

Sclerostin-antibody treatment of glucocorticoid-induced osteoporosis maintained bone mass and strength

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Abstract

Summary This study was to determine if antibody against sclerostin (Scl-Ab) could prevent glucocorticoid (GC)-induced osteoporosis in mice. We found that Scl-Ab prevented GC-induced reduction in bone mass and bone strength and that the anabolic effects of Scl-Ab might be partially achieved through the preservation of osteoblast activity through autophagy.

Introduction Glucocorticoids (GCs) inhibit bone formation by altering osteoblast and osteocyte cell activity and lifespan. A monoclonal antibody against sclerostin, Scl-Ab, increased bone mass in both preclinical animal and clinical studies in subjects with low bone mass. The objectives of this study were to determine if treatment with the Scl-Ab could prevent loss of bone mass and strength in a mouse model of GC excess

and to elucidate if Scl-Ab modulated bone cell activity through autophagy.

Methods We generated reporter mice that globally expressed dsRed fused to LC3, a protein marker for autophagosomes, and evaluated the dose-dependent effects of GCs (0, 0.8, 2.8, and 4 mg/kg/day) and Scl-Ab on autophagic osteoblasts, bone mass, and bone strength.

Results GC treatment at 2.8 and 4 mg/kg/day of methylprednisolone significantly lowered trabecular bone volume (Tb-BV/TV) at the lumbar vertebrae and distal femurs, cortical bone mass at the mid-shaft femur (FS), and cortical bone strength compared to placebo (PL). In mice treated with GC and Scl-Ab, Tb-BV/TV increased by 60–125 %, apparent bone strength of the lumbar vertebrae by 30–70 %, FS-BV by 10–18 %, and FS-apparent strength by 13–15 %, as compared to GC vehicle-treated mice. GC treatment at 4 mg/kg/day reduced the number of autophagic osteoblasts by 70 % on the vertebral trabecular bone surface compared to the placebo group (PL, GC 0 mg), and GC + Scl-Ab treatment.

Conclusions Treatment with Scl-Ab prevented GC-induced reduction in both trabecular and cortical bone mass and strength and appeared to maintain osteoblast activity through autophagy.

W. Yao and W. Dai contributed equally to this work.

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Introduction

Patients treated chronically with glucocorticoids (GCs) have decreased bone formation and increased bone resorption and fragility [1, 2]. The mechanisms that account for GC-induced

inhibition of bone formation include the reduction of lifespan and activity of osteoblasts [2]. GCs alter the function of bone-forming cells through multiple pathways that include the reduction of osteoblast proliferation through its suppression of growth factors BMP2 and TGF β 1 [3]; up-regulation of the Wnt antagonists (Dkk-1, Wif-1, and Sost) and down-regulation of the Wnt receptor complex (frizzled 4, 7, Dsh1, and Axin1) [3, 4], which can suppress osteoblast differentiation (alkaline phosphatase, akp2), maturation (osteocalcin), and activity [5, 6]. GCs may also directly affect osteocytes as genes primarily expressed in osteocytes, *Dmp1*, *Phex*, and *Sost* [7] and are associated with bone formation and mineralization, and were up-regulated following GC treatment.

GCs can also alter osteoblast and osteocyte cell viability through autophagy [8–11]. Autophagy is an intracellular digestive mechanism that removes or recycles the dysfunctional organelles and/or oxidized proteins, and functions as a mechanism for nutrient breakdown to maintain cell survival [12, 13]. The role for autophagy as a metabolic regulator for bone cells has been previously reported. Autophagic proteins, including *Atg5*, *Atg7*, and *Atg4b*, are important for generating the osteoclast-ruffled border, corresponding to the secretory function of osteoclasts, and thereby bone resorption activities in vitro and in vivo [14, 15]. Autophagy is activated during osteoblast differentiation, and the skeleton becomes osteogenic when focal adhesion kinase family interacting protein, a key regulator of autophagy induction, is ablated from osteoprogenitor cells [16]. Selective deletion of *Atg 7* in terminally differentiated osteocytes led to an inhibition of bone turnover and an osteoporotic phenotype [17]. Also, autophagy is an active process in most cells to recycle and then remove waste. We observed that GC treatment of osteocytes in vitro induced autophagy in a dose-dependent manner. The autophagic pathway was still present in osteocytes at a GC dose of 0.7–2.1 mg/kg/day, but this protective mechanism was no longer effective when GC dose was increased (5.6 mg/kg/day) [10]. Changes in osteoblast and osteocyte viability may contribute to GC suppression of bone formation [18], and this may contribute to the observation of a the reduction in bone strength [5] that is independent of the bone mass in these experimental models and in patients treated with GCs [19]. Interventions that maintain the viability of osteoblasts and osteocytes in the presence of GCs may be a therapeutic approach for prevention and treatment of GC-induced osteoporosis.

Sclerostin (*Sost*) is a protein produced by osteocytes that can inhibit osteoblast maturation. [20–24]. A monoclonal antibody to sclerostin (*Scl-Ab*) has been developed that can inhibit the activity of sclerostin, and can stimulate bone formation [25, 26]. Our research group reported that GC treatment for 28 days increased *Sost* gene expression [3] and concurrent PTH treatment modestly reduced the *Sost* expression [27]. The effects of *Scl-Ab* on osteoblast viability through

autophagy are not well known. Since chronic GC use can inhibit osteoblast activity and lifespan [3], the objectives of this study were to determine if treatment with a *Scl-Ab* could rescue the GC-induced suppression of bone formation, and to determine if the anabolic effects of the *Scl-Ab* were associated with autophagy in osteoblasts in a mouse model of GC-induced osteoporosis.

