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Improved Active Disturbance Rejection Control for the Knee Joint Motion Model

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https://doi.org/10.18280/mmep.090225	ABSTRACT
Received: 22 October 2021 Accepted: 8 April 2022	This work focuses on design of trajectory-tracking control based on active disturbance rejection control (ADRC) controller for knee joint exoskeleton device. The device is worn by disable patients and it is actuated by ADRC to perform the exercises prescribed by aburchased on the probabilitation of humansid's lower limb. In order to improve the

Keywords:

exoskeleton system, ADRC controller, PID controller, tracking performance, robustness

This work focuses on design of trajectory-tracking control based on active disturbance rejection control (ADRC) controller for knee joint exoskeleton device. The device is worn by disable patients and it is actuated by ADRC to perform the exercises prescribed by physician doctor for rehabilitation of humanoid's lower limb. In order to improve the tracking performance and robustness characteristics of ADRC, minor modification has been made in its structure, which is represented by adding feed forward control signal to reference angular acceleration. The numerical simulations via MATLAB software environment have been conducted with various model uncertainties and external disturbances to assess the performance of modified control scheme. The proposed controller showed improvement in trajectory tracking error, rejection of exerted disturbances, and robustness against parameter uncertainties.

1. INTRODUCTION

Physically disabled people can take care of themselves in everyday life with the help of an exoskeleton robot. For humans to accomplish daily activities, the lower-limb motions knee is extremely crucial. Up to now, exoskeletons for knee mobility assistance have been proposed for daily use or rehabilitation. Several exoskeleton leg systems have been investigated and built since the 1950s [1, 2]. Sitting is one of the most significant everyday activities that involves knee mobility. In terms of segmental lengths and center of rotation placement, the exoskeleton robot should be adaptive to the human lower limb. Because the exoskeleton robot is intended to be used for everyday tasks, it should be able to generate flexible and smooth motions. When compared to other bodily joints, the knee joint has the most constraints, with strong muscles and ligaments limiting various actions that can harm the knee. The connection between the exoskeleton and the human's leg should be as suitable as possible, with no abrupt movements that could cause discomfort and instability to the user in the interaction zones [3]. As a result, the position controller should avoid trajectory oscillations and overshoot responses. This behavior can be achieved by adjusting a controller properly.

The proportional-integral-derivative (PID) controller can be used to manage the required outcome of the exoskeleton; however, despite its ease of development, the convergence analysis and coefficients adjustment limit its application, and it also suffers when the system is disturbed [4]. Soft computing algorithms, like as fuzzy sets and neural networks (NNs), have been investigated for many years. For the exoskeleton, a fuzzy controller with a bang-bang controller was developed, and a Radial Basis Functions (RBF) neural network was applied to correct for the disturbance, but both of these algorithms require a lot of processing power [5, 6].

Sliding mode control (SMC) may be a useful method because to its adaptability to existing system uncertainty as well as external disturbances, but it suffers from chattering due to discontinuity switching, which can result in sensor damage [7, 8]. In such situations, robust control methods are one solution, but these methods are restrictive and reflect terrible scenarios at the expense of transient response. As a result, such controllers are unable to react quickly enough in the situation of significant disturbances. (ADRC) was created by Gao et al. [9] to overcome these restrictions and offered several advantages. With evident advantages in performance and practicality, ADRC was capable of substituting PID strategy and proposing answers for problems under disturbances [10]. The increasing adoption of ADRC in industry during the last three decades demonstrates its utility in a variety of applications [11-13]. The fundamental premise of ADRC is the capability to predict "total disturbance" induced by unknown simulation model and external disturbances on-line.

