

# Sensitivity of Edge Detection Methods for Quantifying Cell Migration Assays

Katrina K. Treloar<sup>1,2</sup>, Matthew J. Simpson<sup>1,2\*</sup>

**1** School of Mathematical Sciences, Queensland University of Technology, Brisbane, Queensland, Australia, **2** Institute of Health and Biomedical Innovation (IHBI), Queensland University of Technology, Brisbane, Queensland, Australia

## Abstract

Quantitative imaging methods to analyze cell migration assays are not standardized. Here we present a suite of two-dimensional barrier assays describing the collective spreading of an initially-confined population of 3T3 fibroblast cells. To quantify the motility rate we apply two different automatic image detection methods to locate the position of the leading edge of the spreading population after 24, 48 and 72 hours. These results are compared with a manual edge detection method where we systematically vary the detection threshold. Our results indicate that the observed spreading rates are very sensitive to the choice of image analysis tools and we show that a standard measure of cell migration can vary by as much as 25% for the same experimental images depending on the details of the image analysis tools. Our results imply that it is very difficult, if not impossible, to meaningfully compare previously published measures of cell migration since previous results have been obtained using different image analysis techniques and the details of these techniques are not always reported. Using a mathematical model, we provide a physical interpretation of our edge detection results. The physical interpretation is important since edge detection algorithms alone do not specify any physical measure, or physical definition, of the leading edge of the spreading population. Our modeling indicates that variations in the image threshold parameter correspond to a consistent variation in the local cell density. This means that varying the threshold parameter is equivalent to varying the location of the leading edge in the range of approximately 1–5% of the maximum cell density.

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\* E-mail: matthew.simpson@qut.edu.au

## Introduction

Cell migration plays a key role in development [1,2], repair [3–5] and disease [6,7]. Abnormalities in cell migration are associated with malignant spreading [7–9] and slowed wound repair [10]. Potential therapies aimed at treating these abnormalities may seek to manipulate the rate of migration by applying pharmaceutical drugs or topical treatments [8,10,11]. Development and validation of such therapies can be assessed by comparing assays performed under control conditions with an equivalent assay where the treatment has been applied [12]. *In vitro* migration assays can also be used to quantify the role of experimental variations such as the influence of different substrates [3,4]. Regardless of the purpose for performing an *in vitro* cell migration assay, image detection methods that can be used to quantify the rate of cell migration are an essential element of interpreting and quantifying such assays.

Various types of assays have been used to study cell migration including two-dimensional scratch assays [3,4] and three-dimensional Transwell assays [13,14]. More recently, two-dimensional circular barrier assays have become a popular alternative to scratch assays [15] since they do not damage the cell monolayer, or the substrate, and are therefore thought to be more reproducible than scratch assays [8,16]. Barrier assays are performed by placing a population of cells inside a circular barrier. The barrier is lifted and the subsequent spreading of the

population is measured [17]. An essential element of interpreting and quantifying a barrier assay is to locate the position of the leading edge of the spreading population so that the rate at which the cell population spreads across the substrate can be calculated.

A common approach to quantify the cell migration rate in a barrier assay is to report the percentage change in area [15,16,18–20]. This can be expressed as

$$M(t) = \frac{A(t) - A(0)}{A(0)} \times 100, \quad (1)$$

where  $A(0)$  is the initial area enclosed by the population of cells,  $A(t)$  is the area enclosed by the population of cells at time  $t$ , and  $M(t)$  is the percentage change in area at time  $t$ .

Estimates of cell migration rates using equation (1) are often obtained by hand tracing the area enclosing the spreading cell population on an image of the assay [21,22]. Unfortunately, hand tracing the area enclosed by the leading edge of a spreading cell population is subjective [23]. To overcome this limitation, automated image analysis software, including ImageJ [24] and MATLAB's Image Processing Toolbox [25], have become important alternatives to hand tracing [8,26]. These software tools use edge detection and segmentation algorithms to determine the location of the leading edge of the spreading cell population. This data can then be used to quantify the cell migration rate in

terms of equation (1). In addition to using automatic edge detection algorithms, it is also possible to implement user-defined edge detection options in MATLAB's Image Processing Toolbox [25] so that the user has complete control over the choice of image detection thresholds.

Since there is no standardized method for quantifying the location of the leading edge in a barrier assay, it is often difficult, if not impossible, to meaningfully compare published measures of cell migration in terms of equation (1). This difficulty is exacerbated by the fact that previously published results have been obtained using different image analysis techniques and the details are not always reported [27–31]. To address this limitation, here we apply three different edge detection techniques to a set of images from a two-dimensional barrier assay describing the collective spreading of a population of 3T3 fibroblast cells. We apply three different edge detection techniques to the same experimental data set and compare results from two commonly used automatic edge detection techniques and one manual edge detection technique. Our results indicate that the location of the leading edge is sensitive to the details of the edge detection procedure and this can lead to significantly different quantitative estimates of cell migration. Using a reasonable range of threshold values we show that estimates of cell migration, given by equation (1), can vary by as much as 25% for the same data set.

To provide further insight into the edge detection techniques, we also interpret our results using a mathematical model to quantitatively describe the temporal cell spreading process associated with the barrier assay. Using previously-determined estimates of the cell diffusivity [17], we show that the location of the leading edge, as defined by the image detection methods, corresponds to contours of cell density in the range of approximately 1–5% of the maximum cell packing density. Comparing the location of the leading edge determined by the image detection methods and the mathematical model of the cell spreading provides us with a simple, but meaningful, physical interpretation of the threshold parameters used in the image detection methods.

## Materials and Methods

### 0.1 Experimental Methods

Murine fibroblast 3T3 cells (ATCC, CCL-92, Manassas, VA, USA) were grown in T175 cm<sup>2</sup> tissue culture flasks (Nunc, Thermo Scientific, Denmark) using Dulbecco's modified Eagle medium (Invitrogen, Australia) supplemented with 5% fetal calf serum (FCS) (Hyclone, New Zealand), 2mM L-glutamine (Invitrogen) and 1% v/v Penicillin/Streptomycin (Invitrogen) in 5% CO<sub>2</sub> at 37°C. Prior to confluence, cells were lifted using 0.05% trypsin (Invitrogen, Australia) and viable cells were counted using a Trypan blue exclusion test and a haemocytometer.

Cell migration experiments were performed using a circular barrier assay. Metal-silicone barriers, 6 mm in diameter (Aix Scientifics, Germany), were cleaned, sterilized, dried and placed in the center of the wells in a 24-well tissue culture plate with 500  $\mu$ L of culture medium. The wells in tissue culture plate have a diameter of 15.6 mm.

Two different densities of cell suspensions were used: 10,000 and 30,000 cells/ $\mu$ L. Ten  $\mu$ g/mL Mitomycin-C (Sigma Aldrich, Australia) was added to the cell solutions for one hour to inhibit cell proliferation [32]. One  $\mu$ L of cell suspension was carefully inserted in the barrier to ensure that the cells were approximately evenly distributed. Once seeded, the tissue culture plate was left for one hour in a humidified incubator at 37°C and 5% CO<sub>2</sub> to allow the cells to attach to the surface. After the cells attached to the surface, the barriers were removed and the cell layer was washed

with serum free medium (SFM; culture medium without FCS) and replaced with 0.5 mL of culture medium. Plates were incubated at 37°C in 5% CO<sub>2</sub> for four different times,  $t=0, 24, 48$  and 72 hours. Each barrier assay, for each time point, was repeated three times.

