

Elaboration and Characterization of Alumina-Fluorapatite Composites

Awatef Guidara, Kamel Chaari^{*}, Jamel Bouaziz

Laboratory of Industrial Chemistry, National School of Engineering, Sfax, Tunisia. Email: kamel70tn@yahoo.fr

Received November 26th, 2010; received February 20th, 2011; accepted February 28th, 2011.

ABSTRACT

Alumina and fluorapatite powder were mixed in a wet medium in order to elaborate biphasic ceramics composites. The effect of fluorapatite addition (26.5 wt%) in the densification and the mechanical properties of the alumina matrix were measured. The phase developments have been systematically analysed by scanning electronic microscopy, X-ray diffraction, Infrared spectroscopy and ³¹P and ²⁷Al magic angle scanning nuclear magnetic resonance. The Brazilian test was used to measure the mechanical resistance of alumina-26.5 wt% fluorapatite composites. The densification and strength rupture of composites increase versus sintering temperature and holding time. At 1600°C, the composites densities reached 85% and the rupture strength was about 22 MPa. Also, the composites sintering at 1500°C for 5 hours provides samples with similar density and having higher mechanical resistance, above 26 MPa. For longer holding times, the mechanical properties were hindered by the exaggerated grain growth and the formation of intragranular porosity. From 1400°C, the characterization of the alumina-26.5 wt% fluorapatite composites indicates the formation of calcium aluminates.

Keywords: Sintering, Fluorapatite, Alumina, Bioceramics, Composites, Mechanical properties

1. Introduction

Calcium phosphate-based materials have attracted considerable interest in orthopedic and dental applications because of their biocompatibility and tight bonding to bone, resulting in the growth of healthy tissue directly onto their surface [1-4]. Among them, fluorapatite (Fap) has been investigated as an alternative biomedical material [5]. This particular apatite was recognized as the most thermally stable compound [6]. Fluorapatite has also been considered as an attractive material for its similarity in structure and composition to bone with the added benefit of fluoride release [7]. In vitro studies have shown that fluorapatite is biocompatible, has a better stability [8,9] and also provides fluoride release at a controlled rate to ensure the formation of a mechanically and functionally strong bone [10]. However, the mechanical properties of fluorapatite and all other calcium phosphates are generally inadequate for many load-carrying applications [11]. These bioceramics have a low density decreasing the mechanical properties [12-17]. Several combinations between calcium phosphate and other compounds have been proposed in order to improve the

poor mechanical properties of calcium phosphate [2,18-23].

Alumina (α -Al₂O₃) was the first bioceramic widely used clinically. It is used in load-bearing hip prostheses and dental implants because of its combination of excellent corrosion resistance, good biocompatibility, high wear resistance and high strength [1].

The aim of this work was to elaborate a dense material having adequate mechanical properties to be used essentially as dental implants. Implants present the quality of auto-protection against caries proliferation [24]. So, the percentage of Fap is chosen to get the same bone rate of fluoride (approximately 26.5 wt%). In bone, the fluoride content is approximately 1 wt% (10,000 ppm) [5]. Fluoride has also been administered in bone to prevent the reduction in bone density associated with osteoporosis even though results are still controversial [25-27]. High fluoride levels may produce some undesired effects, one of which is linked to an increase in bone fractures [28].

This work focuses on preparing biphasic alumina-26.5 wt% Fap composites sintered at various temperatures for different times and to characterize the resulting composites with density and mechanical properties.

2. Materials and Methods

The fluorapatite powder was synthesized by a wet-chemical method [29-31]. Analytical grade $Ca(NO_3)_2 \cdot 4H_2O$, $(NH_4)2HPO_4$ and NH_4F were used as the starting materials. A calcium nitrate solution is slowly poured using a peristaltic pump into a boiling solution containing diammonium hydrogenophosphate; 28% NH_4OH solution was added to the mixture and the pH was adjusted to 9. The precipitate was aged with stirring at 80°C for 1 h, then filtered, washed, dried at 70°C for 12 h and calcined at 500°C. Each undesirable synthesized powder is instantly eliminated.

High purity α -alumina (α -Al₂O₃) powder (Riedel-de haën, 98%) was used in all experiments. The Fap has been used with 26.5 wt% amount because the human bone contains 1 wt% of fluoride approximately [32].

The Al_2O_3 and Fap powder were mixed in an agate mortar. The powder mixtures were milled in ethanol. After milling and homogenization, the mixtures were dried at 80°C for 24h. After drying, the powder mixtures were moulded in a cylinder having a diameter of 20 mm and a thickness of 6 mm and pressed under 150 MPa. The green compacts were sintered at various temperatures and holding times. The bulk density of the sintered body was calculated from the dimensions and weight. Three tests were made for every experiment. The relative error of apparent porosity value was about 1%.

The particle size dimension of the powder was measured by means of Micrometrics Sedigraph 5000. The specific surface area (SSA) was measured by azotes absorption from the BET method (ASAP 2010) [33]. The main particle size (D_{BET}) was calculated by assuming the primary particles to be spherical [30]:

$$D_{BET} = \frac{6}{S\rho} \tag{1}$$

where ρ is the theoretical density of Al₂O₃ (3.90 g/cm³) or Fap (3.19 g/cm³), and S is the SSA of powder.