Methods

Generation of the dsRed-LC3 reporter mice

Transgenic mice were generated to globally express dsRed fused to LC3, a protein marker for autophagosomes. This mouse line allowed the examination of red fluorescent-LC3 (dsRed-LC3) in autophagic vacuoles in vitro and to identify the autophagic cells, including the osteoblast and osteocytes in vivo. A vector containing a dsRed-LC3 cassette was inserted between the CAG promoter (cytomegalovirus immediate-early (CMVie) enhancer and chicken b-actin promoter) [28] and the SV40 late polyadenylation signal. In this construct, dsRed was fused to the N terminus of rat LC3B (U05784) so as not to affect C-terminal PE conjugation. The 3.4-kbp CAG-dsRed-LC3-SV40 polyA fragment was microinjected into Swiss-Webster fertilized oocytes (Fig. 1a). This approach was derived from the GFP-LC3 transgenic technique that was previously published [29, 30]. The expression of dsRed-LC3 dots (autophagosomes) was confirmed in primary osteoblasts cultured from long bones (Fig. 1b, blue arrows). dsRed-LC3+ cells were observed within the bone marrow, and on bone surface approximate to the calcein-labeled mineralized bone surface (Fig. 1c, white arrows).

Animals and experimental procedures

Two-month-old male dsRed-LC3-reporter mice were maintained on commercial rodent chow (22/5 Rodent Diet; Teklad, Madison, WI) available ad libitum with 0.95 % calcium and 0.67 % phosphate. Mice were housed in a room that was maintained at 20 °C with a 12-h light/dark cycle. The dsRed-LC3-reporter mice were randomized into eight experimental groups. Slow-release pellets (Innovative Research of American, Sarasota, FL) of prednisolone (GC) or placebo were implanted respectively: Group 1, the control group, was implanted with a placebo pellet (PL, $n=10$); groups 2–4 were implanted with slow-release prednisolone pellets, which were equivalent to 0.8, 2.8, and 4 mg/kg/day, respectively ($n=8$ –10/group); group 5 was implanted with PL pellet and received *Scl-Ab* treatment (25 mg/kg, SC, 2 \times /week., $n=7$); and groups 6–8 received GC 0.8, 2.8, or 4 mg/kg/day and *Scl-Ab* treatment (25 mg/kg, SC, 2 \times /week., $n=8$ –10/group). The

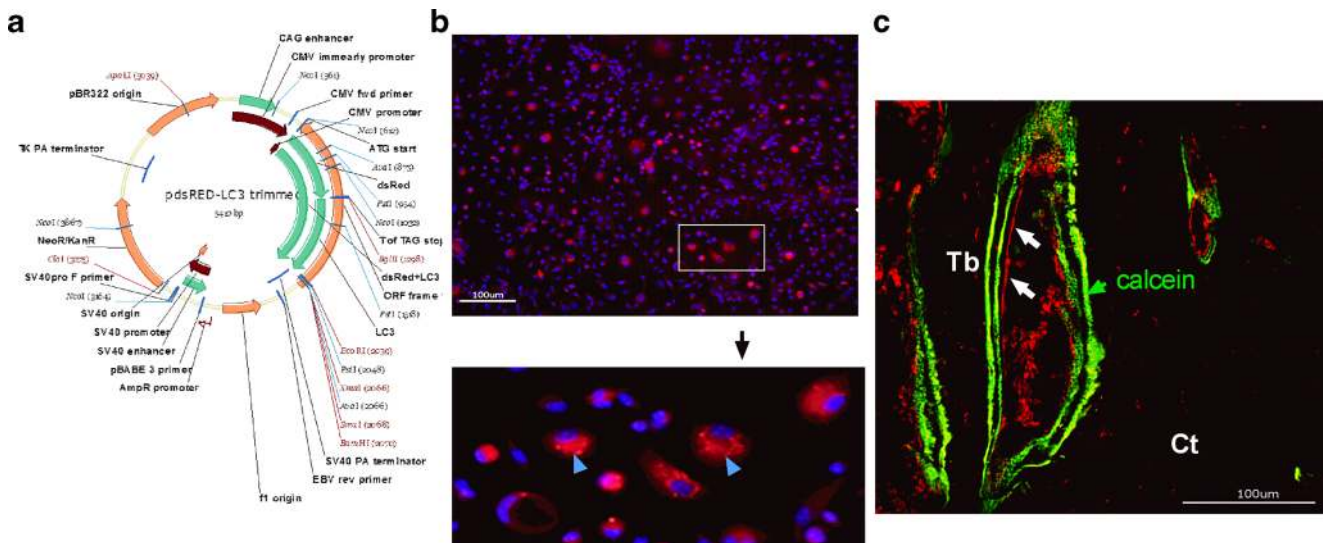


Fig. 1 Generation of the dsRed-LC3 reporter mice. **a** Diagram of the dsRed-LC3 construct. **b** Primary osteoblasts were isolated from long bones of the dsRed-LC3 mice at 1 month of age. A portion of the osteoblasts demonstrated the classic autophagic dots (blue arrow head), a signature appearance for autophagosomes. **c** A representative distal

femur frozen section from a dsRed-LC3 male mouse. Autophagic cells were observed within bone marrow or on the bone surface adjacent to the double calcein-labeled surface (white arrows). Calcein was given to the mice at 20 mg/kg 9 and 2 days prior to sacrifice. *Ct* cortical bone, *Tb* trabecular bone. Scale bar 100 μ m

mice were sacrificed after 3 weeks of treatment. Calcein (20 mg/kg) was injected to all mice 9 and 2 days before sacrifice. All animals were treated according to the USDA animal care guidelines with the approval of the UC Davis Committee on Animal Research.

The mice were fasted for 12 h before sacrifice; serum samples were obtained during necropsy and were stored at -80°C prior to the assessment of biochemical markers of bone turnover. At necropsy, the mice were exsanguinated by cardiac puncture. At the time of sacrifice, the fifth lumbar vertebral body (LVB) and right distal femurs (DF) were used for micro-CT scans. Cryosections were collected from the fourth LVB and the right femoral shafts and used for bone histomorphometry and autophagy evaluations. The sixth LVBs and the left femurs were used for biomechanical compression tests. The right tibiae were used protein extraction for Western blots.

