Surface Based Atlas Matching of the Brain Using Deformable Surfaces and Volumetric Finite Elements

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1   Introduction

The automatic identification and localization of structures in magnetic resonance (MR) brain images are a major part of the processing work for the neuroradiologist in numerous clinical applications, such as functional mapping and surgical planning. To aid in this task, a considerable amount of research has been directed toward the development of 3D standardized atlases of the human brain (e.g. [5]). These provide an invariant reference system and the possibility of template matching, allowing anatomical and functional structures in new scans to be identified and analyzed.

There are mainly two types of methods for doing deformable atlas matching : surface-based and volume based methods. Surface based methods deform key surfaces of the atlas onto the target image and interpolate the surface displacement to obtain a fully volumetric mapping (e.g. [3]). Volumetric methods compute a deformation field that minimizes a similarity criterion between the atlas and the target image under a given regularization constraint (e.g. elastic). To reach convergence, the computations must be done in a multi-resolution fashion (e.g. [1]). The main issue with both methods is the initialization of the volume or surfaces.

In this paper, we propose a surface based method with automatic initialization of the deformable surfaces using a global parametric transformation. We use an elastic volumetric finite element (FE) deformation model to infer a volumetric deformation field from the obtained surface deformations. The method provides us with a fully automated volumetric mapping of the atlas onto a target image.

2   Atlas Matching Algorithm

The landmark deformable surfaces of the atlas (cortical surface and ventricles) are initialized on the target image using a 2nd degree polynomial transform that minimizes a distance measure of the landmark surfaces to the distance transform of the corresponding objects in the target image [2]. The objects are segmented out of the target image using a directional watershed algorithm [2]. We then match the initialized landmark surfaces onto the target image using our deformable surface matching algorithm [4], as illustrated in Figure 1.

We infer a volumetric deformation field from the surface deformations by applying the surface displacements obtained after global registration and active surface deformation as a boundary condition to a volumetric FE tetrahedral mesh we have extracted from the atlas image [4]. After the atlas's volumetric FE mesh has been deformed by the boundary surfaces, the obtained deformation field can be interpolated back onto the image grid to produce a volumetric mapping from the atlas space onto the target image space [4]. Figure 2 illustrates the different volumetric deformation stages of atlas brain onto a target brain. The volumetric mapping can then be used to outline other objects in the target image.
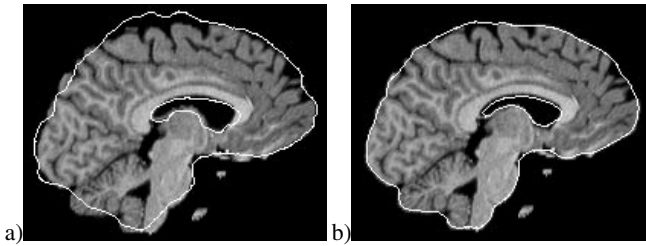
Fig. 1. a) cut through deformable surfaces after 2nd degree polynomial transform overlaid on corresponding cuts through target image. b) Same cut but after active surface deformation.
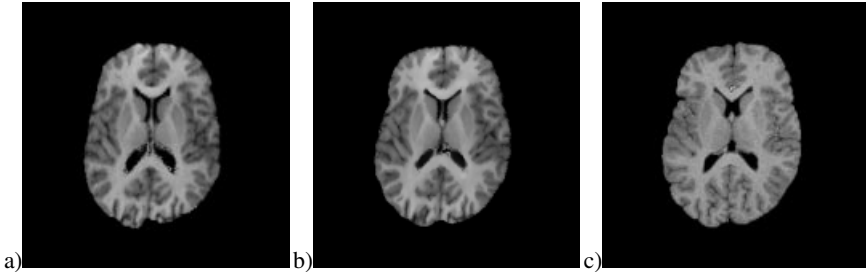

Fig. 2. Volumetric deformations of the atlas MR image illustrating the transformation steps of the algorithm. a) Slice of deformed volume after 2nd degree registration of ventricles and brain surface. b) Same slice after active surface deformation. c) Same slice of target image.

3   Conclusion

We have presented a surface based deformable atlas matching algorithm that automatically initializes the deformable surfaces. An arbitrary number of surfaces can be matched to drive the volumetric warp of the atlas onto a target image, and the finite element formulation of the volumetric match allows for variable elastic deformations of the atlas's objects. Our preliminary experiments show very good correlation of the deformed atlas with the target image.

References

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