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Direct prospective comparison of 18F- FDG PET and arterial spin labelling MR using simultaneous PET/MR in patients referred for differential diagnosis of dementia --Manuscript Draft--

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Full Title:	Direct prospective comparison of 18F- FDG PET and arterial spin labelling MR using simultaneous PET/MR in patients referred for differential diagnosis of dementia
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Abstract:	<p>Purpose: 18F-FDG PET is routinely used as imaging marker in the early and differential diagnosis of dementing disorders and has incremental value over the clinical neurological and neuropsychological evaluation. Perfusion imaging by means of arterial spin labelling (ASL) is an alternative modality to indirectly measure neuronal functioning and could be used as complement measurement in a single MR session in the workup of dementia. Using simultaneous PET-MR, we performed a direct head-to-head comparison between enhanced multiplane tagging ASL (eASL) and 18F-FDG PET in a true clinical context of subjects referred for suspicion of neurodegenerative dementia.</p> <p>Methods: Twenty-seven patients underwent a 20-minute 18F-FDG PET/MR and simultaneously acquired eASL on a GE Signa PET/MR. Data were compared to 30 screened age- and gender-matched healthy controls. Both integral eASL and 18F-FDG datasets were analysed visually by two readers unaware of the final clinical diagnosis, either in normal/abnormal classes, or full differential diagnosis (normal, Alzheimer type dementia [AD], dementia with Lewy Bodies [LBD], frontotemporal dementia [FTD] or other). Reader confidence was assessed in a qualitative four-point scale. Data were also analysed semiquantitatively by VOI and voxel-based analyses.</p> <p>Results: The ground truth diagnosis for the patient group resulted in 14 patients with a neurodegenerative cognitive disorder (AD, FTD, LBD) and 13 patients with no arguments for an underlying neurodegenerative cause. Visual analysis resulted in</p>

	<p>equal specificity (0.70) for differentiating normal and abnormal cases between the two modalities, but in a higher sensitivity (0.93) and confidence rating for 18F-FDG PET compared to eASL (0.64). The same was true for assigning a specific differential diagnosis (18F-FDG PET: 0.61; eASL: 0.39). Semiquantitative analyses revealed prototypical patterns for AD and FTD, with for both a higher effect size on 18F-FDG PET.</p> <p>Conclusion: In a direct head-to-head comparison on a simultaneous GE Signa PET/MR, 18F-FDG PET performs better in term of sensitivity, reader confidence, effect size and more intense abnormalities than ASL. However, using pure semiquantitative analysis, similar diagnostic accuracy between the two modalities was obtained. Therefore, ASL may still serve as complement to neuroreceptor or protein deposition PET studies when a single simultaneous investigation is warranted.</p>
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TITLE PAGE

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Direct prospective comparison of ¹⁸F-FDG PET and arterial spin labelling MR using simultaneous PET/MR in patients referred for differential diagnosis of dementia

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ABSTRACT

Purpose: ^{18}F -FDG PET is routinely used as imaging marker in the early and differential diagnosis of dementing disorders and has incremental value over the clinical neurological and neuropsychological evaluation. Perfusion imaging by means of arterial spin labelling (ASL) is an alternative modality to indirectly measure neuronal functioning and could be used as complement measurement in a single MR session in the workup of dementia. Using simultaneous PET-MR, we performed a direct head-to-head comparison between enhanced multiplane tagging ASL (eASL) and ^{18}F -FDG PET in a true clinical context of subjects referred for suspicion of neurodegenerative dementia.

Methods: Twenty-seven patients underwent a 20-minute ^{18}F -FDG PET/MR and simultaneously acquired eASL on a GE Signa PET/MR. Data were compared to 30 screened age- and gender-matched healthy controls. Both integral eASL and ^{18}F -FDG datasets were analysed visually by two readers unaware of the final clinical diagnosis, either in normal/abnormal classes, or full differential diagnosis (normal, Alzheimer type dementia [AD], dementia with Lewy Bodies [LBD], frontotemporal dementia [FTD] or other). Reader confidence was assessed in a qualitative four-point scale. Data were also analysed semiquantitatively by VOI and voxel-based analyses.

Results: The ground truth diagnosis for the patient group resulted in 14 patients with a neurodegenerative cognitive disorder (AD, FTD, LBD) and 13 patients with no arguments for an underlying neurodegenerative cause. Visual analysis resulted in equal specificity (0.70) for differentiating normal and abnormal cases between the two modalities, but in a higher sensitivity (0.93) and confidence rating for ^{18}F -FDG PET compared to eASL (0.64). The same was true for assigning a specific differential diagnosis (^{18}F -FDG PET: 0.61; eASL: 0.39). Semiquantitative analyses revealed prototypical patterns for AD and FTD, with for both a higher effect size on ^{18}F -FDG PET.

Conclusion: In a direct head-to-head comparison on a simultaneous GE Signa PET/MR, ^{18}F -FDG PET performs better in term of sensitivity, reader confidence, effect size and more intense abnormalities than ASL. However, using pure semiquantitative analysis, similar diagnostic accuracy between the two modalities was obtained. Therefore, ASL may still serve as complement to neuroreceptor or protein deposition PET studies when a single simultaneous investigation is warranted.

Key words: arterial spin labelling ASL MRI; ¹⁸F-FDG PET; dementia; PET/MR; brain imaging.

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INTRODUCTION

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3 The prevalence of dementia is rapidly increasing. Based on the World Alzheimer's Report, almost 50
4 million people worldwide currently have dementia, and with aging population the current prognosis is
5 that more than 130 million individuals will be afflicted worldwide by 2050 [1,2]. Several underlying
6 disorders can cause dementia, but the four most common are Alzheimer's disease (AD), Lewy body
7 dementia (LBD), vascular dementia (VD) and frontotemporal dementia (FTD). Extracellular amyloid
8 plaques, along with neurofibrillary tangles, are a neuropathologic hallmark of AD [1]. The guidelines
9 from the National Institute on Aging-Alzheimer's Association (NIA-AA) suggest a variety of ancillary
10 biomarker tools to increase the clinical confidence in diagnosis of AD, including cerebrospinal fluid
11 biomarkers, MR volumetry, fluorodeoxyglucose (^{18}F -FDG), amyloid and tau PET [3]. Amyloid PET
12 already has a major impact in management of patients suspected for AD [4] and is offered as standard
13 of care in many institutions. Current research efforts address the role of tau PET in the workup of
14 dementia [5–7]. However, ^{18}F -FDG PET still remains the most frequently used, widely available and
15 well-established functional imaging tool to assess neuronal functioning and to differentiate dementia
16 patients with high diagnostic accuracy even early in the course of the disease [3,8,9], with an average
17 sensitivity of 0.91 and specificity of 0.85 for diagnosing AD. ^{18}F -FDG PET also is an established
18 biomarker for distinguishing FTD and LBD from other dementias [10,11].

19
20 Arterial spin labelling (ASL) magnetic resonance imaging has been proposed as an alternative non-
21 invasive, radiation free and practical alternative functional marker, based on the neurovascular coupling,
22 and thus also a proxy marker for neuronal function [12]. Several authors have suggested that ASL could
23 be an emerging biomarker for diagnosing AD and other neurodegenerative conditions [13–15]. ASL can
24 be seen comparable to SPECT perfusion imaging [16] with respect to spatial resolution and has been
25 shown to produce similar regional patterns of hypoperfusion in patients with various types of dementia
26 [13]. Moreover, ASL uses magnetically labelled arterial blood water as an endogenous tracer and can
27 be used to quantify cerebral blood flow (CBF) in an absolute way (ml/100 g brain/min).

