

Locally Enhanced Image Quality with Tunable Hybrid Metasurfaces

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Metasurfaces represent a new paradigm in artificial subwavelength structures due to their potential to overcome many challenges typically associated with bulk metamaterials. The ability to make very thin structures and change their properties dynamically makes metasurfaces an exceptional meta-optics platform for engineering advanced electromagnetic and photonic metadevices. Here, we suggest and demonstrate experimentally a tunable metasurface capable of enhancing significantly the local image quality in magnetic resonance imaging. We present a design of the hybrid metasurface based on electromagnetically coupled dielectric and metallic elements. We demonstrate how to tailor the spectral characteristics of the metasurface eigenmodes by changing dynamically the effective permittivity of the structure. By maximizing a coupling between metasurface eigenmodes and transmitted and received fields in the magnetic resonance imaging (MRI) system, we enhance the device sensitivity that results in a substantial improvement of the image quality.

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I. INTRODUCTION

Metasurfaces [1–3] are artificial subwavelength-patterned structures representing an ultrathin planar realization of the metamaterial concept [4]. An essential advantage of metasurfaces over metamaterials is their simplicity of manufacturing and ability to control reflected and transmitted waves, as well as to specifically sculpt the near-field patterns over a frequency range from radio to optical [5–7]. Structural elements of metasurfaces can be made from different metallic [8], plasmonic [9], or low-loss dielectric materials [10], while their geometrical dimensions and element separations are essentially subwavelength. In this way, homogeneous or nearly homogeneous metasurfaces reflect and transmit plane waves as infinitely thin sheets, supporting both electric and magnetic currents [5]. Metasurfaces have been employed for different applications including flat optical components [11–14], holograms [15,16], vortex generators [17], optical information processing [18], nonreciprocal components [19], chirality enhancement [20], the demonstration of optical spin-orbit interactions [21–23], and the control of surface waves [24].

A majority of these metasurface structures has fixed properties, e.g., operational bandwidth or functionality, but active control of metasurfaces is highly desirable [25]. Recently, several groups reported different methods for

a design of metasurfaces with tunable responses [6]. Metasurfaces can also display extreme nonlinear responses [26,27] that enable full optical control and tunability of material parameters as well as the ability to achieve an efficient generation of the second [28] and third harmonics [29]. As a result, these two significant properties, ultrathin planar geometry and dynamic response, make metasurfaces an exceptional platform for engineering novel photonic metadevices [25].

One important application of metasurfaces is the image-quality enhancement that is crucially important in different areas including biology, medicine, and nanotechnologies. In particular, it has been demonstrated experimentally that a metasurface lens designed for optical frequencies can be used to provide diffraction-limited focal spots [14] and to resolve features with subwavelength spacing, while parity-time symmetric nonlocal metasurfaces allow ideal aberration-free optical images [30]. Another imaging area where metasurfaces can potentially be extremely useful is magnetic resonance imaging (MRI), one of the most important clinical modalities for the detection of various diseases in humans [31]. The MRI image quality and spatial resolution are ultimately limited by the signal-to-noise ratio (SNR) obtainable in a relevant clinical scanning time frame [32]. Recently, a new conceptual idea has been suggested to substantially increase the SNR of commercial MRI with the aid of microwave metasurfaces made by resonant metallic inclusions [33]. This effect has been further advanced in *in vivo* imaging and spectroscopy of the human brain [34].

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However, all previous designs produced a locally enhanced magnetic field that was distinctly nonuniform over the extension of metasurface. Also, fine tuning of the spectral response was impractical. Therefore, compact tunable designs are still very appealing for practical applications.

Here, we propose and realize experimentally a novel type of metasurfaces capable of enhancing significantly the image quality applicable to MRI. To overcome the problem of relatively large physical dimensions, inspired by the recent advances in the development of bilayer metasurfaces [35] for visible light, we employ a hybrid microwave metasurface design based on electromagnetically coupled components of both dielectric materials and metallic elements. In addition, by changing the effective permittivity of the structure we observe a substantial spectral shift of the metasurface eigenmode and can fine-tune its properties for patient-specific MRI experiments. In contrast to previous designs [33,34], where the specific near-field pattern of the metasurface eigenmode has a sinusoidal shape of the radiofrequency (rf) magnetic field along its length, and therefore results in an inhomogeneous SNR enhancement and nonideal images, here by altering the coupling strength between the dielectric and metallic layers we are able to achieve different shapes of the near-field mode profile, including an almost homogeneous one in the region of interest.

