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NOTICE

The above identified patent application is available for licensing. Requests for information should be addressed to:

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1	MOBILE X-RAY UNIT
2	BACKGROUND OF THE INVENTION
3	<u>DACKGROUND OF THE INVERTION</u>
4	1. Field of the Invention
5	
6	The present invention relates to X-ray machines and, more
7	
,	particularly, to a battery operated X-ray machine having an
8	improved circuit arrangement so as to generate intense relatively
9	short pulsed of X-rays. This invention allows for the overall
10	weight of the X-ray machine to be reduced with a corresponding
11	reduction in its physical size so that it more advantageously
12	serves as a portable device.
13	
14	2. Description of the Prior Art
15	X-ray machines that generate X-rays from cold field emission
16	of electrons from the cathode of an X-ray tube are commonly
17	employed in pulsed shadowgraph radiographs. Pulsed or flash
18	shadowgraph radiograph was developed in 1938 as a means for
19	observing extremely rapid motion where the subject was obscured
20	from observation with visible light or debris. To date, flash
21	radiography remains the principal means of observing lensed
22	implosions and ballistic impacts over microsecond and nanosecond
23	time scales. The majority of these X-ray systems utilize the
24	well known Marx generator which can be viewed as a distributed

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transmission-storage line, consisting of n-cascaded high-voltage barium titanate disc capacitors. To produce X-rays, the Marx generator is coupled to a field-emission X-ray tube either directly or by coaxial cables. Coaxial cables provide a low impedance energy store and can be rapidly discharged into the Xray tube.

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When high voltage (H.V.) pulses arrive at the anode of the 8 X-ray tube they establish a large potential gradient in the 9 10 anode-cathode gap. This gradient produces an intense electric field at the tips of the small metal whiskers which are present 11 on the surface of the cathode mesh. The whiskers are heated by 12 the passage of the field emission electron current and vaporize, 13 creating a neutral plasma which acts as a virtual cathode capable 14 of supporting a much larger current. Electrons emitted from the 15 expanding virtual cathode are accelerated by the electric field 16 in the anode-cathode gap and eventually collide with the anode 17 creating X-rays by the usual Bremmstrahlung and line radiation 18 processes. Electrons continue to cross the anode-cathode gap 19 until the expanding cathode plasma reaches the anode at which 20 21 time the X-ray tube impedance drops to a few ohms and effectively 22 shorts the tube.

While Marx generator driven X-ray systems have worked well
in the past, they have employed large transformer-rectifier high

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voltage power supplies for charging the Marx capacitors and 1 generally use heavy coaxial cables to couple the Marx generator 2 to the X-ray tube. The heavy coaxial cables act to sharpen the 3 high voltage pulses produced by the Marx generator but, the 4 physically large bundle of cables disadvantageously adds to the 5 weight of the X-ray machine so as to hinder its portability. 6 Further more, the heavy high voltage power supply also 7 disadvantageously contributed to the weight of the X-ray machine 8 while also hindering its maneuverability. It is desired that a 9 means be provided that reduce the overall weight of the X-ray 10 machine, while also eliminating the need for the heavy coaxial 11 cables with both features contributing to an X-ray unit that is 12 truly portable. More particularly, it is desired that a compact 13 and portable design for X-ray machines be provided so that the X-14 ray machine may advantageously be used in remote locations, as in 15 X-ray imaging devices for medical diagnostics and also for triage 16 related to medical disasters. 17

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OBJECTS OF THE INVENTION

Accordingly, it is a primary object of the present invention to provide an X-ray machine that is of a relatively light-weight, about 26 pounds, occupies less than one half of a cubic foot, and may serve as a compact and portable device for use in remote



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1 locations requiring ease of mobility.

It is the object of the present invention to provide a
portable X-ray machine that develops an intense pulse of X-rays,
but also has variable accelerating voltage so as to accommodate
various X-ray applications.

6 Another object of the present invention is to provide a 7 portable X-ray unit that generates a high dose X-ray pulse, which 8 has a short time duration, 10-100 nanoseconds. This short X-ray 9 pulse eliminates the need for long integration time, so that it 10 advantageously may be used for high resolution digital detector 11 arrays.

Detector arrays, such as charge coupled device(CCD) or a amorphous silicon devices both of which are used in digital processing cameras have high dark currents when integrating over long time exposures unless cooled to about 0° Fahrenheit; the dark current of these devices decreases their sensitivity.

Furthermore, it is an object of the present invention to provide an X-ray unit that may be used for dental X-ray imagery and controlled by a portable computer, such as a notebook computer, when used in remote or confined spaces or used for Xray inspection, security detection, and medical applications requiring high quality X-ray images.

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SUMMARY OF THE INVENTION

The present invention is directed to an X-ray unit which is 3 4 relatively light-weight, thereby contributing to its portability, yet generating hard X-ray pulses without the need of any coaxial 5 cables between its Marx generator and its X-ray tube. 6 The X-rav 7 unit comprises a high vacuum X-ray tube having a conical anode surrounded by a coaxial annulus of stainless steel mesh which 8 serves as the cathode, control electronics, and a plurality of 9 10 spark gap switches and ceramic disc capacitors which form the 11 Marx generator 18. The battery powered control electronics comprises: the H.V. power supply, Ultraviolet (U.V.) flash-gap 12 13 assembly 57, and power management circuit. The control electronics 20 can receive either a manual, an optical, or an 14 electrical pulse and use that pulse to trigger the X-ray unit. 15

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17 The control electronics also generates a sync pulse whenever 18 the Marx generator is triggered and this pulse is brought to the 19 front panel of the control electronics enclosure 20 so that it 20 can be used to synchronize or command other devices to fire with 21 the Marx generator.

