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Development of an empirical process model for adjusted porosity in laser-based powder bed fusion of Ti-6Al-4V

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Abstract

A promising approach to address the mismatch of bone and implant stiffness, leading to the stress-shielding phenomenon, is the application of functionally graded materials with adjusted porosity. Although defect formation and porosity in laser-based powder bed fusion of metals (PBF-LB/M) are already widely investigated, so far there is little research on the influences and parameter interactions regarding the pore characteristics. This work therefore aims to provide an empirical process model for the generation of gas porosity in the PBF-LB process of Ti-6Al-4V. Parts with closed locally adjusted porosity of $\sim 6 \%$ achieved through gaseous pores instead of lack of fusion defects or lattice structures were built by PBF-LB. Parameter variation and evaluation of relative density, pore size and sphericity was done in accordance with the design of experiments approach. A parameter set for maximum gas porosity (laser power of 189 W, scanning speed of 375 mm/s, hatch spacing of 150 m) was determined for a constant layer thickness of 30 m and a spot diameter of 35 m. Tensile tests were conducted with specimens consisting of a core with maximum gas porosity or lack of fusion porosity, respectively, and a dense skin as well as fully dense specimens. Whereas lack of fusion defects can lead to significant reduction of stiffness of 32.2 %, the elastic modulus remained unchanged at 110.0 GPa when implementing spherical pores. Nevertheless, the found superior strength and ductility of specimens with gas porous core (> 1100 MPa and > 0.05 mm/mm, respectively) underline the advantages of adjusted porosity for the application in functionally graded materials and lightweight applications.

Keywords Additive manufacturing \cdot Laser-based powder bed fusion \cdot Porosity \cdot Functionally graded materials \cdot Ti-6Al-4V \cdot Design of experiments

1 Introduction

Additive manufacturing (AM) technologies allow the production of individually shaped parts and small lot sizes without additional costs. A popular example of a promising application is the realization of customized implants [1–4]. The most commonly used metal AM technology is laser-based powder bed fusion of metals (PBF-LB/M) [5], in which the distributed powder layers are selectively melted by a laser under inert gas atmosphere. PBF-LB offers the advantages of a wide range of processable materials [6–9] and the ability to manufacture high-resolution parts [10]. Furthermore, recycling and reuse of the metallic powder is possible [11–14], increasing the material utilization.

One of the most intensively investigated materials for PBF-LB is Ti-6Al-4V (Ti – 6 wt% Al – 4 wt% V) [6, 15, 16]. The (α + β)-titanium alloy is known for its low density, high strength, fracture toughness and corrosion resistance as well as excellent biocompatibility [17–19]. It is therefore a suitable material for load bearing implants. However, as the Young's modulus of titanium is 110 GPa while it is only 10 to 30 GPa for human bone, stress-shielding is a well-known drawback [20, 21]. By shielding the bone from the stress applied to load-bearing implants, it is insufficiently loaded so that, based on Wolff's law [22], bone resorption is increased and bone atrophy (reduction and loss of bone tissue) occurs. The resulting eventual loosening of the implant thus leads to a reduction in implant lifetime [20].

To address this challenge and reduce the implant's stiffness, there mainly exist two different approaches, i.e. the stiffness reduction of the material itself, e.g. by using low stiffness alloys, and the stiffness reduction of the part by adjustment of the design and introduction of porosity. In this work, the second approach, i.e. porous materials, which

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has been proposed by Oh et al. [23], is of major interest. These materials are characterized by the presence of voids, which can be open or closed and of more or less regular kind [24]. Thereby, open means that a fluid from outside the structure could infiltrate the void while closed pores are completely surrounded by dense material and therefore inaccessible for fluids from the outside. Increased porosity generally reduces the mechanical properties [25], so that an increase of pore size can lead to a reduction of the Young's modulus because of wall thickness thinning [26]. As stated by Gibson and Ashby, the mechanical response of porous material is mostly influenced by the relative density ρ_{Rel} , defined as the ratio of the density ρ_P of the porous material and the density ρ_S of the solid material [27]:

$$\rho_{\rm Rel} = \frac{\rho_{\rm P}}{\rho_{\rm S}} \tag{1}$$

According to Eq. 2, ρ_{Rel} has a quadratic influence on the elastic modulus [25], whereby E_P stands for the elastic modulus of the porous material and E_S for the one of the solid material.

$$E_{\rm P} = \left(\frac{\rho_{\rm P}}{\rho_{\rm S}}\right)^2 E_{\rm S} \tag{2}$$

Besides the desired reduction of implant stiffness, the side effects of porous structures on other mechanical properties, e.g. ductility, tensile strength, compressive strength and fatigue, can be detrimental and need to be taken into consideration.

Functionally graded materials (FGM) are a topic that has recently attracted growing attention in terms of application in implants and stiffness adjustment. FGM are characterized by internal variations regarding their composition, microstructure or macrostructure across the volume and therefore by graded properties. These different areas can merge continuously or be clearly delimited from one another and are usually graded in a single direction [28]. According to Mahmoud and Elbestawi, there are three types of gradients: composition gradient, microstructure gradient and porosity gradient [29]. Of these types, the porosity gradient is of special interest in this work.

Additive manufacturing, especially powder bed fusion technologies, are not only capable to overcome the limitations of conventional manufacturing techniques in terms of porosity adjustment, but they also allow the fabrication of complex geometries and therefore cellular materials and lattice structures for FGM [30]. To enable the removal of loose powder after the process, the additively manufactured structures need to exhibit an open-cell lattice structure [31]. To achieve a Young's modulus similar to human bone, a Ti-6Al-4V structure with 65 % porosity would be necessary [32]. This can be achieved with different lattice structures, stochastic and non-stochastic, including TPMS structures (triply periodic minimal surfaces), each

of which offers different advantages [29]. The open porosity also facilitates bone ingrowth and osseointegration, which, if desired, ensures permanent integration of the implant in the body so that additional cementing of the implant is not necessary [33]. Numerous studies have been conducted to examine the additive manufacturing of openporous lattice structures for use in biomedical applications (e.g. [31–35]). However, if bone ingrowth is undesirable, for example with non-permanent implants, open-cellular structures are disadvantageous and closed internal pores are preferable. Additionally, open-cellular structures show anisotropic deformation behavior, affected by pore size and shape as well as orientation, arrangement and distribution of pores [36], which can also be a detrimental property. Since powder cannot be removed from closed voids after processing, the application of lattice structures designed by CAD (computer aided design) is not suitable. Instead, porosity needs to be achieved by adjusting the processing parameters.

Generally, there are two types of process-related pores in parts manufactured by PBF-LB/M, irregular shaped lack of fusion (LOF) defects and spherical pores attributed to gas entrapment [37, 38]. LOF defects are of elongated, irregular shape and of strongly varying size. They cause higher stress concentrations than spherical gas pores due to the notch effect. Consequently, the mechanical behavior is impaired to a greater extent [39], especially when the load is applied in build direction [40]. On the contrary, gas porosity shows a spherical morphology that is less critical for the propagation of cracks [39]. Its impact on the mechanical properties is also independent of the load direction [40]. There have already been previous works that have focused on the active generation of closed process-related porosity by powder bed fusion technology. Yun et al. used TiH₂ as a decomposing pore-forming agent to achieve closed, gaseous pores in PBF-LB of Ti [41]. However, the observed pores were not spherical and could thus be detrimental for the tensile or fatigue properties. Li et al. varied the scanning speed to achieve graded porosities in 316L stainless steel samples based on lack of fusion defects [42]. Jeon et al. investigated the active control of porosity for the direct laser melting process of Fe powders. They demonstrated the feasibility of producing parts with graded porosity by variation of powder morphology and processing parameters. The created pores were mainly of non-spherical morphology [43]. Jafari et al. investigated the influence of processing parameters in the PBF-LB process on porosity characteristics, i.e. total porosity and pore size, with the aim to generate open LOF porosity and to increase wettability of the structures [44]. Elsayed et al. used DoE (Design of Experiments) to find a combination of process parameters that introduces porosity in a component made of Ti-6Al-4V high enough to reach the elastic modulus of human bone [45]. Therefore,

