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1 **Recent advances in emulsion-based delivery approaches**  
2 **for curcumin: From encapsulation to bioaccessibility**

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19

20

21 **Abstract**

22 **Background**

23 Curcumin has been widely acknowledged for its health-promoting effects. However, its application is  
24 often limited by its poor water solubility and biochemical/ structural degradation during physiological  
25 transit that restricts its bioavailability. Emulsion based approaches have attracted the most research  
26 attention to encapsulate curcumin and improve its stability, bioaccessibility and bioavailability.

27

28 **Scope and approach**

29 This review summarizes the recent advances in application of different oil-in-water emulsion-based  
30 approaches, such as, conventional emulsions (surfactants-, protein- and protein-polysaccharide-  
31 stabilized emulsions), nanoemulsions, and Pickering emulsions that have been specifically used to  
32 deliver curcumin. Particular emphasis is given to factors affecting curcumin solubility, change in  
33 crystalline structure of curcumin upon dispersion and encapsulation efficiency. Changes in the droplet  
34 size and emulsion stability during in vitro oral-to-gastrointestinal digestion are discussed, with clear  
35 focus on the bioaccessibility of the encapsulated curcumin.

36

37 **Key findings and conclusions**

38 Key factors that influence curcumin delivery include emulsion droplet size, oil composition, volume  
39 fraction, dispersion conditions of curcumin in the oil phase and the type of interfacial materials.  
40 Nanoemulsions have been the preferred choice for delivery of curcumin up to now. Although scarce in  
41 literature, emulsions stabilized by edible Pickering particles as shown by recent evidence are effective  
42 in protecting curcumin in an in vitro gastrointestinal setting due to their high coalescence stability.  
43 Further studies with emulsions stabilized by food-grade particles and accurate tracking of the  
44 physiological fate (in vitro to human trials) of different emulsion-based delivery vehicles are essential  
45 for rational designing of curcumin-rich functional foods with high bioaccessibility.

46

## 47 **Keywords**

48 Curcumin; Pickering emulsion; Nanoemulsion; Encapsulation efficiency; Bioaccessibility

49

## 50 **1 Introduction**

51 Curcumin is a natural low-molecular-weight polyphenolic compound found in the rhizome of the  
52 perennial herb, turmeric (*Curcuma longa*) (Sharma, Gescher, & Steward, 2005). *Curcuma longa* is  
53 comprised of 3–5% curcuminoids, with the four main types being curcumin (77%),  
54 demethoxycurcumin (17%), bisdemethoxycurcumin (3%), and cyclocurcumin (Goel, Kunnumakkara,  
55 & Aggarwal, 2008; Heger, Golen, Broekgaarden, & Michel, 2014). Curcumin has a molecular weight  
56 of 368.37 g mol<sup>-1</sup> and a melting point of 183 °C (Tapal & Tiku, 2012). In the last few decades, curcumin  
57 has gained significant research attention owing to its wide range of health-promoting properties, such  
58 as anti-inflammatory, anticarcinogenic, and antioxidant activities (Ak & Gülçin, 2008; Fujisawa,  
59 Atsumi, Mariko Ishihara, & Yoshinori Kadoma, 2004; Selvam, Jachak, Thilagavathi, & Chakraborti,  
60 2005). Hence, research has been conducted extensively in recent years to design food-based  
61 encapsulation vehicles that can deliver curcumin effectively in targetted physiological sites.

62 The main challenge in delivering curcumin effectively in human physiology is that curcumin  
63 is a highly lipophilic compound, which limits its absorption in the human body. Besides its poor water  
64 solubility, the relatively high rate of metabolic degradation during physiological transit, inactivity of  
65 the metabolic end-products, and rapid elimination from the body reduce the bioavailability of curcumin  
66 (Bansal, Goel, Aqil, Vadhanam, & Gupta, 2011). To overcome these challenges and to improve the  
67 bioavailability of curcumin upon ingestion, many studies have attempted to encapsulate curcumin using  
68 delivery systems, such as hydrogels (Gong, et al., 2013), nanoparticles (Bisht, et al., 2007), and  
69 liposomes (Hasan, et al., 2014).

70 Particularly, food colloid scientists have shown that emulsions can be facile templates to  
71 encapsulate lipophilic curcumin and improve its stability and bioavailability by manipulating the  
72 bioaccessibility of these colloidal delivery systems. Essentially, two main emulsion-based approaches  
73 have been used to deliver curcumin: emulsion-based delivery systems and excipient emulsion systems.

74 In emulsion-based delivery systems, the isolated curcumin is solubilized first within the oil phase of an  
75 oil-in-water emulsion during the formation of the emulsion. Preliminary evidence has suggested that  
76 emulsion-based delivery systems can be used to encapsulate curcumin to increase its oral  
77 bioaccessibility, permeability, and resistance to metabolic processes during physiological transit (Zhang  
78 & McClements, 2016). On the other hand, in excipient emulsion systems, the curcumin is kept within  
79 its natural environment (used in its original form, such as a powdered spice) and is co-ingested with an  
80 oil-in-water excipient emulsion. Detailed information about excipient emulsion systems that have been  
81 used to deliver curcumin can be found in recent literatures (McClements, et al., 2016; Zhang &  
82 McClements, 2016; Zou, et al., 2015b; Zou, et al., 2016). For excipient emulsion systems the curcumin-  
83 free emulsion needs to be consumed with a curcumin-rich food or food ingredient (Zhang &  
84 McClements, 2016), whereas, for emulsion-based delivery systems, the curcumin-loaded emulsion can  
85 be used as a sole nutraceutical application, the latter has attracted considerable research attention.

86         There has been a strong upsurge in research efforts, in recent years, in delivering curcumin  
87 using emulsions of different sizes, structures and properties, and assessing the ability of these emulsions  
88 to protect curcumin during in vitro oral-to-gastrointestinal digestion. The droplet size distribution and  
89 the microstructure of the emulsions have been tailored to improve the bioaccessibility of curcumin. To  
90 the best of our knowledge, there is no literature source that has systematically reviewed the emulsion-  
91 based delivery systems that have been used for encapsulating curcumin and identified the specific  
92 factors affecting the stability of the encapsulated curcumin pre- and post-ingestion as well as its  
93 bioaccessibility. Such information is crucial in order to exploit emulsion-based approaches to design  
94 next generation curcumin-rich functional foods, functional ingredients and pharmaceutical applications.

95         Hence, the aim of this review is to provide an update of the recent advances in emulsion-based  
96 approaches for the delivery of curcumin. We have specifically focussed on emulsion-based delivery  
97 systems, such as, conventional oil-in-water (O/W) emulsions, Pickering emulsions, and nanoemulsions  
98 stabilized by a surfactant, protein-polysaccharide conjugates and complexes, solid particles that have  
99 specifically been used to encapsulate curcumin. Firstly, we have discussed the structure and  
100 physicochemical properties of curcumin, including research work at our own laboratory, which are key  
101 parameters for selecting the appropriate delivery approach. Specifically, we have discussed the

102 solubility and crystalline structure of curcumin in different solvents in order to enable the optimal  
103 selection of the oils and/or fatty acids, and identified the key challenges encountered in poor  
104 dispersability. Secondly, we have discussed the specific factors in designing the emulsion-based  
105 systems that affect the loading and encapsulation efficiency of curcumin, droplet size change after  
106 curcumin incorporation, and in vitro gastrointestinal stability of the encapsulated curcumin. We have  
107 critically analyzed the release properties and bioaccessibility of curcumin in oral, gastric and intestinal  
108 regimes. Finally, we have highlighted the key research gaps and future trends in the research domain of  
109 delivery and bioaccessibility of curcumin using emulsion-based approaches.

110 The literature search was systematically conducted using three key search engines:  
111 ScienceDirect, PubMed and American Chemistry Society (ACS). In addition, 'Google Scholar' was  
112 also used to search for publications and additional information. Keywords used were 'curcumin',  
113 'curcumin structure', 'curcumin emulsion(s)', 'curcumin nanoemulsion', and 'curcumin Pickering  
114 emulsion'. The initial selection of publications was made on the basis of the title of the publication,  
115 keywords, and abstract screening. Full-text articles were analyzed for inclusion in the review. The  
116 reference list of each paper was carefully checked to identify any relevant previous studies and full-  
117 text screening was conducted for the same.

118

## 119 **2 General aspects of curcumin**

### 120 **2.1 Structure of curcumin**

121 Curcumin is a yellowish powder, with an ordered crystal structure (Rachmawati, Edityaningrum,  
122 & Mauludin, 2013; Zhao, et al., 2015). From a structural viewpoint, curcumin is comprised of two  
123 aromatic rings with methoxyl and hydroxyl groups in the ortho position with respect to each other  
124 (Figure 1). The aromatic rings are connected through seven carbons that contain two  $\alpha,\beta$ -unsaturated  
125 carbonyl groups. As a result, curcumin exists in three possible forms, two isomers in an equilibrating  
126 keto-enol tautomeric form, and a  $\beta$ -diketonic tautomeric form (Payton, Sandusky, & Alworth, 2007).  
127 Under slightly acidic and neutral conditions, the keto-form of curcumin dominates (Jovanovic,  
128 Steenken, Boone, & Simic, 1999). However, when dissolved in ethanol at 70 °C in the dark and in

129 aqueous solutions at pH > 8, curcumin exists primarily in its enolic form; the latter provides its radical-  
130 scavenging ability (Jovanovic, et al., 1999; Kolev, Velcheva, Stamboliyska, & Spiteller, 2005).

131 In crystalline phase, the molecule prefers the enol configuration stabilized by strong  
132 intramolecular hydrogen-bonding (H-bonding) (Tønnesen, Karlsen, & Mostad, 1982). However, as a  
133 result of this intermolecular H-bonding, the molecule loses its planarity (Kolev, et al., 2005).  
134 Polymorphism of crystal structures of curcumin depends on the crystallization conditions. Curcumin  
135 crystals can adopt different shapes, such as monoclinic (acicular), orthorhombic (rice seed like), and  
136 amorphous (Liu, Svärd, Hippen, & Rasmuson, 2015; Mishra, Sanphui, Ramamurty, & Desiraju, 2014;  
137 Sanphui, Goud, Khandavilli, Bhanoth, & Nangia, 2011)

138 Using scanning electron microscopy (SEM), to analyze curcumin particles, in our laboratory has  
139 revealed interesting morphological characteristics, that was dependent on the solvent in which curcumin  
140 was dispersed. Figure 2a presents a SEM image of the curcumin particles dispersed in methanol.  
141 Curcumin showed a long plate-like morphology of around 20-31  $\mu\text{m}$  length and aspect ratio (length-to-  
142 width) varied from 4:1 to 6:1, which is in agreement with previous reports (Kurniawansyah,  
143 Mammucari, & Foster, 2017; Thorat & Dalvi, 2014, 2015). Formation of the repeated stacks of  
144 curcumin plates as observed in Figure 2a has also been described by other authors as an end-to-end  
145 attachment of curcumin particles (Thorat & Dalvi, 2014). This end-to-end attachment creates larger  
146 sized aggregates of the curcumin plates. However, with time, the particles appeared to be more fused  
147 and such stacks were less visible. Figure 2b presents the SEM image of the curcumin crystals dispersed  
148 in dimethyl sulfoxide (DMSO). In DMSO, there appeared to be a shift in aspect ratio to nearly 2:1 to  
149 3:1 with appearance of needle-shaped attachments. The appearance of these acicular structures suggests  
150 an uncontrolled growth of the curcumin particles from dense non-uniform and highly supersaturated  
151 zones in the solution. This uncontrolled nucleation prompted the growth of secondary particles from  
152 the main crystal stem (Kurniawansyah, et al., 2017; Thorat & Dalvi, 2014). In presence of edible oils,  
153 such as sunflower oil, curcumin crystals with dimensions of 13-23  $\mu\text{m}$  (length) and 3-5  $\mu\text{m}$  (width) were  
154 observed (Figure 2c). The particles appeared more fused; possibly caused by a rapid accretion of  
155 primary units into single particles, or by particle growth through the process of molecule-by-molecule

156 bonding (Thorat & Dalvi, 2014). However, the exact mechanism of such crystal fusion remains to be  
157 uncovered.

