CARDIOLOGY

Cardiology 2012;121:263–273 DOI: 10.1159/000338705 Received: February 19, 2012 Accepted: March 23, 2012 Published online: May 22, 2012

The Right Ventricle in Health and Disease: Insights into Physiology, Pathophysiology and Diagnostic Management

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Key Words

 $\label{eq:result} \begin{array}{l} \mbox{Right ventricle} \cdot \mbox{Physiology} \cdot \mbox{Pathophysiology} \cdot \mbox{Heart} \\ \mbox{failure} \end{array}$

Abstract

Until recently, the right ventricle (RV) received little attention in adult patients with congenital heart disease and even less attention in the setting of acquired heart failure. However, in the last two decades, our perspective towards the right side of the heart has begun to change. Advances in imaging modalities have permitted the accurate study of RV physiology and made it apparent that RV function is an important determinant of prognosis in heart failure irrespective of the underlying etiology. This article summarizes the existing data on the unique anatomical and physiological features of the RV. The hemodynamic conditions and cellular and biochemical pathways that lead to right heart failure are presented. Moreover, the imaging modalities that aid in the assessment of RV structure and function are described and the importance of the diagnostic and prognostic information they provide is discussed. Copyright © 2012 S. Karger AG, Basel

Introduction

In 1616, the English physician Sir William Harvey first described the physiology of the pulmonary circulation in his thesis, De Motu Cordis [1]. Nevertheless, over a period

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Accessible online at: www.karger.com/crd of almost four centuries, limited emphasis was placed on the right ventricle (RV) and its role in the pathophysiology of heart disease. In fact, only in the past two decades have we begun to witness a constant increase in the attention paid by researchers and clinicians to the right heart chambers; this interest has been paralleled by the evolution of invasive and noninvasive cardiac imaging methods which have dramatically improved our understanding of the anatomy, physiology and pathophysiology of the right heart as well as pulmonary circulation in both congenital and acquired heart disease.

In this article we summarize the unique anatomical and physiological features of the RV, the pathophysiology underlying right heart failure and the emerging imaging modalities that aid in the assessment of RV function. Moreover, the prognostic impact of RV function under high preload and afterload conditions is discussed.

Right Ventricular Anatomy

In the human heart, the RV is anteriorly situated immediately behind the sternum. In the absence of congenital heart disease, it lies between the annulus of the tricuspid valve and the pulmonary valve. It consists of an inflow (sinus) and an outflow (conus) portion separated by the crista supraventricularis [2–4]. For the sake of standardization in cardiac imaging, it has been divided into an anterior, lateral and inferior segment, as well as

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Table 1. Anatomical features that differentiate the two ventricles

	RV	LV
Shape	crescent-shaped/triangular	elliptic
EDV, mm ³	75 ± 13 (49–101)	66 ± 12 (44–89)
Mass, g/m ² BSA	26 ± 5 (17–34)	87 ± 12 (64–109)
Wall thickness, mm	2–5	7–11

BSA = Body surface area; EDV = end-diastolic volume.

into a basal, mid and apical section [2–4]. Three major muscular bands are present in the RV: the parietal, septomarginal and moderator bands [5]. The following morphological characteristics further distinguish the RV from the left ventricle (LV):

- more apical hinge line of the septal leaflet of the tricuspid valve relative to the anterior leaflet of the mitral valve
- presence of a moderator band
- presence of more than three papillary muscles
- trileaflet configuration of the tricuspid valve with septal papillary attachments
- presence of coarse trabeculations.

These unique anatomic features are particularly helpful for recognizing the RV in the presence of congenital anomalies.

The RV has a more complex shape than the LV, appearing triangular when viewed from the side and semilunar (crescent-shaped) when viewed in cross section; its 3-dimensional shape is more complex, unlike the ellipsoid shape of the LV, a fact which reflects the low resistance in the pulmonary circulation [5]. The RV myocardium is thinner and its mass approximately one sixth of that of the LV, with an almost similar (slightly higher) end-diastolic volume (table 1) [5].

