

1 **Full Title**

2 **Essential Oil Bioactive Fibrous Membranes Prepared *Via* Coaxial Electrospinning**

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47 **ABSTRACT:**

48 A novel antimicrobial composite material was prepared by encapsulating orange
49 essential oil (OEO) in zein prolamine (ZP) *via* the coaxial electrospinning (ES)
50 technique. By manipulating process parameters, the morphological features of ZP/OEO
51 fibers were modulated. Fine fibers with diameters ranging from 0.7 to 2.3 μm were
52 obtained by regulating ZP solution concentration and process parameters during the ES
53 process. Optimal loading capacity and encapsulation efficiency of OEO in fibrous ZP
54 mats were determined to be 22.28% and 53.68%, respectively, and were achieved using
55 a 35 w/v% ZP ES solution. The encapsulation of OEO was found to be reliant on ZP
56 solution concentration (the enveloping medium). SEM analysis indicates the surface
57 morphology of ZP/OEO electrospun fibers is dependent on ZP solution loading volume,
58 with lower ZP concentrations yielding defective fibrous structures (e.g. beaded and
59 spindled-string like morphologies). Furthermore, this loading volume also influences
60 OEO loading capacity (LC), encapsulation efficiency (EE), mat water contact angle and
61 oil retention. CCK-8 assay and cell morphology assessment (HEK293T cells) indicate
62 no significant change with electrospun ZP and ZP/OEO fibrous membranes over an 8h
63 period. Antimicrobial activity assessment using *Escherichia coli*, suggests composite
64 non-wovens possess sterilization properties; elucidating potential application in active
65 food packaging, food preservation and therefore sustainability.

66 **Keywords:**

67 zein prolamine; orange essential oil; food packaging; coaxial electrospinning.

68

69

70 **Abbreviations:**

ZP	Zein Prolamine
EO	Essential Oil
OEO	Orange Essential Oil
ES	Electrospinning
OM	Optical Microscopy
SEM	Scanning Electron Microscopy
LC	Loading Capacity
EE	Encapsulation Efficiency
WCA	Water Contact Angle
FTIR	Fourier Transform Infrared Spectroscopy

71

72 **Practical Application:**

73 Composite ZP/OEO fibrous membranes, fabricated using coaxial electrospinning (ES)
74 technique, exhibit non-toxic in-vitro behavior and antimicrobial potential. This indicates
75 their potential application for bioactive food packaging improving sustainability.

76

77 **Introduction**

78 It is envisaged up to 40% of the total food supply ends up as waste in developed
79 countries, with food ‘loss’ the main cause. This is directly linked to preservation, retail
80 sales and final consumption (Verghese and others 2015). Since food preservation is a
81 crucial factor, advanced packaging materials may provide a valuable reduction in
82 wastage (Chung and others 2003; Neo and others 2013). Food spoilage, caused by
83 microorganisms, contributes towards waste and also poses an increased risk of
84 foodborne illness (Gram and others 2002). Both of these outcomes have socioeconomic
85 impacts, and it is therefore imperative to develop advanced packaging systems with
86 antimicrobial properties capable of promoting quality and safety (Appendini and
87 Hotchkiss 2002; Fernandez 2009; Gillgren and others 2009). Inclusion of actives into
88 non-functional packaging materials (e.g. particles, films or wraps) have been shown to
89 enhance shelf-life (Suppakul and others 2003). However, since there is a risk to oral
90 exposure *via* ingestion or possible migration (Maisanaba and others 2014), it is
91 paramount to assess toxic effects of emerging functionalized packaging materials.

92 Essential oils (EOs) are naturally occurring compounds displaying antimicrobial
93 properties. EOs are categorized as GRAS (Generally Recognized as Safe) by the FDA
94 (Wen and others 2016a) making them ideal for food preservation (Sugumar and others
95 2016). Several studies have shown chamomile blue, eucalyptus, lemongrass and lemon
96 oils to exhibit antibacterial and antifungal properties (Liakos and others 2014; Friedman
97 and others 2010; O'Bryan and others 2008). Citrus fruits possess high quantities of
98 vitamins, minerals and flavonoids. The latter display antioxidant potential which is
99 extremely valuable for anti-inflammatory and antimicrobial activity (Butz and others
100 2003). Moreover, amongst citrus oils, orange essential oil (OEO) exhibit interesting
101 biological functions. OEO's have been part of human diet for hundreds of years, and

102 while they are currently used as additive ingredients, they have been shown to illicit
103 preservative action; preventing growth of pathogens and spoiling microorganisms
104 (Torresalvarez and others 2016). In particular, studies have shown the compounds citral
105 and linalool to be key components for this action (Fisher and others 2007; Liu and
106 others 2012). However, when exposed to open air or ultraviolet light, most EOs undergo
107 oxidation (Alvarenga Botrel and others 2012). In addition, due to their water
108 insolubility and highly volatile character, the application of EOs in food preservation
109 has been limited (Wen and others 2016a; Moomand and Lim 2015a). For this reason,
110 several studies have centered on EO stability and bioactive function while exploring
111 their potential use in the food industry. For example, lemon essential oil has been
112 encapsulated in non-ionic surfactant *via* a colloidal delivery system. Here the EO's
113 properties were optimized by manipulating emulsion composition and altering storage
114 conditions (Ziani and others 2012).

115

116 The electrospinning (ES) technique, a one-step preparation method, which has been
117 used to engineer polymeric fibers on both nanometer and micrometer scales (Fabra and
118 others 2016; Aceituno-Medina and others 2015). For this process, the surface tension of
119 an electrically conducting formulation needs to be overcome by an applied electrical
120 force; which ultimately enables ultra-fine fiber manufacturing. Resulting fibers are
121 initially charged and under optimal conditions this permits further nano-scale
122 modulation. Fiber charge and size are conventionally regulated through conventional
123 process parameters (e.g. liquid flow rate and applied voltage) (Jaworek 2008). The
124 coaxial ES process provides greater encapsulation opportunities such as
125 micro/nano-layering, bioactive loading and controlled release. (McCann and others
126 2005).

127 Compared to other material engineering processes, ES enables fibrous film formation at
128 the ambient environment and with an on-demand aspect. This makes the process
129 friendlier towards volatile materials which may be susceptible to process damage.
130 Fibers possess larger surface areas and also permit a breathable aspect due to inherent
131 porosity control through over-layering. Furthermore, fiber accumulation over time
132 enables film engineering with modulated fiber size which is known to impact active
133 release properties and kinetics. In this regard, these variables allow thin films to be
134 tailor-made for specific applications (Agarwal and others 2008; Quirós and others 2016).
135 The encapsulation of OEO in to polymeric fibers using coaxial ES provides an
136 opportunity to build on current single needle encapsulation work. This is beneficial,
137 since OEO is volatile and complete (shell-like) encapsulation provides greater control
138 on volatile material retention (e.g. EO's) (Chalco-Sandoval and others 2016). Another
139 sister process, driven by formulation aspects, is emulsion ES. Here, additives within the
140 ES medium (consisting of two phases), lead to complexity in process and have potential
141 to impact food applications. Furthermore, the distribution of active (in emulsion form)
142 is randomly distributed. With coaxial ES, well-defined polymer shell structures are
143 achievable, with greater control on size distribution (narrow) making this more ideal
144 than the related emulsion process (Hongxu Qi and others 2006; Jiang and others 2014).
145 In addition, the ES encapsulation process facilitates EO stability and solubility by
146 dispersing oils throughout the polymeric fibrous matrix. This improves EO spacing
147 incorporating them closer to the molecular state rather than coarse oil droplets.

148

149 Zein prolamine (ZP) is a plant protein extract obtained from corn maize. Its intrinsic
150 low hydrophilicity, exceptional membrane forming behavior, high thermal resistance
151 and oxygen barrier properties make it ideal for numerous biological and biomedical

152 applications, including drug delivery and food technology. ZP has been used to
153 encapsulate *via* both single needle and coaxial ES (Neo and others 2013; Yang and
154 others 2013). Several studies have prepared ultra-thin ZP fibers to encapsulate bioactive
155 components (Torres-Giner and others 2008; Jiang and others 2007). For example,
156 ferulic acid (an antioxidant) has been blended with ZP to engineer composite systems
157 with free-radical scavenging properties to improve drug delivery (Yang and others
158 2013).

159

160 In this study, composite ZP/OEO fibrous membranes were engineered *via* coaxial ES to
161 demonstrate food preservation potential. OEO (the core medium) was encapsulated into
162 the polymeric matrix of the enveloping medium (the shell material comprising ZP)
163 functioning as a protective layer. The surface morphology, size distribution, and surface
164 hydrophilicity of fabricated non-woven mats were modulated by varying engineering
165 process parameters, such as ZP solution concentration, applied voltage, and media flow
166 rate. The encapsulation potential of OEO, using solution parameters, was assessed by
167 determining loading capacity (LC), encapsulation efficiency (EE) and oil retention. Mat
168 biocompatibility and antimicrobial activity were assessed using HEK293T cell lines and
169 *Escherichia coli* (*E. coli*), respectively. The results suggest the potential application of
170 the composite electrospun membrane in active food packaging for food preservation and
171 sustainability.

172

173

174 **Materials and Methods**

175 **Materials**

176 Zein prolamine (ZP, from maize corn) (Z 3625) was obtained from Sigma Aldrich (St.

177 Louis, Mo., USA). Ethanol, hexane and phosphate buffer saline (PBS, pH 7.4) were
178 obtained from Sinopharm Chemical Reagent Co., Ltd (Shanghai, China). OEO
179 extracted *via* steam-distillation was purchased from Jinyuan natural flavor Co., Ltd
180 (Jiangxi, China). All chemicals were analytical grade and were used without further
181 purification. A Millipore Milli-Q Reference ultra-pure water purifier (USA) was used to
182 obtain deionized water (DI water) for experimentation.

183

184 **Preparation of ZP solutions for electrospinning**

185 Appropriate quantities of ZP powder were dissolved into aqueous ethanol (80 v/v%) to
186 prepare several ZP solutions (25, 30 and 35 w/v%). A magnetic stirrer (VELP ARE
187 heating magnetic stirrer, Italy) was used to ensure complete dissolution of ZP powder.
188 The solutions were poured into a flask and then mechanically stirred at ~300 rpm at the
189 ambient temperature (25°C) for 1 h.

