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8	Electrochemical Characterization of					
9	Commercial and Home-Made					
10	Screen-Printed Carbon Flactrodes					
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13	Agifa Marrin Anthony I Killard * and Malaalm D. Smyth					
14	Aone worth, Anthony 5. Amaru, and walconn A. Shiyu					
15	National Centre for Sensor Research					
16	School of Chemical Sciences.					
17	Dublin City University, Dublin, Ireland					
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21	ABSTRACT					
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23	Screen-printing technology is widely used for the mass-production of					
24 25	disposable electrochemical sensors. The practical utility of carbon					
20	screen-printed electrodes has been exploited, despite the fact that					
20	little is known about the nature of the electrode reactions. (Wang L: Pedrero M: Sakslund H: Hammerich O: Pingarron L					
28	(wang, J.; Pedrero, M.; Saksiuma, H.; Hammerich, O.; Pingarron, J. Electrochemical activation of screenprinted carbon strips. The					
29	Analyst 1996 121 (3) 345–350) Given the complexity of carbon					
30	electrodes in general, and differences in the composition of commer-					
31	cial carbon inks, the question arises as to how such differences and					
32	complexity affect their electrochemical reactivity. The aim of this					
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35 36 37 38	*Correspondence: Anthony J. Killard, National Centre for Sensor Research, A School of Chemical Sciences, Dublin City University, Dublin 9, Ireland; Fax: 353 1 700 5703; E-mail: Tony.Killard@dcu.ie.					
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work was to compare the electroactivity of both commercial electrodes and electrodes fabricated in-house from various commercial inks, in order to find the electrode most suited to amperometric sensor work. Methods of analysis include cyclic voltammetry, amperometry and linear sweep voltammetry. It was found that the commercial working electrodes were not suited to the high current work of interest, due to their poor charge transfer properties. The in-house electrode had less resistive properties, and was more suited for high current amperometric sensing. Utilizing this electrode configuration, an optimal carbon paste was chosen for the working electrode.

Key Words: Screen-printed electrode; Cyclic voltammetry; Linear sweep voltammetry; Amperometry; Charge transfer.

INTRODUCTION

Carbon electrodes are particularly attractive for sensing applications. 61 These materials have a high chemical inertness and provide a wide range 62 of anodic working potentials with low electrical resistivity. They also 63 have a very pure crystalline structure that provides low residual currents 64 and a high signal to noise ratio.^[2] Many of the devices reported rely on 65 the use of carbon materials such as glassy carbon,^[3] and carbon pastes.^[4] 66 Screen printing of the carbon ink for the fabrication of electrodes has 67 realized commercial success in the glucose sensing field.^[5] Developed for 68 the printing industry, this thick-film technology has been adapted for the 69 electronics industries and biosensor research. Screen-printed electrodes 70 71 have low unit costs and are capable of undergoing mass production, while still maintaining adequate levels of reproducibility. They also 72 have the advantages of miniaturization and versatility. 73

Carbon ink used for working electrodes must contain a binder, sol-74 75 vent, and graphite particles. What is still of some concern with screenprinting, is the level of reproducibility in electrode production. This is 76 mainly due to the nature of the carbon inks-the composition of which are 77 proprietary-and the lack of control of the microscopic structure of indi-78 vidual electrodes. Grennan et al.^[6] investigated the effects of the curing 79 temperature on the physical and electrochemical characteristics of carbon 80 paste C10903D14 (Gwent Electronic Materials). Improved sensor perfor-81 mance and decreased variability was demonstrated at elevated curing 82 temperatures and this was associated with morphological changes to 83 the carbon electrode surface. Wang et al.^[7] compared the electrochemical 84

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behavior and electroanalytical performance of thick film carbon sensors 85 on ceramic substrates fabricated from four different commercially 86 87 available carbon inks. They found that C10903D14 (Gwent Electronic Materials) was optimal for amperometric sensing. This ink possessed an 88 89 attractive electrochemical reactivity but was found to have high residual 90 currents. This would render it most suited to amperometric work as this method is not dependent on background contributions. It would be less 91 suited, however, to voltammetric or stripping voltammetry work. 92

