

Immunoisolation of pancreatic B cells by microencapsulation

An in vitro study

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Summary. The selective permeability of alginate microcapsules, containing isolated rat islets of Langerhans or insulin secreting RINm5F cells, was investigated in vitro. An increase in insulin release was observed when microencapsulated islets were stimulated by glucose + theophylline, and when microencapsulated RINm5F cells were stimulated by arginine + theophylline. These findings demonstrate the permeability of the microcapsule membrane to these B-cell secretagogues and to insulin. Immunoisolation of RINm5F cells by microencapsulation was assessed using a ⁵¹chromium cytotoxicity test. Significant ⁵¹Cr release was observed when non-encapsulated cells were incubated with complement and either the serum of a rabbit immunized with RIN cells or the se-

ra of two patients with recently diagnosed Type 1 (insulin-dependent) diabetes. This effect was not observed with encapsulated cells. Both free and encapsulated cells released 80% of their initial radioactivity when incubated in the presence of HCl. These results clearly demonstrate pancreatic cell immunoisolation by microencapsulation. They also provide a method for the in vitro evaluation of the functional characteristics of microcapsules, in terms of both insulin permeability and immunoprotection.

Key words: Microencapsulation, RINm5F cells, complement fixing cytotoxic antibodies, immunoprotection, bioartificial pancreas.

Microencapsulation of islets of Langerhans [1] has been proposed as a "bioartificial pancreas", whose function is to protect the graft by a membrane permeable to glucose and insulin but not to antibodies or lymphocytes [2]. Both in vitro [1, 3] and in vivo studies [1, 4] demonstrated that encapsulated islets (1) can be cultured for several weeks, (2) can secrete insulin in response to glucose with kinetics compatible with closed-loop insulin delivery, and (3) can correct hyperglycaemia in non syngeneic diabetic rats for several months.

Compared to other systems described so far, the microencapsulation technique devised by Lim and Sun for pancreatic islets has one great advantage as a potential bioartificial pancreas: unlike devices using cuprophane type artificial membranes, it allows microcapsule implantation without a vascular access [2]. However, with this technique, it is more difficult to define the molecular cut-off of the capsule membrane, which will control its selective permeability. The latter parameter is important, since the membrane is assumed to be permeable to glucose and insulin, but not to the factors responsible for immune rejection of the transplanted tissue. On the other hand, a protection against the cytotoxic activity of antibodies directed against pancreatic beta cells might

also be required for islet transplantation in Type 1 (insulin-dependent) diabetic patients, since complement-fixing islet cell cytotoxic antibodies are spontaneously present in many of these patients [5, 6].

The aim of this work was therefore to determine whether microencapsulation is able to efficiently protect pancreatic B cells against cytotoxic antibodies; if confirmed, such immunoprotection would validate the concept of cell immunoisolation in a bioartificial pancreas. We used an in vitro approach in this study.

Materials and methods

Pancreatic islets of Langerhans and RINm5F cells

Pancreatic islets were isolated from adult Wistar rats by the collagenase method [7]. The RINm5F cell line, a gift of H. Oie, was maintained in monolayer culture in our laboratory for more than 1 year in RPMI 1640 medium (Gibco Laboratories, Grand Island, New York) supplemented with heat-inactivated 10% fetal calf serum, 2 mmol L-glutamine, 100 U/ml penicillin and 100 µg/ml streptomycin.

Microencapsulation procedure

Islets or RINm5F cells were encapsulated as described by Goosen et al. [8] with slight modifications. Briefly, islets of Langerhans were en-

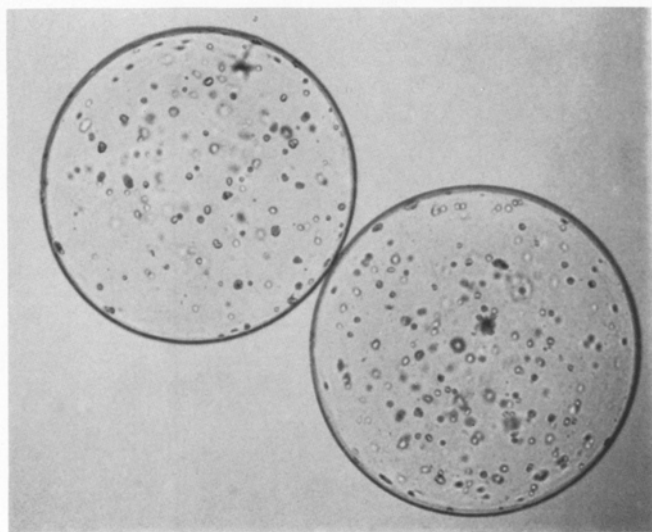


Fig. 1. Microencapsulated RINm5F cells 24 h after preparation. Note the absence of any cell grown outside the capsule