## 158 **2.2 Solubility of curcumin in solvents**

159 The log P value of curcumin (i.e. the measure of the extent to which a solute preferentially  
160 partitions in octanol over the aqueous phase) has been reported to be 3.29 (PubChem-969516). This  
161 confirms that the curcumin molecule is highly lipophilic with a low intrinsic water solubility (11 ng/mL,  
162 ambient temperature) (Tønnesen, Måsson, & Loftsson, 2002). The hydrophobic nature of curcumin is  
163 given by an aliphatic chain (bridge), which separates the highly polar enolic and phenolic groups  
164 (Balasubramanian, 2006). The bridge is composed of lipophilic methine-rich segments connecting the  
165 polar regions of the molecule (Balasubramanian, 2006; Heger, et al., 2014).

166 Curcumin is highly soluble in polar solvents, such as acetone (7.75 mg/ mL), 2-butanone (2.17  
167 mg/mL), ethanol (5.6 mg/mL), methanol (4.44 mg/mL), 1,2-dichloroethane (0.5125 mg/mL) and  
168 isopropanol (3.93 mg/mL) (Heger, et al., 2014; Khopde, Indira Priyadarsini, Palit, & Mukherjee, 2000).  
169 The DMSO is one of the most commonly used solvents for dispersing curcumin as it can dissolve  
170 curcumin up to a concentration of ~20 mg/mL, an order of magnitude higher as compared to most  
171 alcohols (Khopde, et al., 2000).

172 Authors have reported that in alkaline conditions (> pH 7), curcumin can be dissolved sparsely in  
173 water as the acidic phenolic group in curcumin donates its H<sup>+</sup> ion, forming the phenolate ion enabling  
174 dissolution (Jagannathan, Abraham, & Poddar, 2012; Tønnesen & Karlsen, 1985). However, under  
175 alkaline conditions, curcumin is more susceptible to degradation, partly due to the formation of  
176 phenylated anion; this can increase the production of curcumin radicals. These radicals successively  
177 mediate degradation of the molecule by reacting with other curcumin radicals to form dimeric  
178 catabolites, or by reacting with biomolecules in the cells (Heger, et al., 2014). For in vitro and in vivo  
179 studies, curcumin as a free molecule is commonly dissolved in the least toxic-miscible solvents  
180 according to their lethal 50% dose values (Heger, et al., 2014). Curcumin is also soluble in different  
181 edible oils (Table 1) and such solubility depends on the degree of mixing, temperature-time conditions,  
182 which is discussed in detail in Section 5.

183



### 184 **3 Key challenges of delivery of curcumin**

185 A strong scientific consensus exists that orally administrated curcumin has poor bioavailability  
186 due to the poor solubility and limited absorption from the gut of the latter. The bioavailability of  
187 curcumin is determined by its bioaccessibility; latter defined as the fraction of the quantity of bioactive  
188 initially ingested that is solubilized within the gastrointestinal fluid, in a form that can be absorbed by  
189 the epithelium cells (Fernández-García, Carvajal-Lérida, & Pérez-Gálvez, 2009). Since early 1980's,  
190 substantial research has been conducted with respect to curcumin bioavailability in rat models.  
191 Ravindranath & Chandrasekhara (1980) reported that after oral administration of 400 mg of curcumin  
192 in rats, only a trace amount (less than 5 µg/mL) of curcumin remained in the portal blood during 15 min  
193 to 24 hours. More recently, Sharma, et al. (2004) found that after an oral dose of 3.6 g of curcumin,  
194 maximum curcumin level in plasma was 11.1 nmol/L after an hour of dosing. However, no curcumin  
195 was found in plasma from patients who received a lower dose of curcumin. It has been identified that,  
196 in rat plasma, glucuronide and sulfate are the major products of curcumin biotransformation (Sharma,  
197 et al., 2001). Enzymatic hydrolysis of curcumin through glucuronidase and sulfatase may explain its  
198 efficient metabolism and its poor bioavailability when administered orally (Cheng, et al., 2001; Sharma,  
199 et al., 2001).

200 According to the Nutraceutical Bioavailability Classification Scheme (NuBACS), curcumin is  
201 classified as  $B^*(-)_{L,S} A^*(+) T^*(-)_{C,M}$ . The full classification scheme has been discussed in detail  
202 elsewhere (Zhang & McClements, 2016; Zou, et al., 2015b). Briefly, this suggests that the poor degree  
203 and rate of release of curcumin from the food structure (L) and the poor solubility in the gastrointestinal  
204 fluids (S) are the key factors (-) limiting the bioaccessibility ( $B^*$ ) of curcumin. Furthermore, curcumin  
205 absorption ( $A^*$ ) has no major influence on the bioavailability of curcumin. However, the chemical (C)  
206 or metabolic (M) degradation of curcumin during its gastrointestinal passage remains as the key limiting  
207 factor (-) on the transformation ( $T^*$ ) of curcumin. Hence, it is important to understand how emulsion-  
208 based delivery systems can be designed to address these specific challenges. In this review, we have  
209 only focused on bioaccessibility, which has yielded most of the publications in the last decade.

210

## 211 **4 Emulsion-based delivery systems**

212 Considering the high hydrophobicity of curcumin and our physiology being largely an aqueous-  
213 based system, an oil-in-water (O/W) emulsion-based approach has been the most obvious choice to  
214 deliver curcumin. In the last decade, a wide range of curcumin-encapsulated emulsion-based systems  
215 (Figure 3), such as conventional emulsions stabilized by surfactants, monolayers or multilayers of  
216 biopolymers (proteins, polysaccharides), nanoemulsions and Pickering emulsions, have been designed  
217 to deliver curcumin (Tables 2 and 3).

218 In order to set the scene in terms of encapsulation efficiency, protection, retention, stability  
219 and release of curcumin, we have included an overview of emulsion-based delivery vehicles, focussing  
220 on the design principles, formation and stability of emulsions in the next section..

221

### 222 **4.1 Stability of O/W emulsions**

223 An emulsion consists of small droplets of one liquid dispersed in another immiscible liquid. Typically,  
224 these two immiscible liquids are oil and an aqueous phase (McClements, 2015; Sarkar & Singh, 2016).  
225 Depending on their arrangement, they are usually classified as oil-in-water (O/W) or water-in-oil (W/O)  
226 emulsions. Emulsions are thermodynamically unstable systems due to the large interfacial area between  
227 the two immiscible phases. Emulsions can destabilize over time due to their thermodynamic instability,  
228 causing creaming, sedimentation, flocculation and coalescence of the systems (Dickinson, 2009;  
229 McClements, 2015). Creaming and sedimentation are main forms of gravitational separation. When  
230 two or more droplets come together and aggregate, but retain their individual integrity, droplets are said  
231 to flocculate. Such flocculation might occur due to electrostatic attraction (bridging) or osmotic pressure  
232 effects (depletion). When two or more droplets merge together to form a single large droplet, droplets  
233 are said to coalesce. “Oiling-off” occurs when excessive droplet coalescence happens and a separate  
234 layer of oil is formed on top of the aqueous phase

235

## 236 4.2 Types of emulsion structure

237 **Conventional emulsions.** Conventional emulsions have mean droplet radii in the range of 0.2- 100  
238  $\mu\text{m}$  (Figure 3a). They are thermodynamically unstable systems and tend to be optically turbid or opaque  
239 as they scatter light because of the droplet dimension being similar to the wavelength of light. The  
240 droplet size is mainly determined by the oil phase, as the thickness of the interfacial layer ( $\delta \approx 1-15 \text{ nm}$ )  
241 is much smaller than the radius ( $r$ ) of the oil droplet core ( $\delta \ll r$ ). The interfacial layer is generally  
242 made up of surfactants (e.g. tweens (polyethoxylated sorbitan esters or polysorbates), spans (sorbitan  
243 esters), polyoxyethylene (20) sorbitan monolaurate, monooleate and monopalmitate) or monolayers of  
244 biopolymers (e.g. milk proteins (caseins, whey proteins), plant proteins (pea protein, soy protein), and  
245 polysaccharides, such as gum Arabic). The preparation method for the formation of conventional  
246 emulsions involves using a high shear mixer or two-stage valve homogenizer to homogenize the two  
247 immiscible phases, as illustrated schematically in Figure 3d.

248 **Multilayered emulsions.** A multilayered emulsion consist of emulsion droplets electrostatically  
249 stabilized by layers of alternatively charged emulsifiers (Figure 3b). In recent years, there has been  
250 growing interest in the utilization of the layer-by-layer (LbL) electrostatic deposition method to form  
251 such multilayer emulsion structures. In this method, a charged polyelectrolyte is absorbed through  
252 electrostatic attraction onto an oppositely charged droplet surface. Multiple layers can be formed by  
253 alternating adsorption of oppositely charged polyelectrolytes or charged emulsifiers leading to the  
254 formation of a multilayered structure at the interface (Figure 3e) (Dickinson, 2009; McClements, 2015).

255 **Protein-polysaccharide conjugate-stabilized emulsions.** Proteins and polysaccharides possess  
256 different inherent characteristics (Goh, Sarkar, & Singh, 2008, 2014). Proteins are known to adsorb at  
257 oil/water interface due to their surface-active properties, and polysaccharides are known for their water-  
258 binding, gelling and thickening properties. Covalently linked proteins and polysaccharides via maillard  
259 reaction between the amino groups of protein and reducing sugar groups of the polysaccharide are used  
260 to combine and improve their individual characters and stabilize oil-in-water emulsion with better  
261 kinetic stability (Akhtar & Ding, 2017).

262 **Pickering emulsion.** Pickering emulsions are stabilized by solid particles that are irreversibly  
263 adsorbed to the oil-water interface (Figure 3a) (Aveyard, Binks, & Clint, 2003; Dickinson, 2012, 2017;

264 Pickering, 1907; Ramsden, 1903). These particles at the interface should have an average size at least  
265 10-100 times smaller than the emulsion droplet size in order to achieve effective Pickering stabilization.  
266 The stabilization mechanism for a Pickering emulsion is different from that of a conventional emulsion.  
267 In a conventional emulsion, the interfacial materials (e.g. surfactants, biopolymers) with amphiphilic  
268 properties impart kinetic stability to the droplets by decreasing the interfacial tension and by generating  
269 electrostatic repulsion/ steric hindrance between the droplets.

