

Efficacy of Morpho-Geometrical Analysis of the Corneal Surfaces in Keratoconus Disease According to Moderate Visual Limitation

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Abstract. The cornea is a complex hemispheric structure, made of collagen fibres that provide it a homogenous and stable geometry. During keratoconus disease, a loss of tenacity takes place in the collagen fibres that form the corneal structure, producing an alteration of its geometry, this is, a change of its curvature, and therefore, a loss of visual quality of patients. The geometric characterization of the hemispheric structure by means of biometric parameters is a very solid technique of diagnosis, based in a virtual 3D model, which has already been validated for several degrees of severity of keratoconus pathology. In this prospective comparative study, 93 corneas (50 healthy subjects and 43 patients with keratoconus with moderate visual limitation) were geometrically modelled. The results obtained in this work suggest that the best predictive biometric parameters are anterior corneal surface area and posterior apex deviation, and that the strongest correlation is produced between sagittal plane apex area in minimum thickness point and sagittal plane apex area. The studied biometric parameters have shown significant differences between groups. Therefore, the analysis of the biometric parameters that register the geometric decompensation that locally appear in a corneal region, as a response to the asymmetry produced during the development of keratoconus disease with a moderate visual impairment, is a new approach that may lead to a better understanding of the disease with this degree of optical limitation.

Keywords: Computer-Aided Geometric Design (CAGD), Optical Aberrometry, Scheimpflug, 3D Modelling.

1 Introduction

The cornea is an avascular structure with a hemispheric shape that is part of the anterior segment of the human eye [1]. It is a highly differentiated tissue with five layers which

have different functions, being the most important the one of the first ocular refractive element, due to its properties of transparency and curvature along all the structure [2].

One of the main pathologies of the cornea is keratoconus, which is a clinical term that describes a corneal condition characterized by its progressive thinning, which causes a cone-shaped corneal protrusion [3]. This degenerative geometrical deformation leads to a decrease of cornea's optical quality.

The knowledge, from a clinical point of view, of the geometrical characteristics of the cornea is important in clinical practice [1]. There are several studies in scientific literature which have validated indexes or topographic descriptors of the cornea [3,4] in order to define the cut off values that allow the discrimination between normal and keratoconus corneas. From this indexes, several keratoconus classifications have been proposed, such as a morphological classification [1], keratometric [5], of keratoconus severity [6], or Amsler-Krumeich [1]. However, none of these classifications measures the degree of severity of keratoconus depending on the visual limitation level.

In addition, computer-aided design is a widespread tool for biological structure modelling [7-9], and its later use for disease diagnosis [10,11]. Our research group have developed some new virtual geometric models of the human cornea that have been used to characterize corneal ectasia disease basing on Amsler-Krumeich classification [12-14], and for other classification, named RETICS [15], which allows characterizing keratoconus' pathology considering visual performance of patients in its initial phases [16,17].

This investigation work proposes a way to characterize cornea's morphogeometry in keratoconus pathology with a moderate degree of visual performance, and also to quantify the existence of correlations between the geometries of corneal surfaces for this degree of severity of the disease.

2 Materials and Methods

2.1 Participants

This observational case series study evaluated 93 corneas of 93 patients (selected at random to avoid interference) structured in two groups: a normal group (healthy corneas), which included 50 subjects presenting no ocular pathology (36.80 ± 15.67 years); and a second group, composed of 43 patients diagnosed with moderate KC (46.67 ± 24.99 years). The classification protocol for normal or moderate KC cases was run according to reported state of the art of clinical and topographic evaluations [18].

All patients were selected according to the RETICS grading. Inclusion criteria were patients diagnosed as Grade III KC eyes (moderate visual impairment, $0.4 < CDVA \leq 0.6$ in decimal scale, or $6/15 < CDVA \leq 6/9.5$ Snellen), corneal topography revealing a localized steepening, and/or an asymmetric bowtie pattern with or without skewed radial axis. The exclusion criteria were the following: any previous ocular surgery, ocular surface inflammation, moderate to severe dry eye or other active ocular comorbidity, or use of contact lenses within the four weeks prior to the first visit.

These evaluations were made at Vissum Instituto Oftalmologico Alicante, Spain (Vissum) who were adequately informed about the clinical study and voluntarily signed

their consent to participate. The study was ratified by the clinic's Institutional Review Board in compliance with the ethical restrictions established in the Declaration of Helsinki (Seventh revision, October 2013, Fortaleza, Brasil).