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23 The energy storage capacitors within the Marx column are24 surrounded with an insulating pressurized shell 12 and covered by

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1	a close fitting aluminum cylinder 32 which acts as the outer
2	conductor of a lumped coaxial transmission line. The outer
3	aluminum cylinder also functions as a very effective Faraday
4	shield preventing the escape of potentially harmful
5	electromagnetic radiation from the pulsed X-ray unit.
6	BRIEF DESCRIPTION OF THE DRAWINGS
7	
8	These and other objects, features and advantages of the
9	invention, as well as the invention itself, will become better
10	understood with reference to the following detailed description
11	when considered in connection with the accompanying drawings,
12	wherein like reference numbers designate identical or
13	corresponding parts throughout the several views and wherein:
14	
15	Fig. 1 illustrates a mobile X-ray unit in accordance with
16	the present invention.
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18	Fig. 2 is a block diagram of the essential functions related
19	to the present invention.
20	
21	Fig. 3 is a schematic diagram of the portion of the control
22	electronics of the present invention.

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1	Fig. 4 is a schematic diagram of the further section of the
2	control electronics of the present invention.
3	
4	Fig. 5 is a blow-up of the pulsed power circuit of device 57
5	
6	Fig. 6 is a schematic illustrating some of the mechanical
7	features of the Marx generator of the present invention.
8	
9	Fig. 7 is an equivalent circuit of the Marx generator of the
10	present invention.
11	
12	Fig. 8 illustrates the X-ray tube assembly of the present
13	invention.
14	
15	Fig. 9 Details the X-ray unit in one typical application
16	thereof.
17	
18	DETAILED DESCRIPTION OF THE EMBODIMENTS OF THE INVENTION
19	
20	Before the drawings are discussed, it should be noted that
21	the mobile X-ray unit of the present invention is of a relatively
22	light-weight, about 26 pounds, and provides a Marx generator that
23	contributes to the production of high power X-ray pulse having a
24	predetermined duration and adjustable accelerating potential.

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The Marx generator comprises a plurality of capacitors that are
 discharged in several nanoseconds thereby eliminating the need of
 any pulse sharpening commonly performed by coaxial cables
 discussed in the "Background" section.

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6 One embodiment of the present invention is illustrated in 7 Fig. 1 for the mobile X-ray unit 10. The mobile X-ray unit 10 8 comprises two aluminum enclosures 32 and 14, with the enclosure 9 32 housing an X-ray tube assembly 16 and a Marx generator 18, and 10 with enclosure 14 housing control electronics 20 (not shown, but 11 to be described with reference to Figs. 2, 3 and 4,5).

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13 The pressurized housing 12, encloses the Marx generator 18,
14 and forms a pressure seal at o-ring 138 at end plate 133,
15 described with reference to Figs.6

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The Marx generator 18 comprises a plurality of capacitors
C1, C2,... and C10 that operate together with a plurality of
spark-gap switches G1, G2,... and G10. and Clamping diodes Cd1,
Cd2....Cd10 referred to later. The charge state of the marx
capacitors C1, C2 ... C10 is indicated by light emitting diode
bar graph array 42 as M1, M2,... and M10 mounted on enclosure 14.

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The enclosure 14 also contains provisions for accommodating 1 2 a digital volt meter (DVM) 38, a potentiometer 40 that adjusts the voltage generated by the Marx generator 18, and a dot/bar 3 graph display 42 that shows the charged state of the Marx 4 generator 18. The enclosure 14 also provides a housing for 5 receiving a fiber optic trigger input 44, a connector 46 for the 6 receipt of a transistor transistor logic (TTL) trigger input, and 7 a connector 48 making available a TTL trigger sync output. 8 Further, the face of the enclosure 14 allows for mounting of a 9 rotary switch 50, a manual trigger push button 52, a power on-off 10 switch 54, and a battery charge input 56. The enclosure 14, in 11 particular, the control electronic 20 within the enclosure 14 12 provides signals and functions for the Marx generator 18, via a 13 cable 58 carrying, a high voltage (HV) trigger signal and a high 14 voltage cable 60. 15

16

The Marx generator consists of a plurality of high voltage 17 ceramic disc capacitors and spark gap switches. The capacitors 18 contained in the Marx column 18 are charged to a H.V. in parallel 19 via bleeder resisters RA in the resister chain. Each spark gap 20 switch G1-G10, consists of two closely spaced spherical 21 electrodes. The spark gap switches are arranged so that each 22 charged capacitor C1-C10 in the Marx column is isolated from all 23 other capacitors via resistors RA. The spark gap switches are 24

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mounted along a common optical axis together with an ultraviolet
 photoionization source 59, from the control electronics 20, and
 mounted in close proximity to the first spark gap switch G1,
 within the marx column 18.

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Triggering of the Marx column begins with the control 6 electronics 20 which initiates a high voltage trigger pulse from 7 a H.V. trigger transformer 82 via path 102 into spark-gap device 8 57. Breakdown of this spark gap switch causes its impedance to 9 collapse from an open circuit to a low impedance spark channel 10 having a few tens of milliohms of resistance. This device 57, now 11 transfers the energy stored in capacitor C0 to device 59 by way 12 of path 58. The U.V. photoionization source 59 emits a large 13 flash of hard U.V. created by the discharge of capacitor CO into 14 device 59 which is connected to the ground plane of the device 15 10. 16

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18 The hard U.V. emitted from device 59 photoionizes spark gap
19 G1, the closure of this switch places the first capacitor in the
20 Marx column C1 in series with the second capacitors in the column
21 C2 doubling the voltage across the second spark gap switch G2.
22 The increased voltage stress across the second spark gap together
23 with the hard ultraviolet illumination it receives from the
24 closure of the first spark gap switch G1 causes it to break down

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quickly. This process continues at an accelerating rate until
 all capacitors in the Marx column are fully erected in series and
 have formed the center conductor of the coaxial device.