28
29 Several imaging studies have reported good correlations between hypoperfusion as measured with ASL
30 and hypometabolism using ^{18}F -FDG PET, both in patients with AD or FTD [17–23], suggesting that

ASL could be an alternative to ^{18}F -FDG PET in the diagnosis of dementia syndromes. However, the diagnostic value of ASL in clinical dementia diagnosis on an individual basis has yet to be determined. The reported sensitivity and specificity of ASL (range sensitivity: 0.53-0.80; range specificity: 0.62-0.84) compared to ^{18}F -FDG PET largely varies among studies, probably due to differences in ASL techniques, type of comparative analysis and due to the heterogeneity of small cohorts [17–23].

So far, no direct comparison between ASL and ^{18}F -FDG PET has been reported measured by means of simultaneous PET/MR. By using simultaneous imaging, potential day to day variations, medication effects or effect of evolutive comorbidities can be minimalized, enabling an optimal direct comparison.

In this work, we have therefore compared the diagnostic accuracy of ^{18}F -FDG PET and pulsed enhanced multiplane tagging eASL using a simultaneous PET/MR system in the most challenging but clinically relevant setting of patients with suspected dementia, in comparison to carefully screened healthy controls. The aim of the study was to establish visual accuracy for blinded readers, as well as to assess semiquantitative volume-of-interest (VOI) and voxel-based analysis to classify patients as either abnormal (‘neurodegenerative pattern’) or not, as well as to perform a more elaborate differential diagnosis.

MATERIALS AND METHODS

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2 The study was approved by the Ethics Committee Research UZ / KU Leuven (Leuven) and written
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4 informed consent was obtained from all participants.
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Study population

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10 Twenty-seven consecutive patients (age 64.3 ± 11.2 years, 14 M/13 F) were prospectively included
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12 between December 2016 and June 2017. All had been referred from the local tertiary memory clinic for
13
14 a brain ^{18}F -FDG PET scan because of recent cognitive decline and a question of potential
15
16 neurodegenerative dementia. All patients underwent routine clinical, neurological and extensive
17
18 neuropsychological examination in their workup, and in most cases also structural MRI (T1 and FLAIR)
19
20 was performed. CSF $\text{A}\beta$ and tau data were available in 5 patients, no amyloid PET scan results were
21
22 available at the time of ^{18}F -FDG PET/MR. The working diagnosis at the time of ^{18}F -FDG PET scan
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24 referral is shown in Table 1. As ground truth diagnosis, the last available diagnosis made by the memory
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26 clinic physician was taken, based on all routinely available information, and established after follow-up
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28 up to 1.5 years (Table 1).
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33 Thirty healthy controls (CON; age 63.9 ± 10.6 years; 14 M/16 F) were recruited through advertisements
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35 in local newspapers and on the departmental websites. The main exclusion criteria for this group
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37 included: history of neurological or psychiatric disorders, first degree relative with neurodegenerative
38
39 dementia, important systemic pathologies (e.g. diabetes, cancer, liver or kidney disease) or use of any
40
41 central acting medication. All controls underwent a neurological examination by a board-certified
42
43 physician, had a mini-mental state (MMSE) score ≥ 28 , Beck Depression Inventory score ≤ 9 , and a
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45 normal T1 and T2 MRI for their age. The control subjects were part of a large ^{18}F -FDG PET/MR normal
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47 aging database, of which a randomised age- and gender-matched subset was randomly selected for this
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49 study.
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Image acquisition

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57 All subjects fasted at least 4 hours prior to ^{18}F -FDG injection. For patients, intravenous tracer injection
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59 was performed under standardized circumstances (supine, low ambient light, low noise, eyes open).
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1 Patients first underwent clinical routine ^{18}F -FDG brain PET/CT, 30-min post-injection of 150.5 ± 11.5
2 MBq ^{18}F -FDG (range: 110-172 MBq) and were subsequently immediately transferred to the PET/MR
3 unit and received a second 20 minute list-mode PET acquisition on a simultaneous 3 Tesla Signa
4 PET/MR system (GE Healthcare, Chicago, IL, USA). Control subjects underwent a dynamic 60-min
5 PET/MR scan started directly after intravenous injection of 152.2 ± 11.1 MBq ^{18}F -FDG (range: 131-
6 185 MBq). The first 15 minutes of the simultaneous scan, no MR sequences were applied in order not
7 to invoke primary auditory cortex activation and subjects were asked to keep eyes open. From the list-
8 mode data, the last 20-min were reconstructed (40-60 min p.i.) as static scan and used as comparator for
9 this study.

10 Vendor-based MR-based attenuation correction (MRAC) corrected PET images were reconstructed
11 using ordered subset expectation maximization (OSEM) with 6 iterations and 28 subsets, and post-
12 smoothed with a 3 mm isotropic Gaussian filter. MR image acquisition was performed during the PET
13 acquisition using an 8-channel high resolution head array coil (GE Healthcare). In addition to an
14 anatomical volumetric images (T1-weighted 3D BRAVO, TR/TE = 8.5/3.2 ms, 1x1x1 mm voxel size;
15 fluid-attenuated inversion recovery (FLAIR) 3D CUBE, TR/TE = 8500/130 ms, 1x1x1.4 mm voxel
16 size), also a 3D pulsed enhanced multiplane tagged continuous ASL (eASL) image set was acquired
17 (TR/TE = 5917 ms/ 12.4 ms, bandwidth 976.6 Hz/pixel, flip angle 111° , time acquisition = 9:09 min)
18 with 26 contiguous slices of 5.5 mm slice thickness, with voxel size 1.72 x 1.72 x 5.5 mm.

19 ASL images were corrected for arterial transit time (ATT), resulting in transit corrected flow (TCF)
20 images, using vendor-specific software. Because of the noise content, an additional isotropic Gaussian
21 smoothing of 6 mm was applied on the ATT ASL images before analysis.

22 **Visual qualitative analysis of ^{18}F -FDG PET and ASL images**

23 A qualitative visual analysis was performed on both the ^{18}F -FDG-PET and ASL processed images. Prior
24 to analysis, reconstructed images were fully anonymized and randomly number-coded per data type
25 (differently for ASL and ^{18}F -FDG) and processed using the CortexID Suite (GE Healthcare, Chicago,
26 IL, USA). This software allows automatic spatial normalization after which data can be represented in
27

1
2 an orthogonal and surface rendered way. Two experienced nuclear medicine physicians (K.V.L. and
3 K.G.) visually analyzed and rated all images in a blinded fashion, i.e. unaware of clinical information
4 or the working diagnosis at time of ^{18}F -FDG PET. Fig. 1 shows an example of orthogonal slices and
5 surface rendered ^{18}F -FDG PET and ASL TCF images for a typical healthy control and AD patient.
6

7 Both readers visually analyzed the images with the following instructions: firstly, to classify the scan as
8 either ‘normal’ or ‘abnormal’; secondly, if rated abnormal, to classify according to a differential
9 diagnosis from the observed metabolic or flow pattern, in either AD, FTD, LBD or ‘other’. The
10 observers were also asked to score activity or flow abnormalities in relevant regional areas using a 4-
11 point scale: *normal* (4), *mildly decreased* (3), *moderately decreased* (2) or *severely decreased* (1). This
12 rating was applied to the following brain regions (left and right): frontal, temporal, parietal and occipital
13 cortex, precuneus, striatum, thalamus and cerebellum. Finally, observers gave a confidence rating for
14 their normal/abnormal and differential diagnosis classification: *very uncertain* (1), *rather uncertain* (2),
15 *rather certain* (3), *certain* (4).
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28 The observer classifications were analyzed by direct comparison to the ground truth, hereby calculating
29 the diagnostic accuracy (i.e. sensitivity and specificity) for both modalities and for both observers.
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31 Within each modality, measures of sensitivity and specificity calculated for each individual observer
32 were subsequently averaged to compare the abnormality intensity score obtained with both modalities.
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34 The interobserver agreement was reported with the Fleiss kappa coefficient κ , where a κ value between
35 0.21 and 0.40 represents fair agreement, and 0.61 and 0.80 represents substantial agreement.
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37 Abnormality intensity score and confidence scores were plotted on the 4-point scale for both ASL and
38 ^{18}F -FDG for all observed regions/scans, and standardized errors were calculated to determine significant
39 rated intensity differences between both techniques.
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51 **Semiquantitative VOI analysis**

