



Revisiting the cytotoxicity of quantum dots: an in-depth overview

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Abstract

Recently, medical research has been shifting its focus to nanomedicine and nanotherapeutics in the pursuit of drug development research. Quantum dots (QDs) are a critical class of nanomaterials due to their unique properties, which include optical, electronic, and engineered biocompatibility in physiological environments. These properties have made QDs an attractive biomedical resource such that they have found application as both *in vitro* labeling and *in vivo* theranostic (therapy-diagnostic) agents. Considerable research has been conducted exploring the suitability of QDs in theranostic applications, but the cytotoxicity of QDs remains an obstacle. Several types of QDs have been investigated over the past decades, which may be suitable for use in biomedical applications if the barrier of cytotoxicity can be resolved. This review attempts to report and analyze the cytotoxicity of the major QDs along with relevant related aspects.

Keywords Quantum dots · Cytotoxicity · Theranostic agents · Biocompatibility · Biomedical applications

Introduction

Quantum dots (QDs) or semiconductor nanocrystals are inorganic nanomaterials having dimensions in size range of 1–10 nm. They are composed of a semiconductor central core stabilized by a shell composed of inorganic salts (e.g., CdS, ZnS) (Mansur 2010). A semiconductor has an electron-filled region, the “valence band,” and an electron-deficient region, known as the “conduction band.” When photon energy ($h\nu$) equal to the bandgap energy irradiates the semiconductor, an

electron is promoted from the valence to the conduction band. As a result, there will be a “hole” in the valence band due to the absence of the electron. This hole can be phenomenologically treated as a “particle” with a particular effective mass and a positive charge (Simon et al. 2010). QDs have unique optical properties, such as sharp and symmetric emission spectra and high fluorescence and photostability. In the past two decades, QD utilization has attracted significant attention. There are several commercial areas for which QD utilization has been explored, such as biomedical applications. Most of these efforts so far have been devoted to tuning their semiconductor properties to develop smaller and more complex devices with better performance (Field et al. 2020).

The shell and core of QDs are both semiconductors. QD nanoparticles are generally found to be unstable and only slightly soluble in aqueous environments such as the cell cytosol (Hardman 2005). Also, water solubility can be enhanced through charged compounds covalently attached to the surface of QDs via the thiol group (Idowu et al. 2008). Molecules attached to the shell can be selected such that they are further able to conjugate to functional ligands or biomolecules (Mahmoudi et al. 2012; Hardman 2006).

Nanomedicine is a kind of medical intervention that takes place at the molecular scale. The main purposes of nanomedicine are in the treatment of disease and restoration and repair of function to damaged tissues such as the bone, muscle, or nerve (Juliano 2013). In both of these tasks, it is necessary to visualize both cell structures and the molecules

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involved in their metabolism. One solution for this challenge is to label them with a proper marker to make them easily observable. One of the most common labeling techniques in cell biology is fluorescence labeling (Koren et al. 2020). There are two main groups of existing fluorescent labels: organic dyes and inorganic nanocrystals. Organic dyes are the most exploited probes in cell biology. However, fast photobleaching and broad overlapping emission lines are drawbacks of the organic dyes. Their application area can be significantly affected due to these drawbacks, especially in long-term imaging and multicolor detection.

The unique properties of QDs, particularly their optical properties, have made them a promising choice to be used as fluorescent labels in analytical chemistry, cell biology, and medicine. There are some important differences between the common organic dyes and quantum dots as inorganic semiconductor dyes; for instance, the QD emission wavelength can be quickly and precisely tuned by adjusting the nanocrystal size, narrow symmetric emission spectra of QDs (which makes the simultaneous excitation of multiple semiconductor QDs possible) by only a single light source, less photobleaching in QD due to no excitation induced damage, and less exposure of the fluorescence center to solvent. Furthermore, the obtained images using semiconductor QDs often exhibit better contrast due to their high resistance to bleaching, which are among their most important advantages.

Conjugation between QD and biomolecules (such as proteins and enzymes) makes them applicable for use in a wide range of applications, such as nanomedicine (Mansur 2010), tracking proteins in living cell (Parak et al. 2002; Pathak et al. 2001), fluorescence labeling (Dwarakanath et al. 2004; Peppley et al. 1999), biosensors (Sapsford et al. 2006), deep-tissue imaging (Klostranec and Chan 2006), ex vivo/in situ live cell imaging, and in vivo targeting of cells, tissues, and tumors with monitoring by PET and MRI (Bera et al. 2010) and high-throughput screening.

Physiochemical properties of QDs

Achieving an understanding of the interfacial characteristics of QDs helps develop an understanding of how they interact with the different biological systems (Clift and Stone 2012). QD cores consist of elements from II–VI or III–V of the periodic table. QD cores are covered by a shell of semiconductor compounds. A semiconductor is a material that has an electrical conductivity lower than that of an electrically conductive material and higher than that of a non-conductive material. Examples of groups III–IV QDs include indium phosphide (InP), indium arsenide (InAs), gallium arsenate (GaAs), and gallium nitride (GaN) (Male et al. 2008). Examples of groups II–VI QDs include zinc sulfide (ZnS), zinc selenium (ZnSe), cadmium selenium (CdSe), and cadmium tellurium (CdTe)

(Taniguchi et al. 2011). Some studies have also shown that higher atomic mass elemental combinations such as CdTe/CdSe or CdSe/ZnTe can also act as QDs.

The functionalization of the core-shell can give the desired bioactivity to QDs for application in biological systems (Hardman 2006). Many biomolecules, such as proteins, peptides, and lipids, can attach to the surface of the QD shell. As mentioned earlier, the thiol group capping through covalent linkage was reported to be useful for enhancing water solubility to the QDs (Idowu et al. 2008). Also, polymer coatings (such as polyvinyl alcohol (PVA), polymethyl methacrylate (PMMA), and polylactide co glycolides (PLGA)) can be applied to the surface of QDs which makes the semiconductor QDs able to be targeted to specific organs within the body to diagnose, treat, or prevent disease (Wang et al. 2012). The most common polymer shell used, especially for nanomedicine purposes, is polyethylene glycol (PEG). Different methods such as electrostatic interactions, physical adsorption (physisorption), multivalent chelation, and covalent bonding can be used to functionalize the QD outer shell. Applying surface attachments can have a significant effect on the size of QDs (Clift and Stone 2012).