they used higher laser scanning speeds and lower laser powers than would be necessary for a dense component, so that the powder was not completely melted and LOF defects occurred. Lin et al. followed a similar approach, but only varied the laser power for a fixed scanning speed (1250 mm/s), layer thickness (30 m) and hatch spacing (10 m) [46]. The porosity can thus be also attributed to LOF defects. Cylindrical specimens with a porous core and a dense skin with varying thickness were built. The parts can therefore be regarded as FGM. Fousová et al. also followed the approach of mimicking the bone structure and produced cylindrical specimens with radially graded latticebased porosity, showing that the mechanical properties decrease linearly as the porosity increases [47]. A similar approach was also studied by Zhang et al. [48]. Besides the aim to generate FGM, a related technique, the hull-bulkstrategy, is also applied to increase the productivity of the process. For this purpose, the core is typically processed with a larger layer thickness than the hull resulting in higher porosity in the core [49, 50]. The mentioned studies focussed on the realization of porous structures or FGM by implementation of lattice structures or LOF defects. So far, there is little research considering the fabrication of functionally graded materials with adjusted porosity by generation of spherical gas pores. These are typically looked at as undesired defects and thus avoided. In consequence, processing maps and models are not designed for obtaining specific pore characteristics but to achieve components with maximum density. They are also lacking broader porosity information like sphericity or mean pore size. The aim of the presented work therefore is to thoroughly investigate the effects of the main processing parameters on these porosity characteristics as well as their interactions. By employment of the DoE approach, an empirical process model is developed allowing the prediction and adjustment of graded porosity. Feasibility of the fabrication of FGM with porosity gradient is demonstrated and its influence on tensile properties is studied.

2 Materials and methods

2.1 Experimental materials

The powder material used in this work was gas atomized Ti-6Al-4V grade 23 powder supplied by Heraeus additive manufacturing GmbH with a specified particle size of 15–53 m. According to the manufacturer's data sheet, the size distribution of the virgin powder exhibits the *D*-values 22 m (D10), 38 m (D50) and 54 m (D90). Since the reuse of powder is of growing interest for industrial applications, the powder was used after multiple recycling so that a narrower size distribution and a slightly improved

flowability can be assumed [5]. The scanning electron microscopy (SEM) analysis (Fig. 1) showed that the powder particles are mainly spherical with a smooth surface and of similar size.

2.2 Experimental equipment

The specimens were built on an industrial machine, Lasertec 12 SLM by DMG MORI GmbH (Bielefeld, Germany), that is equipped with a 400 W ytterbium fiber laser (single mode, continuous wave, wavelength 1070 nm). It supplies a high-quality laser beam ($M^2 = 1.05$) with a minimum spot diameter of 35 m. The process was carried out under argon atmosphere with a residual oxygen content of 0.13 vol% - 0.15 vol%. A Ti-6Al-4V build plate was used. The tensile tests were performed according to DIN EN ISO 6892-1:2020-06. They were conducted using an MTS Landmark 100 kN and an MTS axial extensometer with a gauge length of 25 mm. A crosshead speed of 0.42 mm/min equivalent to an initial strain rate of 2.5 x 10^{-4} s⁻¹ was implemented.

2.3 Experimental design

In order to develop the empirical process model that describes the influences on porosity and porosity characteristics, three experimental runs were conducted. Therein, cubic specimens with a side length of 5 mm were built upon 3 mm support structures. The experimental design for all runs in accordance with the DoE approach was generated using the statistics software JMP® (SAS Institute Inc.). The first run (screening run) was meant to give an overview over a broad parameter window and to find general parameter settings for high gas porosity. The second run (main

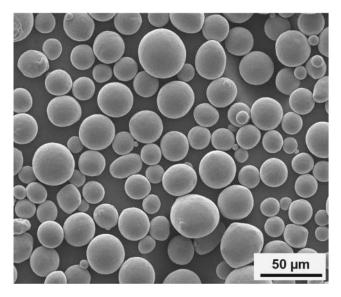


Fig. 1 SEM image of used Ti-6Al-4V powder

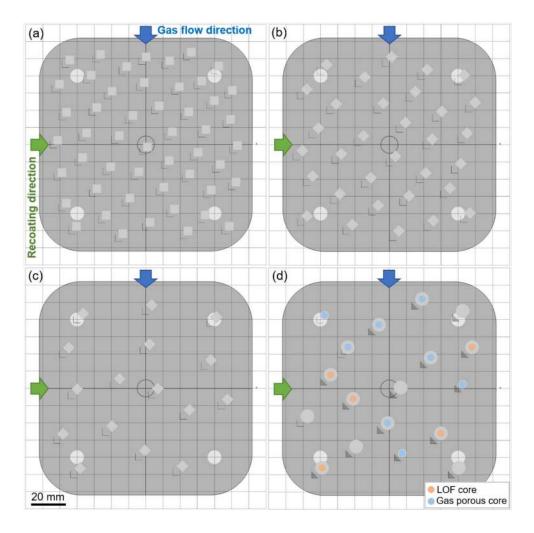
			Factor Levels		
Run	Design	Specimen number	P in W	<i>v</i> in mm/s	<i>h</i> in m
Screening	JMP® Custom	50	50, 100, 150, 200, 250	300, 650, 1000, 1350, 1700	30, 60, 90, 120, 150
Main	Central Composite	32	80, 100, 160, 220, 240	200, 250, 400, 550, 600	30, 45, 90, 135, 150
Verification	Central Composite	16	80, 100, 160, 220, 240	200, 250, 400, 550, 600	30, 45, 90, 135, 150

Table 1 Experimental runs and their experimental design, specimen number and factor levels

run), was conducted to narrow the processing window and was based on the findings of the screening run. As a third run, the verification run was implemented to confirm the results from the previous main run and thus investigate the reproducibility and to refine the statistical model.

Different experimental designs and numbers of specimens were realized for the experimental runs. Table 1 gives an overview of the applied design, specimen number and the levels of the varied factors, i.e. the varied process parameters. Figure 2 shows the build job layouts for all experimental runs. For the screening run, a custom design was selected for a number of 50 specimens. To generate a custom design, the statistics software tailors the experimental design for the specific needs, e.g. a given number of specimens and the effects that the user wants to evaluate. For the following two runs, a circumscribed central composite design (CCD) with $\alpha = 4/3$ (axial distance of star points to the center) was implemented, so that first- and second-order

Fig. 2 Build layouts: (a) screening run; (b) main run; (c) verification run; (d) demonstration parts and tensile test specimens



terms, including two-factor interaction effects, can be estimated. Figure 3 shows a circumscribed CCD. The advantage of this design is that combinations of extreme values are evaded. Within the main run, the central point was repeated four times and all other parameter combinations two times. For the verification run, the main run was repeated with half of the specimens. The verification run served to compare the results between different build jobs and verify that the observed effects are not caused by the build job conduction itself due to possible variation of surrounding factors like temperature or humidity. The mathematical model was fitted based on both, the results from the main as well as from the verification run. A significance level of 5 % was chosen. All not significant terms (*p*-value > 0.05) were excluded under the condition that there were no significant dependent higher order effects following the principle of strong effect heredity. The mathematical model was fitted using the least squares method.

