

Quantum dots in imaging, drug delivery and sensor applications

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Abstract: Quantum dots (QDs), also known as nanoscale semiconductor crystals, are nanoparticles with unique optical and electronic properties such as bright and intensive fluorescence. Since most conventional organic label dyes do not offer the near-infrared (>650 nm) emission possibility, QDs, with their tunable optical properties, have gained a lot of interest. They possess characteristics such as good chemical and photo-stability, high quantum yield and size-tunable light emission. Different types of QDs can be excited with the same light wavelength, and their narrow emission bands can be detected simultaneously for multiple assays. There is an increasing interest in the development of nano-theranostics platforms for simultaneous sensing, imaging and therapy. QDs have great potential for such applications, with notable results already published in the fields of sensors, drug delivery and biomedical imaging. This review summarizes the latest developments available in literature regarding the use of QDs for medical applications.

Keywords: quantum dots, biomedical applications, nanoprobles, theranostic platforms

Introduction

Quantum dots (QDs), also known as nanoscale semiconductor crystals, were first described by Ekimov and Onushenko¹ in a glass matrix, back in 1981, with the first biological imaging application reported in 1998.² Since then the field of QDs has been growing steadily and now includes applications in fields of solar cells, photovoltaic devices, light-emitting diode (LED) fabrication, photodetectors, computing, biomedical imaging and so on.

Most conventional organic label dyes do not offer the near-infrared (NIR) (>650 nm) emission possibility; this region is highly desired for biomedical imaging due to its reduced light scattering and low tissue absorption, it is why QDs with their tunable optical properties have gained a lot of interest.³ These nanometric semiconductors offer unique and fascinating optical properties, such as high quantum yield, size-tunable light emission and good chemical and photo-stability.⁴ QDs, with sizes 2–10 nm, are generally composed of elements (such as Cd, Pb, Hg) from groups II–VI, III–IV and IV–VI in the periodic table. More recently, researchers have developed ternary I–III–VI QDs (where I = Cu or Ag, III = Ga or In, VI = S or Se).⁵ Different types of QDs can be excited with the same light wavelength, and their narrow emission bands can be detected simultaneously for multiple assays. The fluorescence bands of QDs are dependent on their composition, size and shell thickness.⁶ If the particle size is smaller than the bulk materials' Bohr radius, it causes the energy levels to pose atom-like properties and become discrete compared to the continuum energy levels observed in bulk materials; in other words, these unique properties result from the confinement of

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the states of charge carriers by the physical reduction in the size of the nanoparticles.⁷ In order to use QDs under ambient conditions, they must be stabilized or passivated, because of their high reactivity and surface area. When choosing a stabilizer, one has to take into account the absorption and luminescence spectra profile; also the quantum yield and the lifetime depend on the environment composition.⁸

There is an increasing interest in the development of nano-theranostics platforms for simultaneous sensing, imaging and therapy. QDs have great potential for such applications, with promising results published in the fields of sensors, drug delivery and biomedical imaging. The present paper summarizes the latest developments available in literature regarding the use of QDs for the aforementioned medical applications.

Imaging

Although fluorescence imaging has been used in animal models, this approach is limited by the poor transmission of visible light through the biological tissue. This has prompted researchers to make use of the NIR optical window (700–1,700 nm) in order to conduct deep-tissue optical imaging with the aid of QDs.^{9,10} A large number of formulations for QDs bio-imaging is currently available in literature.

Kim et al¹¹ proposed polydentate phosphine-coated QDs for major cancer surgery in large animals as a direct visual guidance throughout the entire sentinel lymph node mapping procedure, which permits a real-time confirmation of complete resection. Capped InP@ZnS QDs were used for cellular imaging by Kobayashi et al¹² in order to simultaneously visualize the draining of five separate lymphatic flows.

Heavy metal-free/cadmium-free biocompatible QDs with a good photoluminescence quantum yield were recently evaluated for their capability for lymph node mapping with the aid of an ex vivo imaging model. These indium-based QDs showed a strong retention confined to the regional lymph, fast localization (minutes) and stable photoluminescence. Moreover, the lack of any Class A elements (Cd, Hg and Pb) in their structure makes suitable candidates for future biomedical applications.¹³ Another interesting approach for biomedical imaging applications was reported by Yu et al, which developed gadolinium-doped carbon dots for fluorescence/magnetic resonance imaging (MRI) imaging. A one-pot hydrothermal method was employed in order to obtain bio-imaging nanoprobcs (~5.5 nm in size, nearly spherical) from citric acid, with high spatial resolution for MRI and enhanced fluorescence compared to that of carbon dots alone.¹⁴

Nitrogen and sulfur co-doped carbon dots (N,S/CDs), 1.7 nm in size, with a high fluorescence quantum yield (39.7%) were obtained by Chen et al. They posed low toxicity and good biocompatibility when co-incubated with HeLa cells. These types of doped CDs can be used to detect Cr (IV) by means of fluorescence quenching.¹⁵ In another case, gadopentetic acid was used as the Gd source and glycine as the surface passivation agent in order to obtain Gd-doped carbon dots with an average size of ~18 nm capable of enhancing irradiation dose deposition.¹⁶