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The full Marx voltage now appears across switch G10 which is 5 connected to power feedthrough device 128 which transmits the 6 H.V. output of the Marxed capacitors to the anode 28 of the X-ray 7 tube 16, via conducting tube 168. The X-ray tube assembly 16 is 8 held within the enclosure 32 by the clamping arrangement 22. The 9 X-ray tube assembly 16 has a vacuum window 24, through which X-10 rays are emitted, and a cathode 26 and an anode 28 having one of 11 its ends connected to a screw connection 30 that is mechanically 12 engaged by a complementary arrangement, to be described with 13 reference to Fig.8 The X-ray tube assembly 16 is mechanically 14 connected to the system 10 by way of a mating contact plugged 15 into feedthrough power connector 128. The outer conducting member 16 162, of the X-ray tube 16, is clamped into the outer shell 32 by 17 means of screws 22 placed 120 degree's apart. Application of 18 the full Marx potential across the anode-cathode gap of the X-ray 19 tube 16 produces an intense electric field between the wires in 20 the mesh of the cathode and the surface of conical shaped anode. 21 This electric field extracts electrons from the cathode by the 22 process of cold field emission. The electrons accelerate towards 23 the anode where they collide and produce Bremmstrahlung and K-24

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line radiation. This radiation continues until the plasma
 produced at the cathode crosses the gap and shorts out the tube.
 Plasma closure in our tube sets the X-ray pulse width at 50
 nanoseconds.

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6 The operation of the control electronics 20 may be further 7 described with reference to Fig. 3 illustrating a plurality of 8 circuit elements indicated by conventional symbols, such as a 9 resistance symbol, and identified by typical component values and 10 also illustrating various logic elements most identified with the 11 term Q serving as their indicated logic function and some of 12 which logic elements are of the type given in Table 1.

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14 15

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TABLE 1

16	NOMENCLATURE	FUNCTION/TYPE
17 18	Ql	HEWLETT PACKARD (HP-R-2503) OPTICAL
19 20	Q2	RECEIVER PULSE STRETCHER (LM555)
21 22	Q5 Q6	5 VOLT REGULATOR (7805) ENCO 300 VOLT SUPPLY)
23	Q9	DUAL TIMER (LM556)

The control electronics 20 have the capability of accepting either of three input signals, each of which serves as a trigger to start the operation of an X-ray mobile unit 10 for the generation of the associated X-rays. The three input signals are: (a) the optical pulse of 650 nanometers, present on signal

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path 68 and received by the Q1 device. (b) the input from connector 46 the pulse generated by the TTL logic present on signal path 66 and accepted by the Q3 device. (c) and a manual pulse generated by the manually activated push-button 52. The selection of either of these three input signals is accomplished by the selection of the rotary switch 50 arranged as shown in Fig. 3.

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Either of these input signals activates the Q2 device so 9 that the control electronics 20 will not respond to another input 10 signal for a predetermined time, such as 330 milliseconds, which 11 reduces the unwanted possibility of repetitive triggering caused 12 by closely spaced input pulses. The Q2 device produces an output 13 pulse which is then shaped by edged differentiation provided by 14 the circuit components on the input stage of the Q4C nand gate 15 which inverts its received signal and transfers it to the base of 16 a common emitter formed by element Q5 and its associated circuit 17 The inverted output of nand gate Q4C is also routed 18 components. to a further nand gate Q4D which, in turn, provides a sync output 19 to connector 48 which, in turn, provides the sync pulse on to 20 signal path 78, to be described with reference to Fig. 9. 21

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23 The collector of the Q5 device is connected to the primary
24 of a toroidal trigger transformer 80. The pulse signal present

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at the primary of transformer 80 appears across the secondary of 1 transformer 80 and triggers an SCR device, indicated as D6, which 2 discharges the 1.0 microfarad capacitor connected to the anode of 3 The energy discharge of the 1 μ f capacitor is applied to D6. 4 signal path 70 that is routed to a H.V. trigger transformer 82 5 that assists in rendering the first spark-gap device 57 6 conductive in a manner as to be described with reference to 7 Fig. 5. 8

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In addition, the control electronics 20 contain a battery 10 charged state indicator circuit Q8-Q11, that indicates when the 11 X-ray mobile unit 10 battery 81, preferably a 12 volt device, 12 needs to be charged. This indication is accomplished by flashing 13 the back light of the digital voltage meter 38, see Fig.1 14 The flashing of the DVM black-light is accomplished by the 15 operation of the Q9 device which uses its first timer as a 16 comparator and provides an output that is used to carry the 17 second timer's reset line high. The second timer of the Q9 18 device is now free to oscillate and strobes, via signal path 84, 19 a transistor switch comprised of transistors Q10 and Q11 which 20 sinks, via signal path 86, the current through the LED back-light 21 of the digital voltage meter DVM 38. The 12V output is applied 22 to signal path 88 which is routed to the control electronics 23 illustrated in Fig. 4. The onslaught of the flashing begins when 24

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1	the voltage of th	e 12 volt battery reaches about 9 volts. The
2	remainder of the	control electronics 20 may be further described
3	with reference to	Fig. 4 which illustrates a plurality of circuit
4	elements indicate	d by conventional symbols, such as those of a
5	resistor, identif	ied by typical component values and also
6	illustrates vario	us logic elements most identified with the term
7	Q, and some of wh	ich are given in Table 2.
8		TABLE 2
9 10	NOMENCLATURE	FUNCTION/TYPE
11 12 13 14 15 16 17 18 19	Q12 Q13 Q14 Q15 Q17 38	0-13 kV SUPPLY OF ENCO MODEL 4300 0-12 VOLT SUPPLY OF ENCO MODEL 9414 VOLTAGE REGULATOR (7805) OPERATIONAL AMPLIFIER (OP295) BAR/DOT DISPLAY DRIVER (LM3916) DIGITAL VOLTAGE METER OF MODUTEC (0-200 mV FULL SCALE)
20	The control	electronics 20 of Fig. 4 includes a DC to DC
21	converter compris	ed of elements Q12, Q13, Q14 and associated
22	circuit component	s arranged as shown in Fig. 4. Element Q13, via
23	signal path 88, a	ccepts a voltage signal of approximately 9 - 14
24	volts DC and prod	luces, on signal path 90, a constant 24 volts DC
25	output for currer	at loads of preferably no more than 1 ampere. The
26	element Q12 which	n is a programmable high voltage supply provides
27	a voltage of betw	ween 0 - 13 kV that is applied to the Marx
28	generator 18, via	a signal path 92. The output of the element Q12
29	is regulated to (1.1% no load to full load and can provide .33

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1 milliamps of current at 13kV.