52 A volume of interest VOI-based analysis was performed using PMOD (version 3.8, PMOD Inc. Zürich,
53 Switzerland). 3D T1 MRI, ^{18}F -FDG PET and eASL images were rigidly matched to account for potential
54 within-scan movement. After T1-based spatial normalization using the PNEURO tool in PMOD (default
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1 parameters for warping), 83 predefined VOIs from the Hammers atlas [24] were used. Then, larger
2 unilateral composite regions were defined to reduce the data (frontal, temporal, parietal, occipital cortex,
3 posterior cingulate, striatum, thalamus and cerebellum). Z-score VOI data were derived by comparing
4 patient VOI data to the mean and SD from the control data ($Z\text{-score} = (\text{VOI}(\text{patient}) - \text{VOI}$
5 $\text{mean}(\text{controls}))/\text{VOI SD}(\text{controls})$). Patient scans were classified as normal/abnormal when any
6 composite VOI Z-score was more than 1.5 SD lower than controls. A comparison between eASL and
7 ^{18}F -FDG Z-score data for the patients was performed similar as with the visual grading, i.e. by plotting
8 these for all patients (according to final diagnosis) to determine if data were correlated and investigate
9 the magnitudes of Z-scores for eASL and ^{18}F -FDG as indicator of sensitivity to detect hypoperfusion or
10 hypometabolism relative to the variability in controls.
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25 **Voxel-based analysis**

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27 A voxel-based group analysis was conducted using Statistical Parametric Mapping (SPM12, Welcome
28 Trust Center for Neuroimaging, London, UK), implemented in MatLab (R2017b, The MathWorks Inc,
29 Natick, MA, USA) to determine the group differences in glucose metabolism and blood flow, and
30 investigate the differences in SPM statistical sensitivity for both techniques.
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36 For this subanalysis, the coregistered image sets were spatially normalized to Montreal Neurological
37 Institute (MNI) space using the SPM TPM template and non-rigid registration with default parameters
38 (16 iterations). Isotropic Gaussian smoothing with full width at half-maximum (FWHM) of 8 mm was
39 performed in a voxel matrix of 2x2x2 mm. Images were analyzed using proportional scaling to the
40 average grey matter activity. Group analysis was performed at cluster level of $p < 0.05$ (FWE-corrected),
41 with a peak height threshold of p_{height} of 0.01 (or more stringent), extent threshold (k_{ext}) of 20 voxels.
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RESULTS

Patient characteristics

Patients and controls were age- and gender matched ($p = 0.48$, $\chi^2 p = 0.9$, respectively). The mean MMSE score in the patient group was $24.1 (\pm 5.5, \text{range: } 11\text{-}30)$; available in 23/27 patients), for the CON group this was 29.3 ± 0.8 (range: 28-30). The working diagnosis for the patient group is given in Table 1 and consisted of: 8 AD, 2 FTD, 1 LBD, 1 cerebellar variant of multiple system atrophy (MSA-c), 1 motor neuron disorder (MND), 1 traumatic brain injury (TBI) and 13 patients with no clear pre-PET arguments for a neurodegenerative cause for the appeared cognitive complaints (NND = no arguments for neurodegenerative disorder). The final diagnosis after a period of follow-up (follow-up range: 3 - 18 mo) was different from the working diagnosis at the clinical ^{18}F -FDG PET request in 6 subjects (Table 1): NND > AD, MND > NND, AD > NND (post-cerebrovascular accident dementia), AD > parkinson-related dementia, FTD > FTD+MND.

Visual analysis of ^{18}F -FDG PET and ASL images

Diagnostic accuracy of the visual read of ^{18}F -FDG PET and ASL for the two readers is given in Table 2. For differentiating a pathological (neurodegenerative) from a normal (no arguments for neurodegenerative pattern, NND) scan, the mean sensitivity of ^{18}F -FDG PET was 0.93 and equal for both readers, while a substantial difference between readers was noted in specificity (0.86 vs 0.53, mean 0.70). For ASL, the mean sensitivity dropped significantly to 0.64 ($p = 0.03$) and remained relatively consistent between readers (0.71 vs 0.57); also specificity was consistent (0.74 vs 0.67; mean 0.71).

Furthermore, for the second and much harder task to assign a specific differential diagnosis, of the 14 pathological ^{18}F -FDG PET images, 9 were diagnosed correctly by the first reader (0.64), and 8 (0.57) by the second reader (average correct classification 0.61). For the ASL images, 7 (0.50) and 4 (0.29) out of 14 images were classified correctly by the first and second reader, respectively (average correct classification 0.39; $p > 0.05$). The corresponding Cohen's Kappa coefficients for interobserver agreement between modalities were 0.34 (SE 0.15, 95% CI 0.04 to 0.65) and 0.20 (SE 0.15, 95% CI -0.11 to 0.50) for ^{18}F -FDG PET and ASL, respectively, suggesting that the agreement between the observers was better for ^{18}F -FDG PET than for ASL.

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Abnormality intensity rating : When the readers were asked to observe and score the ^{18}F -FDG activity/flow abnormality in the relevant brain regions, the average visual intensity rating was comparable between ^{18}F -FDG PET and ASL in the frontal, parietal, temporal cortex, precuneus and cerebellum for each patient group ($p > 0.05$) (Fig. 2, Supplementary Fig. 1). Contrarily, average abnormality scores were significantly lower in the occipital lobe, thalamus and striatum for ASL versus ^{18}F -FDG PET data (“moderately-mildly decreased” with ASL vs “normal” with ^{18}F -FDG PET) (Fig. 2, Supplementary Fig. 1). These findings were also confirmed by the standardized residuals. For the patient groups, the standardized residuals were more than 2, indicating ^{18}F -FDG-based intensity rating was significantly higher than ASL-based intensity rating in 5 patients, and vice versa in one other patients.

Confidence rating: Considering the regional confidence rating for the left and right observed brain regions, the degree of diagnostic confidence for ^{18}F -FDG PET and ASL was comparable in the frontal cortex, parietal cortex, precuneus and cerebellum (Supplementary Fig. 2.a). However, the readers were less confident in scoring ASL-based blood flow compared to glucose metabolism in the temporal cortex, occipital cortex, striatum and thalamus in any group of patients with suspected diagnosis of dementia (NND, AD, FTD, LBD and OTHER), as well as for the control group (Supplementary Fig. 2.b).

Regional pattern scoring: semiquantitative VOI analysis

In a second step, the subjects were classified as normal/abnormal scans based on the composite VOI Z-score assessments. The sensitivity and specificity of ^{18}F -FDG PET-based distinction was 0.79 and 0.63, respectively. ASL yielded a lower rate of correct differential diagnosis in normal vs. abnormal cases, obtaining a sensitivity of 0.57 ($p < 0.001$). On the other hand, the rate of true negatives was significantly higher with ASL (specificity = 0.81; $p < 0.001$). In Fig. 3, the Z-score data are plotted for both ASL and ^{18}F -FDG for all observed regions/scans. Overall, the standardized residuals revealed no significant Z-score-related differences between both techniques (frontal cortex: -0.53 ± 0.83 ; temporal cortex: -0.53 ± 0.45 ; parietal cortex: -0.50 ± 1.18 ; occipital cortex: 0.64 ± 0.82 ; posterior cingulate: -0.61 ± 1.03 ; striatum: -0.69 ± 0.85 ; thalamus : -0.66 ± 0.86 ; cerebellum: 0.70 ± 0.99). ^{18}F -FDG-based VOI Z-scores were significantly higher than ASL-based VOI Z-scores in 5% of the regional values.

