## Network Physiology reveals relations between network topology and physiological function

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The human organism is an integrated network where complex physiologic systems, each with its own regulatory mechanisms, continuously interact, and where failure of one system can trigger a breakdown of the entire network. Identifying and quantifying dynamical networks of diverse systems with different types of interactions is a challenge. Here, we develop a framework to probe interactions among diverse systems, and we identify a physiologic network. We find that each physiologic state is characterized by a specific network structure, demonstrating a robust interplay between network topology and function. Across physiologic states the network undergoes topological transitions associated with fast reorganization of physiologic interactions on time scales of a few minutes, indicating high network flexibility in response to perturbations. The proposed systemwide integrative approach may facilitate the development of a new field, Network Physiology.

Physiologic systems under neural regulation exhibit high degree of complexity with nonstationary, intermittent, scale- invariant and nonlinear behaviors [1, 2]. Moreover, physiologic dynamics transiently change in time under different physiologic states and pathologic conditions [3–5], in response to changes in the underlying control mechanisms. This complexity is further compounded by various coupling [6, 7] and feedback interactions [8–10] among different systems, the nature of which is not well-understood. Quantifying these physiologic interactions is a challenge as one system may exhibit multiple simultaneous interactions with other systems where the strength of the couplings may vary in time. To identify the network of interactions between integrated physiologic systems, and to study the dynamical evolution of this network in relation to different physiologic states, it is necessary to develop methods that quantify interactions between diverse systems.

Recent studies have identified networks with complex topologies [11–13], have focused on emergence of selforganization and complex network behavior out of simple interactions [14–17], on network robustness [18–20], and more recently on critical transitions due to failure in the coupling of interdependent networks [21]. Growth dynamics of structural networks have been investigated in network models [11, 13], and in physical systems [13, 22], and various structural and functional brain networks have been explored [22, 23]. However, understanding the relation between topology and dynamics of complex networks remains a challenge, especially when networks are comprised of diverse systems with different types of interaction, each network node represents a multicomponent complex system with its own regulatory mechanism, the output of which can vary in time, and when transient output dynamics of individual nodes affect the entire network by reinforcing (or weakening) the links and changing network topology. A prime example of a combination of all these network characteristics is the human organism, where integrated physiologic systems form a network of interactions that affects physiologic function, and where breakdown in physiologic interactions may lead to a cascade of system failures [24].

We investigate the network of interactions between physiologic systems, and we focus on the topology and dynamics of this network and their relevance to physiologic function. We hypothesize that during a given physiologic state the physiologic network may be characterized by a specific topology and coupling strength between systems. Further, we hypothesize that coupling strength and network topology may abruptly change in response to transition from one physiologic state to another. Such transitions may also be associated with changes in the connectivity of specific network nodes, i.e., the number of systems to which a given physiologic system is connected can change, forming sub-networks of physiologic interactions. Probing physiologic network connectivity and the stability of physiologic coupling across physiologic states may thus provide new insights on integrated physiologic function. Such a systems-wide perspective on physiologic interactions, tracking multiple components simultaneously, is necessary to understand the relation between network topology and function.

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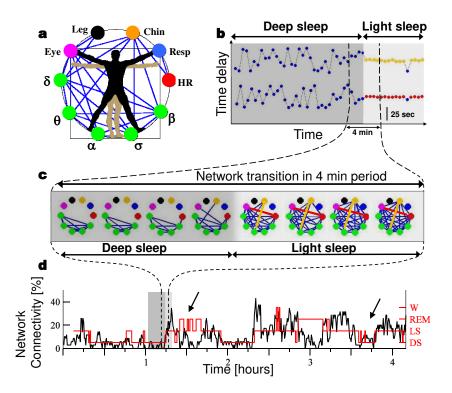


FIG. 1. Transitions in the network of physiologic interactions. (a) Dynamical network of interactions between physiological systems where ten network nodes represent six physiologic systems – brain activity (EEG waves:  $\delta$ ,  $\theta$ ,  $\alpha$ ,  $\sigma$ ,  $\beta$ ), cardiac (HR), respiratory (Resp), chin muscle tone, leg and eye movements. (b) Transition in the interactions between physiologic systems across sleep stages. The time delay between two pairs of signals, (top)  $\alpha$ -brain waves and chin muscle tone, and (bottom) HR and eye movement, quantifies their physiologic interaction: highly irregular behavior (blue dots) during deep sleep is followed by a period of time delay stability during light sleep indicating a stable physiologic interaction (red dots for the HR-eye and orange dots for the  $\alpha$ -chin interaction). (c) Transitions between physiologic states are associated with changes in network topology: snapshots over 30-sec windows during a transition from deep sleep (dark gray) to light sleep (light gray). During deep sleep the network consists mainly of brain-brain links. With transition to light sleep links between other physiologic systems (network nodes) emerge and the network becomes highly connected. The stable  $\alpha$ -chin and HR-eye interactions during light sleep in (b) are shown by an orange and a red network link respectively. (d) Physiologic network connectivity for one subject during night sleep calculated in 30-sec windows as the fraction (%) of present links out of all possible links. (brain-brain links not included, see Fig. 3e). Red line marks sleep stages as scored in a sleep lab. Low connectivity is consistently observed during deep sleep (0:30–1:15h and 1:50–2:20h) and REM sleep (1:30–1:45h and 2:50–3:10h), while transitions to light sleep and wake are associated with a significant increase in connectivity.