The work conducted by Han et al showed that antibody-conjugated QDs can diffuse into the bone marrow and label single cells of rare populations of progenitor and hematopoietic cells. By employing this method, the disadvantages associated with fluorescently labeled antibodies such as low photo-stability, small multiphoton action cross-section and asymmetric emission are no longer an issue.¹⁷

In order to achieve superior biomedical properties, Osifeko and Nyokong have proposed hybrid nanoparticles with phthalocyanines in combination with QDs, magnetic nanoparticles and gold nanoparticles (GNPs). Their results showed an increase in triplet quantum yields for phthalocyanines in the presence of QDs and GNPs, while a general decrease in fluorescence quantum yields for them was observed in the presence of all the nanoparticles investigated (QDs, GNPs and magnetic nanoparticles).¹⁸ Glutathione-capped FePt–CdS bimodal nanoprobcs were proposed by Jha et al for fluorescence imaging and MRI. The synthesis route described thioglycolic acid-capped FePt magnetic nanoparticles used as templates for the development of the CdS QD fluorescent counterparts. In this case, the glutathione coating provided biocompatibility and ligand attachment sites on the nanoprobcs.¹⁹

Core-shell QDs such as CdSe@ZnS were employed in the quantitative determination of micrococcal nuclease, the extracellular nuclease of *Staphylococcus aureus*. In this case, the QDs were conjugated to a single-stranded DNA (ssDNA)-fluorescent dye FRET probe.²⁰ Hafian et al undertook multiphoton imaging of tumor biomarkers by conjugating single-domain antibodies to CdSe@ZnS QDs. These nanoprobcs, with a hydrodynamic diameter of 11.9 nm, offer a viable alternative to conjugates of conventional organic fluorophores for imaging biomarkers.²¹ Yakoubi et al focused on obtaining core-shell Cu-doped CdZnS QDs via a low-temperature aqueous-based route. Their Cu:CdZnS@ZnS QDs presented high stability and high photoluminescence quantum efficiency, with the option to tune the PL from 470 to 620 nm by increasing Cd and Cu²⁺ composition.²²

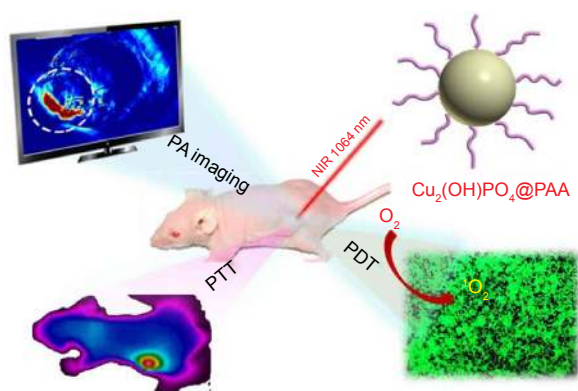


Figure 1 Proposed $\text{Cu}_2(\text{OH})\text{PO}_4@PAA$ “three-in-one” multifunctional theranostic platform.

Notes: Reprinted with permission from Guo W, Qiu Z, Guo C, et al. Multifunctional theranostic agent of $\text{Cu}_2(\text{OH})\text{PO}_4$ quantum dots for photoacoustic image-guided photothermal/photodynamic combination cancer therapy. *ACS Appl Mater Interfaces*. 2017;9(11):9348–9358. Copyright 2017 American Chemical Society.²³

Abbreviations: $\text{Cu}_2(\text{OH})\text{PO}_4@PAA$, polyacrylic acid-coated $\text{Cu}_2(\text{OH})\text{PO}_4$ quantum dots; PA, photoacoustic; PDT, photodynamic therapy; PTT, photothermal therapy.

The work of Guo et al focused on the fabrication of polyacrylic acid-coated $\text{Cu}_2(\text{OH})\text{PO}_4$ quantum dots ($\text{Cu}_2(\text{OH})\text{PO}_4@PAA$ QDs) that exhibit a strong NIR photo-absorptive ability as a “three-in-one” multipurpose cancer theranostic system (Figure 1). A combination phototherapy of photodynamic therapy (PDT) and photothermal therapy (PTT) along with photoacoustic imaging modality was achieved. Under NIR excitation, a local hyperthermia and reactive oxygen species (ROS) were generated realizing the synergetic PTT/PDT therapeutic effects. Also these QDs presented themselves as good candidates for in vivo photoacoustic imaging on the tumor site for realizing an imaging-guided therapeutic process.²³ Iodine-doped carbon dots (I-doped CDs), mono-dispersed spherical nanoparticles ~2.7 nm in diameter, were synthesized by Zhang et al in order to be used as computed tomography contrast agents and fluorescence probes. These I-doped CDs displayed wavelength-dependent excitation and stable photoluminescence, superior X-ray attenuation properties in vitro and good biocompatibility.²⁴

Drug delivery

The development of diagnostic and treatment capabilities into one nanoparticle-based agent has been the focus of several groups. QDs are good candidates as theranostic platforms, as they can act as the main nanocarrier or be part of a more complex architecture as the fluorescent labels.

Paclitaxel (PTX), a widely acknowledged drug choice for the treatment of various human cancers, along with $\text{CdTe}@ZnS$ QDs were co-loaded in nanostructured lipid carriers in order to have theranostic approach in cancer therapy.

