

Swimming speeds of filaments in nonlinearly viscoelastic fluids

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Many micro-organisms swim through gels and non-Newtonian fluids in their natural environments. In this paper, we focus on micro-organisms which use flagella for propulsion. We address how swimming velocities are affected in nonlinearly viscoelastic fluids by examining the problem of an infinitely long cylinder with arbitrary beating motion in the Oldroyd-B fluid. We solve for the swimming velocity in the limit in which deflections of the cylinder from its straight configuration are small relative to the radius of the cylinder and the wavelength of the deflections; furthermore, the radius of the cylinder is small compared to the wavelength of deflections. We find that swimming velocities are diminished by nonlinear viscoelastic effects. We apply these results to examine what types of swimming motions can produce net translation in a nonlinear fluid, comparing to the Newtonian case, for which Purcell's "scallop" theorem describes how time-reversibility constrains which swimming motions are effective. We find that a leading order violation of the scallop theorem occurs for reciprocal motions in which the backward and forward strokes occur at different rates.

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I. INTRODUCTION

Bacteria and other microscopic swimmers live in a world of low Reynolds number, in which viscous effects dominate over inertia.^{1,2} In this regime, the drag forces acting on a swimmer are much greater than the forces necessary to achieve the observed accelerations of these swimmers. At the limit of zero Reynolds number, the sum of the net drag force and any other external forces, such as buoyancy, must vanish. Therefore, the physics underlying the swimming strategies of micro-organisms is markedly different from that of large organisms such as fish. For example, in the absence of inertia, the diffusion of viscous shear waves is essentially instantaneous. Thus, the flows induced by a swimming creature's motions start and stop immediately when the creature's movements start and stop. This phenomenon is closely related to the "scallop theorem," of Purcell,² which states that time-reversible strokes in a Newtonian fluid, such as water, cannot produce net swimming,¹ because there is an equal and opposite net translation for corresponding forward and backward stroke motions. As a result, swimming micro-organisms use strokes with a clear time direction, such as the traveling-wave patterns on the flexible flagella of mammalian sperm, or the rigid-body rotation of the helical flagellar filaments of *Escherichia coli*.

Early theoretical work elucidated the basic principles of swimming at zero Reynolds numbers in a Newtonian fluid. For example, Taylor³ calculated the swimming speed of an infinite two-dimensional sheet as a function of the amplitude, wave number, and wave speed of a traveling wave on the sheet. He also did the same calculation for an infinite cylin-

drical filament.⁴ These calculations showed that the swimming speed is proportional to the wave speed, as expected from dimensional analysis. Since the shape and speed of the waves on the sheet or filament in these calculations are independent of the load, the swimming speed is independent of the viscosity of the fluid. In other work, various groups have calculated how viscous forces and forces internal to a flagellum determine the shape of flexible filaments actuated at one end⁵⁻⁷ or actuated by internal motors distributed along the filament.⁸⁻¹¹

All the calculations just mentioned apply to Newtonian fluids. However, swimming micro-organisms often encounter elastic fluids. For example, mammalian sperm must swim through viscoelastic mucus in the female reproductive tract;¹²⁻¹⁴ the bacterium *Helicobacter pylori* must swim through mucus lining the stomach;¹⁵ and spirochetes must burrow through connective tissue in the course of infection.¹⁶ The theory of swimming in non-Newtonian fluids is much less developed than the Newtonian case. Fulford *et al.* extended the resistive force theory of Gray and Hancock¹⁷ to the case of a linear Maxwell model for viscoelasticity, and found no change in the swimming speed compared to the Newtonian case.¹⁸ More recently, Lauga¹⁹ emphasized that since swimming speed depends nonlinearly on wave amplitude, a realistic treatment of swimming in a non-Newtonian medium should include a nonlinear model for the viscoelastic medium. Lauga investigated several nonlinear fading memory models and found that for a given wave pattern on a two-dimensional sheet, viscoelastic effects slow the swimmer relative to its speed in a Newtonian liquid.¹⁹

In our previous work, we calculated the swimming velocity of an infinite filament with a prescribed waveform in the upper-convected Maxwell model,²⁰ a simple nonlinear model for a viscoelastic material with fading memory.²¹ We

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also studied the effect of the viscoelastic medium on the shape of a beating filament described by a simple sliding filament model,⁸ and showed how altered beating shapes affect swimming velocities. In the current paper, we give a more detailed account of our calculation of the swimming speed of an infinite filament with a prescribed waveform. We refine our previous calculation by including the effects of solvent viscosity with the Oldroyd-B model for a nonlinearly viscoelastic polymer solution. As an application of our calculations, we examine how the scallop theorem is spoiled in a nonlinearly viscoelastic fluid at zero Reynolds number. In this paper we consider prescribed shapes of beating patterns. In actual swimmers with beating filaments, the shape is determined by the interaction of filament structure with hydrodynamic forces, which we address in another publication.¹¹ Here we take the point of view that the beating pattern is already known (for example, from direct observation) and ask what the consequences are for swimming properties. We restrict our discussion to time-periodic motions and associated flows, corresponding to repetitive swimming actions that can be employed to move an arbitrarily large distance by a self-contained organism. For these time-periodic motions, the associated flows will have both time-periodic and constant components. Only the constant, time-averaged component produces net translation over many cycles.

We close this introduction with a summary of the structure of this paper. In Sec. II we review the Oldroyd-B model and how it naturally arises for a material with fading memory. Then, in Sec. III, we calculate the flow fields induced by a helical traveling wave on an infinite cylinder. We work to second order in the deflection of the cylinder, and deduce the time-averaged swimming speed. In Sec. IV we explore the ramifications of our calculation for the scallop theorem, and show quantitatively how a reversible stroke pattern leads to propulsion. Section V is the conclusion. Finally, in the Appendix we calculate the viscoelastic force per unit length to first order acting on a filament with transverse or longitudinal (compressional) traveling waves.

II. NONLINEARLY VISCOELASTIC FLUIDS

Since we consider the zero Reynolds number regime, inertia is irrelevant and the dynamics of an incompressible medium is governed by force balance, $-\nabla p + \nabla \cdot \boldsymbol{\tau} = 0$, where p is the pressure associated with incompressibility, $\nabla \cdot \mathbf{v} = 0$; \mathbf{v} is the flow velocity; and $\boldsymbol{\tau}$ is the deviatoric stress tensor. The particular character of a medium is determined by the constitutive relation, which relates the stress to the strain and rates of strain. In this paper we consider dilute polymer solutions, in which the stress relaxes to the stress of a Newtonian viscous fluid over a time scale λ . A simple constitutive relation for a dilute polymer solution is the single-relaxation-time Maxwell model:

$$\boldsymbol{\tau}_{ij} + \lambda \frac{\partial \boldsymbol{\tau}_{ij}}{\partial t} = \eta \dot{\boldsymbol{\gamma}}_{ij}, \quad (1)$$

where i and j label Cartesian coordinates, η is viscosity, and $\dot{\boldsymbol{\gamma}}_{ij} = \partial v_i / \partial x_j + \partial v_j / \partial x_i$ is the strain rate. This constitutive relation is valid to first order in deformation. However, the

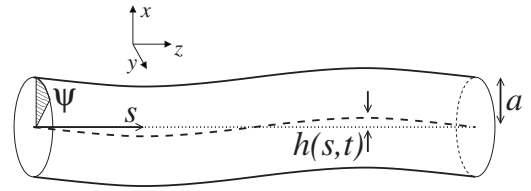


FIG. 1. A section of an infinite filament with prescribed beating pattern $h(s, t)$.