2.2 Examination Protocol

All subjects selected for this study were examined using Sirius System® (CSO, Florence, Italy), and following a validated protocol previously created by our research group, which has been thoroughly described in preceding studies [14,12,13], and that has proved itself successful when used for diagnosis and characterization of KC in asymptomatic (pre-clinical) and mild visually-impaired eyes [17,16].

The final output of this protocol after its application, is a patient-specific 3D virtual model of the cornea, which is then analysed to find several biometric parameters (Figure 1). These biometric parameters studied herein, along with their characteristics, have been previously described in [19], and are summarized in Table 1, but are used for the first time to study KC eyes with moderate visual impairment. In this study, the Rhinoceros' surface was deformed to minimise the nominal distance between the spatial points and the surface. This deviation could be later calculated by the software, providing a mean value of the distance error for the solution surface of $5.560 \times 10^{-17} \pm 5.81 \times 10^{-17}$ mm (mean \pm standard deviation).

Table 1. Biometric parameters analysed in the study.

<i>Biometric parameter</i>	<i>Description</i>
Total corneal volume (Vol _{tot}) [mm ³]	Volume limited by front, back and peripheral surfaces of the solid model generated
Anterior / posterior corneal surface area (Corarea _{ant} / Corarea _{pos}) [mm ²]	Area of the front/exterior and rear/interior surfaces
Total corneal surface area (Corarea _{tot}) [mm ²]	Sum of anterior, posterior and perimeter corneal surface areas of the solid model generated
Sagittal plane apex area (Splarea _{apex}) [mm ²]	Area of the cornea within the sagittal plane passing through the optical axis and the highest point (apex) of the posterior corneal surface
Anterior and posterior apex deviation (Dev _{aapex} / Dev _{papex}) [mm]	Average distance from the optical axis to the highest point (apex) of the anterior / posterior corneal surfaces
Sagittal Plane Area in minimum thickness point (Splarea _{minthk}) [mm ²]	Area of the cornea within the sagittal plane passing through the optical axis and the minimum thickness point (maximum curvature) of the posterior corneal surface
Anterior and posterior minimum thickness point deviation (Dev _{aminthk} / Dev _{pminthk}) [mm]	Average distance in the XY plane from the optical axis to the minimum thickness points (maximum curvature) of the anterior / posterior corneal surfaces
Centre of mass X, Y, Z (COM _X , COM _Y , COM _Z) [mm]	Centre of mass coordinates X, Y, Z of the solid

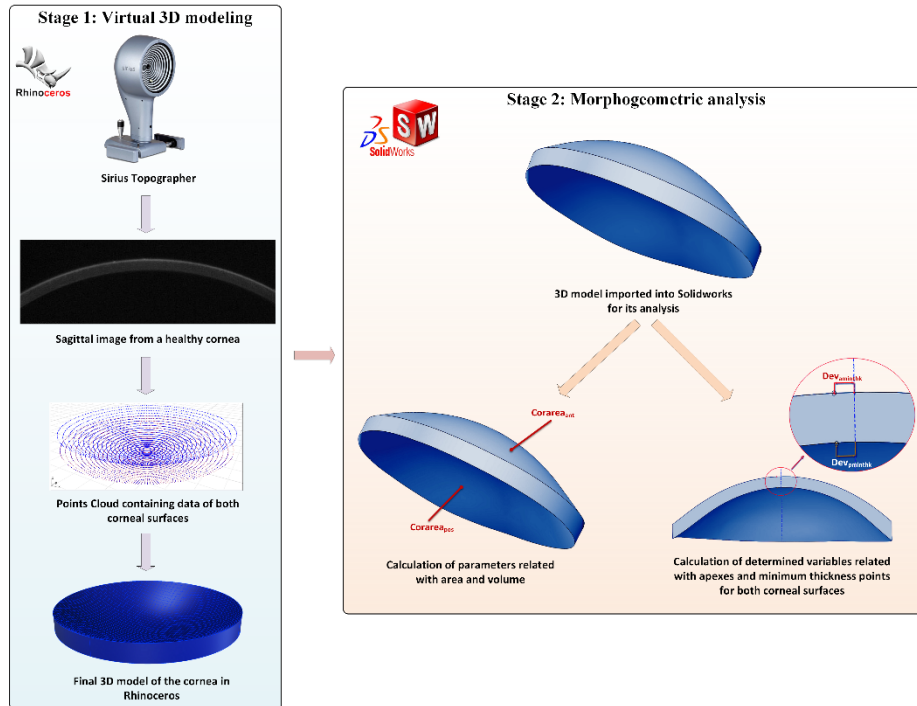


Fig. 1. Scheme of the procedure for the generation of a virtual model and later analysis of the corneal structure.