The results from Olerile et al²⁵ showed an encapsulation efficacy of ~80% and drug loading of 4.68% with a tumor growth inhibition rate of 77.85%. In another study, hybrid silica nanocapsules that were loaded with ZnSe:Mn/ZnS core-shell and the anticancer drug PTX have been proposed by Zhao et al as theranostic platforms for chemotherapy and fluorescence imaging. The setup involved hydrophobic inner cores that contain the PTX molecules and the $\text{ZnSe:Mn}@ZnS$ QDs and a hydrophilic silica outer shell with amino groups on the surface as anchors for the targeting molecules. Results showed that solubility of PTX was enhanced 630 times while the drug could be sustained released in 12 h.²⁶

Doxorubicin (DOX) was loaded on to pH-responsive ZnO QDs by Cai et al. They synthesized ultrasmall QDs (~3 nm) functionalized with poly(ethylene glycol) (PEG) and hyaluronic acid to target the overexpressed glycoprotein CD44 in cancer cells and DOX as the model drug for the study. This drug delivery platform for intracellular controlled release of drugs could release its DOX payload under the acidic intracellular conditions (Figure 2).²⁷ The work of Yang et al focused on quercetin (QE)-loaded $\text{CdSe}@ZnS$ QDs as anticancer and antibacterial nanoplatfroms. Their results showed that QE-loaded $\text{CdSe}@ZnS$ were more effective against drug-resistant *Escherichia coli* and *Bacillus subtilis* and then QE or CdSe nanoparticles alone. The anticancer activity assay was focused on the proliferation and migration of BGC-823 cells, which showed an increase in cytotoxicity of two- to sixfold compared to raw QE and CdSe QDs.²⁸

For the enhanced targeted delivery of 5-fluorouracil (5-FU), the model proposed by Bwatanglang et al made use of folate receptors expressed in malignant tissues. Mn:ZnS QDs were encapsulated in chitosan (CS) biopolymer and functionalized with folic acid (FA). The resulted composite ($5\text{-FU}@FACS\text{-Mn:ZnS}$) was assessed in vivo in tumor-bearing mice, where they contributed to smaller tumor size and less events of metastasis in the lungs compared to the groups treated with just the 5-FU drug. The in vitro results were also encouraging; the $5\text{-FU}@FACS\text{-Mn:ZnS}$ NPs induced higher levels of apoptosis in breast cancer cells (MDA-MB231) compared to the effect of just the 5-FU drug toward the same cell line.²⁹ Gemcitabine (GEM)-programed nanovectors for targeted pancreatic cancer therapy were obtained by functionalizing CdSe/ZnS QDs with matrix metalloproteinase-9 (MMP-9) detachable, PEG, cathepsin B cleavable GEM and targeting ligand CycloRGD. In this case, the PEG corona ensured prolonged blood circulation time and avoided nonspecific interactions. Once the QDs are accumulated in the tumor, the corona is

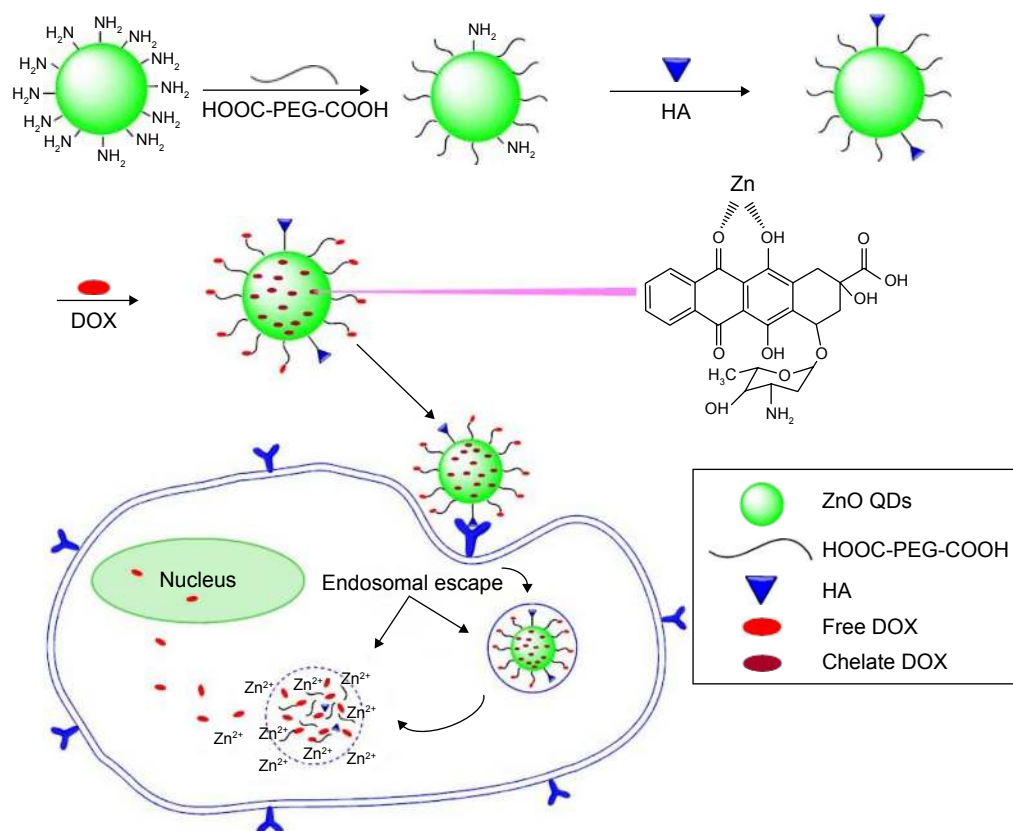


Figure 2 Graphical representation of the hyaluronic acid–ZnO quantum dots–dicarboxyl-terminated poly(ethylene glycol) (HA-ZnO-PEG) drug delivery system.