190

191 **Physical properties of solutions**

192 Viscosities and electrical conductivities of ZP solutions with different concentrations
193 were measured. Solution viscosity was measured using a viscometer (LV DV-II,
194 Brookfield, USA). 2 mL of each solution sample was placed into pre-defined stainless
195 steel wells of the viscometer and then the viscosity value was obtained at 25°C using a
196 S21 spindle at 140 rpm. A YSI 3200 electrical conductivity meter (YSI, USA) was used
197 to measure solution electrical conductivity at 25°C. All characterizations were carried
198 out in triplicate and mean values were obtained.

199

200 **Fabrication of electrospun composite ZP/OEO fiber**

201 The coaxial ES apparatus (**Figure 1a**) includes a high power voltage supply, two

202 precision syringe pumps, a coaxial stainless steel needle and a collector connected to the
203 ground electrode. The coaxial device consists of two concentrically aligned and
204 enveloped needles. The diameter of the inner and outer needles were 0.2 and 0.4 mm,
205 while the dimensions of the outer needle were 0.9 and 1.2 mm, respectively. A selected
206 ZP solution was loaded into a 5 mL plastic syringe. A high-precision syringe pump (KD
207 Scientific KDS100, USA) was used to perfuse the solution (in controlled fashion) from
208 the syringe into the outer inlet of the coaxial stainless needle *via* silicon tubing. The
209 inflow rate of ZP solution ranged from 1.5 to 3.0 mL/h. OEO was loaded into another
210 syringe and perfused into the inner needle of the coaxial device at a flow rate of 1.5
211 mL/h. A high voltage power supply (Glassman high voltage Inc. series FC, USA) was
212 used to generate an electric field between the coaxial needle and the ground electrode,
213 and the voltage ranged from 18.0 to 19.5 kV. Aluminum foil, which was placed directly
214 below the coaxial needle at a distance of 15 cm, was used as the collector and was
215 connected to the grounded electrode. A high-speed camera (Baummer TXG02C,
216 Germany) was used to observe the ES jetting modes. All experiments were performed at
217 the ambient temperature (25°C).

218

219 **Fiber morphology and size assessment**

220 The morphology, diameter and size distribution of generated fibers were studied using
221 optical (OM, Pheonix BMC503-ICCF, China) and field emission scanning electron
222 microscopes (SEM, SU 8000 SEM, Hitachi, Japan). For SEM analysis, micrographs
223 were obtained at an accelerating voltage of 20 kV. Samples were fixed on to metallic
224 stubs by double-backed conductive tape. Prior to analysis, all samples were
225 sputter-coated with a thin layer of gold using a vacuum sputter coater (Ion sputter MC
226 1000, Hitachi, Japan) for 60 s at a current intensity of 25 mA. Micrographs were

227 subsequently analyzed using ImageJ software (National Institute of Health, MD, USA)
228 to measure fiber diameter at various process conditions. All statistical graphs were
229 plotted using Origin software (OriginLab, USA).

230

231 **Loading capacity and encapsulation efficiency of OEO**

232 As a highly volatile medium, OEO at the fiber surface (un-encapsulated) is prone to
233 evaporation (Li and others 2013). Thus, it is crucial to assess the encapsulation effect of
234 OEO in ZP matrix. In this study, encapsulation properties of OEO were determined
235 (loading capacity (LC) and encapsulation efficiency (EE)) following 2 h desiccation
236 post engineering. According to previous studies (Neo and others 2013; Moomand and
237 Lim 2014), these properties were determined by dissolving 100 mg of ZP/OEO
238 composite fibers in 5 ml of 80 v/v% ethanol aqueous solution using a 15 mL centrifuge
239 tube. After complete dissolution of composite fibers, OEO was extracted using 5 mL
240 hexane for 15 min, and this procedure was carried out three times. OEO extracts were
241 collected in 25 mL volumetric flasks, and the quantity of OEO was obtained using UV
242 spectroscopy (UV-2600 spectrophotometer, Shimadzu, Japan). A wavelength of 202 nm
243 was used to establish a standard calibration curve (Li and others 2013). The loading
244 capacity (LC) of OEO in electrospun fibers was calculated by Equation 1:

$$245 \text{LC (\%)} = \frac{\text{Amount of oil content entrapped in the fibers}}{\text{Weight of the fibers}} \times 100\% \quad (\text{Eq. 1})$$

246 The encapsulation efficiency (EE) of OEO in the electrospun fibers was calculated
247 using Equation 2:

$$248 \text{EE (\%)} = \frac{\text{Amount of oil content entrapped in the fibers}}{\text{Theoretical total amount of oil}} \times 100\% \quad (\text{Eq. 2})$$

249 The theoretical quantity of OEO was calculated by obtaining the proportion of oil

250 weight to total weight of composite fibers, which was measured using solution density
251 and the ratio of inner and outer layer solution flow rate. In this study, the theoretical
252 amount of oil within 100 mg fibrous sample was 37 mg.

253

254 **Water contact angle measurements**

255 In general, water contact angle (WCA) measurements were used to represent the
256 hydrophobic/hydrophilic nature of membranes. WCA's were measured using an optical
257 contact angle meter (SL200KB, KINO Industry Co. Ltd., USA). The fibrous non-woven
258 samples with thickness of ~0.1 mm were collected for 15 min and were subsequently
259 layered onto an object slide using adhesive tape at the peripheral regions. WCA of pure
260 OEO was measured by directly depositing the material onto a scribed object slide. The
261 sample was mounted on to a three-axis horizontal tilt stage and the measurement was
262 observed in the sessile drop mode at 25°C. A water droplet (~10 µL) was pipetted on to
263 each membrane sample. The mean value of left and right WCAs on each sample was
264 recorded, when the droplet status acclimatized (2 s after droplet release). The mean of
265 three measurements was recorded.

266

267 **Retention of OEO in fibrous membranes**

268 OEO and electrospun ZP/OEO non-wovens (500 mg per sample, theoretically
269 encapsulating 185 mg of OEO) were placed in 6 cm petri dishes. The samples were then
270 placed into a forced air circulation oven (Heraeus T6, Thermo scientific, UK) at ambient
271 temperature (25°C). The retention of OEO was defined as shown in Equation 3, which
272 was calculated over a 24 h period. The analysis was carried out in triplicate.

$$273 \text{ Retention (\%)} = \frac{\text{Total oil content}}{\text{Theoretical total amount of oil}} \times 100\% \quad (\text{Eq.3})$$

274

275 **Fourier transform infrared spectroscopy**

276 Following OEO retention test (24 h), Fourier Transform Infrared (FTIR) spectroscopy
277 (IR Affinity 1, Shimadzu, Japan) was used to assess material stability, identification and
278 to determine any chemical interactions between encapsulated materials. Prior to FTIR
279 scanning, pellet samples were prepared. Here the KBr pellet pressing method was
280 deployed (Wang and others 2016). For this, 2 μL of OEO, 2 mg of pure ZP powder and
281 2 mg of ZP/OEO electrospun fibers were dispersed in 200 mg of KBr powder by
282 grinding in a mortar, individually. The mixtures were then compressed into transparent
283 pellets (pressure ~ 20 MPa). The spectrum (range ~ 4000 to 400 cm^{-1}) of each sample
284 was acquired from 20 scans using a resolution of 4 cm^{-1} .

285

286 **In-vitro biological evaluation**

287 In food retail and manufacturing industries, deployed composite packaging materials are
288 prone to consumer interaction, either through skin or oral contact. Therefore, it is
289 necessary to assess potential risks of food packaging materials towards humans
290 (Eleftheriadou and others 2016). In this study, HEK293T cell lines were used to assess
291 cytotoxicity of ZP and ZP/OEO fibrous membranes. HEK293T cells were incubated and
292 maintained in DMEM medium supplied with 10% FBS at $37\text{ }^{\circ}\text{C}$, in 5% CO_2 . The
293 culture medium was changed every 2 days. 100 μL HEK293T cell suspension was
294 transferred to a 96-well plate at a density of 1.5×10^4 cells/well and incubated for 24 h. A
295 CCK-8 assay was set to evaluate the proliferation of HEK293T cells at 4 and 8 h during
296 cell culture. Electrospun fibrous non-wovens (collected for 1 h) were cut into discs
297 (diameter = 6 mm). Fibrous discs were sterilized under UV light for 2 h and were then
298 added to the cell culture plate. After incubation for 4 and 8 h, cell viability was
299 measured by adding 20 μL of a CCK-8 solution to each well and incubating for a further

300 3 h. Absorbance was measured at a wavelength of 450 nm using a microplate reader
301 (Multiskan GO, Thermo Fisher Scientific, USA). Cell viability in polystyrene well plate
302 only was used as a control and the culture medium with CCK-8 solution was utilized as
303 a blank. The relative cell viability (%) was calculated using Equation 4:

$$304 \text{ Cell viability (\%)} = \frac{\text{Ab. (sample)} - \text{Ab. (blank)}}{\text{Ab. (control)} - \text{Ab. (blank)}} \times 100\% \quad (\text{Eq.4})$$

305 Where Ab. means the absorbance.

306 In addition, optical microscopy (CKX41, Olympus, Japan) was utilized to observe cell
307 morphology and to further confirm cell biocompatibility.

308

309 **Antimicrobial activity test**

310 Antimicrobial activity of electrospun membranes against *E. coli* was evaluated using an
311 agar diffusion assay. Lysogeny-broth was sterilized in a High-pressure Steam
312 Sterilization Pot (YXQ-LS-S II, Shanghai Boxun Industry & Commerce Co., Ltd.,
313 Shanghai, China) at 120°C after which 10 mL was poured into several 10 cm petri
314 dishes. 200 µL of bacterial suspension was spread on to agar plates once the nutrient
315 medium had coagulated. Then, composite and pure electrospun ZP membranes
316 (collected for 1 h and cut into 15 mm discs) were placed on to inoculated plates. The
317 plates were incubated at 37°C for 24 h. Antimicrobial activity was evaluated by
318 measuring disc inhibition zone as previously reported (Wen and others 2016a).

319

320 **Statistical analysis**

321 All experiments were performed in triplicate and data were presented as the mean ±
322 standard deviation (n=3). Statistical analyses were carried out using SPSS software
323 (SPSS Statistics v18, IBM, UK). Statistically significant differences among variables
324 were performed using a One-way Analysis of Variance (ANOVA) followed by Student's

325 t-Test to establish any significant differences (* $p < 0.05$).