The signal path 60 is routed to the Marx generator 18 by way of a charge line 92 that comprises a ten megohm resistor 93, a seven megohm resistor 95, and a 0.1 microfarad capacitor which is actually capacitor C0 arranged as shown in Fig. 5. The charge line 92 provides an output on signal path 94 that is routed to the Q17 element which is a bar/dot display driver.

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9 The program voltage input to element Q12 is also monitored, 10 via signal path 96, by element Q15A and its associated circuit 11 components acting as a first operational amplifier configured as 12 a voltage follower and which impresses its output voltage across a low voltage divider which is passed onto element Q15B serving 13 as a second operational amplifier. Q15B provides an output signal 14 15 serving as the programming voltage monitor of the H.V. capacitor 16 charging supply, this voltage is routed to the element Q17. The HV output of Q12 is monitored by a 5000x attenuator and is sent 17 18 to element Q17 via signal path 94.

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The difference between the signal developed by elements Q15B and the voltage attenuator is applied to element Q17, this is used to drive Q18 which contains 10 LED's (M1, M2, ... M10 shown in Fig. 4) that indicate the charge state of the Marx generator 18.

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The output voltage (0 - 13 kV) generated by element Q12 is
 adjustable by potentiometers, such as potentiometer 40, that are
 electrically connected, as shown in Fig. 4, to signal paths 96
 and 100.

The charge line 92 that carries the 0 - 13 kV potential has 5 its 10 megohm resistor 93 and its 0.01 capacitor C0 connected 6 between the lower spark-gap terminal 100 or anode electrode of 7 the spark-gap switch 57. A trigger pin wire 102 extends through 8 the outer body of the spark-gap switch 57 and runs, but does not 9 touch, the cathode electrode 100. The trigger pin wire 102 is 10 biased to the fully charged potential of the 0.1 microfarad 11 capacitor (CO) by way of a 7 megohm resistor. The trigger pin 12 wire 102 is connected to a 500 picofarod decoupling capacitor 13 which, in turn, is connected to the trigger transformer 82, whose 14 primary winding is connected to signal on signal path 70 15 previously discussed with reference to Fig. 3. 16

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When the signal present on signal path 70 is applied to the primary side of the trigger transformer 82, it produces a 25 kilovolt pulse at the secondary of transformer 82. When the 25 kilovolt pulse passes through the 500 picofarad decoupling capacitor, it appears as a spark in the air gap between the trigger pin wire 102, the anode electrode 100. The cathode electrode 103 connected to the ground potential via a 100 k

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resistor to be described with reference to Fig. 7. The spark 1 2 photoionizes the region just in front of the cathode 103 which results in the formation of a breakdown channel between the 3 cathode and the anode 100 of the spark-gap switch 57. The plasma 4 produced by the breakdown channel rapidly fills the anode-cathode 5 6 gap of the spark gap device 57, thereby, producing a low resistance path between the 0.1 microfarad capacitor C0 and the 7 U.V. photoionizer source 59 in the Marx generator 18. 8

9 The Marx generator 18 has mechanical features which are
10 important to the present invention and may be further described
11 with reference to Fig. 6.

12

13 Fig. 6 illustrates the enclosure 32 as being cut-away so as 14 to expose the internally housed components primarily related to 15 the Marx generator 18. Enclosure 32 has two inlets 110 and 112 16 which enter the pressurized cylinder, to be described 17 hereinafter, that is confined within the chamber 114. Chamber 18 114 is defined by its conducting aluminum walls, wherein the 19 internal walls thereof fit over an acrylic insulating cylinder 20 116 both of which cooperate in a manner to be described with 21 reference to Fig. 6 to form a return path for the lumped element transmission line formed by the capacitance between the marxed 22 capacitors and the wall of enclosure 32, the connection and 23 24 switching inductance between each capacitor and it's neighbor.

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The Marx generator 18 comprises capacitors C1, C2,...and C10, and
 spark-gap devices G1, G2,... and G10 to be further described
 hereinafter with reference to Figs. 6 and 7 and all of which are
 held by a polycarbonate rod 132.

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The capacitors C1, C2, ... C10 and the spark-gap devices G1, 6 G2,...and G10 are affixed to the polycarbonate rod machined into 7 a spine configuration 132 by appropriate means, known in the art. 8 The polycarbonate spine 132 does not occupy the complete space 9 between the acrylic cylinder 116 but now leaves, at one of its 10 ends, a chamber 120 into which is introduced a pressurized gas, 11 via conduit 122 which may be monitored with a pressure meter 124. 12 The other end of the polycarbonate spine 132 abuts up to within 1 13 mm of the power feedthrough 128. The spine 132 carries and allows 14 for the attachment of a turning mirror 34 previously discussed 15 with Fig. 1, and to be further described with reference to 16 Fig. 6. 17

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19 The power feedthrough 128 also provides a path for the 20 electrical connection between G10 and the X-ray tube 16. More 21 particularly, when the screw electrode 128 is screwed into the 22 insulating spine 132 it causes the Marx generator 18 to be 23 electrically connected to the anode 28. The insulating spine 132 24 shown in Fig. 6, as well as the acrylic cylinder 116, abuts up

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against the O-ring pressurized seal 134. The O-ring pressurized
 seal 134, in cooperation with the aluminum housing 32, provides
 an entrance passageway 136 into which the X-ray tube 16 of Fig. 1
 is inserted. The aluminum enclosure 32 as well as the acrylic
 cylinder 116 mate with a second O-ring pressurized seal 138.

