

Integrated photonic circuit in silicon on insulator for Fourier domain optical coherence tomography

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ABSTRACT

Optical coherence tomography (OCT) is a medical imaging technology capable of producing high-resolution, cross-sectional images through inhomogeneous samples, such as biological tissue. It has been widely adopted in clinical ophthalmology and a number of other clinical applications are in active research. Other applications of OCT include material characterization and non-destructive testing. In addition to current uses, OCT has a potential for a much wider range of applications and further commercialization. One of the reasons for slow penetration of OCT in clinical and industrial use is probably the cost and the size of the current systems. Current commercial and research OCT systems are fiber/free space optics based. Although fiber and micro-optical components have made these systems portable, further significant miniaturization and cost reduction could be achieved through the use of integrated photonic components. We demonstrate a Michelson interferometer using integrated photonic waveguides on nanophotonic silicon on insulator platform. The size of the interferometer is $1500\ \mu\text{m} \times 50\ \mu\text{m}$. The structure has been tested using a mirror as a reflector. We can achieve $40\ \mu\text{m}$ axial resolution and 25 dB sensitivity which can be substantially improved.

Keywords: optical coherence tomography, silicon photonics, integrated photonics, silicon on insulator

1. INTRODUCTION

During the last decade there has been a significant advancement in integrated silicon photonics, specifically due to a need for optical interconnects in multi-core processors. Passive structures like low-loss waveguides, spot size converters, polarization splitters, demultiplexers, resonators and active components such as modulators, switches, and heterogeneously integrated photodetectors and lasers have been demonstrated on silicon¹. Nanophotonic silicon on insulator (SOI) is a versatile platform for a variety of densely integrated silicon photonic components that has been used by many research groups. An SOI wafer consist of a thin top Si (refractive index, $n = 3.45$) layer sitting on silica (SiO_2 , $n = 1.45$) layer, which is carried on a thick Si substrate. Photonic components are realized by etching the top Si layer, resulting in high refractive index contrast in all directions. Using wafer scale CMOS compatible processes, low loss ($<2.4\ \text{dB/cm}$) waveguides with core sizes of $0.1\ \mu\text{m}^2$ and bend radii of $5\ \mu\text{m}$ can be realized. Using such wafer scale processes for silicon, low-cost, high density, integrated photonic components can be mass-fabricated and integrated with CMOS electronics². Due to absorption of the silicon in the visible range, the components are designed for wavelengths above $1100\ \text{nm}$. Although silicon is not an efficient light emitter and detector in the near infrared wavelengths, active elements can be heterogeneously integrated on top of the silicon wafer³. Using the SOI platform together with heterogeneous integration of sources and detectors, significant part of an optical coherence tomography system can be realized on chip in the near future.

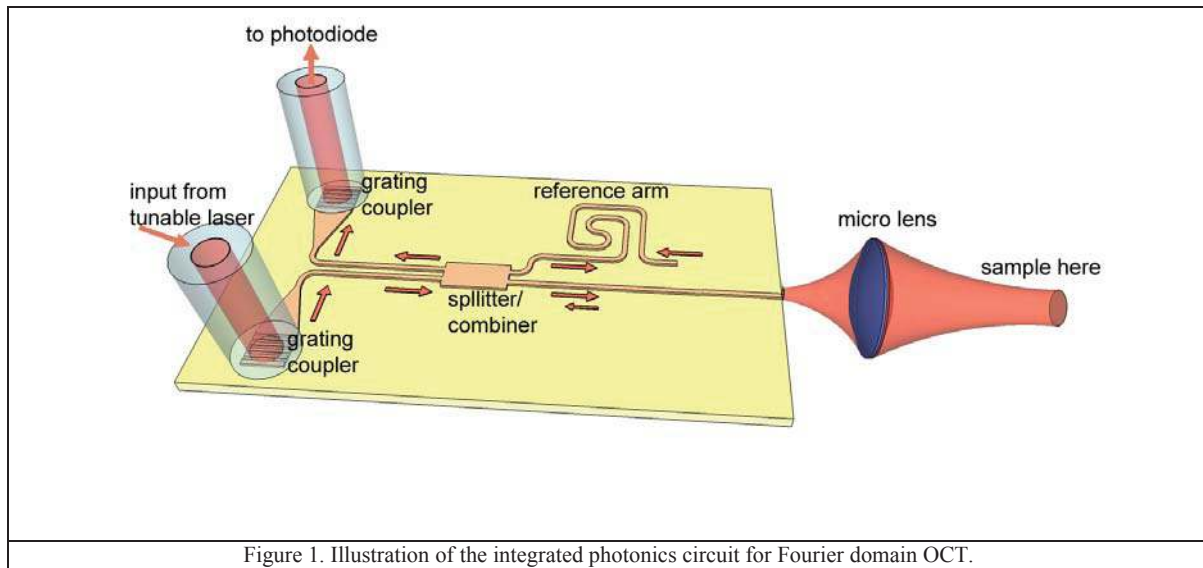
Optical Coherence Tomography (OCT) can benefit from the progress in integrated photonics for miniaturization and cost reduction. However, there has been little research on utilizing integrated photonics for OCT. Culermann et al. demonstrated a passive photonic circuit for OCT fabricated on silica. The device consisted of cascaded splitters and combiners⁴. The photonic structures in glass are very low loss, transparent in the visible, however, due large bend radii, the size of the components are almost two orders of larger than the ones on silicon. In another study, Margallo-Baas et al. demonstrated an integrated photonic structure on silicon on insulator (SOI) for time domain OCT, where the delay line