Several physical properties experience significant changes when the bulk material is in the form of nano-sized particles. For semiconductor nanoparticles, changing the particle size noticeably affects the bandgap. The average distance between the electron, which is photogenerated, and the hole is called the exciton Bohr radius (Zhang et al. 2014). As the particle size of the semiconductor approaches its exciton Bohr radius, the dependence of its optical and electrical properties on its physical dimensions becomes higher (Amelia et al. 2012). Because the QD particles are small, the generated electrons are confined to a smaller space than the natural space they would occupy in bulk semiconductors. This quantum confinement is the reason that the size of QD has a strong effect on the optical and electrical properties (Zhu et al. 2017). As the QD particle size decreases, there is a higher confinement degree, which results in higher bandgap energy.

As a consequence, the QD particle size tunes its bandgap energy and the emission wavelength. By adjusting the particle size, it is possible to prepare a QD for fluorescent emission from the UV into the IR spectra. Multiplexing of QD signals adds the possibility of imaging and tracking multiple molecular targets simultaneously. Furthermore, it creates promising opportunities in medical applications, since numerous genes and proteins are involved in many diseases. QD signals can be multiplexed as a result of broad and narrow absorption bands combination. Emission behavior of QDs can be tuned by their structural modifications which gives the possibility of fabricating materials for efficient light emitting diode applications (Ramalingam et al. 2019). Common organic dyes have wide emission bands, which significantly increase the complexity of detecting multiple signals.

Additionally, there are some essential fluorophores in biological tissues and fluids which produce a background signal. This background signal significantly decreases the detection ability and sensitivity of the probe. Biological fluorescence typically shows high background intensity in the blue-to-green spectral region. This is why most cell and tissue micrographs have a faint greenish color. QDs can minimize such auto-fluorescence since they can be tuned to emit in desired spectral regions.

In summary, a variety of different surface modifications (surface-covered functional groups and biomolecules covering the surface of QDs) can be applied to the surface of QDs, which changes their physicochemical properties. Fig. 1 schematically represents the structure and different core regions of the quantum dot along with the common surface capping agents (Maysinger et al. 2007)

It is important to know that the physicochemical properties of QDs can be adjusted and tuned at their synthesis stage. Generally, it can be said that the physicochemical properties of QDs are considered to be defined by their core-shell conjugate constitution (Hoshino et al. 2004).

Mechanisms of QD cytotoxicity

Although QDs have received much attention and have entered into preclinical use, one key unresolved issue is their potential toxicity. It has been suggested that QD toxicity can be rationalized based on their physicochemical properties, such as core-shell materials, size, surface charge, ligands nature, and interaction with other present molecules in biological media (Oh et al. 2016). In other words, their toxicity may be due to either some inherent chemical feature or their nanoscale properties. Aspects related to inherent toxicity are mostly due to the elements

contained with the QD core, such as cadmium and selenium, which exhibit significant toxicity to both cell cultures and live animals. Such studies have demonstrated toxicity at the supra-micromolar concentrations. Elemental toxicity is considerably dependent upon the accessibility of the core QD atoms to the surrounding solvent (Kirchner et al. 2005).

Regarding this point, cadmium atom toxicity is related to its relative permeability to oxygen and protons of conjugated groups. Oxygen can diffuse to the surface of the QD shell and trigger oxidation of the core atoms. Hydrogen ions can also cause protonation of the ligands and cause them to become detached from the QD surface (Derfus et al. 2004; Aldana et al. 2001). The biochemical mechanisms resulting in QD cytotoxicity are still controversial. Studies were reported which analyzed the effect of QDs on the liver and found that there is a direct correlation between Cd^{2+} release and cytotoxicity based on a mechanism involving inactivation of essential mitochondrial proteins through Cd-sulphydryl group interactions (Derfus et al. 2004). It was demonstrated that the adsorption/accumulation of QDs on the cell surface could also impair cell function. Based on these observations, it was proposed that QD toxicity was a function of cell ingestion/uptake and not due to possible leaching of ions from the QDs into solution external to the cells (Parak et al. 2005). Another possible mechanism of QD toxicity is the generation of reactive oxygen species, such as free radicals and the creation of singlet oxygen (Zhou et al. 2017). Generation of such reactive oxygen species can cause irreversible damage to nucleic acids, enzymes, and cellular components such as mitochondria and both the plasma and nuclear membranes (Samia et al. 2003). Another study observed that CdSe and CdSe/ZnS QDs were able to generate free radicals (Choi et al. 2007). Another study postulated that surface oxidation of QDs leads to the

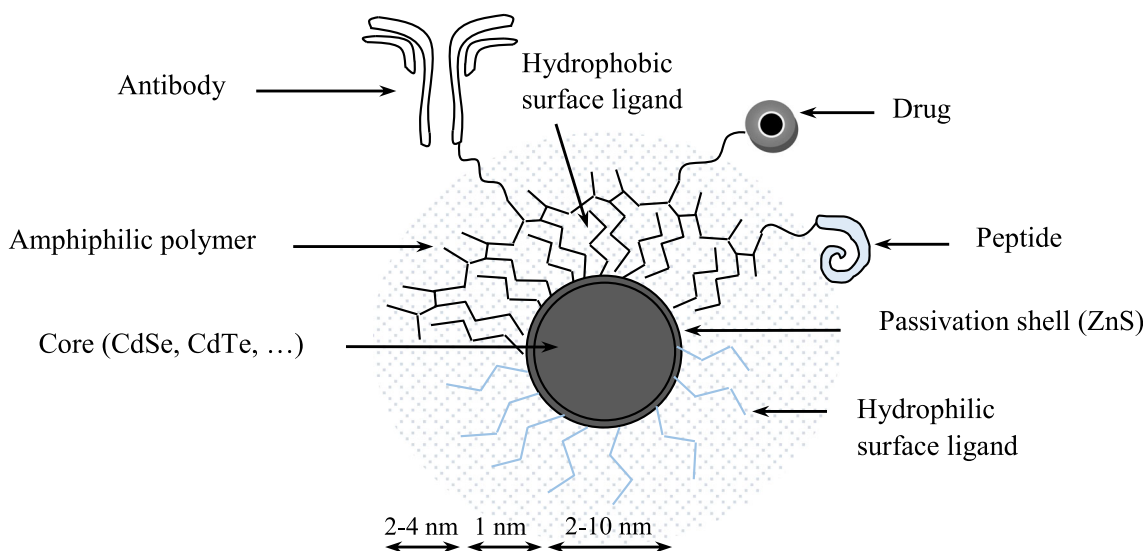


Fig. 1 Structure of quantum dot with surface coating agents. Reprint with permission (Maysinger et al. 2007)

generation and release of free cadmium ions, causing apoptosis (Derfus et al. 2004). It is also reported that cytotoxicity of QDs can be due to the type of molecules adsorbed to the surface of QDs in addition to the monocrystalline particle itself (Kirchner et al. 2005).