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The O-ring pressurized seal 138 and the enclosure 32 have 7 provisions that provide for the mating with a high voltage 8 connection 140 that is connected to a brass member 142 which, in 9 turn, is connected to the high voltage connector 140, via a 10 The brass member 142 has a diameter of about 1.27 11 conductor 144. centimeters and allows for the soldering thereto of a resistor 12 charging ladder network to be described hereinafter with 13 reference to Fig. 7. 14

In operation, the chamber 114 is pumped to a vacuum pressure 15 of approximately 10⁻³ torr and back filled with dry nitrogen gas 16 to a pressure of preferably about 25 to 30 psi.. The 2 atmosphere 17 pressure of nitrogen gas allows for the spark-gap electrodes G1, 18 G2...and G10, previously discussed with reference to Fig. 4, to 19 be separated by about 1 mm. The capacitors C1, C2,.... and C10 20 are respectively physically separated from each other by barriers 21 146, whereas the spark-gap devices G1, G2, ...and G10 are 22 separated from each other by barriers 148. The barriers 146 and 23 148 comprise and the polycarbonate spine 132. Capacitor C1, C2 24

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... and C10 have a very high dielectric constant of about 7000, 1 and may be further described with reference to Fig. 7. 2 3 Fig. 7 illustrates the Marx generator 18 which is a 4 conventional impulse-type high-voltage circuit in which 5 capacitors C1, C2, ... and C10 are charged in parallel through a 6 high-resistive ladder network formed by resistors R1-R19 having a 7 typical value of 100 k and arranged as shown. When the capacitor 8 voltage reaches a critical value, such as 13 kV, the capacitors 9 are discharged in series through the spark-gap devices G1, G2... 10 and G10 in response to a trigger signal, produce a high-voltage 11 pulse which is applied to the anode 28 of the X-ray tube 16. 12 13

Fig.7 shows an equivalent circuit of the Marx generator 18 14 that employs clamping diodes Cd1, Cd2, Cd3, Cd4, Cd5, Cd6, Cd7, 15 Cd8, Cd9 and Cd10 arranged as shown, that act to dampen any 16 negative ringover associated with the capacitors when the 17 capacitors are discharged into the inductance of the X-ray tube 18 The Marx generator 18, in particular the first stage thereof 19 16. having the spark-gap device G1 previously discussed with 20 reference to Fig. 4, preferably utilizes an ultraviolet initiator 21 which may be described with reference to Fig. 7. 22

Fig. 6 illustrates the turning mirror 34, which as discussed
directs the hard, ultraviolet light pulse. Fig. 5 further

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illustrates how the turning mirror is positioned within the 1 insulating spine 132. The turning mirror tilted 45⁰ from the line 2 of sight of spark gap switches G1-G9 so that it directs the 3 ultraviolet light pulse to the region between the electrodes 130 4 and 128 of spark-gap device G10 located at the output stage of 5 the Marx generator 18. As previously discussed with reference to 6 Fig. 4, the discharge of the 1 microfarad capacitor onto signal 7 path 70 is applied to the trigger transformer 82 which develops 8 at its secondary a 25 kV pulse. When the 25 kV pulse passes 9 through the 500-picofarad decoupling capacitor, it appears as a 10 spark in the gap between the trigger pin wire 102 and anode and 11 cathode and anode electrodes 100 and 103. As previously discussed 12 with reference to Fig. 4, the spark transitions the normally high 13 resistance path between the cathode and anode electrodes of 14 device 57 to a low resistance path. One end of the low 15 resistance path is indicated with the reference number 58 16 previously discussed with reference to Fig. 5a. 17

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19 The low resistance spark channel formed in device 57 causes 20 the rapid discharge of capacitor C0 through path 58. Cable 58 21 enters the Marx unit 18 and is connected to the U.V. initiator 59 22 which emits a large flash of hard U.V. and causes the sequential 23 cascaded discharge of the capacitors C1-C10 which have been 24 charged parallel through Resistor chain R1-R19 described in

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fig.7, are then discharged through spark gap switches G1-G10.
 This path formed by the spark gap switches G1-G10 forms the
 center conductor of the coaxial device 10.

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The capacitors C1- C10 have a typical value of 0.01 μf and 5 are arranged on the polycarbonate 118 spine 132 as illustrated in 6 Fig. 6, further, the separation between the capacitors provided 7 by the polycarbonate rod 132 decrease the interstage capacitance. 8 The low interstage capacitance, in cooperation with the 9 relatively low inductance of the spark gap switches G1-G10, 10 allows the capacitors C1- C10 to completely discharge into the X-11 ray tube 16 within nanoseconds. This fast discharge eliminates 12 the need for any coaxial cables which would normally be used to 13 sharpen the high-voltage pulse emerging from the Marx generator. 14 The elimination of these coaxial cables reduces the overall 15 weight of the mobile X-ray unit 10, while increasing its 16 mobility. 17

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19 The mobile unit 10 having the parameters hereinbefore
20 described provides for the generation of a high voltage pulse
21 having a duration of less than 100 nanoseconds. This high
22 voltage, high energy pulse is adjustable by means of the
23 potentiometers shown in Fig. 4, in particular, the potentiometers
24 electrically connected to signal paths 96 and 100. The high

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voltage pulse developed by the Marx generator 18 is applied to
the anode 28 of the X-ray tube 16 by means of the spark gap
electrode 130 shown in Fig.6

The x-ray tube 16, shown in Fig.8, is a field emission type 4 comprised of a geometric arrangement of anode 28 and cathode 26 5 derived from the well known "Siemens-tube" configuration. More 6 particularly, the X-ray tube 16 has a conical copper/tungsten 7 anode 28, and a stainless steel mesh punched to form an anode 8 cathode 26. The X-rays are extracting from the X-ray tube along 9 a tube axis and as a result of a conical anode 28, the emitting 10 area is about 2 mm in diameter. The X-ray tube 16 uses a 11 commercially available 30 kV DC ceramic insulator 158 bonded to 12 conflat flanges 160 and 162 each having a typical diameter of 13 2.75 inches. The conflat flanges 160 and 162 are mated to a 14 stainless steel tube 164 having a typical outer diameter of 1.5 15 inches and an inner diameter of 1.375 inches. The stainless 16 steel tube is connected to an adapter plate 166. 17

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19 The anode stalk 168 is a tube having a typical outer 20 diameter of 0.24 inches and a typical inner diameter of 0.125 21 inches. The x-ray tube is evacuated through the center of the 22 anode tube by way of holes 170,172 and 174 arranged in a spiral 23 so as not to weaken the anode tube 168.