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was implemented with thermal tuning of a waveguide in the reference arm⁵. In this paper, we present an integrated Michelson interferometer for Fourier domain OCT fabricated on SOI using CMOS compatible fabrication process.

2. DESIGN

An illustration of the integrated Michelson interferometer is given in Figure 1. Fiber coupled tunable laser is coupled to the planar photonic chip via a grating coupler which has a FWHM bandwidth of 56 nm and 25% coupling efficiency. The size of the grating coupler is 10 μm and is tapered to a single mode, polarization maintaining waveguide. The waveguides are etched 220 nm deep and 450 nm wide with deep UV lithography. Then the light is split into reference

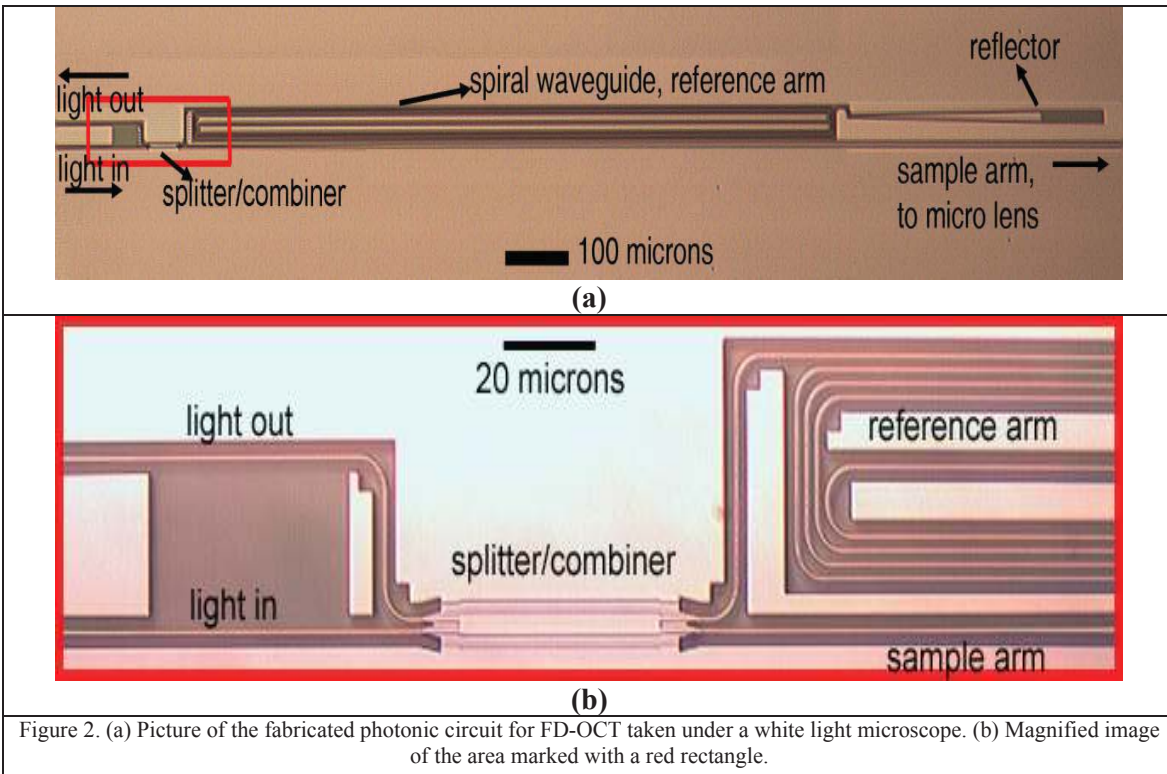


and sample arms with a 50/50 broadband (bandwidth $>100\text{nm}$) multimode interference splitter/combiner. The insertion loss of the splitter/combiner is less than 1 dB. The reference arm consists of a 9 mm long spiral waveguide with 5 μm bend radii and ends with a silicon air interface. The flat waveguide end acts as a broadband reflector with 30 % reflection efficiency. In the sample arm, the light is coupled out of the chip from a waveguide facet. The output from the waveguide facet is imaged onto the