swimming velocity of a prescribed motion is second order in the deformation.^{3,4} To see why, consider a traveling wave of amplitude h on an infinite cylindrical filament (Fig. 1). The swimming velocity may be represented as a power series in h . Replacing h with $-h$ changes the sign of the first-order contribution to the velocity. On the other hand, changing the sign of h amounts to translating the filament by half of a wavelength, and therefore yields no change in the time-averaged swimming velocity. Thus we conclude that the swimming velocity is quadratic in h to leading order, and therefore nonlinear corrections to Eq. (1) will be important for the study of swimming in a viscoelastic medium.¹⁹

It is useful to recall why the constitutive relation (1) is inapplicable for large deformations. First, note that the Maxwell constitutive relation does not respect Galilean invariance. This defect is easily fixed by replacing the partial time derivative of the stress, $\partial \boldsymbol{\tau}_{ij} / \partial t$, with the material derivative, $\partial \boldsymbol{\tau}_{ij} / \partial t + \mathbf{v} \cdot \nabla \boldsymbol{\tau}_{ij}$. However, this modified constitutive relation is still unsuitable for working beyond first order in deformation because it is sensitive to the overall orientation of the material. For example, consider a steady-state flow, for which Eq. (1) predicts that $\boldsymbol{\tau}_{ij} = \eta \dot{\boldsymbol{\gamma}}_{ij}$. Now place the medium on a slowly rotating turntable.²⁰ Since viscous forces are much greater than the fictitious forces arising from rotation, the relation between stress and strain rate in the rotating material is the same as that in the stationary material, to an excellent approximation:²² $\boldsymbol{\tau}'_{ij} = \eta \dot{\boldsymbol{\gamma}}'_{ij}$, where the prime denotes the quantities for the rotating material. On the other hand, the components $\boldsymbol{\tau}'_{ij}$ are time dependent, because $\boldsymbol{\tau}'_{ij} = R_{ik} R_{jl} \boldsymbol{\tau}_{kl}$, where R_{ij} is a time-dependent rotation matrix. Therefore, Eq. (1) cannot hold for the primed quantities, even with the partial time derivative replaced with the material derivative.

In general, changes in the components $\boldsymbol{\tau}_{ij}$ due to motion of the basis vectors should not enter the constitutive relation. The formulation of rheological equations of state requires a time derivative that does not depend on the choice of basis.²³ Any constitutive relation that reflects the small magnitudes of fictitious forces must be formulated in terms of time derivatives of stress or strain that transform homogeneously under change in coordinates. There are many different ways to construct a time derivative of the stress tensor that is insensitive to the rate of change in the basis vectors. In the following we present one way to do so which leads to the nonlinear viscoelastic model used in the rest of the paper.

Due to the small magnitudes of fictitious forces, the constitutive relation should be insensitive not only to global rotations such as that of the turntable described above but also to local rotations and translations of fluid elements. One way to enforce this more general condition is to express the time

derivatives in terms of coordinates which track fluid elements. Suppose $\{\xi^1, \xi^2, \xi^3\}$ are convective coordinates, with $\mathbf{r}(\xi^1, \xi^2, \xi^3, t)$ the position at time t of the particle with Cartesian coordinates $\{x^1, x^2, x^3\}$ at the initial time. Convective coordinates are also known as Lagrangian coordinates. The basis vectors associated with convective coordinates are $\mathbf{g}_i = \partial \mathbf{r} / \partial \xi^i$, and the stress takes the form $\boldsymbol{\tau} = \tau^{ij} \mathbf{g}_i \otimes \mathbf{g}_j$, or more simply $\boldsymbol{\tau} = \mathbf{g}_i \tau^{ij} \mathbf{g}_j$. For Cartesian coordinates, whether an index is raised or lowered has no significance; however, for general coordinates, raised indices signify contravariant coordinates, and lowered indices signify covariant coordinates.²⁰ Since $\partial \mathbf{g}_i / \partial t = \partial \mathbf{v} / \partial \xi^i = (\mathbf{g}_i \cdot \nabla) \mathbf{v}$, we have

$$\left. \frac{\partial \boldsymbol{\tau}}{\partial t} \right|_{\xi^i} = \mathbf{g}_i \left(\frac{\partial \tau^{ij}}{\partial t} \right) \mathbf{g}_j + (\mathbf{g}_i \cdot \nabla \mathbf{v}) \tau^{ij} \mathbf{g}_j + \mathbf{g}_i \tau^{ij} (\mathbf{g}_j \cdot \nabla \mathbf{v}). \quad (2)$$

The second two terms in Eq. (2) arise from the dependence of the basis vectors on time and therefore they cannot enter the constitutive relation. To eliminate the spurious time dependence, define the upper-convected time derivative using convective coordinates:

$$\nabla \boldsymbol{\tau} \equiv \mathbf{g}_i \left(\frac{\partial \tau^{ij}}{\partial t} \right) \mathbf{g}_j. \quad (3)$$

In coordinate-free form, the upper-convected derivative is

$$\nabla \boldsymbol{\tau} = \frac{\partial \boldsymbol{\tau}}{\partial t} + \mathbf{v} \cdot \nabla \boldsymbol{\tau} - \boldsymbol{\tau} \cdot \nabla \mathbf{v} - (\nabla \mathbf{v})^T \cdot \boldsymbol{\tau}. \quad (4)$$

It follows directly from Eq. (3) that the components of $\nabla \boldsymbol{\tau}$ in a general coordinate system transform homogeneously even under a time-dependent change in coordinates.

The upper-convected time derivative is just one way of many to construct a time derivative of the stress tensor that is insensitive to the rate of change in the basis vectors. For example, if we consider the covariant components τ_{ij} of the stress tensor in the convected-coordinate basis, a different natural derivative emerges: the lower-convected derivative.²⁴ The choice of one particular convective derivative over another cannot be justified on symmetry grounds alone, but must be made using information from experiments or the continuum limit of a microscopic model.

For example, a commonly used model for dilute polymer solutions is the Oldroyd-B model.²⁰ We will use this model in this paper. In the Oldroyd-B model, the polymer component is represented by the upper-convected Maxwell model, which is the Maxwell constitutive equation (1) with the time derivative replaced by the upper-convected time derivative. The appearance of the upper-convected time derivative, rather than some other form insensitive to rates of change in basis vectors, can be justified by appealing to a microscopic model of polymer stresses arising from Hookean dumbbells.²⁵ The solvent is represented by the usual Newtonian constitutive relation for a viscous fluid. Thus, the deviatoric stress for the solution is

$$\boldsymbol{\tau} + \lambda \nabla \boldsymbol{\tau} = \eta \dot{\boldsymbol{\gamma}} + \lambda \eta_s \dot{\boldsymbol{\gamma}}, \quad (5)$$

where the total viscosity $\eta = \eta_p + \eta_s$ is the sum of polymer and solvent viscosities. Note that if a patch of fluid under-

goes a spatially uniform rotation or translation, due to the covariant nature of this equation, within the patch the constitutive relation is insensitive to the motion. In Eq. (5), if the solvent viscosity is ignored ($\eta_s = 0$), the Oldroyd-B fluid reduces to the upper-convected Maxwell fluid, and if there is no polymer ($\eta = \eta_s$) the Oldroyd-B fluid reduces to a Newtonian fluid. The model for the Oldroyd-B fluid predicts realistic elastic and first normal stress effects as long as elongational flows are not large; however, it does not capture shear-thinning or yield-stress behaviors observed in some non-Newtonian fluids. The Oldroyd-B model has been used to describe fluids of Boger and Binnington.²⁶ We use the Oldroyd-B fluid as an example. The choice of constitutive relation ultimately depends on accurately modeling the properties of particular real-life fluids and flows. We note that in the case of an infinite sheet, Lauga¹⁹ examined a number of nonlinear models, including finite extensible nonlinear elastic models which remedy the limitations of Oldroyd-B in elongational flows, and found that the swimming speed was not affected by the choice of constitutive model.

