGR5⁺ LY6A⁻ and LGR5⁻ LY6A⁺ cells give rise to organoids of similar morphological heterogeneity
223 (**Figure 3D**). These results indicate that LGR5⁻ LY6A⁺ cells have full stem cell potential,
224 comparable to that of previously described fetal-like stem cells²³. Furthermore, the fact that LGR5⁻
225 LY6A⁺ cells did not display a propensity towards spheroid formation suggests that environmental
226 conditions, e.g. matrix stiffness, rather than the initial cell state dictate the formation of spheroids.

227

228 Beside the *Ly6a*⁺ cell-enriched organoids, our data suggested the presence of additional organoid
229 subtypes in the per organoid mappings (**Figure 3A**). The two most striking additional subtypes
230 were three organoids that contained mostly enterocytes (S2c, S3a, S3d), and two that consisted
231 predominantly of immature and mature goblet cells (S1b and especially S2f). The identity of the
232 observed subtypes was further substantiated when visualizing the cell type abundance per
233 organoid (**Figure 3E**), and marker gene expression in individual organoids (**Supplementary**

234 **Figure 3C**). Similar to the spheroids, both subtypes showed aberrant morphologies, tending to
235 be small and round, as compared to canonical organoids bearing a crypt-villus axis (e.g. S3c,
236 **Supplementary Figure 3A**). To detect more subtle molecular differences, we used psupertime³⁶
237 to identify genes that are dynamically expressed during the development of individual organoids.
238 This analysis revealed additional genes that are expressed in subsets of organoids, such as
239 Gastric inhibitory polypeptide (*Gip*), Zymogen granule protein 16 (*Zg16*), Vanin 1 (*Vnn1*), and
240 Defensin alpha 24 (*Defa24*) (**Supplementary Figure 3D**).

241
242 While organoids dominated by enterocytes were previously described as enterocysts¹⁶, organoids
243 displaying goblet cell hyperplasia, here termed “gobloids”, were so far to our knowledge unknown.
244 To validate the existence of the uncovered organoid subtypes, we utilized RNAscope to localize
245 the expression of enterocyte (*Fabp1*) and goblet cell (*Muc2*) markers (**Figure 3F**, controls in
246 **Supplementary Figure 3B**). In addition, and in agreement with our data and prior research, we
247 detected organoids that exclusively contained *Fabp1*⁺ cells, most likely representing enterocysts.
248 Most importantly, we were able to identify organoids that contained a high number of *Muc2*⁺ goblet
249 cells, confirming the existence of “gobloids”.

250

251 **Discussion**

252 A key feature of our new DisCo approach is the ability to deterministically control the cell capture
253 process. Despite lowering the throughput compared to stochastic droplet systems^{2,3}, our
254 approach provides the advantage of being able to process low cell input samples at high efficiency
255 and at a strongly decreased per cell cost (**Supplementary Table 1**). Thus, we believe that the
256 DisCo approach is filling an important gap in the scRNA-seq toolbox. Moreover, full control over
257 the encapsulation process allows for continuous operation of our platform, which is offsetting to
258 some extent the decreased throughput. Another critical feature of DisCo is the use of machine-
259 vision to obtain full control of the entire co-encapsulation process including particle detection,

260 particle positioning, particle droplet injection, and droplet volume. This enables the correct
261 assembly of most droplets, virtually eradicating confounding factors that arise due to failed co-
262 encapsulations^{37,38}. In concept, DisCo is thus fundamentally different to passive particle pairing
263 approaches such as traps³⁹⁻⁴¹ and, compared to these technologies, offers the advantage of
264 requiring vastly simpler and reusable chips without suffering from cell/particle size and shape
265 selection biases^{13,42}. This renders the DisCo approach universally applicable to any particle co-
266 encapsulation application^{43,44}, i.e. cell-cell encapsulations, with the only limiting factor being
267 particle visibility. Providing further development, we envision that machine learning-based
268 deterministic cell handling will ultimately enable targeted cell selection, e.g. by fluorescence or
269 morphology, transforming DisCo into an end-to-end cell processor for samples with low-to-
270 medium input samples.