Decreasing the toxicity of QDs in biomedical applications

A major goal of QD research is its use in the development of biomedical applications. Among the various applications of QD in the biomedical field are the following: bioimaging, targeted drug delivery, and photodynamic therapy. The following factors determine the criteria of QDs suitable for employing in biomedical applications: (i) biocompatibility, (ii) cytotoxicity, and (iii) fluorescence behavior. Concern over QD cytotoxicity has been an important research topic over the last few decades, and various methods have been reported to reduce the toxicity of QD during their preparation. Silicon QDs are a family of well-studied QDs owing to their excellent biocompatibility and tunable physical and chemical properties, making them good candidates for theranostic applications (Sivasankarapillai et al. 2019). However, when we search through the literature focusing on the cytotoxic properties of all types of QDs, the diverse nature of the individual QD systems makes comparison difficult. This feature creates an attempt to generalize the toxicity of QDs, a nearly impossible task. In this section, we briefly discuss the cytotoxicity aspects of the most explored class of QDs available in the literature.

A significant observation was reported that CdTe QDs are highly cytotoxic due to the release of cadmium ions. The authors demonstrated that the presence of a ZnS outer-layer significantly improves the biocompatibility of QDs, with no observed cytotoxicity even at very high concentrations and long-time exposure in cells. However, it should be noted that the cytotoxicity of CdTe QDs cannot be solely attributed to the toxic effect of free Cd²⁺ ions through a systematic investigation on HEK293 cells (Su et al. 2010). This study demands further investigation of the specific properties of QDs responsible for the observed cytotoxicity of CdTe QDs. Another study investigated the cytotoxicity of a series of aqueous synthesized QDs such as CdTe, CdTe/CdS core-shell structured, and CdTe/CdS/ZnS core-shell-shell structured QDs. The authors suggested that released cadmium ions were responsible for the observed cytotoxicity of cadmium-based QDs (Chen et al. 2012). This study also provides additional features of QDs responsible for cytotoxicity using genome-wide gene expression profiling and subcellular localization of synthesized QDs with synchrotron-based scanning transmission X-ray microscopy (STXM).

Interesting work was reported in which L-cysteine (Cys) capped CdTe QDs were prepared in an aqueous medium. This

study suggested that the capping agent reduced cytotoxicity upon the basis of experiments involving HeLa cancer cell lines (Kim et al. 2015). For cytotoxicity of CdSe/CdS QDs, it was paradoxically found that comparing toxicity based on particle concentrations was extremely difficult (Soenen et al. 2015). QDs possessing significant cytotoxicity have also been found to rapidly degrade under endosomal pH, resulting in leached Cd (II). Cytotoxicity of CdSe, CdTe, and InP based on four QD formulations involving (i) mercaptopropionic acid-modified CdSe/CdS/ZnS QDs (CdSe-MPA), (ii) PEGylated phospholipid encapsulated CdSe/CdS/ZnS QDs (CdSe-Phos), (iii) PEGylated phospholipid encapsulated InP/ZnS QDs (InP-Phos), and (iv) pluronic F127 encapsulated CdTe/ZnS QDs (CdTe-F127) was investigated. Interestingly, two cancer cells (gastric adenocarcinoma (BGC-823) and neuroblastoma (SH-SY5Y)) showed different toxicity responses (Liu et al. 2015). This study gives valuable insight to the fact that the toxicity of QDs does not solely depend on a single factor but rather depends on a combination of elements from the particle formulations and extent of cellular uptake.

Meta-analysis is a valuable tool to apply data from the literature when dealing with a vast amount of scientific documentation. Literature is available, which shows meta-analysis investigation on the toxicity of Cd-based QDs using random forest regression models to analyze the data. The authors reported that the toxicity of QD is closely correlated with surface properties, including shell composition, ligand and surface modifications, QD diameter along with assay type, and exposure time to the biological environment (Oh et al. 2016). Also, aspects of the mechanism of cytotoxicity of Cd containing QDs were reviewed. Using CdTe/CdS 655 (QD 655), the authors showed that this QD elicited toxicity *in vitro* and *in vivo* by activating cell autophagy (Fan et al. 2016).

The effect of negatively charged CdTe QDs (-21.63 ± 0.91 mV) on human umbilical vein endothelial cells (HUVECs) was reported. The authors said that both caveolae/raft- and clathrin-mediated endocytosis were involved in the endothelial uptake of CdTe QDs, and the QDs were transported to the endoplasmic reticulum (ER). The results indicated that the toxicity mechanism is initiated through stress response by upregulation of the ER stress markers GRP78/GRP94 and activation of protein kinase RNA-like ER kinase-eIF2 α which activates the transcription factor 4 pathway. This study reported that all three ER stress-mediated apoptosis pathways were activated and that the ER was involved in the direct participation of CdTe QDs-caused apoptotic cell death in HUVECs (Yan et al. 2016). The cellular uptake of four CdSe/ZnS QDs (COOH CdSe/ZnS 525, COOH CdSe/ZnS 625, NH₂ CdSe/ZnS 525, and NH₂ CdSe/ZnS 625) and their ability to induce physiological responses in *Phanerochaete chrysosporium* (*P. chrysosporium*) was studied and reported (Hu et al., 2017). The authors showed that the four CdSe/ZnS QDs accumulated mostly in the hyphae and

caused oxidative stress to *P. chrysosporium* in the tested concentration range (10–80 nM). Furthermore, this work provided evidence for the fact that cytotoxicity of these QDs was related to the physicochemical properties of the QDs, such as particle size and surface charges. Another exciting study reported nontoxic concentrations of CdSe/ZnS core/shell QDs vary between 4.13 and 12.7 nm/ml and identified the limit of CdSe/ZnS QD concentration at which they manifest themselves as reasonably safe and nontoxic agents for biological applications (Bozrova et al. 2018).