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As seen in Fig. 1, the enclosure 20 encloses and confines the main power producing components that generate the high voltage potentials of 0 - 13 kV. The charge lines 58 and 60 comprise coaxial cable that carries a relatively high voltage of 0 - 13kV and whose outer conductor, enclosure 32 provides a return path for the charge line 92.

It should now be appreciated that the practice of the 8 present invention provides for an X-ray mobile unit 10 having 9 compact electronics so as to provide complete shielding against 10 electromagnetic interference. Further, it should be appreciated 11 that the present invention utilizes electronic components that 12 are relatively small so that the overall weight of the mobile X-13 ray unit 10 is approximately 26 pounds. Further, it should be 14 appreciated that the mobile X-ray unit 10 has the ability, via 15 the potentiometers shown and described with reference to Fig. 4, 16 to develop an excitation that is applied to the Marx generator 18 17 which develops a high voltage output signal having an amplitude 18 which is adjustable to adapt to various applications, one of 19 which may be further described with reference to Fig. 9. 20

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Fig. 9 illustrates an arrangement that includes a notebook
computer 178, known in the art, which is connected to the sync
output 48 of enclosure 14 having thereon a trigger output signal

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1	placed on signal path 78, previously described with reference to
2	Fig. 3. The notebook computer 178 has an output cable that is
3	connected to a CCD x-ray camera 182.
4	
5	Portability of the notebook computer 178, the CCD camera
6	182, and the mobile X-ray unit 10 allows for the practice of the
7	present invention to be utilized in: Dentist's offices, medical,
8	Veterinary offices and security applications. The unit can
9	provide a high quality image; produced by the mobile X-ray unit
10	10 of the present invention.
11	
12	It should now be appreciated that the practice of the
13	present invention provides for a mobile X-ray unit 10 utilized
14	for various applications.
15	
16	It should further be thoroughly understood that many
17	modifications and variations of the present invention are
18	possible within the purview of the claimed invention. It is
19	therefore to be understood
20	, the invention may be practiced otherwise than as
21	specifically described.



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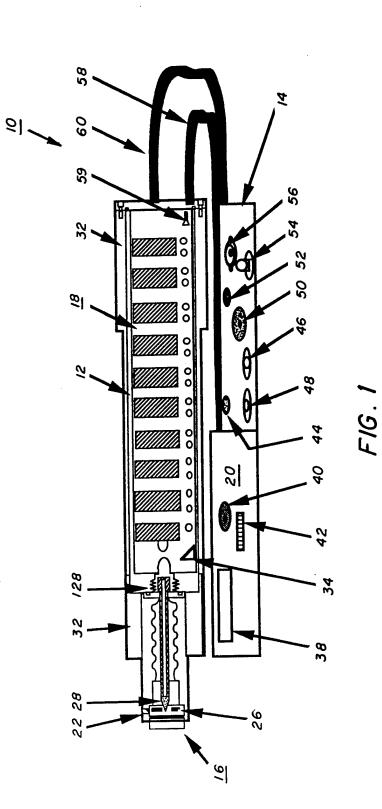
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ABSTRACT OF THE DISCLOSURE

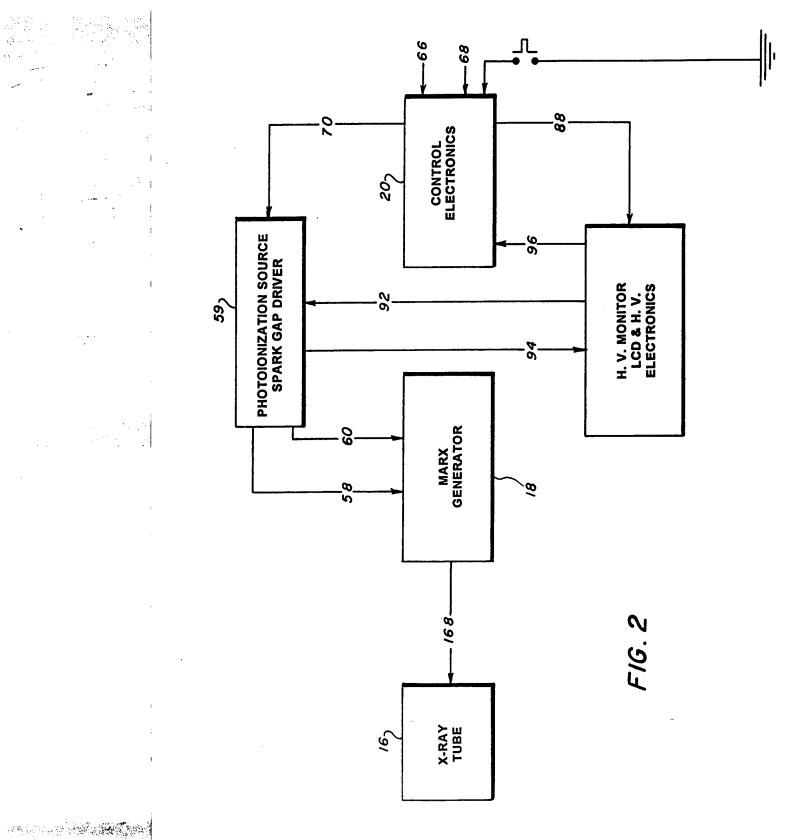
A portable X-ray unit, of a relatively light-weight, occoping 4 a volume of less then one-half a cubic foot containing an x-ray 5 head assembly, a unique Marx generator, a plurality of spark-gap 6 7 switches and control electronics is disclosed. The Marx generator allows for the development of a relatively high voltage 8 9 in excess of 100 kV, yet allows for the discharge thereof within the nanosecond range. The Marx generator is enclosed by an 10 11 acrylic insulator that cooperates with an aluminum enclosure, 12 which functions as a return current path for the capacitors in 13 the Marx generator and also as a shield against the escape of 14 electromagnetic radiation from the pulsed x-ray unit. The Marx 15 generator and spark-gap switches are confined within the 16 pressurized chamber that may contain nitrogen gas to reduce the separation of the gap in the spark-gap switches. 17