271
272 To demonstrate DisCo's capacity to process small tissues/systems that were so far difficult to
273 access experimentally, we have analyzed the cell heterogeneity of chemosensory organs from
274 *Drosophila* larvae⁴⁵ and, as shown here, single intestinal organoids. It is thereby worth noting that,
275 based on our handling of distinct tissues, we found that not DisCo itself, but rather cell dissociation
276 has become the efficiency-limiting factor, a well-recognized challenge in the field^{46,47}. Indeed,
277 substantial cell loss was a regular occurrence, even with optimized dissociation and processing
278 strategies (see **Methods**).

279
280 scRNA-seq of individual organoids led us to uncover organoid subtypes of aberrant cell type
281 distribution that were previously not resolved with pooled organoid scRNA-seq^{16,17,30}. One subtype
282 contained predominantly cells that were strikingly similar to previously described fetal-like stem
283 cells or revival stem cells that occur during intestinal regeneration^{24,25,32}. This subtype, previously
284 described under alternate culture conditions as spheroid-type organoids^{18,22,23}, was identified here
285 under standard organoid differentiation conditions, indicating that these organoids are capable of

286 maintaining their unique state. We isolated LY6A-expressing cells and found that they readily give
287 rise to canonical organoids, indicating that these cells are capable of providing a pool of
288 multipotent stem-cells. Of particular interest was one organoid subtype that we termed “gobloid”
289 given that it predominantly comprises immature and mature goblet cells. Since low Notch
290 signaling is pivotal for the commitment of crypt base columnar (CBC) cells towards secreting
291 progenitors, lack of Notch ligand-providing Paneth cells⁴⁸, may drive gobloid development⁴⁹.
292 However, failure to produce Paneth cells has previously been suggested as a mechanism
293 underlying enterocyst development¹⁶, which in principle requires high Notch signaling. Hence, we
294 believe that our findings establish an important foundation to support further research on the
295 emergence of gobloids and enterocysts from the still elusive PIC cells, providing an exciting
296 opportunity to delineate lineage commitment factors of CBC cell differentiation.

297

298 In sum, we demonstrate that our DisCo analysis of individual organoids is a powerful approach to
299 explore tissue heterogeneity and to yield new insights into how this heterogeneity arises. In
300 comparison to established approaches such as automated microscopy^{16,18}, DisCo is magnitudes
301 lower in experimental scale. Nevertheless, scRNA-seq data acquired from 31 organoids enabled
302 us to recapitulate previous findings, benchmarking DisCo, and most importantly, to uncover novel
303 subtypes, leveraging the key advantage of scRNA-seq, i.e. independence from *a priori*
304 knowledge. Next to catalyzing research on other tissues or systems of interest, we believe that
305 the technology and findings of this study will contribute to future research on intestinal organoid
306 development and thus aid the engineering of more robust organoid systems. Furthermore, we
307 expect this approach to be applicable to rare, small clinical samples to gain detailed insights into
308 disease-related cellular heterogeneity and dynamics.