It is not just the interfacial region between solution and electrode that 93 94 is important in determining the electrode's characteristics, but also the 95 rest of the electrode, including the properties of the conducting path. 96 Carbon inks may have higher resistivities than other types of conducting inks and so may not be suitable as a conductive layer, e.g., for high 97 current work. Cui et al.^[8] characterized a screen-printed strip comprising 98 working, reference, and auxiliary electrodes. Silver acted as the conduct-99 ing path. Erlenkotter et al.^[9] used a similar format with on-board refer-100 101 ence and auxiliary electrodes. However, the difference was that carbon acted as the conducing path for the working and auxiliary electrodes. 102 Both strips described potentially have different charge transfer properties 103 due to their very different compositions, and although both strips were 104 105 successful for their respective applications, they may not necessarily be suited to other applications. It is important when designing any type of 106 screen-printed electrode that the charge transfer properties are suited to 107 the end-use application. 108

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EXPERIMENTAL

Materials

Horseradish peroxidase (HRP, 1100 U/mg and 1310 U/mg, P8672) 115 116 was purchased from Sigma-Aldrich (Poole, Dorset, UK). Aniline was purchased from Aldrich (13,293-4), vacuum distilled and stored frozen 117 118 under nitrogen. Thirty percent (v/v) hydrogen peroxide solution was purchased from Merck. Polyvinylsulphonate (PVS, 27,842-4), potassium 119 hexacyanoferrate(II) (22,768-4) (potassium ferrocyanide trihydrate) and 120 potassium hexacyanoferrate(III) (20,801-9) (potassium ferricyanide) 121 were purchased from Aldrich. EuroflashTM and UltraTM electrode 122 strips were donated from Inverness Medical Ltd. EuroflashTM, 123 UltraTM, Ercon (661901), and LRH (C2010201R15) carbon paste inks 124 were donated by Inverness Medical Ltd. (Inverness, Scotland). 125 LifescanTM silver conductive ink was donated by Inverness Medical 126

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2024 Morrin, Killard, and Smyth Ltd. Seriwash universal screen wash (ZT639) was obtained from Sericol 127 Ltd. (Kent, UK). Glassy carbon and silver/silver chloride (Ag/AgCl) 128 electrodes were purchased from Bioanalytical Systems Ltd. (Cheshire, 129 UK). The platinum mesh (29,809-3) was purchased from Aldrich. 130 131 132 133 **Buffers and Solutions** 134 135 Unless otherwise stated, all electrochemical measurements were car-136 ried out in phosphate buffered saline (PBS), (0.1 M phosphate, 0.137 M 137 NaCl, and 2.7 mM KCl), pH 6.8. 138 139 140 141 Instrumentation 142 143 Screen-printing of in-house (noncommercial) electrodes was 144 performed with a semi-automated DEK 248 printing machine 145 (Weymouth, UK). Nylon screens with varying mesh thickness were 146 used, and mounted at 45° to the print stroke. Blade rubber squeegees 147 were employed, and a flood blade was utilized. All inks were cured in a 148 conventional oven. 149 All electrochemical protocols were performed either on a BAS100/W 150 electrochemical analyzer with BAS100/W software, or a CHI1000 151 potentiostat with CHI1000 software, using either cyclic voltammetry or 152 time-based amperometric modes. An Ag/AgCl reference electrode and a 153 platinum mesh auxillary electrode were used for bulk electrochemical 154 experiments. 155 Scanning electron microscopy (SEM) was performed with a Hitachi 156 S 3000N scanning electron microscope. An acceleration voltage of 20 kV 157 was employed. 158 159 160 **Screen-Printed Electrode Fabrication** 161 162 Five electrode types were fabricated for this study. Two were man-163 ufactured commercially (EuroflashTM and UltraTM) and three by in-164 house screen-printing (designated Ultra-inH, Ercon-inH, and LRH-inH, 165 according to the working electrode carbon used). The structural charac-166 teristics of each of the electrodes are summarized in Table 1. The curing 167 conditions for all inks are summarized in Table 2. 168