The RV wall is mainly composed of superficial and inner (deep) muscle layers; the fibers of the superficial layer are aligned circumferentially parallel to the atrioventricular groove, while the inner fibers are set longitudinally from base to apex. Importantly, the RV and LV myocardium are functionally interdependent: they share a common wall, the interventricular septum, have mutually encircling epicardial fibres and lie within the same intrapericardial space [5].

The blood supply to the RV varies according to the dominance of the coronary system. In a right-dominant system, the right coronary artery supplies the RV free wall in the posterior, right lateral and anterior segments of the heart. In addition, the right coronary artery supplies the inferior third of the interventricular septum. The RV is also supplied with blood from the left anterior descending artery [5]. In the absence of RV hypertrophy or pressure overload, epicardial right coronary artery flow occurs during both systole and diastole. However, beyond the RV marginal branches, blood flow is predominantly diastolic [6].

Right Ventricular Physiology and Hemodynamics

The primary function of the RV is to forward systemic venous return into the pulmonary circulation. In the normal human heart, the RV is connected in series with the LV and therefore ejects, on average, the same stroke volume [5, 6]. RV contraction occurs in a sequential manner, as a peristaltic wave directed from the inflow to outflow tract. Deformation of the RV myocardium is the result of three contraction patterns: inward movement (free wall), longitudinal and circumferential; longitudinal shortening is the major contributor to overall RV contraction, while traction of the RV free wall secondary to LV contraction may contribute to as much as 40% of the stroke volume [7]. In contrast to the LV, twisting and rotational movements do not significantly contribute to RV performance [6, 7].

The physiological hemodynamics of the RV as opposed to the LV are summarized in table 2. In the absence of cardiac or pulmonary disease, right-sided pressures are significantly lower than left-sided pressures [8]. As a consequence, RV filling starts before and finishes after LV filling. RV systolic pressure rapidly exceeds the low pulmonary artery diastolic pressure and thus RV isovolumic relaxation time is shorter when compared to the LV, and filling velocities are lower and with more pronounced respiratory variations. As is the case for the LV, RV performance depends on myocardial contractility, afterload and preload and is influenced by heart rhythm, intraventricular synchrony and ventricular interdependence [6].

Compared to the LV, the less muscular RV (table 1) is more sensitive to afterload alterations; in clinical practice, pulmonary vascular resistance is the most important determinant of RV afterload [6, 8].

In the normal heart, an increased RV preload improves myocardial contraction on the basis of the Frank-Starling law. Nevertheless, excessive and prolonged RV volume overload reduces RV contractility and suppresses LV filling, ultimately leading to impaired global heart function [8]. Factors affecting RV preload include intra-

	RV	LV
Elastance (E _{max}), mm Hg/ml	1.30 ± 0.84	5.48 ± 1.23
PVR vs. SVR, dyn•s•cm ⁻⁵	70 (20–130)	1,100 (700-1,600)
End-diastolic compliance	high	low
Ejection fraction, %	$61 \pm 7 (47 - 76)$	$67 \pm 5 (57 - 78)$
Stroke work index, g/m ² BSA/beat	$8 \pm 2 (1/6 \text{ of LV})$	50 ± 20
Resistance to ischemia	high	low
Adaptation to disease	better for volume overload	better for pressure overload

 Table 2. Physiological hemodynamics of the right as opposed to the left ventricle

vascular volume status, ventricular compliance, heart rate, LV filling pressure and pericardial pressure [8].

Ventricular interdependence refers to the concept that the size, shape and compliance of one ventricle affect the hemodynamic properties of the other [9]. The anatomical background of ventricular interdependence is (1) the presence of the interventricular septum, (2) the continuity of RV myocardial fibers and LV muscular layers and (3) the fact that both ventricles share the same pericardial cavity. Ventricular interdependence plays an essential part in the pathophysiology of RV dysfunction. Interdependence may affect both diastolic and systolic hemodynamic properties. Systolic ventricular interdependence is mediated mainly through the interventricular septum, while the pericardium contributes more to diastolic ventricular interdependence [9]. In acute RV pressure- or volume-overload states, dilatation of the RV increases intrapericardial pressure and shifts the interventricular septum to the left, altering LV geometry. As a consequence, the LV diastolicpressure volume curve shifts upward, leading to a decreased LV preload, increased LV end-diastolic pressure and consequently a low cardiac output [9].