Micro-CT

The fifth lumbar vertebra and right distal femurs were scanned with μ CT (VivaCT 40, Scanco Medical AG, Bassersdorf, Switzerland) at 70 keV and 145 μA with an isotropic resolution of 10.5 μm in all three dimensions. The entire LVB5 was scanned. All trabeculae in the marrow cavity and within cortical shafts were evaluated. Scanning of the DF was initiated at the level of the growth cartilage-metaphyseal junction and extended proximally for 250 slices. Evaluations were performed on 150 slices beginning 0.2 mm proximal to the most proximal point along the boundary of the growth cartilage so as to exclude the growth plates. For each scan, the volume of

interest was defined as ~ 0.25 mm internal to the boundary of the marrow cavity with the cortex. The methods used for calculating trabecular thickness (Tb.Th) and bone mineral density (BMD) have been described previously [5, 31]. For the right mid-femur, the scanning was performed at the middle femur and continued proximally 0.5 mm. All the slides were used to evaluate total volume (TV), cortical bone volume (BV), and cortical thickness (Ct.Th) [32–34].

Biochemical markers of bone turnover

Serum osteocalcin was measured using a Luminex Osteocalcin kit (EMD Millipore, Billerica, MA, USA), and serum CTX-1 was measured by ELISA (Immunodiagnostic Systems Inc., Gaithersburg, MD, USA) following the manufacturer's instructions. The coefficient of variations for these tests in our laboratory was less than 10 %.

Bone histomorphometry

Eight micrometers thick cryosections of the fourth LVB were obtained with a Leica/Cryostat microtome. Bone histomorphometry was performed using a semi-automatic image analysis Bioquant system (Bioquant Image Analysis Corporation, Nashville, TN) linked to a microscope equipped with transmitted and fluorescence light [5]. A counting window, allowing for measurement of the entire trabecular bone and bone marrow within the growth plate and cortex, was created for the histomorphometric analysis. Static measurements included tissue area (T.Ar), bone area (B.Ar), and bone perimeter (B.Pm). Dynamic measurements included single-

(sLS) and double-labeled surface (dLS), autophagic osteoblast surface, and inter-labeled thickness (Ir.L.Th). These indices were used to calculate mineralizing surface (MS/BS) and mineral apposition rate (MAR) and surface-based bone formation rate (BFR/BS) [35, 36]. One section from each mouse was used to stain with tartrate-resistant acid phosphatase for osteoclast measurement (OcS/BS). We used the terminology following the recommendation of the American Society for Bone and Mineral Research [36], and we have reported similar methodology in other experiments in our laboratory [5, 31, 37, 38]. Autophagic osteoblasts were defined as punctuated red-fluorescence staining cells laying on the trabecular surface that co-localized with the calcein labels. The results were presented as the percentage of autophagic osteoblast surface/bone surface [10].

The femoral diaphyses were dissected and fixed in 4 % paraformaldehyde, dehydrated in graded concentrations of ethanol and xylene, embedded un-decalcified in methyl methacrylate, and then cross-sectioned using a SP1600 microtome (Leica, Buffalo Grove, IL) into 40 μm sections. Total cross-sectional bone area (T.Ar), cortical area (Ct.Ar), and cortical width (Ct.Wi) were measured with the Bioquant Image analysis system. Single- and double-labeled surface and inter-labeled width were measured separately at the endocortical (Ec) and periosteal (Ps) bone surfaces. MAR and BFR/BS were calculated thereafter for both the endocortical and periosteal bone surfaces [32, 33, 39].

Real-time RT-PCR

Total RNA was obtained from the tibiae shaft using a modified two-step purification protocol employing homogenization (PRO250 Homogenizer, 10 mm \times 105 mm generator, PRO Scientific IN, Oxford CT) in Trizol (Invitrogen, Carlsbad, CA) followed by purification over a QIAGEN RNeasy column (QIAGEN, Valencia, CA). RNA integrity was monitored by running RNA on 1 % Agarose gel in 120 V for 30 min. Intact RNA has both clear 18S and 28S ribosomal RNA bands with 28S rRNA approximately twice as intense as the 18S rRNA band. RNA was reverse-transcribed to single-stranded cDNA by using High-Capacity cDNA Archive Kit (ABI, California). Gene expressions were presented as fold changes from PL group [3].

Western blot

Tibial cortical bones were lysed in RIPA buffer with homogenization. The bone lysates were resolved on SDS-PAGE and electrophoretically transferred to polyvinylidene difluoride membranes. Membranes were incubated with primary antibodies that include β -actin (Santa Cruz Biotechnology, Santa Cruz, CA), anti-Atg 7, anti-Atg-16L, and anti-LC3 (Cell Signaling Technology, Danvers, MA) followed by species-

specific horseradish peroxidase secondary antibody. Immuno-reactive materials were detected by chemiluminescence (Pierce Laboratories, Thermo Fisher Scientific, Rockford, IL), then were imaged and quantitated by BIO-RAD ChemiDoc MP imaging system and analysis software [10, 40].

Biomechanical testing

For the vertebral bodies, the endplates of the lumbar vertebral body were polished using an 800-grit silicon carbide paper to create two parallel planar surfaces. Before testing, caudal and cranial diameter measurements were taken at the top, middle, and bottom of each vertebrae to obtain six measurements which were averaged as the diameter; the height along the long axis was recorded as well and the vertebrae were modeled as a cylinder. The lumbar vertebra were then loaded to failure under far-field compression along its long axis using an MTS 831 electro-servo-hydraulic testing system (MTS Systems Corp., Eden Prairie, MN) at a displacement rate of 0.01 mm/s with 90 N load cell; the tests were performed in 37 °C HBSS, and sample loads and displacements were continuously recorded throughout each test. Values for the maximum load and the apparent ultimate stress (bone strength) for compression were then determined, where the apparent ultimate stress was calculated using the expression $\sigma = 4P/(\pi d^2)$, where P is the load and d is the average diameter [33, 39, 41].

To analyze the biomechanical properties of the cortical bone, the left femurs were subjected to four-point bending tests, with the bone loaded using an MTS 831 electro-servo-hydraulic testing system (MTS Systems Corp., Eden Prairie, MN) such that the posterior surface was in tension and the anterior surface was in compression; the major loading span was 14.5 mm. Each femur was loaded to failure in 37 °C HBSS at a displacement rate of 0.01 mm/s while its corresponding load and displacement were measured using a calibrated 90 N load cell. Two diameter measurements were taken at the fracture location, and averaged to model the femur as a cylinder. Values for the yield stress and load, maximum load and ultimate stress (bone strength) in the bending tests were then determined, with the apparent stress calculated from $\sigma = PLy/4I$; P is the load, L is the major loading span, y is the distance from the center of mass ($d/2$), and I is the moment of inertia ($\pi d^4/64$), where d is the average diameter [33, 39, 41]. A measure of apparent toughness was estimated in terms of the work of fracture, specifically the area under the load vs. displacement curve normalized by twice the fracture surface area.