capsulated immediately after isolation. RINm5F cells were detached from culture flasks by incubation for 10 min at 37 °C with calcium and magnesium free Hank's balanced salt solution (Flow Laboratory, Rockville, Maryland). Four hundred islets, or 4×10^6 RIN cells were suspended in 5 ml of an 1.5% sodium alginate solution (Kelco, Merck, Rahway, New Jersey). Alginate droplets containing the islets or cells were formed by syringe pump extrusion under an air jet, and collected for 5 min in 1.1% calcium chloride solution to form calcium alginate gel to entrap the cells. The calcium alginate beads were successively coated by washing with L-polylysine (MW 50000, Sigma, St. Louis, Missouri), dissolved at a 5 mg/10 ml concentration in 2-(N-cyclohexylamino) ethan-sulfuric acid (CHES) buffer (Sigma), for 6 min and with sodium alginate 0.075% for 4 min. The alginate gel inside the microcapsule was liquefied by washing with 0.025 mol sodium citrate, pH 7.4 for 16 min, and with 0.05 mol sodium citrate for 6 min. Microcapsules containing islets and RIN cells were washed three times with physiological saline. The islets were transferred into Minimal Eagle Medium (MEM medium, Gibco, Paisley, Scotland), containing 10% fetal calf serum, 2 mmol glutamine, 1 mmol sodium pyruvate, 0.814 mg/l non essential aminoacids and antibiotics, and the cells, into RPMI 1640 culture medium. Fig. 1 represents microcapsules (mean size = 500 μ m diameter) containing RINm5F cells, 24 h after encapsulation, demonstrating that all the cells were inside the microcapsules.

Assessment of glucose, arginine, and insulin permeability

Stimulation of free and encapsulated islets. After 18 h of culture at 37 °C in 6% CO₂, free or encapsulated islets were incubated in wells of microtest plates (10 islets/well), and washed four times with 250 μ l basal medium (MEM medium, containing 5.5 mmol glucose). During each washing, free and encapsulated islets were left in the medium for 10 min to remove insulin which might have built up during the previous culture period. After completion of the washing, free and encapsulated islets were incubated for 30 min in the basal medium and the supernatant was then collected for determination of basal insulin secretion. Both free and encapsulated islets were subsequently washed four times with stimulatory medium, (MEM medium containing 16.5 mmol glucose + 5.5 mmol theophylline); after 30 min incubation in this medium, the supernatant was collected for determination of stimulated insulin secretion.

Stimulation of free and encapsulated RIN cells. The procedure used was similar to that described above except that: (1) Encapsulated cells

were stimulated after 10 days of culture in RPMI 1640 medium. (2) Arginine was used as a secretagogue, since RINm5F cells do not respond to glucose [9]. The stimulatory medium was therefore MEM Eagle medium containing 20 mmol arginine + 5.5 mmol theophylline, and (3) incubation periods in basal and stimulatory medium each lasted for 1 h. In this experimental design, the same batches of free or encapsulated islets or RINm5F cells were therefore sequentially incubated in basal and stimulatory medium to assess the response to the secretagogues. This was important in the case of encapsulated RINm5F cells since the number of cells might vary from one capsule to the other.

Insulin determination. Samples were stored at -20 °C until insulin determination. The insulin concentration was assayed by the radio-immunological method using rat insulin as standard and double anti-body separation [10].