As displayed in Table 1, the varied parameters for all conducted experimental runs were laser power P, scanning speed v and hatch spacing h. The preheating temperature of the build platform and the layer thickness t were kept constant for all experiments at 100 °C and 30 m, respectively. A cross-hatching strategy with a rotation angle of 67° between adjacent layers was applied to realize isotropic properties in horizontal direction. The specimens were placed randomly on the build plate to exclude the influence of the position determined by direction of gas flow and recoater movement. Based on the predictions of the empirical model, cylindrical specimens (height: 5 mm, diameter: 5 mm) with a porous core and a dense skin were processed to demonstrate the feasibility of realizing graded structures with the determined processing parameters and to allow a later transfer to cylindrical tensile test samples. The

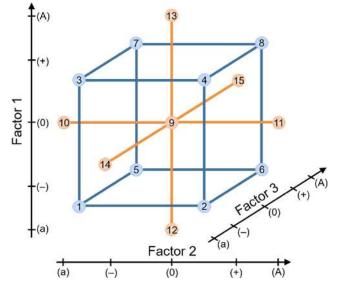


Fig. 3 Central composite design with corner points (1–8), central point (9) and star points (10–15)

porous core had an effective diameter of 3.8 mm and the dense skin had an effective thickness of 0.5 mm. Between them, there was a transition zone with a thickness of 0.1 mm to ensure sufficient bonding (Fig. 4). This zone was processed with both parameter sets for high and low porosity, respectively.

Finally, tensile test specimens were processed in accordance with DIN EN ISO 6892-1:2020-06. For this purpose, they were built with a slightly larger diameter compared to the final geometry and were subsequently machined by turning to eliminate the influence of the rough as-built surface. As a specimen geometry test shape B (Fig. 5) was chosen with the parameters given in Table 2.

Specimens were built in three conditions: fully dense, with porous core due to gas porosity and with porous core due to LOF defects. The dimensions for the core and transition zone were the same as for the cylindrical specimens. The according processing parameter combinations are provided in Table 3. For the demonstration parts and tensile test specimens, different parameter settings were implemented for the core and the skin to generate different densities. They are listed in Table 3. The parameter set that is predicted to lead to maximum gas porosity according to the empirical model was chosen for the porous core. For the skin, a parameter set that leads to high density was used. Three demonstration parts were manufactured to show the feasibility and reproducibility of FGM and

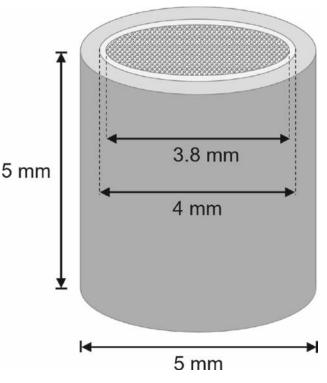
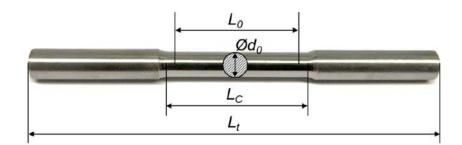


Fig. 4 Geometry of cylindrical specimens with porous core and dense skin

Fig. 5 Geometry of tensile test specimens



five tensile test specimens were manufactured for each modification.

2.4 Porosity analysis

All specimens were cold embedded in epoxy resin (Technovit Epox, Kulzer GmbH, Hanau, Germany), ground and polished (Tegramin, Struers ApS, Ballerup, Denmark). Three cross-sections were made for every specimen parallel to the build direction (BD). For analysis of the metallographic cross-sections light microscopy (Olympus BX60 by Olympus Europa SE & Co. KG) was employed. The single microscopic images were stitched and analyzed using a python script developed at Laser Zentrum Hannover (LZH). This script includes the image transformation to black and white with a given threshold value and a subsequent calculation of the relative density (ratio of black and white pixels), average pore size and average two-dimensional sphericity-equivalent. The relative density in percentage was calculated according to Eq. 3.

$$\rho_{\text{Rel}\,\%} = \left(1 - \frac{\sum Area_{pores}}{Area_{Cross-Section}}\right) \cdot 100\,\% \tag{3}$$

According to Wadell [51], the true three-dimensional sphericity ψ_{3D} can be calculated by comparing the surface, which a sphere with the same volume *V* would have, to the actual surface *O* of the regarded object:

$$\psi_{3\mathrm{D}} = \frac{\pi^{\frac{1}{3}} (6V)^{\frac{2}{3}}}{O} \tag{4}$$

Since the cross-sections only allow a two-dimensional representation of the pores, a two-dimensional equivalent

Table 2Tensile test shape B according to DIN EN ISO 6892-1:2020-06

d ₀	L ₀	L _c	Lt
5 mm	25 mm	28 mm	80 mm

1

of the sphericity ψ_{2D} is needed. Therefore, the ratio of the perimeter of a circle with the same area *A* and the actual perimeter *U* is calculated as shown by the following equation:

$$\psi_{\rm 2D} = \frac{2\sqrt{\pi A}}{U} \tag{5}$$

The sphericity and two-dimensional sphericityequivalent are equal to 1 for a sphere and a circle area, respectively. The demonstrator parts were analyzed using the same procedure as for the cubic specimens as well as computer tomography (CT). This technique enables a threedimensional insight into the pore morphology, volume and pore distribution within the specimens. For the evaluation, the volume energy density E_V was used as an additional metric that allows the combination of the varied processing parameters. It was calculated according to Eq. 6.

$$E_{\rm V} = \frac{P}{vht} \tag{6}$$

3 Results

The results of the described experiments are presented below. This includes the development and verification of an empirical process model from the data obtained in the screening, main and verification run, which describes the relationship between the response variables and the factors. The obtained functionally graded demonstration parts are presented. Moreover, a comparison of the tensile properties of specimens manufactured with different parameter combinations and core porosities is given.

3.1 Screening run

At low volume energy density, relatively low relative densities occurred. High relative densities were achieved with a medium volume energy density around 100 J/mm³ (Fig. 6). At higher volume energy densities, specimens with very different relative densities were found. As Fig. 6 shows, the sphericity-equivalent increases with increasing volume energy density. High porosity of over 10% is only achievable with irregular shaped non-spherical

 Table 3 Parameter settings for demonstration parts and tensile test specimens

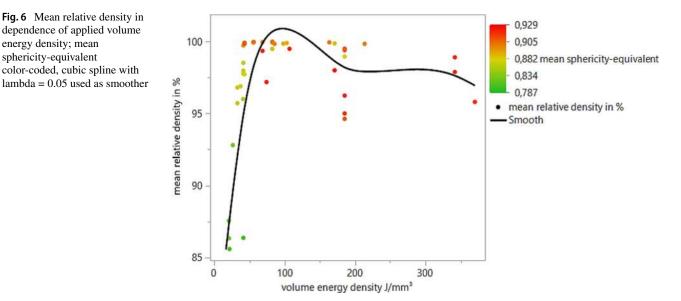
	P in W		v in mm/s		h in m	
Specimen type	Skin	Core	Skin	Core	Skin	Core
Demonstration	145	189	1000	375		150
		189		375	80	150
Tensile test	145	145	1000	1000	80	80
		50		650		120

pores, i.e. LOF defects. This is also demonstrated by the cross-sections (Fig. 7). For all specimens, the pores were randomly distributed within the specimen volume. The mean sphericity-equivalent was between 0.79 (P =100 W, v = 1350 mm/s, h = 150 m) and 0.93 (P =100 W, v = 650 mm/s, h = 30 m). For specimens with a mean sphericity-equivalent below 0.89, LOF porosity could be seen in the cross-sections. With a mean sphericityequivalent of 0.90, high relative densities of over 99.70 % occurred. For mean sphericity-equivalents of over 0.91, there were both high and low density specimens and the microscopic images showed gas porosity. A transition range of the mean sphericity-equivalent of 0.89 to 0.91 could be defined. LOF porosity occurs for lower and gas porosity for higher values. The evaluation of the screening run showed that for high spherical porosity, low scanning speeds and medium to high laser powers are favorable, whereby there is a strong interaction effect between these two parameters based on the resulting volume energy density. The hatch spacing showed a smaller influence. With an increasing hatch spacing, the relative density and sphericity-equivalent decrease. To enable a more precise prediction of the porosity characteristics for gas porosity, the main and verification run were subsequently conducted.

