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3 **Quantitative evaluation of liver function by use of gadoxetate disodium (Gd-EOB-**  
4 **DTPA)-enhanced MR Imaging.**  
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15 **Advance in Knowledge:**  
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17 The liver function corresponding to the plasma disappearance rate of indocyanine green  
18 (ICG-PDR) can be estimated quantitatively ( $R = 0.87$ ) from the signal intensities and the  
19 volumes of the liver and the spleen on gadoxetate disodium-enhanced MR images.  
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27 **Implications for Patient Care:**  
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30 1. Our study results suggest that (Gd-EOB-DTPA)-enhanced MR imaging of the liver may  
31 improve the early detection and treatment of liver diseases by evaluating anatomic and  
32 functional information on the liver by one examination.  
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35 2. Gadoxetate disodium-enhanced MR imaging of the liver may allow quantitative  
36 estimation of segmental liver function.  
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43 **Summary statement:**  
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45 The liver function corresponding with ICG-PDR can be estimated quantitatively from the  
46 signal intensities and the volumes of the liver and spleen on gadoxetate disodium-enhanced  
47 MR images, which may improve the estimation of segmental liver reserve.  
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**Abstract**

Purpose: The purpose of this study was to determine if liver function correlating with indocyanine green (ICG) clearance could be estimated quantitatively from gadoxetate disodium-enhanced MR images.

Materials and Methods: This retrospective study was approved by the Institutional Review Board and the requirement for informed consent was waived. Twenty-three consecutive patients who had ICG clearance test and gadoxetate disodium-enhanced MR imaging with the same parameters as a preoperative examination were chosen. The 'Hepatocellular uptake index' (HUI) was determined by the equation  $V_L(L_{20}/S_{20} - 1)$  from liver volume ( $V_L$ ) and the mean signal intensity of whole liver ( $L_{20}$ ) and whole spleen ( $S_{20}$ ) on 3D-GRE T1-weighted images with fat suppression obtained at 20 min after gadoxetate disodium (0.025mmol/kg body weight) administration. The correlation of the plasma disappearance rate of indocyanine green (ICG-PDR) and various factors derived from MR imaging including HUI, iron/fat deposition in the liver/spleen, and the volume of the spleen ( $V_S$ ) were evaluated by stepwise multiple regression analysis. The difference in future liver remnant ratio between HUI ( $rHUI/HUI$ ) and volumetry ( $rV_L/V_L$ ) was evaluated in 4 patients who had segmental heterogeneity of liver function.

Results: HUI and  $V_S$  were the factors significantly correlate with ICG-PDR ( $R = 0.87$ ). The mean value and its 95% confidence interval for  $rHUI/HUI - rV_L/V_L$  were 0.18 (0.01 – 0.34).

Conclusion: The liver function correlating with ICG-PDR can be estimated quantitatively from the signal intensities and the volumes of the liver and spleen on gadoxetate disodium-enhanced MR images, which may improve the estimation of segmental liver function.

## Introduction

Quantitative evaluation of liver function is important not only for monitoring of that function, but also for preoperative assessment of the liver reserve (1). The plasma disappearance rate of indocyanine green (ICG-PDR) has been regarded as a valuable tool for the quantitative assessment of liver function, because it is removed from the circulation exclusively by the liver (2). However, a reliable method for the quantitative anatomically based evaluation of liver function has not been established to date.

Gadoxetate disodium (Gd-EOB-DTPA; Primovist, Bayer Schering Pharma AG, Berlin) is a paramagnetic hepatobiliary contrast agent that can combine the features of extracellular agents with those of a hepatocellular contrast agent (3). The same transporting mechanisms, i.e., the organic anion transporter, are considered to be responsible for uptake of gadoxetate disodium and ICG in hepatocytes (4, 5); therefore, there is a possibility that gadoxetate disodium-enhanced MR imaging could be the basis of a useful method for quantitative evaluation of liver function similar to IGC clearance but with anatomic delineation of hepatic function, (6-11).

The purpose of this study was to determine if liver function corresponding to indocyanine green (ICG) clearance could be estimated quantitatively from gadoxetate disodium-enhanced MR images

## Materials and Methods

### Subjects

This retrospective study was approved by the Institutional Review Board of the Shinshu University and the University of Chicago, and the requirement for informed-consent was waived.

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3           There were 59 consecutive patients (mean age  $\pm$  SD = 69.9  $\pm$  9.0, M:F ratio = 49:10)  
4 who had 3D-GRE T1-weighted gadoxetate disodium-enhanced MR imaging and an ICG  
5  
6 clearance test as a preoperative evaluation within 4 weeks from June 2008 to December 2009  
7  
8 in the record at the Shinshu University Hospital. However, we selected only 23 patients for  
9  
10 this study, as described below. Five patients (mean age, range = 73.6, 57-87, M:F ratio = 4:1)  
11  
12 were excluded because pre-contrast MR imaging was not performed. Twenty-one patients  
13  
14 (mean age, range = 68.9, 49-80, M:F ratio = 19:2) were excluded because the MR imaging  
15  
16 parameters were different between pre and post-contrast enhanced MR imaging. Finally, 23  
17  
18 patients (mean age, range = 70.0, 41-84, M:F ratio = 17:6) were selected for the evaluation  
19  
20 because they were the largest population in this study subjects whose MR imaging  
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22 parameters (repetition time, TR / echo time, TE / flip angle, FA) were the same in pre and  
23  
24 post-contrast enhanced 3D-GRE MR imaging There was no significant difference of the age  
25  
26 and sex distribution between included and excluded patients. There were 6 patients without  
27  
28 chronic hepatitis or liver cirrhosis, 6 patients with chronic hepatitis, and 11 patients with liver  
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30 cirrhosis in this study group. No patient with renal dysfunction (serum creatinine > 2.0  
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32 mg/dL) was included in this study.  
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#### 43 MR imaging