III. SWIMMING VELOCITY OF FILAMENTS IN VISCOELASTIC FLUIDS

In this section we describe the solution to the problem of an infinitely long cylinder with prescribed beating motion in a viscoelastic fluid. We obtain the swimming velocity in a nonlinearly viscoelastic fluid, and find that, in general, it is decreased relative to the swimming velocity in a Newtonian fluid. Our results are different from the results of Fulford *et al.*,¹⁸ who used the constitutive relation (1) to find that a filament with prescribed beating pattern swims at the same speed in viscous and linearly viscoelastic fluids. Our results are in broad agreement with those of Lauga,¹⁹ who solved the corresponding problem of an infinite sheet with traveling-wave displacements.

Figure 1 shows a snapshot of the swimming filament. The beating motion is represented by a transverse traveling wave. This motion induces flow. To calculate the swimming velocity, we work in the frame of the swimmer and calculate the z -component of the flow far from the swimmer. As argued above, the swimming velocity is second order in the amplitude of the deflections of the filament; therefore we must calculate the z -component of the flow to second order. We calculate the average speed over one period of the motion of the filament.

A. First order solutions for a cylinder with prescribed beating pattern

In this subsection we define the deformation of the filament, prescribe the boundary conditions, and solve for the flow velocity to first order in the deformation of the filament. We consider a cylinder with radius a , with its axis lying along the \hat{z} direction. For the undisturbed, straight cylinder, material points on the surface are parameterized by s , the distance along the axis, and the angle ψ (see Fig. 1). Note that these coordinates are convective coordinates for the filament surface. For a transverse planar traveling wave, the deformation of the cylinder is given by prescribing the posi-

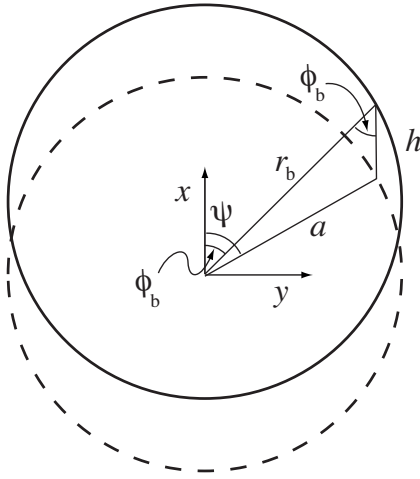


FIG. 2. A cross section of the infinite filament, showing the undeformed (dashed line) and current configuration (solid line), and the relation between ϕ_b and the convective coordinate ψ .

tion $s\hat{\mathbf{z}} + h(s, t)\hat{\mathbf{x}}$ of the centerline of the cylinder. Material points on the surface of the cylinder are parameterized by

$$\mathbf{r}(\psi, s, t) = \hat{\mathbf{x}}[h(s, t) + a \cos \psi] + \hat{\mathbf{y}}a \sin \psi + \hat{\mathbf{z}}s, \quad (6)$$

$$h(s, t) = \text{Re}\{\tilde{h} \exp(iqs - i\omega t)\}.$$

Because the displacement is solely in the $\hat{\mathbf{x}}$ direction, the filament must be extensible. Enforcing inextensibility leads to motion of the filament surface in the $\hat{\mathbf{z}}$ direction with amplitude of order h^2 ; this type of longitudinal motion would give rise to corrections to the swimming velocity of order h^4 , higher order than the results we report in this paper. For technical ease, we solve for arbitrary motion by decomposing into a linear superposition of traveling waves; therefore it is sufficient to assume that the prescribed shape change in Eq. (6), is given by a single propagating mode. As we will show, the swimming velocity, although second order in h , has a form amenable to this decomposition into traveling waves. We also introduce notation for variables with tildes that we use in the remainder of this paper: $A = \text{Re}\{\tilde{A} \exp(iqs - i\omega t)\}$.

Assume that the displacement of the filament from its undisturbed state is small compared to the smallest wavelength of the cylinder motion $h(s, t)$ and the cylinder radius a . This assumption allows us to take advantage of the cylindrical symmetry. Later, we will find it convenient to further demand that $qa \ll 1$. Using cylindrical coordinates, with basis vectors $\hat{\mathbf{z}}$ and

$$\hat{\mathbf{r}} = \hat{\mathbf{x}} \cos \psi + \hat{\mathbf{y}} \sin \psi, \quad (7)$$

$$\hat{\phi} = -\hat{\mathbf{x}} \sin \psi + \hat{\mathbf{y}} \cos \psi, \quad (8)$$

denote the position of points on the surface by (r_b, ϕ_b, z_b) . (The subscript b stands for “boundary.”) To first order in h (see Fig. 2),

$$r_b = a + h \cos \psi,$$

$$\phi_b = \psi - \frac{h}{a} \sin \psi, \quad (9)$$

$$z_b = s.$$

For no-slip boundary conditions on the filament surface,

$$\mathbf{v}[\mathbf{r}(\psi, s, t)] = \left. \frac{\partial \mathbf{r}}{\partial t} \right|_{\psi, s}. \quad (10)$$

Since our goal is to calculate the swimming velocity to leading order, we must expand the boundary condition (10) to second order in the dimensionless displacement $q\tilde{h}$. To all orders in $q\tilde{h}$, the right-hand side of Eq. (10) equals $\dot{h}\hat{\mathbf{x}}$, where here and elsewhere the dot signifies the partial time derivative. Since the leading order contribution to the flow velocity is first order in \tilde{h} , we need only expand the left-hand side of Eq. (10) to first order in the argument of the flow velocity:

$$[\mathbf{v} + h\hat{\mathbf{x}} \cdot \nabla \mathbf{v}]_{a, \psi, s, t} = \dot{h}\hat{\mathbf{x}}. \quad (11)$$

The flow velocity at a fixed point also has an expansion in powers of $q\tilde{h}$:

$$\mathbf{v} = \mathbf{v}^{(1)} + \mathbf{v}^{(2)} + \dots \quad (12)$$

Thus the boundary condition to first order is

$$\mathbf{v}^{(1)}(a, \psi, s, t) = \dot{h}\hat{\mathbf{x}}. \quad (13)$$

To obtain the forces and swimming velocity, we need to solve the Stokes equations mentioned above, $\nabla \cdot \boldsymbol{\tau} - \nabla p = 0$ and $\nabla \cdot \mathbf{v} = 0$, where $\boldsymbol{\tau}$ is now the deviatoric stress tensor that satisfies Eq. (5). To simplify the discussion of the equations of motion for the fluid, we nondimensionalize by measuring length in units of $1/q$, time in units of $1/\omega$, and pressure and stress in units of $\eta\omega$. Hereafter in this and the next section, we use the same variables to denote the nondimensional quantities, unless explicitly stated otherwise. At linear order, all time-dependent quantities are proportional to $\exp(-it)$. To first order, Eq. (5) is

$$\tilde{\boldsymbol{\tau}}^{(1)} = \frac{1 - i \text{De}_2}{1 - i \text{De}} \tilde{\boldsymbol{\gamma}}^{(1)}, \quad (14)$$

where the Deborah numbers $\text{De} = \omega\lambda$ and $\text{De}_2 = \text{De} \eta_s / \eta$. The first-order flow obeys $\nabla \cdot \mathbf{v}^{(1)} = 0$ and

$$\nabla^2(\tilde{\mathbf{v}}^{(1)} e^{-i(t-z)}) - \frac{1 - i \text{De}}{1 - i \text{De}_2} \nabla(\tilde{p}^{(1)} e^{-i(t-z)}) = 0. \quad (15)$$

The first-order boundary condition (13) reduces to $\tilde{\mathbf{v}}^{(1)}(a, \psi) = -i\tilde{h}\hat{\mathbf{x}}$, where $\mathbf{v}^{(1)} = \text{Re}\{\tilde{\mathbf{v}}^{(1)}(r, \phi) \exp(iz - it)\}$ in accord with the convention of Eq. (6).