326

327 **Results and Discussion**

328 **Fabrication of ZP/OEO fibers and fibrous membranes**

329 Two immiscible liquids were simultaneously infused into the coaxial device. For fiber
330 generation, jetting stability is influenced by gravity, applied electrical force and media
331 surface tension (Gao and others 2016b). Amongst all process parameters (e.g. applied
332 voltage, media flow rate, collector distance and physical properties of solution), the
333 applied voltage is a dominant factor in enabling ES and its optimization is essential for
334 stable and continuous fiber generation (Cipitria and others 2011). When the electrical
335 force between the capillary exit and ground electrode was increased to the optimal value,
336 the liquid meniscus on the nozzle exit stretched into a conical shape, forming a cone-jet
337 (mode). When the two solutions (OEO and ZP, flow rates 1.5 and 2.0 mL/h, respectively)
338 were infused without any electrical force acting on the co-flow liquid system, the
339 dripping mode was observed (**Figure 1b**). This comparatively simple liquid deformation
340 and dripping behavior is attributed to gravitational, surface tension and mechanical
341 syringe action. When the applied voltage was increased to ~19 kV, the co-flow liquid
342 behavior at the nozzle exit transitioned from the dripping mode to the stable jetting
343 mode, where typical characteristics of the Taylor cone were observed (**Figure 1c**). The
344 auxiliary lines in the insets of **Figures 1b&c** demonstrate the immiscibility of OEO and
345 ZP in the co-flow system, which is crucial for generating core-shell structures during the
346 coaxial ES process.

347 In this study, the impact of varying enveloping ZP polymer concentration (25, 30 and 35
348 w/v%) on resulting composite (ZP/OEO) fibers was investigated. **Figures 2a-i** show
349 surface morphology and size distribution of composite fibers prepared using ZP

350 solutions at various concentrations. Optical images (**Figures 2a, d&g**) suggest fiber
351 production is achievable using all explored ZP solutions. Further inspection using SEM
352 (**Figures 2b, e&h**) demonstrates the 35 w/v% solution is optimal when compared to 25
353 and 30 w/v% ZP solutions, due to the smooth surface morphology, which facilitates the
354 encapsulation of core medium during the electrohydrodynamic process (Gao and others
355 2016a). Electrospun composite fibers prepared using 35 w/v% ZP solution appear more
356 uniform. Higher magnification micrographs (**Figures 2c, f&i**) show composite fibers
357 prepared using 35 w/v% ZP solution display ribbon like (flattened) morphology with
358 smooth surface topography. Intermittent particle (beaded) and spindled morphologies
359 are apparent for fibers (also ribbon like) prepared using solutions with varying ZP
360 concentrations (25 and 30 w/v%). In addition, crinkled surface topography is also
361 evident on composite fibers prepared from lower ZP concentrations. Rapid volatilization
362 of ethanol in perfused ZP solution (during and subsequently after jetting) and
363 unexpanded β -folds within ZP molecular structure result in ribbon and crinkled
364 structures (Neo and others 2012; Jiang and others 2012). The resulting fiber diameter
365 from structures engineered using solutions with ZP concentrations of 25, 30 and 35
366 w/v%, are 1.05 ± 0.36 , 2.30 ± 0.43 and 1.61 ± 0.41 μm , respectively, as shown in insets of
367 **Figures 2c, f&i**.

368 In general, the rheological behavior, especially solution viscosity, is critical for fiber
369 production and morphology type. Both ZP polymer concentration and molecular weight
370 (M_w) influence solution viscosity (Rieger and others 2016). Polymer chain entanglement
371 concentration (C_e) predicts the spinnability of the polymer solution used in this study,
372 and represents the minimum polymer concentration necessary to fabricate electrospun
373 fibers with a beaded morphology (McKee and others 2004; Palangetic and others 2014).
374 The viscosity of ZP solutions (increasing from 5 to 35 w/v% ZP) shows an increase

375 before and after chain entanglement. In the current study, C_e was determined to be 16.8
376 w/v% for ZP solutions (**Figure 2j**), which suggests concentrations below this (C_e) value
377 will yield particles, and fabrication of defect free composite fibers *via* ES require
378 solutions with greater ZP concentrations (e.g. 35 w/v%).

379

380 **Effect of flow rate**

381 In a coaxial ES set-up, the driving liquid in the co-flowing process possesses the greater
382 electrical conductivity (Loscertales and others 2002). ZP solutions exhibit greater
383 electrical conductivities and viscosities, compared to co-flowing OEO (**Table 1**). The
384 viscosity of ZP solutions increased with increasing polymer concentration (i.e. resulting
385 viscosities were 422.2 ± 0.9 , 745.4 ± 1.5 , and 1197.0 ± 3.0 mPa•S for solutions comprising
386 25, 30, and 35 w/v% ZP, respectively). The electrical conductivity decreased as the
387 solution ZP concentration was increased (i.e. the electrical conductivities were
388 625.6 ± 0.2 , 611.2 ± 0.5 , and 599.5 ± 0.6 μ S/m for ZP concentrations of 25, 30, and 35
389 w/v%, respectively). The effect of flow rate on mean fiber diameter was investigated by
390 varying the enveloping liquid (shell material, ZP infusion rate from 1.5 to 3.0 mL/h (1.5,
391 2.0, 2.5, and 3.0 mL/h). **Figure 3a** highlights the connection between composite
392 (ZP/OEO) fiber diameter distribution and increasing ZP solution infusion rate.

393 Mean fiber diameters were 0.7 ± 0.1 , 0.9 ± 0.2 , 1.0 ± 0.2 and 1.2 ± 0.2 μ m at infusion rates of
394 1.5, 2.0, 2.5 and 3.0 mL/h, respectively. An increase in the enveloping medium flow rate
395 resulted in coarser fibers due to greater quantities of solution (and therefore ZP polymer
396 content) contributing towards the fibrous shell. In addition, as fibers were engineered
397 under stable jetting, the mean fiber diameter appeared uniform with a standard
398 derivation of only ~ 0.2 μ m.

399

400 **Effect of applied voltage**

401 The driving liquid (ZP solution) in the coaxial ES process dictates the co-flow behavior,
402 and electrical stress arising from this medium is transferred to the enveloped OEO *via*
403 viscosity. The effect of voltage on mean fiber size was assessed, using an applied
404 voltage range based on the stable jetting mode window (18.0-19.5 kV) (Bhardwaj and
405 Kundu 2010), with all other parameters (ZP solution concentration, flow rate of inner
406 and outer liquids, and collector distance) constant. Fiber diameter distributions are
407 shown in **Figure 3b**. Increasing the applied voltage results in finer fibers (i.e. mean
408 fiber diameters were 1.3 ± 0.2 , 1.0 ± 0.2 , 0.9 ± 0.2 and 0.8 ± 0.2 μm for applied voltages of
409 18.0, 18.5, 19.0 and 19.5 kV, respectively). This is due to an enhanced stretching force
410 at increased voltages (Bhardwaj and Kundu 2010). The standard deviation for mean
411 fiber diameters were also narrow for applied voltages between 18.0 and 19.5 kV. In this
412 range, the voltage is attributed to engineering within the stable jetting mode. At low
413 applied voltages, superfluous liquid accumulates at the nozzle exit (due to a low
414 drawing and stretching force) which intermittently impedes the ES process, giving rise
415 to fibers with a broader size distribution. At higher applied voltages a multi-jet mode
416 results, which also leads to production of fibers with a broader size distribution (Gao
417 and others 2016b).

418

419

420 **Encapsulation of OEO in ZP fiber matrix**

421 The coaxial ES technique has been shown to be more efficient for bioactive
422 encapsulation when compared to dispersion and emulsification methods (Moomand and
423 Lim 2014; Yao and others 2016a). Although the selected engineering process is crucial
424 for composite material integration, material properties also impact bioactive LC and EE.

425 OEO is volatile and therefore it's LC and EE need to be investigated to determine the
426 suitability of the coaxial ES technique. For this, solutions with various ZP
427 concentrations (contributing towards the shell matrix material) were investigated. As
428 shown in **Figure 4**, both LC and EE of OEO in fibrous ZP membranes using low ZP
429 concentrations (25 and 30 w/v%) were lower than those obtained using 35 w/v% ZP
430 solution. The OEO LC values were 10.19 ± 0.45 , 15.41 ± 0.57 and $22.28\pm 0.27\%$ when
431 using 25, 30 and 35 w/v% ZP solutions, respectively. However, the EE values of OEO
432 were 27.53 ± 1.23 , 42.81 ± 1.58 and $53.68\pm 0.78\%$ when using 25, 30 and 35 w/v% ZP
433 solutions, respectively. LC indicates the quantity, by comparison of the total mass, of
434 OEO in the composite system, while EE defines the entrapment efficiency of OEO
435 within the fibrous structure (i.e. in the core and ZP matrix). Differences in LC and EE
436 are mainly due to the morphological variations of electrospun fibers, increase in
437 polymeric chains arising from greater ZP concentrations and unequal distribution of ZP
438 polymer surrounding encapsulated OEO (Yao and others 2016a). Non-uniform fibers, as
439 shown in **Figures 2a&d**, lead to incomplete and poor encapsulation of OEO within the
440 fiber matrix (i.e. core and also the ZP matrix), which accelerates the volatilization of
441 OEO. Uniform fiber distribution obtained using 35 w/v% ZP solution enables
442 encapsulation of OEO with a ZP shell matrix and fibers possess similar morphologies
443 with equal ZP distribution along the length and width of individual fibers.

444

445 **Surface hydrophilicity**

446 Water contact angle (WCA) measurements provide an indication of membrane
447 interaction at a liquid interface which are crucial for bio-related applications, such as
448 cell adhesion, spreading and availability in the ambient environment (Liao and others
449 2016). WCAs of composite nonwovens prepared using various ZP solution

450 concentrations are shown in **Figure 5a**. Mean WCAs on membranes prepared using 25,
451 30 and 35 w/v% ZP solutions are 31.36 ± 2.44 , 49.65 ± 1.97 and $63.08\pm 2.97^\circ$, respectively,
452 which indicate all composite membranes are hydrophilic. As shown in **Figures 5b&c**,
453 the mean WCA on pure electrospun ZP membrane and OEO (medium scribed on an
454 object slide) are 85.18 ± 2.62 and $22.09\pm 0.24^\circ$, respectively. This demonstrates pure ZP
455 membranes are less hydrophilic than their composite systems. The difference between
456 composite and pure ZP membrane hydrophilicity is due to ZP quantities within various
457 samples. Greater ZP concentrations hinder diffusive movement of OEO from the inner
458 core layer to the external region of fibers and thus membrane surface. Reduced LC and
459 EE of OEO are observed for membranes prepared using lower ZP concentrations during
460 coaxial ES; indicating incomplete OEO encapsulation. This is due to the easier vapor
461 penetration through reduced polymer content (i.e. ZP loading volume is indicative of
462 how much polymer will remain after evaporation). In addition, size distribution and
463 surface morphology of electrospun fibers also influence the hydrophilicity (Yao and
464 others 2016b). At low ZP concentrations, the non-uniform distribution of fibers and
465 varied surface features (crinkled and beaded) lead to rougher surfaces as shown in
466 **Figures 2c&f**. Besides, reduced fiber diameters limit the quantity of trapped air at the
467 fiber membrane-water interface, which results in reduced WCAs (Liu and others 2016;
468 Xu and others 2012).

