

Transcatheter aortic valve replacement—state of the art and a glimpse to the future: 'the Tailored Approach'

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Transcatheter aortic valve replacement determined a paradigm shift in the treatment of high-risk patients with severe symptomatic aortic valve stenosis. Notwithstanding the impressive results of the first-generation prostheses, a fast-paced technological evolution is taking place to overcome their limitations, in particular the vascular access damage and the paravalvular leak. Nowadays, with the availability of several different devices, the expert operator can select the right prosthesis for the specific anatomical and clinical situation. As 'One does not fit all', the 'Tailored TAVR Approach' we describe will conceivably become the future of this therapy.

The 'state of the art'

The first transcatheter aortic valve replacement (TAVR) was performed by Cribier *et al.*¹ in 2002 in a compassionate case of inoperable patient admitted for cardiogenic shock as a consequence of severe symptomatic aortic valve stenosis. After a long period of technical development, a large amount of literature reported promising results confirming the feasibility of TAVR.²⁻⁹ Since then, about 100, 000 transcatheter valves have been implanted worldwide and this number is sharply increasing. The results of several large multicentre registries, 10-18 and some randomized controlled trials, ¹⁹⁻²² consistently showed that TAVR should appropriately be considered the standard of care for high or prohibitive surgical risk patients with severe symptomatic aortic stenosis. The recently published randomized CoreValve US High Risk Pivotal Trial²² was the first to demonstrate a significantly higher rate of survival at 1 year with TAVR compared with surgical aortic valve replacement (SAVR) in high- risk patients. More recent publications²³⁻ ²⁵ have shown by propensity score matching no difference in terms of mortality even in lower-risk patients. These groundbreaking results achieved in the last decade are consequences of the progressive technological improvement of the devices and of operator's experience. The size of the valves and delivery systems has decreased from 24-25 Fr to the current 14-18 Fr, thus increasing the deliverability through the femoral route and reducing the access complication rate. On the other hand, the accurate sizing and procedure planning obtained with the routine use of CT scan allowed the physicians to choose the optimal approach and to minimize the paravalvular leak rate that, however, remains the major Achille's heel of this procedure.

Limitations and complications of first-generation devices

The first phase of TAVR was characterized by a high rate of peri-procedural complications that deeply affect the survival.¹³⁻¹⁹ The main issues were vascular complications, conduction disturbances, paravalvular leaks, stroke, coronary occlusion, and annular rupture.

Vascular complications

Vascular complications have been minimized by the technique of main access protection via the contralateral access as well as by the significant downsize of the delivery systems and devices. $^{10-25}$

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Conduction disturbances

Although generally considered benign, conduction disturbances may portend significant clinical and economic effects, in particular when leading to the implantation of a permanent pacemaker (PM) or to the development of permanent atrial fibrillation.

Left bundle branch block

The main cause of left bundle branch block (LBBB) after TAVR is presumed to be the mechanical compression exerted on the atrioventricular conduction tissue. A persistent LBBB has been associated with a worse outcome in one study,²⁶ whereas in two large multicentre registries with Edwards SAPIEN²⁷ or CoreValve²⁸ this association has been denied. However, the persistence of an LBBB has been consistently associated with a higher incidence of advanced atrioventricular (AV) block requiring a PM implantation.²⁷⁻²⁹

Atrioventricular block and permanent pacemaker implantation

A high-degree atrioventricular block is reported after CoreValve implantation in 14-44% of the cases, while in up to 12% after Edwards SAPIEN implantation.³⁰ These figures are consistent with the subsequent rate of PM implantation of 18-49% for CoreValve and 0-12% after Edwards SAPIEN implantation.^{31,32} Although generally considered a minor issue, PM implantation not only implies an additional intervention that is not free from complications per se, but may also have effects on long-term cardiac function as a consequence of left-to-right ventricle dyssynchrony. The latter will become an issue when TAVR technology will be adopted for younger and lower risk patients. On the other hand, it is well known that the rate of long-term PM dependency is overtly lower than the number of the PMs implanted for an acute high-degree AV block. 33-35 Clearcut guidelines specifically addressing the topic of PM implantation in the setting of TAVR do not exist; however, the common practice is to leave a temporary pace maker for the first 24-48 h post-TAVR and then evaluate on a case-by-case level the risk-benefit ratio of implanting a permanent PM. Being such a lowest risk procedure, it is conceivable that, especially in the early phase of the TAVR experiences, PM has been cautiously implanted in a large number of cases.