Statistical analysis

The group means and standard deviations (SDs) were calculated for all outcome variables. The nonparametric Kruskal-

Wallis test was used to determine the overall differences between the groups followed by Bonferroni post hoc test to compare the treatment groups with PL or GC groups (SPSS Version 14; SPSS Inc., Chicago, IL).

Results

Body weight

Vehicle- or Scl-Ab-treated mice with PL pellets gained body weight from 8 to 11 weeks of age. Mice in the groups treated with GC 2.8 and 4 mg/kg/day groups had nearly a 20 % weight loss from the baseline level during the experiment. Animals treated with Scl-Ab did not alter body weights as compared to the PL or GC vehicle-treated groups (Supplementary Table 1).

Bone volume and bone turnover changes in the trabecular bones

Measurements of trabecular bone at both the lumbar vertebral body (LVB) and the distal femurs (DF) were obtained, and in this manuscript, we report only on the LVB results. For the lumbar vertebra body (LVB), GC at 0.8 and 2.8 mg/kg/day levels did not affect trabecular bone volume/tissue volume (BV/TV), Tb.N, Tb.Th, Conn-Dens, and BMD significantly, while GC 4 mg/kg/day dose decreased BV/TV, Tb.Th, and Conn-Dens by 27, 11, and 19 %, respectively, as compared to the PL (vehicle group ($p < 0.05$)) (Table 1). PL plus Scl-Ab treatment significantly increased the BV/TV compared to PL vehicle alone ($p < 0.05$ vs. PL). The increases in trabecular bone BV/TV were associated with greater Tb.Th and BMD in Scl-Ab-treated groups (Table 1). The changes in the BV/TV of the trabecular bone with GC alone or GC plus Scl-Ab combination treatments were overall more pronounced at the DFM site than the LVB. For example, PL plus Scl-Ab mice increased trabecular bone BV/TV by 139 % as compared to the PL alone. GC-induced reduction in the BV/TV or the

increase in BV/TV with GC and Scl-Ab combination treatment were more pronounced in the DFM than in the LVB that GC + Scl-Ab completely prevented GC-induced bone loss in the DFM (supplementary Table 2).

Dynamic bone turnover was assessed by measuring serum biochemical markers of bone turnover and dynamic histomorphometry on the fourth LVB (Table 2). GC at 4 mg/kg/day decreased serum osteocalcin (OC) by 25 % and increased CTX-1 levels by 68 % compared to the PL ($p < 0.05$ vs. PL). GC at 4 mg/kg significantly decreased MS/MS by 50 % and BFR/BS by 60 % as compared to the PL group ($p < 0.05$ vs. PL). No significant differences in bone turnover markers and bone formation parameters were observed between the lower doses of GC and PL groups. However, Scl-Ab plus PL significantly increased bone formation parameters, MS/BS, MAR, and BFR/BS, by approximately 50 % compared to the PL group treated with vehicle ($p < 0.05$ vs. PL). The Scl-Ab treatments prevented the reduction of bone formation parameters in mice with GC at 4 mg/kg/day. GC at 4 mg/kg or GC + Scl-Ab had significantly higher OcS/BS as compared to the PL plus Scl-Ab group or PL treated with vehicle ($p < 0.05$ vs. PL) (Fig. 2a, Table 2).

Bone volume and bone turnover changes in the cortical bone

Since the trends for total bone volume (TV) and cortical bone volume (BV) were similar for all the groups, we chose to report BV. Compared to the placebo-treated animals, the GC dose of 0.8 mg/kg did not change middle-femoral BV and BMD (Table 3). However, BV was 12 % lowered in GC 4 mg/kg group and BMD was 7 % lower than PL ($p < 0.05$ vs. PL). Also, endocortical bone mineralizing surface was reduced by about 70 % in GC 2.8 and 4 mg/kg/day dose groups ($p < 0.05$ vs. PL). Also, periosteal MS/BS was significantly lowered at GC 4 mg/kg/day dose level and BFR at the periosteal bone surface was reduced by approximately 80 % in both the GC 2.8 and 4 mg/kg/day groups as compared to the PL ($p < 0.05$ vs.

Table 1 Trabecular bone architectural changes measured at the fifth LVB by micro-CT

Treatment groups	N	BV/TV (%)	Tb.N (1/mm)	Tb.Th (mm)	Conn-Dens (1/mm ³)	BMD (mg HA/cm ³)
PL	10	18±5	4.51±0.6	0.047±0.01	224±61	309±47
GC-0.8	8	19±11	4.68±0.7	0.046±0.01	241±42	293±91
GC-2.8	8	20±3	4.73±0.5	0.047±0.00	245±52	296±24
GC-4	10	14±5*	4.27±0.7	0.042±0.01*	184±80*	284±59
PL + Scl-Ab	7	43±6#	5.41±0.3	0.078±0.01#	229±39	541±49#
GC-0.8 + Scl- Ab	8	38±4#	5.07±0.3	0.069±0.01#	195±30	475±31#
GC-2.8 + Scl-Ab	8	31±5#	5.20±0.4#	0.059±0.01#	228±21	411±48#
GC-4 + Scl-Ab	10	30±2#	5.11±0.4	0.059±0.00#	200±25	400±14#

* GC vs. PL $p < 0.05$; # PL/GC + Scl-Ab vs. PL/GC $p < 0.05$ at a same dose level