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45 Imaging of the entire liver and spleen was performed prior to and 20 minutes after  
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47 intravenous administration of 0.025 mmol/kg of gadoxetate disodium by single-breath-hold  
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49 3D-GRE or with fat suppression (TR/TE/FA = 3.5 msec/1.42 msec/15 degree) on a MRI  
50  
51 system (Trio Tim, Siemens, Germany) with 8 channels phased-array body coil and a parallel-  
52  
53 imaging technique (the acceleration factor 2). Pre-contrast 2D-GRE T2\*-weighted images  
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55 (191-280 msec / 10 msec / 20 degree), pre-contrast 2D-dual-GRE T1-weighted images (106-  
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57 165 msec / 1.23 and 2.46 msec / 80 degree) were also obtained to evaluate iron and fat  
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3 deposition in the liver and the spleen. The TEs in dual-GRE sequence were determined  
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5 according to actual magnetic field strength of the MRI system (2.8 T).  
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### 10 Image analysis

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12 Two radiologists (D.K. and M.M. who had 4 years and 3 years experience in diagnostic  
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14 imaging, respectively. They were not included in authors.) independently drew the outlines of  
15  
16 the liver and spleen on every slice of all MR images listed above in MR imaging section. In  
17  
18 this procedure, MR images were presented on DICOM viewer (Osirix, Pixmeo, Geneva,  
19  
20 Switzerland) and the outlines were drawn by free-hand contours (see Fig.1). The post contrast  
21  
22 enhanced-3D-GRE images were always presented at first in order that observers can identify  
23  
24 the liver parenchyma. The time limit for drawing outlines was not specified. In each patient,  
25  
26 the volume of the liver and the spleen ( $V_L$  and  $V_S$ ) on post contrast enhanced images and the  
27  
28 mean signal intensity of the liver and the spleen at pre-contrast on T1-weighted images with  
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30 fat suppression ( $L_0$  and  $S_0$ ), the mean signal intensity of the liver and the spleen at pre-  
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32 contrast on in-phase T1-weighted images ( $L_{in}$  and  $S_{in}$ ), the mean signal intensity of the liver  
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34 and the spleen at pre-contrast on out-of-phase T1-weighted images ( $L_{out}$  and  $S_{out}$ ), the mean  
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36 signal intensity of the liver and the spleen at pre-contrast on T2\*-weighted images ( $L_{T2^*}$  and  
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38  $S_{T2^*}$ ) and the mean signal intensity of the liver and the spleen at pre-contrast at post-contrast  
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40 on T1-weighted images with fat suppression ( $L_{20}$  and  $S_{20}$ ) were obtained within the volume  
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42 included in the outlines. The average values for all parameters ( $V_L$ ,  $V_S$ ,  $L_0$ ,  $S_0$ ,  $L_{in}$ ,  $S_{in}$ ,  $L_{out}$ ,  
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44  $S_{out}$ ,  $L_{T2^*}$ ,  $S_{T2^*}$ ,  $L_{20}$  and  $S_{20}$ ) measured by the two radiologists were used for quantitative  
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46 evaluation.  
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### ICG clearance test

A dose of 0.5 mg/kg ICG was administered intravenously, and blood was withdrawn at 5, 10, and 15 min intervals following ICG administration. ICG-PDR was determined by regression analysis (12). ICG-PDR higher than 0.15 can be considered as normal liver function.

### Feature values derived from gadoxetate disodium-enhanced MR images

We introduced the feature value  $V_L(L_{20}/S_{20} - 1)$  which may be called the 'Hepatocellular Uptake Index' (HUI) as an index for the amount of gadoxetate disodium uptake into hepatocytes measured on gadoxetate disodium-enhanced MR imaging.

The feature value  $L_0/S_0$ ,  $L_{T2^*}/S_{T2^*}$ ,  $L_{out}/L_{in}$ ,  $S_{out}/S_{in}$ , and  $V_S$  were evaluated to see the degree of the signal intensity difference between the liver and the spleen, the degree of the iron deposition difference between the liver and the spleen (13), the degree of fat deposition in the liver (14), the degree of fat deposition in the spleen (14), and the degree of splenomegaly due to portal hypertension, respectively.

### The estimation of the segmental liver function in the patients with segmental heterogeneity of liver function

Conventionally, segmental liver function has been estimated by ICG clearance test and the volumetry (1). In this method, the segmental liver function could be estimated by the future liver remnant volume ratio ( $rV_L/V_L$ ) multiplied by ICG-PDR based on the assumption that the liver function could be homogeneous; therefore, the ratio of the segmental liver function against to total liver function estimated by volumetry could be determined by  $rV_L/V_L$ . On the other hand, the segmental liver function could be estimated by the equation  $rV_L(rL_{20}/S_{20} - 1)$  which may be called the 'Remnant Hepatocellular Uptake Index' (rHUI) as an index for the amount of gadoxetate disodium uptake into hepatocytes in remnant liver volume measured on