Notes: Reprinted with permission from Cai X, Luo Y, Zhang W, et al. pH-Sensitive ZnO quantum dots–doxorubicin nanoparticles for lung cancer targeted drug delivery. *ACS Appl Mater Interfaces*. 2016;8(34):22442–22450. Copyright 2016 American Chemical Society.²⁷

Abbreviations: DOX, doxorubicin; HA, hyaluronic acid; PEG, poly(ethylene glycol); QDs, quantum dots.

removed by the overexpressed MMP-9 and the RGD exposed in order to enhance the cellular internalization process. Inside the pancreatic cells, elevated levels of lysosomal cathepsin B promote the release of GEM; a schematic illustration of the process is presented in Figure 3.³⁰

Chiu et al developed a nanotheranostic platform based on carbon quantum dots (CQDs) doped with S, N and Gd (GdNS@CQDs). In order to have a targeted dual mode fluorescence/MRI, the GdNS@CQDs were functionalized with FA through ECD/Sulfo-NHS reaction and the targeting capability was evaluated on two cancerous cell lines, HeLa and HepG2. The obtained nanoplatforms showed good stability, biocompatibility and low toxicity. Moreover, the drug-loading capacity for FA-GdNS@CQDs with DOX, an anticancer drug, was ~80% and its release proved to be pH-sensitive. Thus, these nanotheranostic platforms have been reported to have bimodal contrast imaging functionality (fluorescence/magnetic resonance), cancer cell targeting and pH-sensitive drug release capabilities.³¹

Unlike semiconductor QDs, CQDs have low toxicity, good biocompatibility and broad excitation spectra. CQDs from sodium alginate for gene delivery applications have

been developed by Zhou et al in a one-step green process. In the proposed one-step hydrothermal carbonization route, alginate is both the carbon source and the cationization agent. The obtained CQDs, with their strong capacity to condense plasmid DNA and high transfection efficiency, could play a dual role as gene vectors and as bioimaging probes.³² Graphene quantum dots (GQDs) were shown to enhance the anticancer activity of cisplatin by Sui et al, mainly through the fact that they enhance cellular uptake of the drug; the proposed mechanism is depicted by Sui et al.³³

Another exciting application for GQDs has been reported in the fight against Alzheimer's disease, where glycine–proline–glutamate-conjugated graphene quantum dots (GQDGs) were developed and evaluated on in vitro and an in vivo murine model. The GQDGs had an inhibitory effect on the aggregation of amyloid- β fibrils, the number of newly generated neuronal precursor cells and neurons increased.³⁴

Sensors

By employing the unique properties of QDs, new strategies for the identification and quantification of biological relevant molecules have been presented in the last years.

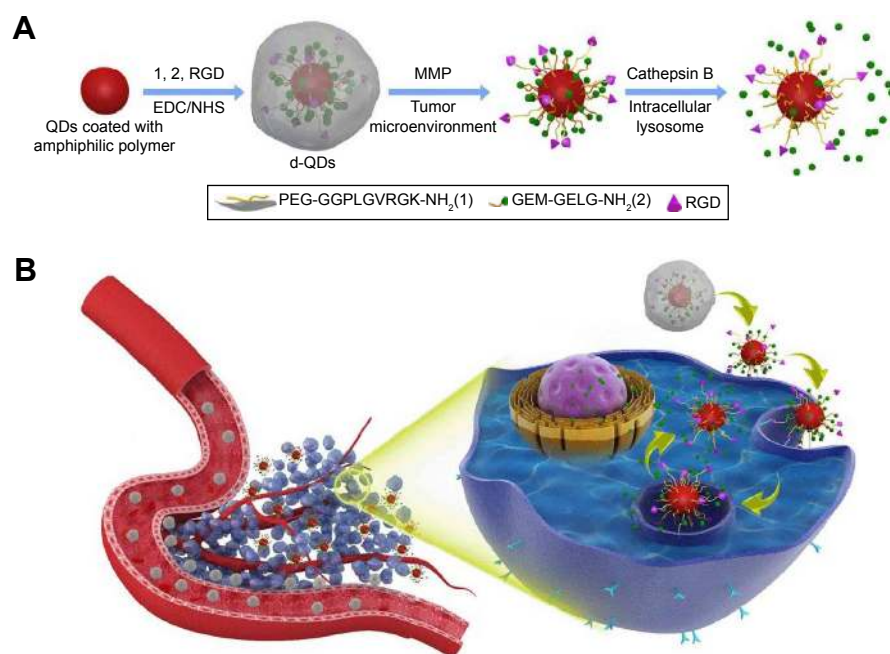


Figure 3 (A) Schematic illustration of the nanovectors preparation protocol and their enzyme sensitive behavior. **(B)** Schematic illustration of the nanovectors delivering GEM to pancreatic cancer cells.