469

470 **Retention of OEO in fibrous membranes**

471 The retention of free OEO and encapsulated OEO in ZP composite fibers was
472 determined by measuring mass loss over 24 h. As shown in **Figure 6a**, the quantity of
473 retained OEO decreased during the test period in all test groups. The retention of free
474 OEO after 24h was only 2.76%, which indicates the volatile nature of OEO. The

475 greatest retention of OEO was 61.54% and was demonstrated by composite membranes
476 prepared using 35 w/v% ZP solution. OEO retention from composite membranes
477 prepared using 30 and 25 w/v% ZP solutions, was 41.12% and 39.44%, respectively.
478 This trend in OEO retention is attributed to ZP content in the co-flow system. Larger
479 quantities of ZP in the enveloping medium impede OEO evaporation from the
480 composite system once atomized and exposed to air. **Figure 6a** shows OEO retention
481 decreased sharply in the first hour (at ambient temperature, 25°C). After this point, OEO
482 retention decreased gradually up to 8 hours after which it remained constant. **Figure 6b**
483 shows OEO retention in the first hour. The retention of OEO was 47.46, 60.78 and
484 72.11% from composite membranes prepared from 25, 30 and 35 w/v% ZP solutions.
485 The retention of free OEO was 7.14%. The sharp decline for free OEO is due to the
486 rapid unhindered volatilization of OEO in air. As shown in **Figure 4**, low LC and EE of
487 OEO in membranes prepared using 25 and 30 w/v% ZP solutions suggest greater OEO
488 exposure to air. These results confirm membranes prepared from solution with higher
489 ZP concentrations retain greater quantities of OEO within the fibrous composite system.

490

491 **Infrared spectra**

492 FTIR was used to investigate the effect of the coaxial ES process on chemical structure
493 stability and material integration. Electrospun membranes were collected, dried for 24h
494 and then analyzed. As shown in **Figure 7a**, infrared spectra of pure ZP powder, OEO
495 and electrospun composite (ZP/OEO) fibers prepared with varying ZP solution
496 concentrations were observed. The peaks at 1515 cm^{-1} and $\sim 1650 \text{ cm}^{-1}$ represent amide
497 II and amide I bands in pure ZP powder, respectively (Gillgren and others 2009;
498 Forato and others 2004). For the pure/free OEO, characteristic peak at 887 cm^{-1}
499 represent non-polymethoxylated flavone residues in the oil, and the peaks at 957, 1050

500 and 1155 cm^{-1} indicate C-H stretching vibration of sinensetin, the C-H stretching
501 vibration of heptamethoxyflavone, and the C-O-C stretching vibration of tangeretin,
502 respectively, which are the polymethoxylated flavone constituents in OEO (Manthey
503 2006). Characteristic peaks are present in all spectra (**Figure 7a**) of ZP membranes
504 (prepared using 25, 30 and 35 w/v% ZP solutions) indicating successful encapsulation
505 and retention (post 24 hours drying) of OEO. The ZP amide I band shifts to a lower
506 wavenumber as the ZP solution concentration is increased. As shown in **Figure 7b**, the
507 characteristic amide I band is displayed at 1653 , 1647 and 1646 cm^{-1} for membranes
508 prepared using 25, 30, and 35 w/v% ZP solutions, respectively. The shift in peak value
509 is due to the variation in the α -helix length; an increase in helical length leads to a lower
510 peak wavenumber. This arises from enhanced hydrogen bonding involving the C=O
511 group as the ZP solution concentration is increased (Dousseau and Pezolet 1990;
512 Torres-Giner and others 2008). Furthermore, longer α -helix structures also favor beaded
513 morphologies, which correlates with spindle and beaded morphologies obtained using
514 low ZP solution concentrations as previously shown in **Figure 2** (Moomand and Lim
515 2015b).

516

517 **Biological evaluation of electrospun fibrous membranes**

518 Cell viability reflects the potential toxic risks of different samples *in vitro*, expressed as
519 a percentage of viable cells within the total cell population, and calculated by comparing
520 the test group (fiber samples) to the control (no samples) (Güney and others 2014).
521 CCK-8 assay was used to evaluate cytotoxicity of electrospun fibrous discs. As shown
522 in **Figure 8a**, cell proliferations on both pure ZP and composite discs exhibit no
523 significant difference compared to the control group at 4 and 8 hours incubation time.
524 Cell viability remained at 105 and 100% for pure ZP and composite (ZP/OEO) discs,

525 respectively, at 4 hours incubation. After 8 hours, cell viability was 94 and 95% for pure
526 ZP and composite discs, respectively. These results clearly demonstrate negligible
527 cytotoxicity towards the HEK293T cell line, further supporting ZP utility as a
528 biomedical biopolymer (Jiang and others 2010).

529 Cell growth behavior was observed using an optical microscope. Cells were incubated
530 in medium with fibrous pure ZP and composite discs. As shown in **Figure 8b**, most
531 HEK293T cells exhibited growth and adherence. Cell morphology further confirmed
532 biocompatibility of ZP and composite discs at the selected assessment times. Cell
533 viability results indicate no significant variation among the test and control groups,
534 which demonstrates negligible cytotoxicity as shown in previous reports (Liao and
535 others 2016; Unlu and others 2010). The results suggest the non-toxicity of the
536 fabricated membranes and the potential to be used in food industry.

537

538 **Antimicrobial activity of ZP/OEO fibrous membranes**

539 The antimicrobial activity of composite fibrous discs was investigated using *E. coli* as
540 the test microorganism over a 24h incubation period. Membranes, and subsequently
541 discs with diameters of 15mm, prepared using 35 w/v% ZP solutions, were selected for
542 assessment, and pure ZP membrane was set as the control group (without OEO). Both
543 membranes were prepared using the same optimal ES conditions (applied voltage = 19
544 kV, flow rate of ZP solution = 2.0 mL/h, for composite membrane-flow rate of OEO =
545 1.5 mL/h, and collector distance = 12.0 cm). **Figures 9a, b&c**, show both disc samples
546 exhibit inhibition zones at 16, 20 and 24 h incubation. Moreover, inhibition zones
547 (diameter) of composite discs was significantly wider than pure ZP samples (i.e.
548 Inhibition zone= 14.44 ± 0.98 mm for composite discs, and 3.57 ± 0.36 mm for pure ZP
549 discs at 16 h) as shown in **Figure 9d**. Fibrous mats present clear inhibition zones.

550 According to a previous study (Wen and others 2016b), the present results indicate
551 fibrous mats to possess antimicrobial function.

552 Over the 24 h test period, the inhibition zone of each sample decreased slightly but
553 showed no significant difference. Composite discs are non-toxic, biocompatible (Liao
554 and others 2016) and demonstrate antimicrobial properties; elucidating potential
555 applications in food packaging to address current challenges in food preservation.

556

557 **Conclusion**

558 In summary, optimized fibrous composite (ZP/OEO) membranes with mean diameters
559 ranging from 750 to 1400 nm were fabricated using the coaxial ES technique.
560 Composite fiber surface morphology and size distribution was regulated using ZP
561 solution concentration, applied voltage and formulation flow rate. FTIR analysis
562 indicates the successful and stable encapsulation of OEO within ZP fiber matrix.
563 Variation in ZP solution concentration leads to the transformation of ZP chemical
564 structure and further influences fiber morphology. By increasing the ZP concentration,
565 fiber uniformity and continuity was achieved. In addition, LC, EE and retention of OEO
566 were also enhanced. Greater ZP solution concentrations yield fibrous membranes (*via*
567 coaxial-ES) with relatively superior hydrophobic properties. CCK-8 assay conducted on
568 HEK293T cell lines demonstrated good cytocompatibility on both electrospun pure ZP
569 and composite discs *in-vitro*. Cell morphology indicates no adverse effects on cell
570 growth. Fibrous composite discs demonstrated antimicrobial activity using *E. coli*,
571 indicating potential application as food packaging material for bioactive food
572 preservation, such as prolonging fruit shelf-life and therefore sustainability.

573

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578

579 **Author Contributions**

580 Zhi-Cheng Yao performed the experimental work and analyzed the data. Si-Cong Chen
581 contributed in the experiments of biological evaluation and antimicrobial activity test.
582 Zeeshan Ahmad, Jie Huang, and Jing-song Li contributed towards data analysis,
583 interpretation and discussion. Ming-Wei Chang directed and designed the experiments.
584 All authors revised the manuscript and approved the final version.