Images of the spreading cell population were obtained by fixing cells with 10% formalin, followed by 0.01% crystal violet (Sigma-Aldrich, Australia). The stain was rinsed with phosphate-buffered saline (Invitrogen, Australia) and the plates were air-dried. Images were acquired using a stereo microscope with a Nixon digital camera (DXM1200C).

### 0.2 Edge Detection Methods

Three methods were used to detect the location of the leading edge: (i) a manual detection method written using MATLAB's Image Processing Toolbox (version 7.12) [25], (ii) an automated method using MATLAB's Image Processing Toolbox (version 7.12) [25] and (iii) an automated method using ImageJ (version 1.46r) [24]. All three methods are based on a Sobel edge detection algorithm [33] but differ in the way that the thresholds are chosen. Although different edge detection methods are available, such as the active contour method [34] and the Canny method [35,36], we choose to focus on MATLAB and ImageJ implementations of the Sobel method since these software tools are widely available.

**0.2.1 Manual edge detection using the MATLAB image processing toolbox.** Customized image processing software was written using the MATLAB Image Processing Toolbox [25]. The following procedure was used to detect the location of the leading edge of the spreading population. The image was imported (*imread*) and converted from color to grayscale (*rgb2gray*). The Sobel method was applied to the grayscale image by specifying a sensitivity threshold value  $S$ , in which all edges weaker than  $S$  are excluded (*edge[grayscale image, 'Sobel', S]*). The lines in the resulting image were dilated to show the outlines of detected edges (*strel(7), imdilate*). Remaining empty spaces in the images were filled and all objects disconnected from the leading edge were removed (*imfill, imclearborder*). The image was smoothed and filtered to remove any noise (*imerode, medfilt2*) and the area enclosed by the detected leading edge was estimated (*regionprops*).

Before we analyzed the experimental images, we undertook a preliminary step where we applied a wide range of threshold values to our experimental images,  $S \in [0.001, 0.5]$ . We found that thresholds in the range  $S \in [0.01, 0.08]$  produced visually reasonable results.

**0.2.2 Automatic edge detection using the MATLAB Image Processing Toolbox.** The manual edge detection method described in section 0.2.1 can be implemented in an automated mode by allowing the MATLAB Image Processing toolbox to automatically determine the threshold,  $S$ , for each individual image [25]. The following procedure was used to detect the location of the leading edge. The image was imported (*imread*) and converted from color to grayscale (*rgb2gray*). The Sobel method was applied in the automatic mode (*edge[grayscale image, 'Sobel']*). The lines in the resulting image were dilated (*strel(7), imdilate*). Remaining empty spaces were filled and all objects disconnected from the leading edge were removed (*imfill, imclearborder*). The image was smoothed and filtered (*imerode, medfilt2*) and the area enclosed by the detected leading edge was estimated (*regionprops*).

**0.2.3 Automatic edge detection using ImageJ.** ImageJ software [24] was used to automatically detect the position of the leading edge. For all images, the image scale was set (*Analyze-Set scale*) and color images were converted to grayscale (*Image-Type-32bit*). The Sobel method was used to enhance edges (*Process-Find Edges*). The image was sharpened (*Process-Find Edges*) and an

automatically determined threshold was applied (*Image-Adjust-Threshold-B&W-Apply*). After applying the Sobel method again (*Process-Find Edges*), the wand tracing tool, located in the main icons box, was used to select the detected leading edge. The area enclosed by the detected leading edge was calculated (*Analyze-Set Measurements-area, Analyze-Measure*).

### 0.3 Mathematical Modeling Tools

To provide a physical interpretation of our image analysis results, we use a mathematical model to relate the edge detection results to the spatial distribution of the cell density. We model the spreading population of cells using a linear diffusion equation [3–5], with previously determined values of the cell diffusivity [17]. The effects of cell proliferation are neglected in our mathematical model, and this is consistent with our experimental protocol where cells were pretreated with Mitomycin-C to suppress cell proliferation [32].

To relate our edge detection results to the cell density, we consider the solution of the two-dimensional axisymmetric diffusion equation.

$$\frac{\partial c}{\partial t} = D \left( \frac{\partial^2 c}{\partial r^2} + \frac{1}{r} \frac{\partial c}{\partial r} \right), \quad (2)$$

where  $r$  is radial position,  $t$  is time,  $c(r,t)$  is the non-dimensional cell density and  $D$  is the cell diffusivity, which is a measure of random, undirected, cell motility [17,37]. The non-dimensional cell density is obtained by scaling the dimensional cell density,  $\bar{c}(r,t)$ , by the carrying capacity density  $K$ . This gives  $c(r,t) = \bar{c}(r,t)/K$ , with  $c(r,t) \in [0,1]$ . The carrying capacity density is estimated by assuming that the maximum packing density of cells corresponds to a square packing density. The average cell diameter is  $25 \mu\text{m}$ , giving  $K \approx 1.6 \times 10^{-3}$  cells per  $\mu\text{m}^2$  [17].

We solve equation (2) on the domain  $0 \leq r \leq 7.8 \text{ mm}$ . The boundary at  $r = 0 \text{ mm}$  corresponds to the center of the well and we apply a symmetry condition,  $\partial c / \partial r = 0$ , here [38]. The boundary at  $r = 7.8 \text{ mm}$  corresponds to the outer edge of the well which is a physical boundary and so we apply a zero flux boundary condition here. The boundary condition at  $r = 7.8 \text{ mm}$  is irrelevant for our barrier assay results since the leading edge of the spreading cell front did not reach this boundary on the time scale of the experiments [17]. The initial condition is given by,

$$c(r,0) = \begin{cases} c_0, & 0 \leq r < 3.0 \text{ mm}, \\ 0, & 3.0 \leq r \leq 7.8 \text{ mm}, \end{cases} \quad (3)$$

where  $c_0$  is the density of cells initially inside the barrier. Assuming that the cells have an average diameter of  $25 \mu\text{m}$  [17], we can pack  $3000/25$  cells across the radius of the barrier. Hence, we estimate that the maximum number of cells that can be packed in a monolayer in the barrier is  $\pi r^2 = \pi(3000/25)^2 = 45,239$ . To specify the initial condition using for equation (3), we assume that either 10,000 or 30,000 cells are uniformly distributed within the barrier giving  $c_0 = 10,000/45,239 \approx 0.22$  and  $c_0 = 30,000/45,239 \approx 0.66$ , respectively.

Numerical solutions of equation (2) are obtained using a finite-difference approximation on a grid with a uniform grid spacing of width  $\delta r$ , and implicit Euler stepping with uniform time steps of duration  $\delta t$  [39,40].