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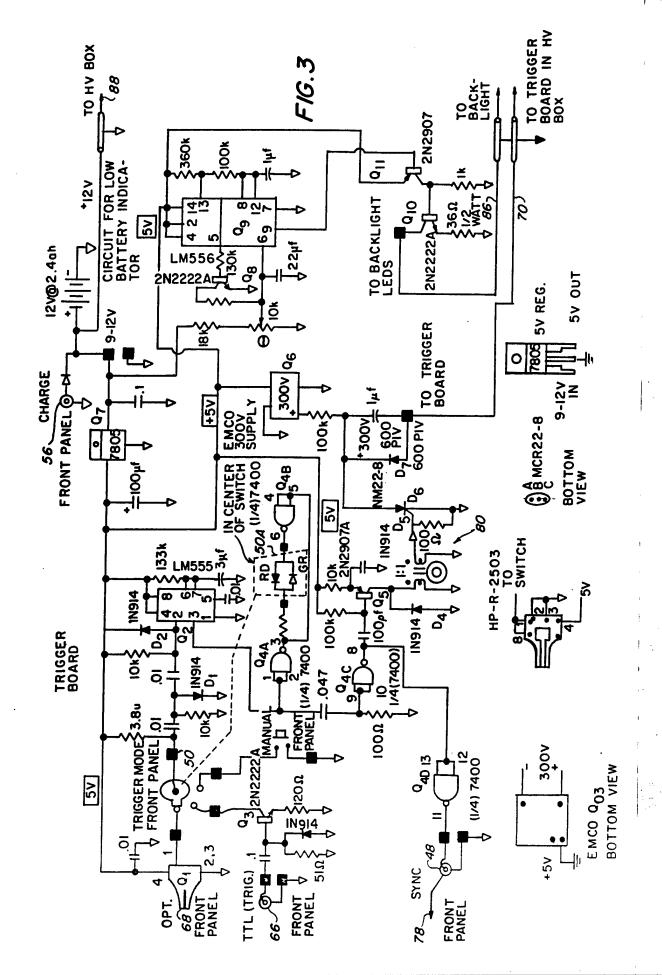
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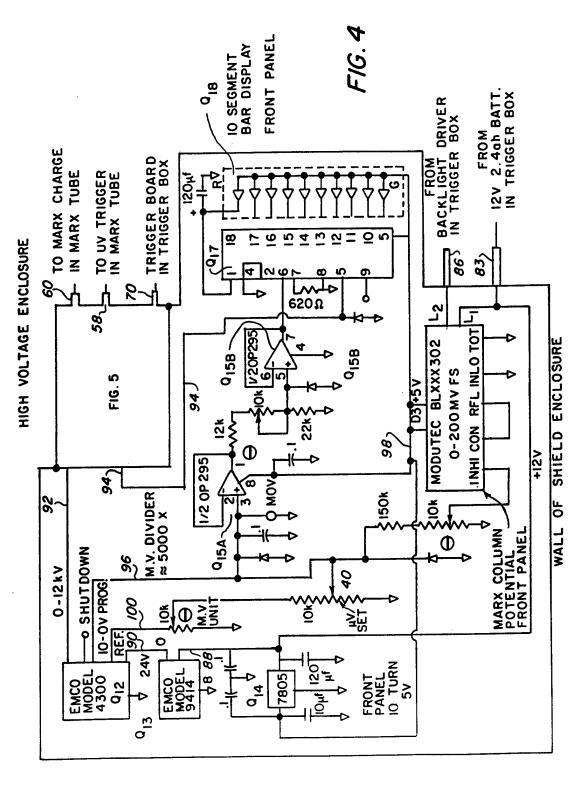