The samples before and after sintering were examined in an X-ray diffractometer using CuK α (PHILIPS-PAN-ALYTICAL; X'PERT pro MPD); the crystalline phases were identified by reference to the International Center for Diffraction Data (ICDD) cards. The samples were also submitted to infrared (IR) spectrometric analysis (Spectrum BX) using KBr. The Al₂O₃-26.5 wt% Fap composites were characterized by high resolution solid state using a Bruker 300WB spectrometer. NMR spectra were recorded at a ³¹P frequency of 121.5 MHz (field of 7.04 T) and ²⁷Al frequency of 78.2 MHz (field of 7.04 T). The ³¹P NMR chemical shifts reference is the phosphoric acid H₃PO₄. The ²⁷Al NMR chemical shifts were referenced to a static signal obtained from an aqueous aluminium chloride solution AlCl₃·6H₂O. The obtained products were examined by scanning electron microscope (SEM) (PHILIPS XL 30).

Differential thermal analysis and thermogravimetry were carried out using about 30 mg of powder (DTA-TG; Model Setaram). The heating and cooling rates were respectively 10°C min⁻¹ and 20°C·min⁻¹. Linear shrinkage was determined by dilatometry (Setaram) using the same thermal cycle as the one used for DTA.

The mechanical resistance was determined by Brazilian test (Lloyd EZ50). The optimum rupture strength σ_r was offered by equation [17]:

$$\sigma_r = \frac{F}{S} = \frac{2F}{\pi De} \tag{2}$$

where F is the tensile strength and D and e are the diameter and the thickness of the samples.

3. Results and Discussion

3.1. Characterization of the Ceramic Powders

The SSA, the calculated average grain sizes D_{BET} (Equation (1)) and the particles size distribution data (measured by granulometric repartition) for Al_2O_3 and Fap powder are showed in **Table 1**. The difference between the value deducted by SSA (D_{BET}) and by granulometric repartition (D_{50}) was probably due to the presence of agglomerates in the initial powder.

The X-ray diffraction pattern of alumina shows only peaks of α phase (**Figure 1(a)**). The X-ray diffraction pattern of fluorapatite powder reveals peaks of Fap and CaO traces (**Figure 1(b**)). It must be kept in mind that XRD analysis does not detect the presence of a small amount of impurities, especially when compounds have poor crystallinity [34]. The presence of CaO is confirmed by the phenolphthalein test. A similar observation has already been made [17,35]. CaO is produced by solid reaction between CaF₂ and H₂O, which can be expressed by the following equation [36]:

$$CaF_2 + H_2O \rightarrow CaO + 2HF$$
 (3)

 CaF_2 was contained in the synthesised Fap powder as impurity.

IR spectra of the alumina and fluorapatite powders (**Figure 2**) illustrate only alumina and fluorapatite characteristic bands. From the IR spectrum of alumina (**Figure 2(a)**), the absorption bands at 422, 452, 500, 558, 594,

Table 1. SSA, average grain size obtained by different analysis of Al_2O_3 and Fap powders.

	SSA	$D_{BET}\left(\mu m\right)\pm0.2$	$D_{50} \left(\mu m\right) \pm$	d ^a
	(m^2/g)		0.2	
Fap	29.00	0.07	3.00	3.19
α -Al ₂ O ₃	2.87	0.53	7.00	3.90
Composites	9.80	0.40	5.94	3.70

^a Theoretical density



Figure 1. XRD patterns for: (a) Al_2O_3 powder; (b) Fap powder (*: CaO).

656 and 770 cm⁻¹ are allotted to the group Al-O [37-40]. From the Fap one (**Figure 2(b**)), the absorption bands which appear to 468, 562, 602 and 900 - 1100 cm⁻¹ are related to phosphate group, whereas those which appear at 1642 and 3448 cm⁻¹ are assigned to the adsorbed water molecule. The absorption bands detected at 798 and 1392 cm⁻¹ are allotted respectively to HPO_4^{2-} and NO_3^{-} groups, present in the form of impurities in the initial powder [29,41,42].

However, it is not excluded that the powders contain other phases not detected by the IR radiations.

The ³¹P MAS-NMR solid spectrum of the fluorapatite powder was presented in **Figure 3(a)**. We observe only one peak which appears at 2.84 ppm (only one environment of the core phosphorus), proving the absence of secondary products accompanying the fluorapatite synthesis. The ²⁷Al MAS-NMR solid spectrum of alumina powder was presented in **Figure 3(b)**. We notice the presence of three peaks characteristic of aluminium; two first ones at 7 ppm and 13 ppm corresponding to octahedral Al sites and the other at 35 ppm which corresponds to pentahedral Al.

3.2. Thermal Characterization of the Ceramic Powders and the Al₂O₃-26.5 wt% Fap Composites

A thermal behaviour study of the initial powders and the composite has proved to be a powerful technique for un-



Figure 2. IR spectra of: (a) Al₂O₃ powder; (b) fluorapatite powder.

derstanding physical phenomena during the sintering. The dilatometric analysis and the differential thermal analysis were used. Dilatometric analysis was performed at 1500°C. The analysis of the alumina powder shows a light expansion followed by an even weaker contraction (Figure 4(a)). The dilatometric measurements of alumina powder showed that shrinkage was not begun even at 1400°C. For the Fap powder, the shrinkage began at 950°C and continued to 1200°C (Figure 4(b)). The optimum sintering temperature of this powder is around 1030°C. Above 1200°C, a slight expansion takes place, which is probably due to the formation of a liquid phase. The addition of 26.5 wt% Fap in the matrix of alumina reduces the shrinkage beginning temperature of about 400°C in comparison with pure alumina (Figure 4(c)). Therefore, the presence of alumina delays the sintering of the Fap. Moreover, we notice the presence of samples retractions of about 10%, indicating the composite densification.