Voxel-based analysis

Voxel-wise statistical analysis results of AD and FTD patients compared to CON are shown in Fig. 4.

Group differences in glucose metabolism and blood flow between the AD diagnostic subgroup compared to CON, showed that ^{18}F -FDG PET and ASL result in similar quantitative hypometabolism/hypoperfusion localized mainly in the mid-cingulate, posterior cingulate-precuneus cortices and parietotemporal areas, typical of AD (Fig. 4.a). Although an agreement between the hypoperfusion and hypometabolism maps was confirmed by a 2nd level factorial analysis (positive effect of condition, with a peak height threshold of p_{height} of 0.001 and k_{ext} of 20 voxels), SPM statistical cluster intensity and extent was greater with ^{18}F -FDG PET ($p_{\text{FWE}} < 0.05$ at cluster level), compared to ASL data. When considering the FTD diagnostic subgroup vs CON, the extent of the anteromedial temporal and inferior frontal cortical abnormality was larger on ^{18}F -FDG PET than on ASL (Fig. 4.b).

A summary of the localization of the clusters, p and t scores for the AD vs CON and FTD vs CON group comparison is shown in Supplementary Table 1 and Supplementary Table 2, respectively.

DISCUSSION

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2 In the past few years, several single-centre studies have reported good correlations between observed
3
4 hypoperfusion in ASL and hypometabolism in ^{18}F -FDG PET in patients with AD or FTD, suggesting
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6 ASL as a potential alternative to ^{18}F -FDG PET in the diagnosis of neurodegenerative dementia [17–23].
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8 However, the diagnostic value of ASL in clinical conditions has yet to be accurately confirmed, based
9
10 on the inconclusive evidence from these group comparisons. Indeed, the reported sensitivity and
11
12 specificity of ASL compared to ^{18}F -FDG PET studies largely varies among the studies, which is likely
13
14 due to differences in ASL techniques, type of comparative analysis, varying PET and MR conditions or
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16 heterogeneity of small cohorts of patients.
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19 In this direct head-to-head comparison between multiplane tagged, pulsed enhanced multiplane tagging
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21 ASL (eASL) and ^{18}F -FDG PET, set in a true clinical context of referrals for cognitive decline in a tertiary
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23 setting, we aimed at a comprehensive evaluation of the diagnostic performance of the two techniques
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25 by using a simultaneous PET/MR system and a combination of visual and semiquantitative analysis, as
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27 is done in standard clinical practice. The main finding of this study was that eASL could be considered
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29 as a potential alternative to ^{18}F -FDG PET to assess neurodegeneration in patients with cognitive
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31 impairment when the latter is unavailable, or in case dual-parameter evaluation (e.g. amyloid or tau PET
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33 + eASL-MR) can be done to provide simultaneous β amyloid deposition, pathologic tau, and
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35 neurodegeneration (ATN) classification [25]. Within the setting of this study, ^{18}F -FDG PET should still
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37 be seen as the primary choice, as it performed better compared to eASL in terms of sensitivity, reader
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39 confidence, effect size and lower variability in key regions in dementia diagnosis. These findings are in
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41 line with previous work on perfusion SPECT and ^{18}F -FDG PET in the individual diagnosis of
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43 Alzheimer's dementia, where 15-20% higher sensitivity and accuracy were found in favour of ^{18}F -FDG
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45 PET [26]. This had physiological (earlier glucose metabolic decline) as well as technical reasons (lower
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47 SPECT spatial resolution).
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51 In order to compare the diagnostic accuracy of ^{18}F -FDG PET and eASL in detecting functional
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53 abnormalities associated with dementia, we first performed a standardized qualitative visual analysis.
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55 This resulted in equal specificity for differentiating normal and abnormal scans for the two modalities,
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57 but in a higher sensitivity for ^{18}F -FDG PET compared to eASL. Considering the previous comparative
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1 qualitative analyses using visual rating methods in AD and/or FTD patients, previous work found similar
2 findings of lower observer agreement for ASL but matched sensitivity between the two modalities
3 [19,21,23]. Fällmar et al. noted a higher specificity and positive predictive value using ASL, but a higher
4 sensitivity and accuracy using ^{18}F -FDG PET images, when visually assessing ASL-based and ^{18}F -FDG-
5 based Z-maps in controls and patients with AD and FTD [17]. Since our study measured diagnostic
6 performance of ASL and ^{18}F -FDG PET in various types of potential neurodegenerative disorders, rather
7 than exclusively AD [23] and/or FTD [19,21], it is challenging to directly compare our results with these
8 prior investigations.
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11 Furthermore, for the second and much harder task to assign a specific differential diagnosis, including
12 blinded evaluation of screened healthy controls, we reported a higher percentage of correct classification
13 with ^{18}F -FDG PET than corresponding ASL image data. We observed a comparable intensity reduction
14 of cerebral perfusion and metabolism, predominantly in the parietal and posterior cingulate cortex in
15 AD. In other regions that are normometabolic/normoperfused in AD, such as the primary visual cortex,
16 cerebellum and subcortical regions, abnormality and confidence scores were lower with ASL which
17 may be due to lower values in normal individuals (see for example Fig. 1.A), watershed artefacts or
18 higher variability across the subcortical regions [27,28]. It is known that central arterial transit times
19 (ATT) are shorter than for the cortex, and that, even for multiplane tagging approaches such as applied
20 in our work, this difference may give rise to an underestimation of CBF as was shown in direct ^{15}O -
21 H_2O -PET versus eASL head to head comparative studies (Ishii et al, 2019; unpublished results). This
22 regional ASL and FDG differences can also be observed in our current work. Fig. 5 shows the
23 hypoperfusion in subcortical regions (such as basal ganglia and thalamus) in both healthy controls and
24 AD patients, obtained comparing ASL vs ^{18}F -FDG PET. In pathological conditions, such as AD, also
25 changes in ATT can give rise to alterations in the flow maps [29,30].
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53 The semiquantitative VOI- and voxel-based analyses at the group-level provided supportive findings
54 that were in line with the visual analysis. The regional Z-score approach confirmed the higher sensitivity
55 of ^{18}F -FDG PET compared to ASL in detecting abnormalities. On the other hand, the specificity was
56 found to be higher with ASL compared to ^{18}F -FDG PET, resulting in a similar overall accuracy between
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1 the two modalities for the classification into normal versus neurodegenerative abnormalities, which is
2 in agreement with Fällmar et al [17].
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4 In this context, it is of importance to note that the two reviewers were nuclear medicine specialists not
5 trained for neuroradiology, and thus had more experience with clinical assessment of ^{18}F -FDG PET. We
6 do not consider this a disadvantage or study design problem, as both had also long-term experience in
7 evaluating clinical routine perfusion SPECT images, and few neuroradiologists perform visual
8 assessment of ASL-MRI in a routine setting of neurodegeneration/dementia workup. Nevertheless, the
9 diagnostic performance of ASL in the visual analysis could be higher if an elaborated reader training
10 was implemented, or the visual analysis was complemented by availability of statistical Z-score maps
11 on a rendered surface projection, similarly to the work of Fällmar et al. [17]. In the latter study, the
12 sensitivity of ^{18}F -FDG-based Z-maps was still higher than in the corresponding ASL-based images [17],
13 and the visual findings in our study were also corroborated by semiquantitative analyses with similar
14 results.
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28 When evaluating voxel-based group differences in glucose metabolism and blood flow in AD compared
29 to controls, we found a similar spatial hypometabolism/hypoperfusion pattern localized in the posterior
30 cingulate, precuneus and parietotemporal areas [31,32], although both cluster intensity and extent of the
31 AD pattern was greater with ^{18}F -FDG PET compared to ASL, again indicating more robustly detectable
32 abnormalities in this subgroup. Similarly, anteromedial temporal and prefrontal abnormalities
33 [17,19,31] were more pronounced in FTD for ^{18}F -FDG PET versus ASL. In a recent simultaneous
34 PET/MR study comparing ASL and ^{18}F -FDG in AD and mild cognitive impairment (MCI) [33], a voxel-
35 wise analysis also revealed similar regional and quantitative abnormalities between ^{18}F -FDG PET and
36 ASL, and ASL images provided a reduced extent compared to ^{18}F -FDG PET, in line with our findings.
37 In patients with MCI, a voxel-wise analysis revealed no CBF reductions between MCI and controls in
38 the study of Riederer et al. [33], in contrast to ^{18}F -FDG PET with quantitative hypometabolism in the
39 precuneus, a brain region known to be one of the first affected in MCI due to AD [34]. A significantly
40 lower sensitivity of ASL Z-maps compared to ^{18}F -FDG PET Z-maps in discrimination of AD+FTD as
41 reported by Fällmar et al. [17], also confirms that regional CBF impairment is milder and/or occurs at a
42 later disease stage compared to regional hypometabolism.
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1 The additional value of the current study over published data can be summarized by the following
2 strengths. First of all, a head-to-head simultaneous and prospective comparison between ^{18}F -FDG PET
3 and ASL was performed in a true clinical context of patients with cognitive impairment referred for
4 exclusion/confirmation of a neurodegenerative disorder after careful clinical and paraclinical workup.
5
6 In contrast to previous comparative studies where the patient cohort was selected retrospectively, timing
7 discrepancies between both scans (disease progression) and selection bias (further imaging when
8 inconclusive previous imaging investigations) may have played a role. The majority of the studies
9 comparing PET and ASL have been performed on both separate PET/CT and MR systems and separate
10 occasions, with an interval between both exams ranging from a few days [21] up to 6 months
11 [17,22,31,35–37]. Simultaneous comparative PET/MR studies in dementia are rare [19,33,38]. Also, the
12 vast majority of these studies are principally based on voxel-wise image analysis at a group level, which
13 is not easily translatable to actual impact in clinical routine. Moreover, we included an age and gender
14 matched healthy control set acquired on the same instrumentation that was evaluated in a blinded fashion
15 and the heterogeneity of final diagnoses represents a true clinical scala of uncertain cases with cognitive
16 impairment.