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Screen-Printed Carbon Electrodes

	Table 1.	Summary of the composition of a	all electrodes used.		
Electrode type	Conducting layer	Working electrode layer	Working electrode area	Insulation layer	Name
Euroflash TM	Lifescan silver and Euroflash TM carbon	Euroflash TM carbon	$8\mathrm{mm}^2$	Ercon	Euroflash TM
Ultra TM	Ultra TM carbon	Ultra TM carbon	$10\mathrm{mm}^2$	"	Ultra TM
Ultra in-house	Lifescan silver	Ultra TM carbon	$9\mathrm{mm}^2$	"	Ultra-inH
Ercon in-house	Lifescan silver	Ercon 661901		"	Ercon-inH
LRH in-house	Lifescan silver	LRH C2010201R15	"	۰,	LRH-inH
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- F1 Figure 1 depicts a schematic of the in-house screen-printed electrode with onboard reference and auxiliary electrodes (Ultra-inH, Ercon-inH, and LRH-inH). Electrodes were screen-printed onto a preshrunk PET substrate (a). Initially, a layer of three Ag/AgCl tracks were deposited as the conducting paths from electrodes to contacts for the reference, auxiliary, and working electrodes (b). A layer of carbon was deposited as the working electrode (c). The Ag/AgCl acted as both reference (d) and

auxiliary (e) electrodes. Finally, an insulation layer was deposited to 211 eliminate cross-talk and to define the working electrode area (9 mm^2) (f). 212 213 214 215 **Cyclic Voltammetry** 216 Glassy carbon or screen-printed electrodes were cycled in equimolar 217 amounts of potassium ferrocyanide and potassium ferricyanide 218 $(1 \times 10^{-3} \text{ M})$ using 1 M KCl as supporting electrolyte. Voltammograms 219 were obtained using scan rates ranging from 10 to $100 \,\mathrm{mV \, s^{-1}}$ and 220 at a sensitivity of 1×10^{-3} AV⁻¹ vs. Ag/AgCl under diffusion limited 221 222 conditions. 223

Determination of Heterogeneous Electron Transfer Rate Constants

Heterogeneous electron transfer rate constants (k^0) were calculated using the method of Nicholson^[10] according to Eq. (1):

$$k^{0} = \Phi \left(D_{0} \pi v \left(\frac{nF}{RT} \right) \right)^{1/2} \left(\frac{D_{R}}{D_{0}} \right)^{\alpha/2}$$
(1)

where Φ refers to a kinetic parameter, D_0 is the diffusion coefficient for 234 the ferricyanide $(7.6 \times 10^{-6} \text{ cm}^2 \text{ s}^{-1})$, D_R is the diffusion coefficient for 235 the ferrocyanide $(6.3 \times 10^{-6} \text{ cm}^2 \text{ s}^{-1})$, and α is the transfer coefficient 236 237 (0.5), R is the universal gas constant (8.314 JK mol⁻¹), T is the absolute 238 temperature (K), n is the number of electrons transferred, and F is 239 Faraday's constant (96,485 C). Φ values for the electrode systems were calculated with the aid of a solver program that generated the sixth 240 241 polynomial plot of ΔE_p vs. log(Φ).