In vitro assessment of immunoprotection

These experiments were performed on encapsulated RINm5F cells cultured for 2 to 4 days, and free cells were used as control. Immunoprotection of microencapsulated RINm5F cells was assessed by an assay for release of ⁵¹Cr, modified from Sai [6]. Free cells were re-suspended in RPMI 1640 medium, to a cell density of 2×10^6 cells/ml, and 500 μ l of the cell suspension was incubated at 37 °C under 6% CO₂ for 1 h with 100 μ l ⁵¹Cr sodium chromate (Amersham France, 1 mCi/ml). Encapsulated RIN cells were allowed to sediment, and the supernatant was discarded. The pellet, i.e. about 1 ml of capsules containing cells, was incubated for 2 h with 200 μ l of the sodium chromate solution. Incubation was followed by 4 washing steps, as described above, to eliminate free ⁵¹Cr. It was verified that chromium uptake by empty capsules was negligible compared to that obtained with capsules containing cells (264 ± 98 cpm, $n=6$, vs 3289 ± 193 cpm, $n=5$, the latter comprising five different preparations of capsules seeded with RINm5F cells). Aliquots of labelled free or encapsulated cells were placed in 5 ml plastic test tubes (5×10^3 cells in 100 μ l medium, or 100 μ l of capsules/tube), and incubated for 1 h at 37 °C under 6% CO₂. Twenty μ l of control or immune sera (see below) were then added to each tube. After incubation for 45 min in a thermostated waterbath under slow shaking, (1 shake/s), 80 μ l of guinea pig complement (diluted three times with culture medium) (Cederlane, Eurobio Paris, France) were added to each tube, and the tubes were incubated for the next hour. The final volume in each tube was thus 200 μ l. The tubes were subsequently centrifuged for 10 min at 1000 rev/min, and radioactivity was determined with a gamma counter (Kontron-Intertechnics, Basel, Switzerland) both in the 100 μ l of supernatant and in the 100 μ l pellet remaining in the tube. Maximum chromium release was determined by incubating the free or encapsulated cells with 100 μ l of distilled water acidified with HCl to pH 2. For determination of non-specific chromium release, RPMI 1640 medium was used instead of serum and complement; the effect of complement alone was also determined by replacing the serum with 20 μ l RPMI 1640 medium during the 45 min incubation; lastly, the effect of heat inactivation of the complement (40 min heating at 56 °C) was assessed.

Control and immune sera consisted of (1) the serum of a normal rabbit (Fauve de Bourgogne, Lessieu, Bray-Lu, France); (2) the serum of the same rabbit after immunization with RINm5F cells, obtained by three subcutaneous injections of 10^6 cells in 500 μ l culture medium with 500 μ l of Freund's adjuvant (one injection every 2 weeks); (3) the sera of six control human subjects and (4) the sera of two recently diagnosed Type 1 (insulin-dependent) diabetic patients. All sera were complement inactivated by heating for 40 min at 56 °C.

Expression of results. The sum of the radioactivities present in the supernatant and the pellet yielded the initial total radioactivity. This was of particular interest in the case of capsules, in which the amount of radioactivity might have varied from one tube to the other. With this

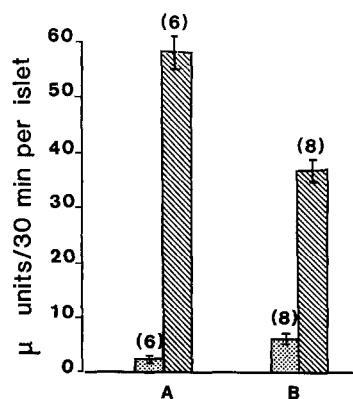


Fig. 2. Insulin release by free islets (A) and microencapsulated islets (B) after 30 min incubation in basal medium (dotted columns) or stimulatory medium (hatched columns). Number of separate experiments are given in parentheses

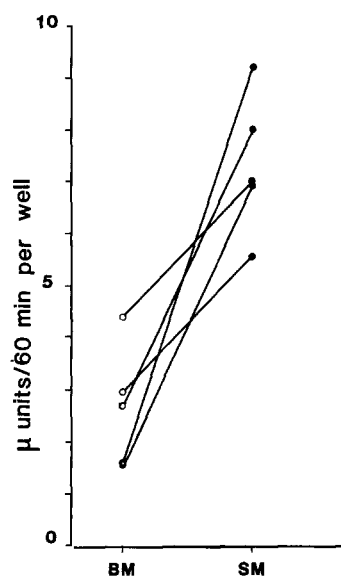


Fig. 3. Insulin release in five separate experiments, by encapsulated RINm5F cells, after 60 min in basal medium (open circles) or in stimulatory medium (closed circles). Each point represents the mean of at least 4 incubation wells

procedure, however, it was possible to determine exactly, for each tube, the percentage of initial radioactivity released under the different incubation conditions by using the formula:

$$^{51}\text{Cr Release (\%)} = \frac{\text{radioactivity in } 100 \mu\text{l supernatant} \times 2}{\text{radioactivity in } 100 \mu\text{l supernatant} + \text{radioactivity in } 100 \mu\text{l pellet}} \times 100$$