energy density; mean sphericity-equivalent

3.2 Main and verification run

Based on the findings from the screening run, lower scanning speeds and a slightly smaller range of the laser power where chosen for the main and verification run (Table 1). This way, the parameter window for the desired spherical porosity was investigated more closely to maximize the porosity for later application in FGM. In general, the verification run led to results comparable to the main experimental run, with a mean relative density of 97.11 % in the main run and 97.10 % in the verification run. However, the parameter combinations for which maximum or minimum values of the porosity characteristics were obtained were partly different for the two runs. Furthermore, it was noticed, that the deviation of properties between specimens built with the same parameter settings were larger than the deviations within a specimen between the evaluated cross-sections. This high variation of properties explains the observed differences between the two runs. The causes of the variations themselves can be of diverse nature. Since the experiments were conducted on different days, environmental influences like temperature and humidity could have influenced the process. Furthermore, there were differences in the build job layouts that might also be



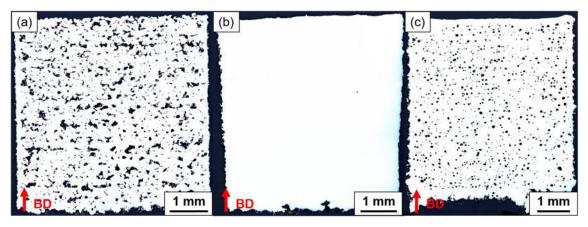


Fig. 7 Light microscopy images of cross-sections: (a) LOF porosity (P = 100 W, v = 1350 mm/s, h = 120 m), (b) nearly fully dense (P = 200 W, v = 1350 mm/s, h = 60 m), (c) gas porosity (P = 100 W, v = 300 mm/s, h = 60 m); red arrow indicates build direction

influential. Nevertheless, the maximum spherical porosity achieved was comparable, with 92.52% relative density in the main run and 92.62% in the verification run (in both runs for P = 100 W, v = 400 mm/s, h = 90 m). Based on the results for the pore characteristics obtained within the main and the verification run, an empirical model was developed to enable the prediction and adjustment of spherical porosity.

3.3 Empirical model

All terms that were not significant according to their *p*-value were removed from the model, except for those terms on which higher order effects depended (principle of strong effect heredity). The parameter estimates, as well as their standard error, *t*-ratios (estimates divided by their standard error) and the respective *p*-values are provided in Table 4.

For the relative density $\rho_{\text{Rel}_{\%}}$, the hatch spacing did not have a significant influence but remained in the model because the dependent interaction effect of hatch spacing and laser power was significant. The interaction effect of laser power and scanning speed was also significant while the one between scanning speed and hatch spacing was not. Furthermore, laser power and scanning speed also had a quadratic influence on the relative density, as it can be seen in Table 4 and in the prediction (7) in the last two terms.

This equation shows the parameter estimates, i.e. the coefficients in front of the different terms, which provide information on the influence of the different effects. It can be seen that the quadratic effect of the laser power has the strongest influence on the relative density with a parameter estimate of 2.87%. Besides the insignificant hatch spacing with a parameter estimate of -0.46%, the linear effect of the scanning speed is the weakest (1.02%). The model

Model	Term	Estimate	Std. error	<i>t</i> -ratio	<i>p</i> -value
$\rho_{\text{Rel}_{\%}}$	Intercept	94.99	0.39	246.66	< 0.0001
	Laser power ²	2.87	0.56	5.09	< 0.0001
	Scanning speed ²	2.24	0.56	3.98	0.0003
	Laser power · scanning speed	-1.26	0.49	-2.58	0.0135
	Laser power	-1.14	0.30	-3.76	0.0005
	Laser power · hatch spacing	-1.10	0.49	-2.26	0.0296
	Scanning speed	1.02	0.30	3.37	0.0017
	Hatch spacing	-0.46	0.30	-1.50	0.1412
$\psi_{ m 2D}$	Intercept	0.924	0.002	407.14	< 0.0001
	Laser power	-0.010	0.004	-2.44	0.0188
	Laser power ²	0.006	0.002	2.77	0.0081
A _P	Intercept	1799.08	103.32	17.41	< 0.0001
	Laser power	411.29	162.09	2.54	0.0147
	Hatch spacing	-359.26	162.09	-2.22	0.0318

 Table 4
 Parameter estimates of the fitted models

can be visualized by the contour plots (Fig. 8). It can be seen that there is an optimum area of minimum relative density (maximum porosity) for a scanning speed between 325 and 425 mm/s and laser power between 150 and 190 W. At scanning speeds under 500 mm/s, there is a stronger influence of the laser power. For low laser powers under

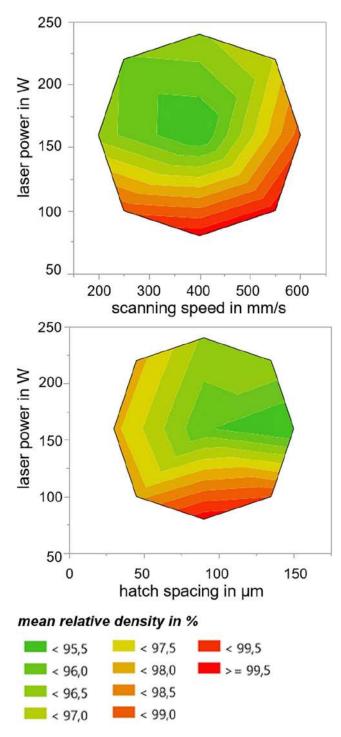


Fig. 8 Contour plots for mean relative density in dependence of laser power, scanning speed and hatch spacing

125 W, the mean relative density is nearly independent of the hatch spacing but for higher laser power, it decreases with increasing hatch spacing. It is also visible that the influence of the laser power is stronger at higher hatch spacings. In general, low relative density can be obtained for medium laser power of around 150 W and high hatch spacings over 100 m.

$$\begin{aligned} \rho_{\text{Rel},\%} &= 94.99\,\% - 1.14\,\% \cdot \frac{P - 160\,W}{80\,W} + 1.02\,\% \cdot \frac{v - 400\,\frac{mm}{s}}{200\,\frac{mm}{s}} \\ &- 0.46\,\% \cdot \frac{h - 90\,m}{60\,m} - 1.26\,\% \cdot \frac{P - 160\,W}{80\,W} \cdot \frac{v - 400\,\frac{mm}{s}}{200\,\frac{mm}{s}} \\ &- 1.10\,\% \cdot \frac{P - 160\,W}{80\,W} \cdot \frac{h - 90\,m}{60\,m} + 2.87\,\% \cdot \left(\frac{P - 160\,W}{80\,W}\right)^2 \\ &+ 2.24\,\% \cdot \left(\frac{v - 400\,\frac{mm}{s}}{200\,\frac{mm}{s}}\right)^2 \end{aligned}$$
(7)

The sphericity-equivalent ψ_{2D} only depended on the laser power. The linear as well as the quadratic influence of this parameter were significant according to their *p*-values (Table 4). Equation 8 represents the prediction equation. According to the empirical model, a maximum sphericity of 0.92 can be achieved for a laser power of 200 W.

$$\psi_{2\mathrm{D}} = 0.92 + 0.01 \cdot \frac{P - 160 W}{80 W} - 0.01 \cdot \left(\frac{P - 160 W}{80 W}\right)^2 (8)$$

For the mean pore area A_P the prediction (9) and Table 4 show that only the linear effects of laser power and hatch spacing are significant whereby the influence of the laser power is stronger. The pore size increases with increasing laser power and decreasing hatch spacing without reaching a maximum or minimum. This is also illustrated in Fig. 9.