## Results

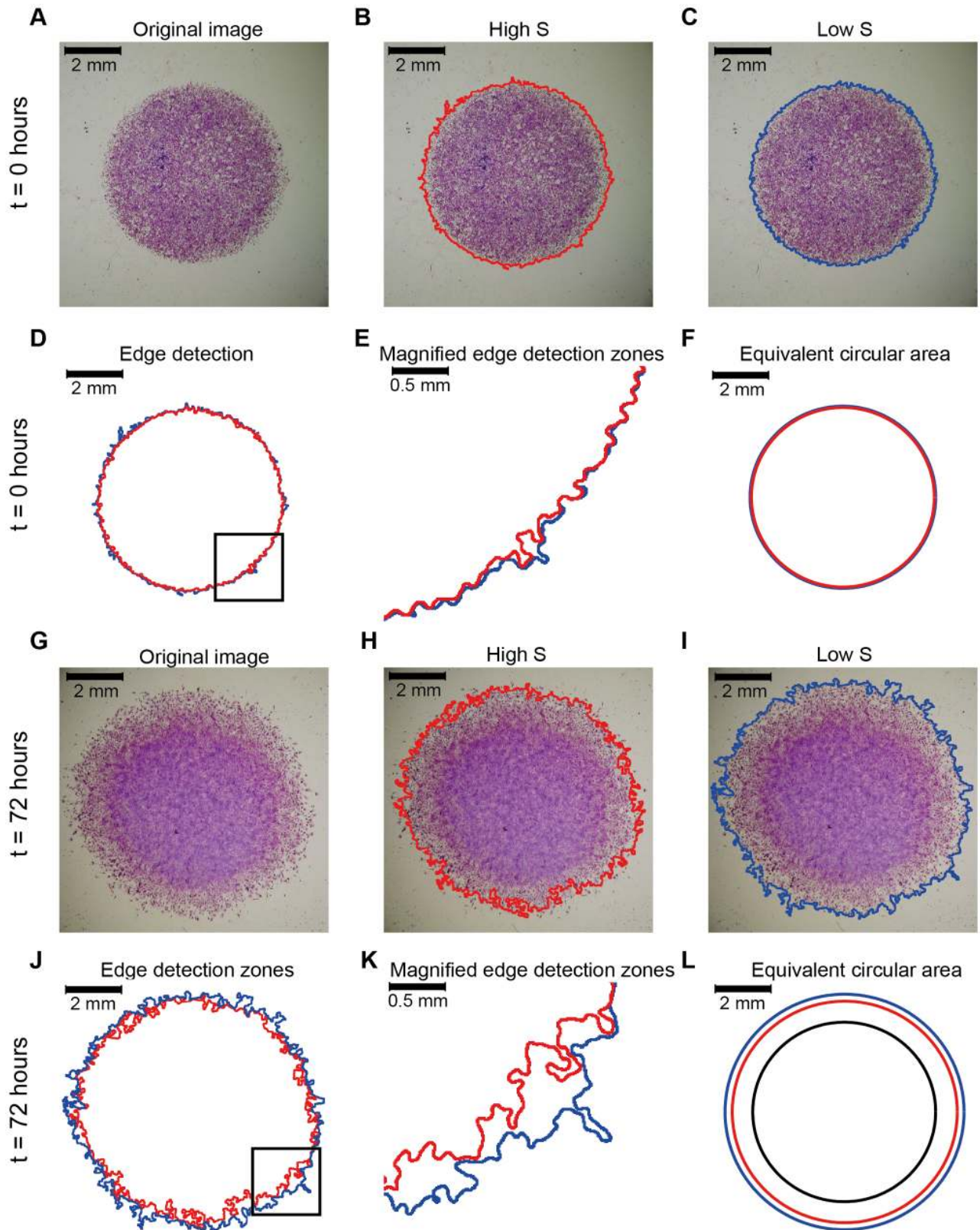
### 0.4 Locating the Leading Edge

To demonstrate the sensitivity of different image processing tools, we apply the manual edge detection method, with different threshold values, to images showing the entire spreading populations in several different barrier assays. Images in Fig. 1A and Fig. 1G show the spreading population in a barrier assay with 30,000 cells at  $t = 0$  and  $t = 72$  hours, respectively. Visually, the leading edge of the cell population at  $t = 0$  (Fig. 1A) appears to be relatively sharp and well-defined. In contrast, the leading edge of the cell population at  $t = 72$  hours (Fig. 1G) is diffuse and less well-defined. This indicates that it is difficult to visually identify the location of the leading edge after the barrier has been lifted and the cell population spreads outwards, away from the initially-confined location.

Our visual interpretation of the images indicate that the precise location of the leading edge is not always straightforward to define. To explore this subjectivity, we use the manual edge detection method (section 0.2.1) by specifying different values of the Sobel threshold,  $S$ . Results in Fig. 1B and Fig. 1C show the detected leading edges at  $t = 0$  hours using a high threshold ( $S = 0.0800$ ) and a low threshold ( $S = 0.0135$ ), respectively. For both thresholds, the detected leading edges appear to be appropriate representations of the leading edge of the spreading population, and are very similar to each other. Results in Fig. 1H and Fig. 1I show the detected leading edges at  $t = 72$  hours for a high threshold ( $S = 0.0565$ ) and a low threshold ( $S = 0.0135$ ), respectively. Both detected edges at  $t = 72$  hours appear to be reasonable approximations to the location of the leading edge of the spreading population, however they are very different to each other which indicates that the results are sensitive to  $S$ .

To qualitatively compare the two leading edges detected at  $t = 0$  hours (Fig. 1B and Fig. 1C) we superimpose the two detected leading edges in Fig. 1D and show a magnified portion of these edges in Fig. 1E. The superimposed edges confirm that the choice of  $S$  has relatively little influence at  $t = 0$  hours. We now compare equivalent results at  $t = 72$  hours from Fig. 1H and Fig. 1I. Superimposing the two leading edges for high and low  $S$  thresholds in Fig. 1J indicates that there is a distinct difference between them. A magnified portion of the detected leading edges is shown in Fig. 1K which also supports our initial observation that it is difficult to visually delineate the leading edge of the spreading population when the leading edge is diffuse.

Our edge detection results at  $t = 0$  hours and  $t = 72$  hours, in Fig. 1A–E and Fig. 1G–K, qualitatively indicate that the threshold value is important in detecting the edge at a later time. To quantitatively compare our edge detection results, we calculate the area enclosed by the detected leading edge and convert this area into an equivalent circle with radius  $\sqrt{A/\pi}$ . Results in Fig. 1F show the equivalent circular areas for low and high thresholds at  $t = 0$  hours. The area of the low and high thresholds are  $32.2 \text{ mm}^2$  and  $31.1 \text{ mm}^2$ , respectively, giving a relatively small difference of  $1.1 \text{ mm}^2$ . These two circles are almost visually indistinguishable at the scale shown in Fig. 1F, confirming there is very relatively little difference regardless of the threshold. Equivalent circular areas in Fig. 1L show the low and high threshold areas at  $t = 72$  hours superimposed on the initial area. The area of the two outer circles in Fig. 1L is  $52.9 \text{ mm}^2$  and  $60.8 \text{ mm}^2$ , giving a relatively large difference of  $7.9 \text{ mm}^2$ . If we take the initial area to be  $A(0) = 31.1 \text{ mm}^2$  then equation (1) gives us  $M(72) = 70.1\%$  for the high threshold leading edge in Fig. 1H and  $M(72) = 95.5\%$  for the low threshold leading edge in Fig. 1I. These results indicate that the



**Figure 1. Locating the leading edge in a barrier assay.** Images of barrier assays containing 30,000 cells at  $t=0$  hours (A–F) and  $t=72$  hours (G–L). (A,G): Images from the barrier assay. (B,H): Leading edge for a high threshold  $S$  in red, superimposed on an image of the spreading population. (C,I): Leading edge for a low threshold  $S$  in blue, superimposed on an image of the spreading population. (D,J): Comparing high and low  $S$  detected edges at  $t=0$  hours. (E,K): Detailed comparison of the detected edges in the boxed area in D and J. (F,L): Comparing equivalent circular areas. The black line in (L) shows the initial circular area. Scales are given in each subfigure. doi:10.1371/journal.pone.0067389.g001

increase in area enclosed within the leading edge of the spreading cell population is very sensitive to the choice of threshold and the results can vary by as much as 25%.