The alumina powder, presents an endothermic peak in the DTA curve (**Figure 5(a)**), the peak around 1051°C probably marks the elimination of impurities potentially present in the commercial powder (commercial Al_2O_3 powder contain approximately 2 wt% of impurity not detected by XRD analysis). Typical DTA curve of Fap powder illustrates two endothermic peaks (**Figure 5(b**)).



Figure 3. ³¹P NMR spectrum of fluorapatite powder and ²⁷Al NMR spectrum of α -alumina powder.

The first is located at 180°C, corresponding to the poder dehydration. The second appearing at 1192°C, probably attributed to the formation of a liquid phase, which is formed from binary eutectic between CaF_2 and Fap [28,29]. For the composite powder DTA, the curve presents the same transitions, but the second arises at higher temperature (1064°C) probably due to the presence of the Fap (**Figure 5(c)**). In addition, we remark the absence of the peak around 1192°C attributed to the liquid phase formation in Fap powder. This absence is probably due to the inhibiting effect of alumina on the mixture.

After thermal analysis, we can notice that alumina was not yet sintered at 1500°C. The addition of Fap powder lets the mixture sinter from a temperature about 1010°C. So, an optimisation of sintering conditions is required to elaborate alumina-Fap composites.

3.3. Sintering and Characterization of the Al₂O₃ -26.5 wt% Fap Composites

3.3.1. Sintering of the Composites

Figure 6(a) shows the mechanical properties of the Al_2O_3 -26.5 wt% Fap composites samples according to the sintering temperature. The rupture strength of sintered



Figure 4. Linear shrinkage versus temperature of: (a) Al₂O₃; (b) Fap; (c) Al₂O₃-Fap composite powders.



Figure 5. DTA curves of: (a) Al_2O_3 ; (b) Fap; (c) Fap- Al_2O_3 composite.

composites was slightly improved up to 1300° C. Above this temperature, it suddenly increases to reach its maximum value at 1600° C (21.7 MPa). This can be attributed to the improvement in the density of sintered composites. So, the relative density passes from 60% at 1300° C to 85% at 1600° C.

The results of the mechanical properties according to the sintering temperature are confirmed by the porosity measurements. Indeed, the apparent porosity remains constant until a temperature of about 1300° C and than decreases with the increase of sintering temperature (**Figure 6(b)**). The minimum of apparent porosity reaches 14% at 1600°C.

In order to lower the sintering temperature while guarding the mechanical properties, other experiments were carried out on some samples fired at 1500° C at various holding times (from 30 minutes to 7 hours). Figure 7(a) shows the mechanical properties evolution of Al₂O₃-26.5 wt% Fap composites versus the holding time. For 5 hours, the rupture strength reaches its maximum value of 26.4 MPa. For longer holding times, the rupture strength decreases abruptly. Those evolutions of mechanical properties can be explained by apparent porosity results (Figure 7(b)). This curve illustrates a minimum



Figure 6. Mechanical resistance and total porosity versus temperature of Al_2O_3 -Fap composites sintered for 1h.



Figure 7. Mechanical resistance and total porosity versus holding time of Al₂O₃-Fap composites sintered at 1500°C.

apparent porosity at about 15% corresponding to the highest rupture strength.

The whole results obtained show that it is possible to obtain a Fap-Al₂O₃ composite well densified. The adopted sintering temperatures and durations are closer to the sintering conditions of the alumina than the fluorapatite ones. Indeed, Fap presents a good aptitude for sintering in the temperature range 900°C - 1100°C during one hour [17,29,30,43]. Whereas the alumina sintering is carried out in the temperatures range between 1400 and 1750°C [44-51]. The thermal study carried out on the Al₂O₃-26.5 wt% Fap composite proved that mixing Al₂O₃ and Fap decreases the temperature of the sintering beginning compared to pure alumina. Indeed, it decreases from a temperature above 1400°C to 1030°C. Moreover, we notice that the alumina inhibits the Fap decomposition and the liquid phase formation revealed in the sintering of pure Fap. Further, the mechanical resistance of Fap-Al₂O₃ composites showed a higher value than that of pure Fap. F. Ben Aved et al and N. Bouslama et al reported that the mechanical resistance of Fap and TCP-Fap ceramics was about 14 MPa and 9.4 MPa, respectively [52,53].

Sintering was driven by many parameters and phe-

nomena. In fact, when powders have different grain size and chemical nature, much driving force and phenomena will appear. The difference of fusion temperatures and densification start of different departure powders conduce to the fluctuation of the sintering process results. All those phenomena will modify the mechanical resistance and the densities of specimens [43].

3.3.2. Characterization of SinteredSamples

After sintering process, the samples have been subjected to various characterization techniques such as the x-ray diffraction (XRD), infrared spectroscopy (IR), ³¹P and ²⁷Al magic angle spinning nuclear magnetic resonance (MAS-NMR) and scanning electronic microscopy (SEM).

The X-ray diffraction patterns of Al_2O_3 -Fap composites sintered at various temperatures (from 1300°C to 1600°C) during one hour were shown in **Figure 8**. The XRD pattern of samples sintered at 1300°C shows the presence of Al_2O_3 and Fap (**Figure 8a**). All the diffraction peaks correspond to the mixture of alumina and Fap. Those spectra are identical to those of initial mixed powders. The XRD patterns of samples sintered at 1400°C,



Figure 8. XRD spectrums of Al₂O₃-Fap composites sintered at various temperatures for 1 h: (a) 1300°C; (b) 1400°C; (c) 1500°C; (d) 1600°C (*: Ca₂Al₂O₅; CaAl₁₂O₁₉).