270 When compared to conventional emulsions, the irreversible absorption of particles creates a  
271 mechanical (steric) barrier in Pickering emulsions that adds long-term physical stability against  
272 coalescence and Ostwald ripening. Solid particles in Pickering emulsion present a partial wettability by  
273 both the oil and water phase. Depending on their degree of wettability in either of the phases and  
274 location at the interface defined by the contact angle of the particle ( $\theta$ ), they can either stabilize O/W  
275 or W/O emulsions (Dickinson, 2009, 2012, 2017). If the contact angle is smaller than  $90^\circ$  ( $\theta < 90^\circ$ ), the  
276 particle will be preferentially wetted by the aqueous phase, favouring the formation of an O/W  
277 emulsion. Pickering emulsions can be prepared in a similar way to that of conventional emulsions  
278 (Figure 3d).

279 Depending on the size of the particles, oil droplets of  $<10\ \mu\text{m}$  diameter can be achieved. However,  
280 in most case, food-grade Pickering emulsions prepared using starch and protein-based microgel  
281 particles have a considerably higher droplet size ( $>10\ \mu\text{m}$ ), as the particles used to stabilize these  
282 droplets are generally sub-micron to micron-sized (Sarkar, et al., 2016a; Yusoff & Murray, 2011). The  
283 concept of Pickering emulsion has been present in different food products since long, such as  
284 homogenized and reconstituted milk (oil-in-water (O/W) emulsions stabilized by casein micelles)  
285 (Dickinson, 2012), it is only recently that there has been an upsurge of research interests to understand  
286 the interfacial properties of particles in O/W emulsions. This is largely due to the laboratory-  
287 manufactured food-grade particles of controlled size being available now, e.g. whey protein microgel,  
288 pea protein microgel, starch, zein, flavonoids etc (de Folter, van Ruijven, & Velikov, 2012; Luo, et al.,  
289 2012; Sarkar, et al., 2016a; Shao & Tang, 2016; Yusoff & Murray, 2011).

290           **Nanoemulsions.** Nanoemulsions have a mean radii between 50 and 200 nm (Figure 4a). They  
291 tend to be transparent or slightly opaque, and have much better stability to aggregation as compared to  
292 that of conventional emulsions due to their very small droplet size. The overall droplet composition is  
293 mainly constituted by the emulsifier layer as the thickness of the emulsifier layer is similar to that of  
294 the radius of the oil droplet ( $\delta = r$ ) (McClements & Rao, 2011). Fabrication methods for nanoemulsions  
295 are typically categorized as either high-intensity or low-intensity and consist of two stages: the pre-  
296 emulsification and emulsification stage. High-intensity methods include use of a high-speed blender,  
297 high-pressure valve homogenizers, microfluidizers and ultrasonic bath or sonicator (Figure 4b)  
298 (McClements & Rao, 2011). These mechanical devices are capable of creating intense disruptive forces  
299 that break up the oil phase into small droplets. The low-intensity methods include phase inversion and  
300 solvent mixing methods (Figure 4c) (Borrin, Georges, Moraes, & Pinho, 2016). In these methods, the  
301 spontaneous formation of tiny oil droplets within the mixed oil–water–emulsifier systems are formed,  
302 when the environmental conditions are altered.

303

## 304 **5 Dispersion of curcumin into the oil phase**

305           Proper dispersion of bioactive compounds into the carrier phase is a key factor for improving the  
306 solubility, dissolution behavior, and administration orally (Zhang & McClements, 2016). Curcumin is  
307 crystalline at ambient temperature and must therefore be dispersed in a suitable carrier before it can be  
308 incorporated into a colloidal delivery system. In an oil-in-water emulsion, the lipid acts as the carrier  
309 phase for lipophilic bioactive components. Table 1 summarizes the solubility values (non-exhaustive)  
310 of curcumin dispersed in different types of edible oils. The dispersion ability of oil is commonly  
311 referred to in the literature, as the ‘loading capacity’ or ‘loading percentage’. The numerical value of  
312 the loading capacity is obtained by calculating the quantity of curcumin dispersed in the oil as a  
313 percentage of the total quantity of curcumin added. The loading capacity of an oil can vary depending  
314 on the molecular weight and polarity of the carrier oil, as well as the physical conditions applied, such  
315 as temperature and times used either in the dispersion or in the incubation process.

316        **Molecular weight and polarity of the carrier oil.** Direct experimental evidence suggests that  
317 quantity of curcumin that can be solubilized in a carrier oil is inversely proportional to the average  
318 molecular weight of the latter (Ahmed, Li, McClements, & Xiao, 2012). For instance, short chain  
319 triglycerides (SCT) have more polar groups (oxygens) per unit mass than long chain triglycerides  
320 (LCT). Hence, SCT present more dipole–dipole interactions between their polar groups and the  
321 curcumin molecules, thereby favoring curcumin solubilization. Also, greater solubilisation is achieved  
322 in SCT compared to LCT due to an excluded volume effect. When curcumin molecules are incorporated  
323 into the oil phase, a depletion zone is formed around curcumin molecules. In this region, the center of  
324 the lipid molecules is excluded, in other words, the lipid concentration is zero. The thickness of the  
325 depletion zone increases with increasing molecular weight of the lipid molecules (Ahmed, et al., 2012).  
326 For example, Joung, et al. (2016) reported that the solubility of curcumin in MCT oil was higher when  
327 compared to coconut oil (LCT:MCT), olive oil (LCT) and corn oil (LCT) (0.25, 0.1, 0.08, 0.07 mg/mL,  
328 respectively) (Table 1). These results were also consistent with a recent study by Ma, et al. (2017a),  
329 who reported that solubility of curcumin in MCT was nearly three times as much as canola oil, and  
330 twice as much as in linseed oil, corn oil and sunflower oil (12.4, 4, 7, 6.2 and 5.4 mg/mL , respectively).

331        **Temperature dependence.** Solubility of curcumin is highly temperature-dependent. When a  
332 crystalline material is fully dissolved, it is said that the material has reached an equilibrium, but above  
333 this level, it will form crystals (supersaturation) (McClements, 2012a). From a theoretical perspective,  
334 increasing the temperature increases the average kinetic energy of both, the solution and the crystalline  
335 molecules. This increase in kinetic energy destabilizes the solid state of the solute (less able to hold  
336 together) and allows the solvent to break apart the solute molecules more effectively and dissolving it  
337 more rapidly.

338        To characterize the temperature dependence of the dissolution of crystalline curcumin in oil, the  
339 common method used is to determine the reduction in magnitude of turbidity of the oil using a UV-Vis  
340 spectrophotometer. For instance, Zou, Liu, Liu, Xiao, & McClements (2015a) observed that the  
341 turbidity of curcumin in corn oil mixtures (LCT) decreased appreciably upon heating from 25 to 100  
342 °C. At a concentration of 3 mg/mL, the turbidity almost reached a value close to zero at 100 °C  
343 indicating that the crystals were fully dissolved at this temperature (Table 3-1). Interestingly, upon

344 cooling, turbidity of the oil was low indicating that the curcumin still remained dissolved within the oil.  
345 This might be attributed to either curcumin being below its saturation temperature even at 25 °C, or the  
346 curcumin concentration did not exceed the supersaturation level to form curcumin crystals  
347 (McClements, 2012a). At 4 mg/mL, the turbidity also decreased as the temperature was increased.  
348 Nonetheless, the final turbidity at 100 °C was considerably greater than that observed for the sample  
349 containing 3 mg/mL curcumin, which implies that excess curcumin crystals had not dissolved  
350 completely. When samples were cooled, the turbidity remained high and even increased slightly, which  
351 further highlights that the solubility of curcumin decreased with decreasing temperature, as well as the  
352 amount of curcumin present was above the saturation level.

353 Similarly, Ma, et al. (2017b) observed increased curcumin concentrations in MCT oil when using  
354 a boiling bath for 3 min as compared to that of ultrasonic (390 W, one second interval for 30 min) and  
355 microwave treatments (780 W, 30 sec). Also, Abbas, Bashari, Akhtar, Li, & Zhang (2014) reported that  
356 a curcumin concentration of  $\leq 6$  mg/mL was successfully dissolved in MCT oil at 100 °C, without a  
357 noticeable sedimentation during one month storage period when incorporated into a nanoemulsion.  
358 However, prolonged heat exposure during solubilization of curcumin in the oil phase can cause  
359 decomposition of curcumin. In fact, Wang, Liu, Xu, Yin, & Yao (2016) reported 10% of curcumin  
360 decomposition after a heat treatment at 90 °C for 1 hour in the dark.

361 **Time dependence.** Dissolution rate of curcumin depends on the nature of the crystals (e.g.  
362 surface area, crystallinity, morphology, structure), the nature of the solvent (e.g. polarity), and the  
363 physical conditions applied (e.g. stirring speed, temperature and sonication) (McClements, 2012a)  
364 (Table 1). Soluble curcumin concentration values varied significantly for soybean oil when mixed for  
365 48 h (ambient temperature) (7380  $\mu\text{g/mL}$ ) (Setthacheewakul, Mahattanadul, Phadoongsombut,  
366 Pichayakorn, & Wiwattanapatapee, 2010) as compared to that for 10 min (0.1834  $\mu\text{g/mL}$ ) (Lin, Lin,  
367 Chen, Yu, & Lee, 2009). In MCT oil, a soluble curcumin concentration range of 7.50 - 250  $\mu\text{g/mL}$  has  
368 been reported when mixed at 60 °C for 10 min, with subsequent 20 min of sonication (Ahmed, et al.,  
369 2012; Joung, et al., 2016). Overall, the results suggest that solubility of curcumin depends on the nature  
370 of the oil, the curcumin-oil interactions, and the processing conditions (temperature, agitation time);  
371 such factors are critical for the maximum incorporation of curcumin into the oil phase. Various studies

372 have shown that a higher curcumin concentration is generally favored by MCT oil when high  
373 temperatures ( $\geq 60^\circ\text{C}$ ) and appropriate agitation times (10 - 30 min) are applied.

374

## 375 **6 Physicochemical stability of curcumin-loaded emulsion systems**

376 Tables 2 and 3 summarize a non-exhaustive list of the emulsion-based approaches used for  
377 delivering curcumin, such as nanoemulsions and macroemulsions stabilized by surfactants, protein-  
378 polysaccharide conjugates, and Pickering particles respectively. In this Section, we reviewed various  
379 factors that can influence the retention capacity of curcumin, the effect of curcumin incorporation on  
380 the droplet size distribution of emulsions and the structural characteristics that promote retention of  
381 curcumin during storage and in vitro release.

382

### 383 **6.1 Loading efficiency**

384 In literature, the terms, such as “yield”, “encapsulation efficiency”, “incorporation efficiency”  
385 and “loading efficiency” have often been used interchangeably for emulsion-based encapsulation  
386 systems. In each case, it essentially refers to the entrapment capacity of an emulsion system.  
387 Quantitative information is obtained by measuring the mass of curcumin entrapped into the delivery  
388 system as a percentage of the total curcumin added (McClements, Decker, Park, & Weiss, 2009). Since  
389 curcumin is required in high concentrations to show therapeutic benefits, one of the prerequisites in the  
390 delivery research is high entrapment of bioactive molecules. The loading efficiency of emulsions is  
391 highly dependent on the type of emulsifier and its structural arrangements at the interface.