A cytotoxic index was also calculated, taking into account, for each experiment, the maximal ^{51}Cr release (in the presence of HCl) and the nonspecific ^{51}Cr release (after incubation with RPMI culture medium), according to the following formula:

$$\frac{\begin{matrix} ^{51}\text{Cr Release with} \\ \text{serum tested} \end{matrix} - \begin{matrix} ^{51}\text{Cr Release with} \\ \text{RPMI} \end{matrix}}{\begin{matrix} ^{51}\text{Cr Release with} \\ \text{HCl} \end{matrix} - \begin{matrix} ^{51}\text{Cr Release with} \\ \text{RPMI} \end{matrix}} \times 100$$

Statistics. In each experiment, each set of incubation was tested at least in quadruplicate, allowing to calculate mean values; these values

Table 1. ^{51}Cr Chromium release from free or encapsulated RINm5F cells, under different incubation conditions

	Free cells	Microencapsulated cells
HCl	91 ± 2 (13)	76 ± 3 (11)
RPMI	13 ± 2 (13)	15 ± 3 (11)
Complement	11 ± 1 (7)	22 ± 3 (7)
Normal rabbit + complement	11 ± 2 (6)	22 ± 3 (6)
Control human subjects		
+ heat inactivated complement	8 ± 1 (6)	9 ± 2 (3)
+ complement	9 ± 1 (6)	13 ± 4 (3)
Immune rabbit		
+ heat inactivated complement	10 ± 1 (8)	27 ± 3 (6)
+ complement	57 ± 8 (8)	18 ± 2 (6)
Type 1 patient A		
+ heat inactivated complement	20 ± 6 (6)	17 ± 5 (6)
+ complement	57 ± 10 (6)	15 ± 6 (6)
Type 1 patient B		
+ heat inactivated complement	15 ± 4 (6)	16 ± 6 (6)
+ complement	47 ± 11 (6)	15 ± 6 (6)

Results are expressed as the percentage of initial radioactivity released after 1 h 45 min incubation, as mean ± SEM, with number of separate experiments in parentheses

were used to calculate final data which are given as mean ± SEM of different experiments (namely different capsule preparations), whose number is given between parentheses. Statistical significance was evaluated by paired, two-tailed Student's t-test [11].

Results

Permeability to glucose, arginine, theophylline and insulin

Insulin secretion by free and encapsulated islets of Langerhans in response to glucose + theophylline. Both free and encapsulated islets responded to incubation in the stimulatory glucose + theophylline medium by significantly increasing their insulin release ($p < 0.001$, Fig. 2), although the magnitude of the response seemed to be larger in case of free islets.

Insulin secretion by encapsulated RINm5F cells in response to arginine + theophylline. Although the magnitude of the response varied from one experiment to the other, stimulation of RIN cells by arginine + theophylline consistently induced an increase in insulin secretion in all of five consecutive experiments ($p < 0.01$, Fig. 3).

Immunoprotection

^{51}Cr Chromium cytotoxicity test on free and microencapsulated RINm5F cells. In both free and microencapsulated cells, incubation with acidified distilled water elicited the release of more than 75% of the initial total radioactivity (Table 1). By contrast, when preparations were in-

cubated with culture medium, or with guinea pig complement, or with complement plus the serum of a normal rabbit, or with complement plus the sera of six control human subjects, chromium release remained at less than 15% in the case of free cells, and less than 25% in the case of microencapsulated cells. These findings demonstrated that the cytotoxic activity of immune sera could be compared in free and microencapsulated cells, i.e. that the protection afforded by the capsule membrane could be assessed *in vitro*.

Incubation of free cells with the sera of the immunized rabbit or of two Type 1 (insulin-dependent) diabetic patients in the presence of complement produced a ^{51}Cr release of more than 45%. This effect was not observed when the complement had been inactivated by heating at 56 °C. By contrast, chromium release by encapsulated cells remained below 20%, even after incubation with native complement. These results were not significantly different from those observed during the control incubations.

A cytotoxic index was calculated which took into account the maximal and non-specific chromium release in each individual experiment. Figure 4 gives the index obtained with the sera of the control human subjects and of the two diabetic patients. In free cells, it was about 50% when they were incubated with immune sera and native complement. However, in encapsulated cells incubated under the same conditions, this index never exceeded 10%.