2.3 Statistical Analysis

Both Kolmogorov-Smirnov test and Shapiro-Wilks test were run to check data normality. According to these tests and thereafter, a Student's T-test or U-Mann Whitney Wilcoxon test were employed, when appropriate. Correlation between parameters was assessed by means of Pearson coefficients (for normally distributed data) or Spearman coefficients (not normally distributed). A significance level of 0.05 was fixed for p-values in all statistical tests. Receiver operating characteristics (ROC) curves were used to determine which parameters could be useful in terms of characterization of diseased corneas, and optimal cut-offs were established using Youden's J index, basing on sensitivity and specificity values [20,21]. Graphpad Prism V 6 (GraphPad Software, La Jolla, USA) and IBM SPSS V 23.0 software (SPSS, Chicago, USA) were used to make all the analyses.

3 Results

Most of the modelled parameters showed statistically significant differences when comparing healthy and moderate KC corneas, as shown in Table 2 below.

Table 2. Descriptive values and differences in the modelled biometric parameters among the normal and moderate KC groups. SD: standard deviation. P: statistical test, Z: z-score.

<i>Biometric Parameters</i>	<i>Normal Group (n = 50)</i>				<i>Moderate KC Group (n = 43)</i>				<i>z</i>	<i>P</i>
	<i>Mean</i>	<i>SD</i>	<i>Min</i>	<i>Max</i>	<i>Mean</i>	<i>SD</i>	<i>Min</i>	<i>Max</i>		
Vol _{tot} (mm ³)	25.71	1.53	23.23	29.07	23.97	1.52	21.06	28.74	-5.16	0.000
Corarea _{ant} (mm ²)	43.08	0.14	42.77	43.33	43.67	0.47	42.79	45.09	-7.37	0.000
Corarea _{pos} (mm ²)	44.24	0.26	43.53	44.71	45.22	0.80	44.17	47.53	-7.24	0.000
Corarea _{tot} (mm ²)	103.87	1.12	100.73	105.66	104.91	1.70	101.91	109.95	-3.47	0.001
Splarea _{papex} (mm ²)	4.32	0.26	3.93	4.87	3.93	0.29	3.19	4.83	6.72	0.000
Splarea _{minthk} (mm ²)	4.31	0.26	3.92	4.86	3.92	0.29	3.19	4.82	6.61	0.000
Dev _{aapex} (mm)	0.00	0.00	0.00	0.01	0.02	0.00	0.00	0.07	-7.57	0.000
Dev _{papex} (mm)	0.07	0.02	0.04	0.09	0.21	0.08	0.03	0.34	-7.37	0.000
COM _X (mm)	0.04	0.02	0.01	0.09	0.02	0.05	-0.15	0.20	3.39	0.001
COM _Y (mm)	0.03	0.02	0.00	0.08	0.00	0.05	-0.14	0.16	-5.14	0.000
COM _Z (mm)	0.77	0.02	0.71	0.81	0.83	0.06	0.72	1.00	-6.26	0.000
Dev _{aminthk} (mm)	0.83	0.21	0.44	1.27	0.81	0.09	0.35	1.81	0.37	0.713
Dev _{pminthk} (mm)	0.76	0.20	0.38	1.24	0.74	0.26	0.30	1.31	0.57	0.570

3.1 Roc Analysis

A ROC analysis was used to ascertain the predictive value of the modelled parameters (Figure 2). Five biometric parameters showed an area under the ROC (AUROC) above 0.7 (Table 3).

Table 3. The area under the ROC results.