Pathophysiology of Right Ventricular Dysfunction and Failure

The pathologic conditions and mechanisms that may lead to RV failure are summarized in figure 1 [10]. Right heart failure is becoming an increasingly frequent entity in current clinical practice as the prevalence of predisposing conditions in the population increases. In the majority of cases, RV function is compromised as a result of pressure overload, volume overload or a combination of both. Impaired RV contractility due to primary loss of RV myocardium can also underlie right heart failure; however, conditions leading to RV myocardial damage are, with the exception of ischemia, rare and generally not confined to the right heart. Importantly, up to 25% of critically ill patients with acute lung injury and up to 50% of those with sepsis may develop acute right heart failure in the intensive care unit due to multiple mechanisms (fig. 2) [10].

Acute pulmonary embolism (PE) is the prototype of RV failure due to acute pressure overload [11]. Increased pulmonary artery pressure occurs in 60-70% of patients who have PE and roughly correlates with the anatomic severity of thromboembolic obstruction; in addition, vasoconstrictive factors released from the thrombus and reaction to hypoxia contribute to the increase in pulmonary vascular resistance [12-14]. Moreover, preexisting cardiac or pulmonary disease may enhance the hemodynamic impact of an acute thromboembolic event. Right ventricular dilatation and hypokinesis result from the interplay of these factors and may initiate a vicious circle of increased myocardial oxygen demand, myocardial ischemia or infarction and left ventricular preload reduction. Ultimately, the inability to maintain the cardiac index and arterial pressure leads to cardiogenic shock (fig. 3) [15, 16]. Thus, RV dysfunction is the critical hemodynamic event and an important determinant of the clinical presentation, course and prognosis of PE.

The pathophysiology of chronic pressure overload, which may lead to repeated episodes of acute decompensation, has been thoroughly studied in the setting of pulmonary arterial hypertension (PAH); at present, we can only assume that similar adaptive mechanisms underlie other high-afterload conditions. The first step in RV adaptation to pressure overload is myocardial hypertrophy and assumption of a spherical geometry in an effort to

RV Physiology in Health and Disease



Fig. 1. Causes and mechanisms of right heart failure. ARVD = Arrhythmogenic right ventricular dysplasia; ASD = atrial septal defect; CABG = coronary artery bypass grafting surgery; MV = mitral valve; PR = pulmonary regurgitation; RVOT = right ventricular outflow tract; SVC = superior vena cava; TR = tricuspid regurgitation.



Fig. 2. Mechanisms of right heart failure in critically ill patients. IL = Interleukin; $TNF\alpha$ = tumor necrosis factor α .



Fig. 3. Right heart failure due to acute pressure overload resulting from pulmonary embolism. PA = Pulmonary artery.

reduce wall stress [17]. The increase in ventricular mass induced by an increase in afterload is predominantly the result of protein synthesis and an increase in cell size through the addition of sarcomeres in parallel. Protein synthesis in the cardiomyocytes is directly induced by stretch and enhanced by autocrine, paracrine and neurohormonal signals including activation of the renin-angiotensin and enhanced sympathetic activity [17, 18]. However, the RV is not capable of sustaining pressure overload over the long term. Cardiac contractile force decreases, probably due to functional and/or structural changes in cardiomyocytes. In fact, pressure-induced growth and proliferation of cardiomyocytes is accompanied by extracellular matrix synthesis, which influences diastolic and systolic function as well as ventricular morphology and provides the background for electrical instability [19, 20]. The RV thus enters a vicious circle of increased wall tension, mismatch in myocardial oxygen demand and RV perfusion, furthering impairment in contractility and dilatation [17]. Maladaptive neurohormonal signaling, oxidative stress and inflammation may further contribute to the development of right heart failure [17].