II. DESIGN OF METASURFACES

In order to realize a novel tunable hybrid metasurface, we start from the microwave metasurface based on resonant elongated metallic particles inserted into a dielectric matrix with a permittivity ϵ [Fig. 1(a)]. Such a metasurface supports a number of eigenstates, which arise due to the splitting of the original resonant frequency into several bands, induced by giant coupling between many resonant particles placed at subwavelength distances [36–40]. In particular, a very interesting phenomenon is observed in the range of frequencies within the first Fabry-Pérot resonance where it is possible to enhance and spatially redistribute the magnetic and electric fields since they correspond to the near-field region, where the electric field and magnetic field distributions of the same eigenstate are decoupled [36]. This property can be employed to increase the SNR in MRI [33]. The sensitivity of the MRI receiver is directly proportional to the ratio of the rf magnetic field in the scanned region to the square root of the absorbed power, and the metasurface increases this sensitivity.

In the simulations a linearly polarized plane wave excites a set of transverse eigenmodes near the first Fabry-Pérot resonance and the lowest mode has a maximum of the magnetic field in the central region of the metasurface [Fig. 1(a)], with the electric field maximum being located near the edges of the wires. The rf magnetic field pattern along the metasurface has a sinusoidal-like shape [right top panel on the Fig. 1(a)] analogous to the conventional

standing waves in optical cavities [41]. This is problematic for MR images since the signal intensities and image contrast are no longer homogeneous across the region of interest, a phenomenon which was observed with previous designs [33,34]. However, this problem can be solved by realizing a hybrid metasurface structure where only the edges of the wires are loaded with high permittivity dielectric material. Because of the very high contrast in permittivity between two regions, the middle part of the metasurface embedded in low epsilon material ϵ_1 while the edges are in a high permittivity material with ϵ_2 , the magnetic field can be extended and its shape becomes almost homogenous [cf. top and bottom central panels in Fig. 1(a)]. At the same time the electric field is still mostly localized inside the high permittivity blocks. Thus, it is possible to achieve a homogeneous local rf magnetic field enhancement, while *minimizing* the electric field amplitude (and therefore the specific absorption rate) in the region of interest. Furthermore, by changing the coupling strength via varying the length of wires inserted in the dielectric blocks [right bottom panel in the Fig. 1(a)], almost any slope of the rf magnetic field pattern can be designed, including realizations of different spatial domains with magnetic field homogeneity around 98%. It is also very important to mention that due to a hybrid nature of the metasurface its dimensions are much smaller than the operational wavelength of the MRI machines [see detailed discussions in Supplemental Material [42]].

Different eigenmodes of the hybrid metasurface have different penetration depths [33] and for the current study the lowest transverse eigenmode, which has the deepest penetration depth and the most homogeneous in-plane magnetic field pattern, has been employed. In order to achieve tunability of the metasurface we externally change the effective permittivity of the dielectric blocks. For the proof-of-principle experiment we use distilled water as a high permittivity material and realize the metasurface coupled to two dielectric blocks from both edges [see the inset of Fig. 1(b) and Appendix A for details]. To demonstrate the effect of eigenmode tunability we numerically calculate the reflection coefficient of a small loop antenna placed above the hybrid metasurface [Fig. 1(b)]. For relatively small values of metasurface effective permittivity, the eigenmode is tuned to a higher frequency [light blue curve in Fig. 1(b)]. By increasing the effective permittivity [e.g., by changing the water level (Δh)] the resonance frequency of the first eigenmode shifts to the lower frequency range, the higher the permittivity—the larger the shift, and in this way the device can be effectively tuned to 63.8 MHz, the working frequency of a 1.5-T MRI system (see Appendix B for further details on the numerical simulations). The effect can be explained by the fact that the eigenmode of the metasurface experiences an effective permittivity ϵ_{eff} which depends on the volume fraction of the dielectric inclusions (ϵ_1 and ϵ_2) in the mixture [43] in