392 **Curcumin-surfactant interactions.** Curcumin molecules contain mainly hydrophobic but also  
393 some hydrophilic groups that can directly interact with surfactant molecules mainly via hydrophobic  
394 and electrostatic interaction, respectively (Yu & Huang, 2010). It has been reported that the enolic and  
395 phenolic groups of curcumin underwent electrostatic interactions with positively charged head group  
396 of cationic-nonionic surfactant micelles mixtures (e.g. Dodecylethyldimethylammonium bromide  
397 (DDAB), Polyoxyethylene 10 oleyl ether, Tyloxapol, Polysorbate 80), while the methylene rich chain  
398 of curcumin interacted with the hydrophobic part of the surfactant micelles mixture (Kumar, Kaur,



399 Kansal, Chaudhary, & Mehta, 2016). The authors revealed using transmission electron microscopy  
400 (TEM) that curcumin was not located within the core of the surfactant micelles, but was rather  
401 interacting with the polar part of the surfactants (head group). This suggests that in emulsions stabilized  
402 by mixed surfactant systems, both hydrophilic and hydrophobic parts of the surfactants might contribute  
403 to the solubilisation of curcumin. Such favorable microenvironment mediated by the surfactant systems  
404 might enable enhancing the solubilisation of curcumin molecules inside the emulsions leading to a high  
405 loading efficiency. For example, when 15 mg of curcumin was added in nanoemulsions stabilized by  
406 optimized mixtures of hydrogenated L- $\alpha$ -phosphatidylcholine (HEPC) (surfactant) and  
407 Polyoxyethylene hydrogenated castor oil 60 (HCO-60) (co-surfactant) or HEPC and Tween 80, loading  
408 efficiencies of 100% or ~97%, respectively, were obtained (Anuchapreeda, Fukumori, Okonogi, &  
409 Ichikawa, 2012a).

410 **Curcumin-protein interactions.** Sodium caseinate, a mixture of  $\alpha_{s1}$ -,  $\alpha_{s2}$ - and  $\beta$ - caseins and  $\kappa$ -  
411 casein is commonly used to stabilize oil droplets (Sarkar & Singh, 2016). The  $\alpha_{s1}$ -,  $\alpha_{s2}$ - and  $\beta$ - caseins  
412 are phosphoproteins and are more hydrophobic than  $\kappa$ -casein. This is because  $\alpha_{s1}$ -casein contains two  
413 tryptophan residues at positions 164 and 199, whereas  $\kappa$ -casein has one tryptophan residue at position  
414 143 (Liu & Guo, 2008). It is highly likely that when sodium caseinate-stabilized emulsions are used to  
415 encapsulate curcumin, any or all of these tryptophan (hydrophobic) residues directed towards the oil  
416 phase could bind to curcumin molecules through hydrophobic interactions and contribute to increasing  
417 the loading efficiency of an emulsion (Pan, Zhong, & Baek, 2013). For example, Rao & Khanum (2016)  
418 observed a considerable increase in the loading efficiency when the sodium caseinate concentration was  
419 increased from 2.5% (89.6%) to 10% (92.3%) in nanoemulsions at a constant curcumin-milk fat ratio  
420 of 1:0.05% (w/w) (Table 2).

421 **Curcumin-polysaccharides interactions.** Curcumin-polysaccharide interactions can also affect  
422 the loading efficiency. Recently, Li, Hwang, Chen, & Park (2016) have investigated the influence of  
423 chitosan multilayer on the physicochemical properties of curcumin-loaded nanoemulsions. The loading  
424 efficiency was found to be 95.1% when a curcumin concentration of 0.548 mg/mL was used. This was  
425 presumably due to the interactions between keto groups of curcumin in either the diketo or the cis-enol  
426 form, and the amine groups of chitosan (Anitha, et al., 2011). Chitosan, which is rich in protonated

427 amino groups possibly facilitated the electrostatic interaction between the cationic groups located on  
428 the polyglucosamine chains of the molecule and the negatively charged anionic curcumin. In addition,  
429 at physiological pH (7.4) conditions, the hydrophobic interactions of curcumin with chitosan was  
430 reported to be more pronounced in the presence of nonionic surfactant (Tween 80) than in the presence  
431 of cationic surfactants, such as, cetyl trimethyl ammonium bromide (CTAB). In Tween 80 systems, the  
432 binding process was hypothesized to be driven by hydrophobic, electrostatic and hydrogen bond  
433 formation between curcumin and chitosan (Boruah, Saikia, & Dutta, 2012).

434 **Interfacial structure.** The development of a protein-polysaccharide conjugate has been reported  
435 to act as a physical barrier that prevents the diffusion of loaded curcumin into the aqueous phase (Qi,  
436 Huang, He, & Yao, 2013; Wang, et al., 2016). Often, one or more co-solvents or surfactants are added  
437 to the formulation to assist the solubilisation of high concentrations of curcumin in the system. For  
438 example, Wang, et al. (2016) investigated protein-polysaccharide conjugates-stabilized emulsions that  
439 are suitable for delivery of curcumin (Table 3). They used a combination of MCT oil with a co-solvent  
440 ethanol (90:10 (v/v) to prepared bovine serum albumin and dextran conjugate (BSA-dextran)-stabilized  
441 emulsion, the conjugate was formed between the e-amino group in BSA and the reducing-end carbonyl  
442 group in the dextran. It was observed that the conjugates form a BSA film at the oil/water interface with  
443 the dextran shell, the latter acted as a steric barrier retaining the loaded curcumin by preventing its  
444 diffusion into the aqueous phase, latter would have been facilitated by the carrier-acting ethanol  
445 otherwise. At BSA concentration of 15 mg/mL in the aqueous phase, the curcumin loading efficiency  
446 was higher than 99% (Qi, et al., 2013; Wang, et al., 2016). Xu, Wang, & Yao (2017) used a similar oil  
447 mixture (90% MCT and 10% ethanol (v/v)) and observed similar behaviour for casein-soy soluble  
448 polysaccharide (CN/SSPS) conjugate-stabilized emulsions at pH 3-4.5, at this pH the protein and the  
449 polysaccharide carried opposite charges forming a rather integrated interfacial film via electrostatic  
450 interactions (Table 3). About 99.9% of curcumin was encapsulated in the droplets (Xu, et al., 2017).

451 Irreversible adsorption of individual particles in Pickering emulsion forms a porous interfacial  
452 layer (pores referring to space between the stabilizing particles at the interface) that may reduce the  
453 curcumin content by facilitating the diffusion of oxidation initiators into the oil droplets, latter may  
454 promote oxidative degradation/ modification or alkalyne hydrolysis of curcumin (Tønnesen, Karlsen,

455 & van Henegouwen, 1986; Tønnesen, et al., 2002). Previously, it has been estimated that the gaps  
456 between particles in a whey protein microgel-stabilized emulsion is ~110 nm for microgel particles of  
457 size  $d_0 = 300$  nm (Sarkar, et al., 2016a). However, such gap dimension can effectively be controlled by  
458 fusing the particles together forming a discrete layer or using smaller-sized particles. This was  
459 successfully shown in emulsions stabilized by smaller-sized kafirin particles (size range of 92–434 nm),  
460 where a loading efficiency of ~90% was achieved because of the reduced gap dimension, latter limited  
461 the degradation of curcumin (Table 3). In another study, emulsions stabilized by non-heated (NHT)  
462 octenyl succinate (OSA) modified quinoa starch granules (2  $\mu$ m) had a relatively low loading efficiency  
463 of curcumin (~ 80%) due to potential diffusion of oxidation initiators through the larger gaps in between  
464 the particles (Marefati, Bertrand, Sjöö, Dejmek, & Rayner, 2017; Xiao, Li, & Huang, 2015; Xiao,  
465 Wang, Gonzalez, & Huang, 2016) (Table 3). Interestingly, a thermal treatment of OSA modified starch  
466 granule-stabilized emulsions had created a rather fused layer of partially gelatinized starch granules,  
467 reducing the gaps between particles and favouring a higher protection of curcumin in undegraded form  
468 within the system.

469

## 470 **6.2 Droplet size of curcumin-loaded emulsions**

471 In theory, incorporation of curcumin should not alter the droplet size of a system if emulsion  
472 droplets are in the order of few microns (McClements & Li, 2010). Curcumin crystal size and emulsifier  
473 concentration can influence the extent of increase of droplet size after curcumin incorporation,  
474 particularly relevant in the case of nanoemulsions.

475 **Curcumin crystal size.** Nanoemulsion droplets usually have a mean diameter between 50 and  
476 200 nm. Hence, it is highly likely that under specific dispersion conditions (e.g. temperature), curcumin  
477 crystal growth could interfere with the droplet size of the nanoemulsions. This clearly limits the amount  
478 of curcumin that can be successfully incorporated within the nanoemulsion droplets, since the concentration  
479 should always remain below the saturation limit (McClements & Rao, 2011). For instance,  
480 incorporation of curcumin into surfactant-stabilized nanoemulsions has been reported to increase the  
481 average droplet size of the emulsion, thereby destabilizing the system. Borrin, et al. (2016) observed  
482 that encapsulating 0.1% curcumin into nanoemulsion stabilized by Tween 80 caused a statistically

483 significant increase in the hydrodynamic diameter from 200 to 270 nm, after 60 days of storage.  
484 However, the increase was not observed in nanoemulsions containing less curcumin (0.03-0.07%).  
485 (Table 2). Similar findings were reported by Anuchapreeda, et al. (2012a) where increasing the amount  
486 of curcumin from 15 to 240 mg increased the mean hydrodynamic diameter of nanoemulsion from 48  
487 to 78 nm.

488 On the contrary, in conventional emulsions and emulsions stabilized by protein-polysaccharide  
489 complex as well as edible Pickering particle-stabilized emulsions (Table 3), the size of curcumin  
490 crystals remains comparatively smaller (10 - 1000 times) as compared to that of the emulsion droplets.  
491 Hence, in these systems no significant change in the emulsion droplet size distribution occurs after  
492 curcumin encapsulation (Marefati, et al., 2017; Shah, et al., 2016a; Wang, et al., 2016; Xu, et al., 2017).  
493 Thus, changes in the droplet size after curcumin incorporation is mainly a phenomenon in nanometer-  
494 sized emulsions. Bioactive components are required in high concentrations to show therapeutic benefits;  
495 therefore, the quantity of curcumin that can be incorporated into nanoemulsions without altering the droplet  
496 size can be a potential limiting factor. Furthermore, protein-polysaccharide conjugates/complexes,  
497 Pickering emulsion systems with a larger droplet size appear to be rather less sensitive to such alteration  
498 in droplet size after curcumin incorporation.