Paravalvular leaks: causes and evolution

Multiple studies have reported the frequency and severity of paravalvular leak (PVL) after TAVR.³⁶ There is, however, significant heterogeneity that is caused by differences in: (i) imaging modalities (transthoracic echocardiography, transoesophageal echocardiography, and angiography); (ii) timing of assessment (immediately after implantation, before discharge, and at 30 days); (iii) transcatheter heart valve (THV) system; (iv) grading scale, and (v) adjudication of events. Paravalvular leak tends to be stable over time and in some cases, it can even improve.³⁶

Although it was generally believed that only moderate or severe regurgitation would impact long-term outcomes,

the 2-year results from the PARTNER trial showed that even mild PVL was associated with significant mortality. $^{\rm 37}$

In general, first-generation prostheses were associated with a higher rate of PVL, especially the CoreValve; secondgeneration valves have been designed yet to overcome this issue. Of note, large data directly comparing first vs. second generation are still lacking.

Stroke and cerebrovascular accident

The risk of cerebrovascular accident (CVA) is inherently related to both patient-based and procedure-related risks. The variability of CVA rates among studies might be due to study design, sample size, methodology, and patient- and site-specific factors, as well as different event ascertainment and definitions.³⁸

In a recent meta-analysis, the early stroke rate (< 30 days) was as low as 2.9% and CVA rates did not differ significantly according to the valve type (SAPIEN 2.9% vs. CoreValve 3.6%, P = not significant).³⁹ The time distribution of strokes is inherently correlated with the underlying pathophysiology. Strokes occurring in the acute (<24 h) and subacute early (<30 days) post-TAVR period are strongly related to procedural factors, whereas late events (1-12 months) are mostly connected to patient and disease factors.³⁸ Cerebral protection devices have been developed and designed to fit the aortic arch or the anonymous and common carotid arteries: these devices have been developed to avert cerebral embolism either by filtration (Claret Montage Device, Claret Medical, Inc., Santa Rosa, CA, USA; and EMBOL-X, Edwards Lifesciences) or by diversion (Embrella Embolic Deflector, Edwards Lifesciences; and TriGuard Cerebral Protection Device, Keystone Heart, Caeserea, Israel) of debris away from the cerebral circulation while maintaining normal cerebral perfusion. Safety, feasibility, and efficacy are currently being tested in ongoing trials.

Antithrombotic treatment is believed to be a cornerstone for the prevention of ischaemic CVAs during and after TAVR. Although TAVR procedures have been performed for more than a decade, little is known about optimal antiplatelet and anticoagulation therapy and recommendations are based over consensus. Thus, there is an unmet need for better antithrombotic therapies, given the fact that major stroke rate has not declined significantly over time.⁴⁰⁻⁴²

Coronary occlusion

Coronary occlusion is a very rare although ominous complication of TAVR with a mortality rate as high as 50%. ^{19,20,22} It is a consequence of the obstruction of coronary ostia by the frame of the prosthesis and immediate countermeasures (snaring of the valve or percutaneous coronary intervention of the coronary ostium) must be performed to restore adequate coronary flow. This complication is far more common during the 'valve-in-valve' procedure, as described in the appropriate section.

Annular rupture/left ventricular outflow tract rupture/periaortic haematoma

According to recent data, this complication happens cumulatively in 1.1.% of the cases. 39



Figure 1 Currently available and under development transcatheter valves. (A) Medtronic Evolut (Medtronic, Inc., Minneapolis, MN, USA). (B) SAPIEN 3 (Edwards Lifesciences, Irvine, CA, USA). (C) Lotus Medical (Boston Scientific Corporation, Natick, MA, USA) valve. (D) Direct Flow Medical valve (Direct Flow Medical, Santa Rosa, CA, USA). (E) Symetis Accurate (Symetis SA, Lausanne, Switzerland) valve. (F) Portico (St Jude Medical, St Paul, MN, USA) valve. (G) Centera (Edwards Lifesciences). (H) Engager (Medtronic, Inc.) transapical valve. (I) Transapical JenaValve (JenaValve Technology, Munich, Germany).

