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Anal. Chem., **Just Accepted Manuscript** • DOI: 10.1021/acs.analchem.0c02143 • Publication Date (Web): 29 Jul 2020

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Highly Doped Upconversion Nanoparticles for *In Vivo* Applications Under Mild Excitation Power

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4 **One of the major challenges in using upconversion nanoparticles (UCNPs) is to improve their**
5 **brightness. This is particularly true for *in vivo* studies, as the low power excitation is required to**
6 **prevent the potential photo toxicity to live cells and tissues. Here, we report that the typical**
7 **NaYF₄:Yb_{0.2},Er_{0.02} nanoparticles can be highly doped, and the formula of NaYF₄:Yb_{0.8},Er_{0.06} can**
8 **gain orders of magnitude more brightness, which is applicable to a range of mild 980 nm**
9 **excitation power densities, from 0.005 W/cm² to 0.5 W/cm². Our results reveal that the**
10 **concentration of Yb³⁺ sensitizer ions plays an essential role, while increasing the doping**
11 **concentration of Er³⁺ activator ions to 6 mol% only has incremental effect. We further**
12 **demonstrated a type of bright UCNPs 12 nm in total diameter for *in vivo* tumor imaging at a**
13 **power density as low as 0.0027 W/cm², bringing down the excitation power requirement by 42**
14 **times. This work re-defines the doping concentrations to fight for the issue of concentration**
15 **quenching, so that ultra-small and bright nanoparticles can be used to further improve the**
16 **performance of upconversion nanotechnology in photodynamic therapy, light-triggered drug**
17 **release, optogenetics, and night vision enhancement.**
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34 Upconversion materials can absorb two or more near-infrared (NIR) photons and emit shorter
35 wavelength luminescence in the visible and ultraviolet (UV) ¹⁻³. Such a fascinating anti-Stokes
36 property has led to a broad range of optoelectronics applications, including full-colour displays ⁴,
37 security inks⁵, photocatalysis ⁶, and photovoltaics ⁷. By taking the advantage of NIR deep penetration
38 through the tissue as well as their exceptional photo stability, long decaying lifetimes⁸, large anti-stoke
39 shifts and sharp emission spectra, the emerging field of lanthanide doped upconversion nanoparticles
40 (UCNPs) has attracted a great deal of interests in bio-imaging⁹⁻¹², light-controlled nanomedicine^{3, 13-16}
41 and NIR night vision enhancement ¹⁷.
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50 One of the major challenges to transform upconversion nanotechnology is to reduce the excitation
51 power requirement and improve the brightness of UCNPs. Due to the constraint of concentration
52 quenching, the dopant concentrations are restricted at relatively low levels, e.g. 20 mol% Yb³⁺ as
53 sensitizers and 2 mol% Er³⁺ or 0.5 mol% Tm³⁺ as activators ^{18, 19}, to minimize luminescence quenching
54 effects. In 2013, we reported that highly Tm³⁺-doped UCNPs can display exceptionally high brightness,
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4 where high excitation power (up to $\sim 10^6$ W/cm²) was necessary to mitigate concentration quenching
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6 ²⁰. Significant efforts have been made to improve the brightness of UCNPs by increasing the doping
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8 concentrations of sensitizers and activators²¹⁻²³. Remarkably, Steven Chu's group recently reported
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10 that highly Yb³⁺ and Er³⁺ doped nanocrystals exhibit a 150-fold enhancement at 8 W/cm² using an inert
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12 shell strategy²², and in parallel, the team led by Cohen, Chan, and Schuck at Berkeley reported that
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14 alloyed UCNPs can realize a deep-tissue imaging under the excitation power of 0.1 W/cm² ²¹.

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16 Low-power excitation is required for the safe *in vivo* applications, e.g. the power densities in the
17
18 range of 0.001 to 0.5 W/cm² are needed for bioimaging¹⁰, NIR-triggered drug release³, photodynamic
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20 therapy^{14, 24}, and night vision enhancement¹⁷. This gap between the high brightness and low power
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22 excitation becomes more evident when the size of UCNPs is within 15 nm, where the number of
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24 dopants per nanoparticles proportionally drops and surface quenching inevitably arises ^{25, 26}.