1500°C and 1600°C show in more the presence of two new phases which are probably attributed to $Ca_2Al_2O_5$ and $CaAl_{12}O_{19}$ (Figures 8(b)-(d)).

In earlier studies, many calcium aluminates phases were produced at high temperature by decomposition of Hap or Fap into CaO and Ca₃(PO₄)₂ and then reacted with alumina to form calcium aluminates [54-56]. This decomposition is demonstrated by a relative decrease of Fap peaks intensity [54]. For our composite, the Fap peaks intensity is steady during the sintering process even at high temperature. So, we can conclude that our Fap was not decomposed and the calcium aluminates formation is probably produced by solid reactions between CaO (as impurity) and Al₂O₃, which is explained as follows [57]:

$$CaO + 6Al_2O_3 \rightarrow CaAl_{12}O_{19}$$
(4)

$$2CaO + Al_2O_3 \rightarrow Ca_2Al_2O_5$$
 (5)

The peaks relative to the new calcium aluminates formed have a low intensity relative to their low amount. In addition, sintering time has not any influence on the composition of the samples. This interpretation is illustrated in **Figure 9**.

Figure 10 and **Figure 11** illustrate the FT-IR spectroscopic analysis; it is performed for composite samples sintered at various temperatures and for various sintering times. A comparison of spectra for various sintering temperatures allows an understanding of the composite structural evolution. Below 1400°C, the vibrational spectrum is not modified. This indicates that the local structure is not modified. Indeed, most bands were characteristic of phosphate (940-1076 cm⁻¹) and of Al-O group of alumina (418-752 cm⁻¹). For higher temperature, a novel band arises at 948cm⁻¹ and becomes well-defined at 1600°C [58]. This band is probably attributed to either the Al-O stretching or bending regions of aluminium in tetrahedral sites. This clearly indicates the formation of the calcium aluminates, as demonstrated by X-ray analysis.

The ³¹P MAS-NMR spectra of Al_2O_3 -26.5 wt% Fap composites sintered for 1h at various temperatures (1300°C, 1400°C, 1500°C and 1600°C) and others sintered at 1500°C for various holding times (1h, 2h, 3h, 4h, 5h and 6h) were presented in **Figure 12(i)** and **Figure 12(ii)** respectively. The spectra show an intense peak at 2.86 ppm and 2.88 ppm respectively related to the phosphorus of Fap. These results prove that the local environment of the phosphorus atoms hasn't changed during the sintering process. Thus, Fap structure was conserved.

Figure 13 show the ²⁷Al MAS-NMR spectra collected for Al₂O₃-26.5 wt% Fap green composites and others sintered for 1h at various temperatures (1300°C, 1400°C, 1500°C and 1600°C). For unsintered Al₂O₃-Fap composites (**Figure 13(a**)), the aluminium is primarily in pentahedral and in octahedral sites. For sintered ones (**Figure 13**



Figure 9. XRD spectrums of Al_2O_3 -Fap composites sintered at 1500°C for: (a) 1 h; (b) 3 h; (c) 5 h; (d) 6 h (*: $Ca_2Al_2O_5$; $CaAl_{12}O_{19}$).

(b)-(e)) the spectra consist of signals of three aluminium environment: that for AlO₄ at about 70 ppm, that for AIO_5 at about 30 ppm and 40 ppm and that for AIO_6 at about 8 ppm and 16 ppm. The intensity of tetrahedral signal is very low compared with that of both pentahedral and octahedral signals. The estimated concentrations of AIO_4 , AIO_5 and AIO_6 are reported in **Table 2**. In heated samples, when the sintering temperature increases, the fraction of both the tetrahedral and pentahedral sites increases at the expense of octahedral sites. In other words, the aluminium in octahedral symmetry is forced into tetrahedral and pentahedral sites. According to these results, sintering of Al₂O₃-Fap composites provoke the structural rearrangement of the aluminium coordination. A similar result was proved by G. Del Angel et al [59]. Indeed, they show that, in presence of lanthanum, the aluminium in octahedral symmetry is forced into tetrahedral sites.

The structural rearrangement of the aluminium coordination is also probably produced by the calcium aluminates formation which is detected by the XRD analysis. In fact, these two products contain aluminium in tetrahedral sites [60,61].

The SEM examination of the fracture surface of the



4000 3600 3200 2800 2400 2000 1600 1200 800 400 1100 1000 900 Wavenumber (cm⁻¹) Wavenumber (cm⁻¹)

Figure 10. FTIR spectra of Al₂O₃-Fap composites sintered at various temperatures for 1 h: (a) 1300°C; (b) 1400°C; (c) 1500°C; (d) 1600°C.

Al₂O₃-Fap composites sintered at various temperatures (1300°C, 1400°C, 1500°C and 1600°C) for one hour was reported in Figure 14. The fracture surface reveals a distinct difference in the samples microstructure. At 1300°C, the sample presents an important intergranular porosity which disappears partially when temperature increases (Figures 14(a)-(d)). In addition, we notice the presence of two grain size ranges: grains which have an average size $3 \mu m$ relative to alumina phases and the others which have an average size about 10 µm relative to Fap phases. Above 1600°C, the microstructure was completely transformed. So, grains went through the stage of partial coalescence, and then a continuous phase was developed with the sintering temperature increase and especially at 1600°C. A dense bioceramic was clearly formed: dense contacts between the grains and well-formed grain boundary zone.