#### RESULTS

# Time delay stability and network of physiologic interactions

The framework we propose is based on a complex networks approach to quantify physiologic interactions between diverse physiologic systems, where network nodes represent different physiologic systems and network links indicate the dynamical interaction (coupling) between systems. This framework allows to quantify the topology and the associated dynamics in the links strength of physiologic networks during a given physiologic state, taking into account the signal output of individual physiologic systems as well as the interactions among them, and to track the evolution of multiple interconnected systems undergoing transitions from one physiologic state to another (Fig. 1). We introduce the concept of time delay stability (TDS) to identify and quantify dynamic links among physiologic systems. We study the network of interactions for an ensemble of key integrated physiologic systems (cerebral, cardiac, respiratory, ocular and muscle activity). We consider different sleep stages (deep, light, rapid eye movement (REM) sleep and quiet wake) as examples of physiologic states. While earlier studies have identified how sleep regulation influences aspects of the specific control mechanism of individual physiologic systems (e.g., cardiac or respiratory [3, 4, 25, 26]) or have

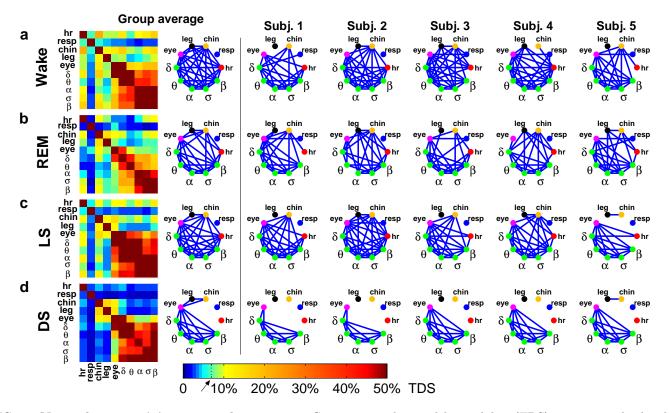


FIG. 2. Network connectivity across sleep stages. Group-averaged time delay stability (TDS) matrices and related networks of physiological interactions during different sleep stages: (a) wake; (b) REM sleep; (c) light sleep (LS); (d) deep sleep (DS). Matrix elements are obtained by quantifying the TDS for each pair of physiologic systems after obtaining the weighted average of all subjects in the group: % TDS =  $(\sum_i s_i/\sum_i L_i) \times 100$  where  $L_i$  indicates the total duration of a given sleep stage for subject *i*, and  $s_i$  is the total duration of time delay stability within  $L_i$  for the considered pair of physiologic signals. Color code represents the average strength of interaction between systems quantified as the fraction of time (out of the total duration of a given sleep-stage throughout the night) when TDS is observed. A network link between two systems is defined when their interaction is characterized by a TDS of  $\geq 7\%$  (arrow), a threshold determined by surrogate analysis (see Methods). The physiologic network exhibits transitions across sleep stages — lowest number of links during deep sleep (d), higher during REM (b) and highest during light sleep (c) and quiet wake (a) — a behavior observed in the group-averaged network as well as for each subject. Network topology also changes with sleep-stage transitions: from predominantly brain-brain links during light sleep to a high number of brain-periphery and periphery-periphery links during light sleep and wake.

focused on the organization of functional connectivity of EEG networks during sleep [27] and under neurological disorders such as epilepsy [28], the dynamics and topology of a physiologic network comprised of diverse systems have not been studied so far. Further, the relation between network topology and function, and how it changes with transitions across distinct physiologic states is not known. We demonstrate that sleep stages are associated with markedly different networks of physiologic interactions (Fig. 2) characterized by different number and strength of links (Figs. 3 and 4), by different rank distributions (Fig. 5), and by specific node connectivity (Fig. 6). Traditionally, differences between sleep stages are attributed to modulation in the sympatho-vagal balance with dominant sympathetic tone during wake and REM [25]: spectral, scale-invariant and nonlinear characteristics of the dynamics of individual physiologic systems indicate higher degree of temporal correlations and nonlinearity during wake and REM compared to non-REM (light and deep sleep) where physiologic dynamics exhibit weaker correlations and loss of nonlinearity [3, 26]. In contrast, the network of physiologic interactions shows a completely different picture: the network characteristics during light sleep are much closer to those during wake and very different from deep sleep (Figs. 2 and 3). Specifically, we find that network connectivity and overall strength of physiologic interactions are significantly higher during wake and light sleep, intermediate during REM and much lower during deep sleep. Thus, our empirical observations indicate that while sleep-stage related modulation in sympatho-vagal balance plays a key role in regulating individual physiologic systems, it does not account for the physiologic network topology and dynamics across sleep stages, showing that the proposed framework captures principally new information.