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26 Here, we find that the concentrations of both Yb³⁺ sensitizers and Er³⁺ activators can be further
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28 fine-tuned and gain the significant enhancement in the brightness of UCNPs for *in vivo* applications
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30 when only mild to ultra-low irradiance are required. We adopt here a series of controlled synthesis of
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32 core@shell@shell UCNPs (NaYF₄@NaYF₄:Yb_x,Er_y@NaYF₄) to exclude the size effect, so that the
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34 influences of sensitizers' and activators' concentrations on the brightness of multi-colour upconversion
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36 emission can be systematically compared and quantified at a range of laser irradiance. For example,
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38 under an irradiance of 0.082 W/cm², compared with the widely-used NaYF₄:Yb_{0.2},Er_{0.02} ones, the new
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40 formula of NaYF₄:Yb_{0.8},Er_{0.06}, yields the luminescence enhancements of 75.3, 40.8, 10.0, and 37.0
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42 folds in ultraviolet, violet, green, and red emissions, respectively. This has further guided us to achieve
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44 a new type of 12 nm highly-doped core-shell UCNPs with much enhanced red emissions for *in vivo*
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46 imaging using an excitation irradiance as low as 0.0027 W/cm².

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48 To quantify the roles of the concentrations of sensitizer ions and activator ions in enhancing the
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50 brightness of UCNPs, it requires the size of single UCNPs should be identical. Due to the difference
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52 in crystalline unit cells, the changes of Yb³⁺ concentrations, particularly at high levels, can significantly
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54 affect the overall size of nanoparticles when they are synthesized by the conventional coprecipitation
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56 method ²³. Therefore, we use an inert NaYF₄ core as the template and design a heterogeneous sandwich
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58 structure of inert-core@active-shell@inert-shell nanoparticles (**Fig. 1a-c**), so that the Yb³⁺ and Er³⁺
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4 concentrations can be arbitrarily tuned within the same volume of the active shell in the middle. The
5 role of the inert NaYF₄ shell is to minimize non-radiative energy loss by preventing the exciton energy
6 transfer to the surface defects and surrounding solvents via Yb³⁺ ions.
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10 As shown in **Fig. 1b-c**, transmission electronic microscopy (TEM) images show the typical
11 batches of highly uniform nanocrystals of NaYF₄, NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}, and
12 NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄, synthesized by the layer-by-layer hot injection method ²⁷. The
13 sizes of core, core@shell, and core@shell@shell nanoparticles are 18 nm, 28 nm and 34 nm,
14 respectively, indicating 5 nm active shell and 3 nm inert shell (**Fig. S1**). With the increase doping
15 concentration of both Yb³⁺ (80%) and Er³⁺ (6%) in the active shell, we get the highly doped
16 core@shell@shell nanoparticles with the similar size (**Fig. 1b-c**). The actual concentrations of Y³⁺,
17 Yb³⁺ and Er³⁺ of core@shell@shell nanoparticles are further characterized by using inductively
18 coupled plasma mass spectrometry. The molar ratios of Y/Yb/Er in active shell of
19 NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ and NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ have been calculated
20 to be 0.79:0.19:0.018 and 0.15:0.78:0.063, respectively, which confirms that rare earth compositions
21 of UCNPs consistent to their feeding ratio. Also, all the synthesized nanoparticles are uniform with
22 narrow size distributions (**Fig. S1**), which supports the following quantitative comparisons of the
23 upconversion luminescence intensities. As shown in **Fig. 1d**, the luminescence spectra of as-
24 synthesized UCNPs have four characteristic peaks at 379 nm (ultraviolet), 407 nm (violet), 540 nm
25 (green) and 650 nm (red), assigned to ⁴G_{11/2} → ⁴I_{15/2}, ²H_{9/2} → ⁴I_{15/2}, ²H_{11/2}/⁴S_{3/2} → ⁴I_{15/2} and ⁴F_{9/2} →
26 ⁴I_{15/2} transitions of Er³⁺, respectively. Quantitatively, highly doped
27 NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ nanoparticles result in 39, 24, 6.4, and 21 fold brightness
28 enhancements in ultraviolet, violet, green, and red, compared with the
29 NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ nanocrystals under the excitation power of 0.25 W/cm².
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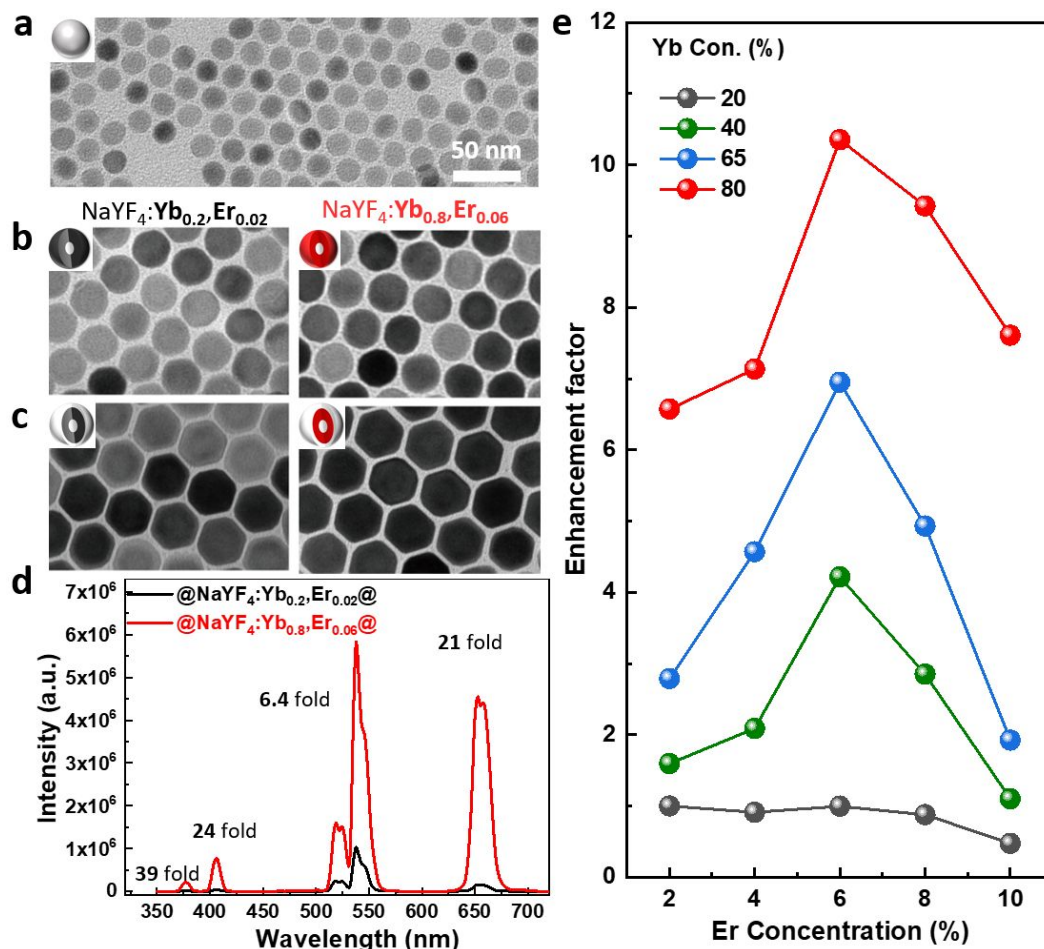