<i>Biometric Parameters</i>	<i>AUROC</i>	<i>Sensitivity</i>	<i>Specificity</i>	<i>Cut off value</i>
Corarea _{ant}	0.945	86.0	96.0	≥ 43.2595 mm ²
Corarea _{pos}	0.937	83.7	96.0	≥ 44.6205 mm ²
Dev _{aapex}	0.910	83.7	94.0	≥ 0.0010 mm
Dev _{papex}	0.945	93.0	99.9	≥ 0.0965 mm
COM _Z	0.878	69.8	98.0	≥ 0.0809 mm

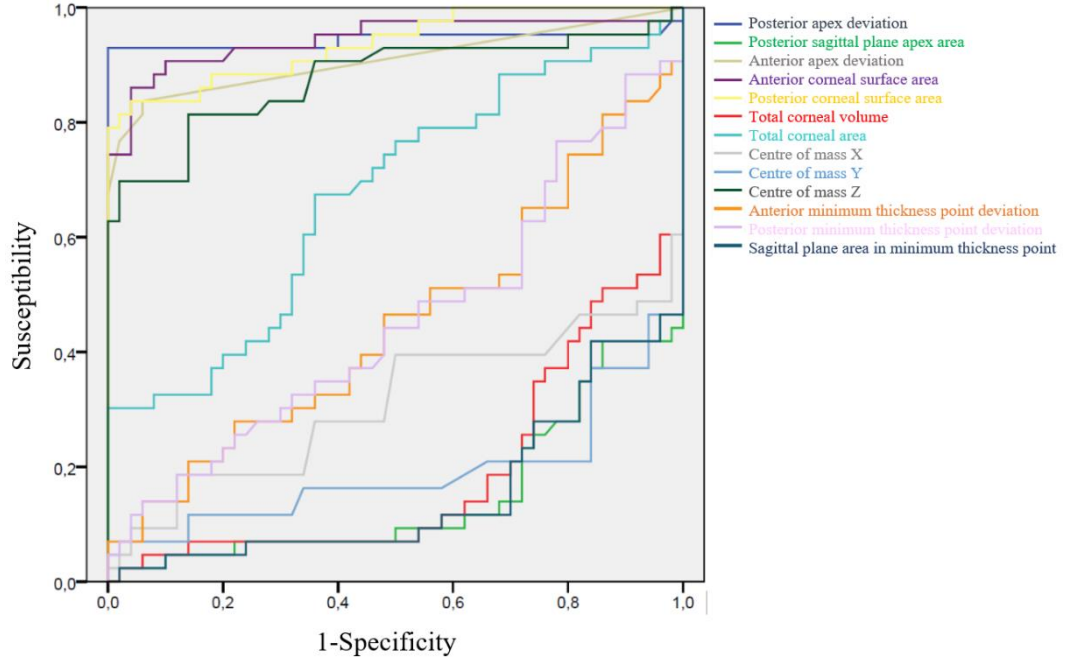


Fig. 2. Curves for modelled parameters detecting moderate KC.

Table 4 summarizes all significant correlations between the modelled biometric parameters for the moderate KC group. Correlation coefficients between parameters for normal group have not been included, as their mutual relations have already been addressed in a previous study [16].

Table 4. The significant correlation coefficient values for the modelled variables in the moderate KC group.

<i>Measurement correlation</i>	<i>Moderate KC group (n = 43)</i>	
	<i>Correlation coefficient</i>	<i>P value</i>
$Splarea_{papex} / Vol_{tot}$	0.965	0.000
$Corarea_{ant} / Dev_{papex}$	0.313	0.041
$Corarea_{pos} / Dev_{papex}$	0.361	0.017
$Corarea_{ant} / Corarea_{pos}$	0.941	0.000
$Corarea_{ant} / Corarea_{tot}$	0.778	0.000
$Corarea_{pos} / Corarea_{tot}$	0.864	0.000
$Vol_{tot} / Corarea_{tot}$	0.354	0.020
$COM_x / Corarea_{ant}$	-0.340	0.025
$COM_x / Corarea_{pos}$	-0.317	0.038
$COM_x / Corarea_{tot}$	-0.361	0.017

COM_x / COM_z	-0.369	0.015
$COM_z / Corarea_{ant}$	0.938	0.000
$COM_z / Corarea_{pos}$	0.882	0.000
$COM_z / Corarea_{tot}$	0.844	0.000
$Dev_{aminthk} / Dev_{papex}$	0.440	0.003
$Dev_{pminthk} / Dev_{papex}$	0.532	0.000
$Dev_{aminthk} / Dev_{pminthk}$	0.979	0.000
$Splarea_{minthk} / Splarea_{papex}$	0.997	0.000
$Vol_{tot} / Splarea_{minthk}$	0.963	0.000
$Dev_{aaapex} / Dev_{papex}$	0.403	0.007

4 Discussion

The cornea is a complex hemispheric structure, made of collagen fibres that provide it a homogenous and stable geometry. In a pathological scenario, a loss of tenacity takes place in the collagen fibres that form the corneal structure, producing an alteration of its geometry, this is, a change of its curvature, and therefore, a loss of visual quality of patients [22].