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Electrode Pretreatment Procedure

246 Glassy carbon electrodes were cleaned by successive polishing on aqueous slurries of 1, 0.3, and 0.05 µm alumina powder, followed 247 by ultrasonic cleaning in Milli-Q water for 10 min. The electrodes 248 were then placed in a solution of 0.2 M H₂SO₄. A single voltammetric 249 250 cycle was carried out between $-1200 \,\mathrm{mV}$ and $1500 \,\mathrm{mV}$ at $100 \,\mathrm{mVs^{-1}}$ vs. Ag/AgCl. The same voltammetric procedure was employed for cleaning 251 the screen-printed electrodes. 252

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Amperometric Electroanalytical Procedure

The electroanalytical procedure was carried out according to 255 Killard et al.^[11] 256

RESULTS AND DISCUSSION

Two commercially manufactured screen-printed working electrodes 261 (WE) were examined; EuroflashTM and One Touch UltraTM. These elec-262 trodes were manufactured by Inverness Medical Ltd., for glucose testing. 263 The WE of the EuroflashTM strip were composed of a silver and carbon 264 conducting path, a carbon working electrode and an insulation layer to 265 define the electrode area. The UltraTM WE electrode, contained only 266 carbon and insulation layers, relying on only carbon to act as the con-267 268 ductor and the electrode. The advantage of using less silver, or none at 269 all, is to allow for reduced cost manufacturing. Electrochemical analyses were initially carried out on the commercial electrodes. However, subse-270 quently the in-house artwork was designed as a result of finding that the 271 commercial electrodes suffered from severe charge transfer problems and 272 273 were not suitable to this amperometric sensor work. This in-house electrode design (Fig. 1) did not encounter charge transfer difficulties as the 274 conducting tracks were composed solely of silver. It was used for the 275 analysis of UltraTM, Ercon, and LRH inks and these electrodes are 276 referred to in this section as Ultra-inH, Ercon-inH, and LRH-inH, 277 respectively. Summaries of all inks used for fabrication and their respec-278 tive curing conditions are given in Tables 1 and 2. 279

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Voltammetric Performance of Screen-Printed Electrodes

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284 The ferri/ferrocyanide redox couple was the redox system used for comparing the voltammetric behavior of screen-printed electrodes. 285 Figure 2 displays the cyclic voltammograms of the redox couple at a F2 286 glassy carbon electrode for comparison purposes, the commercial 287 carbon strip electrodes (EuroflashTM and UltraTM) and the commercial 288 inks printed in-house (Ercon-inH, LRH-inH, and Ultra-inH). The mean 289 peak separations and anodic $(j_{p,a})$ and cathodic $(j_{p,c})$ peak current 290 densities are also illustrated in Fig. 3 (n=3). The commercial electrodes, EuroflashTM and UltraTM, yielded very poor reversibility with ΔE_p F3 291 292 values of 471 (±56) mV and 416 (±37) mV, respectively and $j_{p,a}$ values of -12.313 (±2.025) μ A cm⁻² and -15.107 (±2.638) μ A cm⁻², respectively. 293 294



Figure 2. Cyclic volatmmograms for different electodes in 1×10^{-3} M ferri/ ferrocyanide and 1 M KCl supporting electrolyte. (a) Glassy carbon, (b) EuroflashTM, (c) UltraTM, (d) Ercon-inH, (e) LRH-inH, and (f) Ultra-inH. The commercial electrodes ((b), (c)) showed very poor reversibility. Using the in-house design, ((d), (e), (f)) reversibility improved, with the Ultra-inH exhibiting the best behavior.

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329 330 This behavior was attributed to the poor charge transfer of the electrodes. 331 The conducting paths (composed of segments of silver and carbon for 332 EuroflashTM and fully carbon for UltraTM electrodes) from WEs to 333 contacts had resistive properties that may have become a significant 334 limiting factor in charge transfer. It resulted in the poor reversibility of 335 the redox couple and low $j_{p,a}$ values. This initial work motivated the in-336 house electrode artwork to be designed where the conducting tracks were

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Figure 3. (a) Cyclic voltammetric peak separations (ΔE_p) and (b) anodic and cathodic peak current densities for 1×10^{-3} M ferri/ferrocyanide and 1 M KCl for each of the screen-printed electrodes (n = 3).