Possible predictors are the presence of moderate/severe left ventricular outflow tract (LVOT) calcification and the significant oversize of the prosthesis.⁴³ This mechanical complication is obviously able to acutely worsen the haemodynamic conditions with a very high mortality rate, in particular when the rupture is uncontained.⁴³ Conversion to surgery is almost always required as the only life-saving option.⁴³

Next (and current) generation of transcatheter valves

From the first quarter of 2014, a new generation of transcatheter valves (*Figure 1*) has CE mark approval for clinical use in Europe and under scrutiny for FDA approval in the USA. These new valves aim to overcome or to reduce the major limitations of first-generation valves (Edwards XT and Corevalve) as PVL, vascular complications, cardiac rhythm disturbances, and stroke.

Medtronic Evolut R

The CoreValve Evolut R (*Figure 1*) is designed to be recaptured up to the 80% of the deployment and repositioned during implant, for a maximum of two times. Evolut R has been available since the fourth quarter of 2014 and very

few clinical data are available. In a CE study of 60 patients, Evolut R showed excellent procedural and 30-day outcomes and strong safety profile (0% mortality rate).⁴⁴

Edwards SAPIEN 3

The Edwards SAPIEN 3 (*Figure 1*) is the last evolution of balloon expandable valves and it has been available since the first quarter of 2014. An important new feature of this valve is the presence of a skirt surrounding the distal part of the stent frame to reduce the PVLs with a better contact with calcifications. Recently, at ACC meeting held in San Diego on March 2015, Kodali presented 30-day results of S3 implant in high- and intermediate-risk patients. The rates of mortality and stroke were very low in both populations.⁴⁵ PARTNER 2 randomized trial is enrolled and it will compare S3 results vs. surgical results in intermediate-risk profile.

Boston (BSI) Lotus

The LotusTM device (*Figure 1*) is a transcatheter valve system designed to be released retrogradely. The major advantages of this system are the possibility of a complete resheathing until the valve is released and the presence of the outer adaptive membrane facilitating the contact with the native valve, compensating the anatomical variations

and minimizing the PVL. The bulky delivery system is the major disadvantage of Lotus, but in the fourth quarter 2015 the new trackable and lower profile delivery system will be available. In the REPRISE II CE Mark Study, 6-month mortality rate was 8.4%, and Pace Maker rate 29.4%. In this study, only 1% of patients had more than mild PV regurgitation and no severe aortic regurgitation was reported. At EuroPCR 2015, Van Mieghem presented the first 250 Interim analysis of RESPOND Post Market Safety and Performance Study. All-cause mortality rate was 2.0%, stroke 3.3%, and no moderate or severe aortic regurgitation was reported.^{46,47}

Saint Jude Portico

The Portico valve (*Figure 1*) can be fully recaptured, retrieved, and repositioned until 80–90% of deployment. The acute and 1-year results after implantation of the Portico valve were presented by G. Manoharan at PCR and TCT 2014: 103 high-risk patients were treated. The 1-year mortality rate was 8.7%, stroke rate 3.9%, PM implantation rate 10.7%, and moderate/severe aortic regurgitation 11.7%.⁴⁸ An European post-market registry (PORTICOI) and a prospective randomized study for FDA approval in the USA are ongoing.

Direct Flow

The Direct Flow Medical Transcatheter Aortic Valve System (*Figure 1*) is designed to be fully repositionable and retrievable prior to final deployment, but it cannot be resheathed. Schofer *et al.*⁴⁹ published in 2014 the non-randomized multicentre DISCOVER CE trial. There was 99% freedom from all-cause mortality at 30 days (primary endpoint). VARC criteria defined that 30-day combined freedom from patient safety event rate was 91% and overall device success rate was 93%. The same author presented at EuroPCR 2014 the 1-year results of this trial that confirmed the safety and efficacy of this valve. The survival rate at 1 year was 90% with no more than mild aortic regurgitation and 17% PM rate. The IDE trial SALUS in the USA is ongoing for FDA approval.