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18 A major limitation of this study is the relatively small patient population that underwent additional
19 PET/MR scanning aside from the standard-of-care PET/CT scan. Nevertheless, the conclusions that can
20 be drawn from this study, are already significant and clearly show the differences between both
21 techniques with the current utilized instrumentation. Secondly, ground truth diagnosis was based on
22 clinical assessment including all routinely available information and disease follow-up. It is known that
23 in the setting of a tertiary memory clinic, diagnostic accuracy can approach 90% [26], but in large
24 proportions the final diagnosis may change with advance biomarkers such as amyloid PET [39].
25 Evaluations with CSF $\text{A}\beta$ and tau measurement and/or amyloid PET were only available for a small
26 subgroup of patients at final follow-up. Another limitation is the eASL imaging acquisition used. It is
27 known that the interindividual variance in ASL perfusion is large compared to the variance of
28 standardised uptake ratios in ^{18}F -FDG PET [40] and the sensitivity of eASL could have been improved
29 using higher channel head coils with more (32/64) receiver channels, that may offer up to twice the
30 signal-to-noise ratio (SNR) compared to an 8 channel coils. Improvement of SNR in eASL images may

1 likely decrease the variability across brain regions. It remains to be proven that incorporation of the
2 newest 32- or higher channels would improve sensitivity of detection of neurodegenerative patterns, but
3 the majority of the previous studies that have compared the diagnostic performance of ASL versus ^{18}F -
4 FDG PET in dementia used a similar standard receiver coil [17,19,21,22].
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8 As the data were acquired before implementation and validation of the Zero Echo Time (ZTE)
9 technique, which is now standardly used for individual MR-based attenuation map generation on the
10 GE Signa PET/MR, we used the vendor-supplied MRAC correction, which is known to give rise to a
11 small but significant craniocaudal gradient in the images with an underestimation of the infratentorial
12 ^{18}F -FDG activity [41]. It is unlikely that this would have driven the observed visual classification and
13 semiquantitative evaluation however, as it was also applied to the control data set. Finally, we did not
14 correct for partial volume effects since the primary aim of the study was to resemble clinical routine
15 evaluation as much as possible. Such correction was also not performed on the perfusion maps nor in
16 most previous studies in comparing ^{18}F -FDG and ASL [23,33,42].
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30 In conclusion, in this current direct prospective comparison between ^{18}F -FDG PET and eASL in a true
31 clinical context of differentiating neurodegenerative versus non-neurodegenerative classification of
32 cognitively impaired patients, as well as differentiation in dementia subtypes, we found that, on the GE
33 Signa PET/MR with multiplane tagging enhanced eASL, ^{18}F -FDG PET outperforms eASL in terms of
34 higher sensitivity, reader confidence, effect size and lower variability in key regions in dementia
35 diagnosis. When performing a semiquantitative analysis, a similar diagnostic accuracy between the two
36 modalities was obtained. As such, eASL with appropriate semiquantitative evaluation and comparison
37 to normal data, may complement ^{18}F -FDG PET or be an adjunct parameter to assess the N (neuronal
38 injury) status in patients suspected for dementia where in case of simultaneous acquisition, PET can be
39 directed towards amyloid or tau assessment.
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Compliance with Ethical Standards

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Conflict of Interest: The authors declare that they have no conflict of interest.

Ethical approval: All procedures performed in studies involving human participants were in accordance with the ethical standards of the institutional and/or national research committee and with the 1964 Helsinki declaration and its later amendments or comparable ethical standards.

Informed consent: Informed consent was obtained from all individual participants included in the study.

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FIGURE TITLES and LEGENDS

Figure 1. Typical examples of orthogonal and 3D-surface rendered eASL-MR and ^{18}F -FDG PET images of a healthy control (female, 40y; panel A) and subject with AD (male, 63y; panel B), respectively. Orthogonal and surface rendered images are scaled to the relative maximum value. Both images were classified concordantly and in the correct diagnostic class.

Figure 2. Visual rating of regional intensity for ^{18}F -FDG PET and ASL

Average rating (1 = *severely decreased*, 2 = *moderately decreased*, 3 = *mildly decreased*, 4 = *normal*) for right and left observed brain areas (frontal, parietal, temporal, occipital cortex, striatum, thalamus, precuneus and cerebellum). The ellipses indicates the average intensity rating corresponding to the occipital cortex, thalamus and striatum with the highest disagreement between both modalities. The intermittent line indicates the identity line.

Abbreviations: CON, healthy controls; NND, no arguments for neurodegenerative disorder; AD, Alzheimer's disease; FTD, frontotemporal dementia; LBD, Lewy body dementia; OTHER, rest of the patient group including motor neuron disease, cerebellar variant of multiple system atrophy, vascular dementia, and traumatic brain injury.

Figure 3. Regional semiquantitative analysis for assessment of neurodegenerative versus non-neurodegenerative scans with ^{18}F -FDG PET vs ASL

FDG PET- and ASL-based Z-scores for all observed brain areas (frontal, parietal, temporal, occipital cortex, striatum, thalamus, precuneus and cerebellum)/scans. The intermittent line indicates the identity line.