Figure 1. TEM images of NaYF₄ core (a), NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02} (b, left), NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06} (b, right), NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ (c, left), and NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ (c, right), the scale bar is 50 nm. (d) Luminescence spectra of NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ and NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ under the excitation power of 0.25 W/cm², (e) Integrated luminescence intensity enhancement of NaYF₄@NaYF₄:Yb_x,Er_y@NaYF₄ samples compared with NaYF₄@NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ under the excitation power of 0.25 W/cm².

We then systematically synthesize a series of 20 batches of UCNPs doped with different dopant combinations of sensitizer (x) and activator (y) and study their optical properties. We orthogonally apply four different Yb³⁺ concentrations ($x = 20\%$, 40% , 65% and 80%) and five different Er³⁺ dopant concentrations ($y = 2\%$, 4% , 6% , 8% and 10%). All the nanoparticles have the same structure and size as confirmed by the TEM results (Fig. S2-5). As shown in Fig. 1e, the brightness of UCNPs increases with an increase of Yb³⁺ from 20% to 80% when fixing the doping concentration of Er³⁺, which is due to both the elevated photon harvest efficiency of the sensitizers and the reduced distance between donor and acceptor, as energy transfer rate is proportional to d^{-6} in dipole–dipole interaction (d refers to the average donor–acceptor distance)²⁸. The luminescence intensity first enhances with ascended