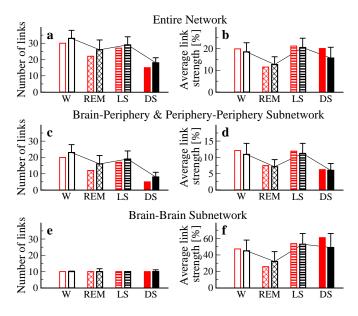


FIG. 3. Sleep-stage stratification pattern in network connectivity and network link strength. Groupaveraged number of links (a) and averaged link strength (b) are significantly higher during wake and light sleep compared to REM and deep sleep (student t-test  $p < 10^{-3}$  for both quantities when comparing REM and deep sleep with wake and light sleep). There is no significant difference between wake and light sleep  $(p > 5 \times 10^{-2})$ . This pattern is even more pronounced for the subnetwork formed by the brainperiphery and periphery-periphery links shown in (c) and (d)  $(p < 10^{-6}$  for both quantities when comparing REM and deep sleep with wake and light sleep). In contrast, the number of brain-brain links remains practically unchanged with sleepstage transitions (e), and the average brain-brain link is  $\approx 5$ times stronger in all sleep stages compared to the other network links (f). The group-averaged patterns in the number of network links and in the average link strength across sleep stages (black bars) are consistent with the behavior observed for individual subjects (red bars in all panels represent the same subject). The group-averaged number of links for each sleep stage is obtained from the corresponding group-averaged network in Fig. 2. The average link strength is measured in % TDS and is obtained by taking the mean of all elements in the TDS matrix for each sleep stage (Fig. 2); it represents the average strength of all links in a network obtained from a given subject during a specific sleep stage which then is averaged over all subjects. Error bars indicate standard deviation obtained from a group of 36 subjects (Methods).

To quantify the interaction between physiologic systems and to probe how this interaction changes in time under different physiologic conditions we study the time delay with which modulations in the output dynamics of a given physiologic system are consistently followed by corresponding modulations in the signal output of another system. Periods of time with approximately constant time delay indicate a stable physiologic interaction, and stronger coupling between physiologic systems results in longer periods of time delay stability (TDS). Utilizing the TDS method we build a dynamical network of physiologic interactions, where network links between physiological systems (considered as network nodes) are established when the time delay stability representing the coupling of these systems exceeds a significance threshold level, and where the strength of the links is proportional to the percentage of time for which time delay stability is observed (Methods).

# Transitions in network topology with physiologic function

We apply this new approach to a group of healthy young subjects (Methods). We find that the network of interactions between physiologic systems is very sensitive to sleep-stage transitions. In a short time window of just a few minutes the network topology can dramatically change — from only a few links to a multitude of links (Fig. 1) — indicating transitions in the global interconnectivity between physiological systems. These network transitions are not associated with random occurrence or loss of links but are characterized by certain organization in network topology where given links between physiological systems remain stable during the transition while others do not — e.g., brain-brain links persist during the transition from deep sleep to light sleep while brain-periphery links significantly change (Fig. 1c). Further, we find that sleep-stage transitions are paralleled by abrupt jumps in the total number of links leading to higher or lower network connectivity (Fig. 1c, d). These network dynamics are observed for each subject in the database, where consecutive episodes of sleep stages are paralleled by a level of connectivity specific for each sleep stage, and where sleep-stage transitions are consistently followed by transitions in network connectivity throughout the course of the night (Fig. 1d). Indeed, the network of physiologic interactions exhibits a remarkable responsiveness as network connectivity changes even for short sleep-stage episodes (arrows in Fig. 1d), demonstrating a robust relation between network topology and function. This is the first observation of a real network evolving in time and undergoing topological transitions from one state to another.

To identify the characteristic network topology for each sleep stage we obtain group-averaged time delay stability matrices, where each matrix element represents the percentage of time with stable time delay between two physiological systems, estimated over all episodes of a given sleep stage throughout the night. Matrix elements above a threshold of statistical significance (Fig. 7, Methods) indicate stable interactions between physiologic systems represented by network links (Fig. 2). We find that matrix elements greatly vary for different sleep stages with much higher values for wake and light sleep, lower values for REM and lowest for deep sleep.

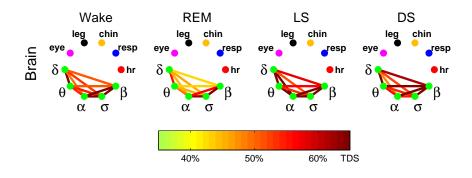


FIG. 4. Network connectivity and link strength of the brain-brain subnetwork for different sleep stages. While the topology of the brain subnetwork does not change, the strength of network links significantly changes with strongest links during light sleep and deep sleep (brown and dark red color), intermediate during wake (red and orange color) and weakest links during REM sleep (yellow color).

This is reflected in higher network connectivity for wake and light sleep, lower for REM and significantly reduced number of links during deep sleep (Fig. 3a). Further, the TDS matrices indicate separate subgroups of interactions between physiologic systems — brain-periphery, periphery-periphery and brain-brain interactions — that are affected differently during sleep stages and form different sub-networks. Specifically, matrix elements representing interactions between peripheral systems (cardiac, respiratory, chin, eye, leg) and the brain as well as interactions among the peripheral systems are very sensitive to sleep-stage transitions, leading to different network topology for different sleep stages (Fig. 2). We find sub-networks with high number of brain-periphery and periphery-periphery links during wake and light sleep, lower number of links during REM and a significant reduction of links at deep sleep (Fig. 3c). In contrast, matrix elements representing brain-brain interactions form a subnetwork with the same number of brain-brain links (Fig. 3e), and stable topology consistently present in the physiologic network during all sleep stages (Fig. 2). Sleep-stage related transitions in network connectivity and topology are not only present in the group-averaged data but also in the physiologic networks of individual subjects, suggesting universal behavior (Fig. 2). Notably, we find a higher number of brain-periphery links during REM compared to deep sleep despite inhibition of motoneurons in the brain leading to muscle atonia during REM [29]. The empirical observations of significant difference in network connectivity and topology during light sleep compared to deep sleep are surprising, given the similarity in spectral, scale-invariant and nonlinear properties of physiologic dynamics during light sleep and deep sleep [3, 4, 25, 26] (both stages traditionally classified as non-rapid eye movement sleep (NREM)), and indicate that previously unrecognized aspects of sleep regulation

may be involved in the control of physiologic network interactions.