The solutions to these equations in cylindrical coordinates are known.^{4,27} Note that although there is no solution to the Stokes equations for dragging a rigid infinite rod through fluid,²⁸ the finite wavelength together with the rod radius provide a cutoff in our problem. The first order results for the pressure and velocity field are presented in Table I. In the table, $K_0(r)$ and $K_1(r)$ are modified Bessel functions of the

TABLE I. Pressure and velocity field for a cylinder with a transverse traveling wave; $\alpha = (1 - i \text{De}) / (1 - i \text{De}_2)$.

\tilde{p}	$-i\tilde{h} \cos \phi A K_1(r)$
\tilde{v}_r	$-i\tilde{h} \cos \phi [\alpha A r K_1(r) + B K_2(r) + C K_0(r)]$
\tilde{v}_ϕ	$-i\tilde{h} \sin \phi [B K_2(r) - C K_0(r)]$
\tilde{v}_z	$-\tilde{h} \cos \phi [\alpha A r K_0(r) + (B + C - \alpha A) K_1(r)]$
αA	$\left\{ K_0(a) + a K_1(a) \left[\frac{1}{2} + \frac{K_0(a)}{2K_2(a)} - \frac{K_0(a)^2}{K_1(a)^2} \right] \right\}^{-1}$
B	$-\alpha A a K_1(a) / [2K_2(a)]$
C	$[1 - a K_1(a) \alpha A / 2] / K_0(a)$

second kind. These results are valid up to leading order in an expansion in $1/\log(a)$. The flow fields are the same as those in the Newtonian case,⁴ but the pressure has an additional complex factor.

These first order solutions are necessary for the calculation of the swimming velocity of the filament, which we present in the next subsection. These solutions are also sufficient for calculating the lowest order effects of viscoelasticity on hydrodynamic forces and the shapes of flexible swimmers.¹¹ In the Appendix, we calculate the force per unit length acting on filaments with transverse and longitudinal traveling waves. These results are consistent with the resistive force theory of Fulford *et al.*¹⁸

B. Velocity of a cylinder with prescribed beating pattern

Turning now to the second-order calculation, we expand the boundary condition (10) to second order:

$$[\mathbf{v}^{(2)} + h \hat{\mathbf{x}} \cdot \nabla \mathbf{v}^{(1)}]_{a, \psi, s, t} = 0. \quad (16)$$

To isolate the nonlinear terms of the equation of motion, it is convenient to rewrite the convected time derivatives as

$$\nabla \cdot \boldsymbol{\tau} = \partial_t \boldsymbol{\tau} + \mathbf{T}, \quad (17)$$

$$\nabla \cdot \dot{\boldsymbol{\gamma}} = \partial_t \dot{\boldsymbol{\gamma}} + \mathbf{G}. \quad (18)$$

The second-order equations are

$$(1 + \text{De} \partial_t) \boldsymbol{\tau}^{(2)} = (1 + \text{De}_2 \partial_t) \dot{\boldsymbol{\gamma}}^{(2)} - \text{De} \mathbf{T}^{(2)} + \text{De}_2 \mathbf{G}^{(2)}, \quad (19)$$

or, invoking force balance $-\nabla p^{(2)} + \nabla \cdot \boldsymbol{\tau}^{(2)} = 0$,

$$(1 + \text{De} \partial_t) \nabla p^{(2)} = (1 + \text{De}_2 \partial_t) \nabla^2 \mathbf{v}^{(2)} - \text{De} \nabla \cdot \mathbf{T}^{(2)} + \text{De}_2 \nabla \cdot \mathbf{G}^{(2)}. \quad (20)$$

Note that $\mathbf{T}^{(2)}$ and $\mathbf{G}^{(2)}$ only have contributions from first order flows and stresses.

We must solve Eq. (20) for $v_z^{(2)}$. The time dependence of $v_z^{(2)}$ is most easily expressed by expanding in modes $e^{im(z-t)}$. In our first order calculations, only $m=1$ appeared. Second order involves $m=0, \pm 2$. Similarly, the azimuthal dependence of velocity and stress fields can be expanded in modes of $\cos(n\phi)$ and $\sin(n\phi)$, with $n=0$ and $n=\pm 2$ appearing at second order. To find the swimming velocity, it is only nec-

essary to solve for the time- and ϕ -averaged z -component of the velocity field, which corresponds to the net flow in the z -direction far from the filament. This net flow is the $m=0, n=0$ mode. In the $m=n=0$ part of the second-order equation (20), all terms with ∂_ϕ , ∂_r , and ∂_z drop out, leaving

$$\frac{1}{r} \partial_r [r \partial_r v_z^{(2)(m=n=0)}] = \text{De} \frac{1}{r} \partial_r \left[r T_{rz}^{(2)(m=n=0)} - \frac{\text{De}_2}{\text{De}} r G_{rz}^{(2)(m=n=0)} \right], \quad (21)$$

where T_{rz} can be expressed in cylindrical coordinates as²⁰

$$T_{rz} = v_r \partial_r \tau_{zr} + v_z \partial_z \tau_{zr} + \frac{v_\phi}{r} \partial_\phi \tau_{zr} - \tau_{rr} \partial_r v_z - \tau_{zr} (\partial_z v_z + \partial_r v_r) - \tau_{zz} \partial_z v_r - \frac{\tau_{r\phi}}{r} \partial_\phi v_z - \frac{\tau_{\phi z}}{r} \partial_\phi v_r. \quad (22)$$

A similar expression holds for G_{rz} , with the components of $\boldsymbol{\tau}$ replaced by the corresponding components of $\dot{\boldsymbol{\gamma}}$. Examination of the real part of G_{rz} reveals that every term is proportional to an odd power of $\sin(z-t)$ or $\cos(z-t)$; therefore, the average of G_{rz} over a period vanishes. Integrating Eq. (21) over r yields

$$v_z^{(2)(m=n=0)} = \text{De} \int dr T_{rz}^{(2)(m=n=0)} - U, \quad (23)$$

where U is a constant. The complete expression for $T_{rz}^{(2)}$ in terms of a and the modified Bessel functions $K_0(r)$ and $K_1(r)$ may be constructed from the entries of Table I. To simplify the resulting expression, it is convenient to expand the coefficients αA , B , and C in powers of a . In this expansion, we only keep the leading logarithms. For example, we approximate $K_0(a) \sim \log 2/a - \gamma - \log a$, where γ is the Euler constant. Since we use the boundary condition for $v_z^{(2)}$ at $r=a$ to determine the swimming velocity, we next expand $T_{rz}^{(2)(m,n=0)}$ in powers of a to find

$$T_{rz}^{(m=n=0)} \sim \frac{|\tilde{h}|^2 \text{De} - \text{De}_2}{2} \frac{\log r}{1 + \text{De}^2} \frac{1}{r \log^2 a}. \quad (24)$$

The second order velocity in the $m=0, n=0$ mode is thus

$$v_z^{(2)(m=n=0)}(r) = \frac{|\tilde{h}|^2 \log^2 r}{2 \log^2 a} \frac{\text{De} - \text{De}_2}{1 + \text{De}^2} - U. \quad (25)$$

To determine the constant U , average the boundary condition (16) over t and ϕ to find

$$v_z^{(2)(m=n=0)}|_{r=a} = \left[-h \cos \phi \partial_r v_z^{(1)} + \frac{h}{a} \sin \phi \partial_\phi v_z^{(1)} \right]_{r=a}^{(m=n=0)} = |\tilde{h}|^2 / 2. \quad (26)$$

The swimming velocity is therefore

$$U = -\omega q \frac{|\tilde{h}|^2}{2} \frac{1 + \text{De}^2}{1 + \text{De}^2} \frac{\eta_s}{\eta}, \quad (27)$$

where we have reinstated the dimensions and used $\text{De}_2 = \text{De} \eta_s / \eta$. The filament swims in the same direction as it

would in a Newtonian fluid, opposite the direction of the traveling wave, but with a reduced speed, since $\eta_s/\eta < 1$. This result is valid up to leading order in $1/\log a$, and to second order in \tilde{h} .