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3 gadoxetate disodium-enhanced MR imaging taking into account of the heterogeneity of the  
4 liver function. Where  $rV_L$  is a remnant liver volume,  $rL_{20}$  and  $S_{20}$  are the signal intensity in  
5 the remnant liver and whole spleen. The future liver remnant function ratio could be  
6 described as  $rHUI/HUI$  by use of gadxetate disodium-enhanced MR imaging. We evaluated  
7  $rV_L/V_L$  and  $rHUI/HUI$  in the patients with segmental heterogeneity of liver function due to  
8 known liver dysfunction such as portal vein embolization or obstructive jaundice affecting  
9 more than one liver subsegment. In this segmental analysis, two radiologists (D.K. and M.M.)  
10 drew the outlines of the non-affected liver on gadxetate disodium-enhanced MR imaging to  
11 obtain  $rV_L$  and  $rL_{20}$ . (see Fig. 2). The difference of two methods ( $rHUI/HUI - rV_L/V_L$ ) was  
12 evaluated.  
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### 29 Statistical analysis

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31 The mean value and its 95% confidence interval (CI) for the correlation coefficient between  
32 ICG-PDR and feature values ( $L_{20}$  and HUI) were determined by a bootstrap method with  
33 2,000 bootstrap samples. The bootstrap sample size was determined according to the  
34 recommendation that the bootstrap sample size should be 1,000 or more to estimate CI (15).  
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41 The step wise multiple linear regression analysis of various feature values including  
42 HUI,  $L_0/S_0$ ,  $L_{T2^*}/S_{T2^*}$ ,  $L_{out}/L_{in}$ ,  $S_{out}/S_{in}$ , and  $V_S$  on ICG-PDR was done to evaluate the  
43 statistical significance of the various influences, such as iron and fat deposition and  
44 splnomegaly, in the correlation between HUI and ICG-PDR. The entrance and exit tolerances  
45 for p-values of F-statistics were specified to 0.05 and 0.10, respectively.  
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53 The mean value and its 95% CI for  $rHUI/HUI - rV_L/V_L$  were evaluated to determine  
54 the statistical significance of the difference between HUI and volumetry in the estimation of  
55 segmental liver function.  
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3 All statistical analyses were carried out by use of MATLAB Version 7.11, R20010b  
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5 (The MathWorks, Inc. Natick, MA, USA). No overlapping in 95% CI or p-value less than  
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7 0.05 were regarded to indicate significance.  
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## 10 11 12 **Results**

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15 The liver characteristics of all patients obtained in this study are shown in Table 1.

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17 The mean value and its 95% CI for correlation coefficients between ICG-PDR and  
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19 feature values ( $L_{20}$  and HUI) were 0.634 (95% CI, 0.629 – 0.640) for  $L_{20}$  and 0.721 (95% CI,  
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21 0.717 – 0.726) for HUI (see Fig. 1, 3, 4).  
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25 The stepwise multiple linear regression analysis revealed that HUI and  $V_S$  were the  
26  
27 factor significantly correlated with ICG-PDR in our study (Table 2). The regression  
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29 coefficients and the R statistic for a multiple linear regression of HUI and  $V_S$  on ICG-PDR  
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31 ( $\text{ICG-PDR} = B_0 + B_1\text{HUI} + B_2V_S + e$ ) were  $B_0 = 0.10$  (95%CI, 0.07 – 0.13),  $B_1 = 0.12$  (0.08  
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33 – 0.15),  $B_2 = -0.23$  (-0.34 – -0.11), and  $R = 0.87$  (see Fig. 5).  
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37 The segmental heterogeneity of liver function affecting more than one liver segment  
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39 was observed in 4 patients in our study. The liver characteristics of the patients are shown in  
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41 Table 3. The mean value and its 95% CI for  $r\text{HUI}/\text{HUI} - rV_L/V_L$  were 0.18 (0.01 – 0.34).  
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## 45 46 **Discussion**