ADRC is used for various robotic rehabilitation devices for tracking applications in the lower limb rehabilitation category. According to Long et al. [14], clinical gait data was employed as a reference and a linear extended state observer (LESO) based ADRC was applied to the lower limb exoskeleton for knee joints. When the results of PID and ADRC are compared for the knee trajectories, the results demonstrate that ADRC outperforms PID by a small margin. To increase tracking performance, a suggested (ADRC) with fast terminal sliding mode control (FTSMC) can not only reduce disturbance but also quickly converge to a limited region, however there is significant chattering [15]. The feedback design, on the other hand, is based on the existence of a Control Lyapunov Function (CLF) and the Sontag's formula rather than a PD controller used with an Extended State Observer (ESO) to design and estimate unknown disturbances on-line and canceled by introducing the ESO output into the feedback loop. Where ARDC's usefulness is demonstrated through experimentation and adaptation. There are numerous rehabilitation control schemes [16], however position tracking is one of the most basic control strategies for robotic rehabilitation devices, in which the controller improves the repeatability and position precision of motion for the patient's recovery [17, 18].

2. MOTION DYNAMIC OF EXOSKELETON KNEE-ASSISTANT DEVICE

Since the exoskeleton knee system is designed to be utilized in everyday tasks, it should be able to provide versatile and smooth motions. As shown in Figure 1-a, one right leg contains a thigh holder, a lower leg holder, a DC motor, and two (position, current) sensors. The knee device is worn by users to assist the motion of their lower-limb in sitting situation. Knee joints have only one active DOF (flexion/extension). The desired control signal generated by ADRC is fed to DC motor to develop the required torque for prescribed motion. The range of angular movement in human knee is usually limited between 135° of flexion and 0° of extension, with 90° being the rest position. For safety, the stopper is attached for motion to prevent the movable range from being exceeded. Furthermore, for reliability, the maximum torque of actuating motor is regulated by equipment and software. Mechanical constraints were designed to allow the human body model and the exoskeleton model to interact freely in a practical condition. The mechanism of actuating the leg at joint level for rehabilitation exercises is shown in Figure 1-b [19].

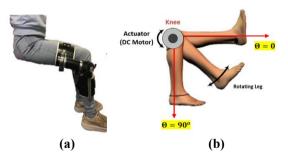


Figure 1. (a) Knee exoskeleton prototype; (b) Mechanism of actuating knee motion [20]

The exoskeleton and human model were modeled as a system of rigid bodies with one degree of freedom for knee part. The nonlinear dynamic for the exoskeleton and human model with one joint, at the knee, is determined through the use of the Euler–Lagrange method. The dynamic modeling of the system can be expressed as follows [21-23]:

$$J\ddot{\theta} = -\tau_g \cos\theta - f_s \, sgn\dot{\theta} - f_v \, \dot{\theta} + \tau_h + \tau$$

where, θ is the knee joint angle between the actual position of the shank and the full extension position, $\dot{\theta}$ and $\ddot{\theta}$ are, respectively, the knee joint angular velocity and acceleration. J, f_s, f_v, τ_g , and τ are the leg inertia, solid friction coefficient, viscous friction coefficient, gravity torque, and the actuating torque, which is applied to the Knee-Exoskeleton system at the knee level, respectively. Letting x_1 and x_2 represent the variables θ and $\dot{\theta}$, the above equation can be written in state variable:

$$\dot{x}_1 = x_2$$

$$\dot{x}_2 = f + b_0 \tau \tag{1}$$

where, $b_o = 1/J$ and f represents the lumped term of uncertainties and nonlinearities, which is given by:

$$\frac{1}{J} \left[\tau_g \cos(x_1) - f_v x_2 - f_s \operatorname{sign}(x_2) + \tau_h \right]$$

3. MODIFIED ACTIVE DISTURBANCE REJECTION CONTROL

As illustrated in Figure 2, the LADRC is composed of three main parts: a tracking differentiator (TD), an extended state observer (ESO), and a state error feedback control law (SEF), where the TD constructs the organized transition process and extracts the differential of each order of the input signal. In some situations, the transition process is extremely useful and even required. The core of ADRC is the ESO, which is used to estimate the total lumped uncertainties and disturbances.