Table 2 Bone turnover measurements

Treatment groups	Bone markers		Fourth LVB bone histomorphometry			
	OC ($\mu\text{g/mL}$)	CTX-1 ($\mu\text{g/mL}$)	MS/BS (%)	MAR ($\mu\text{m/day}$)	BFR/BS ($\mu\text{m}^2/\mu\text{m}^3/\text{day}$)	OcS/BS (%)
PL	13.0 \pm 1.7	18.5 \pm 1.5	26 \pm 9	1.99 \pm 0.51	0.52 \pm 0.10	0.61 \pm 0.12
GC-0.8	13.6 \pm 0.8	18.1 \pm 4.3	33 \pm 10	1.85 \pm 0.15	0.61 \pm 0.22	0.63 \pm 0.14
GC-2.8	12.9 \pm 1.5	16.3 \pm 3.7	29 \pm 9	1.51 \pm 0.19	0.44 \pm 0.16	0.72 \pm 0.19
GC-4	9.7 \pm 2.3*	31.1 \pm 1.9*	13 \pm 8*	1.36 \pm 0.59*	0.18 \pm 0.10*	0.77 \pm 0.10*
PL + Scl-Ab	12.8 \pm 1.6	26.4 \pm 4.2*	32 \pm 9	2.34 \pm 0.27	0.75 \pm 0.19#	0.48 \pm 0.18
GC-0.8 + Scl-Ab	12.6 \pm 1.9	13.4 \pm 3.4*#	36 \pm 10	1.79 \pm 0.15	0.64 \pm 0.2	0.50 \pm 0.11
GC-2.8 + Scl-Ab	14.2 \pm 0.1	16.0 \pm 0.2*#	42 \pm 3#	1.67 \pm 0.28	0.70 \pm 0.17	0.69 \pm 0.11
GC-4 + Scl-Ab	12.1 \pm 1.5	18.1 \pm 4.3	22 \pm 3#	2.14 \pm 0.45#	0.47 \pm 0.13#	0.87 \pm 0.16*

OC osteocalcin, MS/BS mineralizing surface, MAR mineral apposition rate, BFR/BS bone surface-based bone formation rate, OcS/BS osteoblast surface, OcS/BS osteoclast surface

* GC vs. PL $p < 0.05$; # PL/GC + Scl-Ab vs. PL/GC $p < 0.05$ at a same dose level

PL). PL plus Scl-Ab increased cortical BV by 20 % over PL group alone ($p < 0.05$ vs. PL). Bone formation at the endocortical bone surface was increased by 160 % in PL plus Scl-Ab compared to PL alone ($p < 0.05$ vs. PL). No significant differences were observed in Ec. and Ps-MS

and BFR between vehicle- and Scl-Ab-treated groups in mice treated with lowest dose of GC. Treatment with GC plus Scl-Ab prevented the reduction in both endocortical and periosteal bone formation observed with GC treatment alone (2.8 and 4 mg/kg/day) (Fig. 2b).

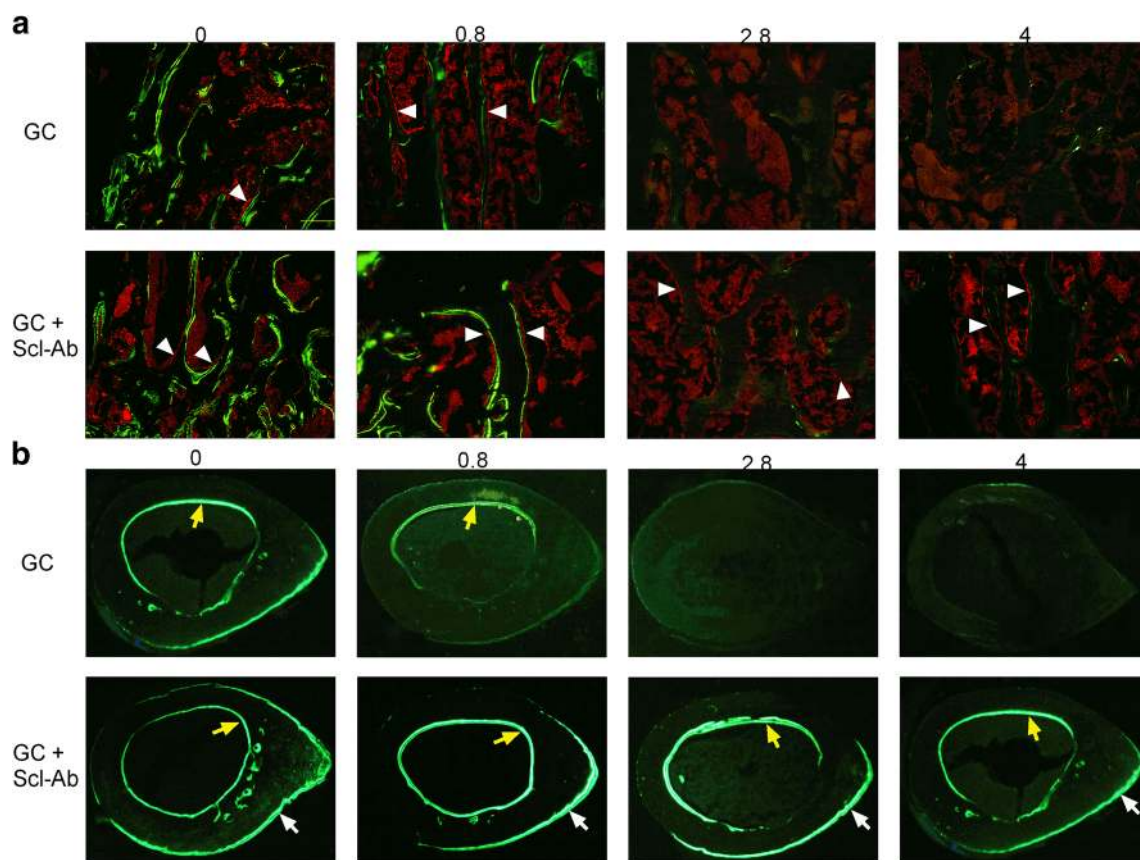


Fig. 2 GC reduced bone formation, which were preserved by Scl-Ab co-treatment. **a** Representative frozen section obtained from the fourth LVB in dsRed-LC3 reporter mice treated with vehicle or various doses of GC or GC plus Scl-Ab. Scale bar 100 μm . **b** Representative cross-sections were

obtained from the middle-femoral shaft. Yellow arrows illustrate double-labeled endocortical surface and white arrow illustrate double-labeled periosteal surface. Original magnification $\times 4$. All the mice received two calcein labels at days 2 and 9 prior to sacrifice