353 composed solely of silver. Each in-house thick-film carbon electrode exhibited different electron-transfer reactivities towards ferri/ferro, with 354 the Ultra-inH electrode yielding the most reversible behavior. For 355 example, the redox couple gave a ΔE_p value of 264 (\pm 7) mV for Ultra-356 inH, as compared to 314 (\pm 25) mV and 562 (\pm 52) mV for Ercon-inH and 357 LRH-inH, respectively. The Ultra-inH also offered the highest j_p values 358 and lowest overvoltage of all the in-house electrodes (i.e., anodic peak 359 potentials for ferrocyanide of 392 mV, compared to 452, 460, 410, and 439 mV for UltraTM, EuroflashTM, Ercon-inH, and LRH-inH, respectively). 360 361

Of all the electrodes examined, the Ultra-inH electrode exhibited the 362 best behavior towards the redox couple. It was observed immediately that 363 364 the commercial electrodes, manufactured by Inverness Medical Ltd., 365 were not suited to present purposes because of poor charge transfer properties. The in-house design had more optimal charge transfer proper-ties, and in conjunction with the UltraTM commercial ink as the WE, 366 367 behaved as the best screen-printed electrode. This work demonstrates the 368 importance of optimizing both the conducting path and the carbon of the 369 370 WE when designing a new screen-printed electrode. Both parameters have profound effects on the behavior of the electrode. 371

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All k^0 values are given in Table 3. Recalling that for all the screenprinted electrodes the ΔE_p values were considerably greater than the 59 mV value expected for Nernstian one-electron reactions, k^0 values were then also inevitably low compared to glassy carbon. Commercial electrodes (EuroflashTM and UltraTM) exhibited k^0 values 2000-fold and 1250-fold lower than that obtained for glassy carbon, respectively. The LRH-inH electrode proved the poorest with regard to k^0 , being

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379 380	Table 3. Table of heterogeneous electron transfer constant (k^0) for glassy carbon and each of the so				
381	printed electrodes.				
382	Flectrode	$k^0 (\text{cm s}^{-1})$			
383		κ (cm s)			
384	Glassy carbon	5.9×10^{-2}			
385	Euroflash TM	2.83×10^{-5}			
386	Ultra TM	4.7×10^{-5}			
387	Ercon-inH	1.74×10^{-4}			
388	LRH-inH	1.67×10^{-5}			
389	Ultra-inH	3.09×10^{-4}			

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3500-fold lower than glassy carbon. Ercon-inH and Ultra-inH both had 392 the best k^0 values of the screen-printed electrodes, yielding k^0 values only 393 300-fold and 200-fold lower than glassy carbon, respectively. Thus, 394 Ultra-inH exhibited the best k^0 value, even if this was still two orders 395 of magnitude lower than glassy carbon. Such decreases in the electron-396 397 transfer reactivity may be consistent with the composition of the ink, being composed only partly of conductive carbon particles. In view of 398 399 the proprietary composition of all the inks, it is difficult to explain why the Ultra-inH electrode displayed the most favorable redox behavior. 400 Observed changes in redox behavior may be dictated by varying graphite 401 content (good redox behavior suggests a high graphite loading), 402 the nature of the graphite particles, and the presence or absence of an 403 adherent (inhibitory) organic layer. Further studies employing energy 404 405 dispersive x-ray analysis (EDX), and scanning electrochemical microscopy (SECM) may help to establish the relationship between carbon 406 407 content and electrode performance.

Although Ultra-inH was shown to have the best behavior of all the 408 screen-printed electrodes to ferri/ferrocyanide, its behavior was still 409 410 far from ideal. Attempts to improve its behavior (by electrochemical pretreatment and optimization of curing conditions) were carried out 411 412 and discussed in a later section.

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Amperometric Performance of Screen-Printed Electrodes

The electrochemical performance of the screen-printed electrodes 417 was investigated by incorporating them into a batch cell set-up.^[9] 418 Previous work by this group had used these types of screen-printed 419 carbon electrodes as the basis of a biosensor using electrodeposited 420



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Figure 4. Amperometric sensor responses for successive additions of 0.5 mM hydrogen peroxide to a solution containing 2 mg/mL horseradish peroxidase.
Electrodes used were (●) Ultra-inH, (□) Ercon-inH, and (▲) LRH-inH. Electrodes held at -100 mV vs. Ag/AgCl wire electrode.