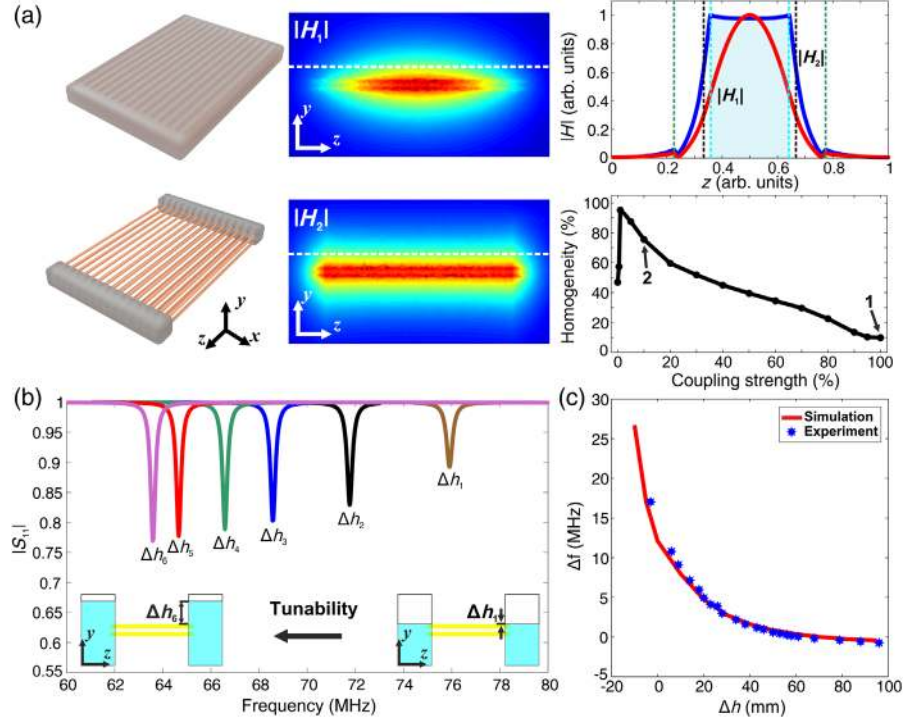


FIG. 1. Basic concept and electromagnetic properties of tunable hybrid metasurfaces. (a) A comparison between the metasurface from the previous study [33] realized by an array of 14×2 brass wires placed inside a homogeneous dielectric medium (top panel) and the new hybrid metasurface (bottom panel). The central panel demonstrates 2D maps of the magnetic field distribution in the yz plane for both cases. The right top panel demonstrates the near-field mode profile of the first eigenmode of different metasurfaces calculated along white dashed lines (shown in the central panel) at the distance of 15 mm above the wires. The magnetic near-field profile of the first eigenmode of the hybrid metasurface has a flat shape in comparison with the field pattern observed in another type of metasurface which has an inhomogeneous sinusoidal form within the region of interest (shown by the shaded area and light blue dashed lines). The boundaries of the wires are shown by black dashed lines, the boundaries of dielectric blocks with green lines. The right bottom panel shows the dependences of the rf magnetic field homogeneity in the region of interest as a function of coupling strength. The two markers indicate the field homogeneity in homogeneous (1) and hybrid (2) designs. The homogeneity level has been determined relative to the metasurface length and is represented as the region of space where rf magnetic field amplitude variations are less than 1%. (b) Numerical simulation results of the reflection coefficient ($|S_{11}|$) of a small loop antenna (with a radius of 40 mm) placed above the hybrid resonator at a 100-mm distance from the wires as a function of the dielectric level (Δh): $\Delta h_1 = 0$ mm; $\Delta h_2 = 10$ mm; $\Delta h_3 = 20$ mm; $\Delta h_4 = 30$ mm; $\Delta h_5 = 50$ mm; $\Delta h_6 = 80$ mm. The insets schematically illustrate the hybrid metasurface geometry and the tunability principle. (c) Resonance frequency ($\Delta f = f_{\text{resonance}} - 63.8$ MHz) as a function of the dielectric level (Δh).

the region close to the resonator and by changing this fraction to a certain extent it is possible to tune the resonance. The resonance shift saturates for some values of ϵ_{eff} (water level Δh) due to the finite penetration depth of the eigenmode [Fig. 1(c)].