### 0.5 Comparing Edge Detection Techniques

To explore and quantify the sensitivity in detecting the leading edge for our barrier assays, we now extend our initial investigation and detect the location of the leading edge across all experimental images acquired at different time points. We applied the manual edge detection technique to all images using thresholds within the range  $S \in [0.015, 0.8]$ . For each threshold value, we calculated the area enclosed by the detected leading edge and we analyzed the images from each experimental replicate separately so that we could calculate the mean area enclosed by the leading edge,  $\langle A(t) \rangle$ . We estimated the variability amongst the experimental replicates by calculating the standard deviation about the mean,  $\sigma$ . Our results are summarised in Table 1, where we see that the variability amongst the experimental replicates is small with typical values of  $\sigma / \langle A(t) \rangle < 5\%$ . From this point onward we will report all our experimental results in terms of the mean area,  $\langle A(t) \rangle$ , and for convenience we will drop the angle bracket notation.

We now compare the sensitivity of our manual edge detection results by analyzing the images at using a range of threshold values for several different time points for barrier assays with two different initial cell densities. Results in Fig. 2A and Fig. 2B show the relationship between the average area enclosed by the detected leading edge and the threshold value  $S$  for a barrier assay with 10,000 and 30,000 cells, respectively. Initially, for the barrier assay with 10,000 cells, the minimum average area enclosed by the detected leading edge is 27.4 mm<sup>2</sup> and the maximum area is 30.1 mm<sup>2</sup>. For the barrier assay with 30,000 cells, the minimum and maximum initial average area enclosed by the detected leading edge is 31.1 mm<sup>2</sup> and 33.5 mm<sup>2</sup>, respectively. For both initial cell densities, the difference between the maximum and minimum detected initial area is relatively small compared to the differences we observe at later times, as we will now demonstrate.

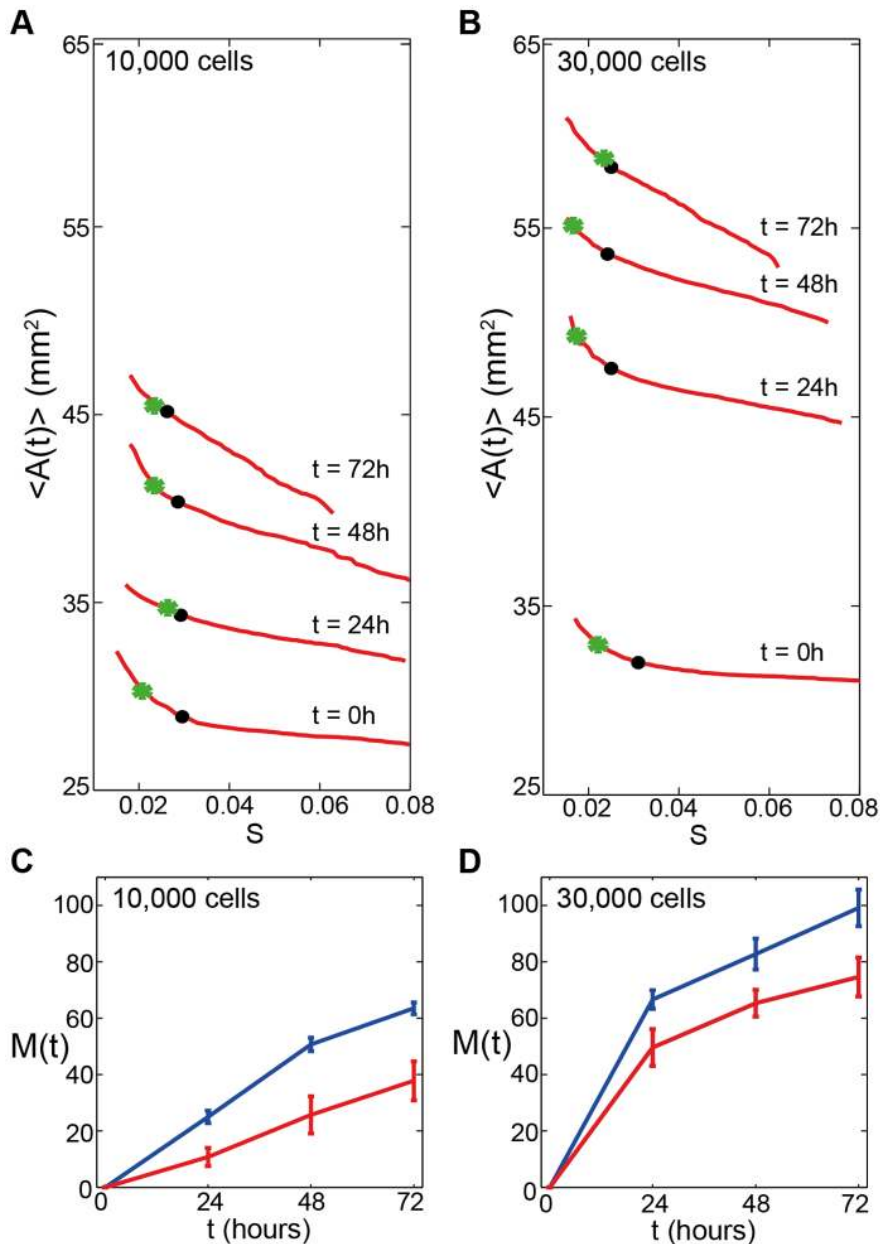
Results in Fig. 2A and Fig. 2B show that the average area enclosed by the detected leading edges increases with time as the cell population spreads outwards from the barrier. We expect that the sensitivity in detecting the location of the leading edge will increase with time as the population spreads and the leading edge becomes increasingly diffuse. For the barrier assays initialized with 10,000 cells, results in Fig. 2A show that the minimum area detected at  $t=24$  hours is 31.9 mm<sup>2</sup> and the maximum area detected is 36.0 mm<sup>2</sup>, giving a difference of 4.1 mm<sup>2</sup>. At  $t=48$  hours the minimum area is 36.2 mm<sup>2</sup> and the maximum area is 43.4 mm<sup>2</sup>, giving a difference of 7.2 mm<sup>2</sup>. At  $t=72$  hours, the minimum area is 39.7 mm<sup>2</sup> and the maximum area is 47.1 mm<sup>2</sup>, giving a relatively large difference of 7.4 mm<sup>2</sup>. These results indicate that the sensitivity in detecting the leading edge is relatively large and that the results depend on the choice of the threshold, and this sensitivity increases with time as the leading edge of the spreading population becomes increasingly diffuse.