Table 3 Bone structure and bone formation changes measured at the mid-femurs

Treatment group	Micro-CT measurements		Bone histomorphometry measurements			
	BV (mm ³)	BMD (mgHA/cm ³)	Ec-MS/BS (%)	Ec-BFR (μm ² /μm ³ /day)	Ps-MS/BS (%)	Ps-BFR (μm ² /μm ³ /day)
PL	0.530±0.07	1197±16	62.1±18.6	1.33±0.63	47.9±12.9	1.14±0.3
GC-0.8	0.542±0.07	1174±12	71.1±6.4	2.17±0.5	38.2±6.9	1.09±0.3
GC-2.8	0.511±0.08	1112±15*	18.8±7.7*	0±0*	45.3±9.5	0.23±0.3*
GC-4	0.465±0.06*	1170±31	19.8±9.9*	0.12±0.16*	17.0±12.8*	0.21±0.2*
PL + Scl-Ab	0.639±0.07#	1213±14	122.8±52.4	3.47±0.82#	50.4±21.1	1.54±0.6
GC-0.8 + Scl-Ab	0.618±0.04	1183±12	85.5±13.9	2.28±0.75	45.3±9.5	1.58±0.3
GC-2.8 + Scl-Ab	0.565±0.04	1184±17#	78.6±9.7#	1.73±0.49#	38.2±9.3	1.02±0.4#
GC-4 + Scl-Ab	0.547±0.08#	1206±12	69.3±27.1#	0.93±0.79#	34.3±23.5#	0.65±0.8#

BV bone volume, Ec endocortical, Ps periosteal

* GC vs. PL $p<0.05$; # PL/GC + Scl-Ab vs. PL/GC $p<0.05$ at a same dose level

Bone strength

GCs dose-dependently decreased vertebral maximal load and ultimate stress (Table 4). Toughness was reduced by 40 % in the GC 4 mg/kg group compared to the PL group ($p<0.05$ vs. PL). PL plus Scl-Ab treatment increased the apparent ultimate stress and toughness by 31 and 108 %, respectively, as compared to PL alone ($p<0.05$ vs. PL) (Table 4). Maximum load, apparent ultimate stress, and toughness were also greater in Scl-Ab plus GC groups compared with respective controls with significant differences observed in mice with GC treatments of 2.8 and 4 mg/kg/day (Table 4).

Mice treated with GC 0.8 mg/kg/day tended to have higher maximum load and apparent ultimate stress of the femur diaphysis than PL but the overall cortical strength, apparent toughness, was decreased by 30 % compared to PL. Mice treated with GCs at 0.8–2.8 mg/kg/day did not have changes in cortical bone strength compared to the PL group; however, mice treated with the GC at the 4 mg/kg/

day dose had 10–30 % decreased apparent ultimate stress and toughness as compared to PL ($p<0.05$ vs. PL). PL plus Scl-Ab-treated mice had statistically significant increased maximum load and apparent ultimate stress as compared to PL group treated with vehicle. No significant differences in femoral bone strength parameters were observed between vehicle- and Scl-Ab-treated mice with low dose of GC. GC plus Scl-Ab treatment prevented the reduction in apparent ultimate stress and toughness in mice with GC at 2.8 and 4 mg/kg/day alone ($p<0.05$ vs. respective GC group) (Table 4).

Osteoblast autophagic in vivo

Exploratory studies to assess autophagic osteoblasts in vivo were performed in the high-dose GC (4 mg/kg/day) group, and the GC plus Scl-Ab combination treatment group. RNA was extracted from the distal tibia, and each sample included both the cortical shaft and the periosteum. We found the mice treated with GC at 4 mg/kg/

Table 4 Bone strength measurements

Treatment Groups	Lumbar vertebral compression test			Femoral four-point bending test		
	Max load (N)	Apparent ultimate stress (MPa)	Apparent toughness (kJ/m ²)	Max load (N)	Apparent ultimate stress (MPa)	Apparent toughness (kJ/m ²)
PL	32.7±11.2	4.89±1.5	0.39±0.2	13.1±2.1	182±16	2.93±0.9
GC-0.8	23.1±6.4	3.77±1.1	0.56±0.1	19.7±2.0	218±36	1.91±0.2
GC-2.8	16.6±5.0*	2.73±0.7*	0.42±0.1	15.7±1.5	163±23	2.13±0.4
GC-4	12.7±2.8*	2.11±0.3*	0.24±0.1*	13.4±2.5	139±15*	1.68±0.4*
PL + Scl-Ab	46.7±15.8	6.40±2.0	0.81±0.2#	17.9±3.5#	252±44#	3.02±1.3
GC-0.8 + Scl-Ab	36.0±11.5	4.95±1.6	0.65±0.3	21.5±3.8	190±20	1.80±0.4
GC-2.8 + Scl-Ab	30.2±7.4#	5.00±0.9#	0.71±0.1#	18.9±3.4	172±43#	2.41±0.4#
GC-4 + Scl-Ab	21.2±3.6#	3.32±0.4#	0.32±0.1#	15.0±1.2	190±6#	1.94±0.4#

* GC vs. PL $p<0.05$; # PL/GC + Scl-Ab vs. PL/GC $p<0.05$ at a same dose level

day had reduced levels of autophagy-related genes, Atg7 and Atg-16L by 1.8- and 3.4-fold, respectively, in the tibial shafts. Concurrent treatment with GC plus Scl-Ab maintained autophagic gene expression at approximately twofold above PL level (Fig. 3a). We also evaluated the protein levels of autophagy-related proteins (Atg7, Atg-16L, and LC3-II) expressed in the tibial shafts, and found that the levels of the autophagy-related proteins were similar between WT and DsRed-LC3-reporter mice (data not shown). Western blot analyses performed from the tibial shafts found that GC exposure reduced the gene expression of Atg-7, Atg-16L, and the amount of LC3-II/LC3-I by more than 50 %, calculated as a semi-quantitative assessment of the intensity of the Western blots, suggesting reduced induction and formation of autophagosomes. Concurrent treatment with GC plus Scl-Ab maintained the expression of ATG-7 and ATG-16L, and LC3-II at the PL levels (Fig. 3b, c). At the lumbar vertebral body, autophagic osteoblast surface/BS was reduced by nearly 70 % in GC 4 mg/kg group compared to the PL on the vertebral trabecular bone surface ($p < 0.05$ vs. PL). When compared to GC 4 mg/kg/day, high dose alone, GC plus Scl-Ab treatment significantly increased the autophagic osteoblast surface/BS by 133 % as compared to GC alone ($p < 0.05$ vs. GC) (Fig. 3d).