To confirm these dependences experimentally we have realized a hybrid metasurface as an array of nonmagnetic metallic wires coupled to the dielectric blocks, fillable by water [schematically shown in the inset of Fig. 1(b), see Appendix A for details]. We gradually add water inside two hollow blocks and measure the reflection coefficient of a loop antenna placed above the metasurface as a function of Δh . Figure 1(c) demonstrates the ability to tune the metasurface resonance frequency. Excellent agreement is seen between the experimental measurements and the simulation results. It is worth noting that the MRI machine works in a narrow frequency band around the Larmor

frequency (here for the hydrogen imaging it is equal to 63.8 MHz) and the metasurface should be tuned exactly to this frequency. However, the variation of the electrical properties of a subject (a patient) located closely to the metasurface may shift the resonance from the Larmor frequency, decreasing the metasurface efficiency. Therefore, the ability to easily fine-tune the resonant frequency is very useful from a practical standpoint, and a unique feature of this new metasurface design.

III. IMPACT OF METASURFACES ON RECEIVER SENSITIVITY

We investigate the performance of the tunable hybrid metasurface on a 1.5-T MRI system. As a test object, we chose a rectangular phantom placed on the top of the metasurface. We use the birdcage body coil of the system,

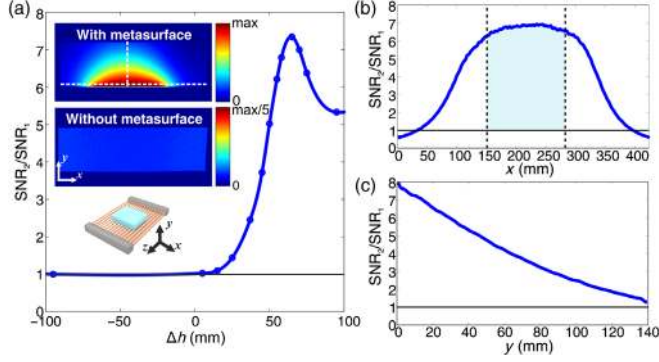


FIG. 2. MRI sensitivity vs metasurface adjustment. (a) Experimentally measured ratio between the SNR with the metasurface (SNR_2) and without it (SNR_1) as a function of Δh . The insets correspond to the MR images of the phantom for the cases with the tuned metasurface present and without it and also show the schematic position of the phantom on the metasurface. (b),(c) Experimentally measured ratio between the SNR with metasurface and without it along the x (b) and y (c) directions in the phantom [shown by white dashed lines in the inset of panel (a)]. The black dashed lines correspond to the wire boundaries and the blue shaded area to the region of interest.

which is embedded in the bore of the scanner, for transmitting and receiving the rf signal. Figure 2 shows the ratio between the SNR with the hybrid metasurface (SNR_2) and without it (SNR_1) as a function of Δh calculated in the phantom. Initially, when the water level is below the level of the wires ($\Delta h < 0$) no SNR enhancement is observed since the eigenmode is detuned. This also confirms that the metasurface itself does not increase the noise in the images. Then, by gradually increasing the water level, we observe a smooth increase in the SNR. The maximum SNR enhancement of 7.34 is achieved for $\Delta h = 65$ mm, which corresponds to the resonant frequency of the hybrid metasurface tuned to the Larmor frequency. The slight difference in the Δh value in comparison with numerical simulation is due to imperfections in the shape of dielectric blocks. MRI scans of the phantom in an axial plane for two cases with a hybrid metasurface, tuned to the maximum efficiency, and without it are shown in the inset in Fig. 2(a). A large increase in the signal intensity can be clearly observed near the metasurface resonator. By further increasing Δh the impact of the metasurface on the MR sensitivity becomes less pronounced due to the fact that the coupling of the metasurface eigenmode to the Larmor frequency decreases. A very important advantage of the hybrid metasurface is an almost homogeneous in-plane profile of the rf magnetic field near the metasurface that results in a nearly uniform signal from the region of interest [Fig. 2(b)]. Furthermore, the lowest eigenmode of the metasurface enables a high penetration depth of the enhanced transmit field, which leads to a SNR enhancement up to a 150-mm distance from the resonator [Fig. 2(c)]. Near the metasurface the gain is a factor of 8, while at the distance of 140 mm from the wires inside the