499

## 500 **7 In vitro gastrointestinal stability and bioaccessibility of curcumin-** 501 **loaded emulsions**

502 An important parameter for characterizing the effectiveness of a delivery system is the protection  
503 of the encapsulated material until it reaches the targeted location. For curcumin, oxidative degradation/  
504 modification that are mediated by reactive oxygen species (ROS), such as, hydroxyl radical ( $\bullet\text{OH}$ ),  
505 superoxide anion ( $\text{O}_2^{\bullet-}$ ), peroxy radicals and alkaline hydrolysis are the two major challenges  
506 encountered in in vitro stability studies that hinder the use of curcumin as a pharmaceutical (Wang, et  
507 al., 1997). The most common pharmaceutical approach to assess in vitro degradation and release of  
508 curcumin from emulsion based systems involves addition of a buffer solution at different pH, or  
509 phosphate buffer containing cosolvents, such as, ethanol/methanol, salts (e.g.  $\text{CaCl}_2$ ) and in some cases

510 bile salts in a dialysis bag (e.g. 3,500-8,000 Da) subjected to mechanical forces (e.g. shaking, stirring)  
511 at temperature in the range of 22-37 °C. In these pharmaceutical approaches, the degradation of  
512 curcumin under various pH conditions are investigated. In other cases, release of curcumin is facilitated  
513 by the use of polar solvents mixed with the buffer solution, here, the quantity of curcumin released from  
514 the emulsion to the buffer containing ethanol/ methanol is generally expressed as the percentage of the  
515 original curcumin encapsulated within the emulsion systems. However, for in vitro digestion models  
516 used by food scientists, this “release” term can be misleading as no such cosolvents are employed. In  
517 these studies, curcumin can only be released from an emulsion as part of an oil phase i.e. within the free  
518 fatty acids (FFAs), mono and/or diacylglycerols released during lipid digestion in the intestinal phase.  
519 Since pH change is a crucial parameter in in vitro gastrointestinal models and curcumin degradation is  
520 highly dependent on pH conditions, in vitro digestion results can be better interpreted in terms of  
521 degradation of curcumin rather than release, latter is only relevant when discussing the curcumin release  
522 along with the lipid digestion products as indicated above.

### 523 **7.1 In vitro storage stability and release**

524 Encapsulation of curcumin in Pickering emulsions have shown to significantly improve the storage  
525 stability of curcumin. For example, Tikekar, Pan, & Nitin (2013) assessed the storage stability  
526 comparing the rate of curcumin degradation between curcumin solubilized in a buffer solution (3%  
527 (v/v) methanol) at pH 5.7, and curcumin encapsulated in silica-stabilized Pickering emulsions at pH  
528 6.5. When incorporated into a Pickering emulsion system the time required for 50% reduction in  
529 curcumin concentration (half-life) was approximately 87 hours, compared to 50 minutes observed for  
530 free curcumin (Table 3). Considering that the stability of curcumin decreases in buffered systems at  
531 neutral to alkaline pH conditions (Wang, et al., 1997), these results show that encapsulation of curcumin  
532 in Pickering emulsion significantly improved the storage stability of curcumin.

533 Unfortunately, the non-biodegradable and non-digestible character of silica has limited its  
534 application as delivery systems; increasing the interest in food-based particles, such as protein-based,  
535 and carbohydrate-based particles as Pickering emulsion stabilizers (Sarkar, et al., 2016a; Yusoff &  
536 Murray, 2011). Chitosan-tripolyphosphate nanoparticles (CS-TPP-NPs) have been recently used due to

537 its non-toxic (solvent free) and easy formation technique through ionic gelation process (Table 3). The  
538 CS-TPP nanoparticles were formed by cross-linking the primary positively charged amino groups of  
539 CS with the polyanion TPP, which is negatively charged. Shah, et al. (2016a) observed that the  
540 curcumin degradation was ~14 wt% after 24 hours storage in the dark (22°C) for CS-TPP-NPs  
541 emulsions prepared with 5 and 20 wt% MCT oil. The half-life (50 wt%) of curcumin was more than  
542 120 hours.

543 Additionally, during an in vitro release model consisting of phosphate buffer containing ethanol  
544 (15% v/v) at acidic conditions (pH 2), which relates to gastric conditions, the release of curcumin from  
545 CS-TPP-stabilized Pickering emulsion after 24 and 96 hours was 56% and 82%, respectively. In almost  
546 neutral conditions (pH 7.4), which relates to blood fluid, 37% and 74% of curcumin was released within  
547 the same time interval. This lower curcumin retention, under acidic conditions, was also reported by  
548 Kakkar, Singh, Singla, & Kaur (2011) for curcumin-loaded solid lipid nanoparticles, and attributed to  
549 the increase of solubility of curcuminoids under acidic conditions previously discussed in section 2.1.  
550 Compared to silica-stabilized Pickering emulsions, curcumin storage stability was higher in Pickering  
551 emulsions stabilised with CS-TPP-NPs (Table 3).

552

## 553 **7.2 In vitro gastrointestinal stability of curcumin**

554 In vitro digestion models are commonly used to study the stability and digestibility of encapsulated  
555 bioactive compounds in different parts of the gastrointestinal tract (GIT) (Laguna, Picouet, Guàrdia,  
556 Renard, & Sarkar, 2017; Minekus, et al., 2014; Sarkar, Goh, & Singh, 2010a; Sarkar, Goh, Singh, &  
557 Singh, 2009b; Sarkar, Horne, & Singh, 2010b, 2010c; Sarkar, et al., 2016a; Sarkar, Ye, & Singh, 2016b;  
558 Singh & Sarkar, 2011). Simulated gastric fluids (SGF) involve the addition of salts (e.g. NaCl), acids  
559 (e.g. HCl) and digestive enzymes (e.g. pepsin) at a highly acidic pH value (e.g. 1.2- 4) for a fixed period  
560 of time (e.g. 2 hours) at a body temperature of 37 °C. Simulated intestinal fluids (SIF) involve the  
561 addition of bile salts (or bile extract), pancreatin (trypsin, amylase, lipase) and salts (e.g. CaCl<sub>2</sub>, NaCl,  
562 KH<sub>2</sub>PO<sub>4</sub>), at around neutral to alkaline pH values (e.g. 6.5–7.5) for a fixed period of time (e.g. 2- 3  
563 hours) at a body temperature of 37 °C. In some digestion models, an initial oral stage is also included,

564 which contains salts, glycoproteins (e.g. mucin) and  $\alpha$ -amylase, around a neutral pH value for a fixed  
565 period of time (e.g. 5- 10 min.) at a body temperature of 37 °C (Sarkar, Goh, & Singh, 2009a; Sarkar &  
566 Singh, 2012; Sarkar, Ye, & Singh, 2017a).

567 **Proteolysis and/or displacement of interfacial materials.** The structural conformations of  
568 proteins determines the ability of pepsin to hydrolyse the proteins. Native  $\beta$ -lactoglobulin has been  
569 reported to be resistant to pepsin breakdown in simulated gastric digestion due to its compact globular  
570 structure (Fu, Abbott, & Hatzos, 2002; Sarkar, et al., 2010a; Sarkar, et al., 2009b; Scanff, et al., 1990;  
571 Singh & Sarkar, 2011). However, when present at the interface, it can be hydrolysed by gastric and  
572 pancreatic enzymes (Sarkar, et al., 2009b; Sarkar, Zhang, Murray, Russell, & Boxal, 2017b). This is  
573 particularly important for protein-based particle stabilized interfaces, such as whey protein microgel,  
574 kafirin and bovine serum albumin. Kafirin's structure comprises of an  $\alpha$ -helix and  $\beta$ -sheet secondary  
575 structure, and exhibits extensive disulphide-induced cross-linking (Belton, Delgadillo, Halford, &  
576 Shewry, 2006). Xiao, Wang, Perez Gonzalez, & Huang (2016) observed that under gastric digestion,  
577 without the addition of pepsin, curcumin loaded kafirin-stabilised Pickering emulsions (KPE) suffered  
578 less droplet coalescence after 30 min of digestion as compared to that in the presence of pepsin (Table  
579 3). With the addition of pepsin to the SGF, KPE showed coalescence with the appearance of larger  
580 droplets within 30 min. At the end of the gastric treatment (1 hour), the majority of the oil droplets lost  
581 their integrity and macro-scale phase separation occurred.

582 Protein-stabilized interfaces are highly responsive to intestinal conditions. Bile salt, a bio-surfactant  
583 in intestinal fluids can competitively displace the  $\beta$ -lactoglobulin protein from the droplet interface  
584 (Sarkar, et al., 2010b; Sarkar, et al., 2016a; Sarkar, et al., 2016b), thereby favouring lipase activity and  
585 degradation of curcumin through exposure to ROS such as hydroxyl radical. For example, Sari, et al.  
586 (2015) reported that curcumin nanoemulsions, stabilized by whey protein concentrate (WPC) and  
587 composed of 50-60%  $\beta$ -lactoglobulin, were stable to gastric digestion (2 hours) with 90% of the  
588 encapsulated curcumin stable in the nanoemulsion (Table 2). However, during intestinal digestion 77%  
589 of the curcumin was degraded, attributed to the destabilization of the emulsions after 2 hours of  
590 incubation in the intestinal phase.

591 **Barrier properties of interfacial materials.** When treated under specific thermal conditions,

592 Pickering particle-based interface can provide a certain degree of barrier to the access of bile salts or  
593 lipase to the oil-water interface. For example, in case of Pickering emulsions stabilized by gelatinised  
594 starch (Marefati, et al., 2017) or whey protein microgel (Sarkar, et al., 2016a), a thermal treatment was  
595 necessary for the formation of a fused barrier layer of connected particles at the interface (as discussed  
596 in Section 6) and might restrict the penetration of bile salts and/or enzymes. For example, Marefati, et  
597 al. (2017) reported higher curcumin stability after 60 min of oral (~95%) and 2 hours of intestinal  
598 (~86%) digestion for heated Pickering-stabilized emulsions (HT) stabilized with OSA-treated quinoa  
599 starch granules, as compared to that of the non-heated samples (NHT) (~70% and ~40%, respectively)  
600 (Figure 3). However, no statistically significant difference between these samples was seen after 120  
601 min of gastric digestion (Table 5a) (~82% for HT and ~86% NHT). This suggests that a fused layer of  
602 starch granules was significantly effective as a barrier layer against amylase attack (oral and intestinal  
603 regimes) as compared to that of intact starch granules, by reducing the gap dimensions. A recent study  
604 has shown that gastric destabilization of protein stabilized interfaces can be hindered by binding a  
605 secondary layer of oppositely charged polysaccharide-based particles, such as cellulose nanocrystals  
606 (Sarkar, et al., 2017b). As cellulose nanocrystals are not digested by pepsin and provide a high surface  
607 viscosity, they provide a strong barrier to the pepsin attacking the whey protein at the droplet surface  
608 (Sarkar, et al., 2017b). However, use of such secondary layer of particles in a proteinaceous particle-  
609 stabilized interface and role of such secondary layer of particles at interface in protecting curcumin in  
610 the entire gastrointestinal regime is yet to be explored in literature.

611 Through the implementation of in vitro digestion models, it has been demonstrated that,  
612 curcumin degradation is higher during simulated intestinal digestion or neutral pH than in simulated  
613 gastric digestion, regardless of the emulsion-based approach. Emulsions stabilized by ionic surfactants,  
614 proteins and electrostatically charged protein-polysaccharide multilayered complexes are highly  
615 sensitive to any pH and ionic strength alterations, which are essentially abundant in physiology. In in  
616 vitro digestion regimes, Pickering particles appear to be more capable to protect curcumin from  
617 degradation in emulsions than that of the low molecular weight emulsifiers/ protein owing to the strong  
618 adsorption of the particles to the oil-water interface and not being displaced by 'bio-surfactant' bile  
619 salts (Sarkar, et al., 2016a). The effective formulation of emulsion systems exhibiting a mass transport



620 barrier to enzyme attack, stability to changes in pH and delayed act of bile salts and lipid-lipase  
621 interactions through the establishment of a protective fused interface enclosing the droplet can be an  
622 effective strategy to encapsulate curcumin (Marefati, et al., 2017).