Notes: Reprinted with permission from Han H, Valdeperez D, Jin Q, et al. Dual enzymatic reaction-assisted gemcitabine delivery systems for programmed pancreatic cancer therapy. *ACS Nano*. 2017;11(2):1281–1291. Copyright 2017 American Chemical Society.³⁰

Abbreviations: d-QDs, dual-enzyme quantum dots; EDC, 1-Ethyl-3-(3-dimethylaminopropyl)carbodiimide; GEM, gemcitabine; MMP, matrix metalloproteinase; NHS, N-hydroxysuccinimide; RGD, CycloRG; QDs, quantum dots.

One of the first reports of QDs (ZnS@CdSe) for ultrasensitive nonisotopic detection was published by Chan and Nie.³⁵ For the detection of the CA-125 serum biomarker in patients with ovarian cancer, Johari-Ahar et al proposed an impedimetric immunosensor that consisted of a mercaptopropionic acid-modified gold electrode functionalized with silica-coated gold nanoparticles, CdSe QDs and the anti-CA-125 monoclonal antibody. This setup allowed for the detection of the targeted biomarker down to 0.0016 U/mL.³⁶

Leishmaniasis is a parasitic disease, one of the six most important diseases that affects humans and various animal species. Andreadou et al developed a Leishmania-specific surface antigens detection method based on a combination of magnetic beads and CdSe QDs with a specificity of 100% and a low limit of detection of 3,125 ng/μL for *Leishmania* DNA. The method was based on the fact that the analytes were isolated from the solutions with the aid of the magnetic beads and the detection part was played by the QDs.³⁷ A sensitive sensor for probing the interaction of clofazimine (an effective drug multidrug-resistant tuberculosis and breast cancer) with proteins with the aid of fluorescence spectroscopic techniques was proposed by Yang et al. They developed CdZnSeS/ZnS alloyed core/thick-shell QDs as energy donors Förster resonance energy transfer (FRET) applications (Figure 4). These QDs were capped with multifunctional polymer ligands containing dihydrolipoic acid via a direct ligand-exchange

method and further functionalized with cyanine 3-labeled human serum albumin.³⁸

Zn²⁺-modulated L-cysteine-capped CdTe QDs were used for the detection of adenosine 5'-triphosphate (ATP) in human serum samples. In this case, the Zn²⁺ ions can bind with the ATP molecules through Zn–O–P bonds, and the initial quenching process resulted from the interaction of Zn²⁺ ions with the L-cysteine layer from the CdTe QDs would be avoided.³⁹

Another application of CdTe QDs has been proposed in combination with the immunomagnetic separation technique for rapid enumeration of *E. coli*. For this, magnetic Fe₃O₄@Au nanoparticles were functionalized with biotinylated *E. coli*-specific antibodies, while CS was used to modify the CdTe QDs. By using magnetic nanoparticles for bacteria separation and QDs for labeling, the method achieves a detection limit of 30 cfu/mL⁻¹ of *E. coli* and a high specificity.⁴⁰

In order to investigate heme iron absorption, Geng et al proposed using hemin-conjugated CdSe@ZnS nanoprobe in *in vitro* and *in vivo* experimental setups. Their results showed that this QD configuration is a suitable tracer for the heme iron absorption and that both active transport hemoglobin carrier protein-1 and endocytosis pathways are involved in heme uptake in Caco-2 cells.⁴¹ In another approach, core/multishell QDs (CdSe@ZnS@CdS@ZnS) with photoluminescence quantum yields as high as 100% were obtained by layer-by-layer precursor deposition. In this case, each layer