309

310

311

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327

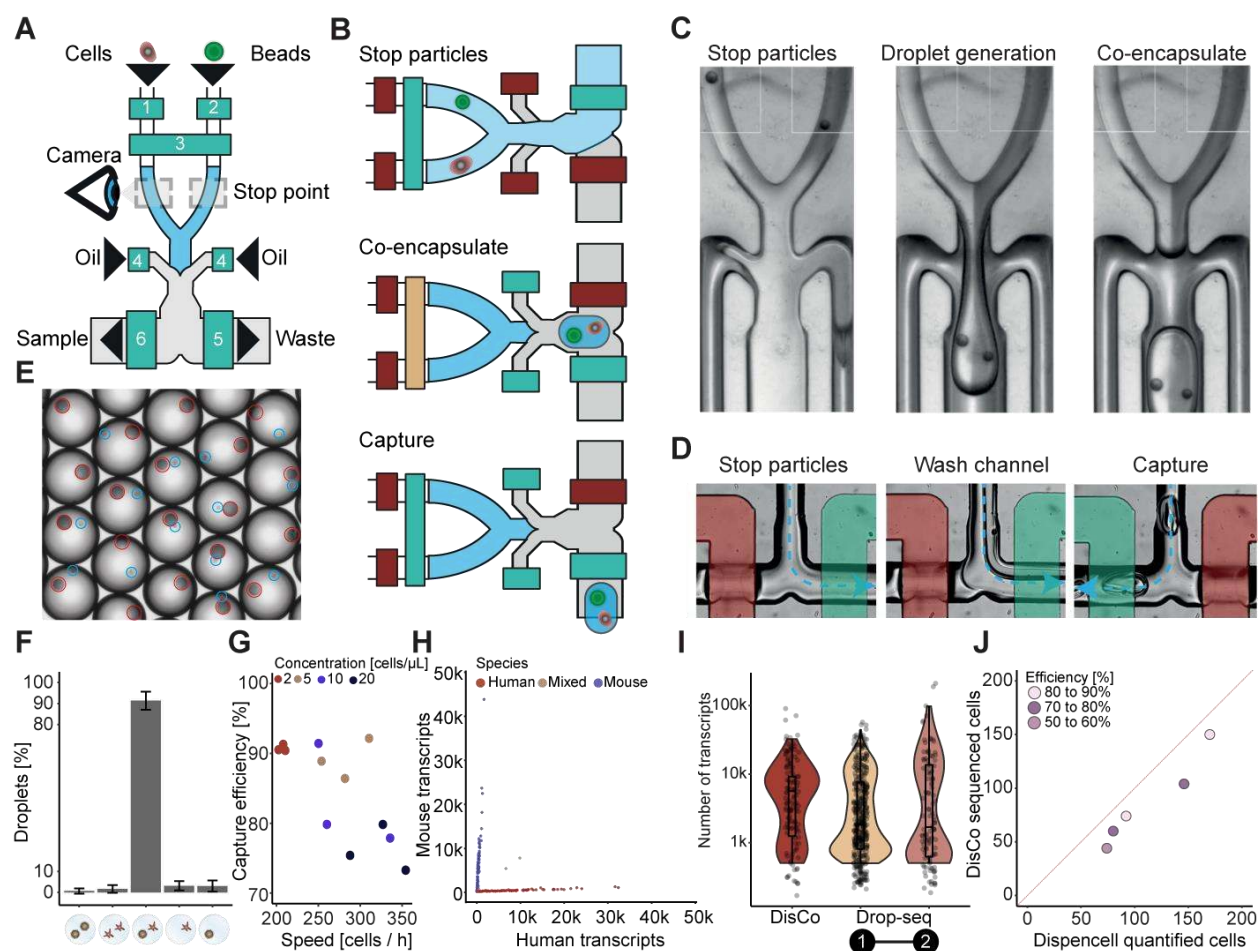
328 **Contributions**

329 BD, JB, and MB designed the study. BD, JB, MB, and JP wrote the manuscript. JB and RD
330 designed and fabricated microfluidic chip. JB developed the machine-vision integration for DisCo.
331 JB and MB benchmarked the system and performed all single-cell RNA-seq experiments. JP, JB,
332 MB, WS, VG, and RG performed data analysis related to single organoid scRNA-seq
333 experiments. JB, SR and MB performed all organoid and cell culture assays. JB, AC, and JR,
334 performed all imaging assays. EA provided critical comments regarding microfluidic chip design
335 and fabrication. MC provided critical comments on intestinal organoid scRNA-seq data analysis.
336 ML provided critical comments regarding intestinal organoid scRNA-seq data and design of critical
337 confirmation experiments. All authors read, discussed, and approved the final manuscript.