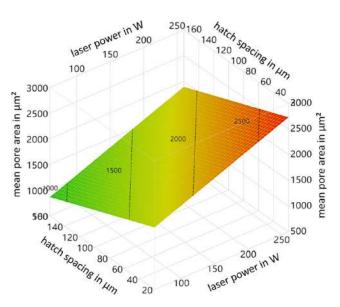


Fig. 9 Response surface of mean pore area in dependence of laser power and hatch spacing

 Table 5
 Predicted pore characteristics for maximized gas porosity

$\rho_{\text{Rel}_{\%}}$ in %	$\psi_{2\mathrm{D}}$	A_P in m^2
94.06 ± 1.01	$0.92\pm0.00^*$	1588.91 ± 404.84

*< 0.005

$$A_{\rm P} = 1799.08 \quad m^2 + 411.29 \quad m^2 \cdot \frac{P - 160 W}{80 W}$$
$$-359.26 \quad m^2 \cdot \frac{h - 90 \ m}{60 \ m} \tag{9}$$

Since the aim of this study was to obtain maximum spherical porosity to reduce the stiffness, the parameter setting for the demonstration parts was chosen according to the predicted relative density. Here, a minimum can be realized with P = 189 W, v = 375 mm/s and h = 150 m. For this parameter combination, the porosity characteristics given in Table 5 are predicted by the developed model.

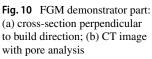
3.4 Functionally graded demonstration parts

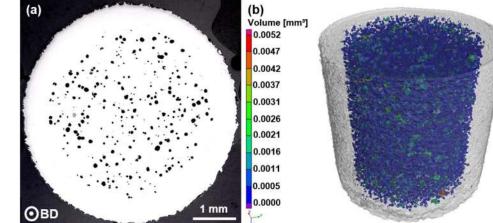
The cylindrical specimens with dense skin and porous core could all successfully be realized with the determined parameters for high spherical porosity. No significant differences between the three specimens could be observed. The density was evaluated for the entire part as well as only for the core. For the core a mean relative density of 94.39 % and for the entire part a mean relative density of 96.11 % was obtained, which was higher due to the inclusion of the dense skin. Figure 10 shows a metallographic cross-section (a) as well as a CT image (b) with analysis of pore volumes. The porous core can be clearly distinguished from the dense skin. The analysis of the pore volume shows a homogeneous color distribution within the core are of a similar size (blue

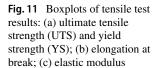
and green) and there are only a few exceptionally large pores (orange and red).

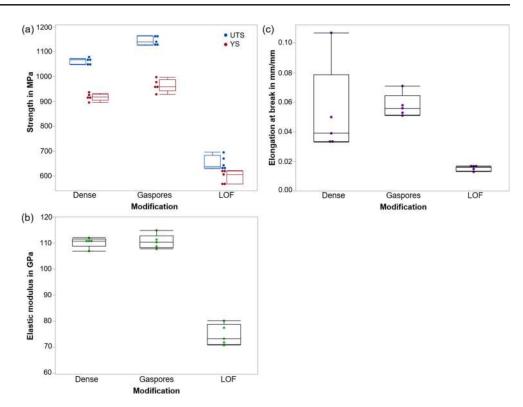
3.5 Tensile tests

Tensile tests were conducted for specimens with three different conditions: fully dense, dense skin and porous core with gas pores and dense skin with porous core with LOF defects. The used implemented processing parameters were selected based on the machine manufacturers recommendations and based on previous results leading to maximum gas porosity ($\sim 6\%$) and high LOF porosity ($\sim 15\%$), respectively (Table 3). Figure 11 shows the results regarding ultimate tensile strength (UTS), yield strength (YS), the elongation at break and the elastic modulus with the respective boxplots. The detailed values of all specimens can be found in Table 6. It can be seen that the specimens with gas pores had the highest strength while the lowest strength was achieved for the specimens with a LOF core. However, the dense specimens showed the smallest standard deviation of the strength values. Regarding the elongation at break, a similar trend could be observed in comparison to the strength. Although one of the fully dense specimens had a significantly larger elongation of over 0.10 mm/mm, the other specimens all showed elongations between 0.03 and 0.05 mm/mm. In contrast, specimens with a gas porous core showed larger elongations between 0.03 and 0.07 mm/mm, the specimens with LOF core showed significantly smaller elongations below 0.02 mm/mm. Fully dense and gas porous specimens showed the same mean elastic modulus of 110.0 GPa with a small standard deviation whereas a significant reduction of the elastic modulus could only be achieved by the porous core with LOF defects (74.6 GPa). This is equivalent to a stiffness decrease of 32.2 %. For this specimen modification the standard deviation was also larger than for the fully dense or gas porous specimens.









4 Discussion

This research showed the correlations between processing parameters and porosity characteristics by developing an empirical process model and demonstrated differences in the mechanical behaviour for different types of porosity. Table 7 summarizes the findings regarding the implemented core porosity and the resulting mechanical properties (means and standard deviations).

The aim was to find suitable parameters for high spherical porosity for the application in FGM to evade the disadvantages of porosity achieved through LOF defects and reduce the stiffness. To do so, three experimental runs were conducted. It could be shown that the volume

Table 6 Results of tensile tests for the three modifications dense, gas porous core and core with LOF defects

	Specimen-ID	Elastic modulus in GPa	Yield strength in MPa	Ultimate tensile strength in MPa	Elongation at break in mm/mm
Dense	D1	106.9	895.99	1050.26	0.107
	D2	112.0	931.46	1069.30	0.039
	D3	111.1	917.61	1066.85	0.033
	D4	110.7	924.72	1072.92	0.050
	D5	110.6	913.36	1048.20	0.034
Gas pores	G1	108.7	928.99	1140.25	0.052
	G2	114.9	997.75	1165.43	0.056
	G3	110.3	958.50	1159.15	0.051
	G4	110.6	977.78	1124.46	0.058
	G5	107.7	959.21	1133.04	0.071
LOF defects	L1	73.3	606.65	638.36	0.013
	L2	77.5	617.88	670.37	0.014
	L3	70.8	568.88	634.56	0.017
	L4	71.4	567.82	630.03	0.016
	L5	80.2	622.60	695.20	0.016

Core Type	Core porosity in %	Mean elastic modulus in GPa	Mean yield strength in MPa	Mean ultimate yensile strength in MPa	Mean elongation at break in mm/mm
Dense	< 0.5 %	110.26 ± 1.75	916.63 ± 12.03	1061.51 ± 10.23	0.053 ± 0.028
Gas	$\sim 6\%$	110.44 ± 2.47	964.45 ± 22.83	1144.47 ± 15.52	0.058 ± 0.007
LOF	$\sim \! 15 \%$	74.64 ± 3.64	596.77 ± 23.78	653.70 ± 25.15	0.015 ± 0.001