In the Appendix we describe the first-order solutions for a longitudinal wave. The same steps just outlined lead to a swimming velocity of

$$U_{\text{long}} = \omega q \frac{|\tilde{h}|^2}{2} \frac{1 + \text{De}^2 \eta_s/\eta}{1 + \text{De}^2}. \quad (28)$$

For a longitudinal wave, the filament again swims in the same direction as it would in a Newtonian fluid, along the direction of the traveling wave, and with a reduced speed. To see why an object with longitudinal propagating waves swims in the direction of the propagating wave, see Ref. 29.

To apply these results to filaments with generic beating patterns, we must consider the swimming velocity of a cylinder with a beating pattern described by a superposition of transverse or longitudinal traveling waves,

$$h(s, t) = \sum_{q, \omega} \tilde{h}_{q, \omega} e^{i(qs - \omega t)}, \quad (29)$$

written in dimensional form. Since the first-order equations are linear, the first order flow is a superposition of flows corresponding to the individual Fourier components $\tilde{h}_{q, \omega}$. As above, the swimming velocity is affected only by $T_{rz}^{(m=n=0)}$ and $G_{rz}^{(m=n=0)}$. Due to the averaging over t involved in obtaining the $m=0$ mode of T_{rz} , the first order flows with different wavelengths do not interact, yielding

$$T_{rz}^{(m=n=0)} = \sum_{q, \omega} T_{rz}^{(m=n=0)}(q, \omega), \quad (30)$$

where $T_{rz}^{(m=n=0)}(q, \omega)$ is $T_{rz}^{(m=n=0)}$ calculated for a single traveling wave. This separation of modes holds for the swimming velocity, and we obtain the dimensional result

$$U = - \sum_{q, \omega} \frac{1 + (\omega\lambda)^2 \eta_s/\eta}{1 + (\omega\lambda)^2} q \omega |\tilde{h}_{q, \omega}|^2. \quad (31)$$

Note that the factor of 2 difference between Eqs. (27) and (31) arises since the single wave $\cos(s-t)$ has $\tilde{h}=1$ in Eq. (6), and $\tilde{h}_{11}=\tilde{h}_{-1-1}=1/2$ in Eq. (29). Finally, we note that for three-dimensional transverse motion,

$$h(s, t) = \sum_{q, \omega} [\hat{\mathbf{e}}_x \tilde{h}_{q, \omega}^x e^{i(qx - \omega t)} + \hat{\mathbf{e}}_y \tilde{h}_{q, \omega}^y e^{i(qx - \omega t)}], \quad (32)$$

the two polarizations decouple upon averaging over ϕ to obtain the $n=0$ mode, leading to

$$U = - \sum_{q, \omega} \frac{1 + (\omega\lambda)^2 \eta_s/\eta}{1 + (\omega\lambda)^2} q \omega (|\tilde{h}_{q, \omega}^x|^2 + |\tilde{h}_{q, \omega}^y|^2). \quad (33)$$

IV. RAMIFICATIONS FOR THE SCALLOP THEOREM

As mentioned in Sec. I, the kinematic reversibility of Stokes equations leads to the scallop theorem for viscous fluids, which states that reciprocal motion of a body leads to no net translation. A reciprocal motion is one which is time reversible, up to a reparametrization in time. In this section, we use the swimming velocity in an Oldroyd B fluid, Eq. (31), to examine how the scallop theorem breaks down in viscoelastic fluids. Equation (31) is only valid to second order in displacements, and all of our statements have the same limitation. Due to this limitation, motions which we identify as having zero swimming speed may have nonzero swimming speeds at higher order; nonetheless, the reciprocal motions that have nonzero swimming speed in Eq. (31) serve to identify the leading order violations of the scallop theorem.

We start with some specific classes of beating motions that satisfy the hypotheses of the scallop theorem. In these examples the motion is confined to a plane, but the conclusions can be generalized to three-dimensional motion. Consider a strictly time-reversal invariant beating motion, $h(s, t) = h(s, -t)$, where h is a transverse deflection, and, without loss of generality, the origin has been chosen as the midpoint of the period. In this case, the Fourier coefficients satisfy $h_{q, \omega} = h_{q, -\omega}$, and therefore the sum in Eq. (31) vanishes. Note that the same argument can be made for space reflection symmetric beating patterns as well. Next, consider a beating motion which has effectively only one degree of freedom: $h(s, t) = f(t)g(s)$. In this case, the Fourier coefficients are also factorizable, so $h_{q, \omega} = f(\omega)g(q)$. Since both $f(t)$ and $g(s)$ are real functions, $f(\omega) = f^*(-\omega)$ and $g(q) = g^*(-q)$, and therefore $|h_{q, \omega}|^2 = |h_{q, -\omega}|^2$. As a result, the summand in Eq. (31) is odd in ω , and the swimming speed vanishes. More generally, any motion with $|h_{q, \omega}| = |h_{q, -\omega}|$, which corresponds to a superposition of standing waves, leads to no net translation.

These examples demonstrate how time-reversible motions lead to zero swimming speed at leading order in an Oldroyd B fluid. In a Newtonian fluid at zero Reynolds number, more general reciprocal motions, such as a fast power stroke followed by a slow return stroke, also lead to zero swimming speed. To see how this conclusion does not apply to the Oldroyd B fluid, it is convenient to write the swimming speed U in the time domain and in real space,

$$U = \int_0^T \frac{dt}{T} \int_0^L \frac{ds}{L} \int_{-\infty}^t dt' \frac{\partial h}{\partial s}(s, t) M(t, t') \frac{\partial h}{\partial t'}(s, t'), \quad (34)$$

where the memory kernel $M(t, t')$ is the operator

$$\frac{1}{\lambda} e^{-(t-t')/\lambda} \left(1 - \frac{\lambda^2 \eta_s}{\eta} \frac{\partial^2}{\partial t'^2} \right). \quad (35)$$

Any reciprocal motion $h(s, t)$ with period T may mapped to a strictly time-reversal invariant motion by a reparametrization $t_1 = F(t)$, where F is monotonic, $F(0)=0$, and $F(T)=T$. For convenience we have chosen the origin as the beginning of the period. In the Newtonian case, $\lambda=0$, and the kernel in Eq. (34) becomes a Dirac delta function, $M(t, t') = \delta(t - t')$, with the interpretation that the singularity of the delta function lies

within the region of integration. Inspection of the resulting expression for U reveals that it is reparametrization invariant, and we conclude that our formula for the swimming speed obeys the scallop theorem for general reciprocal motions in a Newtonian liquid at zero Reynolds number. However, when $\lambda \neq 0$, the kernel $M(t, t')$ spoils reparametrization invariance, and the speed need not vanish. The physical interpretation is

that the distance covered per period in a non-Newtonian fluid depends on the rate of motion as well as the sequence of shapes.