The biochemical background of cardiomyocyte dysfunction under pressure overload is partly unclear. A constant finding in maladaptive cardiac remodeling is the alpha to beta isotype switch of the myosin heavy chains (MCH). In the normal adult RV, the alpha-MHC isotype makes up approximately one third of total MHC. The reduction in alpha-MHC content that is encountered in PAH-associated right heart failure can have important functional consequences [21]: beta-MHC has lower adenosine triphosphatase activity than alpha-MHC, resulting in a significant decrease in systolic function [22]. Stressed hearts not only exhibit thick filament changes but also show increased expression of the thin filaments alpha-skeletal actin and alpha-smooth-muscle actin at the cost of alpha-cardiac actin [22-25]. However, the functional consequences of the alpha actin switch are not clear. The myocardial regulatory proteins troponin, tropomyosin and tropomodulin may also be involved in the pathobiology of right heart failure [26]. Phosphorylation of troponin T by protein kinase C inhibits troponin T binding to tropomyosin, which may contribute to the inhibition of maximal myofibrillar adenosine triphosphatase and contractile performance [26, 27]. Finally, abnormalities in enzymes and ion channels involved in myocyte stimulation/contraction, mitochondrial defects, depletion of myocardial adenosine triphosphate and modifications of myocardial substrate use (from fatty acids to glucose) have been implicated in maladaptive remodeling [18].

In addition to pressure effects, conditions including adult congenital heart disease and acquired valvular heart disease may place substantial volume loads on the RV. Such conditions include atrial septal defect, pulmonary artery regurgitation and tricuspid regurgitation. The RV responds to volume overload with an enhancement of contractile properties. Eccentric hypertrophy, during which terminally differentiated cardiomyocytes increase in size without undergoing cell division, is the initial adaptive response of the heart to volume overload. Initially, the hypertrophic response may serve to maintain cardiac function; however, prolonged hypertrophy becomes detrimental, resulting in cardiac dysfunction and heart failure via mechanisms similar to those operating under pressure overload as explained above. Overall, the RV tolerates volume overload better than pressure overload and may therefore stay well adapted for extended periods of time. For example, in volume overload associated with left-to-right shunt, the condition may remain relatively asymptomatic until pulmonary vasculopathy develops and the shunt reverses. In fact, even with established Eisenmenger's pathophysiology, the outcome of these patients is better than that of patients with idiopathic PAH [28–29].

Invasive Assessment of Pulmonary Circulation Hemodynamics

Despite the evolution of noninvasive cardiac imaging, cardiac catheterization remains the gold standard for the assessment of hemodynamic indices of the pulmonary circulation, by directly measuring pressures and indirectly estimating flow. Right heart catheterization confirms the presence of pulmonary hypertension, defines the underlying cause and provides prognostic information. For the measurement of cardiac output, both the thermodilution and Fick methods are reliable in most PAH patients in the absence of severe tricuspid regurgitation. Vasodilator challenge at the time of diagnosis provides prognostic information and aids in therapeutic decision-making [30].

Pulmonary hypertension is defined as an increase in mean pulmonary arterial pressure (PAP) ≥ 25 mm Hg at rest as assessed by right heart catheterization. This value has been widely used in randomized controlled trials and registries of PAH. Recent reevaluation of available data has shown that the normal mean PAP at rest is 14 ± 3 mm Hg, with an upper limit (of normal) of 20 mm Hg [30]; the significance of a mean PAP between 21 and 24 mm Hg is less clear. With regard to the formerly proposed threshold of a mean PAP of 30 mm Hg during exercise, the data to support this as a disease state are much less robust. In fact, healthy individuals can reach much higher PAP values upon exertion [30].

Noninvasive Assessment of Right Ventricular Function

Assessment of the RV is limited by its complex geometry and pronounced trabeculation that limit accurate endocardial visualization. The excellent accuracy and reproducibility of cardiac magnetic resonance imaging (MRI) is well established, making MRI the gold standard

RV Physiology in Health and Disease

Table 3. Echocardiographic parameters for the assessment of RV function

Echocardiographic index	Definition	Normal value	Reference
RVOT-FS, mm	Change in RVOT diameter in diastole and systole	61 ± 13	[27]
RVFAC, %	Change in RV area between end-diastole and end-systole	56 ± 13	[28]
TAPSE, mm	Systolic motion of the lateral portion of the tricuspid ring towards the apex	20 ± 2.8	[29]
RV MPI	Ratio between RV isovolemic time and ejection time	0.28 ± 0.04	[30]
RV dp/dt, mm Hg/s	Rate of rise of RV pressure	>1,000	[31]

FS = Fractional shortening; MPI = myocardial performance index; RVFAC = RV fractional area change; RVOT = right ventricular outflow tract.

technique for quantifying the RV chamber [31]. However, MRI is expensive and is only available in tertiary centers. Thus, echocardiography remains the most widely used modality for the assessment of RV size and function.