sample with a micro lens. The reflections from the sample and reference arms are combined with the splitter/combiner and coupled to a fiber which guides the light to a photodiode. The sample is coated with 1 μm thick benzocyclobutene (BCB, refractive index $n = 1.54$) to reduce the group velocity dispersion of the waveguides.

3. FABRICATION

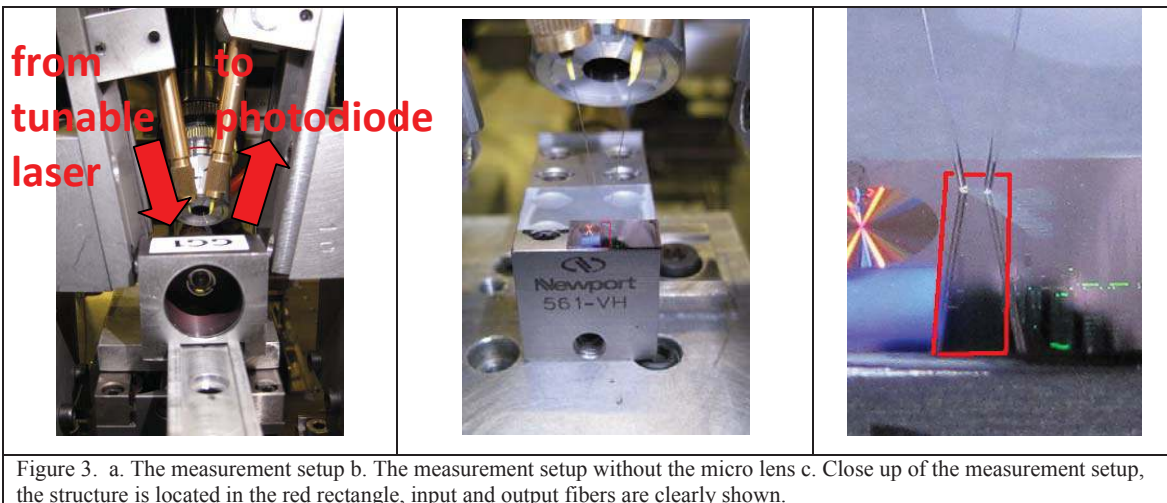
The device is fabricated on a 200 mm diameter SOI wafer with 220 nm thick Si top layer on top of 2 μm thick SiO_2 using 193nm deep-UV lithography in combination with inductively coupled plasma reactive ion etching. The fabrication was done through ePIXfab silicon photonics platform (www.epixfab.eu) at IMEC nanoelectronics and nanotechnology research center, Belgium. The sample is cleaved to create the facet at the end of the sample arm to couple the light out of the chip. A light microscope image of the fabricated structure is given in Figure 2. The size of the Michelson interferometer is only 1500 x 50 μm . In a wafer scale process, hundreds of these structures can be fabricated in a single run. In addition to advantages of cost and size, miniaturization of OCT through integrated photonics components will also provide more stable polarization maintaining interferometers compared to fiber

based systems.