For example, consider a helical wave which propagates forward by one wavelength in the first third of the time period, and then backward by one wavelength in the final two-thirds of the period:

$$\mathbf{h}(s, t) = \begin{cases} b \cos(s - 3t)\hat{\mathbf{e}}_x + b \sin(s - 3t)\hat{\mathbf{e}}_y, & 0 < t < 2\pi/3, \\ -b \cos(s + 3t/2)\hat{\mathbf{e}}_x - b \sin(s + 3t/2)\hat{\mathbf{e}}_y, & 2\pi/3 < t < 2\pi. \end{cases} \quad (36)$$

For this motion, the Fourier amplitudes for $\omega=3$ are $h_{1,3}^x = h_{-1,-3}^x = ih_{1,3}^y = -ih_{-1,-3}^y = b/6$. For $\omega \neq 3$, we have $h_{-1,-\omega}^x = (h_{1,\omega}^x)^*$, $h_{1,\omega}^y = -ih_{1,\omega}^x$, and $h_{-1,-\omega}^y = (h_{1,\omega}^y)^*$, where

$$h_{1,\omega}^x = \frac{9b \exp(-i\pi\omega/3) \sin(\pi\omega/3)}{4\pi (\omega - 3)(\omega + 3/2)}. \quad (37)$$

All other $h_{q,\omega}$ are zero. Note that these coefficients do not obey the criterion $|h_{q,\omega}| = |h_{q,-\omega}|$. Inserting these coefficients into Eq. (33) and using contour integration to evaluate the resulting sums³⁰ yields the dimensionless speed

$$U = - \left(1 - \frac{\eta_s}{\eta} \right) \frac{27\text{De}^2 b^2}{\pi} \left[\frac{-\pi(4 + 45\text{De}^2 + 81\text{De}^4) + \frac{18\text{De}(2 + 9\text{De}^2) \sinh \frac{2\pi}{3\text{De}}}{3\text{De}}}{1 + 2\cosh \frac{2\pi}{3\text{De}}} \right] \frac{1}{(4 + 45\text{De}^2 + 81\text{De}^4)^2}, \quad (38)$$

where $\text{De} = 2\pi\lambda/T$ and T is the dimensional period of the motion.

The swimming speed vanishes in the Newtonian limits of no polymer, $\eta_s = \eta$, or zero relaxation time, $\text{De} = 0$. For these cases, the swimmer moves in the negative direction during the first third of the period, and in the positive direction by the exact same amount during the last two-thirds of the period. In the viscoelastic case, the swimmer moves more slowly during the first third of the period when the wave frequency is high. Thus, the scallop theorem is rendered inapplicable and the net motion of the swimmer is in the positive (forward) direction. Formula (38) for the swimming speed is complicated due to memory effects: the speed of the swimmer during each stroke depends on its motion during previous strokes. However, we can make a simple estimate for the swimming speed by disregarding these memory effects and using Eq. (27) to estimate the speed during each stroke of the waveform of Eq. (36):

$$U_{\text{est}} = b^2 \left[\frac{1 + (9/4)\text{De}^2(\eta_s/\eta)}{1 + (9/4)\text{De}^2} - \frac{1 + 9\text{De}^2(\eta_s/\eta)}{1 + 9\text{De}^2} \right]. \quad (39)$$

Figure 3 shows the exact second-order [Eq. (38)] and estimated [Eq. (39)] swimming speeds for the waveform [Eq. (36)], with dimensional wavelength $2\pi/q$.

Helical waves provide a convenient experimental system to explore the fate of the scallop theorem in viscoelastic fluids, since the backward and forward traveling waves could be easily actuated by rotating a rigid helical filament

wrapped in a flexible rubber sleeve.⁴ For a cylinder of radius $a = 1$ cm deformed into a helix with pitch $2\pi/q = 12$ cm and helical radius $h = 0.5$ cm rotating with a period $T = 1.5$ s, the swimming velocity of a helix in a Newtonian fluid is $U = \omega q h^2 \sim 0.5$ cm/s, which corresponds to unity on the vertical axis of Fig. 3. Note that these values are chosen to make $aq \approx 0.5$, $bq \approx 0.25$, and $h/a \approx 0.5$. The time constant needed

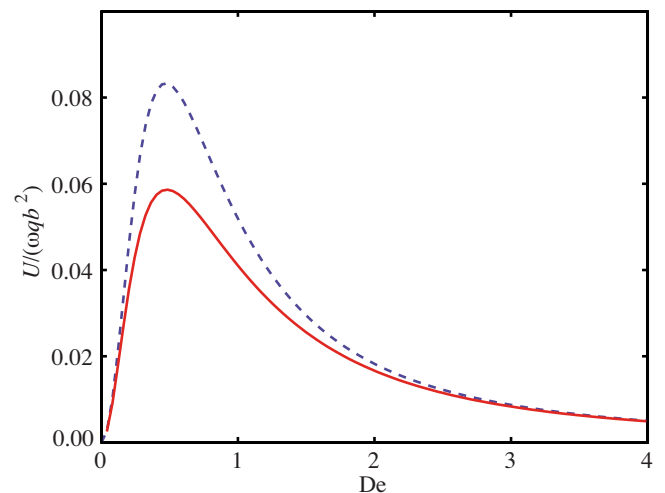


FIG. 3. (Color online) The swimming velocity of the reciprocal motion of Eq. (36) vs $\text{De} = 2\pi\lambda/T$, for $\eta_s/\eta = 0.75$. The (red) solid curve is the exact second-order result of Eq. (38); the (blue) dashed curve corresponds to the estimate of Eq. (39).

to place the swimming velocity around the maximum value would be on the order of 0.1 s, which is within the range of time constants found in Boger fluids.²⁶ Also assuming that $1 - \eta_s/\eta = \eta_p/\eta_s \approx 0.25$, again typical for Boger fluids,^{26,31} the swimming velocity for our example time-varying reciprocal motion is 0.1–0.5 mm/s. Note that larger swimming speeds might be obtained by using fluids with smaller time constant λ , but care must be taken to remain in the low Reynolds number regime. For the parameters we used above, the Reynolds number is less than 0.01 for a Boger fluid with viscosity in the range of 0.2–0.5 Pa s.

V. CONCLUSION

In this paper we have calculated the swimming velocity for an infinite cylinder undergoing arbitrary periodic beating motion in a nonlinearly viscoelastic Oldroyd-B fluid. We have assumed that the amplitude of deflection is small compared to the wavelength of deformations and compared to the radius of the cylinder. We find that in general, nonlinear viscoelastic corrections decrease the swimming velocity relative to the Newtonian case. It is interesting to note that the decrease in swimming velocity depends on the nonlinearity: in a linear Maxwell fluid, even though the time-reversal invariance of the constitutive relation is manifestly broken by memory effects through the time derivative of the stress, for a given swimming motion, the flows are exactly the same as the Newtonian case (although the stresses are modified).¹⁸ Nonlinearity in the constitutive relation is required to rectify the changes in the stress into changes in flows. We have used our calculation to examine the breakdown of the scallop theorem in a nonlinearly viscoelastic fluid. Within our assumptions of small amplitude deflections of an infinitely long filament, time-reversal-invariant motions lead to no net translation. We further showed that net motion in a nonlinearly viscoelastic fluid is possible for a more general reciprocal motion, in which the backward and forward strokes occur at different rates. These predictions could be readily tested with simple tabletop experiments. The nonlinearity of our constitutive relation necessarily limited our analytical results to the case of small deflection. It would be of great value to develop a proper local resistance theory for slender rods in a nonlinearly viscoelastic fluid.