Er³⁺ concentration from 2% to 6% and then declines with the Er³⁺ concentration above 6%, showing a sign of the cross-relaxation induced energy loss. By fixing the Er³⁺ concentration at 6%, we further increase the Yb³⁺ concentration to 94% (**Fig. S6**), and find that the luminescence intensity of NaYF₄@NaYbF₄:Er_{0.06}@NaYF₄ is lower than that of NaYF₄@NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ (**Fig. S7**), which is consistent to the previous report.²⁹ To further study the effect of Yb³⁺ concentration on the energy transfer process, we examine the time-resolved green emission of the samples with different Yb³⁺ concentrations. As shown in **Fig. S8**, the luminescence lifetime decreases from 252 to 99 μs as the Yb³⁺ concentration increases from 20% to 94%, which indicates the back-energy-transfer process from Er³⁺ to Yb³⁺ in the highly doped samples. Therefore, the optimal Yb³⁺ concentration at 80% is to balance the effects of increasing absorption and reducing back-energy-transfer.

The luminescence enhancement of UCNPs can be strongly power-dependent. As shown in **Fig. 2a**, when the excitation power density increases from 0.25 W/cm² to 0.5 W/cm², the enhancement factors slightly decrease from 39, 24, 6.4, and 21 folds to 23, 13, 3.7, and 19 folds, at the ultraviolet, violet, green, and red emission bands, respectively. When the excitation power density decreases to 0.005 W/cm², the enhancement by the highly doped UCNPs is more obvious, e.g. 16 folds at the green band (**Fig. 2b**). To further understand the brightness enhancement of highly doped UCNPs, we systemically conduct power dependent luminescence measurements in the range of 0.005 to 0.5 W/cm², integrate the emissions from different bandwidth (**Fig. S9**) and further calculated the enhancement factors, as shown in **Fig. 2c**. The emission intensity ratio at 407 nm increases from 13.0 to 49.0 when the irradiance decreases from 0.5 to 0.062 W/cm². Similarly, luminescence enhancement at 379 nm increases around 3 times and achieves 75.3 at the irradiance of 0.081 W/cm². Also, the brightness enhancement factors of green and red luminescence (540 nm and 650 nm) increase from 3.7 and 19.0 to 15.2 and 38.0, respectively, when the irradiance reduces from 0.5 to 0.016 W/cm². This trend is consistent with the increased probability of highly efficient energy absorption of the highly Yb³⁺-doped UCNPs at relatively low irradiance.

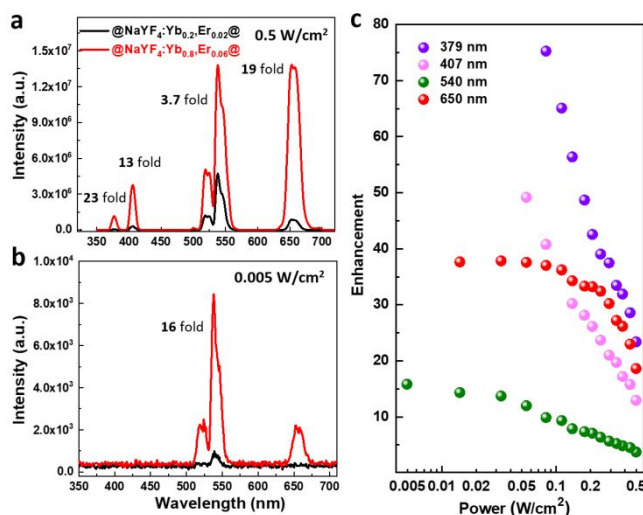


Figure 2. Luminescence spectra of $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$ and $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ under the irradiance of 0.5 W/cm^2 (a) and 0.005 W/cm^2 (b). (c) Comparison of power-dependent luminescence intensity enhancements between $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$ and $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ at UV (379 nm), violet (407 nm), green (540 nm), and red (650 nm) bands, respectively.