Discussion

The development of bioartificial pancreas systems, separating pancreatic cells from the host by an artificial membrane, should permit non syngeneic transplantation for the cure of human diabetes mellitus without immunosuppression [2]. However, effective cell immunoprotection is essential for two reasons: First, it is necessary to protect the graft against the humoral and cellular factors responsible for its immune rejection; second, in the specific case of diabetes mellitus, complement fixing antibodies, whose cytotoxic activity against pancreatic cells has been demonstrated *in vitro*, are spontaneously present in many Type 1 (insulin-dependent) diabetic patients [5, 6]. Therefore, the concept of a bioartificial pancreas assumes that the membrane is not permeable to antibodies and complement. For instance, in experiments using "diffusion chambers", it was possible to avoid graft rejection by protecting the transplanted tissue with a membrane fully permeable to antibodies, provided that cellular contact with the host tissue was prevented [12]; however, such protection was not observed in experimental models with preformed antibodies [13]. So far, assessment of long-term immunoprotection by different kinds of bioartificial pancreas, namely diffusion chambers, hollow fibers, microcapsules [2], was only investigated in drug-induced models

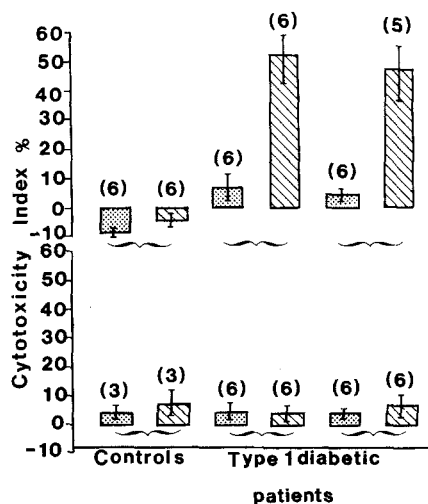


Fig. 4. Cytotoxicity index determined on free RINm5F cells (upper part), and on microencapsulated RINm5F cells (lower part), after incubation with sera from control human subjects, or two Type 1 (insulin-dependent) diabetic patients, in the presence of heat-inactivated (dotted columns) or native complement (hatched columns)

of diabetes, in which the presence of an immune response against the pancreas has not been documented. Consequently, these experimental conditions were not suitable for demonstrating the efficiency of immunoprotection by the membrane.

Our data demonstrate clearly that microcapsules, which are permeable to glucose, arginine, theophylline and insulin, are nevertheless able to efficiently protect the pancreatic B cell against the cytotoxic factors present in the serum of a rabbit immunized with pancreatic cells or in the sera of Type 1 (insulin-dependent) diabetic patients. This demonstration validates the concept of cell immunoprotection in a bioartificial pancreas.

To evaluate the protection against cytotoxic antibodies, we set up a cytotoxic test based on ^{51}Cr uptake and release in encapsulated cells. The difficulty was to determine the initial radioactivity taken up by these cells, which varied from one capsule to the other, since the number of cells per capsule is different; this obstacle was overcome by performing the assay in test tubes, which proved a simple accurate method of determining initial radioactivity by double counting of both the supernatant and pellet after centrifugation following incubation. This method could be used for other purposes.

It can be observed that encapsulated RINm5F cells released apparently less ^{51}Cr when incubated in the presence of HCl. This might be due to an incomplete diffusion of ^{51}Cr across the membrane, which would in turn decrease the calculated percentage of ^{51}Cr release. We therefore calculated a cytotoxicity index taking into account, in each experiment, both the maximal (HCl), and minimal, non specific (RPMI incubation), chromium release (Fig. 4).

In conclusion, the present results do not demonstrate that these kinds of microcapsules allow for long-term islet survival in allogeneic graft transplantation, since other problems are also involved such as the long-term biocompatibility of the membranous material against the host or against the graft. In vivo experiments using the animal models closest to man are required to deal with these questions. However, this study does provide a method for in vitro evaluation of the selective permeability to insulin and anti-islet complement fixing-antibodies of a specific capsule preparation. The method could therefore be recommended for testing microencapsulated islet preparations before transplantation, in order to establish that the graft is effectively protected by the microcapsules against the cytotoxic activity of the serum of the patient himself.

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