Equivalent manual edge detection results for barrier assays containing 30,000 cells in Fig. 2B show similar trends to the results previously reported for the barrier assays with 10,000 cells. The minimum detected average areas at 24, 48 and 72 hours are 44.8 mm<sup>2</sup>, 50.0 mm<sup>2</sup> and 52.9 mm<sup>2</sup>, while the maximum detected average areas are 50.3 mm<sup>2</sup>, 55.5 mm<sup>2</sup> and 60.8 mm<sup>2</sup>, respectively. Comparing the minimum and maximum average areas for the barrier assay with 30,000 cells gives differences of 5.5 mm<sup>2</sup>, 5.5 mm<sup>2</sup> and 7.9 mm<sup>2</sup> at  $t=24$ , 48 and 72 hours, respectively.

**Table 1.** Edge detection area (mm<sup>2</sup>) results.

Number of Cells	Time (hours)	Mean Area (mm <sup>2</sup> )		Standard Deviation (mm <sup>2</sup> )		Mean Area (mm <sup>2</sup> )		Standard Deviation (mm <sup>2</sup> )	
		Manual S High	Manual S Low	Manual S High	Manual S Low	ImageJ	Auto ImageJ	Matlab	Auto Matlab
10,000	0	27.4	30.1	0.67	1.61	30.3	0.83	29.0	1.64
	24	31.9	36.0	0.91	0.63	35.0	2.26	34.2	0.78
	48	36.2	43.4	1.91	0.68	41.3	1.11	39.1	2.64
	72	39.7	47.1	1.98	0.62	45.8	0.81	44.6	0.81
30,000	0	31.1	33.5	0.21	0.34	33.1	1.40	30.0	1.56
	24	44.8	50.3	2.11	1.08	49.9	1.40	45.0	2.12
	48	50.0	55.5	1.52	1.78	55.2	1.57	51.4	1.47
	72	52.9	60.8	2.25	2.11	55.9	3.01	54.6	3.10

Summary of edge detection results comparing the manual edge detection technique (Manual), the MATLAB Image Processing Toolbox automatic technique (Auto MATLAB) and the ImageJ automatic technique (Auto ImageJ). All results show the average area estimated using three identically-prepared and analyzed experimental replicates. The variability amongst experimental replicates is estimated using the standard deviation.  
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**Figure 2. Comparing edge detection techniques.** Comparing three edge detection techniques for barrier assays with two different cell densities: 10,000 cells (A,C) and 30,000 (B,D) cells. (A–B): Comparison of the three edge detection techniques showing the mean area enclosed by the leading edge at  $t = 0, 24, 48$  and  $72$  hours with time points indicated. Red lines correspond to the manual edge detection technique using MATLAB's Image Processing Toolbox for a range of the threshold parameter  $S \in [0.015, 0.08]$ . Black dots correspond to the automatic MATLAB results and the green asterisks correspond to the automatic ImageJ results. (C–D): The migration rate of cells in the barrier assays expressed as  $M(t)\%$  using equation (1). Results correspond to the minimum (red) and maximum (blue) average areas detected using the manual MATLAB technique. Error bars correspond to one standard deviation about the mean. doi:10.1371/journal.pone.0067389.g002

Our results using the manual edge detection method illustrate that there are many plausible approximations of the leading edge of the spreading populations for a range of threshold values. We now compare the manual edge detection algorithm with two automatic edge detection methods. We applied the automatic MATLAB and ImageJ techniques (section 0.2.3 and section 0.2.2), to the same images we previously analysed using the manual edge detection method. For both automatic techniques, the average area enclosed by the detected edge was calculated and compared to the average areas obtained using the manual edge detection

method. Results in Fig. 2A and Fig. 2B show the automatic edge detection results relative to the manual results, and estimates of the mean and standard deviation of the area obtained using the automatic techniques are given in Table 1. The MATLAB and ImageJ results confirm that both automatic techniques give estimates that are consistent with those obtained using the manual edge detection method. However, the automatic techniques are restricted in the sense that they can only detect one particular location whereas the manual edge detection method can produce

many different results, all of which are reasonable estimates of the position of the leading edge of the spreading cell population.

We now use equation (1) to quantify the observed cell migration in our barrier assays. This approach requires that we use an estimate of  $A(0)$ , the initial average area. Our previous results indicate that the initial average area of the spreading population ranged from 27.4 to 30.1 mm<sup>2</sup> for the barrier assay with 10,000 cells while the initial average area of the spreading population ranged from 31.1 to 33.5 mm<sup>2</sup>. To estimate  $A(0)$  we will take the average of these maximum and minimum estimates so that we have  $A(0) = 28.8$  and  $A(0) = 32.3$  mm<sup>2</sup> for the barrier assays with 10,000 and 30,000 cells, respectively. To estimate the sensitivity of our results as a function of the threshold value in the manual edge detection technique, we apply equation (1) using the minimum and maximum detected average areas from our manual edge detection method. The details of the results for all three edge detection techniques are given in Table 2. Although we observe that the two automatic methods produce similar results for certain assays at certain times, the differences between the results for the two automatic edge detection methods can be very large with  $M(72) = 68.9$  % for the barrier assay with 30,000 cells according to the ImageJ results whereas  $M(72) = 82.0$  % for the same assay according to the automatic MATLAB method. Profiles in Fig. 2C and Fig. 2D show how  $M(t)$  varies with time according to the results obtained from the manual edge detection method applied to the images from the barrier assays initialized with 10,000 and 30,000 cells, respectively. Figure 2C and Fig. 2D each contain two sets of results corresponding to the average estimate of  $M(t)$  calculated using the low  $S$  threshold, and the average estimate of  $M(t)$  calculated using the high  $S$  threshold. The differences between the low and high threshold results in Fig. 2C is 14.2 %, 25.0 % and 25.7 % for  $t = 24, 48$  and  $72$  hours, respectively. The difference between the low and high threshold results in Fig. 2D (30,000 cells) is 17.0 %, 17.0 % and 24.5 % for  $t = 24, 48$  and  $72$  hours, respectively. These results indicate that estimates of cell migration using equation (1) are very sensitive to the details of the edge detection technique and that this sensitivity increases with time.

## 0.6 A Physical Interpretation of the Leading Edge

Previously, we used three different edge detection techniques to determine the location of the leading edge of spreading cell populations in several barrier assays. Although these techniques produce visually reasonable approximations to the position of the leading edges, the techniques do not give us any physical measure, or definition, of the leading edge. To address this, we now interpret our edge detection results using a mathematical model of

the cell spreading process. For each barrier assay experiment, we solve equation (2) using the appropriate boundary and initial conditions (section 0.3) and previous estimates of the cell diffusivity [17]. The solution profiles in Fig. 3A and Fig. 3D, show the predicted cell density near the leading edge of the spreading cell populations in the barrier assay at  $t = 24, 48$  and  $72$  hours. The difference between the two initial cell densities in the barrier assays is shown in these profiles since we have  $c_0 = 0.22$  in the center of the barriers for the assays initialized with 10,000 cells (Fig. 3A) whereas we have  $c_0 = 0.66$  in the center of the barriers for the assays initialized with 30,000 cells (Fig. 3D).