Graphene has generated much interest due to its unique electronic properties. Significant theoretical investigations on graphene quantum dots (GQDs) using molecular dynamics simulations were reported (Liang et al., 2016). At high GQD concentrations, the GQDs aggregated in water but disaggregated upon entering into the membrane interior. Moreover, high concentrations of GQDs could induce changes in the structural properties and fluidity of the lipid bilayer. On this basis, the authors speculated that QDs might affect cell signal transduction. On the other hand, the authors found that GQDs of relatively small size was not large enough to mechanically damage the lipid membrane and thus concluded that cytotoxicity of GQDs was size-specific and that small-sized QDs may be more appropriate for biomedical application.

Gradient-alloyed quantum dots (GA-QDs) are a novel class of QDs for biomedical imaging applications due to their improved fluorescent and luminescent properties over conventional QDs. Toxicity aspects of these compounds are of great importance to fully utilize their superior luminescent properties for clinical applications. Peynshaert and coworkers report on the relation between the surface coating of GA-QDs and their cytotoxicity. The authors carefully examined the toxicity of two identical gradient-alloyed QDs, differing only in their surface coatings, namely 3-mercaptopropionic (MPA) acid and polyethylene glycol (PEG) on HeLa cells. Both types have a gradient $\text{CdSe}_x\text{S}_{1-x}$ core surrounded by a ZnS shell. The authors observed that PEGylated QDs were significantly more toxic due to increased ROS production and lysosomal impairment, which further caused autophagy dysfunction (Peynshaert et al. 2017). Toxicity of halloysite nanotube stabilized CdS QDs on cell lines derived from human skin fibroblasts and prostate cancer cells was reported. The authors suggest that the immobilization of QD onto the surface of halloysite nanotubes may lower the cytotoxicity induced by released Cd (II) ions (Stavitskaya et al. 2018). Towards this point, the azine-mixed system, HNTs-azine- $\text{Cd}_{0.7}\text{Zn}_{0.3}\text{S}$, showed the lowest cytotoxicity due to the lowest release of Cd (II). Another study compared the cytotoxicity of CdTe QDs against the rate and extent of their degradation within the cell. The authors used a validated high-content screening approach, and QD degradation was monitored through the loss of fluorescence intensity (Manshian et al., 2017). This work established the strong dependence of the cytotoxicity of CdTe QD with its degradation. As mentioned, targeted drug delivery is

a significant area of QD research since QDs can be used as both drug carrier vehicles and also for the bioimaging process for diagnostic purposes. Several works report on the cytotoxicity evaluation of drugs conjugated with QDs, especially anticancer drugs. Methotrexate (MTX) is a potent anticancer drug which is limited in use due to the development of drug resistance by malignant cells. An exciting work synthesized MTX-conjugated l-cysteine capped CdSe QDs (MTX-QD nano-conjugates) and evaluated their uptake and cytotoxicity in KB cells with/without resistance to MTX (Johari-Ahar et al. 2016). The authors observed that MTX-QD nanoconjugates efficiently internalized into the cancer cells, and induced markedly high cytotoxicity (IC_{50} , 62 $\mu\text{g}/\text{mL}$) in the MTX-resistant KB cells as compared to the free MTX molecules (IC_{50} , 105.0 $\mu\text{g}/\text{mL}$), whereas these values were respectively about 3.1 and 3.6 ng/mL in the MTX-sensitive KB cells.

Graphene QDs (GQDs) are essential candidates for biological applications, and these aspects are recently reviewed and available in the literature (Li et al., 2019). An interesting genotoxicity analysis of N-doped GQDs was reported (Şenel et al., 2019). DNA binding analysis showed that N-doped GQDs interact with CT-DNA via both intercalation and electrostatic binding. The study of the DNA cleavage patterns showed that the N-doped GQDs cleaved DNA without any external agents and thus established significant genotoxicity. Also, siRNA loaded GQDs showed an excellent possibility to act as potential antitumor agents through the induction of DNA and mRNA breakage. Surface functional groups play an essential role in determining the toxicity of QDs as they act as the first point of contact between the compound and biological environment. Thus it is essential to analyze the influence of functional groups regarding their role in the toxicity of QDs. Also, the influence of functional groups on the toxicity of graphene QDs was investigated and reported. The authors selectively deposited either ketone carbonyl, carboxylic, or hydroxyl groups on GQDs and then compared the ROS generating ability of the different GQD derivatives (Zhou et al. 2017). This study reports that the ROS production ability of GQDs is closely related to the reduced state of the surface oxygen functional group. Removal of the oxygen functional groups on GQDs can increase the photostability and lower the photo-induced cytotoxicity.

A number of investigations have examined the change in toxicity of GQDs when in association with other metal ions like silver nanoparticles (Ag NPs). Literature suggests that the use of PEGylated silver nanoparticles decorated with graphene quantum dots (Ag-GQDs) for targeted delivery of doxorubicin (DOX) against HeLa and DU145 cancer cells was reported in vitro (Habiba et al. 2015). The authors used a photosensitizer to investigate the synergistic effect of chemo and photodynamic therapy in this system. The treatment of Ag-GQDs conjugated with doxorubicin under irradiation with a 425-nm lamp

significantly increased the death in DU145 and HeLa cells. Interestingly, the toxicity of graphene oxide (GO) QDs is found to be rectified on the coating with other biomolecules like folic acid. Another study demonstrated the lack of cytotoxicity of folic acid-modified graphene oxide (GO) quantum dots using HaCaT cells (Goreham et al. 2018). The modified GO QDs were found to be non-toxic to macrophage cells even after prolonged exposure and high concentrations. This finding needs to be further investigated as it raises the possibility of implementing GQDs for biomedical applications by resolving their toxicity through the surface coating.