We determine that the sensitizers' concentration dominates the power-dependent properties, as shown in **Fig. 3**. For the highly Yb^{3+} -doped $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.02}@ \text{NaYF}_4$ nanoparticles, the brightness enhancement factors across all the emission bands significantly increase with the decrease of irradiance (**Fig. 3a**). For example, the enhancement factors of the UV emissions increase significantly from 17.1 to 52.5. In contrast, the irradiance has negligible effect in the brightness enhancement factors for the highly Er^{3+} -doped $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.06}@ \text{NaYF}_4$ nanoparticles (**Fig. 3b**). Similarly, with the optimal Yb^{3+} concentration of 80%, the increase of Er^{3+} doping concentration from 2% to 6% only slightly increases the luminescence with the enhancement factor around 1.8 (**Fig. 3c**). Also, the enhancement factors do not change with the excitation power density. These results suggest the increased NIR photon sensitization becomes critical to increase the brightness of highly doped UCNP s under the mild and low irradiance conditions.

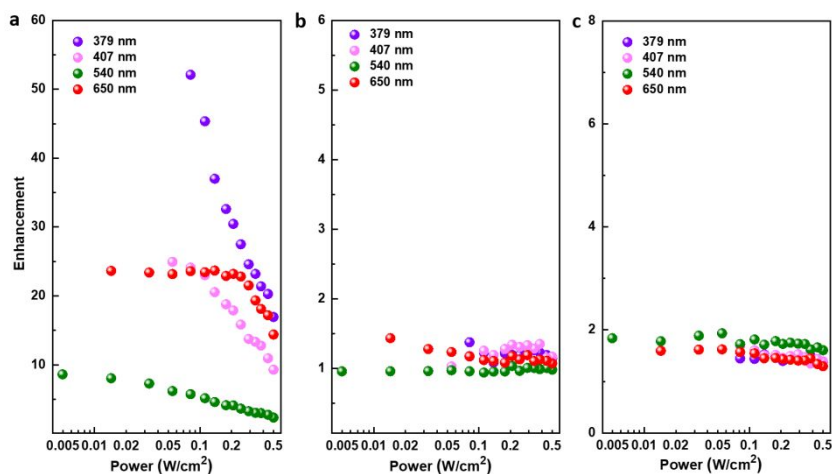


Figure 3. The power-dependent upconversion enhancement factors for $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.02}@ \text{NaYF}_4$ compared with $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ (a), $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.06}@ \text{NaYF}_4$ compared with $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ (b), and $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$ compared with $\text{NaYF}_4@ \text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.02}@ \text{NaYF}_4$ (c) at different emission bands.

We then survey the broad range of demonstrated *in vivo* applications using the conventional $\text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ UCNPs, as summarized in **Table 1**. We anticipate that the new formula of highly doped UCNPs will immediately offer at least one order of magnitude brightness enhancement or to achieve the same performance with a much reduced irradiance. For bioimaging, the red upconversion emissions are the preferable due to the less extinction through the tissues^{10, 30}, therefore the enhancement factor of 37 in red band using the $\text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$ will significantly improve the imaging sensitivity. Similarly, the improved photodynamic therapy treatment will be achieved by using the $\text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$, as the red emission from Er^{3+} -doped UCNPs is commonly used to active photosensitizer (Zinc phthalocyanine)^{14, 24}. For NIR light-triggered drug release, the green emission of $\text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ could be used to photolysis Roussin's black salt to generate NO under the excitation power of 5-30 W/cm²^{3, 31}. Also, relatively high excitation power (0.5-400 W/cm²) is needed for $\text{NaYF}_4:\text{Yb}_{0.2}, \text{Er}_{0.02}@ \text{NaYF}_4$ to generate the strong green light for optogenetics applications^{13, 32}. With the usage of $\text{NaYF}_4:\text{Yb}_{0.8}, \text{Er}_{0.06}@ \text{NaYF}_4$, the excitation power could be significantly reduced for safety *in vivo* drug delivery and optogenetics applications. Recently, Ma et al. developed ocular injectable photoreceptor-binding UCNPs to extend the mammalian visual spectrum into the NIR range under the excitation power of 0.0016 W/cm²¹⁷. We anticipate the new doping formula will improve the green emission for around 15 times and significantly improve the

sensitivity to the NIR light.