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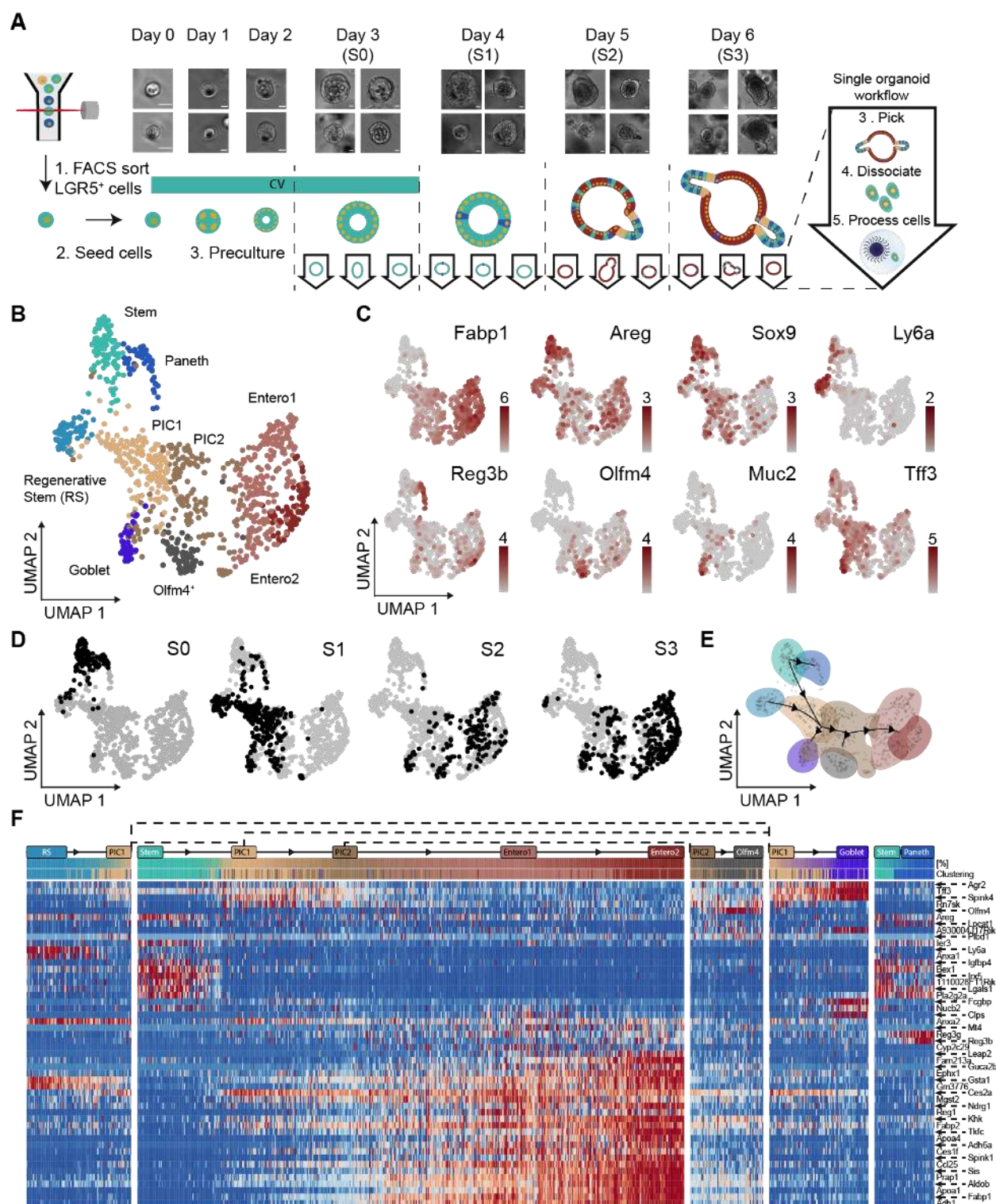
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 446 **Figure 1. Overview and critical feature assessment of the deterministic co-encapsulation (DisCo)**
 447 **system:** (A) Schematics of the DisCo microfluidic device. The device contains three inlet channels for cells,
 448 beads, and oil, and two outlets for waste and sample liquids. All inlets and outlets are augmented with
 449 Quake-style microvalves (green boxes): 1. cell valve, 2. bead valve, 3. dropletting valve, 4. oil valve, 5.
 450 waste valve, 6. sample valve. The device is continuously monitored by a high-speed microscopy camera
 451 to detect and coordinate placement of particles at the Stop point. (B) Illustration of the particle co-
 452 encapsulation process on the DisCo device. Initially, two particles (here a bead and a cell) are stopped
 453 (Stop particles) in close proximity to the channel junctions by closing the channel valves (red: closed, green:
 454 open). Next, by pressurizing the dropletting valve (yellow), both particles are ejected into the junction point,
 455 and the droplet is sheared by opening the oil valve (Co-encapsulate). Finally, the produced droplet is
 456 captured in the Sample channel (Capture). (C) The co-encapsulation process of two beads and droplet
 457 generation as observed on chip. Dyed liquids were used to examine the liquid interface of the carrier liquids.
 458 Channel sections with white squares are 100 μm wide. (D) The droplet capture process as observed on-
 459 chip. Valves are highlighted according to their actuation state (red: closed, green: open). While particles
 460 are stopped, excess buffers are discarded through the waste channel and the channel is flushed with oil
 461 prior to droplet capture. Upon co-encapsulation, the waste valve is closed, the sample valve opened, and
 462 the produced droplet captured in the Sample channel. (E) Images of DisCo droplet contents. Cells (blue
 463 circle) and beads (red circle) were co-encapsulated, and captured droplets imaged. Mean bead-size is
 464 approximately 30 μm. (F) Droplet occupancy of DisCo-processed cells and beads for cell concentrations
 465 ranging from 2 to 20 cells per μl (total encapsulations n = 1203). Error bars represent standard deviation.
 466 (G) Cell capture efficiency and cell capture speed for varying cell concentrations (total encapsulations n =
 467 1203). Cells were co-encapsulated with beads at concentrations ranging from 2 - 20 cells per μl, and co-
 468 encapsulation events quantified by analyzing recordings of the process. (H) DisCo scRNA-seq species
 469 separation experiment. HEK 293T and murine pre-adipocyte iBA cells were processed with the DisCo
 470 workflow for scRNA-seq, barcodes merged, and species separation visualized as a Barnyard plot. (I)