623

### 624 **7.3 Bioaccessibility of curcumin-loaded emulsions**

625 Oil droplets are composed of digestible lipids such as triacylglycerols and they generate free fatty  
626 acids (FFAs) and monoacylglycerols (MAGs) upon digestion. Mixed micelles are formed by the  
627 interactions of these FFAs and MAGs that are released from the oil droplets, phospholipids, bile salts,  
628 and cholesterol (Devraj, et al., 2013). These mixed micelles have non-polar domains capable of  
629 solubilizing hydrophobic bioactive compounds, and certain types of micelles are small enough to  
630 transport the bioactives through the mucus layer to the epithelium cells where they are absorbed (Zhang  
631 and McClements, 2016). In particular, bioaccessibility of curcumin is influenced by many factors,  
632 including oil composition, droplet size and curcumin-emulsifier interactions.

633 **Oil composition.** Various studies have revealed that the bioaccessibility of curcumin is clearly  
634 dependent on the type and amount of carrier lipid. Ahmed, et al. (2012) observed that the  
635 bioaccessibility of curcumin in  $\beta$ -lactoglobulin-stabilized nanoemulsions increased substantially when  
636 the carrier lipid was composed of medium-chain triacylglycerols (MCT) or long-chain triacylglycerols  
637 (LCT) due to their ability to form mixed micelles (~41% for LCT and ~58% for MCT oil at a lipid  
638 concentration of 2 wt%) (Table 3). The authors also reported higher curcumin bioaccessibility values  
639 when the total lipid concentration of MCT oil was increased because more mixed micelles were formed  
640 to solubilise the curcumin (~8% at 1% lipid concentration and ~58% at 2% lipid concentration).  
641 However, for LCT oil, the bioaccessibility was similar with increased lipid content because a greater  
642 fraction of lipid phase was not digested, this means that some of the curcumin was not solubilised from  
643 the droplets into the surrounding micellar phase (~20% at 1% lipid concentration, ~40% at 1.5% lipid  
644 concentration and ~41% at 2% lipid concentration) (Table 3).

645 Conversely, other authors have reported that micelles are more likely to be formed by LCT than  
646 for MCT fatty acids. Medium chain triglycerides form a mixed micellar phase that contains hydrophobic  
647 domains that could not be large enough to accommodate large hydrophobic bioactive molecules such

648 as curcumin (Zou, et al., 2016). For example, Shah, Zhang, Li, & Li (2016b) deliberately prepared  
649 chitosan-tripolyphosphate nanoparticle-stabilized Pickering emulsions (PMCT, PLCT) and  
650 nanoemulsions stabilized by non-ionic surfactants (Span 80: Tween 80) (NEMCT, NELCT). A  
651 significant difference in curcumin bioaccessibility was reported when using MCT and corn oil (LCT)  
652 as the carrier lipids (Tables 2 and 3). The bioaccessibility was ~32% for NEMCT; ~65% for NELCT  
653 against 21% for PMCT and 53% for PLCT.

654 **Droplet size.** Emulsions with a smaller droplet size have higher lipid/water surface area to  
655 volume ratio that may result in higher degree of lipolysis (Armand, et al., 1999). Under physiological  
656 conditions, lipases are in excess relative to the quantity of oil droplets, hence a larger lipid/water  
657 interface will allow the anchoring of more lipase molecules to the oil/water interface (Armand, et al.,  
658 1999). For example, Pinheiro, et al. (2013) reported nearly 10-fold increase in curcumin bioaccessibility  
659 during sequential digestion (initial, stomach, duodenum, jejunum, ileum) for nanoemulsions stabilized  
660 by Tween 20 (e.g. ~15% in ileum) when compared with nanoemulsions stabilized by  
661 dodecyltrimethylammonium bromide (DTAB) (e.g. ~1.5% in ileum) (Table 3). This increased  
662 bioaccessibility for Tween 20 nanoemulsions correlated well with the reduced size of the emulsion  
663 droplet that was present throughout the simulated digestion (~100-310 nm), especially during  
664 duodenum, jejunum and ileum phases as compared to that of the size of DTAB nanoemulsions (~80 –  
665 890 nm) (Table 2). Increasing the concentration of surfactants in nanoemulsions can decrease the  
666 emulsion droplet size (McClements, 2012b) and consequently the degree of lipid digestion. On the other  
667 hand, studies have found that increasing the surfactant concentration can also result in barrier effect that  
668 could also hinder the amount of FFA released (Joung, et al., 2016). This suggests that the amount of  
669 surfactant concentration in curcumin nanoemulsions affects the FFA release and the size of the  
670 emulsion droplets (the lipid/water interfacial area), which is a key physicochemical factor in curcumin  
671 bioaccessibility. Other studies comparing the bioaccessibility of curcumin in  $\beta$ -lactoglobulin-stabilized  
672 conventional and nanoemulsions observed that the bioaccessibility of curcumin was fairly similar for  
673 both samples, with 58% for nanoemulsions, and 59% for conventional emulsions (Ahmed, et al., 2012)  
674 (Table 3). Hence, it appears that there is no consensus in findings so far on advantages of using  
675 nanoemulsions over conventional emulsions to encapsulate curcumin from bioaccessibility stand point.

676 **Curcumin-emulsifier interactions.** Some multilayer-stabilized nanoemulsions studies have  
677 shown that curcumin in these systems had relatively low total curcumin bioaccessibility, potentially  
678 due to emulsifier-curcumin interactions (Pinheiro, Coimbra, & Vicente, 2016). For example,  
679 nanoemulsions stabilized by lactoferrin (L-NE) and lactoferrin/alginate (L/A-NE) multilayer structure  
680 have shown relatively low curcumin bioaccessibility of around ~2.5- 3.1% in jejunum and ileum. These  
681 results may be explained by the fact that curcumin may have been bound to the lactoferrin molecules  
682 or digestion products of lactoferrin after lipid hydrolysis, hence curcumin was not detected in the  
683 micellar phase (Tokle, Mao, & McClements, 2013). Similarly, it has been suggested that cationic  
684 polymers may electrostatically inhibit lipase and bile salt action during lipolysis in the small intestine,  
685 decreasing the bioaccessibility of lipophilic compounds (Kido, et al., 2003). However, experiments with  
686 chitosan-coated nanoemulsions stabilized by Tween 80 have suggested that chitosan coating had a very  
687 limited effect on the bioaccessibility of curcumin despite the possible interactions between curcumin  
688 and the amine groups of chitosan (Li, et al., 2016). Hence, further studies using standardized in vitro  
689 digestion protocol is needed to arrive at a clear consensus on the influence of droplet size and emulsifier  
690 charge on curcumin bioaccessibility.

## 691 **8 Conclusions and Future Outlook**

692 Oil-in-water emulsions have been used as delivery systems for encapsulating and orally  
693 administering curcumin. The key factors affecting the stability, release, and bioaccessibility of  
694 curcumin in various emulsion-based systems are emulsion droplet size, oil composition and volume  
695 fraction, dispersion conditions of curcumin in the oil phase/oil type and structure/density/ type of  
696 interface and susceptibility of the interface to physiological breakdown. These factors may act either  
697 individually or synergistically.

698 Extensive studies have been performed to optimize and design effective nanoemulsion systems  
699 with improved physicochemical stability, release and bioaccessibility. Emulsions with smaller particle  
700 size tend to have better kinetic stability than that of conventional emulsions. Nevertheless, higher  
701 emulsifier concentrations are needed to produce smaller droplet size and some surfactants are allowed  
702 at significantly low levels. Furthermore, the size of the nanoemulsions seems to be altered on

703 incorporation of micron-sized curcumin crystals. There are some evidences that nanoemulsions might  
704 result in higher degree of lipid digestion products by virtue of their high interfacial area and thus, form  
705 of higher quantities of mixed micelles. However, there is still debate on specific advantage from the  
706 bioaccessibility point of view, in using nanoemulsions versus conventional emulsions to encapsulate  
707 curcumin, which requires further investigation. Conventional emulsions on the other hand, particularly  
708 the ones stabilized by ionic surfactants, biopolymers, protein-polysaccharide complexes suffer from  
709 destabilization in the gastrointestinal regime due to their responsiveness to physiological pH, ionic  
710 strengths and enzymes. Thus, they cannot protect the curcumin from physiological destabilization and  
711 oxidation before the encapsulated curcumin can reach the targeted sites.

712 Literature on Pickering emulsion for encapsulating curcumin is relatively scarce till date due to  
713 the very recent availability of laboratory-designed food-grade Pickering stabilizers. Nevertheless, at  
714 this early stage, Pickering emulsion shows promises in terms of in vitro gastrointestinal stability and  
715 barrier property to bile salts-induced displacement. Although bioaccessibility studies in nanoemulsions  
716 have been well documented in literature, very few studies have been conducted to assess the  
717 bioaccessibility of curcumin using Pickering emulsion approach. Further research is needed in this area  
718 of Pickering emulsions stabilized by intact or fused layer of particles of biodegradable origin to create  
719 highly stable emulsion that can be used to deliver curcumin. It will be important to identify innovative  
720 design principles for these Pickering emulsions to release the encapsulated curcumin in a controlled  
721 manner in targeted sites in human physiology and generate mechanistic insights in mixed micelles  
722 formation. Finally, designing emulsion structures loaded with curcumin together with mapping of their  
723 physical, chemical and biological fates during physiological lipid digestion (using in vitro, in vivo and  
724 clinical trials) is necessary to rationally design future curcumin-rich food, pharmaceuticals and  
725 nutraceuticals.

726

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732

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## 1092 **Figure Captions**

1093

1094 **Figure 1.** Functional groups in curcumin.

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1096 **Figure 2.** Scanning electron micrographs (SEM) of curcumin crystals dispersed at 10 mg/ mL  
1097 in methanol (a), DMSO (b), and sunflower oil (c) in lower ( $\times 5,000$ , left) and higher  
1098 magnifications ( $\times 10,000$ , right).

1099

1100 **Figure 3.** Schematic diagram of conventional emulsion (a), multilayered emulsion (b) and  
1101 Pickering emulsion (c). Preparation method of conventional and Pickering emulsion (a) and  
1102 multilayered emulsion (e).

1103

1104 **Figure 4.** Schematic diagram of nanoemulsion (a) and its preparation method by high-  
1105 intensity (b) and low-intensity (c) techniques.