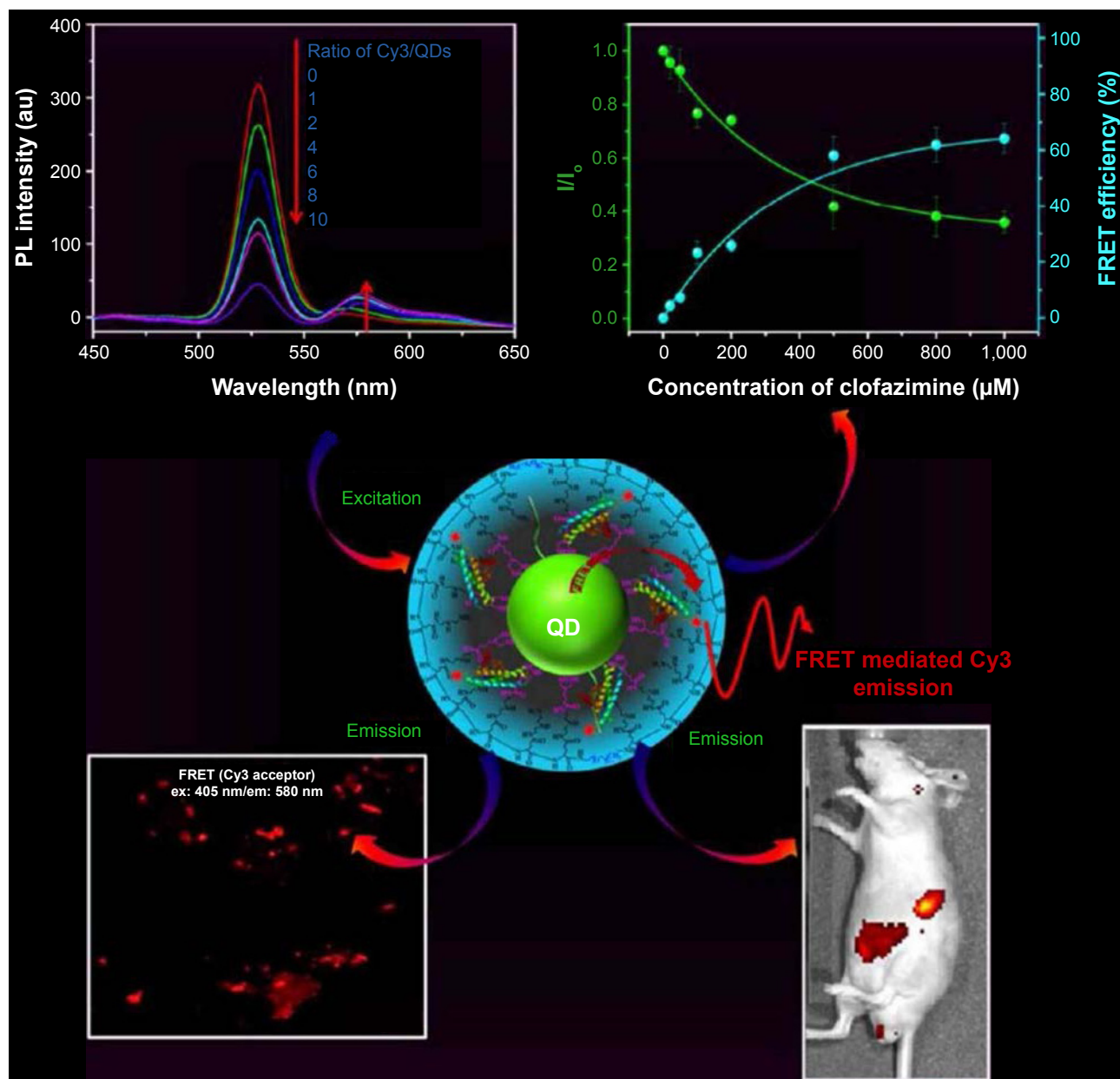


Figure 4 CdZnSeS/ZnS alloyed core/thick-shell QDs as energy donors for FRET applications.

Notes: Adapted with permission from Yang HY, Fu Y, Jang MS, et al. Multifunctional polymer ligand interface CdZnSeS/ZnS quantum Dot/Cy3-labeled protein pairs as sensitive FRET sensors. *ACS Appl Mater Interfaces*. 2016;8(51):35021–35032. Copyright © 2016 American Chemical Society.³⁸

Abbreviations: Cy3, cyanine 3; em, emission; ex, excitation; FRET, Förster resonance energy transfer; PL, photoluminescence; QD, quantum dot.

deposited on to the CdSe core had a specific role: the first ZnS shell acts as a potential barrier for electron-hole pairs, the CdS shell is a separator between the two ZnS shells, increasing shell thickness, and the outer ZnS shell is an additional potential barrier, compatible with already known protocols for QD functionalization.⁴² A QD aggregation-based detection strategy to quantify heparin was proposed by Dong et al, where antithrombin III (AT III)-labeled QDs specifically bind to active heparin molecules to form complexes that aggregate upon the addition of cationic surfactant

micelles (Figure 5). This approach had a linearity in the range of 4.65×10^{-4} U/mL to 0.023 U/mL and a limit of detection of 9.3×10^{-5} U/mL.⁴³

The specific recognition of transferrin (TRF), a 77 kDa glycoprotein responsible for iron transport, was achieved by Chang et al by using mercaptophenylboronic acid-capped Mn-doped ZnS QDs (QDs-MBA). The method is based on a turn-on effect by the fact that TRF binds to the MBA via boronate affinity interaction to efficiently enhance the fluorescence of the QD@MBA, with a limit of detection

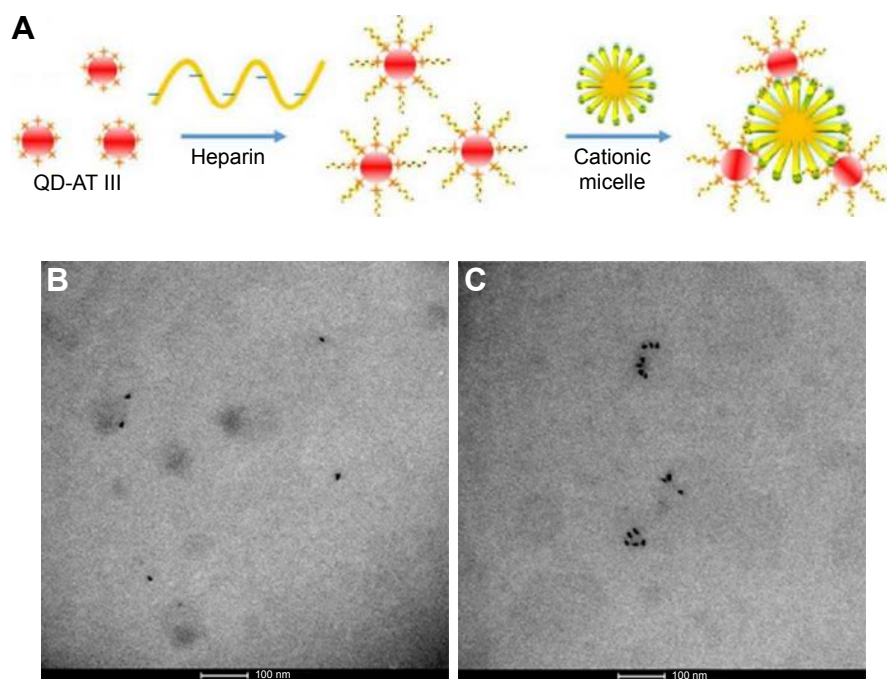


Figure 5 (A) Scheme of aggregated QD formation. (B) TEM image of QD-AT III-heparin without CTAB. (C) TEM image of QD aggregation with CTAB.