Abbreviations: NND, no arguments for neurodegenerative disorder; AD, Alzheimer's disease; FTD, frontotemporal dementia; LBD, Lewy body dementia; OTHER, rest of the patient group including motor neuron disease, cerebellar variant of multiple system atrophy, vascular dementia, and traumatic brain injury.

1
2 **Figure 4.** Results of the SPM group analysis for ^{18}F -FDG PET and ASL: *a*) 30 CON versus 8 AD
3 patients; *b*) 30 CON versus 2 FTD patients. Evaluations at $p_{\text{height}} < 0.01$ and extend threshold $k_{\text{ext}} = 20$
4 $(2 \times 2 \times 2 \text{ mm}^3)$ voxels.
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9 **Figure 5.** Transversal, parasagittal and coronal average eASL-MR (top row) and ^{18}F -FDG PET maps
10 (bottom row) for healthy controls (CON) (left panel) and AD patients (right panel). Images are scaled
11 to the global grey matter value.
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14 White triangles indicate $\text{eASL} < ^{18}\text{F}$ -FDG PET in subcortical regions such as in the basal ganglia and
15 thalamus.
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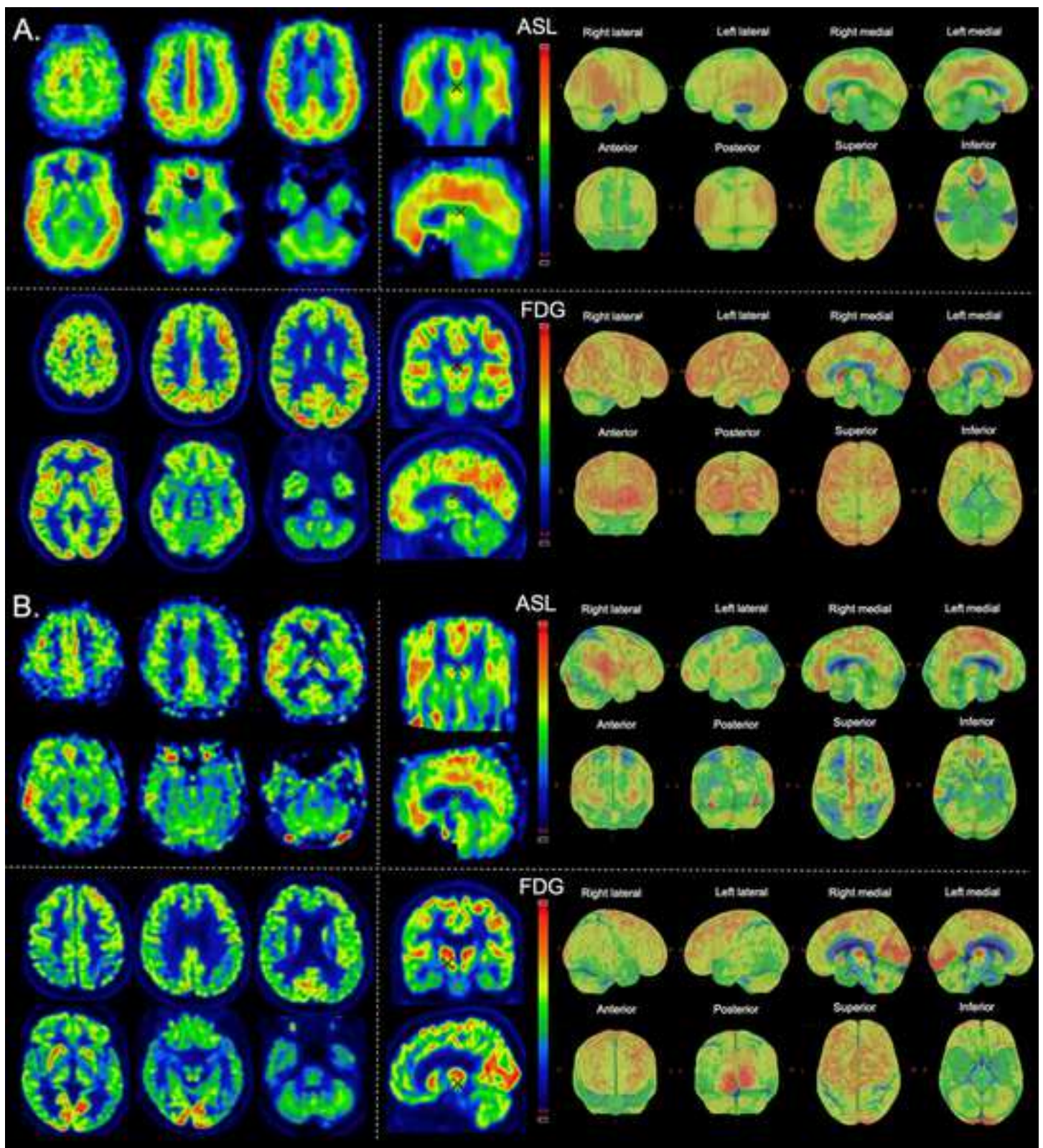
Table 1. Patient demographics and diagnoses.

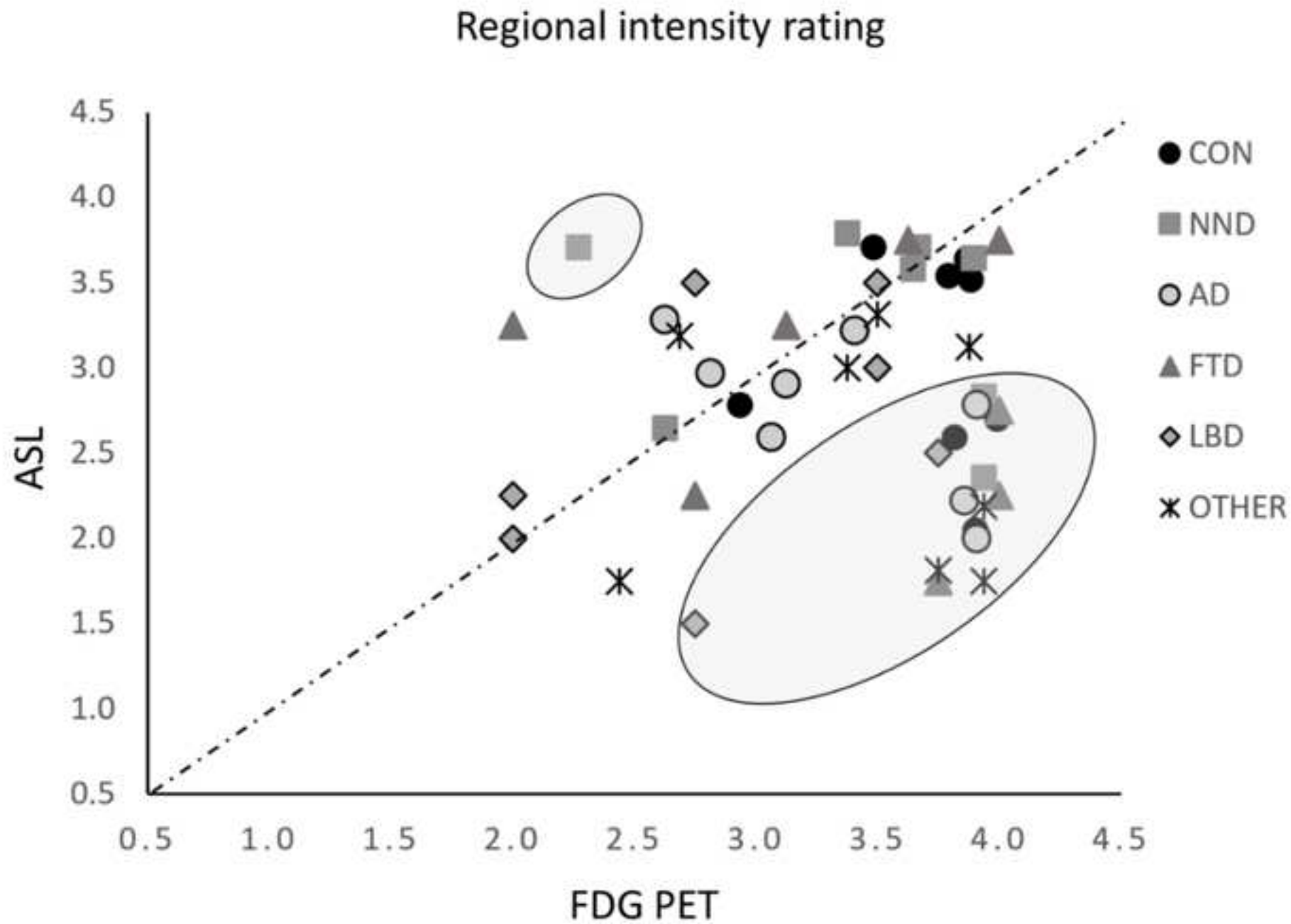
Patients number	Age (years)	Gender (M/F)	MMSE	Working diagnosis at ¹⁸ F-FDG PET	Final Dx	Years of symptoms prior to ¹⁸ F-FDG PET
1	69	F	27	NND	NND	2.1
2	63	M	30	NND	NND	2.8
3	55	F	28	NND	NND	2.1
4	76	M	26	AD	AD	6.5
5	40	F	30	NND	NND	1.9
6	47	M	30	TBI	TBI	31.4
7	70	F	23	FTD	FTD	0.2
8	68	F	28	NND	AD*	2.3
9	47	M	n/a	NND	NND	n/a
10	73	F	25	AD	AD	1.0
11	56	F	11	MND	NND*	1.0
12	72	M	18	AD	NND (post-CVA)*	0.7
13	73	M	12	AD	AD	0.8
14	71	F	17	AD	AD	0.7
15	66	M	22	AD	AD	3.2
16	40	M	25	NND	NND	1.6
17	77	M	n/a	AD	Parkinsonism*	n/a
18	77	F	21	NND	AD*	0.5
19	70	F	27	NND	NND	2.5
20	63	M	24	AD	AD	0.7
21	73	M	29	MSA-c	MSA-c	1.9
22	69	F	n/a	LBD	LBD	n/a
23	57	M	n/a	NND	NND	1.6
24	55	F	27	NND	NND	1.6
25	78	F	23	NND	NND	2.0
26	59	M	30	NND	NND	1.6
27	71	M	21	FTD	FTD (+MND)*	0.5