To determine a physical relationship between the threshold value  $S$  and the cell density at the corresponding detected edge, we compare our manual edge detection results to solutions of equation (2). For each set of averaged edge detection results, we scale the threshold values to match the corresponding solution of equation (2). The scaling is given by.

$$S_{\text{scaled}} = c_{\min} + (c_{\max} - c_{\min}) \frac{S - S_{\min}}{S_{\max} - S_{\min}}, \quad (4)$$

where  $c_{\min}$  and  $c_{\max}$  are the minimum and maximum contours of the solution of equation (2),  $c(r, t)$ , which enclose the same average area detected by the manual edge detection method applied with the minimum and maximum thresholds,  $S_{\min}$  and  $S_{\max}$ , respectively.

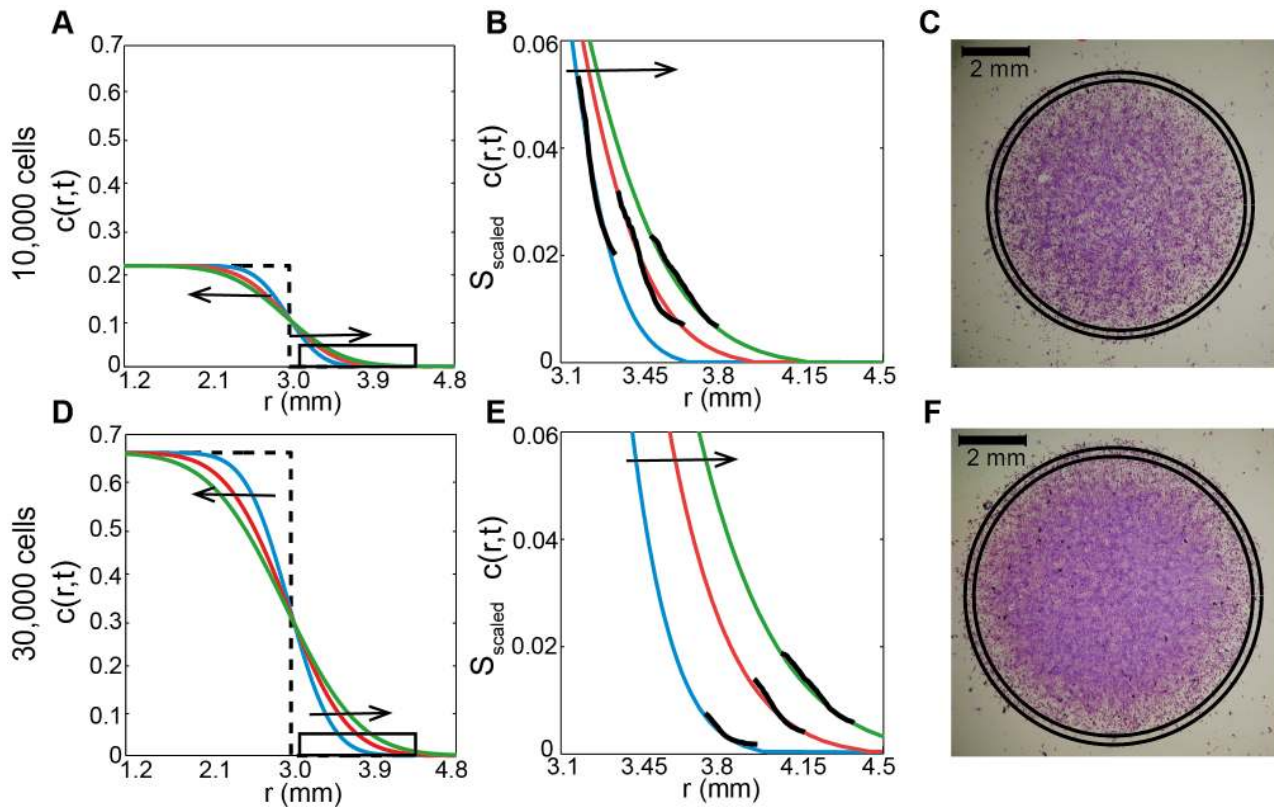
Profiles in Fig. 3B and Fig. 3E compare the scaled edge detection results to corresponding solutions of equation (2) at  $t = 24, 48$  and  $72$  hours for barrier assays with 10,000 and 30,000 cells, respectively. For both initial density experiments at all time points, the shape of the  $c(r, t)$  density profiles matches the shape of the edge detection results. This match indicates that varying the threshold value  $S$  corresponds to a consistent variation in the spatial distribution of cell density in the spreading cell population. Comparing the edge detection results to the corresponding contours of the cell density, we observe that the manual edge detection technique identifies a range of leading edges corresponding to cell densities of 2–5.5 % at  $t = 24$  hours, 0.9–3.2 % at  $t = 48$  hours and 0.8–2.5 % at  $t = 72$  hours for the barrier assays with 10,000 cells. Equivalent results in Fig. 3E indicates that the manual edge detection technique identifies a range of leading edges corresponding to cell densities of 0.2–0.8 %, 0.5–1.5 % and 0.8–1.8 %, for  $t = 24, 48, 72$  hours for the barrier assay with 30,000 cells. In summary, the manual edge detection technique identifies a range of leading edges corresponding to cell densities of approximately 1–5 % of the maximum packing density.

**Table 2.** Quantifying the cell migration rate using equation (1).

Number of Cells	Time (hours)	M(t) Manual S High	M(t) Manual S Low	M(t) Auto ImageJ	M(t) Auto Matlab
10,000	24	10.8	25.0	14.4	17.9
	48	25.7	50.7	35.0	34.8
	72	37.8	63.5	49.7	53.8
30,000	24	49.6	66.6	50.8	50.0
	48	65.6	82.7	66.8	71.3
	72	74.6	99.1	68.9	82.0

The cell migration rate in terms of  $M(t)$  using equation (1) and the average area results from Table 1. Results are reported for the manual edge detection technique with a high threshold (Manual S high), the manual edge detection technique with a low threshold (Manual S Low), the MATLAB Image Processing Toolbox automatic technique (Auto MATLAB) and the ImageJ automatic technique (Auto ImageJ).