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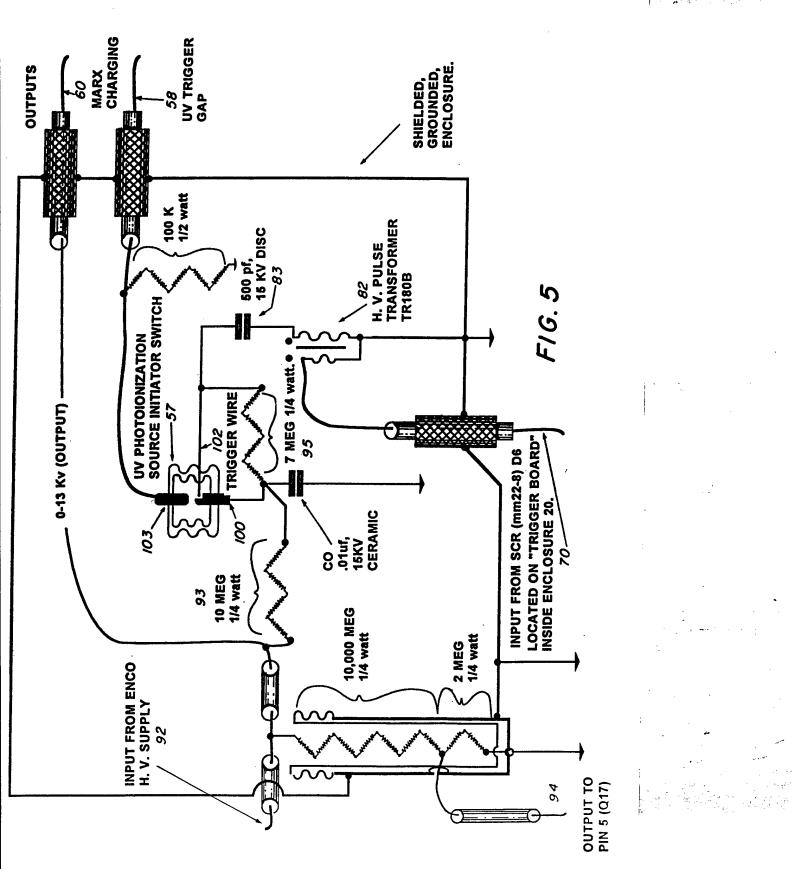
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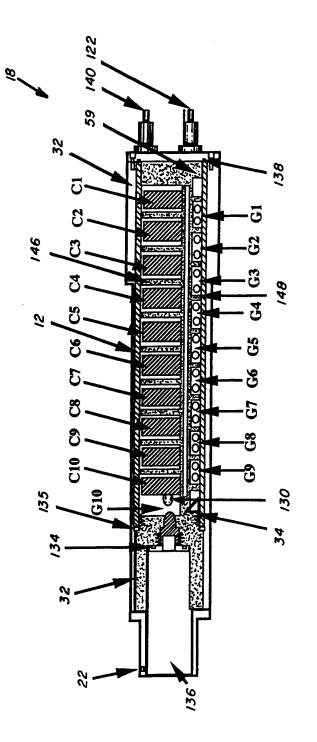
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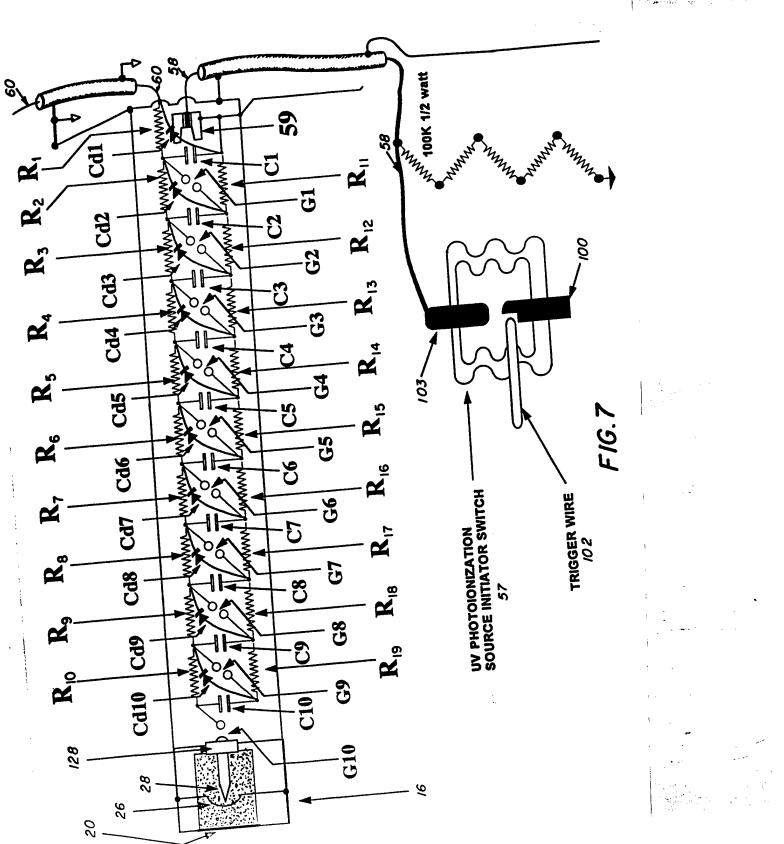
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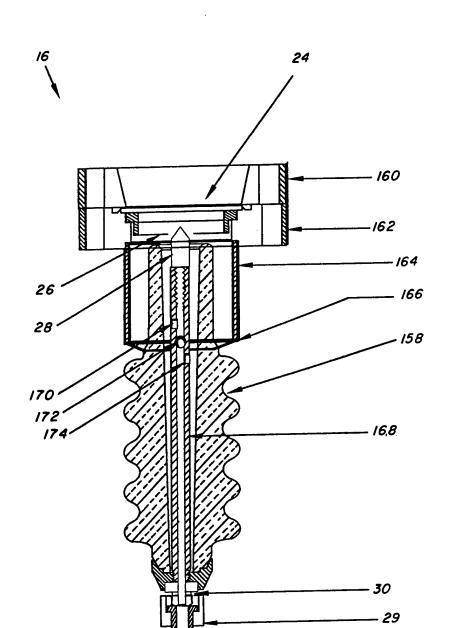
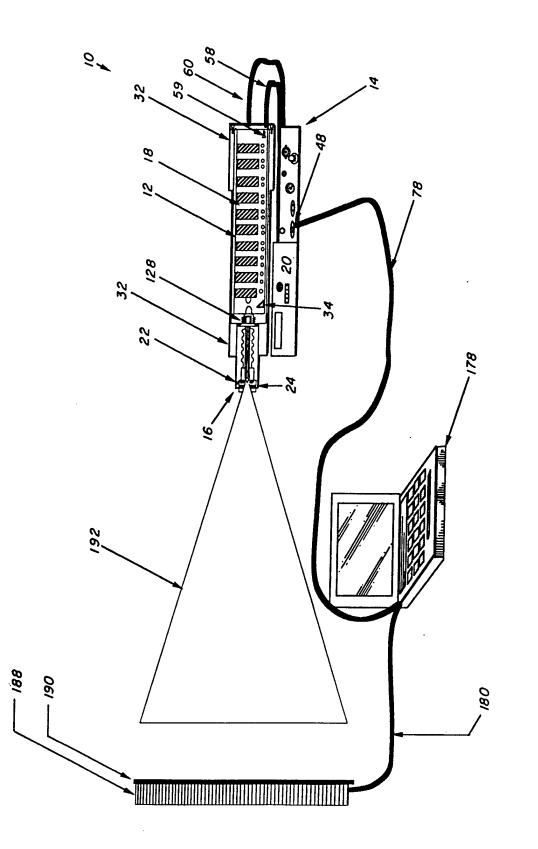


FIG. 8

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