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48 The feature value  $V_L(L_{20}/S_{20} - 1)$  which may be called the ‘Hepatocellular Uptake Index’  
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50 (HUI) showed good correlation with ICG-PDR and the correlation was significantly higher  
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52 than  $L_{20}$ . This result can be explained by two correction factors additional to the signal  
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54 intensity of the liver on gadxetate disodium-enhanced MR imaging. One is the extracellular  
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56 fluid (ECF) contrast enhancement effect of gadoxetate disodium in the liver approximated by  
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3 the signal intensity of the spleen ( $S_{20}$ ) and the other is the inter-individual variation in the  
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5 liver volume ( $V_L$ ).  
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8 The local concentration of ICG and gadoxetate disodium taken up by hepatocytes  
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10 decreases during the development of cirrhosis because of the decrease in hepatocytes and the  
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12 increase in fibrous tissue (16). In addition,, the fibrosis of the liver results in a decrease in the  
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14 incoming blood flow, and restriction of molecular movement within the extravascular space  
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16 (17), which could be another possible cause of decreased uptake of ICG and gadoxetate  
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18 disodium by hepatocytes. Although the cause of weak contrast enhancement of gadoxetate  
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20 disodium in cirrhosis has not been fully clarified, the correlation between contrast  
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22 enhancement of gadoxetate disodium and the degree of fibrosis has been observed in an  
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24 animal model (18).  
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29 Gadoxetate disodium equilibrates rapidly between the intravascular and extravascular  
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31 spaces according to the concentration gradient, following intravenous administration.  
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33 Therefore the contrast enhancement effect of the gadxetate disodium is due not to uptake only  
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35 in the hepatocytes but also it's presence in the ECF space (the sum of the intravascular and  
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37 extravascular spaces) must be taken into account in the signal intensity of the liver on  
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39 gadxetate disodium-enhanced MR imaging ( $L_{20}$ ). After the gadxetate disodium reaches  
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41 equilibrium state in ECF space (about two minutes after venous administration), the  
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43 concentrations of gadoxetate disodium distributing in ECF spaces of the liver and the other  
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45 organs fall in parallel as a result of renal and hepatic excretion. This phenomenon has been  
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47 observed on MR imaging with use of gadoxetate disodium in extrahepatic organs such as the  
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49 spleen (19). The distribution volume of gadoxetate disodium in the ECF correlates closely  
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51 with the ECF volume after the equilibrium is reached, and the ECF volume is similar between  
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53 the liver and spleen in normal liver and spleen (20). Therefore, the parameter  $L_{20}/S_{20} - 1$   
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3 could serve as an index for the hepatocellular contrast enhancement effect corrected by the  
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5 ECF contrast enhancement effect approximated by the signal intensity of the spleen.  
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8 The relation between the distribution volume and the degree of the liver fibrosis is  
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10 controversial (21, 22). Van Beers et al reported that distribution volume of the liver would  
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12 not be affected by the degree of liver fibrosis (21). In contrast, Hagiwara et al demonstrated  
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14 significant increase in distribution volume between normal liver and liver fibrosis, however,  
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16 the increase of distribution volume due to liver fibrosis comparing to normal liver has been  
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18 reported as 10% (22). On the other hand, the relaxivity of gadoxetate disodium in ECF space  
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20 (8.7 L/mmol) is about half comparing to that in hepatocytes (16.6 L/mmol), related to  
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22 differences in micro viscosity (23). Therefore, the influence of various distribution volume in  
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24 the liver according to liver fibrosis could be less than 10% and negligible in the signal  
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26 intensity of the liver at 20 min after gadoxetate disodium administration ( $L_{20}$ ).  
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31 On the other hand, our result showed that the volume of the spleen ( $V_S$ ) could be a  
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33 significant factor affecting the correlation between HUI and ICG-PDR. This can be explained  
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35 by the effect of splenomegaly due to portal hypertension in splenic ECF volume. There have  
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37 been several reports showing the hyperplasia of the red pulp and decrease of the vascular  
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39 space density in the spleen during the development of splenomegaly due to portal  
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41 hypertension (24). The increase of splenic hematocrit due to congestion may decrease the  
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43 ECF space density in the spleen as has been suggested in the animal model with portal  
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45 hypertension (25). Therefore, the decrease of ECF space density correlating with  
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47 splenomegaly (increase in  $V_S$ ) may lead the weak contrast enhancement of the spleen after  
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49 the equilibrium point (decrease in  $S_{20}$ ) and resulting in increase of HUI [ $V_L(L_{20}/S_{20} - 1)$ ] on  
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51 gadxetate disodium-enhanced MR imaging, however, this hypothesis must be confirmed by  
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53 further investigation. In the future, more accurate index derived from HUI to estimate liver  
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3 function taking into account the volume of the spleen could be possible by use of gadxetate  
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5 disodium-enhanced MR imaging.  
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8         If the parameter ( $L_{20}/S_{20} - 1$ ) was analogous to the concentration of gadoxetate  
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10 disodium taken up by hepatocytes, the total amount of gadoxetate disodium taken up by  
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12 hepatocytes which can correlate with ICG-PDR would be found by the volume integration of  
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14  $L_{20}/S_{20} - 1$ . The similar idea has been proposed in the relation with histological evaluation of  
15  
16 liver fibrosis. It was shown by Hashimoto et al. (26) that ICG-PDR was proportional to the  
17  
18 total hepatic parenchymal cell volume, determined as the histologic parenchymal cell volume  
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20 ratio multiplied by the liver volume obtained from computed tomography. The liver volume  
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22 differs depending on not only the severity of chronic liver disease, but also on the physical  
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24 constitution (27), and the total hepatic parenchymal cell volume differs individually. Thus, a  
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26 correction for liver volume is necessary for estimation of ICG-PDR from the hepatobiliary  
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28 contrast enhancement of gadoxetate disodium in the liver.  
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34         The signal intensity of the liver and the spleen in gadxetate disodium-enhanced MR  
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36 imaging can be affected by various factors including liver function but also the difference of  
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38 tissue specific relaxation time and the iron/fat deposition. However, our multiple regression  
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40 analysis revealed that these effects were not significant in the correlation between HUI and  
41  
42 ICG-PDR. This could be explained by the use of very short TE 3D-GRE sequence in the  
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44 measurement of HUI in this study. The shorter TE is, the less T2\*-weighted and the more T1-  
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46 weighted image could be obtained. Thus, correlation of the contrast enhancement effect in the  
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48 liver to liver function is much greater than to other factors affecting the signal intensity of the  
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50 liver and the spleen in gadxetate disodium-enhanced MR imaging.  
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55         The uptake of ICG and gadoxetate disodium into hepatocytes reflects not only the  
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57 hepatic cell function but also the hepatic blood flow (28); therefore the ICG-PDR and HUI  
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59 might show discrepancy from the galactosyl-human serum albumin (GSA) scintigraphy  
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3 which is less affected by the hepatic blood flow, in some circulation disorders such as  
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5 portosystemic shunts, the increased plasma volume, and the decreased cardiac output.  
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8 The liver volume and a quantitative liver function test such as the ICG clearance test  
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10 have been reported to be significant predictors of postoperative liver failure and mortality (1,  
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12 29). However our result showed that the segmental liver reserve estimated by volumetry  
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14 ( $rV_L/V_L$ ) was significantly smaller than that estimated by HUI ( $rHUI/HUI$ ). Therefore,  
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16 volumetry could underestimate the segmental liver reserve because it could not take the  
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18 heterogeneity of the liver function into account. Because the HUI can correlate with ICG-  
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20 PDR very well and it can be determined directly from the volume and the signal intensity of a  
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22 region of interest in the liver, the quantitative estimation of total and segmental liver function  
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24 may be feasible. Therefore, gadoxetate disodium-enhanced MR imaging has the potential to  
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26 provide the required information for the diagnosis and management of liver diseases by one  
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28 examination, which can be essential to early detection and treatment.  
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34 Our study has several limitations. First, the study population was small, and further  
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36 prospective validation with a large population especially on segmental variation in liver  
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38 function is needed. Second, our eventual model did not use pre-contrast images; however, the  
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40 effect of the difference in the pre-contrast signal intensity between the liver and the spleen  
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42 was not significant. Therefore, HUI can be more convenient to apply for clinical practice than  
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44 using signal intensity change between pre and post-enhanced images.  
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48 In conclusion, the **liver function corresponding with ICG-PDR can be estimated**  
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50 **quantitatively from the signal intensities and the volumes of the liver and spleen on**  
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52 **gadoxetate disodium-enhanced MR images, which may improve the estimation of**  
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54 **segmental liver reserve.**  
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**Tables**
**Table 1** Liver characteristics of the 23 patients.