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**Figure 3. Physical interpretation of the edge detection results.** (A, D): Solutions of equation (2) showing the density profiles near the leading edge at  $t=0$  (dotted black),  $t=24$  (blue),  $t=48$  (red) and  $t=72$  hours (green). Arrows indicate the direction of increasing time. The initial conditions is given by equation (3) with  $c_0=0.22$  and  $c_0=0.66$  for barrier assays with 10,000 and 30,000 cells, respectively. Numerical solutions of equation (2) are obtained with  $\delta r=1.0 \mu\text{m}$  and  $\delta t=0.005$  hours, with  $D=1700 \mu\text{m}^2/\text{hour}$  and  $D=2900 \mu\text{m}^2/\text{hour}$  for barrier assays with 10,000 and 30,000 cells, respectively. (B,E) The detail of the solutions of equation (2) from the boxed area in (A,D) compared with the scaled manual edge detection results (black) from Figure 2 (A,C). (C,F) Images of a barrier assay with 10,000 and 30,000 cells at  $t=72$  hours, respectively. The contours of the solution of equation (2) are superimposed. The values of the contours are  $c_{\min}=0.007$  and  $c_{\max}=0.026$  for the barrier assay with 10,000 cells, and  $c_{\min}=0.008$  and  $c_{\max}=0.020$  for the barrier assay with 30,000 cells. doi:10.1371/journal.pone.0067389.g003

The images in Fig. 3C and Fig. 3F show snapshots from two barrier assays at  $t=72$  hours with 10,000 and 30,000 cells, respectively. To illustrate the location of the leading edge, defined by contoured solutions of equation (2), we superimpose the  $c_{\min}$  and  $c_{\max}$  contour of the appropriate solution of equation (2). In both cases we observe that the  $c_{\min}$  and  $c_{\max}$  contours are reasonable approximations to the location of the position of the leading edge of the spreading populations. In each experiment, the difference between the  $c_{\min}$  and  $c_{\max}$  contours are relatively large and this recapitulates the sensitivity observed previously in Fig. 1H and Fig. 1I.

## Discussion and Conclusions

Cell migration is an essential aspect of development [1,2], repair [3–5] and disease [6,7]. *In vitro* cell migration assays are routinely used to assess the migration potential of different cell types [8,9] as well as assessing the potential for different types of treatment strategies aimed at regulating cell migration [10–12,16]. Currently, many studies report results from cell migration assays without specifying the details of how the assays are measured or interpreted [27–31]. In an attempt to address this limitation we compare three different image processing techniques to quantify the migration rate of cells in a two-dimensional barrier assay [17]. Our visual interpretation of the images from the barrier assays

indicate that the position of the leading edge of the spreading population is relatively sharp and well-defined at the beginning of the assay. However, we observe that the leading edge of the spreading cell population becomes increasingly diffuse and less well-defined at later times as the cell population spreads across the substrate. We quantify the rate of cell migration using a standard measure, given by equation (1), describing how the area enclosed by the leading edge of the spreading population increases with time. To explore how such a standard measure of cell migration depends on the edge detection methods we calculate the location of the leading edge of the spreading population using three different image processing tools. In summary, our results indicate that estimates of the cell migration rate are very sensitive to the details of the image processing tools and we show that our estimates of the cell migration rate can vary by as much as 25% for the same data set. These differences depend on the choice of threshold used in the edge detection technique. Our measurements indicate that the concept of the area enclosed by the leading edge is poorly defined and we suggest that one way to overcome these difficulties is to use a direct measurement of cell density. For example, a nuclear stain could be used to reveal the locations of individual cells within the spreading population [17].

In addition to comparing estimates of cell migration using different image processing techniques, we also provide a physical interpretation of the results from the manual edge detection



technique by using a mathematical model of the cell spreading process. We use a previously-parameterised [17] mathematical model to describe the spatial and temporal variation in cell density associated with the barrier assays and we compare our modelling results with the edge detection results. For all images processed by the manual edge detection technique, we identified a range of Sobel threshold values, from  $S_{\min}$  to  $S_{\max}$ , that could be used to produce a reasonable estimate of the location of the leading edge of the spreading populations. We scaled these values so that they corresponded with a range of cell density contours, from  $c_{\min}$  to  $c_{\max}$ , corresponding to the minimum and maximum contours of the relevant solution of equation (2). Our results indicate that varying the threshold  $S$  corresponds to a consistent variation in the spatial distribution of cell density in the spreading cell population. In particular, the manual edge detection technique identifies the leading edge of the population within a range of the cell density of approximately 1-5% of the maximum packing density. The close match between the position of the leading edge as a function of the Sobel threshold and the solution of the partial differential equation describing the spreading process suggests that this type of information could be used to estimate the diffusivity of the cells,  $D$ . This could be a useful method for estimating the cell diffusivity since it is well known that estimates of cell diffusivity can vary by as much as an order of magnitude and these variations depend on the kind of cell and the substrate being considered [41].

As a result of this study, we recommend that the location of the leading edge of a spreading cell population in a cell migration assay should not be determined using any kind of hand tracing technique. Instead, a computational image processing technique should be used to reduce the impact of the subjectivity of the analyst. Our results demonstrate that the computational edge detection techniques can be very sensitive to the choice of threshold applied to the image. Therefore, we recommend that images of cell migration assays should be analysed using a manual

edge detection technique and that the details of the image thresholds should be reported.

We anticipate that our results for the two-dimensional barrier assay will also be relevant to other types of cell migration assays such as scratch assays [3,4], or different types of circular barrier assays that include the outward migration of cells away from an initially-confined circular population [17] as well as barrier assays describing the inward migration of cell populations into an initially-vacant circular region [8,9,16]. We also expect that our results for the two-dimensional barrier assay could be extended by considering other types of experimental conditions. For example, here we chose to present results for cells that were pretreated to prevent cell proliferation [32] so that we could study cell spreading processes driven by cell migration alone in the absence of cell proliferation. Given that the shape of the leading edge of the spreading cell population depends on the relative contribution of cell migration and cell proliferation [6,17], we expect that comparing different edge detection results for different cell populations with different relative rates of cell proliferation and cell migration will also be of interest [37,42]. Finally, although we have presented our image analysis techniques in the context of analyzing an *in vitro* cell migration assay, these concepts will also be relevant when considering *in vivo* cell spreading, such as in the detection of the leading edge of spreading melanomas [34,43].

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## Author Contributions

Conceived and designed the experiments: KKT MJS. Performed the experiments: KKT. Analyzed the data: KKT MJS. Contributed reagents/materials/analysis tools: KKT MJS. Wrote the paper: KKT MJS.