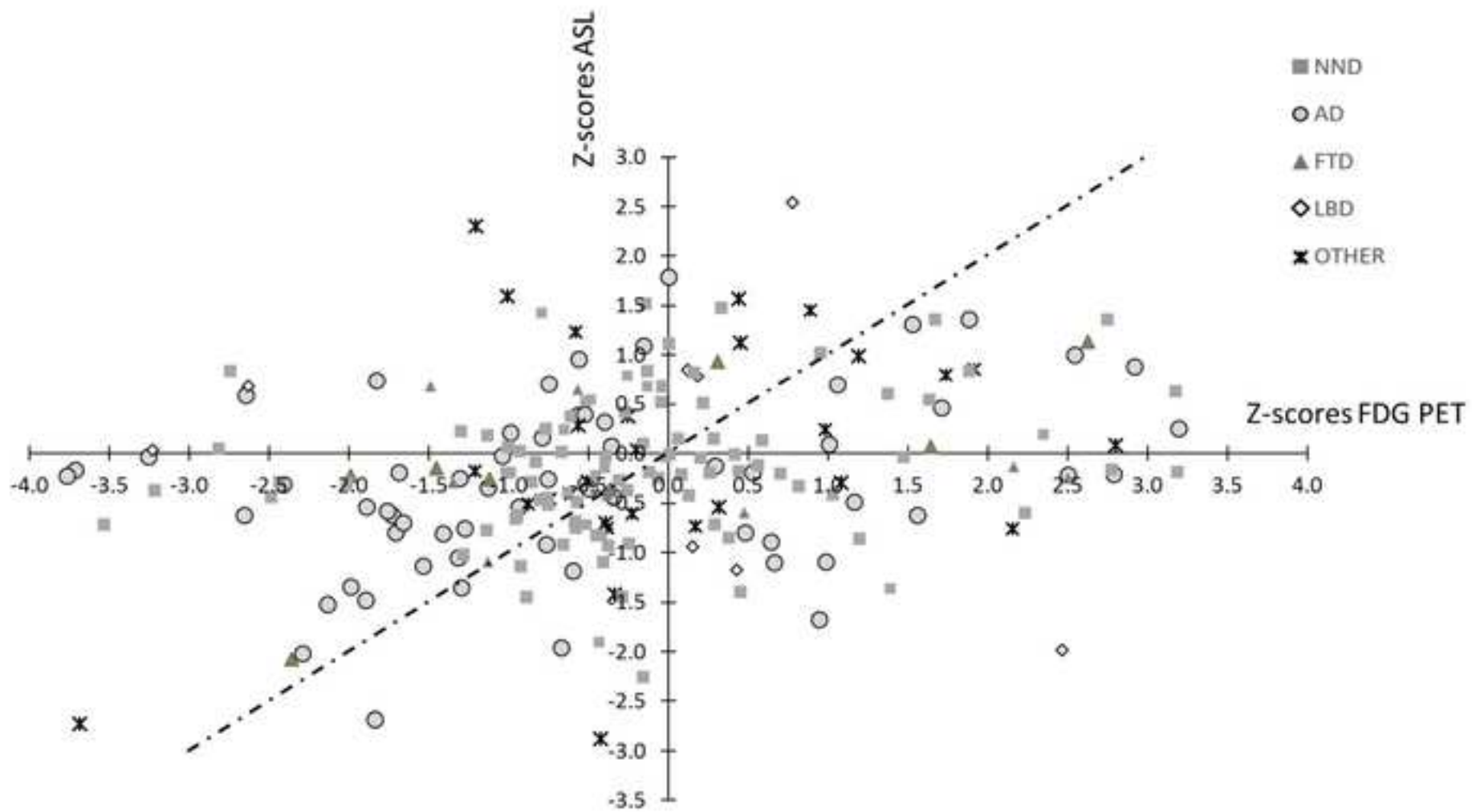
Dx, diagnosis; AD, Alzheimer's disease; FTD, frontotemporal dementia; LBD, Lewy body dementia; MND, motor neuron disease; MSA-c, cerebellar variant of multiple system atrophy; CVA, cerebrovascular accident dementia; NND, no arguments for neurodegenerative disorder; TBI, traumatic brain injury; n/a, data not available. * indicates alterations from the working diagnosis (Dx) at the time of ¹⁸F-FDG PET.