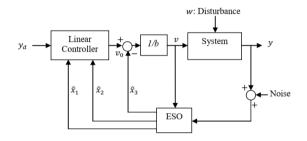


Figure 2. Block Diagram of the ADRC control strategy

The following state space form can be used to express the standard system of Eq. (1) [24-26]:

$$\dot{x}_{1} = x_{2}
\dot{x}_{2} = x_{3} + b_{o} \tau
\dot{x}_{3} = f
y = x_{1}$$
(2)

where f represents the total disturbance and model uncertainties.

The proposed structure of observer dynamics for the system described by Eq. (2) is given by:

$$\hat{\mathbf{z}} = \mathbf{A}\,\hat{z} + \mathbf{B}\,\tau + \boldsymbol{\beta}\,(y - \hat{y})
\hat{y} = \mathbf{C}\,\hat{\mathbf{z}}$$
(3)

where, $\hat{\mathbf{z}} = [\hat{z}_1 \, \hat{z}_2 \, \hat{z}_3]^T$ is the vectors of estimates of y, \dot{y} , and f, respectively. The observer described above is known as the LESO and $\boldsymbol{\beta}$ is termed as observer gain matrix. The elements of observer gain matrix $\boldsymbol{\beta}$ can be obtained using the pole-placement method. When properly designed and implemented, the estimated states of observer will track that of the plant defined by Eq. (2).

Based on pole-placement control technique, one can establish the following characteristic equation based on structure of extended state observer:

$$Q(s) = |s\boldsymbol{I} - (\boldsymbol{A} - \boldsymbol{\beta} \boldsymbol{C})| = (s + \omega_o)^3$$
(4)

The observe gain matrix can be evaluated as follows:

$$\boldsymbol{\beta} = \begin{bmatrix} 3 \,\omega_o & 3 \,\omega_o^2 & \omega_o^3 \end{bmatrix} \tag{5}$$

In order to determine the elements of observer gain matrix, the bandwidth ω_o of LESO is only required. However, this simple tuning technique combines the trade-off between performance and noise-sensitivity. However, other modern and efficient optimization techniques can be consulted for tuning purposes of these parameters [27-32].

The task of TD is to perform time-derivative of the desired input and to provide both the original and derivative versions of reference input y_d . Both signals are fed to PD controller, which works according to the following expression:

$$v_o = K_p \left(y_d - \hat{z}_1 \right) + K_d \left(\dot{y}_d - \hat{z}_2 \right) \tag{6}$$

where, K_p and K_d are proportional and derivative gains, respectively. The performance of ADRC can be improved with an addition reference angular acceleration in feed forward path so that Eq. (6) can be rewritten as:

$$v_o = K_p \left(y_d - \hat{z}_1 \right) + K_d \left(\dot{y}_d - \hat{z}_2 \right) + \ddot{y}_d \tag{7}$$

The disturbance, represented by x_3 , is estimated by \hat{z}_3 and compensated by the following control law:

$$v = v_o - \hat{z}_3 / b_o \tag{8}$$

It is worthy to notify that the actuated torque τ to the exoskeleton system is equivalent to the control law described by above equation.

Theorem: If the ESO is well-performed, the improved structure of ADRC used for controlling the system described by Eq. (1) can lead to $y \rightarrow y_d$ as $t \rightarrow \infty$.

Proof: If the ESO has been properly designed, and if y_d is firstly and secondly differentiable, then $\hat{z}_1 \rightarrow y_d$ and $\hat{z}_2 \rightarrow \dot{y}_d$ as $t \rightarrow \infty$. According to Eq. (7), the value of $v_o \rightarrow \ddot{y}_d \rightarrow \ddot{y}$ as $t \rightarrow \infty$. This leads to $y = y_d$.

Pursuing the analysis in Ref. [33] and recalling form the control theory that the bandwidth of the system has the following expression:

$$\omega_c = 10/T_s \tag{9}$$

where T_s is the settling time of the system. In this study, the open-loop system has a settling time of $T_s=0.408$ sec. The bandwidth will be determined according to above equation to be 2.45 Hz.