 Table 7
 Summary of study results for mechanical properties

energy density influences the relative density and the

sphericity of pores and therefore the type of porosity. Low energy densities result in insufficient melting of the powder layer and thus a lack of fusion between adjacent layers. Consequently, large, irregular shaped LOF defects can be observed. On the other hand, high energy inputs lead to large melt pools, evaporation and keyhole formation. Gas bubbles are entrapped in the melt and due to high solidification rates, they cannot escape before solidification and remain in the part in form of spherical pores [39]. However, the influences of the process parameters included in the volume energy density (see Eq. 6) on the porosity are quite different, as it was also stated by Elsayed et al. [45]. Hence, although it might be convenient, when investigating the PBF-LB/M process, one should not focus on this metric alone but rather should take a closer look on the underlying parameters and their interactions. As this study focused on the spherical gas porosity, the parameter ranges for the main and verification runs were adjusted so that porosity due to LOF defects was excluded. An essential finding was that there is an optimum area for maximum gas porosity within the investigated parameter range of laser power and scanning speed. At this point, it should be noted that the fitted model is only valid in the examined parameter space. It was shown, that gas porosity increases with increasing laser power and scanning speed up to a certain point and then decreases with further increasing of these parameters, i.e. there is an optimum region as shown in Fig. 8. The scanning speed largely determines the cooling rate since with increasing scanning speed the time for which a certain area is exposed to the laser beam decreases. For a slow scanning speed and small cooling rate, the gas has more time to escape the melt. If the scanning speed is high enough, keyhole formation and evaporation and thus pore formation can be avoided due to the lower volume energy density. Regarding the laser power, the influence on the volume energy density and resulting melt behavior is also underlined by the results. While too high laser powers lead to larger melt pools and lower melt viscosity due to high melt temperature [52], allowing the entrapped gas to escape, a laser power below a scanning speed dependent threshold is insufficient to cause evaporation and thus gas porosity. Within the investigated parameter range, the hatch spacing showed no significant influence on the relative density. This could be explained by the thermal behavior of the processed Ti-6Al-4V. Due to its relatively poor thermal conductivity, the formed melt pool is much larger than the laser spot size and also larger than the investigated hatch spacings. Consequently, there are no unmelted voids between adjacent scan tracks even at large hatch spacings and therefore the hatch spacing has less influence on pore formation. These results, however, are only valid within the investigated parameter window. In general, the achievable maximum amount of gas porosity is much smaller than it is for the LOF type of porosity. First, this can be attributed to the parameter interactions described before that lead to a limited area where high gas porosity can be realized. Another aspect to mention is that while gaseous pores typically have sizes of under 100 m [37], mostly of 5–20 m [53], LOF defects can reach sizes of 100–150 m [39] and can be of branched and irregular morphology. Due to their overall larger size, LOF defects can therefore yield higher part porosities that are also only limited by the mechanical stability of the part. Besides the porosity itself, also the pore characteristics, two-dimensional sphericityequivalent and mean pore area, were evaluated. The sphericity-equivalent only showed dependence on the laser power within the evaluated parameter range. A high gas porosity is associated with a high mean sphericityequivalent of the pores because only gas pores are present within the specimens manufactured with the respective high volume energy density parameter combinations. As stated by Kasperovich et al. the two dimensional circularity of pores, that is similar to the sphericity-equivalent applied in this work, generally shows the same trends as the threedimensional sphericity [40]. Accordingly, it is assumed that the sphericity-equivalent represents the behavior and dependencies of the true sphericity. The pore size increases with increasing laser power and decreasing hatch spacing and thus with increasing volume energy input. A higher energy input leads to increased evaporation and could therefore promote pore formation. In the investigated parameter range, neither a maximum nor a minimum pore size could be obtained according to the models prediction since the significant effects were of linear nature. Presumably, a widening of the parameter window would provide further information in this regard.

The feasibility of manufacturing parts with locally adjusted porosity, i.e. cylindrical specimens with dense skin and porous core could be demonstrated in this work. Based on these results, the targeted variation of porosity within a part can be transferred to more complex parts with also more than two levels of porosity in the future. A prerequisite is the local adjustability of the processing parameters that is not given by default to the necessary degree in typical preprocessing software. Although there is software that enables the implementation of a hullcore-strategy, the geometry of the core always follows the outer geometry. Geometries that are independent of one another cannot be implemented in an automated manner. The technique of dividing the actual part into sub-units to which the respective parameter sets are then assigned is time-consuming and error-prone. To realize such complex parts, further development of preprocessing software is therefore necessary.

The tensile tests showed significant differences between the different specimen modifications. Both, the fully dense and the specimens with the gas porous core showed mechanical properties comparable to those reported in the literature [6]. The specimens with gas porous core showed the highest strength as well as the highest elongation but without a change of the elastic modulus. The high strength and elongation despite the presence of a high amount of defects can be explained by two aspects. First, round pores are less detrimental for the mechanical properties compared to LOF defects [39, 40]. A second aspect to consider is the microstructure that can be influenced by variation of the processing parameters as it depends on the energy input, the resulting cooling rate as well as the melt pool size [6, 53]. It is therefore likely that due to the high energy input und lower cooling rates for the gas porous specimens, a higher amount of β -phase and less α '-martensite was generated. A small amount of β -phase in as-built specimens was also detected by Yang et al. [54]. However, this aspect needs further microstructural investigation in future works. Moreover, a subsequent heat-treatment could further adjust the microstructure and mechanical properties [55]. The results also imply that a porosity of nearly 6% in the core resulting in even less porosity based on the entire part is not enough to significantly influence the stiffness of a specimen. According to Eq. 2 the overall mean relative density of 96.11% in the cylindrical specimens should lead to a stiffness reduction of 7.6%. The fact that such a decrease of the elastic modulus could not be observed could be attributed to the realization of only a porous core with a dense shell that increases the stiffness instead of a completely porous part. Another possible explanation is the overall relatively low porosity compared to the amount that would be necessary to obtain the stiffness of human bone as given by Yadroitsava et al. [32]. To obtain large changes of stiffness, the relative density therefore has to be significantly lower. This can be achieved by the implementation of LOF defects. With this approach, a significant decrease of stiffness (32.2%) could be observed. This result even exceeds the prediction based on Eq. 2 for an absolute porosity of 15%, i.e. a decrease by 27.8%. However, this reduction of stiffness comes at the cost of strongly reduced ductility and strength. This can be attributed to the notch effect of the irregular shaped LOF defects that often have sharp edges that are likely to function as crack initiation sites due to stress concentration [39]. As a comparison, Lin et al. achieved a minimum elastic modulus of 35 GPa (mean elastic modulus for LOF defects in this study was 74.64 GPa, Table 7) using a core with LOF defects, but also at the cost of a strongly reduced UTS of 286 MPa (mean UTS for LOF defects in this study was 653.70 MPa, Table 7) [46]. In terms of lattice structures, Liang et al. obtained an elastic modulus of 1.93-5.24 GPa for compressive tests of trabecular-like Ti-6Al-4V scaffolds, wich is similar to that of human bone [56]. For diamondlattice radially graded structures Zhang et al. obtained an elastic modulus of 10.44 GPa [48].

In terms of spherical gas porosity, based on the results of this study, stiffness reduction may not be a suitable application. Nevertheless, the superior mechanical properties of the specimens with a gas porous core suggest that an implementation in load-bearing lightweight applications could be suitable. Here, weight reduction without stiffness reduction would be of great interest. However, it is known, that pores are detrimental for the fatigue strength [57, 58]. Regarding the limitations of this study it should be mentioned that all presented models are only valid within the examined parameter range, for the used machine set up and for the investigated geometries. To overcome this, the study should be expanded to a larger parameter window and machine set-ups with different specifications. For different geometries and different filling levels of the build platform, the thermal conditions, e.g. energy input or heat conduction, will be different. As a result, the optimum parameters for maximum gas porosity could vary. Therefore, the scalability of the results should be further investigated together with the influence of the parameters on the geometrical accuracy and fatigue properties.

5 Conclusion

In this work, an empirical process model for spherical porosity in additively manufactured Ti-6Al-4V was developed. Based on the model predictions a parameter combination for high spherical porosity was selected for application in functionally graded demonstration parts. These could be successfully built and served as a basis for the subsequently manufactured tensile test specimens. Tensile tests were conducted to investigate the influence of the graded porosity on tensile properties. The following conclusions can be given:

- There is a strong correlation of volume energy density, relative density and pore sphericity. A twodimensional sphericity-equivalent of < 0.89 was found to indicate LOF porosity, whereas a value > 0.91 stands for spherical gas porosity. Between these values, a transition area with both types of porosity could be found. An increasing volume energy density leads to an increasing 2D sphericity-equivalent. The minimum relative density achievable by LOF porosity is significantly higher than the one achievable by gas porosity.
- Empirical models were fitted for the relative density as well as the 2D sphericity-equivalent and the mean pore area. In all models, the laser power had the strongest influence on the respective response variable. The porosity can therefore most effectively be adjusted by tuning the applied laser power.
- For maximized spherical gas porosity, the parameter combination of P = 189 W, v = 375 mm/s and h = 150 m for a layer thickness of 30 m was determined, leading to a predicted relative density of 94.06%.
- The feasibility of manufacturing parts with locally adjusted porosity could be demonstrated for cylindrical specimens with a porous core and a dense skin.
- Tensile tests revealed that specimens with a gas porous core were superior to fully dense specimens regarding their strength and elongation at break. However, the elastic modulus did not change by implementing gas porosity. In contrast, the realization of a core with LOF defects led to a decrease of the elastic modulus from 110.0 GPa for fully dense specimens to 74.6 GPa (32.2%), but at the cost of significantly reduced strength and elongation.