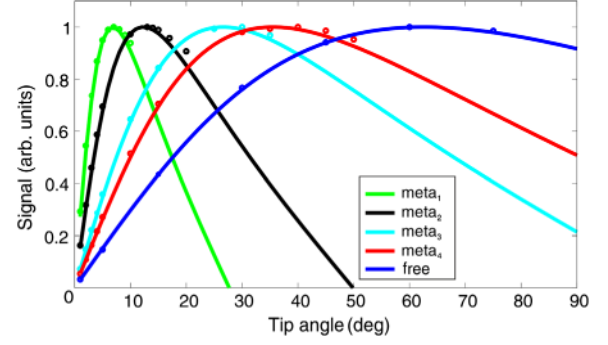


FIG. 3. MR signal vs tip angle (applied rf power) and coupling strength between an artificial resonator and nuclear magnetic resonance frequency. meta_1 is tuned to 64 MHz; meta_2 to 66.3 MHz; meta_3 to 71.2 MHz; and meta_4 to 74.7 MHz. The circles correspond to the experimental data and solid lines represent the theoretical results. Amplitudes are normalized by the following coefficients: $A_1 = 2175$ for meta_1 ; $A_1 = 2175$ for meta_2 ; $A_3 = 133$ for meta_3 ; $A_4 = 96$ for meta_4 ; $A_5 = 53$ for a phantom without the metasurface.

phantom it is about 1.5. In order to investigate the increase in transmit efficiency, as well as to compare the SNR with and without the metasurface using optimum rf transmit conditions for both, we acquire gradient-echo images with different tip angles. The dependence of the received MR signal on the tip angle for a gradient-echo sequence is given by [32]

$$\text{Signal}(r) \sim A(r) \frac{\sin[\lambda(r)\theta_{\text{nominal}}]}{1 - e^{-[TR/T_1(r)]} \cos[\lambda(r)\theta_{\text{nominal}}]}, \quad (1)$$

where $A(r)$ is a spatial coefficient which includes local spin density, $B_1^-(r)$ is the receive sensitivity, T_2 the transverse relaxation time, $T_1(r)$ the longitudinal relaxation time, TR the repetition time, and θ_{nominal} the tip angle which is set in the scan parameters. The transmit efficiency $\lambda(r)$ is directly proportional to the transmit rf magnetic field $B_1^+(r)$. When we consider only the phantom without a hybrid metasurface and use a birdcage coil for transmitting and receiving the MR signal we obtain an optimal tip angle (corresponding to an optimal applied rf power level) where there is a maximum in the received signal (blue curve in Fig. 3). Generally, for a spin-echo sequence, the optimal tip angle is equal to 90° and for a gradient-echo sequence, it is much lower than 90° unless the TR is set to be at least three times the T_1 value, which would result in a very long scan time [32]. The detuned metasurface has no effect on this dependence, i.e., the signal dependence on the tip angle in this case coincides with the curve for the case without the metasurface. However, when the metasurface is tuned to a frequency close to 63.8 MHz (Fig. 3) the curves shift horizontally to the left, meaning that $\lambda(r)$ increases, or in other words, the metasurface enhances the transmitted rf magnetic field $B_1^+(r)$ in the region of interest for the same applied power.