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588 **References**

- 589 Aceituno-Medina M, Mendoza S, Rodríguez BA, Lagaron JM, López-Rubio A. 2015. Improved
590 antioxidant capacity of quercetin and ferulic acid during in-vitro digestion through
591 encapsulation within food-grade electrospun fibers. *Journal of Functional Foods* 12:332-41.
- 592 Agarwal S, Wendorff JH, Greiner A. 2008. Use of electrospinning technique for biomedical
593 applications. *Polymer* 49(26):5603-21.
- 594 Alvarenga Botrel D, Vilela Borges S, Victória de Barros Fernandes R, Dantas Viana A, Maria Gomes
595 da Costa J, Reginaldo Marques G. 2012. Evaluation of spray drying conditions on properties
596 of microencapsulated oregano essential oil. *International Journal of Food Science &
597 Technology* 47(11):2289-96.
- 598 Appendini P, Hotchkiss JH. 2002. Review of antimicrobial food packaging. *Innovative Food Science
599 & Emerging Technologies* 3(2):113-26.
- 600 Bhardwaj N, Kundu SC. 2010. Electrospinning: a fascinating fiber fabrication technique.
601 *Biotechnology advances* 28(3):325-47.
- 602 Butz P, Fernandez GA, Lindauer GR, Dieterich S, Bogner A, Tauscher B. 2003. Influence of ultra
603 high pressure processing on fruit and vegetable products. *Journal of Food Engineering*
604 56(2):233-6.
- 605 Chalco-Sandoval W, Fabra MJ, López-Rubio A, Lagaron JM. 2016. Development of an encapsulated
606 phase change material via emulsion and coaxial electrospinning. *Journal of Applied
607 Polymer Science* 133(36).
- 608 Chung D, Papadakis SE, Yam KL. 2003. Evaluation of a polymer coating containing triclosan as the
609 antimicrobial layer for packaging materials. *International journal of food science &
610 technology* 38(2):165-9.
- 611 Cipitria A, Skelton A, Dargaville T, Dalton P, Hutmacher D. 2011. Design, fabrication and
612 characterization of PCL electrospun scaffolds—a review. *Journal of Materials Chemistry*
613 21(26):9419-53.
- 614 Dousseau F, Pezolet M. 1990. Determination of the secondary structure content of proteins in
615 aqueous solutions from their amide I and amide II infrared bands. Comparison between
616 classical and partial least-squares methods. *Biochemistry* 29(37):8771-9.
- 617 Eleftheriadou M, Pyrgiotakis G, Demokritou P. 2016. Nanotechnology to the rescue: using
618 nano-enabled approaches in microbiological food safety and quality. *Current Opinion in
619 Biotechnology* 44:87.
- 620 Fabra MJ, López-Rubio A, Lagaron JM. 2016. Use of the electrohydrodynamic process to develop
621 active/bioactive bilayer films for food packaging applications. *Food Hydrocolloids* 55:11-8.
- 622 Fernandez A. 2009. Novel route to stabilization of bioactive antioxidants by encapsulation in
623 electrospun fibers of zein prolamine. *Food Hydrocolloids* 23(5):1427-32.
- 624 Fisher K, Rowe C, Phillips CA. 2007. The survival of three strains of *Arcobacter butzleri* in the
625 presence of lemon, orange and bergamot essential oils and their components in vitro and on
626 food. *Letters in applied microbiology* 44(5):495-9.
- 627 Forato LA, Doriguetto AC, Fischer H, Mascarenhas YP, Craievich AF, Colnago LA. 2004.
628 Conformation of the Z19 prolamin by FTIR, NMR, and SAXS. *Journal of agricultural and
629 food chemistry* 52(8):2382-5.
- 630 Friedman M, Henika PR, Levin CE, Mandrell RE. 2010. Antimicrobial Wine Formulations Active
631 Against the Foodborne Pathogens *Escherichia coli* O157: H7 and *Salmonella enterica*.

632 Journal of Food Science 71(71):M245-M51.

633 Güney G, Kutlu HM, Genç L. 2014. Preparation and characterization of ascorbic acid loaded solid
634 lipid nanoparticles and investigation of their apoptotic effects. *Colloids and Surfaces B:*
635 *Biointerfaces* 121:270-80.

636 Gao Y, Chang MW, Ahmad Z, Li JS. 2016a. Magnetic-responsive microparticles with customized
637 porosity for drug delivery. *Rsc Advances* 6(91).

638 Gao Y, Zhao D, Chang M-W, Ahmad Z, Li J-S. 2016b. Optimising the shell thickness-to-radius ratio
639 for the fabrication of oil-encapsulated polymeric microspheres. *Chemical Engineering*
640 *Journal* 284:963-71.

641 Gillgren T, Barker SA, Belton PS, Georget DM, Stading M. 2009. Plasticization of zein: a
642 thermomechanical, FTIR, and dielectric study. *Biomacromolecules* 10(5):1135-9.

643 Gram L, Ravn L, Rasch M, Bruhn JB, Christensen AB, Givskov M. 2002. Food
644 spoilage—interactions between food spoilage bacteria. *International journal of food*
645 *microbiology* 78(1):79-97.

646 Hongxu Qi, Hu P, Jun Xu A, Wang A. 2006. Encapsulation of Drug Reservoirs in Fibers by
647 Emulsion Electrospinning: Morphology Characterization and Preliminary Release
648 Assessment. *Biomacromolecules* 7(8):2327-30.

649 Jaworek A. 2008. Electrostatic micro- and nanoencapsulation and electroemulsification: a brief
650 review. *Journal of Microencapsulation* 25(7):443.

651 Jiang H, Wang L, Zhu K. 2014. Coaxial electrospinning for encapsulation and controlled release of
652 fragile water-soluble bioactive agents. *Journal of Controlled Release* 193:296.

653 Jiang H, Zhao P, Zhu K. 2007. Fabrication and characterization of zein-based nanofibrous scaffolds
654 by an electrospinning method. *Macromolecular Bioscience* 7(4):517.

655 Jiang Q, Reddy N, Yang Y. 2010. Cytocompatible cross-linking of electrospun zein fibers for the
656 development of water-stable tissue engineering scaffolds. *Acta Biomaterialia* 6(10):4042-51.

657 Jiang Y-N, Mo H-Y, Yu D-G. 2012. Electrospun drug-loaded core–sheath PVP/zein nanofibers for
658 biphasic drug release. *International journal of pharmaceutics* 438(1):232-9.

659 Li Y, Ai L, Yokoyama W, Shoemaker CF, Wei D, Ma J, Zhong F. 2013. Properties of
660 chitosan-microencapsulated orange oil prepared by spray-drying and its stability to
661 detergents. *Journal of agricultural and food chemistry* 61(13):3311-9.

662 Liakos I, Rizzello L, Scurr DJ, Pompa PP, Bayer IS, Athanassiou A. 2014. All-natural composite
663 wound dressing films of essential oils encapsulated in sodium alginate with antimicrobial
664 properties. *International journal of pharmaceutics* 463(2):137-45.

665 Liao N, Joshi MK, Tiwari AP, Park C-H, Kim CS. 2016. Fabrication, characterization and
666 biomedical application of two-nozzle electrospun polycaprolactone/zein-calcium lactate
667 composite nonwoven mat. *Journal of the Mechanical Behavior of Biomedical Materials*
668 60:312-23.

669 Liu K, Chen Q, Liu Y, Zhou X, Wang X. 2012. Isolation and Biological Activities of Decanal,
670 Linalool, Valencene, and Octanal from Sweet Orange Oil. *Journal of Food Science*
671 77(11):C1156–C61.

672 Liu Z, Zhao J-h, Liu P, He J-h. 2016. Tunable surface morphology of electrospun PMMA fiber using
673 binary solvent. *Applied Surface Science* 364:516-21.

674 Loscertales IG, Barrero A, Guerrero I, Cortijo R, Marquez M, Ganan-Calvo A. 2002. Micro/nano
675 encapsulation via electrified coaxial liquid jets. *Science* 295(5560):1695-8.

676 Maisanaba S, Pichardo S, Jordábeneyto M, Aucejo S, Cameán AM, Jos Á. 2014. Cytotoxicity and
677 mutagenicity studies on migration extracts from nanocomposites with potential use in food
678 packaging. *66(4):366-72.*

679 Manthey JA. 2006. Fourier transform infrared spectroscopic analysis of the polymethoxylated
680 flavone content of orange oil residues. *Journal of agricultural and food chemistry*
681 *54(9):3215-8.*

682 McCann JT, Li D, Xia Y. 2005. Electrospinning of nanofibers with core-sheath, hollow, or porous
683 structures. *Journal of Materials Chemistry* *15(7):735-8.*

684 McKee MG, Wilkes GL, Colby RH, Long TE. 2004. Correlations of solution rheology with
685 electrospun fiber formation of linear and branched polyesters. *Macromolecules*
686 *37(5):1760-7.*

687 Moomand K, Lim L-T. 2014. Oxidative stability of encapsulated fish oil in electrospun zein fibres.
688 *Food Research International* *62:523-32.*

689 Moomand K, Lim L-T. 2015a. Effects of solvent and n-3 rich fish oil on physicochemical properties
690 of electrospun zein fibres. *Food Hydrocolloids* *46:191-200.*

691 Moomand K, Lim L-T. 2015b. Properties of encapsulated fish oil in electrospun zein fibres under
692 simulated in vitro conditions. *Food and Bioprocess Technology* *8(2):431-44.*

693 Neo YP, Ray S, Easteal AJ, Nikolaidis MG, Quek SY. 2012. Influence of solution and processing
694 parameters towards the fabrication of electrospun zein fibers with sub-micron diameter.
695 *Journal of Food Engineering* *109(4):645-51.*

696 Neo YP, Ray S, Jin J, Gizdavic-Nikolaidis M, Nieuwoudt MK, Liu D, Quek SY. 2013. Encapsulation
697 of food grade antioxidant in natural biopolymer by electrospinning technique: A
698 physicochemical study based on zein–gallic acid system. *Food chemistry* *136(2):1013-21.*

699 O'Bryan CA, Crandall PG, Chalova VI, Ricke SC. 2008. Orange Essential Oils Antimicrobial
700 Activities against *Salmonella* spp. *Journal of Food Science* *73(6):M264–M7.*

701 Palangetic L, Reddy NK, Srinivasan S, Cohen RE, McKinley GH, Clasen C. 2014. Dispersity and
702 spinnability: Why highly polydisperse polymer solutions are desirable for electrospinning.
703 *Polymer* *55(19):4920-31.*

704 Quirós J, Boltes K, Rosal R. 2016. Bioactive Applications for Electrospun Fibers. *Polymer Reviews*
705 *56(4):631-67.*

706 Rieger KA, Birch NP, Schiffman JD. 2016. Electrospinning chitosan/poly (ethylene oxide) solutions
707 with essential oils: Correlating solution rheology to nanofiber formation. *Carbohydrate*
708 *Polymers* *139:131-8.*

709 Sugumar S, Singh S, Mukherjee A, Chandrasekaran N. 2016. Nanoemulsion of orange oil with non
710 ionic surfactant produced emulsion using ultrasonication technique: evaluating against food
711 spoilage yeast. *Applied Nanoscience* *6(1):113-20.*

712 Suppakul P, Miltz J, Sonneveld K, Bigger SW. 2003. Active Packaging Technologies with an
713 Emphasis on Antimicrobial Packaging and its Applications. *Journal of Food Science*
714 *68(2):408–20.*

715 Torres-Giner S, Gimenez E, Lagaron J. 2008. Characterization of the morphology and thermal
716 properties of zein prolamine nanostructures obtained by electrospinning. *Food*
717 *Hydrocolloids* *22(4):601-14.*

718 Torresalvarez C, González AN, Rodríguez J, Castillo S, Leosrivas C, Báezgonzález JG. 2016.
719 Chemical composition, antimicrobial, and antioxidant activities of orange essential oil and

720 its concentrated oils. 00:1-7.