Therefore, the bandwidth of the system can be calculated as $\omega_c = 24.5$. If one chooses the bandwidth of observer ω_o to be equal to $\omega_o = 4 \omega_c$, then it easy to calculate the elements of observer matrix gains $(\beta_1, \beta_2, \beta_3)$ according to Eq. (5) and the values of controller gains are given by $k_p = \omega_c^2$, $k_d = 2 \omega_c$.

4. RESULTS AND DISCUSSION

This study considered a healthy man who is 33 years old, weighs 75 kilograms, and stands 1.73 meters tall. The tested system, shown in Figure 1, comprises of a person in a sitting position wearing a lower limb exoskeleton, and selected parameters for this scenario based on Table 1 [21].

The computer simulations have been conducted via Matlab/Simulink environment to verify the effectiveness of proposed control approach for rehabilitation system. Two types of reference trajectory were presented to test the performance of modified ADRC. The first reference signal is represented by [5];

$$y_{d1} = 60 \sin(0.5 \pi t)$$

Table 1. Lists the numeric values of system parameters

Parameter	Value
Inertia (J)	$0.348 \ kg. m^2$
Solid Friction Coefficient (f_s)	0.998 N.m
Viscous Friction Coefficient (f_v)	0.872 N.m.s./rad
Gravity Torque (τ_g)	3.445 N.m

The other reference profile is inspired from real motion of rehabilitation exercises for knee [34, 35]

$$y_{d2} = 0.766 \cos (0.\pi t) - 0.099 \cos(\pi t) - 0.342 \sin (\pi t) - 0.219 \cos(2\pi t) + 0.168 \sin(2\pi t) + 0.008 \cos(3\pi t) + 0.084 \sin(3\pi t) - 26.127$$

Figure 3 shows the profile of reference trajectory y_{d2} for the knee joint.

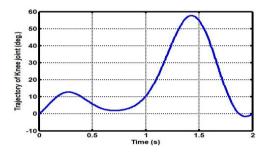


Figure 3. The profile of real trajectory y_{d2}

Two cases have been addressed in the numerical simulation. Case I discussed the control performance without disturbance, while Case II has accounted for the disturbance effect. Two types of disturbances have been given; one is a random disturbance and the other has stationary behavior.

4.1 Case I: Tracking performance without disturbance

The exoskeleton device can be adjusted to aid the human knee to recover its natural activities. The rehabilitation exercises are either using expert physician or utilizing exoskeleton system, which is fed by desired or prescribed reference motion. In this scenario, two types of desired trajectories can be applied as reference signal for the controlled system. These trajectories are described by y_{d1} and y_{d2} .

Figure 4 shows the performance of modified ADRC (MADRC) as compared to the PID controller without external disturbance and subjected to reference input y_{d1} . The setting of classical PID controller's terms are found based on try-anderror procedure and they are $k_p = 150$, $k_d = 15$, $k_i = 80$. Figure 5 show the trajectory tracking errors for both MADRC and PID controller. The Root Mean Square of Error (RMSE) is used as index for evaluation of tracking performance between the PID control and MLADRC. Based on Figure 5, the RMSE has been calculated to be (0.00588) and (0.5565) for MADRC and PID controller, respectively. This indicates that the MADRC is better than PID control in terms of accuracy.