The micrograph investigation realised for various holding times shows that samples fired during 1 hour until 5 hours present an improvement of structure by a partial disappearance of porosity which reaches its maximum during 5 hours (Figure 15(b)). For a holding time about 6 hours, micrograph shows a reappearance of inter and intragranular porosity which is caused by an exaggerated grain growth and probably by impurities



Figure 11. FTIR spectra of Al_2O_3 -Fap composites sintered at 1500°C for: (a) 1 h; (b) 3 h; (c) 5 h; (d) 6 h.



Figure 12. ³¹P NMR spectra of Al_2O_3 -Fap composites (i) sintered at different temperatures for 1 h; (ii) sintered at 1500°C for different holding times.



Figure 13. 27 Al NMR spectra of (a) unfired Al₂O₃-Fap composites; (b) sintered at 1300°C; (c) at 1400°C; (d) at 1500°C; (e) at 1600°C.

volatilisation. These observations are a confirmation of mechanical properties and porosity.

It has been shown in the present work that a fluoride dental implant was elaborated and then characterized. Optimum conditions of sintering were obtained. Unfor tunately, the rupture strength of our bioceramic does not exceed a value of about 26.4 MPa as compared to 500



Figure 14. SEM micrographs of Al2O3-Fap composites sintered at various temperatures for 1 h: (a) 1300°C; (b) 1400°C; (c) 1500°C; (d) 1600°C.

Table 2. Observed proportions of AlO₄, AlO₅, AlO₆ in Al₂O₃ -26.5 wt% Fap composites sintered at different temperature for 1h.

T° (°C)	AlO_4	AlO ₅	AlO_6
1300	0.09	21.49	78.42
1400	0.11	21.79	78.09
1500	0.13	22.94	76.95
1600	0.30	24.42	75.29



Figure 15. SEM micrographs of Al₂O₃-Fap composites sintered at 1500°C for: (a) 1 h; (b) 5 h; (c) 6 h.

MPa for dental enamel. However, with comparison to the other bioceramics, such as Hydroxyapatite, fluorapatite or tricalcium phosphate [16,17,54], our bioceramic presents higher mechanical properties with an important porosity. And compared to alumina, properties are lower, but the elaboration was performed at lower temperature. As a prospect, microstructure improvement of our composite can be realised by the addition of sintering agents, like CaO, TiO₂, which react at the alumina-Fap interface, so they increase the bending forces, or by the utilisation of physical inert reinforcement such as glass or carbon nanofibers.

4. Conclusions

In order to imitate its higher stability and better densification and mechanical properties, alumina was used. But its manufacturing reclaims a very high sintering temperature. Fap also presents a good sinterability, an excellent biocompatibility and direct bond formation with adjacent hard tissue. A marriage of both materials was developed, and a new material was successfully elaborated for the dental replacement. Physical and mechanical properties were studied, as well as structural characteristics. The following results were obtained.

(1) Dilatometric curve of alumina indicates that the powder was not sintered, even if we reach a temperature about 1500°C. However, for Fap and composite the specimens were sintered. So Fap addition decreases the sintering temperature of alumina.

(2) A better densification of the composite was reached for a sintering temperature of about 1600°C for 1 hour holding time and with rupture strength near to 22 MPa.

(3) An improvement of the rupture strength above 26 MPa, with guarding the same density, was obtained by decreasing the temperature of 100°C (became 1500°C), but for a holding time about 5 hours.

(4) The presence of CaO, in synthesized Fap, improves the mechanical resistance by formation of the calcium aluminates.

From the last notification, an improvement of densification and mechanical properties of our composite can be reached by adding an adequate proportion of CaO as a sintering agent or reinforcing the structure with inert fibers. This work is currently underway.

5. References

- [1] L. L. Hench, "Bioceramics," Journal of the American Ceramic Society, Vol. 81, No.7, 1998, pp. 1705-1728.
- [2] A. Clifford and R. Hill, "Apatite-Mullite Glass-Ceramics," *Journal of Non-Crystalline Solids*, Vol. 19, No. 6, 1996, pp. 346-351. doi:10.1016/0022-3093(95)00611-7
- [3] L. L. Hench, "Bioceramics," *Journal of the American Cramic Society*, Vol. 81, No. 7, 1998, pp. 1705-1728.
- [4] S. M. Best, A. E. Porter, E. S. Thian and J. Huang, "Bioceramics: Past, Present and for the Future," *Journal of European Ceramic Society*, Vol. 28, 2008, pp. 1319-1327. doi:10.1016/j.jeurceramsoc.2007.12.001
- [5] L. M. Rodriguez-Lorenzo, J. N. Hart and K. A. Gross, "Influence of Fluorine in the Synthesis of Apatites. Synthesis of Solid Solutions of Hydroxyl-Fluorapatite," *Biomaterials*, Vol.24, 2003, pp. 3777-3785. doi:10.1016/S0142-9612(03)00259-X
- [6] S. M. Barinova, L. I. Shvorneva, D. Ferro, I. V. Fadeeva and S. V. Tumano, "Solid Solution Formation at the Sintering of Hydroxyapatite-Fluorapatite Ceramics," *Science* and Technology of Advanced Materials, Vol. 5, 2004, pp. 537-541. doi:10.1016/j.stam.2004.02.012
- [7] M. J. Larsen and A. Thorson, "A Comparaison of Some Effects of Fluoride on Apatite Formation *in Vitro* and *in Vivo*," *Calcified Tissue International*, Vol. 36, No. 6, 1984, pp. 690-696. doi:10.1007/BF02405391
- [8] L. Gineste, M. Gineste, X. Ranz, A. Ellefterion, A. Guilhem, N. Rouquet and P. Frayssinet, "Degradation of Hydroxylapatite, Fluorapatite and Fluorhydroxyapatite Coatings of Dental Implants in Dogs," *Journal of Biomedical Materials Research*, Vol. 48, No. 3, 1999, pp. 224-234. doi:10.1002/(SICI)1097-4636(1999)48:3<224::AID-JBM 5>3.0.CO:2-A
- [9] B. H. Yoon, H. W. Kim, S. H. Lee, C. J. Bae, Y. H. Koh,Y. M. Kong and H. E. Kim, "Stability and Cellular Responses to Fluorapatite-Collagen Composites," *Biomaterials*, Vol. 26, 2005, pp. 2957-2963. doi:10.1016/j.biomaterials.2004.07.062
- [10] K. A. Gross and K. A. Bhadang, "Sintered Hydroxyfluorapatite. Part III: Sintering and Resultant Mechanical Properties of Sintered Blends of Hydroxyapatite and Fluorapatite," *Biomaterials*, Vol. 25, 2004, pp. 1395-1405. doi:10.1016/j.biomaterials.2003.08.051
- [11] S. V. Dorozhkin, "Bioceramics of Calcium Orthophosphates," *Biomaterials*, Vol. 31, 2010, pp. 1465-1485. doi:10.1016/j.biomaterials.2009.11.050