Symetis Acurate Neo

The system consists of two components: the bioprosthetic aortic valve Acurate Neo (*Figure 1*) and a disposable delivery system, the Acurate TFTM System. The transapical CE mark trial that was conducted between 2009 and 2011 in 90 patients achieved 80% 1-year survival rate,⁵⁰ and recently, the transfemoral valve received the CE mark after the accurate TF CE mark trial that achieved 3.4% 30-day morality rate, 2.2% stroke, 9.0% PM rate, and only 4.9% \geq grade 2 paravalvular leak.⁵¹

The 'Tailored Approach'

These second-generation valves associated with the increasing experience of operators are leading to a dramatic improvement in the results and to a simplification of the procedure that is now safer and more predictable. An overview of studies reporting 30-day results of first-generation

	CoreValve ²² (US Pivotal Extreme Risk)	SAPIEN (PARTNER) ²⁰	SAPIENT 21 (PARTNER 1)	SAPIEN 3 58	Direct Flow 66	Lotus Valve 52	Portico 63
Jeath (%)	7.9	5.0	3.5	2.1	1.3	4.2	2.9
Stroke (disturbing) (%)	2.4	5.0	5.2	0.0	4.0	1.7	2.9
Vew pacemaker (%)	22.2	3.4	5.4	12.5	17.0	28.6	9.8
MI (%)	1.5	0.0	1.6	2.1	1.3	3.3	2.0
Wajor vascular complications (%)	6.3	16.2	9.6	5.2	2.7	2.5	3.9
Disabling bleeding (%)	11.7	16.8	7.8	2.1	2.7	5.0	3.9
Wean gradient (mmHg)	8.5	11	10	10.7	12.5	11.5	8.7
oVL (moderate/severe) (%)	11.5	11.8	24.2	2.5	2.0	1.0	3.0
A comparison between first- and sec PVL, paravalvular leak; MI, myocardi	ond-generation transcatheter valves. ial infarction.						



Figure 2 (A) Horizontal aorta frequently leads to challenging implantation, mostly due to inadequate coaxiality between the device shaft and the aorta/ventricle axis. (B) Optimal result after SAPIEN 3 implantation.



Figure 3 (A) Aortic annulus in the heavy calcified bicuspid valve. (B) Final result after Lotus valve implantation; its adaptive seal ensures good sealing even in such challenging anatomy. (C) Extremely eccentric annulus with diffuse calcifications in the bicuspid aortic valve. (D) Moderate paravalvular leak (arrows) after CoreValve implantation. (E) Incomplete valve expansion due to severe calcifications.

vs. second-generation valves is reported in *Table 1*. There is evidence of reduction in terms of death rate, PVL, and bleeding complications. The major advantage in terms of efficacy was reached by the new devices in reducing the degree of aortic regurgitation due to the PVL. Any further improvement in the results largely relies on the possibility to individualize the treatment. Every patient shows peculiar clinical and anatomical features that can significantly affect the overall result of the TAVR procedure. Thus, the selection of the proper device requires the knowledge of



Figure 4 (A) Severe aortic regurgitation. (B) Final result with Lotus valve, showing no paravalvular leak. (C) Arrows showing severe aortic regurgitation. (D) No paravalvular leak after the Direct Flow valve.

the different available prostheses as well as a clear understanding of the behaviour of that specific device in that specific situation.

In other words, 'One does not fit all'. We thus hereby describe how to select the appropriate device for different clinical and/or anatomical situations that are common in the real world.

Small, tortuous, diseased peripheral arteries

Femoral access portends the best long-term results, thus the possibility to use that approach with a low-profile device with adequate trackability is of extreme value. In case of tor-tuous or diseased ilio-femoral axes, Evolut R and Sapien 3 valves seem to ensure the best chance of optimal safety.

Tortuous, Porcelain aorta

In this setting, self-expandable devices with low-profile and good trackability should be preferred: Evolut R, Portico, and Symetis. On the other hand, the use of stiffer devices such as the currently available Lotus is contraindicated.

Horizontal aorta

This setting is associated with a high risk of malapposition, inadequate coaxiality, and subsequent PVL. Thus, devices with very good handling of the tip, perhaps a steerable tip such as in the case of Sapien 3 (*Figure 2*), may be the optimal solution. Valid alternatives are the Direct Flow or the Symetis valves. The Lotus valve has also a good performance in this setting.

Bicuspid/extremely eccentric aortic valve annulus

Bicuspid aortic valve has always been a challenging situation, and often misdiagnosed and thus managed in improper way. An extremely eccentric annulus, diffuse calcifications, and the frequent coexistence of aortic regurgitation make the bicuspid aortic valve a very peculiar setting in which the Lotus device, when slightly undersized, with its adaptive seal seems to be the best option (*Figure 3*). When the Lotus is not available, the suprannular function of the Evolut R is the only acceptable alternative although results are suboptimal (*Figure 3*).