The toxicity of CuInS₂ quantum dots (CIS QDs) was analyzed using *Caenorhabditis elegans* (*C. elegans*) as a model organism (Chen et al. 2015). The authors synthesized CIS QDs through the hydrothermal method and observed that QDs have no significant cytotoxicity in the organism and have excellent chemical stability. A similar work evaluated the cytotoxicity of CuInS₂/ZnS QDs coated with polymeric shells and found them to have good hemo-compatibility and negligible cytotoxicity even after their penetration into cells (Speranskaya et al. 2016). This study reveals that cellular uptake is not necessarily the reason for cytotoxicity. The toxicity of ZnO QDs was found to be enhanced in the presence of Cu (II) ions along with the concomitant production of ROS species in *Escherichia coli* cells (Moussa et al. 2016).

Similarly, the cytotoxicity of InP/ZnS QDs having three different surface functional groups, NH₂, COOH, OH, were evaluated and reported. The uptake efficiency of QDs, the cell apoptosis, and ROS generation was assessed on two different cell lines (human lung cancer cell HCC-15 and alveolar type II epithelial cell RLE-6TN). The authors observed that all the InP/ZnS QDs were able to enter the cells, with high uptake efficiency for InP/ZnS-COOH and InP/ZnS-NH₂ exhibited at low concentrations of QD (23 nm/ml) (Chen et al. 2018). High doses of InP/ZnS QDs caused the cell viability to decrease, and InP/ZnS-COOH QDs and InP/ZnS-NH₂ QDs appeared to be more toxic than InP/ZnS-OH QDs. Besides, all these InP/ZnS QDs promoted cell apoptosis and intracellular ROS generation after being co-cultured with cells.

To summarize this section, we emphasize the following points: Despite the many advantages shown by QDs, there are concerns regarding their cytotoxicity. It is difficult to provide a blanket evaluation of the toxicity of QDs because there are so many different categories according to their method of production, size, composition, charge, concentration, outer coating (capping material, functional groups), oxidative properties, photolytic conversion rate, and mechanical stability. All of these factors are determining factors in QD toxicity. Several studies have shown that QDs can cause damage to cells and produce significant DNA damage due to acute toxic effects. Evidence showed that if QDs were retained in cells or accumulated in the body for an extended period, their coatings might be degraded, yielding “naked” QDs can induce damage

to the plasma membrane, mitochondrion, and nucleus, leading to cell death (Lovrić et al. 2005). Significant work was reported. The study of Clift et al. [13] that assessed the effects of a series of different surface-coated QDs on J774.A1 macrophage by cytotoxic examination (MTT assay and LDH release) showed that hydrophobic QDs caused a significant reduction in the cell metabolic activity (MTT assay) with subsequent release of LDH from J774.A1 macrophages (Clift and Stone 2012). It was also reported that QDs might induce cytotoxic effects in L929 fibroblasts at high exposure concentrations (Zhang et al. 2015a, b). The QDs were also found to cause oxidative stress, which led to DNA damage and subsequent apoptosis in liver cells. From a broader perspective, an assessment of QD blood compatibility showed that concentration of 29 ng/mL might serve as a threshold level for the types of QDs used in this study (also perhaps particular to their use in L929 fibroblast studies). Commercially available CdSe core/ZnS shell QDs of two different sizes (QD 565 and QD 655) and three different surface coatings (PEG, PEG-amines, and carboxylic acids) were used to test the hypothesis that QDs would be differentially taken up by the human epidermis (Ryman-Rasmussen et al. 2007). The authors concluded that grouping or classification of QDs about their potential toxicity based on size or other physicochemical properties alone would prove troublesome. They suggested that each QD type needs to be characterized individually to assess their potential toxicity. The findings in that work indicate that under certain conditions, QDs may affect environmental and human health, which needs to be individually determined for utilizing QDs for various applications.

Effect of QDs on environment and ecosystem

Particle size and surface area are important material characteristics from a toxicological perspective. As the size of a particle decreases, its surface area to volume ratio increases allowing a more significant proportion of its atoms or molecules to be displayed on the surface rather than the interior of the material. The change in the physicochemical and structural properties of engineered nanomaterial with a decrease in size could be responsible for a number of material interactions that could lead to toxicological effects. The very properties of nanoscale particles being exploited in certain applications (such as high surface reactivity and the ability to cross cell membranes) might also be responsible for their adverse health and environmental impacts. As a result, nanomaterials may present new health and environmental risks that have not been encountered before.

An increase in nanomaterial research will undoubtedly lead to the effective dumping of a lot of QDs into the environment, which may ultimately result in environmental toxicity (Zhang et al. 2012; Rocha et al. 2017). To date, there are no detailed

Table 1 Results for toxicity associated with graphene quantum dots

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
Cu ²⁺ ion-labeled GQD	Mice, GC-1 spg (ts) (ATCC # CRL-2053) and TM3 (ATCC # CRL-1714) cell lines	Oral gavage and intravenous injection	Oral: 0 (PBS), 60, 100, and 24 h 300 mg GQDs/kg mouse (500 µL per mouse) IV: 0 (PBS), 25, 75, and 150 mg GQDs/kg mouse (200 µL per mouse)		High doses of GQDs administered via oral gavage or intravenous injection produce no discernible short- and long-term toxic effects on male re- productive ability and health of off- spring	Zhang et al. 2019
Nitrogen- doped graphene quantum dots (N-GQDs) GQD	Zebrafish embryos	Feeding	0, 25, 50, and 100 µg/mL	72 h	N-GQDs could perturb the endogenous antioxidant enzyme system via transcriptional or posttranscriptional repression of antioxidant enzymes	Deng et al. 2019
	Rats	Intraperitoneal injection	10 mg/kg/day	(i) From the day of immunization until the end of the experiment, (ii) during the first 7 days, (iii) from day 8 post-immunization until the end of the experiment, (iv) or from the day when first symptoms appeared until the end of the experiment	Neuroinflammation and alleviating immune-mediated CNS damage	Tosic et al. 2019
GQDs	Zebrafish	Well dispersions of aqueous solutions of GQDs	0–100 µg/mL	7 days	Molecular regulatory networks are comprised of different signaling pathways triggered by GQDs	Deng et al. 2018
GQD	Zebrafish	Direct exposure	12.5–200 µg/m	96 h	GQDs induced developmental nanotoxicity, which resulted in persistent effects on zebrafish larvae. Therefore, the exposure to high concentrations (> 50 µg/mL) of GQDs might constitute a developmental hazard to zebrafish	Wang et al. 2015a, b
N-GQDs	RBC	Hemolysis assay	3.1, 6.2, 12.5, 25, 50, 100, 200 µg m/L	3 h	Lots of echinocytes were observed unexpectedly which may be due to the incorporation of small N-GQDs into the lipid membrane	Wang et al. 2015a, b