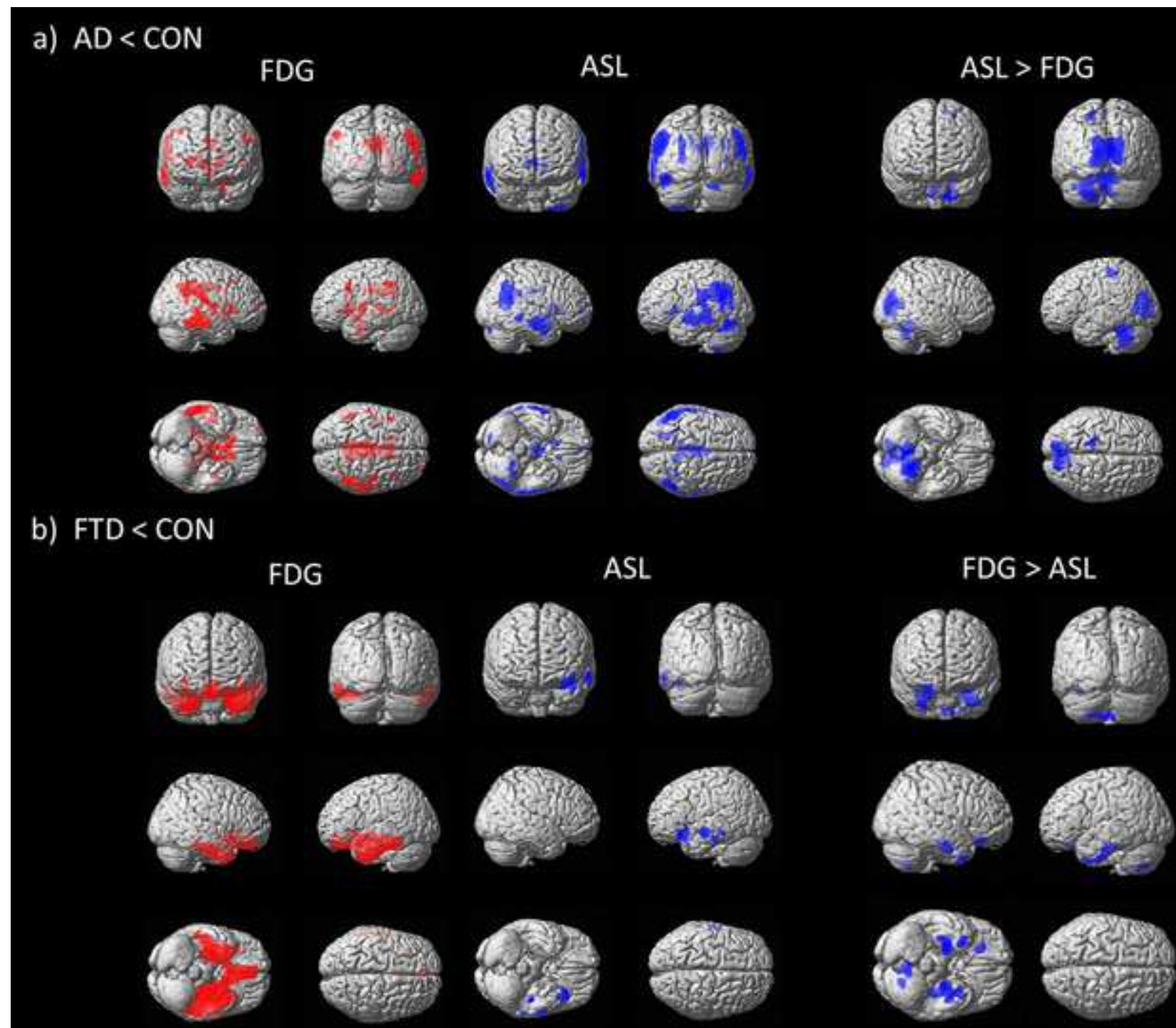
Table 2. Visual read results for ^{18}F -FDG PET and ASL, classified into normal and abnormal neurodegenerative (ND) pattern.

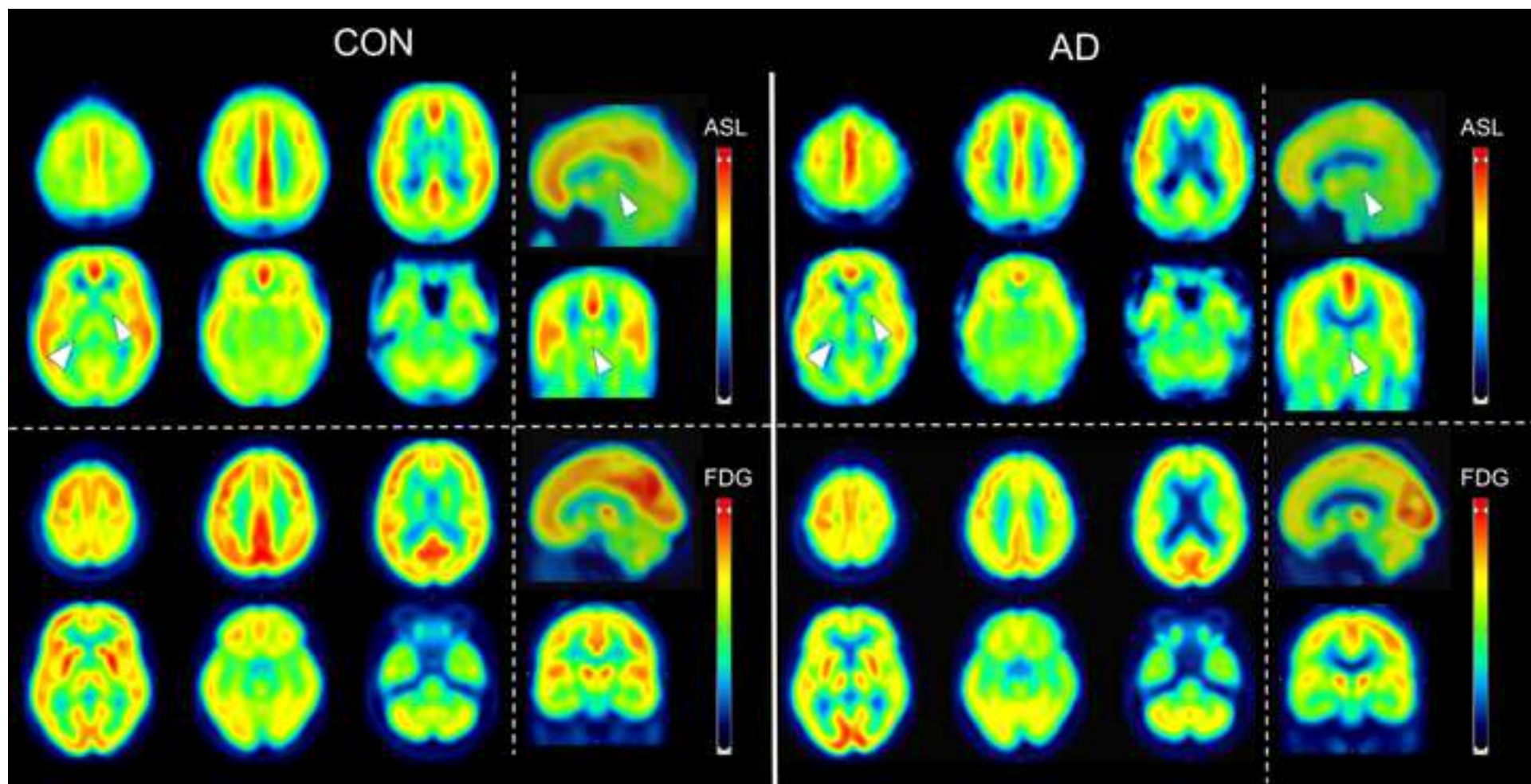
^{18}F-FDG				
	PET ND pattern		PET normal	
Final diagnosis	Reader 1	Reader 2	Reader 1	Reader 2
Neurodegenerative disorder (14)	13	13	1	1
Normal / no neurodegenerative disorder (30 CON + 13)	6	20	37	23
Sensitivity	0.93	0.93		
Specificity	0.86	0.53		
ASL				
	ASL ND pattern		ASL normal	
Final diagnosis	Reader 1	Reader 2	Reader 1	Reader 2
Neurodegenerative disorder	10	8	4	6
Normal / no neurodegenerative disorder	11	14	32	29
Sensitivity	0.71	0.57		
Specificity	0.72	0.67		













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Supplementary Material

FDG PET vs ASL in dementia - PETMR
study_Ceccarini_Sup Mat.docx