Echocardiography

A qualitative hemodynamic evaluation of the RV can be obtained from the parasternal short-axis view. In conditions associated with hemodynamic overload, the crescent RV shape is lost and the septum becomes flat. The LV assumes a nonspherical shape (D shape) that results in impaired LV filling and a decrease in cardiac output [4, 31].

The complex structure of RV does not allow geometrical assumptions on echocardiography; thus, only diameters and areas are used in the echocardiographic assessment of RV size. Determining the RV diameter in the parasternal long-axis view with a perpendicular line on the septum has been proven reproducible and less variable than the RVOT diameter measured in a parasternal shortaxis view [4]. From the same view, the limit of normal RV free wall thickness is 5 mm, above which the ventricle is considered to be hypertrophied [4]. In the apical 4-chamber view, both the long- and short-axis diameters can be measured and the end-systolic and end-diastolic area can be determined. In normal individuals, RV area and midcavity diameter should be smaller than those of the LV, thus allowing a rough visual estimation of RV area. Assessment of the structure and architecture of the RV walls can identify features which suggest a particular etiology, such as RV infarction or arrhythmogenic RV cardiomyopathy. However, visual echocardiographic assessment is an inaccurate basis for identification of functional abnormalities. Novel quantitative echocardiographic techniques may help in more accurate evaluation [4].

The complex shape of the RV cavity also prohibits a quantitative approach to evaluating global RV function. Therefore, alternative parameters have been developed and validated using cardiac MRI and radionuclide ventriculography as a gold standard [32–37] (table 3). Among them, tricuspid annular plane systolic excursion (TAPSE) is most commonly used in clinical practice. TAPSE is easily measured using an M-mode cursor passed through the tricuspid lateral annulus in a 4-chamber view. This parameter measures the extent of systolic motion of the lateral portion of the tricuspid ring towards the apex. It has been reported to exhibit a good correlation with isotope-derived RV ejection fraction [35, 36].

Tissue Doppler imaging (TDI) is a technique that measures myocardial velocities, allowing a quantitative assessment of myocardial function during the entire cardiac cycle. Using TDI, several global and regional parameters such as timing, direction and amplitude of the velocity of the ventricular wall can be determined [38, 39]. The technique is less dependent on chamber geometry, and since no endocardial border definition is needed, it can be used in suboptimal echocardiographic images. Pulsed TDI is simple to use and has high temporal resolution [38, 39]. It is limited by angle dependency and the fact that the sample volume is fixed and does not enable tracking of the whole region of interest. The latter limitation can be overcome with color TDI. Color TDI allows an offline analysis of several myocardial segments during the same cardiac cycle. Sample volumes can be set to follow cardiac motion. Color TDI values represent the median of the velocity spectrum [39, 40].

Doppler myocardial imaging-based techniques allow not only for the evaluation of myocardial velocities but also for extracting myocardial deformation parameters. Strain and strain rate represent deformation and deformation rate, respectively. Strain is defined as deformation of an object compared with its initial shape and is expressed as percentage. Strain rate or deformation rate defines the speed of the deformation. Strain rate correlates well with regional contractility and provides information which is less dependent on RV preload and afterload [40].

Another technique that can be employed for determining regional deformation is speckle tracking-based myocardial deformation imaging. Compared to Doppler techniques, speckle tracking techniques are angle-independent and more user-friendly. On the other hand, they are limited by the need for excellent image quality [41, 42].

Three-dimensional echocardiography could facilitate the study of RV morphology and function overcoming the complexity of RV shape [43, 44]; it can determine volumes and, consequently, ejection fraction accurately without geometrical assumptions. Measurements of RV volumes and RV ejection fraction by real-time 3-dimensional echocardiography have been proved accurate and reproducible when compared with cardiac MRI [43– 46].