Patients	Degree of LF	ICG-PDR [sec <sup>-1</sup> ]	HUI [L]	V <sub>S</sub> [L]	L <sub>T2*</sub> /S <sub>T2*</sub>	L <sub>0</sub> /S <sub>0</sub>	L <sub>out</sub> /L <sub>in</sub>	S <sub>out</sub> /S <sub>in</sub>
#1	LC	0.064	0.425	0.403	0.643	1.434	1.008	0.915
#2	LC	0.071	0.239	0.157	0.736	1.040	0.868	0.939
#3	LC	0.072	0.270	0.115	0.654	1.123	1.035	0.946
#4	LC	0.082	0.203	0.079	1.073	1.068	0.975	0.978
#5	CH	0.083	0.588	0.296	0.712	1.304	0.987	0.898
#6	CH	0.105	0.419	0.136	0.839	1.221	0.859	0.905
#7	LC	0.121	0.365	0.194	0.810	1.102	0.996	0.936
#8	NL	0.122	0.787	0.292	1.028	1.229	1.010	0.972
#9	LC	0.130	1.046	0.413	0.631	1.125	0.991	0.911
#10	LC	0.134	0.451	0.122	0.732	1.143	1.003	0.841
#11	NL	0.135	0.961	0.150	0.684	1.137	0.957	0.912
#12	LC	0.149	1.165	0.324	0.624	1.632	1.018	0.930
#13	LC	0.149	0.721	0.125	0.560	1.434	0.882	0.902
#14	NL	0.152	0.930	0.043	0.769	1.215	1.018	0.926
#15	CH	0.153	0.515	0.148	0.690	1.214	0.967	0.887
#16	LC	0.158	0.464	0.156	0.820	1.167	0.953	0.913
#17	CH	0.179	0.698	0.089	0.840	1.151	0.978	0.888
#18	LC	0.181	0.874	0.099	0.788	1.376	0.981	0.915
#19	CH	0.182	0.407	0.102	1.163	1.108	0.963	0.957
#20	NL	0.193	1.296	0.274	0.785	1.286	0.992	0.957
#21	NL	0.207	1.068	0.139	0.890	1.040	1.013	0.898
#22	NL	0.215	1.001	0.077	0.984	1.464	0.977	0.872
#23	CH	0.267	1.475	0.108	0.836	1.049	0.960	0.913

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3 LF = liver fibrosis, NL = normal liver, CH = chronic hepatitis, LC = liver cirrhosis, ICG-PDR  
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5 = plasma disappearance rate of indocyanine green, HUI = Hepatocellular uptake index,  $V_S$  =  
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7 volume of the spleen,  $L_{T2^*}/S_{T2^*}$  = signal intensity ratio of the liver to the spleen in T2\*  
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9 weighted images,  $L_0/S_0$  = signal intensity ratio of the liver to the spleen in pre-contrast  
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11 enhancement T1-weighted images with fat suppression,  $L_{out}/L_{in}$  = signal intensity ratio of the  
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13 liver in out-of-phase T1-weighted images to in in-phase T1-weighted images,  $S_{out}/S_{in}$  = signal  
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**Table 2** Stepwise multiple linear regression analysis of various factors on ICG-PDR.

Variables	Coefficients	p-value
HUI	0.116	< 0.01
$V_S$	-0.229	< 0.01
$L_{T2^*}/S_{T2^*}$	0.075	0.06
$L_0/S_0$	-0.016	0.69
$L_{out}/L_{in}$	-0.001	0.99
$S_{out}/S_{in}$	-0.152	0.42

HUI = Hepatocellular uptake index,  $V_S$  = volume of the spleen,  $L_{T2^*}/S_{T2^*}$  = signal intensity ratio of the liver to the spleen in T2\*-weighted images,  $L_0/S_0$  = signal intensity ratio of the liver to the spleen in pre-contrast enhancement T1-weighted images with fat suppression,  $L_{out}/L_{in}$  = signal intensity ratio of the liver in out-of-phase T1-weighted images to in in-phase T1-weighted images,  $S_{out}/S_{in}$  = signal intensity ratio of the spleen in out-of-phase T1-weighted images to in in-phase T1-weighted images.