721 Unlu M, Ergene E, Unlu GV, Zeytinoglu HS, Vural N. 2010. Composition, antimicrobial activity and
722 in vitro cytotoxicity of essential oil from *Cinnamomum zeylanicum* Blume (Lauraceae).
723 *Food & Chemical Toxicology An International Journal Published for the British Industrial
724 Biological Research Association* 48(11):3274-80.

725 Verghese K, Lewis H, Lockrey S, Williams H. 2015. Packaging's Role in Minimizing Food Loss and
726 Waste Across the Supply Chain. *Packaging Technology & Science* 28(7):603-20.

727 Wang B, Zheng H, Chang MW, Ahmad Z, Li JS. 2016. Hollow polycaprolactone composite fibers
728 for controlled magnetic responsive antifungal drug release. *Colloids & Surfaces B
729 Biointerfaces* 145:757-67.

730 Wen P, Zhu D-H, Wu H, Zong M-H, Jing Y-R, Han S-Y. 2016a. Encapsulation of cinnamon essential
731 oil in electrospun nanofibrous film for active food packaging. *Food Control* 59:366-76.

732 Wen P, Zhu DH, Feng K, Liu FJ, Lou WY, Li N, Zong MH, Wu H. 2016b. Fabrication of electrospun
733 polylactic acid nanofilm incorporating cinnamon essential oil/ β -cyclodextrin inclusion
734 complex for antimicrobial packaging. *Food Chemistry* 196:996-1004.

735 Xu X, Jiang L, Zhou Z, Wu X, Wang Y. 2012. Preparation and properties of electrospun soy protein
736 isolate/polyethylene oxide nanofiber membranes. *Acs Appl Mater Interfaces* 4(8):4331.

737 Yang J-M, Zha L-s, Yu D-G, Liu J. 2013. Coaxial electrospinning with acetic acid for preparing
738 ferulic acid/zein composite fibers with improved drug release profiles. *Colloids and
739 Surfaces B: Biointerfaces* 102:737-43.

740 Yao Z-C, Chang M-W, Ahmad Z, Li J-S. 2016a. Encapsulation of rose hip seed oil into fibrous zein
741 films for ambient and on demand food preservation via coaxial electrospinning. *Journal of
742 Food Engineering* 191:115-23.

743 Yao Z-C, Gao Y, Chang M-W, Ahmad Z, Li J-S. 2016b. Regulating poly-caprolactone fiber
744 characteristics in-situ during one-step coaxial electrospinning via enveloping liquids.
745 *Materials Letters* 183:202-6.

746 Ziani K, Fang Y, McClements DJ. 2012. Fabrication and stability of colloidal delivery systems for
747 flavor oils: Effect of composition and storage conditions. *Food Research International*
748 46(1):209-16.

749

750 **Tables**

751

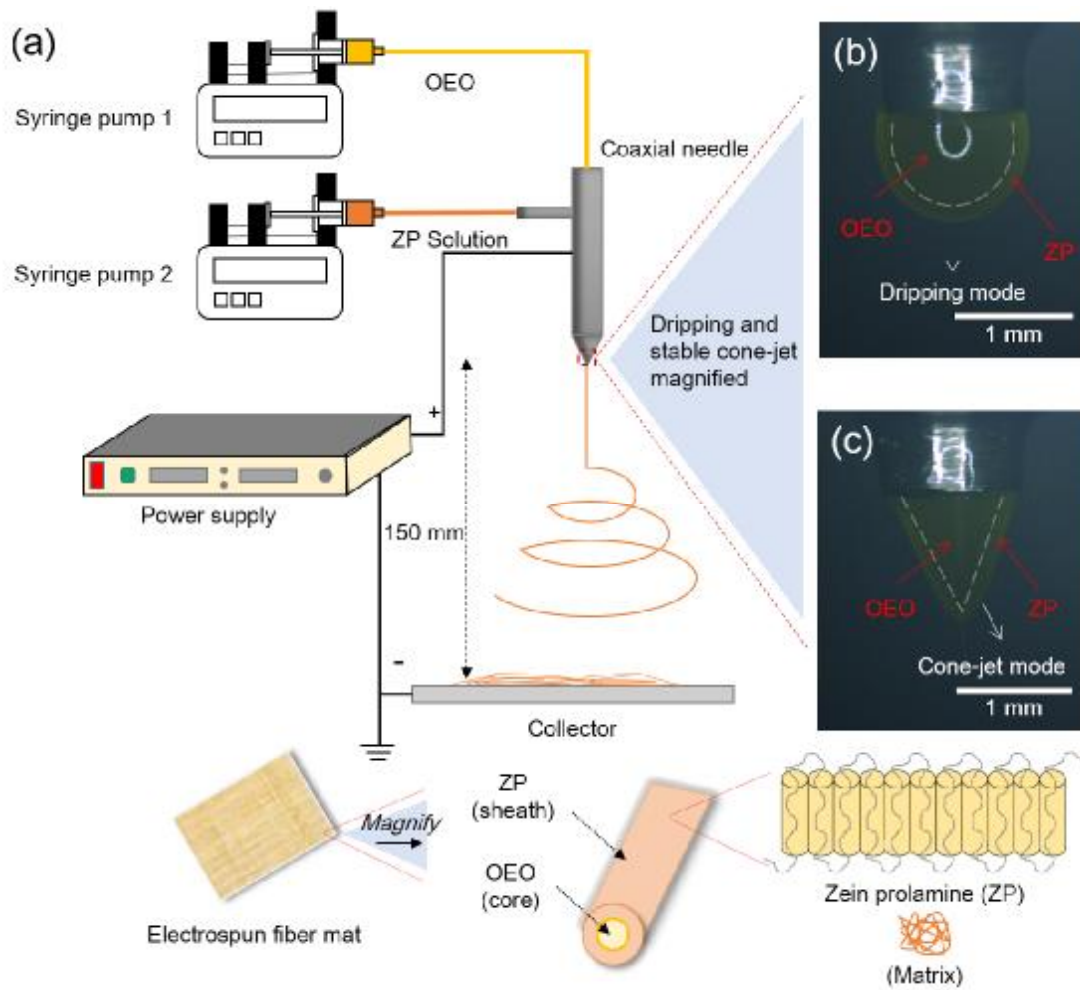
752 **Table 1.** Viscosity and electrical conductivity of solutions used in this study

753

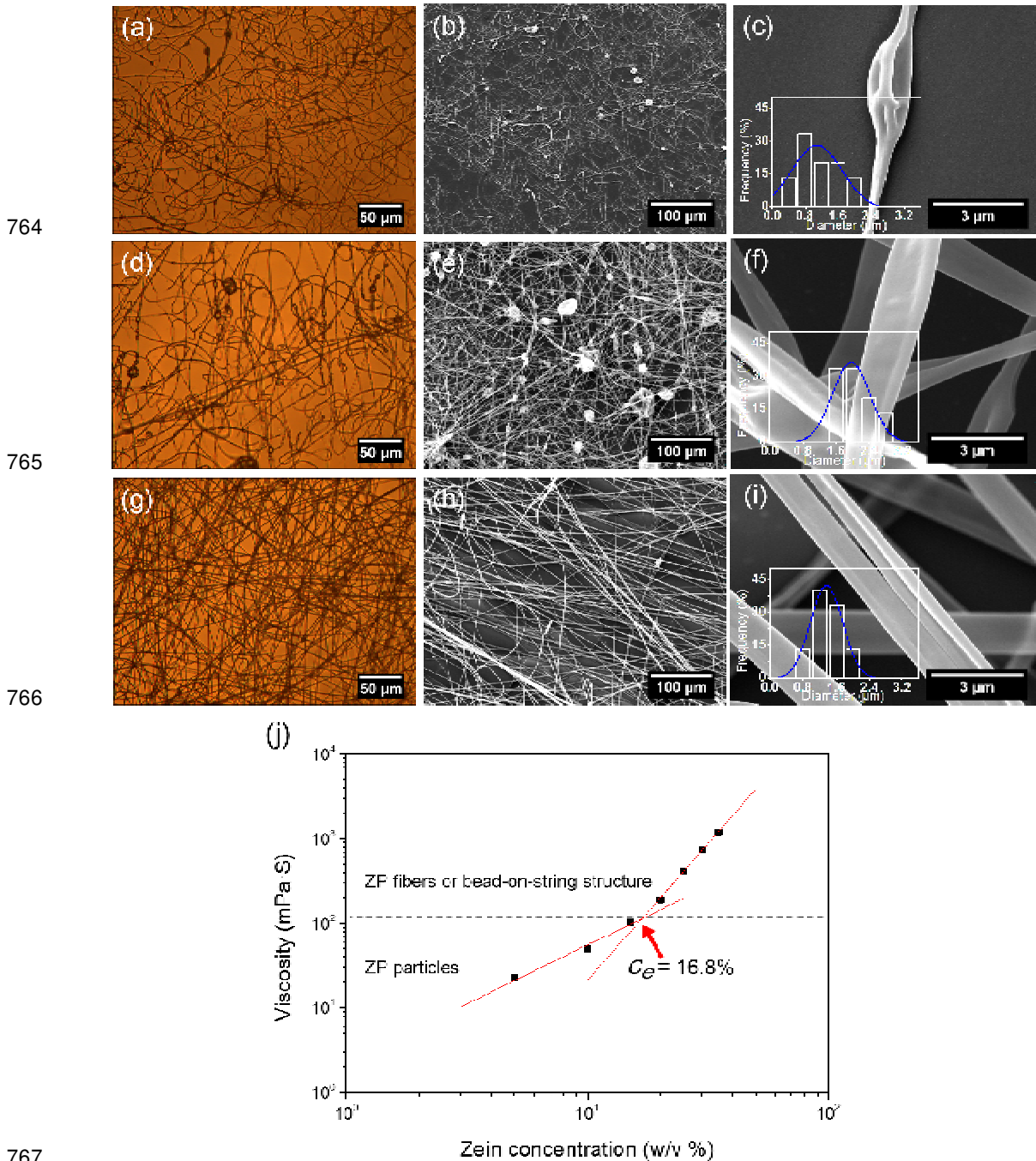
	25 w/v% ZP	30 w/v% ZP	35 w/v% ZP	OEO
Viscosity (mPa•S)	422.2±0.9	745.4±1.5	1197.0±3.0	6.7±0.5
Elec. Conduct. (μS/m)	625.6±0.2	611.2±0.5	599.5±0.6	<0.1

754

755



759 **Fig. 1.** (a) Schematic diagram of coaxial system used in this study. Inserts show two
 760 images exhibiting characteristic coaxial electrospinning modes; (b) dripping mode at 0
 761 kV and (c) cone-jet mode at 19 kV. [For both images, flow rate of the enveloping
 762 medium (ZP) = 2.0 mL/h, flow rate of the enveloped medium (OEO) = 1.5 mL/h]