This work showed that a significant stiffness reduction is possible by the local generation of LOF defects rather than by spherical gas porosity. Due to the superior mechanical properties of specimens with gas porous core, this is suggested for lightweight applications, where a high stiffness is important.

Author contribution Nicole Emminghaus: conception; analysis; interpretation; visualisation; writing—original draft preparation

Johanna Paul: conception; execute trials; analysis; interpretation; visualisation

Christian Hoff: writing—review and editing; supervision Jörg Hermsdorf: writing—review and editing; supervision Stefan Kaierle: writing—review and editing; supervision

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Data availability Data will be available upon request.

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Declarations

Conflict of interest The authors declare no competing interests.

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References

- Harrysson OLA, Cansizoglu O, Marcellin-Little DJ, Cormier DR, West HA (2008) Direct metal fabrication of titanium implants with tailored materials and mechanical properties using electron beam melting technology. Mater Sci Eng C 28(3):366–373. https://doi.org/10.1016/j.msec.2007.04.022
- Cronskär M, Bäckström M, Rännar LE (2013) Production of customized hip stem prostheses – a comparison between conventional machining and electron beam melting (EBM). Rapid Prototyp J 19(5):365–372. https://doi.org/10.1108/RPJ-07-2011-0067
- Jardini AL, Larosa MA, Zavaglia CAdC, Bernardes LF, Lambert CS, Kharmandayan P, Calderoni D, Filho RM (2014) Customised titanium implant fabricated in additive manufacturing for craniomaxillofacial surgery. Virtual Phys Prototyp 9(2):115–125. https://doi.org/10.1080/17452759.2014.900857
- Merkt S, Kleyer A, Hueber AJ (2014) The additive manufacture of patient-tailored finger implants. Laser Technik J 11(2):54–56. https://doi.org/10.1002/latj.201400029
- Santecchia E, Spigarelli S, Cabibbo M (2020) Material reuse in laser powder bed fusion: side effects of the laser—metal powder interaction. Metals 10(3):341. https://doi.org/10.3390/met10030 341
- Liu S, Shin YC (2019) Additive manufacturing of Ti6Al4V alloy: a review. Mater Des 164:107552. https://doi.org/10.1016/j.mat des.2018.107552
- Tian Z, Zhang C, Wang D, Liu W, Fang X, Wellmann D, Zhao Y, Tian Y (2020) A review on laser powder bed fusion of inconel 625 nickel-based alloy. Appl Sci 10(1):81. https://doi.org/10.3390/app10010081
- Yan Q, Song B, Shi Y (2020) Comparative study of performance comparison of AlSi10Mg alloy prepared by selective laser melting and casting. J Mater Sci Technol 41:199–208. https://doi.org/10.1016/j.jmst.2019.08.049
- Zhang Wn, Wang Lz, Feng Zx, Chen Ym (2020) Research progress on selective laser melting (SLM) of magnesium alloys: a review. Optik 207:163842. https://doi.org/10.1016/j.ijleo.2019. 163842
- Brandl E, Heckenberger U, Holzinger V, Buchbinder D (2012) Additive manufactured AlSi10Mg samples using Selective Laser Melting (SLM): microstructure, high cycle fatigue, and fracture behavior. Mater Des 34:159–169. https://doi.org/10.1016/j.mat des.2011.07.067

- Asgari H, Baxter C, Hosseinkhani K, Mohammadi M (2017) On microstructure and mechanical properties of additively manufactured AlSi10Mg_200c using recycled powder. Mater Sci Eng A 707:148–158. https://doi.org/10.1016/j.msea.2017.09.041
- Lutter-Günther M, Gebbe C, Kamps T, Seidel C, Reinhart G (2018) Powder recycling in laser beam melting: strategies, consumption modeling and influence on resource efficiency. Prod Eng 12(3):377–389. https://doi.org/10.1007/s11740-018-0790-7
- Cordova L, Campos M, Tinga T (2019) Revealing the effects of powder reuse for selective laser melting by powder characterization. JOM 71(3):1062–1072. https://doi.org/10.1007/s11837-018-3305-2
- Heiden MJ, Deibler LA, Rodelas JM, Koepke JR, Tung DJ, Saiz DJ, Jared BH (2019) Evolution of 316L stainless steel feedstock due to laser powder bed fusion process. Addit Manuf 25:84–103. https://doi.org/10.1016/j.addma.2018.10.019
- Agius D, Kourousis KI, Wallbrink C (2018) A review of the as-built SLM Ti-6Al-4V mechanical properties towards achieving fatigue resistant designs. Metals 8(1):75. https://doi.org/10.3390/met8010075
- 16. Shipley H, McDonnell D, Culleton M, Coull R, Lupoi R, O'Donnell G, Trimble D (2018) Optimisation of process parameters to address fundamental challenges during selective laser melting of Ti-6Al-4V: A review. Int J Mach Tools Manuf 128:1–20. https://doi.org/10.1016/j.ijmachtools.2018.01.003
- Donachie MJ (2000) Titanium: a technical guide, 2nd edn. ASM International, Almere. google-Books-ID: HgzukknbNGAC
- Leyens C, Peters M (2006) Titanium and titanium alloys: fundamentals and applications. Wiley Online Library, Hoboken
- Cui C, Hu B, Zhao L, Liu S (2011) Titanium alloy production technology, market prospects and industry development. Mater Des 32(3):1684–1691. https://doi.org/10.1016/j.matdes.2010.09.011
- Krishna BV, Bose S, Bandyopadhyay A (2007) Low stiffness porous Ti structures for load-bearing implants. Acta Biomater 3(6):997–1006. https://doi.org/10.1016/j.actbio.2007.03.008
- Bhattarai SR, Khalil KAR, Dewidar M, Hwang PH, Yi HK, Kim HY (2008) Novel production method and in-vitro cell compatibility of porous Ti-6Al-4V alloy disk for hard tissue engineering. J Biomed Mater Res A 86A(2):289–299. https://doi.org/10.1002/jbm.a.31490
- 22. Wolff J (1893) Das gesetz der transformation der knochen. DMW 19(47):1222–1224. https://doi.org/10.1055/s-0028-1144106
- Oh IH, Nomura N, Masahashi N, Hanada S (2003) Mechanical properties of porous titanium compacts prepared by powder sintering. Scr Mater 49(12):1197–1202. https://doi.org/10.1016/j.script amat.2003.08.018
- Palka K, Pokrowiecki R (2018) Porous titanium implants: a review. Adv Eng Mater 20(5):1700648. https://doi.org/10.1002/ adem.201700648
- Yuan L, Ding S, Wen C (2019) Additive manufacturing technology for porous metal implant applications and triple minimal surface structures: a review. Bioact Mater 4:56–70. https://doi.org/10.1016/j.bioactmat.2018.12.003
- 26. Ran Q, Yang W, Hu Y, Shen X, Yu Y, Xiang Y, Cai K (2018) Osteogenesis of 3D printed porous Ti6Al4V implants with different pore sizes. J Mech Behav Biomed Mater 84:1–11. https://doi.org/10.1016/j.jmbbm.2018.04.010
- Gibson LJ, Ashby MF (1997) Cellular solids: structure and properties. Cambridge Solid State Science Series, 2nd edn. Cambridge University Press, Cambridge. https://doi.org/10.1017/ CBO9781139878326
- Anthoine A (2010) Second-order homogenisation of functionally graded materials. Int J Solids Struct 47(11):1477–1489. https://doi.org/10.1016/j.ijsolstr.2010.02.004
- 29. Mahmoud D, Elbestawi MA (2017) Lattice structures and functionally graded materials applications in additive manufacturing

of orthopedic implants: a review. J Manuf Mater Process 1(2):13. https://doi.org/10.3390/jmmp1020013