**Table 3** Characteristics of 4 patients with segmental heterogeneity of liver function

Patients	Affected segment	Cause	$r\text{HUI}/\text{HUI} - rV_L/V_L$
#4	S5, S6, S7, S8	OJ	0.428
#8	S8	OJ	0.120
#13	S5, S6, S7, S8	OJ	0.068
#22	S5, S6, S7, S8	PVE	0.083

OJ = obstructive jaundice, PVE = portal vein embolization,  $r\text{HUI}/\text{HUI}$  = HUI ratio of the unaffected liver to the total liver,  $rV_L/V_L$  = the volume ratio of the unaffected liver to the total liver.

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3 **Fig. 1** Axial 3D-GRE T1-weighted MR images with fat suppression (TR 3.5 msec/TE 1.42  
4 msec/FA 15°) at 20 min after gadoxetate disodium administration obtained from a 64 years  
5 old female patient (#23) with metastatic liver tumor. The contrast between the liver and  
6 spleen is high on gadxetate disodium-enhanced MR image. The surrounding liver was proven  
7 to be normal liver at surgical resection. HUI is high (1.068) consistent with high ICG-PDR  
8 (0.207). The outlines of the liver and the spleen are shown by green lines.  
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17 **Fig. 2** Axial 3D-GRE T1-weighted MR images with fat suppression (TR 3.5 msec/TE 1.42  
18 msec/FA 15°) at 20 min after gadoxetate disodium administration obtained from a 78 years  
19 old female patient (#22) with hilar bile duct carcinoma. Portal vein embolization (PVE) was  
20 performed in right branch of portal vein, and the signal intensity in the right hepatic lobe is  
21 decreased compared to that in the left hepatic lobe. The HUI ratio of the unaffected liver to  
22 total liver (rHUI/HUI) is 0.43, whereas the volume ratio of the unaffected liver to total liver  
23 (rV<sub>L</sub>/V<sub>L</sub>) is 0.32 and lower than rHUI/HUI. The outlines used to obtain rHUI and rV<sub>L</sub> are  
24 shown by green lines.  
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36 **Fig. 3** Axial 3D-GRE T1-weighted MR images with fat suppression (TR 3.5 msec/TE 1.42  
37 msec/FA 15°) at 20 min after gadoxetate disodium administration obtained from a 73 years  
38 old male patient (#4) with hepatocellular carcinoma. The contrast between the liver and  
39 spleen is low on gadxetate disodium-enhanced MR image. The surrounding liver was proved  
40 to be cirrhotic at surgical resection. HUI was low (0.203) consistent with a low ICG-PDR  
41 (0.082).  
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50 **Fig. 4** Correlation of HUI and ICG-PDR: The patients with splenomegaly (V<sub>s</sub> > mean + 1SD)  
51 are indicated by a red circle. The patients without splenomegaly (V<sub>s</sub> < mean + 1SD) are  
52 shown with blue circles. HUI: hepatocellular uptake index, ICG-PDR: plasma disappearance  
53 rate of indocyanine green, V<sub>s</sub> = volume of the spleen, SD = standard deviation.  
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3 **Fig. 5** Regression analysis of HUI and  $V_S$  on ICG-PDR: The patients with splenomegaly ( $V_S$   
4  $> \text{mean} + 1\text{SD}$ ) are indicated by a red circle. The patients without splenomegaly ( $V_S < \text{mean}$   
5  $+ 1\text{SD}$ ) are shown with blue circles. HUI: hepatocellular uptake index, ICG-PDR: plasma  
6 disappearance rate of indocyanine green,  $V_S$  = volume of the spleen, SD = standard deviation.  
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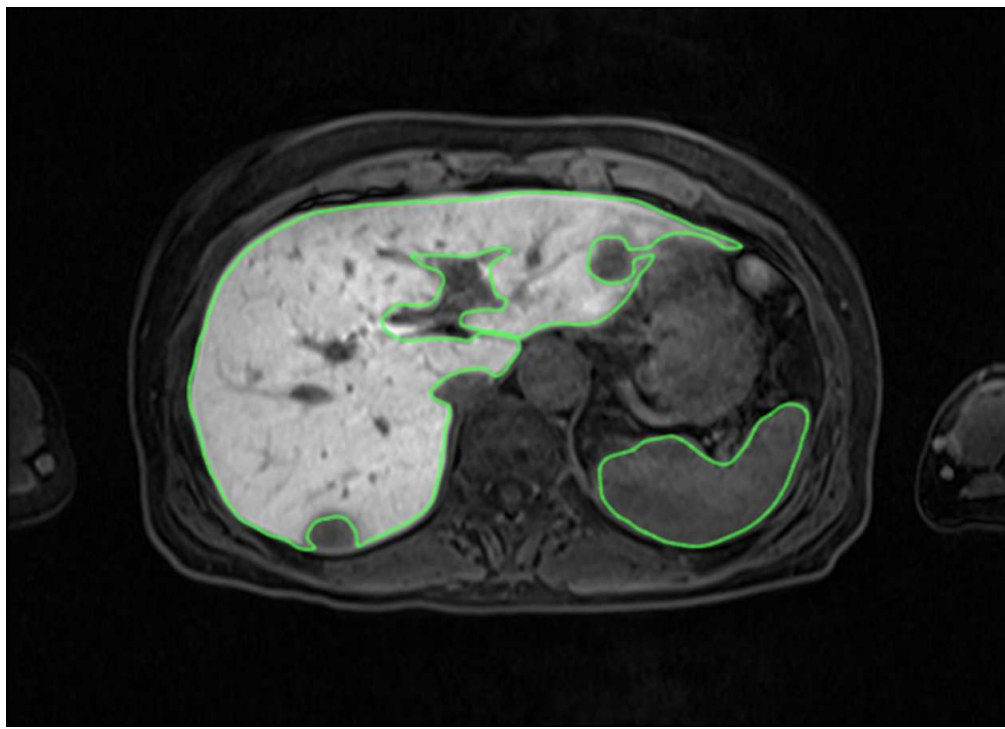