# Physiologic states and network link strength stratification

Networks with identical connectivity and topology can exhibit different strength of their links. Network link strength is determined as the fraction of time when TDS is observed (Methods). We find that the average strength of network links changes with sleep-stage transitions: network links are significantly stronger during wake and light sleep compared to REM and deep sleep — a pattern similar to the behavior of the network connectivity across sleep stages (Fig. 3a, b). Further, subnetworks of physiologic interactions exhibit different relationship between connectivity and average link strength. Specifically, the subnetwork of brain-periphery and peripheryperiphery interactions is characterized by significantly stronger links (and also higher connectivity) during wake and light sleep, and much weaker links (with lower network connectivity) during deep sleep and REM (Fig. 3c, d). In contrast, the subnetwork of brain-brain interactions exhibits very different patterns for the connectivity and the average link strength — while the group average subnetwork connectivity remains constant across sleep stages, the average link strength varies with highest values during light sleep and deep sleep, and a dramatic  $\approx 40\%$  decline during REM. The observation of significantly stronger links in the brain-brain subnetwork during NREM compared to REM sleep is consistent with the characteristic of NREM as EEG-synchronized sleep and REM as EEG-desynchronized sleep [29]. During NREM sleep adjacent cortical neurons fire synchronously with a relatively low frequency rhythm [30] leading to coher-

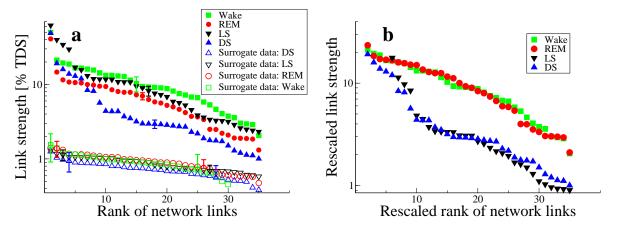


FIG. 5. Rank distributions of the strength of network links. Group-averaged strength of individual physiologic network links for different sleep stages. Rank 1 corresponds to the strongest link in the network, i.e., highest degree of time delay stability (TDS) (shown are all periphery-periphery and brain-periphery links). (a) The rank distributions for different sleep stages are characterized by different strength of the network links measured in % TDS — consistently lower values for most links during deep sleep, higher values during REM and highest during light sleep and wake, indicating that the stratification pattern in Fig. 3d is present not only for the average link strength (when averaging over different types of links in the network) but also for the strength of individual links. Indeed, links from all ranks are consistently stronger in light sleep compared to deep sleep and REM: such rank-by-rank comparison of links across sleep stages is possible because the rank order of the links does not change significantly from one sleep stage to another (Wilcoxon signed-rank test for all pairs of rank distributions yields  $0.77 \le p \le 0.93$ ). A surrogate test based on TDS analysis of signals paired from different subjects, which eliminates endogenous physiologic coupling, leads to significantly reduced link strength ( $p < 10^{-3}$ ) and close to uniform rank distributions with no difference between sleep stages (open symbols), indicating that the TDS method uncovers physiologically-relevant information. Error bars for the original and surrogate data indicate the standard error for a specific link when averaged over all 36 subjects or over 36 surrogate pairs respectively. (b) Rescaling the plots reveals two distinct forms of rank distributions: a slow decaying distribution for wake and REM, and a fast decaying distribution for light sleep and deep sleep with a pronounced plateau in the middle rank range corresponding to a cluster of links with similar strength, most of which related to the cardiac system.

ence between frequency bands in the EEG signal, and thus to stable time delays and strong network links (Fig. 3f). In contrast, during REM sleep cortical neurons are highly active but fire asynchronously [30], resulting in weaker links (Fig. 3f). Our findings of stronger links in the brain-brain subnetwork during non-REM sleep (Fig. 3f and Fig. 4) indicate that bursts (periods of sudden temporal increase) in the spectral power of one EEGfrequency band are consistently synchronized in time with bursts in a different EEG-frequency band, thus leading to longer periods of time delay stability and correspondingly stronger network links. This can explain some seemingly surprising network links — for example, we find a strong link between  $\alpha$  and  $\delta$  brain activity during non-REM sleep (Fig. 2) although  $\alpha$  waves are greatly diminished and  $\delta$  waves are dominant [29]. Since the spectral densities of both waves are normalized before the TDS analysis (Methods), the presence of a stable  $\alpha$ -  $\delta$  link indicates that a relative increase in the spectral density in one wave is followed, with a stable time delay, by a corresponding increase in the density of the other wave — an intriguing physiologic interaction which persists not only during deep sleep but is also present in light sleep, REM and quiet wake (Fig. 2). Notably, the average link strength of the brain-brain subnetwork is by a factor of  $\approx 5$  higher compared to all other links in the

physiologic network (Fig. 3d, f).