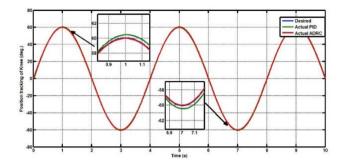


Figure 4. Tracking performance based on PID controller and MADRC without disturbance

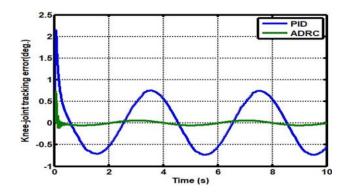


Figure 5. Track error of MADRC and PID controller

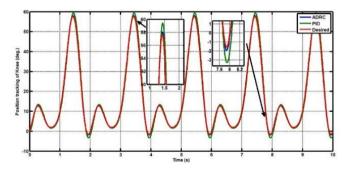


Figure 6. Transient responses of joint angle subjected to reference y_{d2}

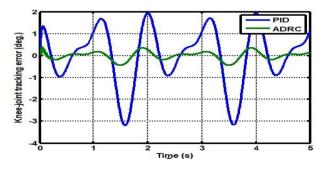


Figure 7. Tracking error based on MADRC and PID controller subjected to reference y_{d2}

In the next simulation, the signal represented y_{d2} is applied to controlled system based on both proposed controllers. Figure 6 shows the tracking performances of MADRC and PID control. The transient responses of errors based on these controllers are shown in Figure 7. According to measures of RMSE, one can conclude that the MADRC outperforms the PID controller, where MADRC gives 0.1438 and the PID controller has 1.08 in terms of index RMSE.

4.2 Case II: Tracking performance with disturbance

In the next scenarios, two types of disturbances are exerted: stationary and random-type disturbance. These disturbances are added to torque control signal v_o and represent gravity disturbance torque. However, the scenarios have been simulated when the controlled system commanded only by actual-like reference trajectory y_{d2} .

The first simulation is implemented by exerting constant disturbance of amplitude 100 N.m. at time t = 2 sec. The responses of knee angular positions based on PID control and MADRC are shown in Figure 8. Figure 9 demonstrates the behaviors of error dynamic resulting from both controllers. Based on REMSE measure, it is clear that the MADRC has better tracking accuracy than the PID controller, where the MADRC has recorded 0.3007 and the PID controller gives 1.953.

In the next scenario, the performance of MADRC is compared with the PID controller when the controlled system is encountered a random disturbance within bounds (-10, 10) N.m. The responses of knee angular angles due to PID controller and MADRC as shown in Figure 10. The behaviors of tracking error are illustrated in Figure 11. It has been shown that the RMSE for PID controller is equal to (1.076), while the RMSE value for MADRC is equal (0.144). Based on these records, the accuracy resulting from MADRC is better than that resulting from PID controller.

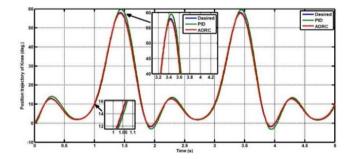


Figure 8. Tracking performance based on PID controller and MADRC subjected to constant disturbance

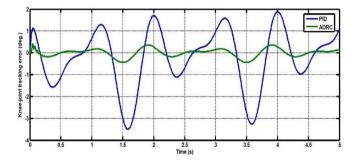


Figure 9. Behaviors of error due to MADRC and PID controller with constant disturbance

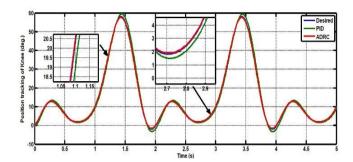


Figure 10. Transient responses of joint angle subjected to random disturbance

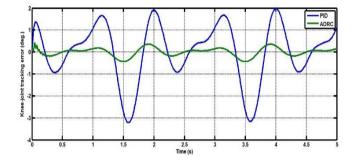


Figure 11. show tracking errors of MADRC and PID controller with random disturbance

4.3 Performance Study of ESO

The main part in the structure of MADRC is the ESO. Better performance of ESO leads to improved performance of MADRC. Therefore, this simulation part is devoted to study the performance of ESO in the presence of disturbance. The main interesting state in ESO is the \hat{z}_3 , which is responsible for estimating the total disturbance, represented by f(t) in extended dynamic system of Eq. (2).