- [12] M. Fulmer and P. W. Brown, "Low-Temperature Formation of Fluorapatite in Aqueous Solution," *Journal of the American Ceramic Society*, Vol.75, No.12 1992, pp. 401-407.
- [13] P. Uwe, E. Angela and R. Christian, "A Pyrolytic Route for the Formation of Hydroxyapatite-Fluorapatite Solid Solutions," *Journal of Materials Science, Material Medical*, Vol. 4, No. 3, 1993, pp. 292-295.
- [14] J. C. Elliott, "Structure and Chemistry of the Apatite and Other Calcium Orthophosphates," Elsevier Science., Amsterdam, 1994.
- [15] E. D. Franz and R. Telle, "Reaction Hot Pressing of Fluorapatite for Dental Implants," In: P. Vincenzini, Ed., Hight Tech Ceramics, Elsevier Science, Amsterdam, 1987, pp. 31-41.
- [16] E. Landi, A. Tampieri, G. Celotti and S. Sprio, "Densification Behaviour and Mechanisms of Synthetic Hydroxyapatites," Journal of European Ceramic Society, Vol. 20, 2000, pp. 2377-2387. doi:10.1016/S0955-2219(00)00154-0
- [17] F. Ben Ayed, J. Bouaziz and K. Bouzouita, "Résistance Mécanique de la Fluorapatite," *Annales de Chimie-Science des Materiaux*, Vol. 31, No. 4, 2006, pp. 393-406. doi:10.3166/acsm.31.393-406
- [18] S. Agathopoulos, D. U. Tulyaganov, P. A. A. P. Marques, M. C. Ferro, M. H. V. Fernandes and R. N. Correia, "The Fluorapatite-Anorthite System in Biomedicine," *Biomaterials*, Vol. 24, 2003, pp. 1317-1331. doi:10.1016/S0142-9612(02)00468-4
- [19] K. A. Gross and L. M. Rodriguez-Lorenzo, "Biodegradable Composite Scaffolds with an Interconnected Spherical Network for Bone Tissue Engineering," *Biomaterials*, Vol. 25, 2004, pp. 4955-4962. doi:10.1016/j.biomaterials.2004.01.046
- [20] A. Rapacz-Kmita, A. Slosarczyk and Z. Paszkiewicz, "Mechanical Properties of Hap-ZrO₂ Composites," *Journal of European Ceramic Society*, Vol. 26, 2006, pp. 1481-1488. doi:10.1016/j.jeurceramsoc.2005.01.059
- [21] W. Zhenjun, H. Liping and Z. Chen, "Composite Biocoating of Hydroxyapatite/Al₂O₃ on Titanium Formed by Al Anodization and Electrodeposition," *Materials Letters*, Vol. 61, 2007, pp. 2952-2955. doi:10.1016/j.matlet.2006.10.050
- [22] B. Viswanath and N. Ravishankar, "Interfacial Reactions in Hydroxyapatite/Alumina Nanocomposites," *Scripta Materialia*, Vol. 55, 2006, pp. 863-866. doi:10.1016/j.scriptamat.2006.07.049
- [23] B. T. Lee, C. W. Lee, A. K. Gain and H. Y. Song, "Microstructures and Material Properties of Fibrous Hap/ Al₂O₃-ZrO₂ Composites Fabricated by Multi-Pass Extrusion Process," *Journal of European Ceramic Society*, Vol. 27, 2007, pp. 157-163. doi:10.1016/j.jeurceramsoc.2006.02.038
- [24] J. M. Ten Cate and J. D. B. Featherstone, "Mechanistic Aspects of the Interaction between Fluoride and Dental Enamel," *Critical Reviews in Oral Biology and Medicine*, Vol. 2, 1991, pp. 283-296.