767

768 **Fig. 2.** Optical micrographs of electrospun fibers obtained at ZP solution concentrations

769 of: (a) 25, (d) 30, and (g) 35 w/v%. Scanning electron micrographs of electrospun fibers

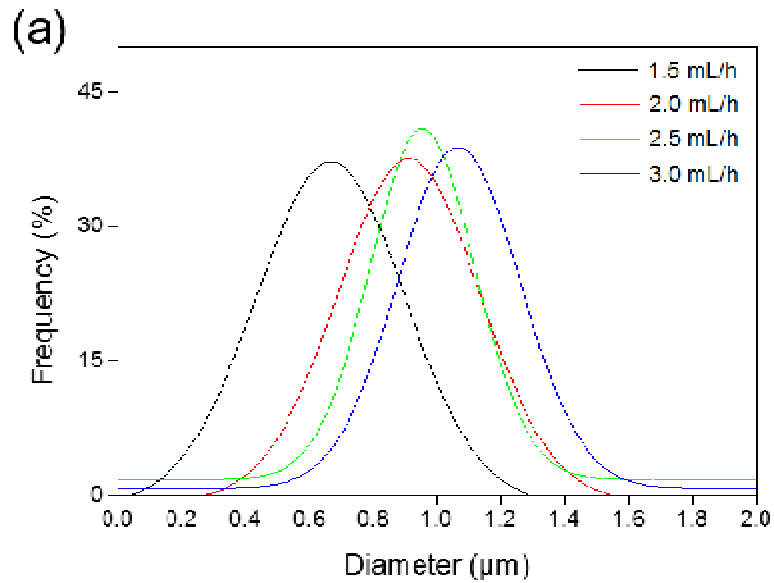
770 obtained at ZP solution concentrations of: (b) 25, (e) 30, and (h) 35 w/v%. Micrographs

771 (c), (f), and (i) are higher magnifications of (b), (e), and (h), respectively, with size

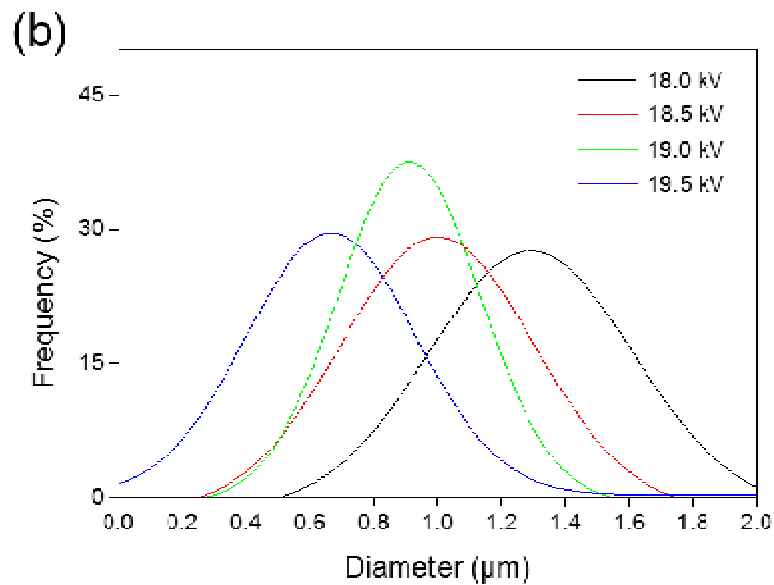
772 distribution insets. (j) Fiber forming dynamics as a function of ZP solution viscosity vs.

773 polymer (ZP) concentration.

774



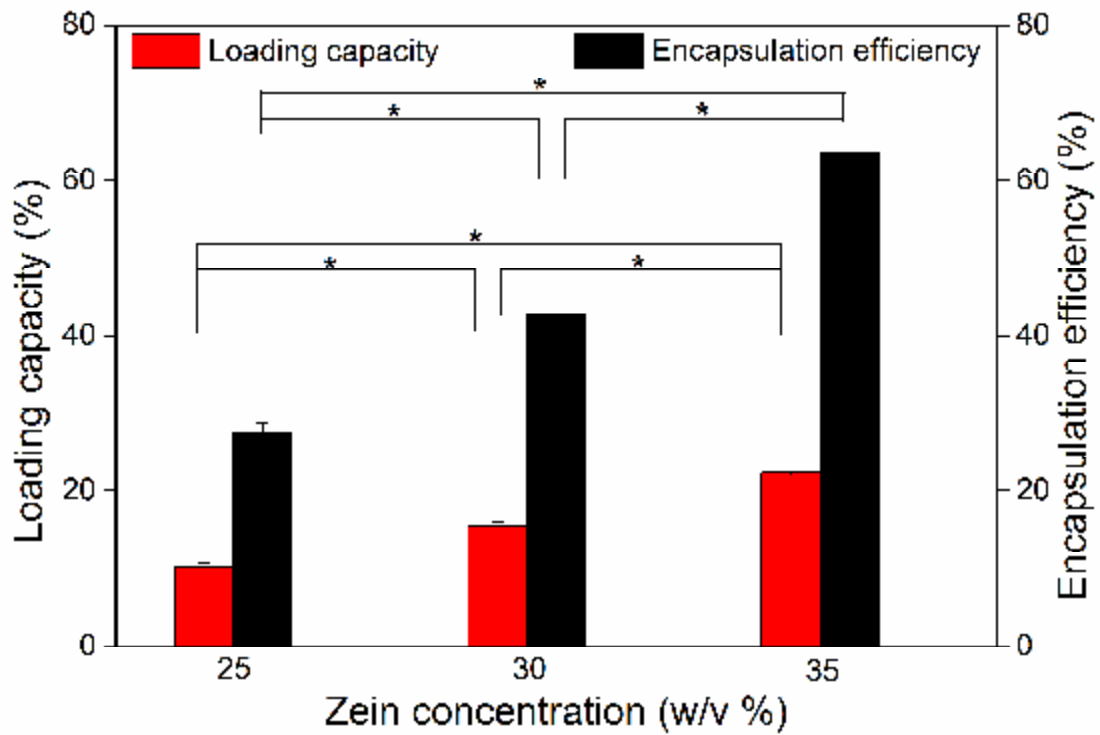
775



776

777 **Fig. 3.** Gaussian curves of fibers size distribution generated with different process
 778 parameters. (a) Effect of enveloping medium flow rate on mean fiber diameter.
 779 [experimental conditions: ZP solution concentration = 35 w/v%, enveloped medium
 780 flow rate (OEO) = 1.5 mL/h, applied voltage = 19.0 kV and collector distance = 12.0
 781 cm]. (b) Effect of applied voltage on mean fiber diameter. [experimental conditions: ZP
 782 solution concentration = 35 w/v%, flow rate of the enveloping medium (ZP) = 2.0 mL/h,
 783 flow rate of the enveloped medium (OEO) = 1.5 mL/h, and collector distance = 12.0
 784 cm].

785



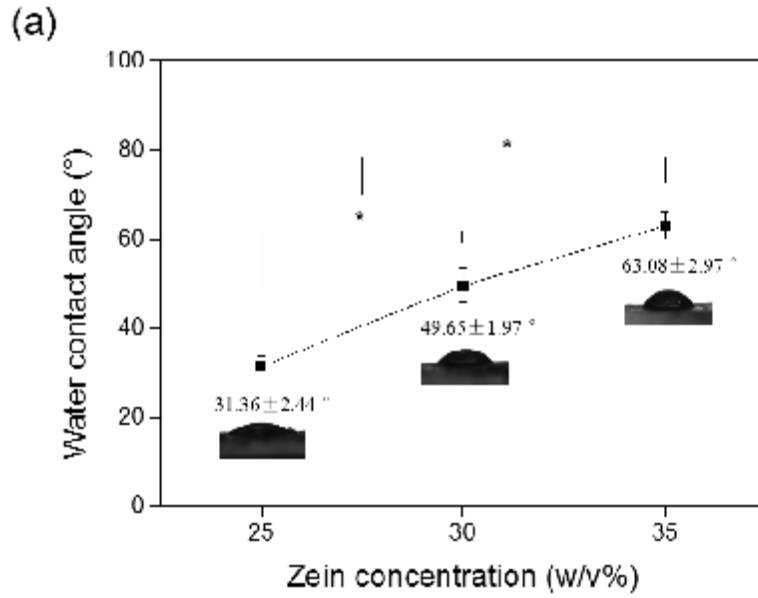
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787 **Fig. 4.** Loading capacity and encapsulation efficiency of OEO using ZP solutions

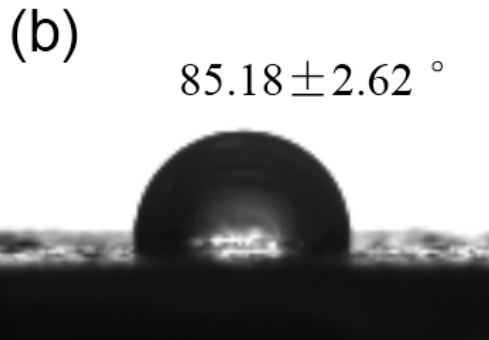
788 (during ES) with various concentrations. (*P<0.05)

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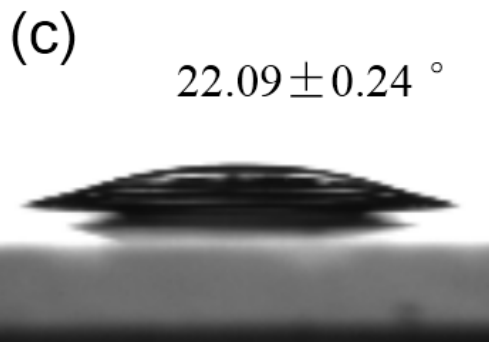
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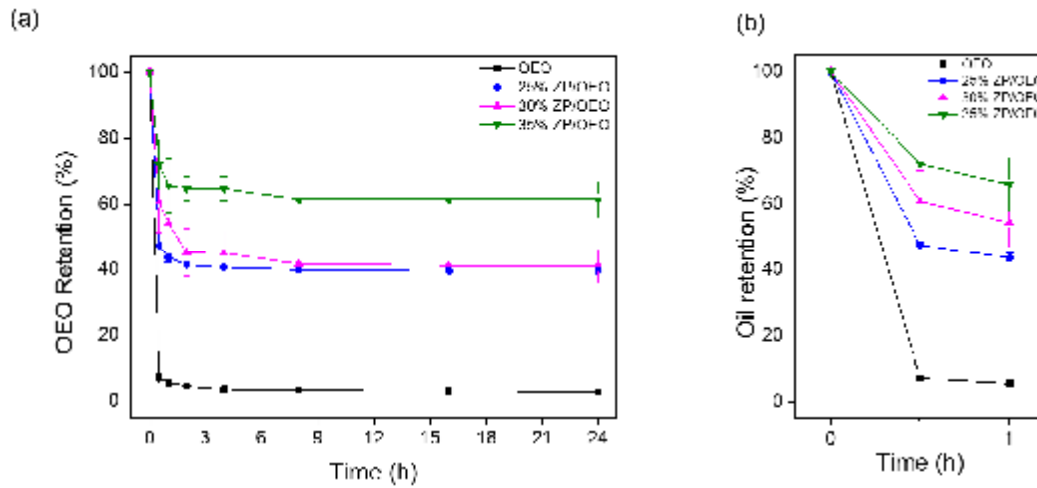
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794 **Fig. 5.** Water contact angles (WCAs) on fibrous membrane samples and OEO. (a)
 795 WCAs on electrospun ZP/OEO coaxial fibrous membranes prepared using various ZP
 796 solution concentrations (*P<0.05), (b) WCA on single needle electrospun ZP membrane,
 797 (c) WCA on pure OEO.