Table 1. A summary of the anticipated improvements for the highly doped UCNPs in bio applications

Recommended applications	Upconversion nanoparticles	Desirable emission band	Irradiance range	Ref.	Anticipated improvement if using the new doping formula
<i>In vivo</i> bio-imaging	NaYF ₄ :Yb _{0.2} ,Er _{0.02}	Red (600 ~ 700 nm)	0.12 W/cm ²	³⁰	38 times luminescence enhancement
Photodynamic therapy	NaYF ₄ :Yb _{0.2} ,Er _{0.02}	Red (~650 nm)	0.39-0.415 W/cm ²	^{14, 24}	26 times luminescence enhancement or reduce the irradiance to < 0.1 W/cm ²
Drug release and delivery	NaYF ₄ :Yb _{0.25} ,Er _{0.02}	Green (510 ~ 560 nm)	0.5-400 W/cm ²	³¹	~ 15 times luminescence enhancement or reduce the irradiance to < 0.5 W/cm ²
Optogenetics	NaYF ₄ :Yb _{0.2} ,Er _{0.02} @NaYF ₄	Green (510 ~ 560 nm)	0.44-140 W/cm ²	^{13, 32}	~ 10 times luminescence enhancement or reduce the irradiance to < 0.8 W/cm ²
Night vision enhancement	NaYF ₄ :Yb _{0.2} ,Er _{0.02} @NaYF ₄	Green (~550 nm)	0.0016 W/cm ²	¹⁷	~ 15 times luminescence enhancement

We further validate the advantage of the highly doped UCNPs for *in vivo* tumor imaging. In this experiment, as ideal nanoparticles with the smaller size are preferred due to higher efficiency in cargos delivery, and their improved body clearance and biocompatibility³³, we simplify our design into NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ so that smaller sized highly doped UCNPs can be synthesized. The NaYF₄:Yb_{0.8},Er_{0.06} active cores display a narrow size distribution with an average diameter of 8.6 nm, and the final size of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ is measured to be 11.9 nm (**Fig. S10a-b**), smaller than the size of dye-labelled IgG antibody³⁴. It should be noted that the formula of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ UCNPs displays the enhanced emission compared with that with low doping concentrations (**Fig. S10c**), suggesting that the optimal concentrations of Yb³⁺ and Er³⁺ ions are independent on the size of the nanoparticles.

To demonstrate the improved brightness and tissue penetration ability of the 12 nm highly doped UCNPs, we first test them underneath the pork tissue (**Fig. S11**). As shown in **Fig. 4a-b**, using an irradiance of 0.5 W/cm², the strong 660 nm band upconversion image of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ can be detected at a tissue depth of 4.0 mm, while the signal of conventional

NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ UCNPs can only penetrate 1.0 mm. Quantitatively, the signal to noise ratio (SNR) of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ covered by 1 mm pork tissue is around 20, which is 5 times higher than the SNR of NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ UCNPs (**Fig. 4c**). The penetration ability of green luminescent signals from both NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ and NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ is relative weak, as the green SNR of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ covered by 1 mm pork tissue is 6.1 while the SNR of NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ UCNPs is only 1.5 (**Figure S12**).