- [25] C. L. Deal, "Osteoporosis: Prevention, Diagnosis, and Management," *American Journal of Medicine*, Vol. 102, No. 1A (Supplement), 1997, pp. 35S-9S. doi:10.1016/S0002-9343(97)00415-4
- [26] F. Menaa, B. Menaa and O. Sharts, "Fluoro-Raman Spectroscopy as New Analytical Tool for Pharmaceutical and Biomedical Applications," *Faraday Discussions*, Vol. 149, 2011, pp. 269-278. doi:10.1039/c005252c
- [27] L. L. Demos, H. Kazada, F. M. Cicuttini, M. I. Sinclair and C. K. Fairly, "Water Fluoridation, Osteoporosis, Fractures— Recent Developments," *Australian Dental Journal*, Vol. 46, No. 2, 2001, pp. 80-87. doi:10.1111/j.1834-7819.2001.tb00561.x
- [28] F. Ben Ayed, J. Bouaziz and K. Bouzouita, "Pressureless Sintering of Fluorapatite under Oxygen Atmosphere," *Journal of European Ceramic Society*, Vol. 20, No. 8, 2000, pp. 1069-1067. doi:10.1016/S0955-2219(99)00272-1
- [29] F. Ben Ayed, J. Bouaziz and K. Bouzouita, "Calcination and Sintering of Fluorapatite under Argon Atmosphere," *Journal of Alloys and Compounds*, Vol. 322, No.1-2, 2001, pp. 238-245. doi:10.1016/S0925-8388(01)01200-2
- [30] J. C. Heughebaert, "Contribution à L'Étude de L'Évolution des Orthophosphates de Calcium Précipités en Orthophosphates Apatitiques," *Thèse*, INP, Toulouse, 1977.
- [31] G. E. Cootea, R. J. Sparksa and P. Blattnerb, "Nuclear Microprobe Measurement of Fluorine Concentration Profiles, with Application in Archaeology and Geology," *Nuclear Instruments Methods*, Vol. 197, 1982, pp. 213-221. doi:10.1016/0167-5087(82)90139-9
- [32] S. Brunauer, P. H. Emmet and J. Teller, "Absorption of Gases in Multimolecular Layers," *Journal of the American Chemical Society*, Vol. 60, 1938, pp. 310-319. doi:10.1021/ja01269a023
- [33] R. Z. Legeros, "Crystallography Studies of the Carbonate Substitution in the Apatite Structure," PhD thesis, New York University, New York, 1967.
- [34] N. Senamaud, D. Bemache-Assollant, E. Champion, M. Heughebaertb and C. Reyb, "Calcination and Sintering of Hydroxyfluorapatite Powders," *Solid State Ionics*. 101-103, 1997, pp. 1357-1362. doi:10.1016/S0167-2738(97)00242-7
- [35] S. Kim, Y. M. Kong, I. S. Lee and H. E. Kim, "Effect of Calcinations of Starting Powder on Mechanical Properties of Hydroxyapatite-Alumina Bioceramic Composite," *Journal of Materials Science: Material Medical*, Vol. 13, 2002, pp. 307-310. doi:10.1023/A:1014019103240
- [36] D. Santhiya, S. Subramanian, K. A. Natarajan and S. G. Malghan, "Surface Chemical Studies on Alumina Suspensions Using Ammonium Poly(Methacrylate)," *Colloids and Surfaces A: Physicochemical and Engineering Aspects*, Vol. 164, 2000, pp. 143-154. doi:10.1016/S0927-7757(99)00347-7
- [37] Y. Chen, S. Liu and G. Wang, "Kinetics and Adsorption Behavior of Carboxymethyl Starch on A-Alumina in Aqueous Medium," *Journal of Colloid and Interface Science*, Vol. 303, 2006, pp. 380-387.

doi:10.1016/j.jcis.2006.08.011

- [38] A. Boumaza, L. Favaro, J. Lédion, G. Sattonnay, J. B. Brubach, P.Berthet, A. M. Huntz, P. Roy and R. Tétot, "Transition Alumina Phases Induced by Heat Treatment of Boehmite: An X-Ray Diffraction and Infrared Spectroscopy Study," *Journal of Solid State Chemistry*, Vol. 182, 2009, pp. 1171-1176. doi:10.1016/j.jssc.2009.02.006
- [39] K. A. Bhadang and K. A. Gross, "Influence of Fluorapatite on the Properties of Thermally Sprayed Hydroxyapatite Coatings," *Biomaterials*, Vol. 25, 2004, pp. 4935-4945. doi:10.1016/j.biomaterials.2004.02.043
- [40] M. Hidouri, K. Bouzouita, F. Kooli and I. Khattech, "Thermal Behaviour of Magnesium-Containing Fluorapatite," *Materials Chemistry and Physics*, Vol. 80, No. 2003, pp. 496-505. doi:10.1016/S0254-0584(02)00553-9
- [41] M. Hidouri, K. Bouzouita, A. Aissa and M. Debbabi, "Étude Structurale des Fluorapatites Contenant du Magnésium en Substitution," *Comptes Rendus Chimie*, Vol. 7, 2004, pp. 699-705. doi:10.1016/j.crci.2004.04.003
- [42] K. Chaari, F. Ben Ayed, J. Bouaziz and K. Bouzouita, "Elaboration and Characterization of Fluorapatite Ceramic with Controlled Porosity," *Materials Chemistry* and Physics, Vol. 113, No.1, 2009, pp. 219-226. doi:10.1016/j.matchemphys.2008.07.079
- [43] Z. He and J. Ma, "Constitutive Modeling of Alumina Sintering: Grain-Size Effect on Dominant Densification Mechanism," *Computational Materials Science*, Vol. 32, 2005, pp. 196-202. doi:10.1016/j.commatsci.2004.08.006
- [44] J. F. Roy, M. Descemond, C. Brodhag and F. Thevenot, "Alumina Microstructural Behaviour under Pressureless Sintering and Hot-Pressing," *Journal of European Ceramic Society*, Vol. 11, 1993, pp. 325-333. doi:10.1016/0955-2219(93)90032-M
- [45] P. Quirmbach, M. Wolf and R. J. Brook, "Development of Microstructure during Pressureless Sintering of Alumina," *Journal of European Ceramic Society*, Vol. 10, 1992, pp. 51-57. doi:10.1016/0955-2219(92)90118-W
- [46] M. Azar, P. Palmero, M. Lombardi, V. Garnier, L. Montanaro, G. Fantozzi and J. Chevalier, "Effect of Initial Particle Packing on the Sintering of Nanostructured Transition Alumina," *Journal of European Ceramic Society*, Vol. 28 2008, pp. 1121-1128. doi:10.1016/j.jeurceramsoc.2007.10.003
- [47] H. Fischer, R. Weiß and R. Telle, "Crack Healing in Alumina Bioceramics," *Dental Materials*, Vol. 24, 2008, pp. 328-332.
- [48] X. Teng, H. Liu and Ch. Huang, "Effect of Al₂O₃ Particle size on the Mechanical Properties of Alumina-Based Ceramics," *Materials Science and Engineering: A*, Vol. 452-453, 2007, pp. 773-780. doi:10.1016/j.msea.2006.10.073
- [49] H. M. Lee, C. Y. Huang and C. J. Wang, "Forming and Sintering Behaviors of Commercial α-Al₂O₃ Powders with Different Particle Size Distribution and Agglomeration," *Journal of Materials Processing Technology*, Vol. 209, No. 2, 2009, pp. 714-722. doi:10.1016/j.jmatprotec.2008.02.047