Notes: Reprinted with permission from Dong S, Liu X, Zhang Q, et al. Sensing active heparin by counting aggregated quantum dots at single-particle level. *ACS Sens.* 2017;2(1):80–86. Copyright 2017 American Chemical Society.⁴³

Abbreviations: AT III, antithrombin III; CTAB, cetyl trimethylammonium bromide; QD, quantum dot; TEM, transmission electron microscopy.

for TRF down to 5.69×10^{-9} M and a serum sample recovery from 87.9% to 96.5%. This approach can be employed for the detection of trace glycoproteins in complex biological samples.⁴⁴

Graphene quantum dots (GQDs) present an interesting approach for L-ascorbic acid detection and alkaline phosphatase (ALP) activity. Huang et al demonstrated that GQDs can act as sensors, their fluorescence quenched in the presence of para-benzoquinone (BQ) and then turned on when L-ascorbic acid reduces the BQ molecules. For ALP activity evaluation, the ALP hydrolyzed L-ascorbic acid-2-phosphate and produced ascorbic acid, which turned on the fluorescence of the nanoprobe.⁴⁵

Caballero-Diaz et al⁴⁶ proposed using nitrogen-doped grapheme quantum dots (N-GQDs) as the fluorescent probe along with acetylcholinesterase (AChE) enzyme as the biorecognition element for the detection of fenoxycarb pesticide.

For the detection of Pb^{2+} ions, carbon dots (CDs) obtained through a green synthesis method from *Ocimum sanctum* leaves was proposed by Kumar et al. CDs, 4–7 nm in size, were fabricated in a one-step hydrothermal method from the natural source with no supplementary functionalization steps needed in order to use them for lead sensing and cell imaging. The detection of Pb^{2+} was based on the fact that the lead ions induce fluorescence quenching of the CDs with a

linear detection range of 0.01–1 μ M and a limit of detection of 0.59 nM.⁴⁷

Toxicity

The toxicity concerns regarding QDs are mainly related to their chemical composition, especially in the case of QD containing heavy metal ions such as Cd and Hg. In order to use QDs in clinical applications, they must exhibit minimal toxicity.⁴⁸ This can be ensured by functionalizing the QD surface with biocompatible molecules. One approach for QD functionalization is to take advantage of the fact that mercapto groups can bind easily to zinc atoms and small cysteine-rich proteins that can bind up to monovalent or up to seven divalent heavy metal ions.⁴⁹ Tmejova et al investigated the interactions between mercaptosuccinic capped CdTe (CdTe-MSA) QDs and metallothionein (MT) proteins. Their work showed that, along with electrostatic forces, QD size has a strong influence on MT proteins and QDs, with the smallest QDs having a higher affinity for this type of interaction.⁵⁰

CdTe QDs were used as a model for investigating the effects of QDs on the nuclear factor- κ B (NF- κ B) signaling pathway in in vitro and in vivo experiments. In this case, it was found that QDs can selectively inhibit both canonical and the non-canonical NF- κ B activation, which can lead to new

directions in anti-cancer, anti-inflammatory and anti-viral drug therapies.⁵¹ In addition, it was found by Wu et al that CdTe QDs can alter the molecular basis of fatty acid synthesis and degradation, without influencing the degradation of phospholipids in the *Caenorhabditis elegans* animal model. The increased fat storage in the intestines of the nematodes was attributed to the prolonged defecation cycle length and not to the cadmium ions released from the QDs. These findings shed light on the environmental impact of CdTe QDs on the lipid metabolism in certain animals.⁵²

The work conducted by Fan et al focused on CdTe@CdS QDs toxicity in in vitro and in vivo experimental setups. QD-induced nanotoxicity was observed in the studied cell lines, with autophagy as the general response to QD exposure. For the murine model, the injection of QDs determined splenic injury, liver injury, nephrotoxicity and hematopoietic disorders, with ROS involved in toxicity induction and autophagy initiation.⁵³

Cadmium oxide nanoparticle toxicity was evaluated by Balmuri et al on a zebrafish model. They studied two types of CdO nanoparticles: one where CdO was obtained through calcination of Cd(OH)₂ to yield nanoparticles without any organic molecules on the surface (CdO-1) and another type

that involved the calcination of Cd-citrate (CdO-2). The toxic effect registered for the CdO-2 was lower than for the CdO-1; this result could be attributed to a carbon layer that covered the surface of CdO-2 during the calcination process. Thus, by using organic molecules in the preparation of CdO nanoparticles, their toxicity can be reduced by forming carbon surface coverage that impedes the release of Cd²⁺ ions in biological systems.⁵⁴