Table 2 Results for toxicity associated with cadmium quantum dots

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
CdS-QDs	Soybean plants	Growth medium	50–200 mg/L	14 days	Peroxidases play the predominant role in quenching the oxidative stress caused by CdS-QD exposure. At the highest CdS-QD treatment (200 mg/L), root lignification allowed the plants to restrict Cd accumulation, except in QD-PVP, where lignification was reduced by 21% leading to higher Cd content in shoots	Majumdar et al. 2019
CdSe and CdSe/ZnS	<i>Escherichia coli</i> (<i>E. coli</i> , represents a prokaryotic system) and <i>Phanerochaete chrysosporium</i> (<i>P. chrysosporium</i> , represents eukaryotic system)	In vitro and growth medium	0, 10, 20, 50, and 80 nM	48 h	Bioaccumulation amounts of CdSe QDs by <i>E. coli</i> and <i>P. chrysosporium</i> were larger than those of CdSe/ZnS QDs due to the smaller particle size and less negative surface charges of CdSe QDs.	Hu et al. 2019
CdSe QD, CdSe/ZnS QD	<i>Shewanella oneidensis</i> MR-1	In vitro	A total volume of 150 μ L at varying concentrations	15 min	QD interaction leads to membrane disruption, which is mechanical and depends on the QD concentration and their affinity to the liposome membranes	Williams et al. 2018
CdSe/ ZnS	SPF grade female and male BABL/c mice	Subcutaneous injection	5.0, 1.0, and 0.1 pmol/day/mouse	14 days	QDs are found in the ovaries, but no changes are detected on the behavior and estrous cycle on the female mice. The mRNA downregulations of FSHr and LHr are observed, and the number of matured oocytes had shown a significant decrease when the QDs dosage was above 1.0 pmol/day along with a decrease in fertilization rate	Xu et al. 2016
CdSe/ZnS	Human hepatic cell line L02 and 8-week-old male C57BL/6 mice	In vitro (L02), IV injection (mice)	20, 40, and 80 nM (L02) 10 nmol/kg body weight (mice)	48 h (L02) 2 weeks (mice)	CdSe/ZnS QDs conjugated with carboxyl groups induced hepatocyte pyroptosis, and liver inflammation and dysfunction. The in vitro and in vivo hepatic toxicity of QDs was mediated by QDs-induced NLRP3 activation which was attributed to Ca ²⁺ mobilization and mtROS production after exposure to QDs	Lu et al. 2016
CdSe/ZnS	TK6, BEAS-2B, and HFF-1	In vitro	0–20 nM	24 h		

Table 2 (continued)

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
CdSe@MSA and CdSe(S)@MSA QDs	<i>Escherichia coli</i>	In vitro	0–4000 nM	100 min	Cytotoxicity and genotoxicity are strongly affected by a multitude of parameters including (1) differences in cell type potentially resulting in varying surface area contact with the exposed material, in addition to inherent cellular differences in internalizing NPs and ability to cope with an exogenous insult; (2) the nature of the QD surface chemistry; (3) the degree of QD agglomeration in the presence of varying amounts of serum proteins; (4) differences in cell culture media composition; and (5) time of exposure	Lin et al. 2015
TGA/TGH-CdTe	HeLa cells and Kunming mice	In vitro, intravenous injection (in vivo)	In vitro: 45 mg mL In vivo: 0.4 (low dose), 2.0 (representing medium dose) and 10.0 (representing high dose) mg kg ⁻¹	24 h	The toxicity observed for CdSe QDs may be directly linked to •OH radicals produced	Kauffer et al. 2014
GSH-CdQDs and MPA-CdQDs	<i>Leishmania minor</i>	Direct exposure	0–15 mg/L	168 h	PEG modification played an important role in reducing the toxicity of the QDs. PEG conjugated with the QD surface through chemical bonds and thus altered their surface state. Furthermore, PEG formed a fence-like structure on the QD surface, which could more effectively prevent Cd ²⁺ release, which was induced by the diffusion effect from the QD surface to the solution	Du et al. 2019
CdS QDs	Yeast strains	Transcriptomic analysis	0.25 mg/L	24 h	GSH- and MPA-capped Cd-based QDs have similar toxicity for <i>L. minor</i> but are significantly less toxic than CdCl ₂ In this case, yeast can be a good model to correlate genes with human orthologues in a cross-species comparison that might help to elucidate the response to toxic insults, like to CdS QDs, at a system level as well as to predict the mode of action of	Modlitbova et al. 2018 Pasquali et al. 2017

Table 2 (continued)