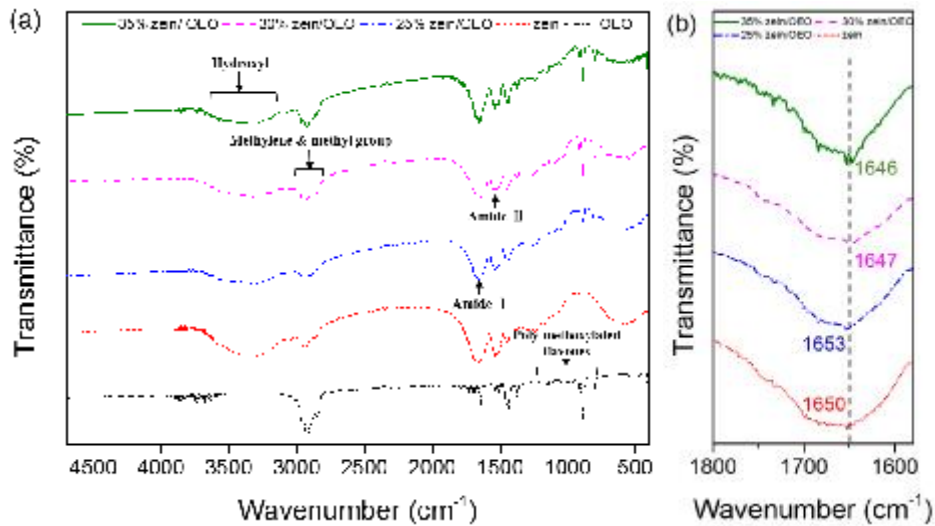
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800 **Fig. 6.** Retention of free OEO and encapsulated OEO in fiber during (a) 24h, (b) 1h.

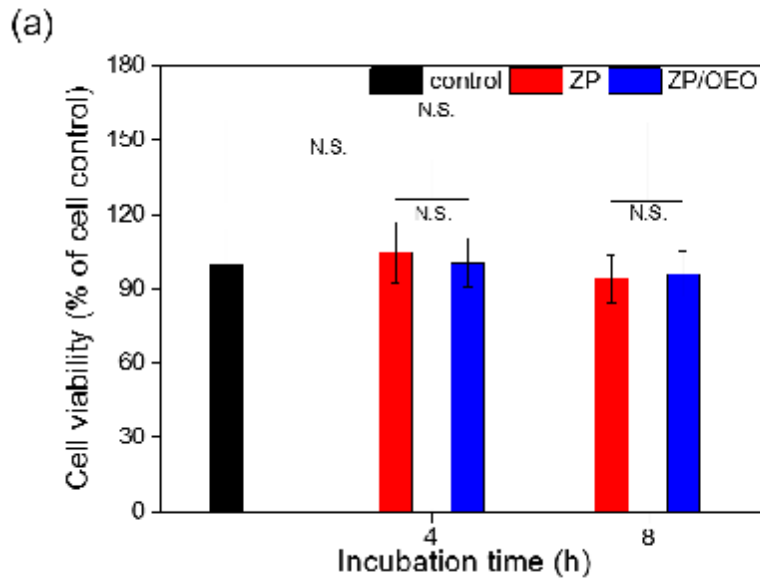
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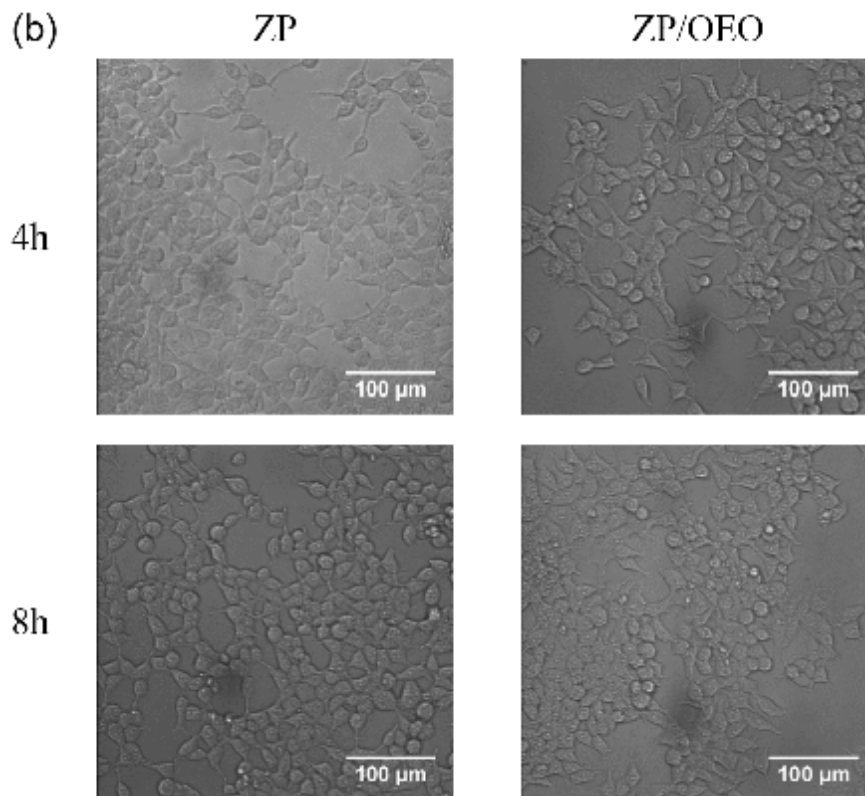
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803 **Fig. 7.** FTIR spectra of materials and samples in this study. (a) FTIR spectra of pure ZP
 804 electrospun membrane, pure OEO and ZP/OEO fibrous membranes fabricated with
 805 different ZP solution concentrations. (b) The shift in characteristic amide I band for ZP.

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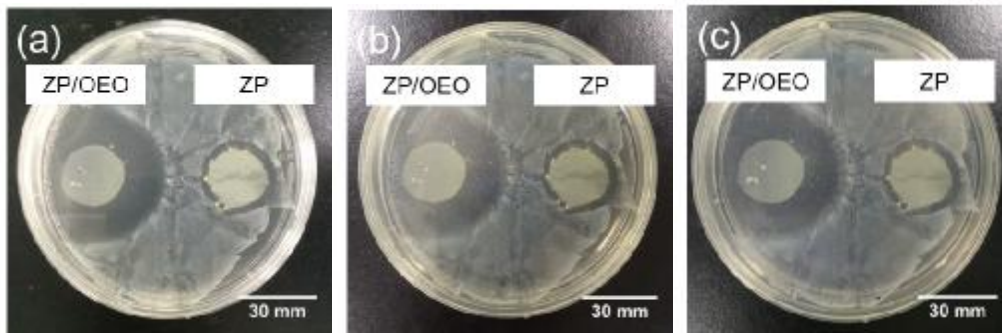


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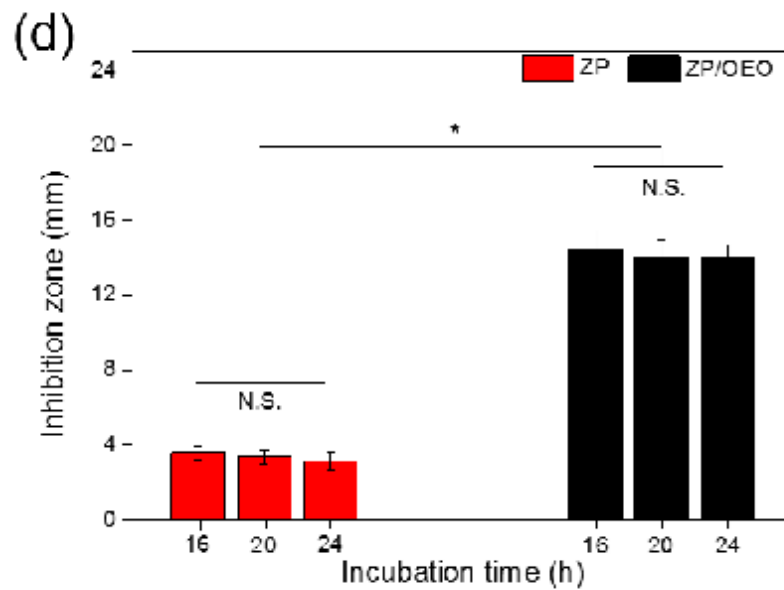
809 **Fig. 8.** Evaluating cell viability using CCK-8 assay. (a) CCK-8 test on electrospun ZP
 810 and ZP/OEO membranes after 4 and 8 hours cell culture. The viability of the control
 811 cells was set to 100%. (N.S. means no significant difference) (b) Optical micrographs
 812 showing cytocompatibility of ZP and ZP/OEO fibrous membranes incubated with
 813 HEK293T cells after 4 and 8 hours.

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818 **Fig. 9.** Inhibition zones (*E. coli*) generated using ZP membranes and 35 w/v % ZP/OEO
819 membranes at (a) 16 (b) 20 and (c) 24h. (d) Diameter of inhibition zones at various
820 assessment times. (N.S. means no significant difference; * $p < 0.05$, comparing inhibition
821 zone areas of ZP and ZP/OEO groups at identical time intervals).