- 30. Zhang C, Chen F, Huang Z, Jia M, Chen G, Ye Y, Lin Y, Liu W, Chen B, Shen Q, Zhang L, Lavernia EJ (2019) Additive manufacturing of functionally graded materials: A review. Mater Sci Eng A 764:138209. https://doi.org/10.1016/j.msea.2019.138209
- Bertol LS, Júnior WK, FPd Silva, Aumund-Kopp C (2010) Medical design: Direct metal laser sintering of Ti–6Al–4V. Mater Des 31(8):3982–3988. https://doi.org/10.1016/j.matdes.2010.02.050
- 32. Yadroitsava I, du Plessis A, Yadroitsev I (2019) Chapter 12 Bone regeneration on implants of titanium alloys produced by laser powder bed fusion: A review. Elsevier, Amsterdam, pp 197–233. https://doi.org/10.1016/B978-0-12-815820-3.00016-2
- Dhiman S, Sidhu SS, Bains PS, Bahraminasab M (2019) Mechanobiological assessment of Ti-6Al-4V fabricated via selective laser melting technique: a review. Rapid Prototyp J 25(7):1266–1284. https://doi.org/10.1108/RPJ-03-2019-0057
- Parthasarathy J, Starly B, Raman S (2011) A design for the additive manufacture of functionally graded porous structures with tailored mechanical properties for biomedical applications. J Manuf Process 13(2):160–170. https://doi.org/10.1016/j.jmapro.2011.01.004
- Wally ZJ, Van Grunsven W, Claeyssens F, Goodall R, Reilly GC (2015) Porous titanium for dental implant applications. Metals 5(4):1902–1920. https://doi.org/10.3390/met5041902
- 36. Yang L, Yan C, Fan H, Li Z, Cai C, Chen P, Shi Y, Yang S (2019) Investigation on the orientation dependence of elastic response in Gyroid cellular structures. J Mech Behav Biomed Mater 90:73–85. https://doi.org/10.1016/j.jmbbm.2018.09.042
- Zhang B, Li Y, Bai Q (2017) Defect formation mechanisms in selective laser melting: a review. Chin J Mech Eng 30(3):515–527. https://doi.org/10.1007/s10033-017-0121-5
- Kyogoku H, Ikeshoji TT (2020) A review of metal additive manufacturing technologies: mechanism of defects formation and simulation of melting and solidification phenomena in laser powder bed fusion process. Mech Eng Rev 7(1):19–00182–19– 00182. https://doi.org/10.1299/mer.19-00182
- Vilaro T, Colin C, Bartout JD (2011) As-fabricated and heattreated microstructures of the Ti-6Al-4V alloy processed by selective laser melting. Metall Mater Trans A 42(10):3190–3199. https://doi.org/10.1007/s11661-011-0731-y
- 40. Kasperovich G, Haubrich J, Gussone J, Requena G (2016) Correlation between porosity and processing parameters in TiAl6V4 produced by selective laser melting. Mater Des 105:160– 170. https://doi.org/10.1016/j.matdes.2016.05.070
- Yun HJ, Abolhasani D, Hwang TW, Lee T, Kim JH, Moon YH (2020) Fabrication of porous titanium parts by powder bed fusion of Ti–TiH2 blended powder. J Mater Res Technol 9(3):3026– 3037. https://doi.org/10.1016/j.jmrt.2020.01.033
- 42. Li R, Liu J, Shi Y, Du M, Xie Z (2010) 316L stainless steel with gradient porosity fabricated by selective laser melting. J Mater Eng Perform 19(5):666–671. https://doi.org/10.1007/s11665-009-9535-2
- Jeon TJ, Hwang TW, Yun HJ, VanTyne CJ, Moon YH (2018) Control of Porosity in Parts Produced by a Direct Laser Melting Process. Appl Sci 8(12):2573. https://doi.org/10.3390/app8122573
- 44. Jafari D, Wits WW, Vaneker THJ, Demir AG, Previtali B, Geurts BJ, Gibson I (2020) Pulsed mode selective laser melting of porous structures: structural and thermophysical characterization. Addit Manuf 35:101263. https://doi.org/10.1016/j.addma.2020.101263
- Elsayed M, Ghazy M, Youssef Y, Essa K (2018) Optimization of SLM process parameters for Ti6Al4V medical implants. Rapid Prototyp J 25(3):433–447. https://doi.org/10.1108/RPJ-05-2018-0112
- Lin WS, Starr TL, Harris BT, Zandinejad A, Morton D (2013) Additive manufacturing technology (direct metal laser

sintering) as a novel approach to fabricate functionally graded titanium implants: preliminary investigation of fabrication parameters. Int J Oral Maxillofac Implants 28(6):1490–1495. https://doi.org/10.11607/jomi.3164

- Fousová M, Vojtech D, Kubásek J, Jablonská E, Fojt J (2017) Promising characteristics of gradient porosity Ti-6Al-4V alloy prepared by SLM process. J Mech Behav Biomed Mater 69:368– 376. https://doi.org/10.1016/j.jmbbm.2017.01.043
- 48. Zhang XY, Fang G, Leeflang S, Zadpoor AA, Zhou J (2019) Topological design, permeability and mechanical behavior of additively manufactured functionally graded porous metallic biomaterials. Acta Biomater 84:437–452. https://doi.org/10.1016/j.actbio.2018.12.013
- 49. de Formanoir C, Paggi U, Colebrants T, Thijs L, Li G, Vanmeensel K, Van Hooreweder B (2020) Increasing the productivity of laser powder bed fusion: influence of the hullbulk strategy on part quality, microstructure and mechanical performance of Ti-6Al-4V. Addit Manuf 33:101129. https://doi.org/10.1016/j.addma.2020.101129
- 50. Grüne JG, Knoop D, Domagala T, Av Hehl (2021) Laser beam melting of aluminum alloys with hull-core build strategy by using an initial meso-scale simulation. Mater Werkst 52(1):8–18. https://doi.org/10.1002/mawe.201900215
- Wadell H (1935) Volume, Shape, and Roundness of Quartz Particles. J Geol 43:250–280. https://doi.org/10.1086/624298
- 52. Khorasani M, Ghasemi A, Awan US, Hadavi E, Leary M, Brandt M, Littlefair G, O'Neil W, Gibson I (2020) A study on surface morphology and tension in laser powder bed fusion of Ti-6Al-4V. Int J Adv Manuf Technol 111(9):2891–2909. https://doi.org/10.1007/s00170-020-06221-w

- Thijs L, Verhaeghe F, Craeghs T, Humbeeck JV, Kruth JP (2010) A study of the microstructural evolution during selective laser melting of Ti–6Al–4V. Acta Mater 58(9):3303–3312. https://doi.org/10.1016/j.actamat.2010.02.004
- 54. Yang J, Yu H, Yin J, Gao M, Wang Z, Zeng X (2016) Formation and control of martensite in Ti-6Al-4V alloy produced by selective laser melting. Mater Des 108:308–318. https://doi.org/10.1016/j.matdes.2016.06.117
- 55. Vrancken B, Thijs L, Kruth JP, Van Humbeeck J (2012) Heat treatment of Ti6Al4V produced by Selective Laser Melting: microstructure and mechanical properties. J Alloys Compd 541:177–185. https://doi.org/10.1016/j.jallcom.2012.07.022
- 56. Liang H, Yang Y, Xie D, Li L, Mao N, Wang C, Tian Z, Jiang Q, Shen L (2019) Trabecular-like Ti-6Al-4V scaffolds for orthopedic: fabrication by selective laser melting and in vitro biocompatibility. J Mater Sci Technol 35(7):1284–1297. https://doi.org/10.1016/j.jmst.2019.01.012
- Du L, Qian G, Zheng L, Hong Y (2021) Influence of processing parameters of selective laser melting on high-cycle and very-highcycle fatigue behaviour of Ti-6Al-4V. Fatigue Fract Eng Mater Struct 44(1):240–256
- Mahmoud D, Al-Rubaie KS, Elbestawi MA (2021) The influence of selective laser melting defects on the fatigue properties of Ti6Al4V porosity graded gyroids for bone implants. Int J Mech Sci 193:106180. https://doi.org/10.1016/j.ijmecsci.2020.106180

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