The finding of completely different sleep-stage stratification patterns in key network properties of the brain-brain subnetwork compared to the peripheryperiphery/brain-periphery subnetworks suggests a very different role these sub-networks play in coordinating physiologic interactions during sleep. The similarity in the brain-brain subnetwork during deep sleep and light sleep indicates that the proposed TDS approach is sensitive to quantify synchronous slow-wave brain activity during NREM sleep that leads to stronger brainbrain links during light sleep and deep sleep ( $\approx 50-60\%$ TDS) compared to REM ( $\approx 35\%$  TDS), as shown in (Fig. 3f and Fig. 4). The significant difference between light sleep and deep sleep observed for the peripheryperiphery/brain-periphery subnetwork in the number of links (t-test:  $p < 10^{-12}$ ) as well as in the average link strength (t-test:  $p < 10^{-11}$ ), indicates that the interactions between physiologic dynamics outside the brain are very different during these sleep stages.

Our finding that the average link strength exhibits a specific stratification pattern across sleep stages (Fig. 3) raises the question whether the underlying distribution of the network links strength is also sleep-stage dependent. To this end we probe the relative strength of individual links, and we obtain the rank distribution of the

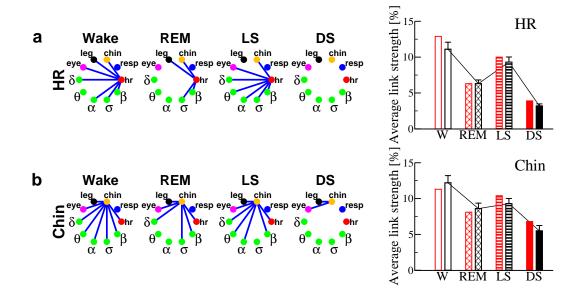


FIG. 6. Transitions in connectivity and link strength of individual network nodes across sleep stages. The number of links to specific network nodes significantly changes, with practically no links during deep sleep, a few links during REM and much higher connectivity during light sleep and wake. Notably, the average strength of the links connecting a given network node is also lowest during deep sleep and highest during light sleep and wake. Shown are connectivity and average link strength for two network nodes: (a) heart and (b) chin. This sleep-stage stratification pattern in individual node connectivity and in the average strength of the links connecting a specific network node is consistent with the transitions of the entire network across sleep stages shown in Fig. 3 c and d. Networks for (a) heart and (b) chin are obtained by averaging the corresponding networks for all subjects. During deep sleep no links to the heart are shown since the strength of each link averaged over all subjects is below the significance threshold (Fig. 2 and Fig. 7, Methods). Right bars in the panels represent for different sleep stages the group mean of the average strength of network links connecting heart and chin respectively, and error bars show the standard deviation. Left bars represent an individual subject. Note that the absence of a link between heart rate and respiration in the physiologic network does not indicate absence of cardio-respiratory coupling but rather that this coupling as represented by time delay stability (TDS) is rarely stable for periods longer than 2–4 min (where 2 min is the minimum window over which TDS is determined; Method section), and that cardio-respiratory TDS episodes form less than 7% of the recordings, which is the significance threshold level (Method section). Such "on" and "off" intermittent interaction between these two systems is observed also in other independent measures of cardio-respiratory coupling — respiratory sinus arrhythmia (RSA) [41, 42] and the degree of phase synchronization [6] — where relatively short "on" episodes are separated by periods of no interrelation as quantified by these measures.

strength of network links for each sleep stage averaged over all subjects in the group (Fig. 5a). We find that the rank distribution corresponding to deep sleep is vertically shifted to much lower values for the strength of the network links, while the rank distribution for light sleep and wake is for all links consistently higher than the distribution for REM. Thus, the sleep-stage stratification pattern we find for the average strength of the network links (Fig. 3d) originates from the systematic change in the strength of individual network links with sleep-stage transitions. Notably, while the strength of individual network links changes significantly with sleep stages, the rank order of the links does not significantly change. After rescaling the rank distributions for light sleep and REM (by horizontal and vertical shifts), we find that they collapse onto the rank plots of deep sleep and wake respectively, following two distinct functional forms: a slow and smoothly decaying rank distribution for REM and wake, and a much faster decaying rank distribution for deep sleep and light sleep with a characteristic plateau in the mid rank range indicating a cluster of links with similar strength (Fig. 5b). We note that, although the form of the rank distributions for deep sleep and light sleep as well as for wake and REM are respectively very similar, the average strength of the links is significantly different between deep sleep and light sleep and between wake and REM (Fig. 3d).