## References

- Nishiyama C, Uesaka T, Manabe T, Yonekura Y, Nagasawa T, et al. (2012) Trans-mesenteric neural crest cells are the principal source of the colonic enteric nervous system. *Nat Neurosci* 15: 1211–1219.
- Wolpert L (2011) Principles of development. 4th Edition. Oxford: Oxford University Press.
- Maini PK, McElwain DLS, Leavesley DI (2004) Traveling wave model to interpret a wound-healing cell migration assay for human peritoneal mesothelial cells. *Tissue Eng* 10: 475–482.
- Maini PK, McElwain DLS, Leavesley DI (2004) Travelling waves in a wound healing assay. *Appl Math Lett* 17: 575–580.
- Sengers BG, Please CP, Oreffo ROC (2007) Experimental characterization and computational modelling of two-dimensional cell spreading for skeletal regeneration. *J R Soc Interface* 4: 1107–1117.
- Swanson KR, Bridge C, Murray JD, Alvord Jr EC (2003) Virtual and real brain tumors: using mathematical modeling to quantify glioma growth and invasion. *J Neurol Sci* 216: 1–10.
- Weinberg RA (2006) The biology of cancer. USA: Garland Publishing.
- Kam Y, Guess C, Estrada L, Weidow B, Quaranta V (2008) A novel circular invasion assay mimics *in vivo* invasive behaviour of cancer cell lines and distinguishes single-cell motility. *BMC Cancer* 8: 198–210.
- Kam Y, Karperien A, Weidow B, Estrada L, Anderson AR, et al. (2009) Nest expansion assay: a cancer systems biology approach to *in vitro* invasion measurements. *BMC Cancer* 9: 130–139.
- Upton Z, Cuttle L, Noble A, Kempf M, Topping G, et al. (2008) Vitronectin: growth factor complexes hold potential as a wound therapy approach. *J Invest Dermatol* 128: 1535–1544.
- Upton Z, Wallace HJ, Shooter GK, van Lonkhuyzen DR, Yeoh-Ellerton S, et al. (2011) Human pilot studies reveal the potential of a vitronectin: growth factor complex as a treatment for chronic 417 wounds. *International Wound Journal* 8: 522–532.
- Decaestecker C, Debeir O, Van Ham P, Kiss R (2007) Can anti-migratory drugs be screened *in vitro*? a review of 2d and 3d assays for the quantitative analysis of cell migration. *Med Res Rev* 27: 149–176.
- Dixit VD, Weeraratna AT, Yang HY, Bertak D, Cooper-Jenkins A, et al. (2006) Ghrelin and the growth hormone secretagogue receptor constitute a novel autocrine pathway in astrocytoma motility. *J Biol Chem* 281: 16681–16690.
- Simpson MJ, Towne C, McElwain DLS, Upton Z (2010) Migration of breast cancer cells: Under4 standing the roles of volume exclusion and cell-to-cell adhesion. *Phys Rev E* 82: 041901.
- Gough W, Hulkower KI, Lynch R, Mcglynn P, Uhluk M, et al. (2011) A quantitative, facile, and high-throughput image-based cell migration methods is a robust alternative to the scratch assay. *J Biomol Screen* 16: 155–163.
- Van Horssen R, Ten Hagen TLM (2010). Crossing barriers: the new dimension of 2D cell migration assays. *J Cell Physiol* 226: 288–290.
- Simpson MJ, Treloar KK, Binder BJ, Haridas P, Manton KJ, et al. (2013) Quantifying the roles of cell motility and cell proliferation in a circular barrier assay. *J R Soc Interface*. 10, 20130007.
- Ashby WJ, Zijlstra A (2012) Established and novel methods of interrogating two-dimensional cell migration. *Integr Biol* 4: 1338–1350.
- McKenzie AJ, Campbell SL, Howe AK (2011) Protein Kinase A activity and anchoring are required for ovarian cancer cell migration and invasion. *PLoS One* 6: e26552.
- Zaritsky A, Natan S, Horev J, Hecht I, Wolf L, et al. (2011) Cell motility dynamics: a novel segmentation algorithm to quantify multi-cellular bright field microscopy images. *PLoS One*. 6: e27593.
- Goetsch KP, Nielser CU (2011) Optimization of the scratch assay for *in vitro* skeletal muscle wound healing analysis. *Anal Biochem* 411: 158–160.
- Yue PYK, Leung EPY, Make NK, Wong RNS (2010) A simplified method for 444 quantifying cell migration/wound healing in 96-well plates. *J Biomol Screen* 4: 427–433.
- Topman G, Sharabani-Yosef O, Gefen A (2012) A standardized objective method for continuously measuring the kinematics of cultures covering a mechanically damaged site. *Med Eng Phys* 34: 225–232.
- Research Services Branch, National Institute of Health (2012) ImageJ user guide. Available: <http://rsbweb.nih.gov/ij/docs/guide/146-29.html>. Accessed 2013 Jan 01.
- Mathworks (2012) Image acquisition toolbox. Users guide R2012b. Available: <http://www.mathworks.com.au/products/image/>. Accessed 2013 Jan 01.
- Zordan MD, Mill CP, Riese DJ, Leary JF (2011) A high throughput, interactive imaging, bright4 field wound healing assay. *Cytom Part A* 79: 227–232.

27. Hidalgo-Grass C, Mishalian I, Dan-Goor M, Beloterkovsky I, Eran Y, et al. (2006) A streptococcal protease that degrades CXC chemokines and impairs bacterial clearance from infected tissues. *EMBO J* 25: 4628–4637.
28. Lee J, Wang YL, Ren F, Lele TP (2010) Stamp wound assay for studying couple cell migration and cell debris clearance. *Langmuir* 26: 16672–16676.
29. Nizet V, Ohtake T, Lauth X, Trowbridge J, Rudisill J, et al. (2001) Innate antimicrobial peptide protects the skin from invasive bacterial infection. *Nature* 414: 454–457.
30. Okumara CYM, Hollands A, Tran DN, Olson J, Dahesh S, et al. (2012) A new pharmacological agent (AKB-4924) stabilizes hypoxia inducible factor (HIF-1) and increases skin innate defenses against bacterial infection. *J Mol Med* 90: 1079–1089.
31. Wang X, Cui M, Wang L, Chen X, Xin P (2010) Inhibition of neurotrophin receptor p75 intramembranous proteolysis by gamma-secretase inhibitor reduces medulloblastoma spinal metastasis. *Biochem Biophys Res Commun* 403: 264–269.
32. Sadeghi MH, Seitz B, Hayashi S, LaBree L, McDonnell PJ (1998). In vitro effects of mitomycin on human keratinocytes. *J Refract Surg* 14: 534–540.
33. Abdou IE, Pratt WK (1979) Quantitative design and evaluation of enhancement/thresholding edge detectors. *Proc IEEE* 67: 753–763.
34. Mete M, Sirakov NM (2010) Lesion detection in microscopy images with novel density-based and active contour approaches. *BMC Bioinformatics* 11 (Suppl 6) S23.
35. Gebäck T, Schulz MMP, Koumoutsakos P, Detmar M (2009) TScratch: a novel and simple software tool for automated analysis of monolayer wound healing assays. *Biotechniques* 46: 265–274.
36. Gebäck T, Koumoutsakos P (2009) Edge detection in microscopy images using curvelets. *BMC Bioinformatics* 10: 75.
37. Simpson MJ, Landman KA, Hughes BD (2010) Cell invasion with proliferation mechanisms motivated by time-lapse data. *Physica A* 389: 3779–3790.
38. Simpson MJ, Ellery AJ (2012) An analytical solution for diffusion and nonlinear uptake of oxygen in a spherical cell. *Appl Math Model* 36: 3329–3334.
39. Bradie B (2006) A friendly introduction to numerical analysis. USA: Pearson Prentice Hall.
40. Simpson MJ, Landman KA, Clement TP (2005) Assessment of a non-traditional operator split algorithm for simulation of reactive transport. *Math Comput Simulat* 70: 44–60.
41. Swanson KR, Harpold HLP, Peacock DL, Rockne R, Pennington C, et al. (2008) Velocity of radial expansion of contrast-enhancing gliomas and the effectiveness of radiotherapy in individual patients: a proof of principle. *Clin Oncol* 20, 301–308.
42. Simpson MJ, Baker RE (2011) Corrected mean-field models for spatially dependent advection-diffusion-reaction phenomena. *Phys Rev E* 83: 051922.
43. Guitera P, Menzies SW (2011) State of the art of diagnostic technology for early-stage melanoma. *Expert Rev Anticancer Ther* 11: 715–723.