In this paper we have worked in the frequency domain, building arbitrary motions through superposition. This allows us to easily treat time-periodic motions, but does not lend itself to a physical understanding of motions that suddenly stop or start, which require a complicated superposition of many frequencies. In numerical studies of peristaltic flows, Teran *et al.*³² explored the buildup of stresses from an initial fluid stress given by an isotropic pressure. In this context, time-periodic flows correspond to asymptotic long-time behavior, which may take a long time to develop in numerical simulations. The numerical studies provide a complementary viewpoint well-suited to revealing transient behavior in flows.

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APPENDIX: FORCES ON A CYLINDER WITH PRESCRIBED BEATING PATTERN

The force per unit length acting on the cylinder is found by integrating the stress tensor around the circumference,

$$\mathbf{f}(s) = a \int \hat{\mathbf{n}}(\psi, z) \cdot \boldsymbol{\sigma}(r_b, \phi_b, z_b) d\psi, \quad (\text{A1})$$

where the dependence of the cylindrical coordinates $\{r_b, \phi_b, z_b\}$ on ψ and s depends on the deformation. First consider the force per unit length \mathbf{f}_\perp for a transverse wave with polarization in the x -direction only, Eq. (6). Mirror symmetry about the xz -plane implies that $f_{\perp y} = 0$. To lowest order, $\hat{\mathbf{n}} = \hat{\mathbf{r}}$, $r_b = a$, $\phi_b = \psi$, and $z_b = s$ [see Eq. (9)]. Upon integration over ψ , the force in the $\hat{\mathbf{z}}$ -direction arising from $\sigma_{rz}^{(1)} = \tau_{rz}^{(1)}$ vanishes, and the force per unit length arising from $\sigma_{rr}^{(1)} = -p^{(1)} + \tau_{rr}^{(1)}$ and $\sigma_{r\phi}^{(1)} = \tau_{r\phi}^{(1)}$ is

$$\mathbf{f}_\perp^{(1)} = \text{Re} \left\{ \frac{4\pi}{\log a} \frac{1-i\text{De}_2}{1-i\text{De}} (-i\tilde{h}e^{i(s-t)}) \right\} \hat{\mathbf{x}}. \quad (\text{A2})$$

This force is accurate to lowest order in $1/\log(a)$.

Now consider longitudinal traveling waves:

$$\mathbf{r}(s, \psi) = \hat{\mathbf{x}}a \cos \psi + \hat{\mathbf{y}}a \sin \psi + \hat{\mathbf{z}} \text{Re}[\tilde{h}e^{i(qs-\omega t)} + s]. \quad (\text{A3})$$

Using cylindrical coordinates, the position of the surface can also be described by (r_b, ϕ_b, z_b) . To first order in h ,

$$r_b = a,$$

$$\phi_b = \psi, \quad (\text{A4})$$

$$z_b = s + h.$$

As in the transverse case, the no-slip boundary conditions at the filament surface are found by expanding the argument of the flow velocity at the surface to first order,

$$[\mathbf{v} + h\hat{\mathbf{z}} \cdot \nabla \mathbf{v}]_{a, \psi, s, t} = \dot{\tilde{h}}\hat{\mathbf{z}}. \quad (\text{A5})$$

The nondimensional first and second order flow equations are the same as in the transverse case, but the boundary condition is different. At first order, $\tilde{v}_z(a, \psi) = -i\dot{\tilde{h}}\hat{\mathbf{z}}$. The first order velocity field and pressure are shown in Table II. Using these solutions in general expression for the force per unit length, Eq. (A1), we find that the first order force for a longitudinal traveling wave is

$$\mathbf{f}_\parallel^{(1)} = \text{Re} \left\{ \frac{2\pi}{\log a} \frac{1-i\text{De}_2}{1-i\text{De}} [-i\dot{\tilde{h}}e^{i(s-t)}] \right\} \hat{\mathbf{z}}. \quad (\text{A6})$$

As explained before, the first order force is sufficient for calculating the lowest order changes to swimming properties

TABLE II. Pressure and velocity field for a cylinder with a longitudinal traveling wave; $\alpha=(1-i\text{De})/(1-i\text{De}_2)$.

\bar{p}	$\tilde{h}K_0(r)$
\tilde{v}_r	$\tilde{h}[\alpha ArK_0(r)/2+BK_1(r)]$
\tilde{v}_ϕ	0
\tilde{v}_z	$-i\tilde{h}[(B-\alpha A)K_0(r)+\alpha ArK_1(r)/2]$
αA	$-2K_1(a)/\{a[K_0(a)^2-K_1(a)^2]+2K_0(a)K_1(a)\}$
B	$aK_0(a)/\{a[K_0(a)^2-K_1(a)^2]+2K_0(a)K_1(a)\}$

that result from shape changes in beating patterns in viscoelastic media. To apply Eq. (A2), we interpret it in a manner consistent with resistive force theory.¹⁷ Since the quantity $-\tilde{h}\exp(is-it)$ is the transverse velocity of the cylinder, the force per unit length has a complex transverse resistance coefficient of $-(4\pi/\log a)(1-i\text{De}_2)/(1-i\text{De})$ for motion occurring with dimensional space and time dependence $\exp(iqs-i\omega t)$. This resistance coefficient depends on q through the dimensionless parameter a . As is commonly done in resistive force theory, to treat general motion involving a superposition of traveling waves with multiple wavelengths, we replace the slow logarithmic dependence on q with a constant involving a typical wavevector $\langle q \rangle$. The error introduced in this process is of order $(q-\bar{q})/(\bar{q}\log\bar{q})$. After this replacement we obtain a resistance coefficient, in dimensional form, of

$$\zeta_{\perp}^{\text{Oldroyd}} = -\zeta_{\perp} \frac{1-i\text{De}_2}{1-i\text{De}}, \quad (\text{A7})$$

$$\zeta_{\perp} = -\frac{4\pi\eta}{\log\langle q \rangle a}. \quad (\text{A8})$$

The parallel resistance coefficient is obtained by a similar analysis for the longitudinal wave, and is given by $\zeta_{\parallel}^{\text{Oldroyd}} = \zeta_{\perp}^{\text{Oldroyd}}/2$ and $\zeta_{\parallel} = \zeta_{\perp}/2$. Generalization to motion with multiple frequencies or helical waves may be accomplished by linear superposition. This choice of ζ_{\perp} and ζ_{\parallel} is consistent with those previously introduced for the Newtonian resistive force theory.

With this choice of resistance coefficients, the first-order force per unit length obeys

$$\mathbf{f} + \lambda \dot{\mathbf{f}} = \mathbf{f}_{\text{vis}} + \frac{\eta_s}{\eta} \lambda \dot{\mathbf{f}}_{\text{vis}}, \quad (\text{A9})$$

where \mathbf{f}_{vis} is the force per unit length from Newtonian resistive force theory,

$$\mathbf{f}_{\text{vis}}(s,t) = \zeta_{\perp} \mathbf{v}_{\perp}(s,t) + \zeta_{\parallel} \mathbf{v}_{\parallel}(s,t) \quad (\text{A10})$$

and $\mathbf{v}_{\perp}(s,t)$ and $\mathbf{v}_{\parallel}(s,t)$ are the perpendicular and parallel components of the flow velocity *relative to the rod* at the point s on the rod. The velocity \mathbf{v} must be interpreted as a relative velocity to maintain Galilean invariance. In the limit of zero solvent viscosity, $\eta_s=0$, these equations are equivalent to the resistive force theory proposed by Fulford *et al.* for the linear Maxwell model.¹⁸

We can now see why the resistive force theory [Eq. (A9)] leads to no change in swimming speed relative to

Newtonian resistive force theory. First note that in resistive force theory, the swimming velocity of a body is determined by demanding that the total force $\mathbf{F} = \int d\mathbf{s} \mathbf{f}$ on the body vanishes. Integrating Eq. (A9) over arclength s and then averaging over a period leads to the condition $\int d\mathbf{s} \mathbf{f}_{\text{vis}} = 0$, the same condition for determining the swimming velocity in the Newtonian case.