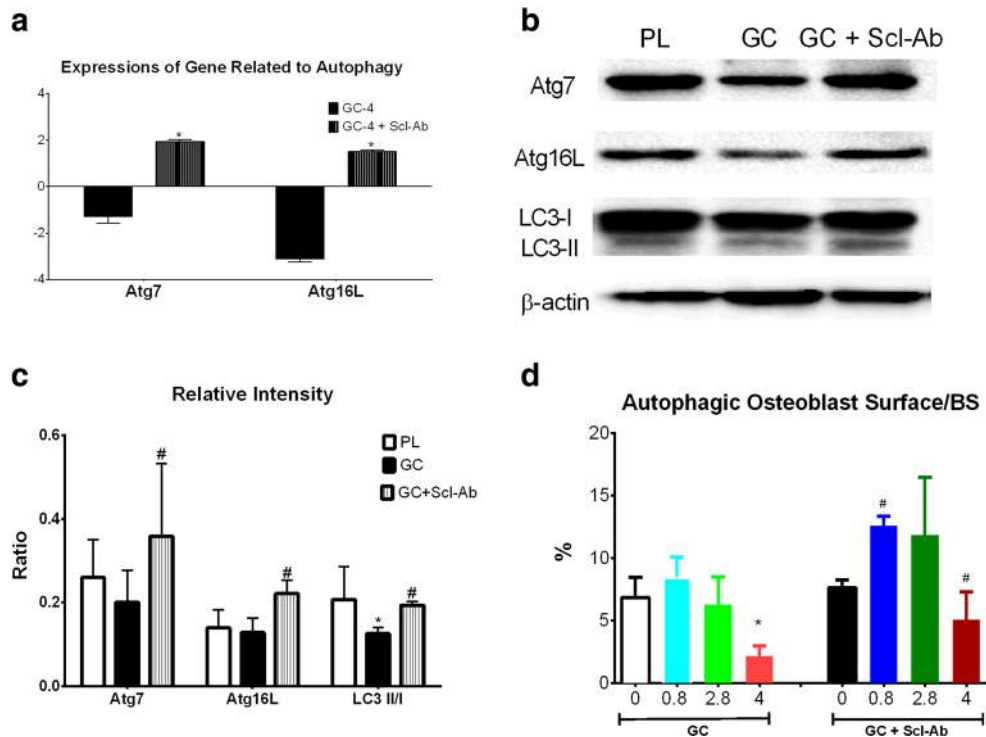


Fig. 3 Activation of autophagy in vivo. **a** RNA was extracted from the tibial cortical bone including periosteum for autophagy quantitative RT-PCR. GC-4 or GC-4 plus Scl-Ab ($n=3$) were used. Gene expression is shown by fold changes from PL group, which was set to "1". **b** Protein was extracted from the tibial cortical bone. Samples were collected from PL, GC-4, or GC-4 plus Scl-Ab, ($n=3$) respectively. Western blotting was

Discussion

Glucocorticoid-induced osteoporosis (GIOP) is the most common cause for secondary osteoporosis as 30–50 % of patients on chronic prednisolone treatment sustain a fracture [42]. Several clinical studies have demonstrated that bisphosphonates increase bone mineral density (BMD) at the spine and hip [43–48] and decrease the incidence of vertebral fractures, especially in post-menopausal women treated with GCs [49]. A new anti-resorptive agent, denosumab, which inhibits RANKL action, also prevented GC-induced loss of bone mass and strength in a hRANKL-knockin mouse model [50], and improved BMD of the lumbar spine and hip in rheumatoid arthritis patients treated with GCs [51]. A bone anabolic agent, rhPTH (1–34), is generally considered as a second-line treatment option for GIOP patients. In clinical studies, rhPTH significantly increased bone formation markers and BMD at the spine and hip in GIOP patients [52–54], and it is more effective than bisphosphonates for increasing spine BMD and reducing the incidence of new vertebral fractures in GIOP-treated populations [47, 55–57].

Sclerostin is a Wnt antagonist that is secreted primarily by osteocytes. Once it is released, it is thought to move through the canaliculi of the osteocytes and into the bone marrow where it will inhibit osteoblast maturation and activity. The

performed for select proteins related to autophagy activation, Atg7 and Atg16L and autophagosome formation (LC3-II/I). **c** Quantitative density evaluation for the Western blots. **d** Quantitative measurement of the autophagic osteoblasts/total osteoblasts at the vertebral trabecular bone surface. * GC vs. PL $p < 0.05$; # PL/GC + Scl-Ab vs. PL/GC $p < 0.05$ at a same dose level

efficacy of Scl-Ab on augmentation of bone formation and bone mass have been demonstrated in intact, estrogen-deficient, hind-limb immobilization rodent models [58–61], as well as in primates and humans [62]. The effect Scl-Ab treatment in glucocorticoid-induced bone loss was studied in 7-week-old BLAB/C mice. The mice were treated with 3 mg/kg/day dexamethasone by oral gavage for up to 9 weeks. GC treatment alone reduced trabecular bone volume and femoral areal BMD, and these changes were prevented by concurrent Scl-Ab treatment of 25 mg/kg, 2×/week [63]. In our study, we used 2-month-old male mice and evaluated if Scl-Ab would prevent the negative effects of GCs on bone formation. We found that Scl-Ab treatment increased bone formation primarily by increasing the osteoblast surface and activity (mineral apposition rate) such that surfaced-based (BFR/BS) and tissue-based (BFR/TV) bone formation were increased. These observations are consistent with other reports of Scl-Ab treatment in intact rats or mice [25, 63, 64], and confirm that Scl-Ab directly stimulates modeling-dependent gain in bone mass [65, 66] resulting in more than 100 % increase in both the vertebral trabecular bone both in mice with or without concurrent GC exposure. The increase in trabecular bone volume was associated with increased trabecular bone thickness and overall bone strength. Treatment with Scl-Ab also increased the mineral apposition at the endocortical bone surface and resulted in higher cortical bone volume and BMD that was associated with significantly higher cortical bone strength.