Despite promising results, the additive diagnostic or prognostic information that novel echocardiographic techniques may provide in clinical practice remains questionable. Certainly, these techniques need further validation in larger populations and in varied disease settings.

Radionuclide Techniques

Radionuclide techniques were developed and used as the gold standard of RV assessment in the pre-MRI era. They permit the determination of several parameters including ejection fraction, systolic ejection time, peak filling rates, peak ejection fraction and rate of contractility [47]. In radionuclide ventriculography, 99mTc-labeled erythrocytes are injected into the circulation. LV and RV function can be evaluated by first-transit studies (a type of beat-to-beat evaluation) or by gated (ECG-synchronized) blood pool imaging done over several minutes (multiple-gated acquisition). Both studies can be done during rest or after exercise. First-transit studies are fast and relatively easy, but multiple-gated acquisition provides better images and is currently more widely used. In first-transit studies, 8-10 cardiac cycles are imaged as the marker mixes with blood and passes through the central circulation. First-transit studies are ideal for assessing RV function and intracardiac shunts [47-49]. In multi-gated acquisition, imaging is synchronized with the R wave of the ECG. Multiple images are taken. Computer-assisted



Fig. 4. Ventricular contraction and interdependence demonstrated by MRI [adapted from 66, with permission].

analysis generates an average blood pool configuration for each portion of the cardiac cycle and synthesizes the configurations into a continuous cinematic loop resembling a beating heart [47–49].

Magnetic Resonance Imaging

There have been major advances in MRI techniques in the past years including ECG gating and respiratory suppression, diminishing imaging artifacts and allowing automatic trace of RV volumes (fig. 4). The high accuracy and reproducibility of MRI measurements without the need of geometrical assumptions have made cardiac MRI the current gold standard for the study of RV size and function (table 4) [31, 50]. Moreover, using magnetic resonance angiography, a detailed 3-dimensional pulmonary angiogram can be obtained with injection of gadolinium in a peripheral vein allowing a global assessment of the pulmonary circulation.

Early studies using the phase-contrast technique and velocity-encoded MRI showed the feasibility of estimating right-side hemodynamics, but the accessibility and reproducibility of Doppler echocardiography has limited the use of these techniques in clinical practice. Recent advances in magnetic resonance angiography have made it possible to calculate regional quantitative perfusion parameters in the lung on the basis of 3-dimensional contrast-enhanced dynamic MR perfusion and principles of

RV Physiology in Health and Disease

Table 4. Cardiovascular magnetic resonance-derived reference

 values for RV volumes, systolic function and mass

Women, mean ± SD (95% CI)	Men, mean ± SD (95% CI)
48±11 (27, 69)	66±14 (38, 94)
$28 \pm 5 (18, 38)$	$34 \pm 7 (20, 47)$
126 ± 21 (84, 168)	$163 \pm 25 (113, 213)$
$73 \pm 9 (55, 92)$	$83 \pm 12 (60, 106)$
$43 \pm 13 (17, 69)$	$57 \pm 15 (27, 86)$
$25 \pm 7 (12, 38)$	$29 \pm 7 (14, 43)$
83 ± 13 (57, 108)	106 ± 17 (72, 140)
$48 \pm 6 (36, 60)$	$54 \pm 8 (38, 70)$
$66 \pm 6 (54, 78)$	$66 \pm 6 (53, 78)$
	Women, mean \pm SD (95% CI) 48 \pm 11 (27, 69) 28 \pm 5 (18, 38) 126 \pm 21 (84, 168) 73 \pm 9 (55, 92) 43 \pm 13 (17, 69) 25 \pm 7 (12, 38) 83 \pm 13 (57, 108) 48 \pm 6 (36, 60) 66 \pm 6 (54, 78)

BSA = Body surface area; EDV = end-diastolic volume; EF = ejection fraction; ESV = end-systolic volume; SV = stroke volume. Reference values adapted [65].

the indicator dilution theory. Such a direct and quantitative measurement would be desirable in the clinical assessment of PAH patients' response to therapy and could be a valuable end point in clinical trials. Moreover, although the quantification of vascular remodeling by angiography has not been validated in the assessment of PAH, there is no doubt that MRI also possesses the advantage of providing information on RV global function and pulmonary vasculature physiology in a single setting [49–51].