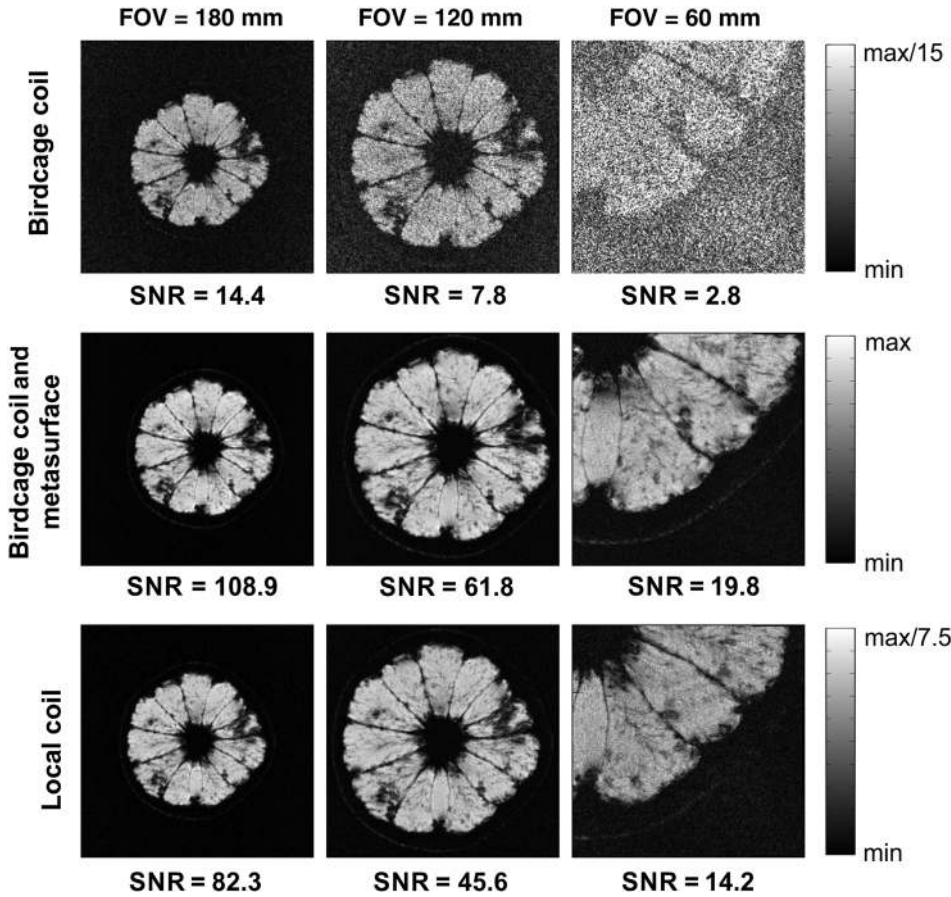


FIG. 4. Experimental demonstration of improved image quality with hybrid metasurfaces. MR images of grapefruit obtained with the birdcage coil only (top panel), with the birdcage coil and metasurface (middle panel), and with a four-channel local receive coil (bottom panel) for different fields of view (FOV) corresponding to different voxel dimensions.

An ability to locally enhance the transmitted rf magnetic field in the region of interest leads to the global reduction of applied rf power and improves the safety of the patient. Additionally, due to the reciprocity principle, the metasurface increases the receive magnetic field $B_1^-(r)$, and the amplitude of the curves is higher (note that the values shown in Fig. 3 are normalized). This directly confirms the SNR enhancement due to an increase in the receiving sensitivity via the coupling with the metasurface eigenmode. The maximum effect is observed when a hybrid metasurface is tuned to 63.8 MHz.

IV. ENHANCED IMAGE QUALITY

MRI quality depends on both the spatial resolution and the SNR. The MRI system can reach a subwavelength spatial resolution since typically the voxel sizes are far smaller than the wavelength, e.g., details with the sizes around 0.5 mm can be resolved at 1.5 T, whereas the wavelength at 63.8 MHz is 4.7 m. This is achieved with the aid of gradient coils which produce a spatially variable magnetic field in addition to the main static magnetic field: this results in very slight modifications in the spatial distribution of the Larmor frequencies over the volume and results in a spatial encoding of the received signal [32]. Higher spatial resolution results in the reduction of

the SNR due to the lower number of protons per voxel [32], and this reduction in the SNR ultimately limits the spatial resolution of the image. It is important to note that small features can be visualized by time averaging the signal through multiple scans, but this results in very long scanning times which are not practical in human applications.

The metasurface improves the SNR, so the image quality should also be enhanced. We perform several MRI scanning sessions by using a grapefruit (Fig. 4) and a birdcage coil for transmitting and receiving the rf signal. In the absence of the metasurface, it is possible to achieve an MR image of a grapefruit with a low spatial resolution using a large field of view (FOV) (see Fig. 4, top left and middle images), while for smaller voxels (smaller FOV) the SNR becomes very low, so that image details such as segments of the grapefruit cannot be resolved properly (see Fig. 4, top-right image). By placing the hybrid metasurface under the grapefruit, we obtain a higher SNR resulting in an enhanced image quality allowing higher-resolution scans to be acquired with an adequate SNR to see more features. In this particular case, more informative images of a pulp structure can be acquired, together with a clear separation of the grapefruit segments, as well as details of a boundary between the pulp and peel (cf. right top and middle images in Fig. 4).