Figure 1. Case #23: A case with metastatic liver tumor: The contrast between the liver and spleen is high on gadxetate disodium-enhanced MR image. The background liver was proved to be normal liver by surgical resection. HUI is high (1.068) representing high ICG-PDR (0.207). The outlines of the liver and the spleen are shown by green lines.  
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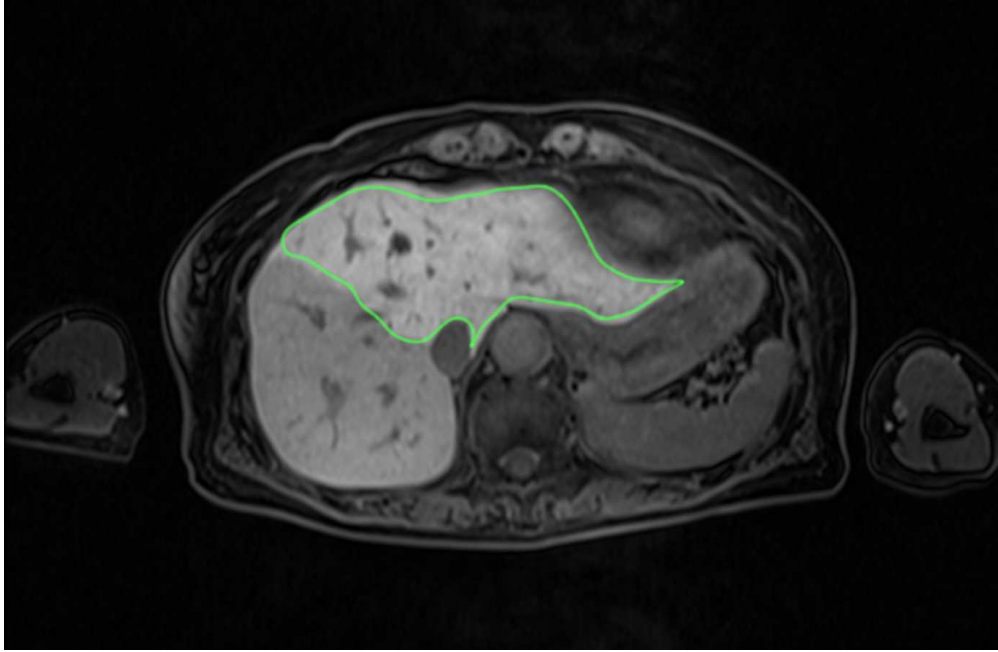


Figure 2. Case #22: A case with portal vein embolization (PVE): PVE was performed in right branch of portal vein, and the signal intensity in the right hepatic lobe is decreased compared to that in the left hepatic lobe. The HUI ratio of the unaffected liver to total liver ( $r_{HUI}/HUI$ ) is 0.43, whereas the volume ratio of the unaffected liver to total liver ( $r_{V_L}/V_L$ ) is 0.32 and lower than  $r_{HUI}/HUI$ . The outlines to obtain  $r_{HUI}$  and  $r_{V_L}$  are shown by green lines.  
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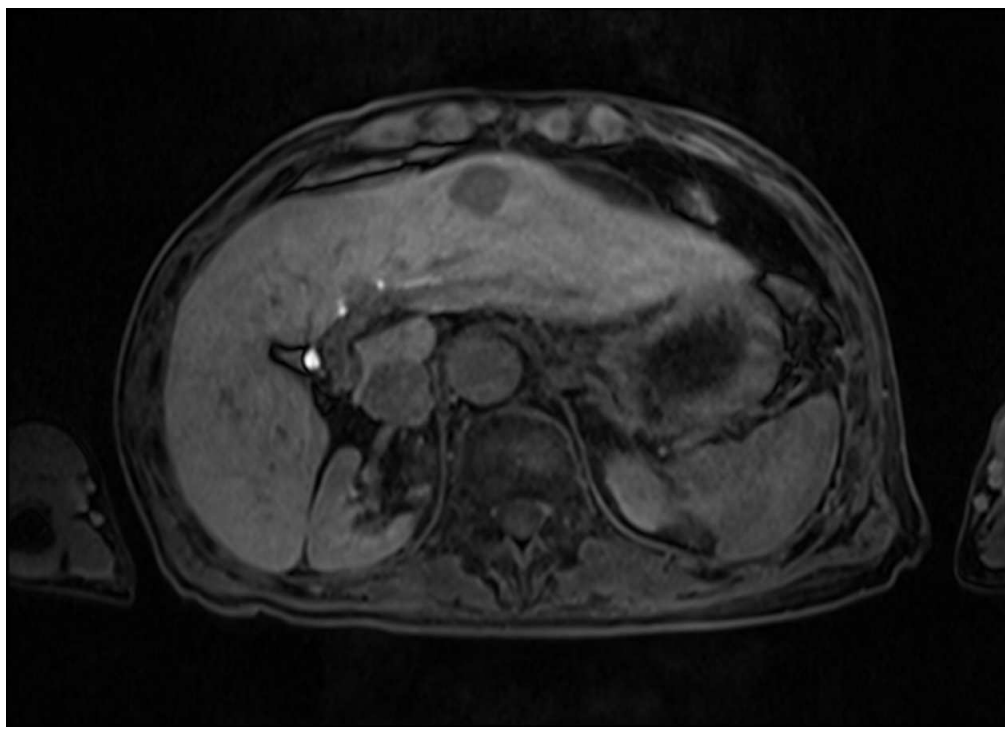