# Local topology and connectivity of the physiologic network

Our observations that physiologic networks undergo dynamic transitions where key global properties significantly change with sleep-stage transitions, raise the question whether local topology and connectivity of individual network nodes also change during these transitions. Considering each physiologic system (network node) separately, we examine the number and strength of all links connecting the system with the rest of the network. Specifically, we find that the cardiac system is highly connected to other physiologic systems in the network during wake and light sleep (Fig. 6). In contrast, during deep sleep we do not find statistically significant time delay stability in the interactions of the cardiac system, which is reflected by absence of cardiac links (Fig. 6). Further, we find that the average strength of the links connected to the cardiac system also changes with sleep stages: stronger interactions (high % TDS) during wake and light sleep, and significantly weaker interactions below the significance threshold during deep sleep (Fig. 6). Such 'isolation' of the cardiac node from the rest of the network indicates a more autonomous cardiac function during deep sleep — also supported by earlier observations of breakdown of long-range correlations and close to random behavior in heartbeat intervals in this sleep stage [3]. Transition to light sleep, REM and wake, where the average link strength and connectivity of the cardiac system is significantly higher indicating increased interactions with the rest of the network, leads to correspondingly higher degree of correlations in cardiac dynamics [3]. Similarly, respiratory dynamics also exhibit high degree of correlations during REM and wake, lower during light sleep and close to random behavior during deep sleep [26]. Such transitions in the number and strength of links across sleep stages we also find for other network nodes (Fig. 6). Moreover, the sleep-stage stratification pattern in connectivity and average link strength for individual network nodes (Fig. 6) is consistent with the pattern we observe for the entire network (Fig. 3). Our findings of significant reduction in the number and strength of brain-periphery and periphery-periphery links in the corresponding sub-networks during deep sleep indicate that breakdown of cortical interactions, previously reported during deep sleep [31], may also extend to other physiologic systems under neural regulation. Indeed, the low connectivity in the physiologic network we find in deep sleep may explain why people awakened during deep sleep do not adjust immediately and often feel groggy and disoriented for a few minutes. This effect is not observed if subjects are awakened from light sleep [29] when we find the physiologic network to be highly connected (Fig. 2). Further, since risk of predation modifies sleep architecture [32–34] and since abrupt awakening from deep sleep is associated with increased sleep inertia, higher sensory threshold, and impaired sensory reaction and performance [35, 36] that may lead to increased vulnerability, the fact that deep sleep (lowest physiologic network connectivity) dominates at the beginning of the night and not close to dawn, when many large predators preferably hunt, may have been evolutionarily advantageous.

Introducing a framework based on the concept of TDS we identify a robust network of interactions between physiologic systems, which remains stable across subjects during a given physiologic state. Further, changes in the physiologic state lead to complex network transitions associated with a remarkably structured reorganization of network connectivity and topology that simultaneously occurs in the entire network as well as at the level of individual network nodes, while preserving the hierarchical order in the strength of individual network links. Such network transitions lead to the formation of sub-networks of physiologic interactions with different topology and dynamical characteristics. In the context of sleep stages, network transitions are characterized by a specific stratification pattern where network connectivity and link strength are significantly higher during light sleep compared to deep sleep and during wake compared to REM. This can not be explained by the dynamical characteristics of the output signals from individual physiologic systems which are similar during light sleep and deep sleep as well as during wake and REM. The dramatic change in network structure with transition from one physiologic state to another within a short time window indicates a high flexibility in the interaction between physiologic systems in response to change in physiologic regulation. Such change in network structure in response to change in the mechanisms of control during different physiologic states suggests that our findings reflect intrinsic features of physiologic interaction. The observed stability in network topology and rank order of links strength during sleep stages, and the transitions in network organization across sleep stages provide new insight into the role which individual physiologic systems as well as their interactions play during specific physiologic states. While our study is limited to a data-driven approach these empirical findings may facilitate future efforts on developing and testing network models of physiologic interaction. This system-wide integrative approach to individual systems and the network of their interactions may facilitate the emergence of a new dimension to the field of systems physiology [8] that will include not only interactions within but also across physiologic systems. In relation to critical clinical care, where multiple organ failure is often the reason for fatal outcome [24, 37], our framework may have practical utility in assessing whether dynamical links between physiologic systems remain substantially altered even when the function of specific systems is restored after treatment [38]. While we demonstrate one specific application, the framework we develop can be applied to a broad range of complex systems where the TDS method can serve as a tool to characterize and understand the dynamics and function of real-world heterogeneous and interdependent

networks. The established relation between dynamical network topology and network function has not only significant medical and clinical implications, but is also of relevance for the general theory of complex networks.

#### METHODS

#### Data

We analyze continuously recorded multi-channel physiologic data obtained from 36 healthy young subjects (18 female, 18 male, with ages between 20-40, average 29 years) during night-time sleep [39] (average record duration is 7.8 hours). This allows us to track the dynamics and evolution of the network of physiologic interactions during different sleep stages and sleep-stage transitions (Fig. 1). We focus on physiologic dynamics during sleep since sleep stages are well-defined physiological states, and external influences due to physical activity or sensory inputs are reduced during sleep. Sleep stages are scored in 30 sec epochs by sleep lab technicians based on standard criteria. In particular, we focus on the electroencephalogram (EEG), the electrocardiogram (ECG), respiration, the electrooculogram (EOG), and the electromyogram (EMG) of chin and leg. In order to compare these very different signals with each other and to study interrelations between them, we extract the following time series from the raw signals: the spectral power of five frequency bands of the EEG in moving windows of 2 sec with a 1 sec overlap:  $\delta$  waves (0.5-3.5 Hz),  $\theta$  waves (4-7.5 Hz),  $\alpha$  waves (8-11.5 Hz),  $\sigma$  waves (12-15.5 Hz),  $\beta$ waves (16-19.5 Hz); the variance of the EOG and EMG signals in moving windows of 2 sec with a 1 sec overlap; heartbeat RR-intervals and interbreath intervals are both re-sampled to 1 Hz (1 sec bins) after which values are inverted to obtain heart rate and respiratory rate. Thus, all time series have the same time resolution of 1 sec before the TDS-analysis is applied.

Utilizing sleep data as an example we demonstrate that a network approach to physiologic interactions is necessary to understand how modulations in the regulatory mechanism of individual systems translate into reorganization of physiologic interactions across the human organism.