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conducting PANI/PVS films onto which was deposited HRP or anti-444 bodies. The nature of these biosensors has been described elsewhere.^[11,12] 445 Briefly, PANI/PVS was deposited on the surface of the electrode and the 446 potential was cycled the required number of times. No protein was 447 448 immobilized onto the surface of the polymer. Ultra-inH, Ercon-inH, 449 and LRH-inH electrodes were subjected to successive additions of $0.5 \,\mathrm{mM}$ hydrogen peroxide added freshly to a solution of $2 \,\mathrm{mg}\,\mathrm{mL}^{-1}$ 450 451 horseradish peroxidase and the amperometric response monitored. All 452 three sensors responded to the changes in peroxide concentration (Fig. 4). Similar response times and noise levels were observed (data not shown). 453 Ultra-inH offered the highest sensitivity $(4 \mu A m M^{-1} \text{ peroxide})$, with 454 Ercon-inH exhibiting a slightly lower sensitivity $(3.2 \,\mu A \,m M^{-1} \text{ peroxide})$. 455 LRH-inH showed the poorest sensitivity $(1.8 \,\mu\text{A}\,\text{m}\text{M}^{-1}\text{ peroxide})$. 456 This correlates with the voltammetric behavior. Ultra-inH exhibited the 457 highest sensitivity in terms of j_p values while LRH-inH exhibited the 458 lowest values. 459

Amperometric experiments could not be carried out on either of the
 commercial electrodes as the charge transfer properties of the electrodes
 hindered deposition of adequate polymer. For example, the in-house

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strips required seven cycles to immobilize polymer to the required thickness, whereas the commercial electrodes needed 20 cycles in order to reach only one fifth the required thickness. The experiments on these strips were abandoned at this point.

Linear Sweep Voltammetric Performance of **Screen-Printed Electrodes**

The background current of thick-film carbon electrodes is strongly 472 affected by the carbon ink employed.^[7] Figure 5 compares the back-473 F5 474 ground voltammograms for the different carbon electrodes in degassed phosphate buffer (pH 6.8). Several electrodes of each type were analyzed 475 and Fig. 5 shows data representative of all analyses. LRH-inH exhibited 476 the widest potential window particularly with respect to the cathodic potential limit (i.e., high hydrogen overvoltage). Its potential window 479 had a range of 1150 to $-300 \,\mathrm{mV}$, where the nonfaradaic current remained constant (\approx 5.2 µA) in this electrolyte solution. The background current 480 of Ercon-inH was narrow and poor, exhibiting a lot of interference. Ultra-inH also had a narrow potential window (1097 to 60 mV) but 482 483



502 Figure 5. Linear sweep voltammograms in degassed PBS buffer (pH 6.8). 503 Electrodes used were (solid line) LRH-inH, (long dash) Ultra-inH, and (short dash) Ercon-inH. 504

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was not affected by major interferences. The non-faradaic current was of
the same magnitude as for LRH-inH. The anodic potential limits (i.e.,
oxygen overvoltage) were approximately the same for each of the inks.

A carbon ink possessing a narrow potential is not necessarily a 508 509 negative property for amperometric sensing. It should be noted that an 510 electrode of choice for fixed potential amperometric biosensors need not necessarily have the widest potential window as amperometric measure-511 ments are less affected by differences in the background contributions, as 512 they are usually performed after the decay of transient currents to steady 513 state values.^[7] However, the nonfaradaic background current measured 514 in linear sweep voltammetry, could potentially have an effect on the 515 516 sensitivity of the electrode. The background current can limit the lowest current that can be measured, and so could affect the detection 517 limits of an assay. 518

Optimization of Ultra-inH

Although Ultra-inH did exhibit the best properties of all electrodes, for the purpose of designing an electrode suited towards amperometric sensing, there were major concerns that the UltraTM ink for the WE was still not ideal. This was highlighted in the cyclic voltammetric study of ferrocyanide. Attempts to decrease the ΔE_p values were done by varying the curing temperature and length of curing time of the carbon ink, and also the effect of electrochemical pretreatment was studied.