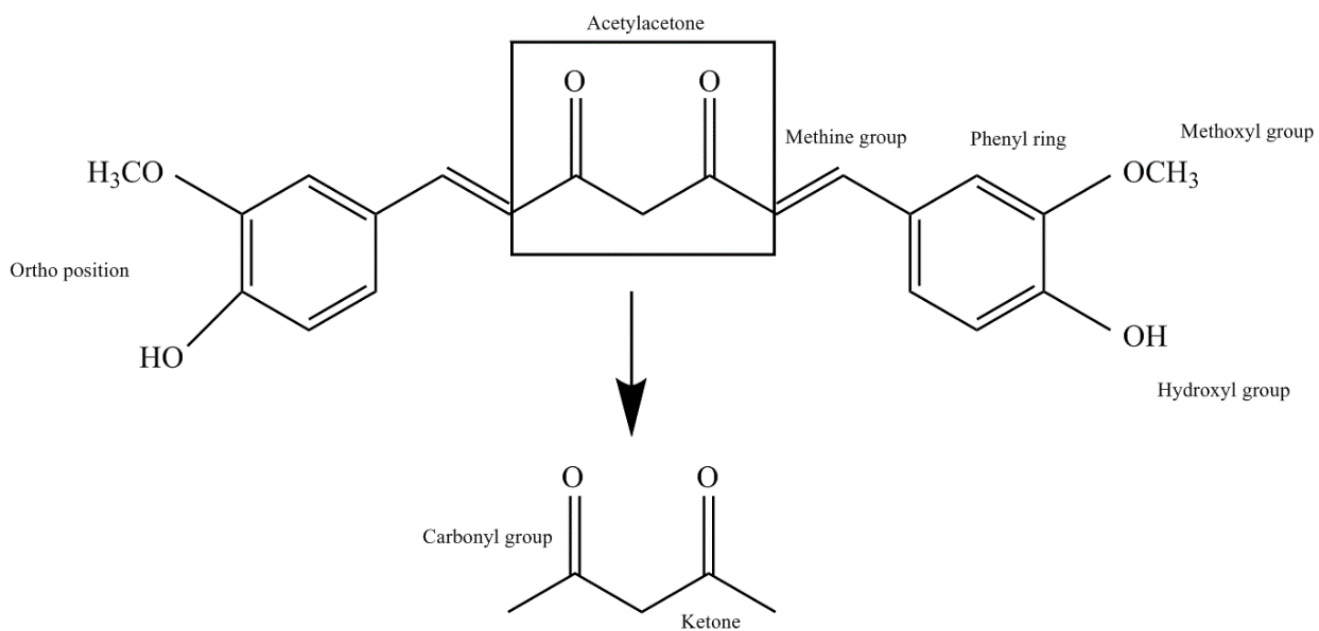
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1110 **Figure 1.**



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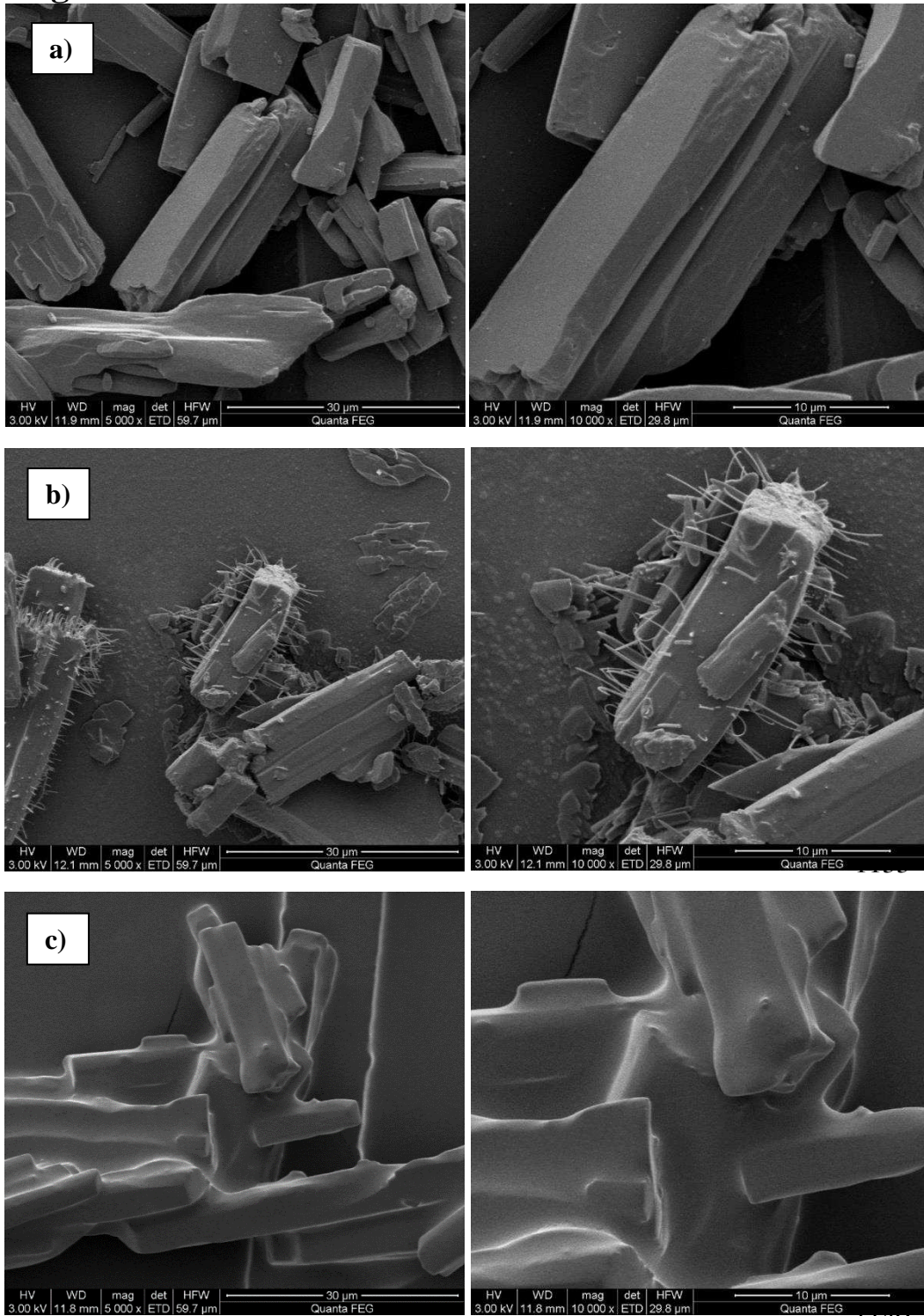
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1119 **Figure 2.**



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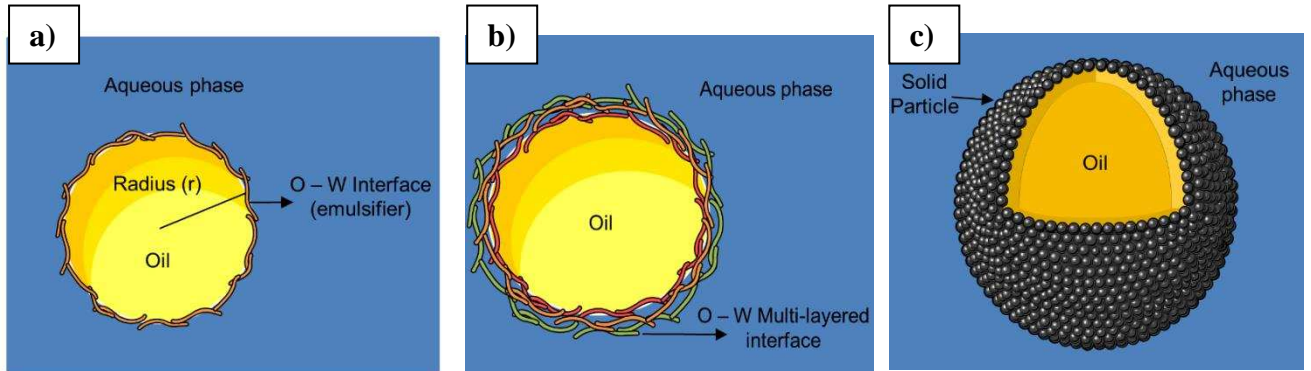
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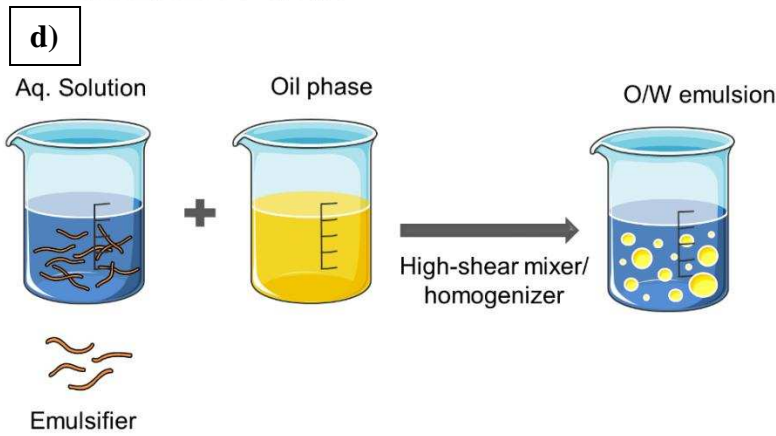
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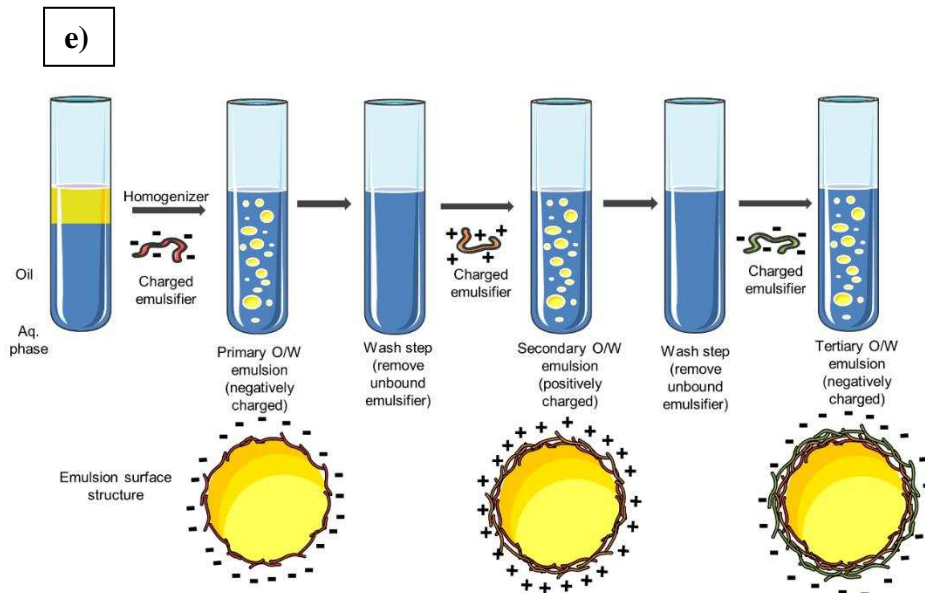
1144 **Figure 3.**



Mean radii 0.2 - 100  $\mu\text{m}$   
 Thermodynamically unstable  
 Optically turbid or opaque



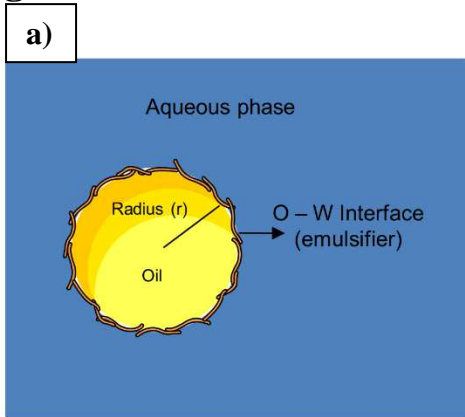
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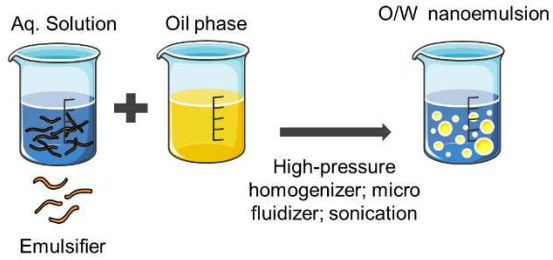