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
Negatively charged: MPA-CdTe/ZnS QDs, MPA/MPO-CdTe/ZnS QDs, NAC-CdTe/ZnS QDs, GSH-CdTe/ZnS QDs Positively charged: CA-CdTe QDs and CA-CdTe/ZnS QDs	<i>E. coli</i>	Optical density (OD) assays		2 h	similar compounds in other species QDs decrease the growth rate of <i>E. coli</i> . The inhibition ratio of positive QDs is higher than that of negative QDs	Lai et al. 2017
CdTe	Liver mitochondria from female Wistar rats	Direct exposure	100 nM	60 min	Two kinds of QDs, coated with MPA and TGA respectively, could impair mitochondrial energy metabolism and affect mitochondrial lipid peroxidation	Xiang et al. 2017
CdTe	Male BALB/c mice	IV injection	High dose of 2.0 nmol per mouse and a low dose of 0.2 nmol per mouse	90 days	Bodyweight measurements demonstrated there was no overt toxicity for both dose at day 90 after exposure, but the high dose CdTe affected body weight up to 15 days after exposure	Lin et al. 2015
CdTe	8-week-old male mice	Intravenous administration	4.125, 8.25, and 16.5 mg/kg	4 weeks	Increased the level of lipid peroxides marker, MDA, in the liver	Zhang et al. 2015a, b
CdTe and CdTe@ZnS QDs	<i>Caenorhabditis elegans</i>	Foraging behavior assay	0.001, 0.01, 0.1, and 1 g/L (CdTe) 0.1 and 1 g/L (CdTe@ZnS QDs)		Neurotoxicity of CdTe QDs at concentrations of 0.1–1 g/L on both the development and function of RMEs motor neurons in nematodes. Data demonstrate the impairment of foraging behavior after CdTe QDs exposure and imply the possible severe ecological risk of long-term exposure to low concentrations of CdTe QDs to environmental animals	Zhang et al. 2015a, b
CdTe	<i>Bombyx mori</i>	IV injection	0.08 nM and 0.32 nM	48 h	Time and dose-dependent damage in the hematopoietic organ and hematocytes. With ROS might be one of the influencing mechanisms	Liu et al. 2014
CdS	<i>Mytilus galloprovincialis</i>	In vitro	0.001, 0.01, 0.1, 1, 10, 25, 50, and 100 mg Cd/L	24 h	CdS QDs exposures decreased the cell viability of both hemocytes and gill cells. Main mechanisms	Katsumiti et al. 2014

Table 2 (continued)

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
Phospholipid micelle encapsulated CdSe/CdS/ZnS QDs	Kunming mice	IV injection	0.81 mg (7.2 μmol)/kg	14 days	of toxicity of CdS QDs in mussel hemocytes and gill cells involve ROS production and genotoxicity QD exposure with a short buffering period before conception does not cause overt pregnancy complications or significant toxicity effects	Xiang et al. 2017

studies on the mechanism of transport and biodegradation or association of QDs with biological materials that may eliminate nanomaterials. The presence of nanomaterials in the environment also affects the ecosystem. In a recent study, the toxicity of fullerene-C60 in two aquatic species, *Daphnia* and *Pimephales*, showed elevated lipid peroxidation (LPO) in the brain, significantly increased LPO in gill, and resulted in a significant increase in expression of genes related to the inflammatory response and metabolism. Processes that control transport and removal of NPs in water and wastewater have not yet been investigated to understand the fate of QDs. Studies on the effect of QDs on plants and microbes are also largely absent. The fate of nanomaterials in an aqueous environment is controlled by many biotic/abiotic processes such as solubility/dispersibility, interactions between the nanomaterials, and natural/anthropogenic chemicals in the ecosystem. Ecological risk assessment is essential to understand the environmental implications of nanomaterials. Before unknowingly dumping a large number of dangerous nanomaterials into the environment, we need to investigate the solubility and degradability of engineered NPs in soils and waters, to establish baseline information on their safety, toxicity, and the adaptation of soil and aquatic life.

Until now, there are different opinions about the toxicity of QDs. Thus, we list here the limited number of toxicity studies conducted at four levels of organism complexity (i) in amoeba (as a primary eukaryote), (ii) in plants, (iii) in animals, and (iv) in aquatic life (Valizadeh et al. 2012).

- (i). **In amoeba:** It has been determined that QD labeling had no detectable effect on cell growth and had no deleterious effects on cellular signaling and motility during the development of the *Dictyostelium discoideum* cells (Jaiswal et al. 2003).
- (ii). **In-plant:** The ratio of reduced glutathione levels (GSH) relative to the oxidized glutathione (GSSG) in plants suggests that QDs caused oxidative stress on the plant at this condition (Navarro et al. 2012).
- (iii). **In animal:** Yan et al. investigated the potential vascular endothelial toxicity of mercaptosuccinic acid (2-sulfanylbutanedioic acid)-capped QDs in vitro. Their results suggested that QDs could not only impair the mitochondria but also exert endothelial toxicity through activation of the mitochondrial death pathway and induction of endothelial apoptosis (Yan et al. 2011).

More recently, Chen et al. have studied the cytotoxicity of CdTe/CdS (core-shell) structured and also CdTe/CdS/ZnS (core-shell-shell) structured aqueous synthesized QDs, and their results suggest that the cytotoxicity of CdTe QDs not only comes from the release of Cd²⁺ ions but also intracellular distribution of QDs in cells and the associated nanoscale effects as discussed earlier (Chen et al. 2012).

(iv). **In aquatic ecosystems:** zebrafish embryos provide an economical medium for screening the toxicity of QDs (Fako and Furgeson 2009). Assessment of nanotoxicity can be semi-quantified as sublethal toxicities (viz. survival of the embryo and the severity of phenotypic and gross morphological differences). This screening toolkit allows several parameters to be varied, including concentration, nanomaterial size, chemical composition, density, route of exposure, time of exposure, and the point of embryonic development at which the nanomaterial is administered. To semi-quantify these physicochemical metrics and associated-toxicity in the zebrafish model, a modified scoring spectrum was used based on the phenotypic changes of the zebrafish embryos, ranging from (normal phenotype) 1 (minor phenotypic changes), 2 (moderate alterations), 3 (severe embryo deformation), and 4 (embryo death) (Deng et al. 2018). Unlike traditional biochemical assays that explore specific molecular targets, the zebrafish model relies on the analysis of phenotypic changes. This method allows researchers to bypass several roadblocks commonly associated with current drug discovery efforts, which are based on in vitro biochemical screens followed by in vivo mammalian studies. The zebrafish model, therefore, potentially serves as a rapid and cost-effective method to conservatively assess the toxicity of novel pharmaceuticals, flagging those samples displaying toxicity for closer scrutiny and possible removal from continued drug development.

Most of the current literature on the toxicity of NPs comes from studies on mammalian cells, but it is essential to know their potentially harmful effects on the environment. Frequent detection of NPs in the aquatic environment reflects a rapidly growing number of engineered nanoparticles being used and their incomplete removal during passage through sewage treatment plants and relatively high persistence in water matrices (Farkas et al. 2011; Mühlhling et al. 2009). Particularly, hotspots of NPs could be present in hospital wastewater due to their ever more frequent use in medical applications for drug delivery.