### Time Delay Stability (TDS) Method

Integrated physiologic systems are coupled by feedback and/or feed forward loops with a broad range of time delays. To probe physiologic coupling we propose an approach based on the concept of time delay stability: in the presence of stable/strong interactions between two systems, transient modulations in the output signal of one system lead to corresponding changes that occur

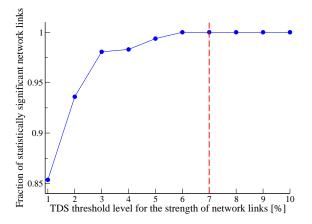


FIG. 7. Determining significance threshold for the strength of network links. With increasing the time delay stability (TDS) threshold level which allows only stronger links with higher TDS values to be considered in the physiologic network, the fraction of statistically significant network links that carry physiologically relevant information also increases, and at a significance threshold of  $\approx 7\%$  TDS (marked by a vertical dashed line) all network links (100%) are statistically significant. Periphery-periphery and brain-periphery links during all sleep stages are considered when determining this threshold. Statistical significance of a specific physiologic link is estimated by comparing the strength distribution of this link across all subjects in the group with a distribution of surrogate links representing "interactions" between the same systems paired from different subjects). Based on this surrogate test, a p-value  $< 10^{-3}$  obtained from the student ttest indicates statistically significant strength of a given link.

with a stable time lag in the output signal of another coupled system. Thus, long periods of constant time delay indicate strong physiologic coupling.

The TDS method we developed for this study consists of the following steps:

(1.) To probe the interaction between two physiologic systems X and Y, we consider their output signals  $\{x\}$ and  $\{y\}$  each of length N. We divide both signals  $\{x\}$ and  $\{y\}$  into  $N_L$  overlapping segments  $\nu$  of equal length L = 60 sec. We choose an overlap of L/2 = 30 sec which corresponds to the time resolution of the conventional sleep-stage scoring epochs, and thus  $N_L = [2N/L] - 1$ . Prior to the analysis, the signal in each segment  $\nu$  is normalized separately to zero mean and unit standard deviation, in order to remove constant trends in the data and to obtain dimensionless signals. This normalization procedure assures that the estimated coupling between the signals  $\{x\}$  and  $\{y\}$  is not affected by their relative amplitudes.

(2.) Next, we calculate the cross-correlation function,  $C_{xy}^{\nu}(\tau) = \frac{1}{L} \sum_{i=1}^{L} x_{i+(\nu-1)\frac{L}{2}}^{\nu} y_{i+(\nu-1)\frac{L}{2}+\tau}^{\nu}$ , within each segment  $\nu = 1, \ldots, N_L$  by applying periodic boundary conditions. For each segment  $\nu$  we define the time delay  $\tau_0^{\nu}$  to correspond to the maximum in the absolute value of the cross-correlation function  $C_{xy}^{\nu}(\tau)$  in this seg-

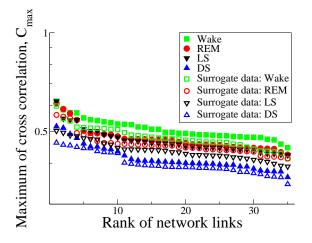


FIG. 8. Cross-correlation and surrogate analysis. Rank plots obtained from cross-correlation analysis show no statistically significant differences between real and surrogate data, indicating that cross-correlation is not a reliable measure to identify physiologic interactions.

ment  $\tau_0^{\nu} = \tau |_{|C_{xy}^{\nu}(\tau)| \ge |C_{xy}^{\nu}(\tau')|} \forall \tau'$ . Time periods of stable interrelation between two signals are represented by segments of approximately constant  $\tau_0$  (light shade region in Fig. 1b) in the newly defined series of time delays,  $\{\tau_0^{\nu}\}_{\nu=1,...,N_L}$ . In contrast, absence of stable coupling between the signals corresponds to large fluctuations in  $\tau_0$  (dark shade region in Fig. 1b).

(3.) We identify two systems as linked if their corresponding signals exhibit a time delay that does not change by more than  $\pm 1$  sec for several consecutive segments  $\nu$ . We track the values of  $\tau_0$  along the series  $\{\tau_0^{\nu}\}$ : when for at least four out of five consecutive segments  $\nu$  (corresponding to a window of  $5 \times 30$  sec) the time delay remains in the interval  $[\tau_0 - 1, \tau_0 + 1]$  these segments are labeled as stable. This procedure is repeated for a sliding window with a step size one along the entire series  $\{\tau_0^{\nu}\}$ . The % TDS is finally calculated as the fraction of stable points in the time series  $\{\tau_0^{\nu}\}$ .

Longer periods of TDS between the output signals of two systems reflect more stable interaction/coupling between these systems. Thus, the strength of the links in the physiologic network is determined by the percentage of time when TDS is observed: higher percentage of TDS corresponds to stronger links. To identify physiologically relevant interactions, represented as links in the physiologic network, we determine a significance threshold level for the TDS based on comparison with surrogate data: only interactions characterized by TDS values above the significance threshold are considered.

The TDS method is general, and can be applied to diverse systems. It is more reliable in identifying physiologic coupling compared to traditional cross-correlation and cross-coherence analyses (Fig. 8) which are not suitable for heterogeneous and nonstationary signals, and are affected by the degree of auto-correlations in these signals [40].