Although Eq. (A9) gives internally consistent predictions for the swimming speed of a filament with a traveling wave, it is nevertheless flawed. To see why, recall our motivation of the nonlinear constitutive relation for a fluid with fading memory in Sec. II. There we saw that without the nonlinear terms of the upper-convective derivative, the Maxwell constitutive relation for an element is sensitive to the local rate of rotation of that element. To illustrate this effect, consider shear flow in a channel on a slowly rotating table. A short calculation shows that the zero-frequency shear viscosity depends on the rate of rotation of the table, an unphysical result if the rate of rotation is low enough that the fictitious forces acting on the polymers in solution are small compared to the viscous forces.²⁰

Likewise, we may consider a slender filament on a table rotating with speed Ω , and ask if Eq. (A9) predicts forces that are independent of Ω . Set $\eta_s=0$ for convenience. Both the fluid and the filament are rotating with the same speed. Suppose further that the filament is moved with steady velocity \mathbf{v} relative to the fluid. Unless Ω is enormously large, we expect the force per unit length \mathbf{f} to eventually relax to the viscous force per unit length [Eq. (A10)]. However, writing Eq. (A9) in terms the perpendicular and parallel components, and solving for the force in the steady state yields

$$f_{\parallel} = \frac{\zeta_{\parallel} v_{\parallel} + \lambda \Omega \zeta_{\perp} v_{\perp}}{1 + \lambda^2 \Omega^2}, \quad (\text{A11})$$

$$f_{\perp} = \frac{\zeta_{\perp} v_{\perp} - \lambda \Omega \zeta_{\parallel} v_{\parallel}}{1 + \lambda^2 \Omega^2}. \quad (\text{A12})$$

Thus, we see explicitly that the resistive force theory for the Maxwell constitutive relation predicts spurious dependence on the rotation speed Ω . Equation (A9) is only truly reliable when working to linear order in deflection.

¹W. Ludwig, "Zur Theorie der Flimmerbewegung (Dynamic, Nutzeffekt, Energiebalanz)," *Zeitschrift für Vergleichende Physiologie* **13**, 397 (1930).

²E. M. Purcell, "Life at low Reynolds number," *Am. J. Phys.* **45**, 3 (1977).

³G. I. Taylor, "Analysis of the swimming of microscopic organisms," *Proc. R. Soc. London, Ser. A* **209**, 447 (1951).

⁴G. I. Taylor, "The action of waving cylindrical tails in propelling microscopic organisms," *Proc. R. Soc. London, Ser. A* **211**, 225 (1952).

⁵K. E. Machin, "Wave propagation along flagella," *J. Exp. Biol.* **35**, 796 (1958).

⁶C. H. Wiggins and R. E. Goldstein, "Flexive and propulsive dynamics of elastica at low Reynolds number," *Phys. Rev. Lett.* **80**, 3879 (1998).

⁷T. S. Yu, E. Lauga, and A. E. Hosoi, "Experimental investigations of elastic tail propulsion at low Reynolds number," *Phys. Fluids* **18**, 091701 (2006).

⁸S. Camalet, F. Jülicher, and J. Prost, "Self-organized beating and swimming of internally driven filaments," *Phys. Rev. Lett.* **82**, 1590 (1999).

⁹S. Camalet and F. Jülicher, "Generic aspects of axonemal beating," *New J. Phys.* **2**, 24 (2000).

- ¹⁰I. H. Riedel-Kruse, A. Hilfinger, J. Howard, and F. Julicher, "How molecular motors shape the flagellar beat," *HFSP J.* **1**, 192 (2007).
- ¹¹H. C. Fu, C. W. Wolgemuth, and T. R. Powers, "Beating patterns of filaments in viscoelastic fluids," *Phys. Rev. E* **78**, 041913 (2008).
- ¹²S. S. Suarez and H. Ho, "Hyperactivation motility in sperm," *Reprod. Domest. Anim.* **38**, 119 (2003).
- ¹³S. Suarez, D. Katz, D. Owen, J. Andrew, and R. Powell, "Evidence for the function of hyperactivated motility in sperm," *Biol. Reprod.* **44**, 375 (1991).
- ¹⁴S. Suarez and X. Dai, "Hyperactivation enhances mouse sperm capacity for penetrating viscoelastic media," *Biol. Reprod.* **46**, 686 (1992).
- ¹⁵C. Montecucco and R. Rappuoli, "Living dangerously: How *Helicobacter pylori* survives in the human stomach," *Nat. Rev. Mol. Cell Biol.* **2**, 457 (2001).
- ¹⁶C. W. Wolgemuth, N. W. Charon, S. F. Goldstein, and R. E. Goldstein, "The flagellar cytoskeleton of the spirochetes," *J. Mol. Microbiol. Biotechnol.* **11**, 221 (2006).
- ¹⁷J. Gray and G. J. Hancock, "The propulsion of sea-urchin spermatozoa," *J. Exp. Biol.* **32**, 802 (1955).
- ¹⁸G. R. Fulford, D. F. Katz, and R. L. Powell, "Swimming of spermatozoa in a linear viscoelastic fluid," *Biorheology* **35**, 295 (1998).
- ¹⁹E. Lauga, "Propulsion in a viscoelastic fluid," *Phys. Fluids* **19**, 083104 (2007).
- ²⁰R. B. Bird, R. C. Armstrong, and O. Hassager, *Fluid Mechanics, Dynamics of Polymeric Liquids Vol. 1*, 2nd ed. (Wiley, New York, 1987).
- ²¹H. C. Fu, T. R. Powers, and C. W. Wolgemuth, "Theory of swimming filaments in viscoelastic media," *Phys. Rev. Lett.* **99**, 258101 (2007).
- ²²P. de Gennes, "Comment contributed to discussion," *Physica A* **118**, 43 (1983).
- ²³J. G. Oldroyd, "On the formulation of rheological equations of state," *Proc. R. Soc. London, Ser. A* **200**, 523 (1950).
- ²⁴F. A. Morrison, *Understanding Rheology* (Oxford University Press, New York, 2001).
- ²⁵R. B. Bird, R. C. Armstrong, and O. Hassager, *Kinetic Theory, Dynamics of Polymeric Liquids Vol. 2*, 2nd ed. (Wiley, New York, 1987).
- ²⁶D. V. Boger and R. J. Binnington, "Constant viscosity elastic liquids," *J. Rheol.* **29**, 887 (1986).
- ²⁷J. Happel and H. Brenner, *Low Reynolds Number Hydrodynamics* (Prentice-Hall, Englewood Cliffs, NJ, 1965).
- ²⁸L. D. Landau and E. M. Lifshitz, *Fluid Mechanics*, 2nd ed. (Butterworth-Heinemann, Oxford, 1987).
- ²⁹K. M. Ehlers, A. D. Samuel, H. C. Berg, and R. Montgomery, "Do cyanobacteria swim using traveling surface waves?" *Proc. Natl. Acad. Sci. U.S.A.* **93**, 8340 (1996).
- ³⁰G. F. Carrier, M. Krook, and C. E. Pearson, *Functions of a Complex Variable* (McGraw-Hill, New York, 1966).
- ³¹N. Phan-Thien, "Stagnation flows for the Oldroyd-B fluid," *Rheol. Acta* **23**, 172 (1984).
- ³²J. Teran, L. Fauci, and M. Shelley, "Peristaltic pumping and irreversibility of a Stokesian viscoelastic fluid," *Phys. Fluids* **20**, 073101 (2008).