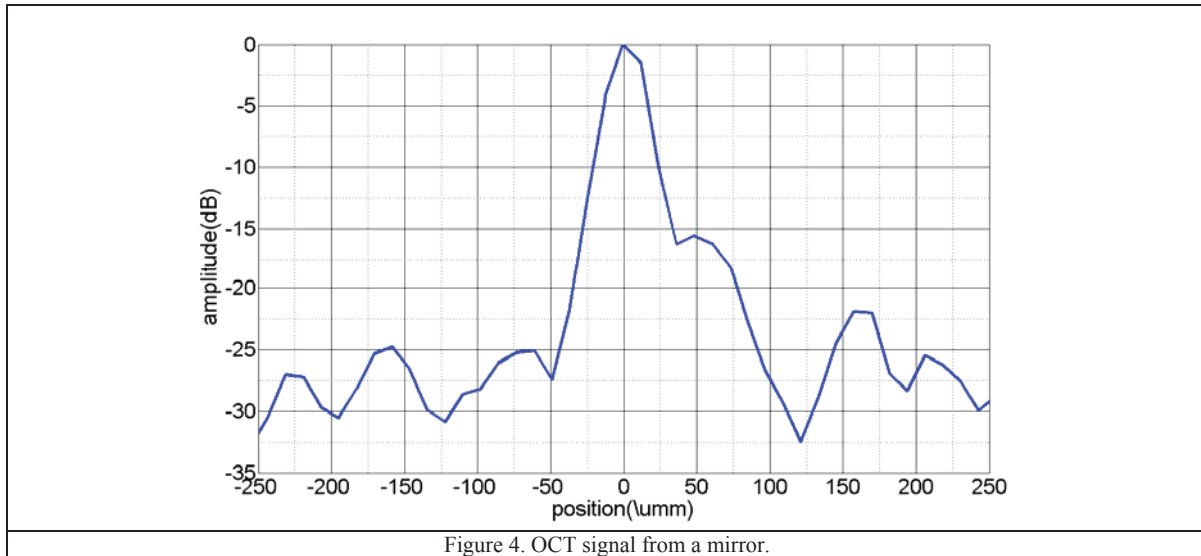


4. MEASUREMENT

The measurement setup is given in Figure 3. The chip is placed on vacuum holder. A single mode fiber from a tunable laser (1510 – 1610 nm, 1Hz tuning frequency) couples the light to the chip. A micro lens with an NA of 0.53



is used to collimate the light and send onto a gold mirror. The interference of the reference arm and sample arm are coupled out of the chip with a grating coupler to a fiber and send to a photodiode. The OCT signal from the mirror is given in Figure 4. The axial resolution is around $40\ \mu\text{m}$, which is higher than theoretical $27\ \mu\text{m}$ in air for $40\ \text{nm}$ FWHM bandwidth and no group velocity dispersion (GVD). From fully vectorial simulations with Fimmwave mode solver (Photon Design, Inc), the group velocity dispersion of the fundamental TE mode of a $220\text{nm} \times 450\text{nm}$ waveguide with BCB cladding is found to have a GVD of $-250\ \text{fs}^2/\text{cm}$. The GVD of $5\ \mu\text{m}$ bends are also calculated to be in that order. The broadening of the axial resolution is probably due to GVD mismatch, which can be reduced by engineering the GVD of the waveguides by changing their dimensions. Flexibility of engineering the GVD of silicon waveguides may also be used to fully compensate the GVD mismatch for tissue imaging,



The sensitivity of the system is around 25 dB. One of the main reasons for a low sensitivity is the facet where we have loss of 10 dB power for each pass, reducing the sensitivity by 40 dB. The facet was defined by cleaving the sample and is not polished. The efficiency of the grating couplers also reduces the sensitivity by 24 dB. Rather than a facet and grating couplers, a broadband ($> 100\ \text{nm}$) spot size converter, which has a loss of only $< 2\ \text{dB}$ can be used⁶ to couple the light in and out of the chip. This would bring the sensitivity to a level where tissue imaging can be possible.

5. CONCLUSIONS

In this study, we have demonstrated a Michelson interferometer for OCT with an ultra small footprint. The axial resolution and sensitivity can be easily improved to a level sufficient for in-vivo imaging with small changes in the design. Passive structures for OCT, such as waveguides, splitters/combiners, couplers, tapers, reflectors are the first step towards integrated OCT. Even without inclusion of active structures such as sources, detectors and modulators, OCT can benefit from such compact and robust components. A complete OCT system on a single chip will be also possible in near future with inclusion of active components.

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