Heavy calcifications: diffuse, aortic valve, left ventricle outflow tract

This condition is a frequent challenge where the selfexpandable prostheses may have suboptimal results for the insufficient adherence of the frame to the calcific nodules which can also determine a deformation of the frame stent itself. Nevertheless, a balloon expandable prosthesis poses a higher risk of annulus rupture. As in the bicuspid aortic valve, the conformability of the Lotus



Figure 5 (A) Stented bioprostheses and severe stenosis. (B) Evolut R final result; its suprannular position is indicated in stented valves. (C) Stentless bioprostheses with severe aortic regurgitation (arrow). (D) Final result with Portico; due to high risk of coronary occlusion, left main protection technique is advisable.

valve, as it can be adapted to the irregular shape of the valve, LVOT and aortic root, may ensure the best results

Pure aortic regurgitation

Previous experience^{52,53} are limited and aortic regurgitation is still off label. There are technical issues related to the poor anchoring of the prosthesis in the absence of calcification and to the common presence of very large annuli. The treatment of a pure aortic regurgitation is characterized by a higher incidence of PVL when compared with the stenosis, and a high incidence of 'valve in valve'.^{52,53} In this setting, the use of balloon expandable seems inadequate as a consequence of the poor fixation of the device.

On the other hand, we observed good results with oversized Direct Flow and Lotus (*Figure 4*) with respect to the manufacturers' indications. Transapical Jena Valve and Engager have interesting features for these indications, but are currently not available.

Valve in valve for degenerated surgical bioprostheses

The widespread use of surgical bioprostheses has determined an increasing rate of failed bioprostheses over time. As a consequence of the high risk of comorbidity/ mortality of a surgical redo, the indication to TAVR is expanding sharply^{54,55} This is a completely different setting when compared with the diseased native aortic valve and every surgical prosthesis has its own features and poses specific procedural issues. In this setting, the risk of acute coronary occlusion is much higher than that in the native aortic valve treatment and it appears to be related with specific bioprosthesis. The residual valve orifice and gradient are the predictors of mortality at follow-up. Both corevalve revalving system and ESV showed to be safe and effective, thus it is conceivable that their evolution such as the Evolut R and the Sapien 3 could be the devices of choice. Perhaps, in small annuli, the Evolut R should be preferred because of its suprannular position (Figure 5). Very good alternatives are the Portico valve as being retrievable, and having large frame cells that allow a good coronary access: despite being intrannular, the residual gradient is usually acceptable. In the case of a high risk of coronary occlusion, the use of a coronary protection technique is advisable.

Low ejection fraction/severe hypertrophy

In these settings, the risk of PVL must be minimized as patients do not tolerate suboptimal results. Thus, the devices that showed the lowest percentage of PVL, namely, Lotus, Sapien 3, and DFM could be the devices of choice. However, Lotus has some limitations regarding the LV size/ hypertrophy, Sapien 3 requires rapid pacing that can harm patients with low-flow, low-gradient condition, and the DFM has limitations regarding small annuli as they are prone to determine significant gradients.

Conclusions

Over the years, operators gradually developed the necessary experience to safely perform the procedure and rapidly manage possible complications. Meticulous riskstratification and accurate procedural planning with the necessary imaging modalities should always be performed as they were pivotal for the observed groundbreaking results of TAVR. In the upcoming 5 years, the results from randomized trials and large registries with the new devices, the awaited long-term durability data, and the expected further downsizing of the vascular access sheaths will definitely lead to an even safer and more predictable procedure: in the long term, this will be an essential requirement to challenge the TAVR procedure against surgical aortic valve replacement in lower-risk patients.

On the other hand, as the 'perfect transcatheter aortic valve prosthesis' does not exist, the very next future of the TAVR will be the 'Tailored TAVR Approach', i.e. an individualized treatment that will take into account all the clinical and anatomical features that an operator can face during its daily practice. It requires a deep knowledge of the different available devices and enough experience to master the TAVR procedure with all of them: 'One does not fit all'.

Conflict of interest: F.B. is medical proctor for Medtronic, St Jude and Boston Scientific. N.B. is medical proctor for Boston Scientific.

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