Curing Parameters

535 Due to the composition of carbon inks, the parameters of curing can 536 have a profound effect on their performance.^[6] ΔE_p values and i_p values 537 for the ferri/ferrocyanide redox couple were monitored over a range of 538 curing temperatures and it was found that above a temperature of 70°C, 539 ΔE_p values increased greatly and the $i_{p,a}$ decreased (Fig. 6).

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Carbon inks may be composed of three basic constituents: graphite,
vinyl, or epoxy-based polymeric binders and solvent to enhance the ink's
affinity for the substrate in terms of adhesion, and to improve viscosity
for the screen-printing process. It has been suggested that increases in
curing temperature may result in evaporation of the solvent and decomposition of the polymeric binder to give a greater definition of the
graphite or carbon particles. This would mean that the increases in

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Figure 6. Mean cyclic voltammetric peak separations (n=4) (bar) and mean anodic peak currents (n=4) (line) for 1×10^{-3} M ferrocyanide and 1 M KCl for varying curing temperatures of the UltraTM ink on the Ultra-inH electrode. A curing temperature of 70°C showed optimal voltammetric performance for ΔE_p and $i_{p,a}$ values.

temperature should result in an increase in the microparticulate nature of 568 the carbon and greater definition of the graphite particle surface area.^[6] 569 According to this theory, electron transfer rates should increase as the 570 graphite particle surface area becomes increasingly defined (i.e., with 571 increasing temperature). This behavior was not observed for the Ultra 572 573 ink. Increases in temperature above 70°C resulted in reduced reaction 574 kinetics. This demonstrates that that the individual nature of the 575 ink and its unknown constituents can have a profound effect on its characteristics. The Ultra ink seemed to maintain a very defined micro-576 particulate character (Fig. 7), which was quite different from the Gwent 577 electrode.^[6] This difference in behavior could be attributed to different 578 579 solvents with different evaporation rates, different graphite particles 580 or binders or other additives, and their relative concentrations/ solubilities etc. If the viscosity of inks differ, the film thickness after a 581 582 single print will most likely also differ and may cause a difference in the electrochemical and physical characteristics. Below 70°C, ΔE_p values 583 584 were relatively constant. There were no resistive effects observed that one might expect if there was excess polymeric binder present at the 585 586 electrode surface due to curing at lower temperatures. $i_{p,a}$ values peaked at 70°C, and this temperature was chosen as optimum, as greatest 587 sensitivity was exhibited at this curing temperature. 588

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Figure 7. Typical scanning electron micrograph of the Ultra ink cured at 70° C for 13 min (2500 X magnification). The surface topography shows good definition of graphite particles.

Scanning electron microscopy (SEM) was carried out on all of these
electrodes, and no discernible differences were noted at the different
curing temperatures. Therefore, any changes in charge transfer effects
by varying the curing temperature cannot be attributed to physical
changes in the morphology of the surfaces. Figure 7 shows a typical
UltraTM ink carbon surface cured at 70°C.

615 The effect of curing time on electrode performances was monitored at a curing temperature of 70°C. Over a range of 0-20 min, there did not 616 617 appear to be any significant effect on electrode performance. ΔE_p values for ferrocyanide did not vary significantly (data not shown). This data 618 appears to suggest that curing had very little impact on the performance 619 620 of the ink at all. Even at 0 min (no curing), ΔE_p was only marginally 621 higher. This correlates with the curing temperature data in that up to 622 about 70°C, there is very little gain in electrochemical performance. Heat 623 may serve only to physically dry the constituents of the ink. This may also 624 suggest that any solvents present are extremely volatile or extremely non-volatile and ink-drying may be brought about by polymerization 625 processes rather than evaporative processes. It certainly suggests a very 626 different composition for the Ultra ink, as opposed to the Gwent ink 627 previously characterized.^[6] 628

629 Since curing temperature and time were not found to be such 630 important factors, it was decided not to deviate from the standard

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631 using conditions of 70° C for 13 min. For all future work, these curing 632 parameters would be used for the UltraTM ink.