However, in clinical MRI, a signal from a patient is received by an array of closely fitted local receiver coils rather than a much larger single birdcage body coil, which is typically used for transmit. Since the birdcage coil is far from the body, the filling factor is poor and so is the sensitivity to reception. Therefore, we compare a hybrid metasurface with a commercial dedicated four-channel flexible receive coil (Fig. 4, bottom panel). The quality of the image obtained with the metasurface is comparable with the image received by the state-of-the-art local coil (cf. middle and bottom panels in Fig. 4). However, the hybrid metasurface enables us to increase the SNR. Figure 4 (left top panel) shows the MRI image of a grapefruit with a transmit-receive birdcage coil: the SNR in the region of interest is 14.4. Next, the local receive coil has been placed under the object, and an SNR enhancement of 5.7 times in comparison with a birdcage coil is obtained, due to the higher sensitivity of the receive coil and its placement in the close vicinity of the object. Finally, we use a hybrid metasurface and achieve an SNR increase of 7.6 times vs the birdcage coil, and 32% in comparison with the local receive coil. Such a SNR enhancement remains unchanged for different voxel sizes (larger and smaller FOV). The analysis of the metasurface effect on the image quality acquired with different acquisition matrices is included in the Supplemental Material [42]. Hence, the proposed hybrid metasurface can be considered to be more efficient than the commercial coils currently used in clinical MRI. As is mentioned above, a higher SNR potentially leads to more informative images or an ability to perform faster examinations with the same MRI machine.

We note that the SNR decreases with the depth being a physical limitation of any nonvolumetric coil. In the analysis above we consider one of the middle slices of the grapefruit (which is chosen from the multislice data set). The metasurface improves the SNR in comparison with the local coil up to 8 cm in depth (see discussions and experimental results in the Supplemental Material [42]).

V. CONCLUSION AND FUTURE DIRECTIONS

We propose and study experimentally a design of microwave metasurfaces capable of substantially enhancing image quality of commercial MRI machines. Because of a hybrid nature of the design, this metasurface provides a homogeneous enhancement of the rf magnetic field in the region of interest that is particularly relevant to MRI applications. Another distinct advantage of the suggested design is its ability to perform a fine-tuning of the metasurface properties for patient-specific or object-specific investigations. It is worth noting that its eigenmode can be adjusted to a specific frequency of MRI operation even in the presence of different objects, and such a metasurface can be used for the MRI of different nuclei. For the proof-of-principle experiment we change the effective permittivity of the metasurface, thus affecting the properties of the

eigenmode, while in practice other advanced approaches to achieving such a tunability can be involved, e.g., photo-sensitive [44] and nonlinear meta-atoms [45]. The hybrid tunable metasurface acts as a wireless coil enhancing the SNR compared to a body coil transmit-receive more than 7 times in the region of interest leading to a better image quality.

It is important to mention that there have been many alternative concepts proposed to increase the intrinsic sensitivity of MRI, such as the use of multiple receivers [46], dielectric pads [47], passive resonant repeaters [48,49], the dissolution dynamic nuclear polarization method [50], digitally controlled passive elements [51], and magnetoinductive waveguides [52]. The proposed metasurface-based approach can be seen very much as a complementary method that could be combined with the recently developed fully functional, printed, and flexible MRI coils [53] or with structures based on very high permittivity materials [54], to provide an even greater practical impact. Equally well, the design of advanced electromagnetic structures based on metatechnologies can be regarded as a step towards completely novel devices with superior characteristics and techniques for clinical MRI applications.

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APPENDIX A: EXPERIMENTAL SETUP

We realize the hybrid metasurface as an array of 14×2 brass wires. Edges of the wires are inserted up to 25 mm into the plastic boxes, fillable by distilled water with a permittivity of $\epsilon = 78 + 0.2i$ at room temperature. First, we perform measurements of the resonance frequency shift as a function of the water level. For this purpose, the copper loop antenna is placed on top of the phantom (filled with tap water) located in the central part of the metasurface. The phantom parameters are material $\epsilon = 78 + 3.8i$, length = 130 mm, width = 90 mm, and height = 80 mm. The structure is placed inside a 1.5-T Siemens Magnetom Espree MRI machine and we analyze the reflection

coefficient of the loop antenna with the aid of a Planar TR1300/1 compact network analyzer.