Positron Emission Tomography

Positron emission tomography can quantify glucose uptake. Increased glucose uptake is usually associated with a glycolytic phenotype. A switch from mitochondria-based glucose oxidation to cytoplasm-based glycolysis, even in the absence of hypoxia, is detected in many disease states characterized by increased proliferation and suppressed apoptosis. This has also recently been reported in PAH-associated vascular remodeling [29]. In addition, a switch from fatty acid oxidation to glycolysis characterizes cardiac hypertrophy. It is thus possible that the degree of glucose uptake (as measured by the standardized uptake value of 18F-fluorodeoxy-glucose) might correlate with both the degree of vascular remodeling and RV function in PAH [52].

Prognostic Impact of Right Ventricular Remodeling

Over a century ago, it was hypothesized that left heart failure could affect function of the RV. Inversely, the impact of right heart function on LV performance and clinical outcomes still remains understudied [53]. As already emphasized, RV pressure overload may compromise LV function and lead to the clinical presentation of congestive heart failure. Furthermore, the failing RV is unable to maintain adequate LV preload, leading to the clinical presentation of low-output heart failure [54–55].

Even though RV performance, as assessed with the modalities discussed above, may per se remain a questionable therapeutic target in current clinical practice, it is already considered a strong prognostic clinical marker under various conditions of heart failure. In the setting of PAH, survival correlates inversely with hemodynamic parameters such as mean pulmonary arterial pressure, right atrial pressure and cardiac index [54, 55]. Moreover, treatment of PAH is not translated into better clinical outcomes unless accompanied by a parallel improvement in RV function [31]. More specifically, RV mass and size and right atrial pressure are better correlated with functional status and are better predictors of survival than pulmonary arterial pressure per se [55–57]. Accordingly, functional capacity assessed with the 6-minute walking distance correlates better with RV function than with pulmonary arterial pressure.

In the setting of left heart failure, there is consensus that evidence of RV dysfunction predicts poor outcome. Patients with ischemic cardiomyopathy and low LV ejection fraction who died during a 2-year follow up period had had a worse RV ejection fraction than survivors [58]. Accordingly, in the setting of acute myocardial infarction, it was demonstrated that the presence of a low radionuclide-determined RV ejection fraction, in addition to a low LV ejection fraction, has a $3 \times$ higher association with 1-year mortality than that of poor LV function on its own [59]. In patients with myocarditis, poor RV function as defined by a low TAPSE was associated with a greater likelihood of death or of transplantation than the presence of normal RV function [60]. In idiopathic dilated cardiomyopathy, the RV ejection fraction as assessed by cardiac catheterization was correlated linearly with echocardiographic LV ejection fraction, and emerged in a multivariate analysis as one of the strongest predictors of survival [61]. Multiple other indices of RV size and function have been correlated with the prognosis of patients with dilated cardiomyopathy including echo-derived diastolic RV chamber area and tricuspid annular plane systolic excursion [60–62]. Finally, RV performance has also been associated with better exercise tolerance in patients with advanced heart failure [63]. In fact, RV ejection fraction assessed by radionuclide angiography correlated better with functional capacity than LV ejection fraction [64].

Conclusion

Until recently, the RV received little attention in patients with acquired heart disease. Advances in imaging modalities have recently enabled us to accurately study RV physiology in health and disease. It has become apparent that the function of the RV strongly affects the function of the LV and vice versa. Disappointingly, the improvement in our knowledge in RV physiology has not yet resulted in advances in the clinical management of RV failure; indeed, specific therapeutic options for patients with clinically established RV failure are still scarce and treatment continues to be based on extrapolations from studies on LV failure. However, while awaiting progress in this field, clinicians should not come to think that assessment of RV function is futile. In this regard, it has to be kept in mind that multiple studies have demonstrated, beyond any doubt, that RV function is an important determinant of prognosis in heart failure irrespective of the etiological background. Therefore, RV function has to be considered as an important variable in therapeutic decision-making and should also be assessed as a marker of response to treatment in patients with heart failure.

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