To compare interactions between physiologic systems which are very different in strength and vary with change of physiologic state (e.g., transitions across sleep stages), we define the significance threshold as the percent of TDS for which all links included in the physiologic network are statistically significant. To identify statistical significance of a given link between two physiologic systems, we compare the distribution of TDS values for this link obtained from all 36 subjects in our database with the distribution of TDS values obtained for 100 surrogates of this link where the signal outputs from the same two physiologic systems taken from different subjects are paired for the analysis in order to eliminate the endogenous physiologic coupling. A student t-test was performed to determine the statistical significance between the two distributions. This procedure is repeated for all pairs of systems (links) in the network, and network links are identified as significant when the t-test pvalue  $< 10^{-3}$ . The significance threshold level for TDS is then defined as the value above which all network links are statistically significant, and thus represent endogenous interactions between physiologic systems. We find that a threshold of approximately 7% TDS is needed to identify networks of statistically significant links for all sleep stages (Fig. 7).

#### Surrogate tests

To confirm that the TDS method captures physiologically relevant information about the endogenous interactions between systems, we perform a surrogate test where we pair physiologic signals from different subjects, thus eliminating physiologic coupling. Applying the TDS method to these surrogate data, we obtain almost uniform rank distributions with significantly decreased link strength (Fig. 5a) due to the absence of physiologic interactions. Further, all surrogate distributions conform to a single curve, indicating that the sleep-stage stratification we observe for the real data reflects indeed changes in physiologic coupling with sleep-stage transitions. In contrast, the same surrogate test applied to traditional cross-correlation analysis does not show a difference between the rank distributions from surrogate and real data (Fig. 8).

We find that the TDS method is better suited than the traditional cross-correlation analysis in identifying networks of endogenous physiologic interactions. Rank plots obtained from cross-correlation analysis (Fig. 8) show that the cross-correlation strength  $C_{max}$  (global maximum of the cross-correlation function) is consistently lower for all links during deep sleep, higher for light sleep and REM and highest during wake — a stratification related to the gradual increase in the strength of autocorrelations in the signal output of physiologic systems [3, 26],

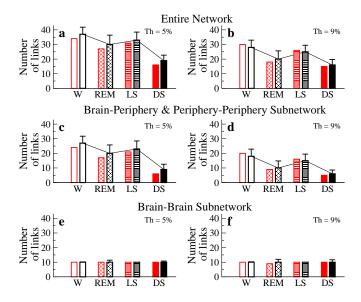


FIG. 9. Stability of sleep-stage stratification pattern in network connectivity. Group-averaged number of network links for two different thresholds (Th) during wake, REM, light and deep sleep. Results for threshold of Th = 5% time delay stability (TDS) are shown in a, c and e, and results for threshold of Th = 9% TDS are shown in b, d and f. The sleep-stage stratification pattern observed for the significance threshold of 7% TDS (shown in Fig. 3) is preserved also for thresholds of 5% and 9% TDS, indicating stability of the results. Note, that the number of links in the brain-brain subnetwork remains unchanged for different sleep stages (e, f), since the strength of all links in this subnetwork is well above 9% TDS (Fig. 3f).

which in turn increases the degree of cross-correlations [40]. Surrogate tests based on pairs of signals from different subjects, where the coupling between systems is abolished but physiologic autocorrelations are preserved, show no statistical difference between the surrogate (open symbols) and original (filled symbols) rank distributions of  $C_{max}$ , suggesting that in this context cross-correlations do not provide physiologically relevant information regarding the interaction between systems. Indeed, even for uncoupled systems high autocorrelations in the output signals lead to spurious detection of cross-correlations [40]. In contrast, the TDS method is not affected by the autocorrelations — surrogate rank plots for different sleep stages collapse and do not exhibit vertical stratification as shown in (Fig. 5a).

To test the robustness of the stratification pattern in network topology and connectivity across sleep stages (shown in Fig. 2 and Fig. 3), we repeat our analyses for two additional thresholds: 5% TDS and 9% TDS. With increasing the threshold for TDS from 5% to 9% the overall number of links in the network decreases (compare Fig. 9a,c,e with Fig. 9b,d,f). However, the general sleep-stage stratification pattern is preserved with highest number of links during light sleep and wake, lower during REM, and significant reduction in network connectivity during deep sleep (Fig. 9). The stability of the observed pattern in network connectivity for a relatively broad range around the significance threshold of 7% TDS indicates that the identified network is a robust measure of physiologic interactions.

### ACKNOWLEDGMENTS

We thank T. Penzel for providing data and helpful comments, and A. Y. Schumann for help with data selection, data pre-processing and discussions. We acknowledge support from NIH Grant 1R01-HL098437, the US-Israel Binational Science Foundation (BSF Grant 2008137), the Office of Naval Research (ONR Grant 000141010078), the Israel Science Foundation, the European Community (projects DAPHNet/FP6 IST 018474-2 and SOCIONICAL/FP7 ICT 231288) and the Brigham and Women's Hospital Biomedical Research Institute Fund. R.P.B. acknowledges support from the German Academic Exchange Service (DAAD fellowship within the Postdoc-Programme).

### AUTHOR CONTRIBUTIONS

A.B. and R.P.B. contributed equally to this work. A.B., R.P.B., J.W.K., S.H. and P.Ch.I. designed research. A.B. and R.P.B. wrote the algorithm. A.B., R.P.B. and P.Ch.I. analysed the data. R.P.B. and P.Ch.I. wrote the paper with contributions from all.

#### ADDITIONAL INFORMATION

Competing financial interests: The authors declare no competing financial interests.

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