Interestingly, the lowest dose of GCs used in this study (0.8 mg/kg/day) modestly increased endosteal bone formation and increased trabecular and cortical bone volume compared to the placebo-treated mice. However, higher GC doses of 2.8 and 4 mg/kg/day resulted in a dose-dependent decrease in serum osteocalcin levels, bone formation indices (mineralized bone surface, mineral apposition rate, and bone formation rates), and trabecular bone volume, including trabecular thickness at both the distal femurs and the lumbar vertebrae. Additionally, GCs decreased periosteal bone formation at 2.8 and 4 mg/kg/day doses. However, the combination of GCs plus Scl-Ab was effective in maintaining endocortical and periosteal bone formation, cortical bone volume, and bone strength. Since GCs at 2.8 and 4 mg/kg/day levels reduced the body weights of the study mice by more than 20 %, it was possible that the reduced body weights might have contributed to the GC-induced bone loss as well as the reduction in treatment efficacy with Scl-Ab as the GC dose was increased. Marenzana et al. treated mice with dexamethasone alone and with Scl-Ab [63] and reported a reduction in bone formation when Scl-Ab was combined with higher doses of GCs [3, 27]. Also, a retrospective post hoc analysis was performed on the effects of 18-month clinical study in which nearly 400 patients that were on low (≤ 5 mg/kg/day), medium (> 5 and < 15 mg/kg/day), and high (≥ 15 mg/kg/day) of GCs and treated with Teriparatide (20 μ g/kg/day). It was found that the

increase in lumbar spine BMD was greater in low GC group treated with teriparatide than in the high-dose GC group [67]. These findings suggest that high doses of GCs might impair bone active agents from preserving bone mass and bone strength.

Glucocorticoids have multiple effects on bone cells that alter bone remodeling and induce rapid bone loss [1, 2]. We have demonstrated that GC treatment of mice resulted in an early elevation in the expression of genes involved with osteoclast activities within the first 7 days of GC exposure [3], which was followed by a delayed but prolonged suppression of osteoblastogenesis [3, 68] with reduced bone formation measured by serum osteocalcin and surface-based histomorphometry [34]. Indeed, GC doses of 4 mg/kg significantly reduced the percentages of osteoblasts that underwent autophagy, suppressed bone formation at all bone surfaces, and reduced bone strength at both the trabecular and cortical bone. We also observed preservation of autophagic osteoblasts with Scl-Ab plus GC treatment that with GC alone suggesting that Scl-Ab treatment may sustain osteoblast viability which was otherwise depressed by GC excess. It is extremely challenging to monitor the level of autophagy in bone. Nevertheless, we used multiple approaches such as RT-PCR, Western blotting, and the dsRed-LC3 reporting mouse line to monitor osteoblast autophagy at the tissue level. We found that the higher GC dose level (4 mg/kg/day) suppressed autophagic gene expression and reduced autophagic osteoblast surface while GC (4 mg/kg/day) plus Scl-Ab maintained the autophagic osteoblasts at the placebo levels. These data support a mechanism for the Scl-Ab to override the suppressive effects of GC on bone formation and bone strength by partially maintaining the viability of bone forming cells through autophagy.

This study has a number of strengths including a validated mouse model for GIOP and the use of a number of doses of glucocorticoids to determine a dose response for the study endpoints. We explored the potential mechanism of Scl-Ab on autophagy, via a novel dsRed-LC3 reporter mouse line. However, there are also a number of limitations. We only studied male mice and at one time point (21 days). Also, we only addressed the effect of Scl-Ab on prevention of GC-induced bone loss, and we did not evaluate the therapeutic effects of Scl-Ab in this model. Lastly, we used young mice with skeletons that were still maturing and accruing bone mass. To confirm our results and allow for extrapolation to older age groups, our studies will need to be repeated in older animals. The shortcoming of this mouse line is that it is a global reporting mouse line, and all cells undergoing autophagy express dsRed fluorescent. Another interesting finding from this study is that we found Scl-Ab by itself tended to lower osteoclast number but increase serum CTX-1. We have carefully reviewed the CTX-1 data from all study groups, and we truly have no explanation as to why the CTX-1 level was

higher in the placebo plus sclerostin-antibody group. While we tend to be confident that CTX-1 is a good reflection of bone turnover or osteoclast activity; in this case, we cannot be sure because osteoclast surface was not significantly different in the placebo plus Scl-Ab groups. One possible explanation is that the Scl-Ab could augment RANKL release from osteocytes and osteoblasts during the treatment, which could increase osteoclast activity and CTX-1 levels. While serum RANKL levels were not measured in this study, we did measure serum levels of OPG, and it was not different in the placebo plus Scl-Ab group as compared to the placebo. Additionally, Scl-Ab might presumably block endogenous sclerostin activity and if the high-dose GC treatment induced osteocyte apoptosis and reduced sclerostin synthesis and activity, Scl-Ab treatment may have been less efficacious. However, it is beyond the scope of this report to study apoptosis, and we do not have *ex vivo* data regarding the live/dead ratio of osteocytes that would have supported this potential mechanism.

In summary, treatment of young male mice with GCs at 2.8 or 4 mg/kg/day doses for 21 days reduced bone formation, bone mass, and bone strength of both the trabecular and cortical bone. Treatment with a Scl-Ab prevented the detrimental effects of GCs on bone formation, and improved both trabecular architecture and integral bone strength. These findings warrant further evaluation of Scl-Ab in patients on chronic glucocorticoids.

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Conflicts of interest Wei Yao, Weiwei Dai, Li Jiang, Evan Yu-An Lay, Zhendong Zhong, Robert O. Ritchie and Nancy Lane declare that they have no conflict of interest. Xiaodong Li and Huazhu Ke were employees of Amgen at the time when the study was performed.

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