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Electrochemical Pretreatment

Pre-treatment of working electrodes is a method employed by many 637 researchers in order to enhance the electrochemical activity of their 638 screen-printed electrodes.^[1,8,13] It is generally agreed that pretreatment 639 effectively removes organic binders and contamination that occur at elec-640 641 trode surfaces such as carbon and gold and may bring about an increase 642 in the numbers of chemically reactive sites on the electrode surface. Wang et al.^[1] employed an electrochemical pretreatment method 643 involving short preanodization (30s to 3 min in the 1.5 to 2.0 V range) 644 of screen-printed electrodes in phosphate buffer solution (0.05 M). This 645 646 pretreatment method appeared to increase the surface functionalities and roughness or to remove surface contaminants and resulted in enhanced 647 electrochemical activity. Electrochemical pretreatment of electrodes can 648 also be carried out by cycling the potential in acidic media. Gue et al.^[13] 649 simply used a chemical cleaning step with sulphuric acid and hydrogen 650 651 peroxide solution for gold microelectrodes. This step was critical for sensor sensitivity. 652

The electrochemical pretreatment method of Killard et al.^[11] has 653 been employed in this work. Cycling the screen-printed electrode in 654 sulphuric acid (0.2 M) is believed to have the effect of stripping the 655 surface of the carbon electrode. Any insulative materials present at the 656 surface may be removed. The procedure may even have the effect of 657 renewing the surface by removing the whole outer layer of the ink. To 658 assess the effect of electrode pretreatment on the UltraTM ink, the 659 electrodes were subjected to varying numbers of cycles in 0.2 M H₂SO₄, 660 and the effect of this on electrode behavior was examined by looking at 661 662 the ferri/ferro couple. By electrochemically pretreating the Ultra electrode, its behavior towards the ferri/ferrocyanide redox couple 663 improved dramatically. ΔE_p values decreased by 50%. Before 664 pretreatment, electrodes were exhibiting an average ΔE_p value of 665 222 mV (RSD=2.0%, n=9). After pretreatment, this was reduced to 666 112 mV (RSD = 3.5%, n = 9). i_p current values also increased as a 667 result. One pretreatment cycle was sufficient to observe this behavior. 668 Increasing the number of pretreatment cycles did not have a significant 669 effect. k^0 values increased from 3.09×10^{-4} cm s⁻¹ (no pretreatment) to 670 3.97×10^{-3} cm s⁻¹ (pretreated); a 10-fold improvement. These figures 671 suggest that the electrochemical pretreatment of the screen-printed 672

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electrode greatly improved their electrochemical performance. After pre treatment, the kinetics and charge transfer rates at the UltraTM electrode
 were enhanced greatly.

CONCLUSION

680 Initially, commercial screen-printed electrodes were examined with a 681 view to using them for amperometric immunosensing. It was found how-682 ever, that although the working electrodes of the strips may have been 683 suitable, the charge transfer properties of the strips were not high enough 684 for the high current work of interest. This was due to the fact that the 685 electrode surfaces and conducting paths were too resistive and hindered 686 the required current flow from the working electrode to the potentiostat. 687 A new in-house electrode was designed with a silver conducting path. The 688 charge transfer properties of the electrode were not limiting, and this 689 design was used for the electrochemical analysis of various working 690 electrode carbon inks. The inks were analyzed using voltammetry, 691 linear sweep voltammetry, and amperometry and it was found that the 692 Ultra-inH electrode had the most preferable electrochemical properties 693 (i.e., a k^0 value of 3.09×10^{-4} cm s⁻¹, and a high sensitivity in the 694 amperometric experiments). These properties were further enhanced 695 by electrochemical pretreatment rendering it the most suitable for 696 amperometric sensing. 697

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