To obtain the dependence of the signal as a function of the tip angle (Fig. 2) the birdcage coil is used for transmitting and receiving the signal. We collect images for cases, with and without the metasurface, and calculate the SNR in each scenario. The SNR is determined by the average value of the signal in the region of the phantom divided by the standard deviation of the noise in the signal-free area of the image. We use a spoiled gradient-echo sequence with the following parameters: FOV $163 \times 326 \text{ mm}^2$, TR/TE1010/12.2 ms. Owing to the fact that the hybrid metasurface also enhances the rf transmitted magnetic field amplitude, each point in Fig. 2(a) has been acquired for an optimal rf power level, corresponding to the maximum of the signal, in order to avoid overtipping [the phenomenon when $\lambda(r)\theta_{\text{nominal}} > \pi/2$] in the region of interest. By tuning the eigenmode frequency closer to the nuclear magnetic resonance frequency the rf power level is decreased. Also, it is important to note that in the case of the metasurface we use distilled water as dielectric blocks; this slight influence on the level of the MR signal due to the water provides an additional signal to the phantom signal. To properly account for this effect, for all scans without the metasurface we place similar blocks with the water around the phantom. The data from Fig. 3 are acquired in the same way.

To perform the image-quality evaluation (see Fig. 4), we take a grapefruit that provides a rather good contrast in gradient-echo MR images. We consider one of the middle slices of the grapefruit (which is chosen from the multislice data set) at approximately 4 cm from the metasurface. A spoiled gradient-echo sequence with the following settings is used to perform MRI scans: acquisition matrix, 256×256 ; TR/TE 900/28 ms; optimal tip angle (corresponding to maximum of the signal) for the case with a metasurface, 14° ; for the case without a metasurface, 75° ; for the local receive coil, 65° . For comparison with a commercial receive coil, we employ a four-channel large flex receive coil from Siemens. The rf power level is adjusted in each case to obtain the maximum signal. To image different voxel sizes, we use FOV = $180 \times 180 \text{ mm}^2$, FOV = $120 \times 120 \text{ mm}^2$ and, in order to get the smaller voxel size, we reduce the FOV to $60 \times 60 \text{ mm}^2$. Also, it is important to notice that the signal strength decreases for images with a smaller voxel size, so color bars (Fig. 4) correspond only to the images with the same voxel size.

APPENDIX B: NUMERICAL SIMULATIONS

The numerical simulations are performed by using the Frequency Domain solver of CST Microwave Studio 2016. We use the plane-wave excitation (propagating in the x direction with the electric field polarized along the wires) and the PML boundary conditions to calculate the eigenmode

profile [Fig. 1(a)]. The used parameters of the metasurface are an array 14×2 , wire length $L = 255 \text{ mm}$, period $a = 10 \text{ mm}$, and radius $r = 1 \text{ mm}$. The wires are brass placed in a dielectric background material with $\epsilon = 78$. The hybrid metasurface is placed in the background with $\epsilon_1 = 1$ and the edges of wires (25 mm of metal from each side) are inserted into high-permittivity dielectric pads with $\epsilon_2 = 78$ and the following geometrical dimensions: height (variable) = 106–198 mm; length = 130 mm; width = 380 mm. The metasurface is inserted in the center of the dielectric pads. In order to shift the hybrid metasurface eigenmode closer to the 63.8 MHz, the wire length is increased to $L = 331 \text{ mm}$.

In order to analyze the effect of metasurface tunability, we study the reflection coefficient of a loop antenna made from the brass material with the radius of 40 mm and wire diameter of 2 mm. To properly evaluate the resonance frequency shift, we include the MRI phantom to the simulations. The phantom is placed on top of the metasurface in the center and is represented by the following parameters: material $\epsilon = 78 + 0.2i$, length = 130 mm, width = 90 mm, and height = 80 mm. The distance between the loop and surface of wires is 100 mm. In the numerical simulations, we also place our structure inside a copper cylinder with an internal diameter of 589 mm and a length of 1200 mm, which mimics the properties of a real scanner bore, to include the impact of a rf shield of a scanner on the metasurface resonance frequency shift.

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