Recent studies have confirmed that NPs are released into the environment and, in particular, the aquatic environment. For example, significant concentrations of nano-Ag can be released from AgNP-containing textiles during washing (Geranio et al. 2009). At the same time, contamination of sewage sludge with Ag and AgNPs has been detected (Kim et al. 2010), and $0.1 \mu\text{g L}^{-1}$ AgNPs have been identified in wastewater effluents (Mitrano et al. 2012). Zinc oxide nanoparticles (ZnO NPs) are also one of the most used NPs, and consequently, they are also significantly dispersed in the environment (Kahru and Dubourguier 2010).

To summarize this section: Environmental risk assessment is required to ensure the safety of nanomaterials and to protect the

Table 3 Results for toxicity associated with indium quantum dots

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
InPZnS QDs	<i>Hydra vulgaris</i>	Direct exposure	70 nM	72 h	Hydra is very susceptible to aquatic pollutants; these QDs may not represent a concrete risk for environmental health	Allocca et al. 2019
Indium-based QDs (CFQD)	Female Lister Hooded rats	IV injection	12.5 mg/kg and 50 mg/kg	90 days	QDs mainly accumulated in the liver and spleen and were excreted from the body gradually and possess good biocompatibility	Yaghini et al. 2018
InZnP and InZnPS QD	Human skin samples	In vitro	6.25–200 nM (cytotoxicity and cell proliferation), 12.5–100 nM (oxidative stress) or 50 nM (comet assay, X-ray absorption spectroscopy, electron microscopy)	24 h	Toxicity of pristine QDs was essentially non-toxic and the toxicity of aged QDs, which proved to be all toxic	Tarantini et al. 2019

Table 4 Results for toxicity associated with other quantum dots

QD	Model	Administration	QD concentration	Exposure duration	Toxicity	Ref
Ag ₂ S QD	Chinese hamster lung fibroblast (V79)	In vitro	5–2000 µg/mL	24 h	The cytotoxic effects of DMSA/Ag ₂ S QDs may occur at high doses through the apoptotic pathways	Vardar et al. 2019
PEGylated CuInS ₂ /ZnS	Male BALB/c mice of 7 weeks old	IV injection	100 µL	90 days	No significant difference in body weight, no histopathological and no biochemical abnormalities	Zou et al. 2019
CQDs	Zebrafish (<i>Danio rerio</i>), zooplankton (<i>Daphnia magna</i>), and phytoplankton (<i>Scenedesmus obliquus</i>)	Direct exposure	0–200 mg/L	96 h (zebrafish) 48 h (<i>D. magna</i> and <i>S. obliquus</i>)	Results indicated trophic level-specific toxicity of CQDs, and the oxidative stress and pH alterations served as potential mechanisms underlying the toxicity of CQDs on <i>S. obliquus</i> , which may separately or jointly disturb the physiological processes in algal cells and affect growth	Yao et al. 2018
PEG-coated Ag ₂ Se	Male CD-1 (ICR) mice	IV injection	8 µmol/kg body weight	28 days	Ag ₂ Se QDs-PEG only showed slight toxicity to the liver at day 28 post-exposure	Tang et al. 2016

environment from unintentional adverse effects. In a regulatory context, this requires reliable and relevant environmental hazard data upon which predicted no-effect concentration (PNEC) values could be estimated. For nanomaterials, it is well-known that ecotoxicity testing is not straightforward and that the applicability of commonly used test guidelines and guidance can be questioned. Nanomaterials are known to behave very differently in ecotoxicity test systems compared to soluble chemicals, for which most guidelines were intended. This current lack of appropriate guidance implies that previous and current guideline-based hazard testing may not be suitable for testing of engineered nanomaterials (ENMs). It further entails that the data, upon which currently available PNEC values have been established, may not correctly reflect the actual ecotoxicity of these ENMs. This means that existing data from non-standard tests—or tests following modified test guidelines—in some cases may provide information on equal or higher reliability compared to strictly guideline-based tests. This would be the case if these modifications were applied to cater for nanomaterial properties and behavior in the test system. Such data should therefore not per se be considered less reliable as a basis for PNEC estimation.

One key area of research is the improvement of stability, safety, and efficacy of NPs through binding to peptides or peptidomimetics. Modifications of the surface of NPs with peptides will allow a reduction of their toxicity and enhancement of stability, while perhaps also determining an improvement of the properties of the peptides. NPs can serve as innovative drug delivery systems for antimicrobial peptides (AMPs) offering the possibility to target the delivery of AMPs to a specific site with controlled-release over time, thus minimizing side effects and increasing efficacy also due to NPs potential multi-valency (Vale et al. 2016; Galdiero et al. 2015). Inorganic nanomaterials have attracted significant attention since they display their antimicrobial activity, which may provide additive or synergistic effects when combined with AMPs (Tal et al. 2002).

Tables 1, 2, 3, and 4 summarize more results for toxicity associated with various QDs available in the literature.

Conclusion

The world of nanomaterials is extremely different from the world of bulk materials. Size-dependent properties make it nearly difficult to generalize when comparing the properties and behavior of different QD. There has been tremendous advancement in material science research after the discovery of QDs. Multiple factors make QDs useful for a wide range of purposes, and more applications are still in exploration. QD research has allowed the fabrication of new classes of QDs having tunable properties using easy preparation processes. Even though these new classes of QDs possess ever-better physical properties, aspects related to their cytotoxicity have

held QD research back. Thus in order to address the challenges of QD research, it is essential to look deeply into what features make QDs toxic. In this review, we have made a detailed survey of recent works reported regarding the toxicity of QDs and summarized the cytotoxicity of QDs at the cellular, organism, and environmental levels. It is evident and worth mentioning that the toxicity of QDs depends on various factors and varies in a complex manner, which makes it difficult to generalize the aspects of toxicity. These factors include the nature of the biological environment, physiological parameters, nature of agent used for surface capping or surface functionalization, the extent of cellular uptake, and also on the nature of the QD employed. Thus there is urgency for novel analytical and predictive tools to provide a clearer understanding of the factors influencing QD toxicity.

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