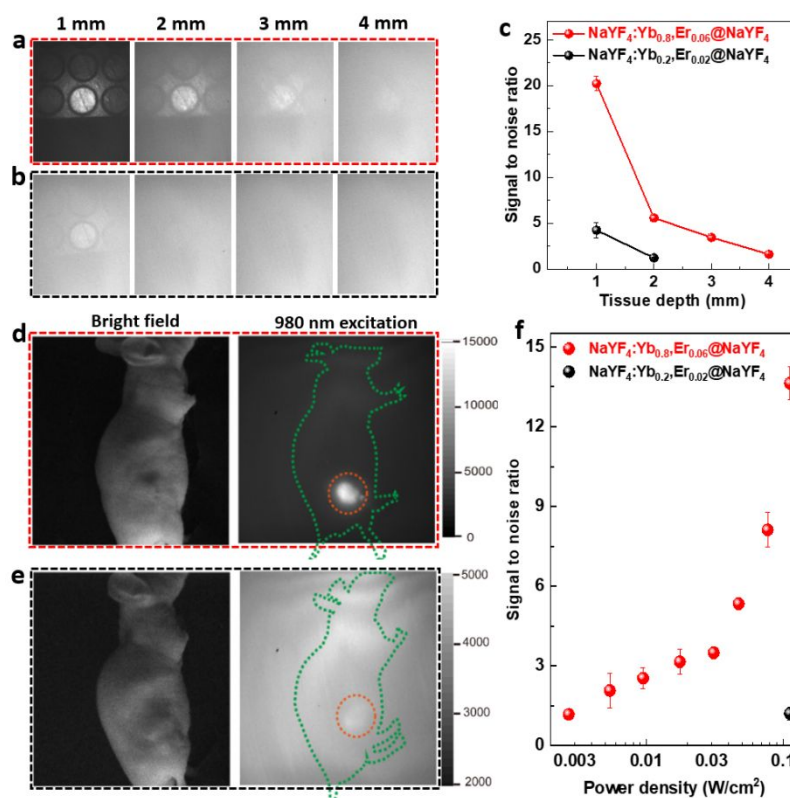


Figure 4. Luminescence imaging of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ (**a**) and NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ (**b**) at 660 ± 13 nm under different thickness of pork tissue. (**c**) Quantitative analysis of luminescent signal to noise ratio. *In vivo* tumor imaging of mice injected with NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ (**d**) and NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ (**e**) with the 980 nm laser intensity of 0.112 W/cm². (**f**) The power-dependent signal to noise ratio of the tumor site injected with the upconversion contrast agents.

To demonstrate NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ UCNPs as a more efficient contrast agent for bio imaging, we perform an *in vivo* tumor imaging experiment in the mouse model. As shown in **Fig. 4 d-e**, the tumor site shows an obvious luminescence signals after the administration of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ under the excitation power density of 0.112 W/cm², while the tumor site injected with NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ only shows a quite weak signal. Further reducing the excitation power, the luminescence signals of both samples becomes weaker (**Fig. S13**). The minimum

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4 excitation laser intensity of 0.112 W/cm² is required and the signals are barely distinguished from
5 background for the tumor area injected with NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ UCNPs. In contrast, though
6 the irradiance decreases from 0.112 to 0.0027 W/cm², the NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ UCNPs are still
7 detectable with a SNR of 1.4, as shown in **Fig. 4f**. The new formula of NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄
8 UCNPs allows an extremely low excitation power density of 0.0027 W/cm² to ignite the marginal area
9 of tumor. This intensity is sufficiently low for their safety usage in the eye region ¹⁷, which is
10 potentially useful for mammalian vision repair and enhancement. The reduced dependency of UCNPs
11 on the high excitation power is prospective for non-invasive in vivo imaging to avoid the serious
12 damage in biological tissues.

13
14 In conclusion, we identified that 80% Yb³⁺ sensitizers and 6% Er³⁺ activators as the optimal
15 concentrations to yield the highest brightness of UCNPs when mild irradiance of 0.005 to 0.5 W/cm²
16 is required for many in vivo bio applications. The optimized formula leads to more than one orders of
17 magnitude enhancements of the upconversion emissions. We further realized the controlled synthesis
18 of 12 nm NaYF₄:Yb_{0.8},Er_{0.06}@NaYF₄ for in vivo tumor imaging with 980 nm excitation irradiance as
19 low as 0.0027 W/cm². This work suggests the many recently demonstrated applications of the
20 conventional NaYF₄:Yb_{0.2},Er_{0.02}@NaYF₄ UCNPs in photodynamic therapy, light-triggered drug
21 release, optogenetics, and night vision enhancement will immediately benefit by achieving at least one
22 order of magnitude better performance or significantly reduced power requirement to improve the
23 safety concerns associated with high power irradiance.

24 **Associated Content**

25 Supporting Information

26 The Supporting Information is available on the ACS Publications website including:

27 Detailed experiment sections, UCNPs synthesis, TEM images and size distribution histograms,
28 luminescent spectra, integrated luminescent signals, In vitro and in vivo luminescence images

29 **Acknowledgement**

30 We thank S. Lindsay and C. Shen in Microscope Unit at Macquarie University for TEM
31 characterization. This project is financially supported by Australia-China Joint Research Centre for
32 Point-of-Care Testing (ACSRF65827, SQ2017YFGH001190), Science and Technology Innovation
33 Commission of Shenzhen (KQTD20170810110913065), National Natural Science Foundation of
34

China (NSFC, 61729501, 51720105015). D. L. and Y. L. acknowledge the financial support from China Scholarship Council scholarships (Du Li: No. 201506630038; Yongtao Liu: No. 201607950010.)

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