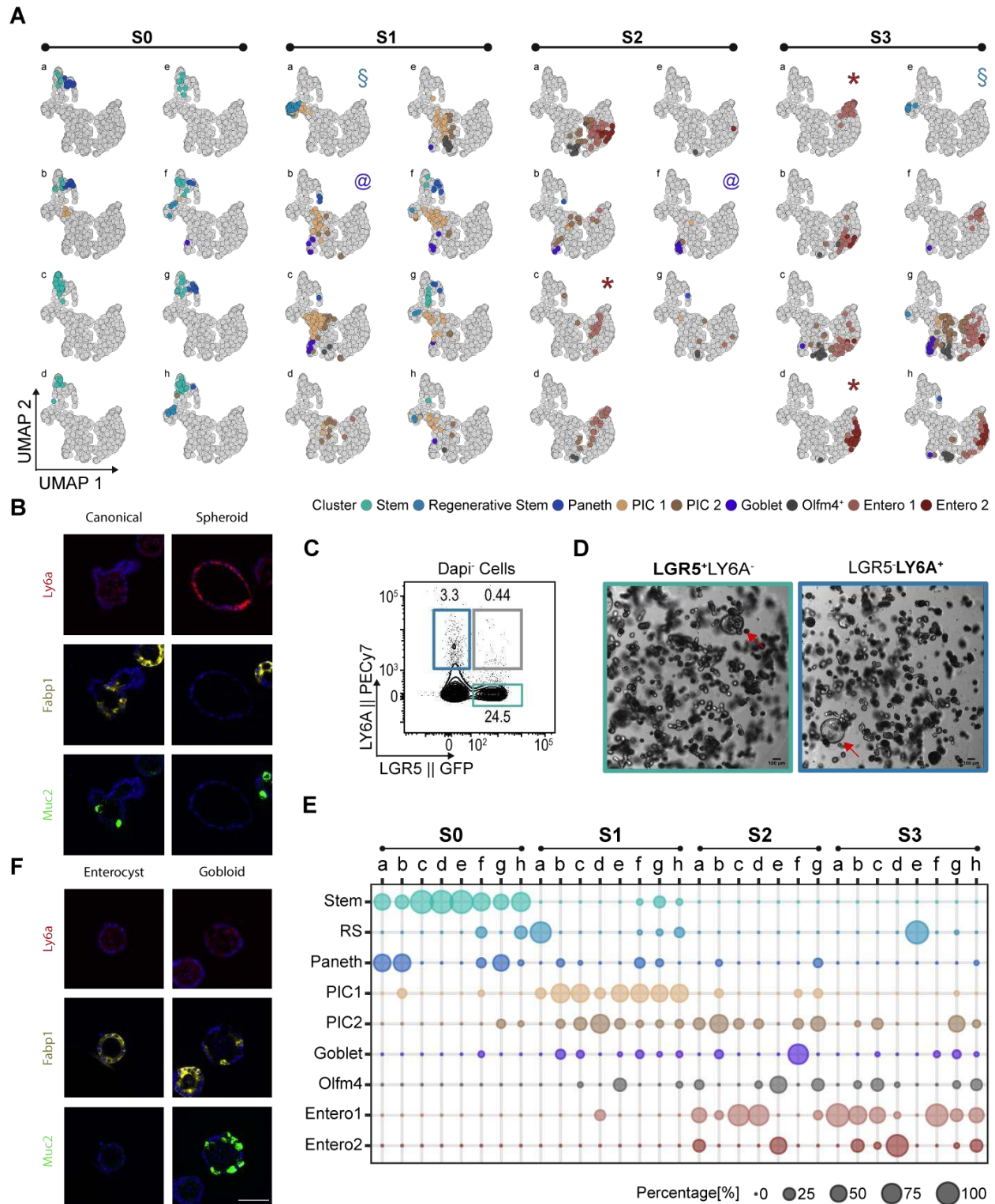
471 Comparison of detected UMIs per cell of conventional Drop-seq experiments. UMIs per cell from HEK 293T
472 data for conventional Drop-seq experiments ([1] - from Biočanin, Bues *et al.* 2019²⁷ and [2] - from Macosko
473 *et al.* 2015²), compared to the barcode-merged HEK 293T DisCo data. Drop-seq datasets were down-
474 sampled to comparable sequencing depth. Box elements are described in the **Materials and Methods**
475 section. (J) Total cell processing efficiency of DisCo at low cell inputs. Input cells (HEK 293T) ranging from
476 74 to 170 were quantified with the Dispencell system. Subsequently, all cells were processed with DisCo,
477 sequenced, and quality filtered (> 500 UMIs). The red line represents 100% efficiency, and samples were
478 colored according to recovery efficiency after sequencing.