There are in scientific literature several works that have studied the geometry of corneas with a moderate degree of optical aberration [23,13,24]. Several studies [23] observed that corneal thickness is not constant in this pathology, as a thinning is produced in the region in which the loss of structural tenacity appears. These results are consistent with the ones obtained by other researchers [24] that analysed the thickness of corneas with an advanced degree of optical aberration. Other recent study has demonstrated that some morphological singularities as well as corneal thickness are related with disease progression [13]. Therefore, the cornea in this pathology shows a region of geometrical decompensation as a non-symmetric response to the disease progress. However, the parametrization and study of the correlation between the biometric parameters that register this decompensation, which allow to evaluate the progression of keratoconus with moderate visual loss, have not been analysed for each patient from a virtual model of their own eye.

In this study, all measures made have resulted consistent, and almost all mean differences have been statistically significant between healthy corneas and corneas with keratoconus showing a moderate degree of visual impair, except for the anterior/posterior minimum thickness point deviation. These results are in accordance with the ones reported by previous studies that evaluated some of these anatomic parameters with equipment based in Scheimpflug technology [25]. In our study, we have used a technology based in a double rotating camera based in the Scheimpflug projection system. This system has shown, in a previous study [26], being a robust and repeatable system for spatial data acquisition of the hemispheric structure, from which basing the generation of the virtual model with CAD software [17].

Regarding the AUROC, four parameters from all the ones analysed in our study showed very high discriminant values ($AUROC > 0.9$). Two parameters, which are the anterior and posterior corneal surface areas showed AUROC values of 0.937 y 0.945 respectively, due to the fact that in the pathological scenario a biomechanical weakening takes place, caused by the loss of tenacity of the hemispheric structure and consequently, an increase of the corneal surface curvature is produced. This tendency is in line with some previous works that made ratio studies between anterior and posterior areas for different degrees of severity of the disease [25]. The other two parameters with high discrimination values were anterior apex deviation ($AUROC= 0.910$) and posterior apex deviation ($AUROC= 0.945$), this is because the corneal apex is the point of maximum curvature in corneal surfaces, therefore, according with other authors [27], the apex deviation is a parameter that could affect the visual performance of the patients.

In this study, we have analysed the correlation between biometric parameters that register the structural alteration which manifests during the disease development. So, the parameters related with the areas show a strong positive correlation, specifically between anterior and posterior surface areas ($R^2= 0.941$, $p = 0.000$), anterior surface area and total corneal surface area ($R^2= 0.778$, $p = 0.000$) and posterior and total corneal surface areas ($R^2= 0.864$, $p = 0.000$), due to the fact that corneal surfaces tend to behave proportionally during the evolution of the disease. These results are consistent with the ones obtained for corneal curvature in eyes with keratoconus, with the biomechanical weakening of the cornea, and with the possible effect of intraocular pressure in the weakened corneal structure [28].

Regarding anterior and posterior deviations, both between corneal apex points ($R^2= 0.832$, $p = 0.000$) and minimum thickness points ($R^2= 0.997$, $p = 0.000$), there is a strong positive correlation, this is in line with the results reported by other authors [25] that demonstrated a robust correlation between apex deviation and the minimum thickness points and their relation with the pachymetric progression of corneal thickness.

5 Conclusion

The analysis of the biometric parameters that register the geometric decompensation that locally appear in a corneal region, as a response to the asymmetry produced during the development of keratoconus disease with a moderate degree of optical aberration, is a procedure that provides the ophthalmologist a new tool for the diagnosis of this pathology with this degree of development. In this work it has been ascertained that the most predictive biometric parameters are the anterior corneal surface area and the deviation of the posterior apex, detecting that the strongest correlation is the one between the areas of the sagittal planes defined through the minimum thickness points and the posterior corneal apex. The studied biometric parameters showed significant differences between groups. Therefore, this new approach based in the personalised diagnosis from a computational model may lead to a better understanding of the disease with this degree of optical limitation.

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7 Additional Information

Conflict of Interest: The authors have no conflict of interest to declare.

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