Figure 3. Case #4: A case with heparocellular carcinoma: The contrast between the liver and spleen is low on gadxetate disodium-enhanced MR image. The background liver was proved to be cirrhosis by surgical resection. HUI is low (0.203) representing low ICG-PDR (0.082).  
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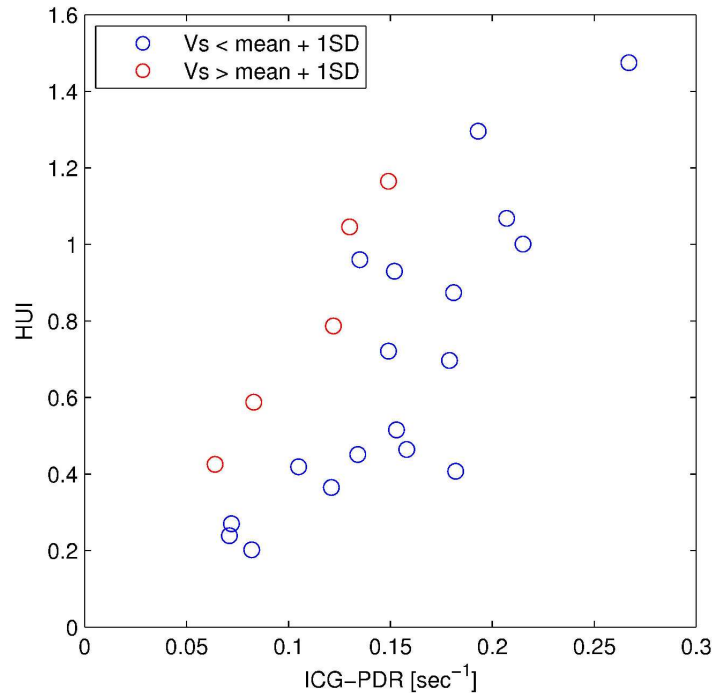


Figure 4. Illustration of correlation between HUI and ICG-PDR: The cases with splenomegaly ( $V_s > \text{mean} + 1\text{SD}$ ) are shown by red circle. The cases without splenomegaly ( $V_s < \text{mean} + 1\text{SD}$ ) are shown by blue circle. HUI: hepatocellular uptake index, ICG-PDR: plasma disappearance rate of indocyanine green,  $V_s$  = volume of the spleen.  
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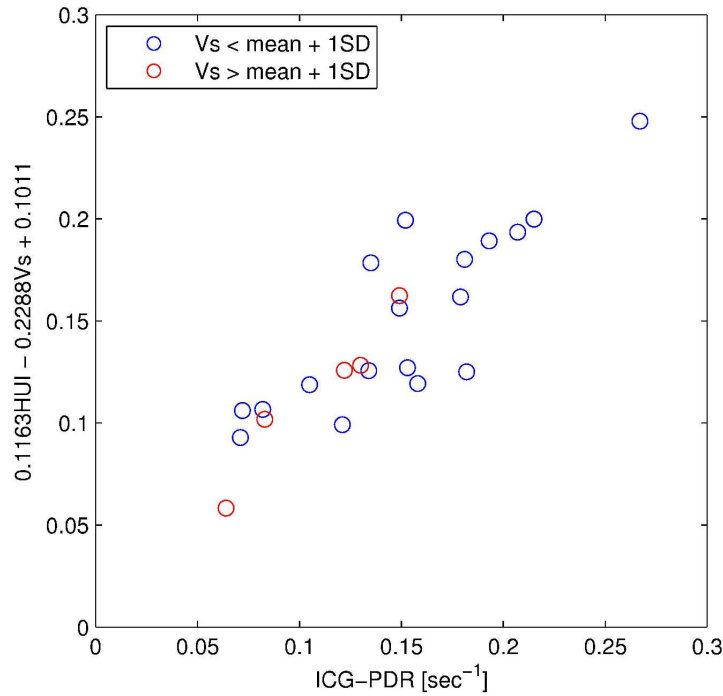


Figure 5. Regression analysis of HUI and VS on ICG-PDR: The cases with splenomegaly ( $V_s > \text{mean} + 1\text{SD}$ ) are shown by red circle. The cases without splenomegaly ( $V_s < \text{mean} + 1\text{SD}$ ) are shown by blue circle. HUI: hepatocellular uptake index, ICG-PDR: plasma disappearance rate of indocyanine green,  $V_s$  = volume of the spleen.  
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