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Figure 2. Utilizing DisCo to map intestinal organoid cell heterogeneity along development: (A) Overview of the experimental design for DisCo'ing individual organoids. Single LGR5⁺ intestinal stem cells were isolated via FACS and precultured for 3 days under stem cell maintenance conditions (ENR CV Day 0 to 3). On Day 3, CV was removed from the culture, and organoids differentiated under ENR conditions for up to 3 days. For each day during development (S0 - S3), individual organoids were isolated, dissociated, and processed on the DisCo platform. Representative bright-field imaging examples of

487 individual organoids for each day are shown on top. Scale bar 50 μm . **(B)** UMAP embedding of all
488 sequenced cells. All 945 processed cells from 31 organoids were clustered with k-means clustering, after
489 which clusters were annotated according to marker gene expression. **(C)** UMAP-based visualization of the
490 expression of specific markers that were used for cluster annotation. **(D)** Temporal occurrence of cells.
491 Cells are highlighted on the UMAP embedding according to sampling time point (S0 - S3). **(E)**
492 Developmental trajectory based on the cluster annotation and the sampling time point derived by
493 slingshot³⁴. Cells were annotated in accordance with clustering in (B). **(F)** Heat map of differentially
494 expressed genes along the waypoints of the trajectory. Waypoints are annotated in accordance with cell
495 clustering as in (B). Cluster abbreviations: Stem cells (Stem), Regenerative stem cells (RS), Potential
496 intermediate cells (PIC)³³, Enterocytes cluster 1/2 (Entero1/2).



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Figure 3. Cell type distribution and marker gene expression across individual intestinal organoids during development: (A) Projection of cell types onto 31 individual organoids. Cells per single organoid were colored according to their global clustering and highlighted on the UMAP embedding of all sequenced cells. Projections are grouped according to their sampling time. Manually classified organoids were annotated with the following symbols: “*” enterocysts, “§” spheroids, “@” gobloids. (B) *in situ* RNA detection

504 of *Ly6a*, *Fabp1*, and *Muc2* expression. A representative canonical and *Ly6a*-expressing organoid is
505 displayed. Scale bar (displayed in F) 50 μm . **(C)** Surface LY6A and LGR5-GFP expression under ENR CV
506 conditions. The dot plot depicts LGR5-GFP and LY6A expression in organoid-derived single cell
507 suspensions. The numbers indicate frequencies (%). **(D)** Culturing outcomes of LGR5⁺ cells and LY6A⁺
508 cells. Single LGR5⁺ LY6A⁻ and LGR5⁻ LY6A⁺ cells were isolated by FACS and seeded in Matrigel. Cells
509 were cultured as depicted in **Figure 2a** and imaged using bright-field microscopy at S3. Red arrows point
510 to spheroid morphologies. Scale bar 100 μm . **(E)** Dotplot depicting the distribution of annotated cell types
511 per organoid. Dot size depicts the percentage of cells associated to each cluster per organoid. **(F)** *in situ*
512 RNA detection of *Fabp1* and *Muc2* expression. Selected images resembling the enterocyst and gobloid
513 subtypes. Scale bar 50 μm .