**Figure 4.**

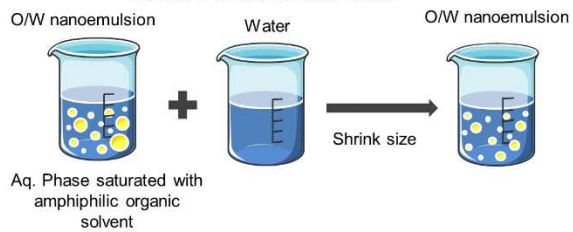


Mean radii 50 - 200 nm  
Thermodynamically unstable  
Optically transparent or slightly turbid

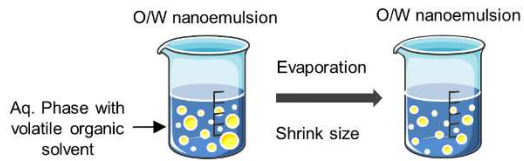
**b)** **High-intensity nanoemulsions formation (O/W):**



*i) Emulsification/solvent displacement method for further reduce the size:*

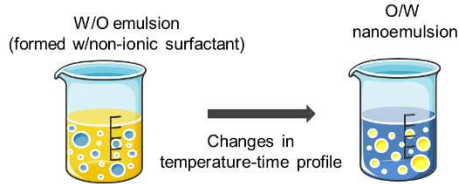


*ii) Emulsification/solvent evaporation method for further reduce the size:*

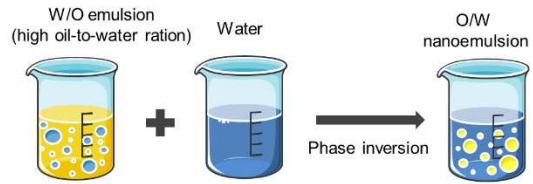


**c) Low-intensity nanoemulsions formation (O/W):**

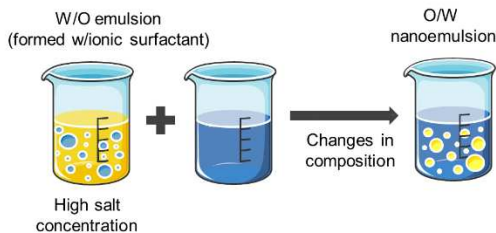
*i) Phase inversion temperature (PIT):*



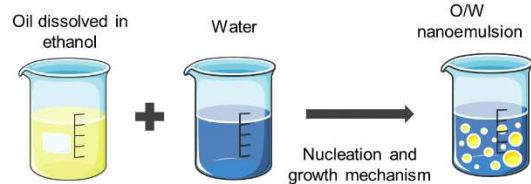
*iii) Emulsion inversion point (EIP):*



*ii) Phase inversion composition (PIC):*



*iv) Solvent demixing "Ouzo" method:*



1151 **Tables**1152 **Table 1.** Solubility ( $\mu\text{g/mL}$ ) of curcumin in various edible oils.

Oil	Solubility ( $\mu\text{g/mL}$ )	Curcumin dispersion conditions	References
Corn oil	7580	AT/ 48 h	(Setthacheewakul, et al., 2010)
	70	60 °C/ 10 min, 20 min sonication	(Joung, et al., 2016)
	2.76	60 °C/ 10 min, 20 min sonication	(Ahmed, et al., 2012)
Soybean oil	7380	AT/ 48 h	(Setthacheewakul, et al., 2010)
	0.1834	AT/ 10 min	(Lin, et al., 2009)
Oleic acid	1390	AT/ 48 h	(Setthacheewakul, et al., 2010)
MCT	250	60 °C/ 10 min, 20 min sonication	(Joung, et al., 2016)
	7.505	60 °C/ 10 min, 20 min sonication	Ahmed, et al. (2012)
Ethyl oleate	310.59	37°C/ 24 h	(Cui, et al., 2009)
	12170	AT/ 48 h	(Setthacheewakul, et al., 2010)
	0.348	AT/ 10 min	(Lin, et al., 2009)
Peppermint oil	0.2694	AT/ 10 min	(Lin, et al., 2009)
Peanut oil	129.22	37°C/ 24 h	(Cui, et al., 2009)
Castor oil	256.59	37°C/ 24 h	(Cui, et al., 2009)
Coconut oil	100	60 °C/ 10 min, 20 min sonication	(Joung, et al., 2016)
Olive oil	80	60 °C/ 10 min, 20 min sonication	(Joung, et al., 2016)

1153

1154 Abbreviations: AT, ambient temperature; MCT, medium chain triacylglycerol.

**Table 2.** Composition and formation of nanoemulsions for delivery of curcumin.

Emulsifier(s)	Oil (wt%)	Curcumin loading in oil phase (wt%)	Curcumin dispersion method	Emulsification process	References
Octenyl-succinic-anhydride (OSA) modified starch, OSA modified starch - coated with chitosan or sodium carboxymethyl cellulose	MCT (0.02-0.14)	0.00028 – 0.0020	Magnetic stirring (100 °C, 7 min)	High-speed blender (14,000 rpm, 2 min/ High-intensity sonication (20 kHz, 1-13 min, 40-45 °C).	(Abbas, et al., 2014; Abbas, et al., 2015)
Hydrogenated L- $\alpha$ -phosphatidylcholine (HEPC) (surfactant), Tween 80 and Polyoxyethylene hydrogenated castor oil 60 (co-surfactant)	Soybean Oil (~3)	0.041 – 0.66	Curcumin initially dissolved in chloroform, then oil, evaporation of chloroform	Rotary evaporation, vacuum desiccation (3-5 h) / Hydrate in bath type sonicator (55-60 °C) / Vigorous mixing and sonication (5 min) / Sonication (30-60 min, N <sub>2</sub> atmosphere, 55-60 °C).	(Anuchapreeda, Fukumori, Okonogi, & Ichikawa, 2012b)
$\beta$ -lactoglobulin	LCT, MCT, SCT, LCT: SCT (10)	0.15	Magnetic stirring (60°C, 10 min, 20 min sonication)	High-speed blender (2 min) / High-pressure homogenizer (9,000 psi, 5 cycles)	Ahmed, et al. (2012)
Tween 20, 60 and 80	Soybean oil (10-20)	0.03, 0.07, 0.1	Magnetic stirring (15 min)	Peristaltic pump (mechanical stirring 300-500 rpm) / 30 min (Inversion point (EIP) method)	(Borrin, et al., 2016)
Tween 20	Olive Oil, Coconut oil, Corn Oil and MCT (1.9-55.5)	0.3	-	High-speed homogenizer (13500 rpm, 15 min) / High-pressure homogenizer (1,000 bar, 5 cycles).	(Joung, et al., 2016)

Tween 80 (surfactant), lecithin (co-surfactant) – coated with high, medium and low molecular-weight chitosan	MCT (10)	0.65	Heating and stirring (overnight)	Stirring (10 min) / High-speed blender (1600 rpm, 5 min) / Ultrasonication (20 min, 150 W).	(Li, et al., 2016)
Tween 80, lecithin, Acacia gum and whey protein	MCT, Canola Oil, Linseed Oil, Sunflower Oil (0.5 – 3)	1.18	Ultra-sonication	High-speed blender (6 min, 10000 rpm) / High-pressure homogenizer (60 MPa, 3 cycles)	(Ma, et al., 2017a)
Poloxamer-407, Tween 20, Sodium dodecyl sulphate (SDS), Dodecyltrimethylammonium bromide (DTAB)	Cottonseed Oil (0.0010 - 0.0.0048*)	0.220 - 1.099*	Magnetic stirring (70°C, 1000 rpm)	Magnetic stirring (~70 °C, 1,000 rpm) / Magnetic stirring (650 rpm, 45 min).	(Malik, Ameta, & Singh, 2016)
Lactoferrin, lactoferrin coated with alginate, Tween 20 (T20), sodium dodecyl sulphate (SDS) and dodecyltrimethylammonium bromide (DTAB)	Corn oil (5)	0.1	-	High-speed blender (2 min) / High-pressure or Microfluidizer (20,000 psi, 5-20 cycles).	(Pinheiro, et al., 2016; Pinheiro, et al., 2013)
Sodium caseinate	Milk fat (1)	0.05	-	Sonication (60 °C, 5 min) / Sonication (30 min) / Spray dried	(Rao & Khanum, 2016)
Tween 80 (surfactant), whey protein concentrate	MCT (0.5-2)	0.0047 – 0.075	-	Magnetic stirring/ Sonication	(Sari, et al., 2015)

70 (co-surfactant)

Phosphatidylcholine 80%, coated with chitosan and chitosan 2-iminothiolane conjugate	Soybean Oil (24)	2.2	High-speed blender (60 °C, 500 rpm), Sonication	Sonication / High-pressure homogenization (2,000 bar).	(Vecchione, et al., 2016)
Tween 20	MCT (10)	1	-	High-speed homogenizer (10 min) or high-pressure homogenizer (6 cycles)	(Wang, et al., 2008)
Papain hydrolysate soy protein isolate (SPIH) – coated with microcrystalline cellulose (MCC)	MCT (10)	0.1	-	Two-speed hand-held homogenizer (3 min) / Microfluidizer (50 MPa, 3 cycles)	(Xu, Zhang, Cao, Wang, & Xiao, 2016)

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\* mol/kg.

Abbreviations: NE, nanoemulsion

**Table 3.** Composition and formation of conventional emulsions (protein-polysaccharide conjugates/ complexes-stabilized) and Pickering emulsions (particle-stabilized systems) for delivery of curcumin.

Emulsifier(s)	Oil (wt%)	Curcumin loading in oil phase (wt%)	Curcumin dispersion method	Emulsification process	References
Tween 80	Corn oil (10)	0.00279	Stirring (85 °C, 2 h)	High shear mixer / High-pressure homogenizer (12,000 psi, 5 cycles)	(Zheng, Zhang, Chen, Luo, & McClements, 2017)
Bovine serum albumin - dextran conjugate (BSA-dextran)	MCT (20 or 40)	0.22 - 0.56	Heating (90 °C, dark, 1 h)	Homogenizer (10,000 rpm, 1 min) / High-pressure homogenizer (900 bar, 4 min) / Samples heated (90 °C, dark, 1 h)	(Wang, et al., 2016)
Casein - soybean soluble polysaccharide complex (CN/SSPS)	MCT (16.7)	0.15	Solutions of 10% ethanol, 90% MCT	Homogenizer (10,000 rpm, 1 min) / High-pressure homogenizer (800 bar, 4 min)	(Xu, et al., 2017)
<b>Particles</b>					
Kafirin	Vegetable Oil (0.2 - 0.8)	0.0005 – 0.002	-	High-speed homogenizer (13,000 rpm, 3 min)	(Xiao, et al., 2015)
OSA quinoa starch granules	MCT (7)	0.0016	Rotor-stator high-shear homogenizer (22,000 rpm, 20 min)	High-shear homogenizer (22,000 rpm, 20 and 70 °C, 30 s)	(Marefati, et al., 2017)
Chitosan-tripolyphosphate nanoparticles	MCT and LCT (5-50)	0.1	-	Stirring overnight / High-speed blender (10,000 rpm, 3 min)	(Shah, et al., 2016a; Shah, et al., 2016b)
Colloidal silica	Canola Oil (5)	0.0046	Vigorously mixed (20 min)	Hand-held dispenser (8,000 rpm) / Single-stage homogenizer (600 bar)	(Tikekar, et al., 2013)