Copyright © 2011 SciRes.

112

- [50] N. Louet, H. Reveron and G. Fantozzi, "Sintering Behaviour and Microstructural Evolution of Ultrapure A-Alumina Containing Low Amounts of SiO₂," *Journal* of European Ceramic Society, Vol. 28, 2008, pp. 205-215. doi:10.1016/j.jeurceramsoc.2007.04.015
- [51] F. Ben Ayed, "Frittage Et Caractérisation de la Fluorapatite," Faculté des Sciences de Sfax, 2003.
- [52] N. Bouslama, F. Ben Ayed and J. Bouaziz, "Sintering and Mechanical Properties of Tricalcium Phosphate-Fluorapatie Composites," *Ceramics International*, Vol. 35, 2009, pp. 1909-1917. doi:10.1016/j.ceramint.2008.10.030
- [53] F. Ben Ayed and J. Bouaziz, "Sintering of Tricalcium Phosphate-Fluorapatite Composites by Addition of Alumina," *Ceramics International*, Vol. 34, 2008, pp. 1885-1892. doi:10.1016/j.ceramint.2007.07.017
- [54] H. Ji and P. M. Marquis, "Sintering Behaviour of Hydroxyapatite Reinforced with 20 wt% Al₂O₃," *Journal of Materials Science*, Vol. 28, 1993, pp. 1941-1945. doi:10.1007/BF00595767
- [55] H.Y. Juang and M.H. Hon, "Fabrication and Mechanical Properties of Hydroxyapatite-Alumina Composites," *Material Science and Engineering*, Vol. 12, 1994, pp. 77-81. doi:10.1016/0928-4931(94),90033-7
- [56] D. Asmi, I. M. Low, B. H. O'Connor and C. Buckley, "Phase Compositions and Depth Profiling of Calcium Aluminates in a Functionally-Graded Alumina/Calcium-

Hex-aluminate Composite," *Journal of Materials Proc*essing Technology, Vol. 118, 2001, pp. 219-224. doi:10.1016/S0924-0136(01)00963-3

- [57] A. Gutiérrez-Alejandre, M. Gonzalez-Crus, M. Trombetta, G. Busca and J. Ramirez, "Chracterisation of Alumina-Titania Mixed Oxide Supports, Part II: Al₂O₃-Based Supports," *Microp. Mesop. Mat.*, Vol. 23, 1998, pp. 265-275. doi:10.1016/S1387-1811(98)00121-8
- [58] G. Del Angel, C. Guzman, A. Bonilia, G. Torres and J. M, "Padilia, Lanthanum Effect on the Structural Properties of γ-Al₂O₃ Obtained from Bohemite," *Materials Letters*, Vol. 59, 2005, pp. 499-502.
- [59] K. J. D. MacKenzie, M. SchmuÈcker, M. E. Smith, I. J. F. Poplett and T. Kemmitt, "Evolution of Crystalline Aluminates from Hybrid Gel-derived Precursors Studied by XRD and Multinuclear Solid State MAS NMR IV: Calcium Dialuminate, CaAl₄O₇ and Calcium Hexaluminate," *Thermochemical Acta*, Vol. 363, 2000, pp. 181-188. doi:10.1016/S0040-6031(00)00630-4
- [60] B. Lazic, H. Kriiger, V. Kahlenberg, J. Konzett and R. Kaindl, "Incommensurate Structure of Ca₂Al₂O₅ at High Temperature-Structure Investigation and Raman Spectroscopy," *Acta Crystallographica*, 2008, pp. 417-425.
- [61] J. M. Poujade, C. Zerbib and D. Serre, "Céramiques dentaires," *EMC-Dentisterie*, Vol. 1, 2004, pp. 101-117. doi:10.1016/j.emcden.2003.11.002