Saccharomyces cerevisiae yeast was used, as a model, by Pasquali et al in order to shed light on the effect of CdS QDs on the complex genetic networks that regulate nucleomitochondrial interaction. The results showed the disruption of the mitochondrial morphology, a reduced mitochondrial function and induced oxidative stress.⁵⁵ The in vivo and in vitro assessment of nanotoxicity of CS-functionalized CdS QDs was reported by de Carvalho et al. Results showed that even when CdS QDs were coated with this biocompatible aminopropylsaccharide shell induced a severe inhibition of cell viability for human osteosarcoma cells (SAOS) and for human embryonic kidney cells (HEK293T). However, for the in vivo experiments, BALB/c mice were intravenously injected with the CS-coated CdS QDs where they showed no evident toxicity after 30 days.⁵⁶ Blood clearance, distribution,

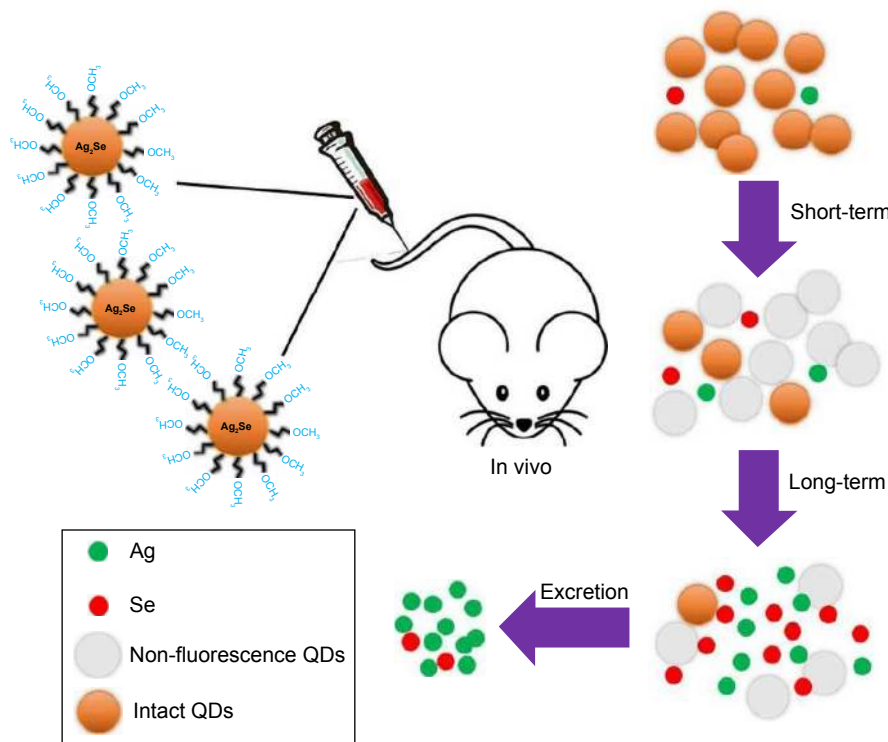


Figure 6 Biotransformation of Ag₂Se, where Ag released from the QDs is excreted through feces and urine and the Se element is hardly excreted.

Notes: Reprinted with permission from Tang H, Yang ST, Ke DM, et al. Blood clearance, distribution, transformation, excretion, and toxicity of near-infrared quantum dots Ag₂Se in mice. *ACS Appl Mater Interfaces*. 2016;8(28):17859–17869. Copyright 2016 American Chemical Society.⁵⁷

Abbreviation: QDs, quantum dots.

transformation, excretion and toxicity of PEG-coated Ag₂Se QDs (fluorescent probes in the second NIR window) in mice after intravenous was assessed by Tang et al. They found that Ag₂Se QDs-PEG prefer to accumulate in the spleen and liver but transformed and/or cleared within 1 day after administration. The released Ag from the QDs is excreted through both feces and urine, and the Se element is hardly excreted (Figure 6).⁵⁷

In order to passivate QDs for biological applications. They can be encapsulated in phospholipid micelles. This approach has several advantages, such as it does not alter their surface, the optical properties of the QDs are retained, due to the highly dense surface of the micelles nonspecific adsorption is prevented and the supramolecular architecture is maintained by local hydrophobic interactions.⁵⁸ Other functionalization strategies in order to confer biological activity and low toxicity to QDs is to conjugate them to antibodies. For example, a QD with a 4 nm diameter can have its surface functionalized with 2–5 protein molecules or 50 small molecules.⁵⁹ There are a number of available methods ranging from non-covalent binding (electrostatic interactions⁶⁰ or biotin–avidin systems⁴) to covalent binding (between amine and carboxylic acid groups, between aldehyde and hydrazine functions and between amino and sulfhydryl groups⁶¹). The potential toxicity of different types of QDs such as metal-free or CQDs remains one of the main interests of the scientific community with the need of better understanding the interactions between QDs and biological macromolecules.

Conclusion

It is clear that QDs have great potential for applications in areas such as drug delivery, sensors and bio-imaging. In order to see QDs realistically translated in clinical applications, several issues still need to be addressed, such as overall toxicity, body clearance, synthesis protocol scalability, environmental impact, manufacturing costs and so on. By combining QDs with other types of nanoparticles and/or biological active molecules, theranostic platforms are constantly being developed. This review summarizes the latest developments available in literature regarding the use of QDs for medical applications.

Acknowledgments

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Disclosure

The authors report no conflicts of interest in this work.

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