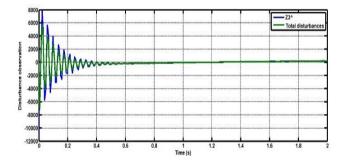


Figure 12. The behavior of state estimate \hat{z}_3 for f with freedisturbance ($\tau_h = 0$) and the reference is y_{d1}

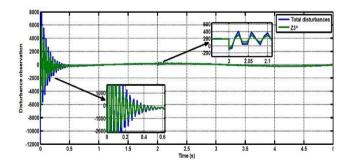


Figure 13. The behavior of state estimate \hat{z}_3 for f with disturbance ($\tau_h = 10 \text{ N.m}$) and the reference is y_{d1}

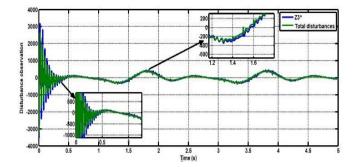


Figure 14. The behavior of state estimate \hat{z}_3 for f with disturbance ($\tau_h = 0$) and the reference is y_{d2}

In addition, this part focuses on the robustness characteristics of observer to estimate the total disturbance subjected to different load conditions (τ_h) with two types of commanded references. In Figure 12, the estimated state \hat{z}_3 is demonstrated when the system is free from any disturbance $(\tau_h = 0)$ and the controlled system is commanded with sinusoidal reference y_{d1} . In this case, the estimated state \hat{z}_3 will estimate all nonlinearity and uncertainty function f as indicated in Eq. (1), but with the term associated with τ_h is set to zero. Figure 13 shows the behavior of state estimate \hat{z}_3 when a constant disturbance ($\tau_h = 10 \text{ N}.\text{ m}$) is applied to the controlled system at time 2 sec based on reference y_{d1} . It is clear from the figure that the ESO could successfully track the applied load together with all terms of uncertainty function fin such a way the MADRC could compensate this load change. Figure 14 repeats the scenario of Figure 12, but with presence of reference trajectory y_{d2} . Again, the state \hat{z}_3 of ESO could estimate the applied change f(t) very closely.

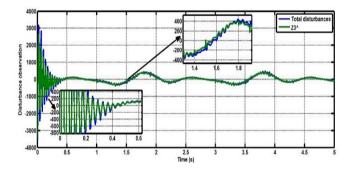


Figure 15. The behavior of state estimate \hat{z}_3 for f with random disturbance $\tau_h = [-10, 10]$ and reference y_{d2}

In Figure 15, a random disturbance τ_h with bounds (-10 to 10) N.m has been exerted at 2 sec when the controlled system is commanded with reference trajectory y_{d2} . It is evident form the figure that the estimate state \hat{z}_3 tracks f(t) very closely.

5. CONCLUSIONS

This study presented the design of modified ADRC for motion control of joint angle for exoskeleton knee-device. The performance of modified ADRC has been assessed via numerical simulation and compared to conventional PID controller in terms of transient and robust characteristics. The computer simulations have been conducted for two types of commanded signals and the simulated results showed that the MADRC could give better robustness and transient features than the PID controller. In addition, the effectiveness of ESO, which is the core part of ADRC, has been studied and evaluated via computer simulation for specified load exertion. The simulated results showed that the ESO could successfully estimate the uncertainties irrespective the type of commanded reference trajectories. This study can be extended for future work either by including recent observation techniques or to design other control schemes either for enhancing the ADRC or for the purpose of comparison in performance [36-40].

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NOMENCLATURE

Exoskeleton Inertia (Kg.m²) J Gravity Torque (N.m) $\tau_{\rm g}$ \mathbf{f}_{s} Solid Friction (N.m) fv Viscous Friction (N.m.sec./rad) Knee joint angle (rad) θ Applied Torque (N.m) τ Controller Bandwidth (rad/sec) ω Observer Bandwidth (rad/sec) ωο PID Proportional integral derivative DOF Degree of Freedom ESO Extended state observer SEF State error feedback TD Tracking differentiator RMSE Root-Mean-Square of Error MADRC Modified Active Disturbance Rejection Control